

The Role of Dynamic Contrast-Enhanced Magnetic Resonance Imaging in Predicting Treatment Response for Cervical Cancer Treated with Concurrent Chemoradiotherapy

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Purpose: To evaluate the role of dynamic contrast-enhanced magnetic resonance imaging (DCE-MRI) in predicting early treatment response.

Materials and Methods: Patients with locally advanced cervical cancer (LACC) treated with concurrent chemoradiotherapy (CCRT) were enrolled. Pelvic DCE-MRI scans were performed before RT (pre-RT), in the middle of RT (mid-RT), and at the end of RT (post-RT), separately. Parameters (ie, K^{trans} , K_{ep} , and V_e) were measured. Pre-, mid-, and post-RT K^{trans} were denoted as K^{trans} -preTx, K^{trans} -midTx, and K^{trans} -postTx, respectively. And the same denoting rule also went for K_{ep} and V_e . Difference for the same parameter such as K^{trans} measured between two consecutive time points was calculated as second K^{trans} value minus first K^{trans} value. The differences in K^{trans} between pre-RT and post-RT, between pre-RT and mid-RT, and between mid-RT and post-RT were denoted as ΔK^{trans} -post-preTx, ΔK^{trans} -mid-preTx, and ΔK^{trans} -post-midTx, respectively, and the same denoting rule was also applied to K_{ep} and V_e .

Results: A total of 57 patients were enrolled. After the treatment, 31 patients had complete response (CR group). The remaining 26 patients had partial response (NCR group). Significant differences were found in K^{trans} -postTx, K_{ep} -postTx, V_e -midTx, ΔK^{trans} -post-preTx, ΔK^{trans} -post-midTx, ΔK_{ep} -post-preTx, ΔK_{ep} -mid-preTx and ΔK_{ep} -post-midTx between the two groups. Receiver operating characteristic (ROC) analysis for their performances in predicting treatment response showed an area under curve (AUC) of 0.656–0.849, sensitivity of 61.3–93.5%, specificity of 46.1–73.1%, and maximal Youden Index of 36.5–66.6. Among those parameters, K_{ep} -postTx was the best, and its AUC, sensitivity, specificity, maximal Youden Index, and cutoff value were 0.849, 87.1%, 73.1%, 60.2, and 0.341, respectively. These combined parameters showed an AUC of 0.952, with sensitivity of 87.1%, specificity of 96.1%, and maximal Youden Index of 83.2.

Conclusion: DCE-MRI parameters can predict early treatment outcome. Among those parameters, K_{ep} -postTx is the best predictor. The combination of multi-parameters can increase the predictive potency.

Keywords: cervical cancer, locally advanced disease, dynamic contrast-enhanced magnetic resonance imaging, concurrent chemoradiotherapy, prognosis prediction

Introduction

Cervical cancer is one of the most common malignancies for females. Worldwide, the incidence of cervical cancer is ranked as the fourth disease among female malignancies, with new cases of about 530,000 and 270,000 deaths annually.

Approximately, 85% of cervical cancer patients are found in less developed and developing countries, and countries with low-income and moderate-income, the mortality rate is 18 times higher than that in rich countries.^{1,2}

In the management of cervical cancer, early assessment and prediction of treatment response may facilitate the modification of treatment strategy in order to improve treatment outcome and minimize side effects. A retrospective study conducted by Li and colleagues found that in cervical cancer patients treated with neoadjuvant chemotherapy, responders had a significantly higher disease-free survival than non-responders, and both univariable and multivariable analyses revealed that treatment response was an independent factor to predict long-term survival. A following prospective study by the same research team confirmed the findings.³ However, traditional imaging techniques like computed tomography (CT) and magnetic resonance imaging (MRI) assess the treatment response or disease progression largely based on changes in morphology and dimension. It is a commonly held belief that changes in morphology often lag behind the changes in biology and molecule, thus they are unlikely to reflect the real anti-tumor effects. In addition, different portion within a tumor may respond to a certain treatment differently due to the heterogeneity present in the tumor. Therefore, there is an urgent need to find out more reliable imaging biomarkers capable of assessing early treatment response.⁴⁻⁶

The vasculature system in tumor presents with apparent abnormality comparing with the normal tissues. In addition, anti-tumor treatment can also change the tumor vasculature system. Therefore, growing attentions have been paid to imaging biomarkers capable of evaluating the function of tumor vasculature system. In comparison with traditional imaging methods, imaging biomarkers are considered non-invasive to evaluate the tumor vasculature system. They can be performed in both vivo and longitudinal settings. Currently, functional imaging to evaluate angiogenesis includes dynamic contrast-enhanced magnetic resonance imaging (DCE-MRI), positron emission tomography (PET), and diffusion-weighted imaging (DWI). Each technique has its own advantages and disadvantages regarding sensitivity, accessibility, reproducibility, and measuring range.

At present, DCE-MRI, as one of most important imaging tools, has been used in cancer diagnosis and differentiation, staging, outcome assessment, and prediction of

recurrence and metastasis for various cancer types, including head-and-neck cancer, breast cancer, and esophagus cancer.⁷⁻⁹ However, few studies are specifically focused on cervical cancer, and the sample sizes are often too small. This prospective study was conducted to evaluate the role of DCE-MRI parameters in assessing and predicting early treatment response, and to provide evidence for individualized approach for cervical cancer patients treated with concurrent chemoradiotherapy (CCRT).

Materials and Methods

Inclusion Criteria

Ages between 18 and 75 years old; histologically proven and newly diagnosed cervical squamous carcinoma or adenocarcinoma; stages between IB2-IVA according to the FIGO Staging System (version 2014); performance status (PS) 0-2; measurable lesion according to the RECIST criteria; no distant metastases confirmed by abdominal ultrasound, chest CT, and bone emission computed tomography (ECT); white blood cell count $\geq 4.0 \times 10^9$ /L, platelet count $\geq 100 \times 10^9$ /L; normal prothrombin time; measuring values of liver and renal functions ≤ 1.25 x upper normal limits. The study was approved by the Institutional Review Board of the People's Hospital of Guangxi Zhuang Autonomous Region and complied with the Declaration of Helsinki. All patients were required to sign a written informed consent prior to the initiation of the study.

Exclusion Criteria

Distant metastases upon diagnosis; coexistence of other malignance; preceding treatment with anti-tumor therapies; contraindication to RT or chemotherapy, including severe infection, myocardial infarct, severe arrhythmia, severe cerebrovascular disease, mental disorder, and uncontrolled diabetes; lactating or pregnant women.

External Beam Radiotherapy

Ninety minutes before CT simulation and each subsequent treatment, patients were asked to empty their rectum and bladder, and then drink 500 mL of water and hold urine. During the simulation, patients were required to lie down on a wide-bore CT simulator couch (Somatom Sensation Open, Siemens Medical Solutions, Erlangen, Germany) in a prone position with two arms crossed upward and holding contralateral elbow. Tailored thoracoabdominal thermoplastic masks were designed to cover the scanning area

(from upper abdomen to upper third of thigh). Radiopaque markers were placed on the edge of anus and vaginal orifice. Intravenous contrast-enhanced CT using 4 mm slice from the upper border of the L1 vertebral to 2 cm below the ischial tuberosity was performed for planning. Scanning range was extended to 4 cm below the vulva if the whole length of vagina or inguinal lymph node was involved.

Gross tumor volume (GTV) was defined as any primary disease and involved lymphadenopathy, determined by imaging and clinical findings. There were 3 clinical target volumes (CTV1, CTV2, and CTV3): CTV1 included GTV, uterus, and cervix; CTV2 included parametrial and paravaginal tissues, ovaries, and vagina according to the involvement (ie, upper half if no vagina involvement or only slight involvement; upper two-thirds if upper vagina involvement; or entire vagina if more vagina involvement); CTV3 included common iliac, internal iliac, external iliac and presacral lymph nodes. Planning target volumes (ie, PTV1, PTV2, and PTV3, respectively) were formed by adding 5–10 mm margins to CTV1, CTV2, and CTV3 in three-dimensions. The plans were designed and optimized using the Pinnacle inverse planning system. The prescribed radiation dose delivered to PTV1, PTV2, and PTV3 was 50–54 Gy, 45–48.6 Gy, and 45–48.6 Gy, respectively, in 25–27 fractions. A boost dose was added to the positive pelvic lymph node to ensure the total dose reached 60 Gy. IMRT was delivered via 5 or 7 fixed-gantry angles with an Elekta Synergy Linear Accelerator (Elekta Ltd., Stockholm, Sweden). Verification based on cone beam computed tomography (CBCT) or electronic portal imaging device (EPID) was required before treatment was initiated. This was done prior to the first treatment and every week thereafter. If CBCT was used, consecutive verifications were performed for the first five fractions, and if the setup error was not significant, weekly verification was considered appropriate.

Intracavitary Brachytherapy

High-risk CTV (HR-CTV) included any macroscopic tumor found in imaging studies and examination. Intermediate risk CTV (IR-CTV) included significant microscopic disease and initial tumor extension before external beam RT. Doses to HR-CTV and IR-CTV were assessed by D_{90} and D_{100} (minimal doses received by 90% and 100% of volumes, respectively). High-dose volume was assessed by V_{150} and V_{200} (volumes receiving 150%

and 200% of prescribed doses, respectively). The doses to organs at risk (OARs) were assessed by $D_{0.1}$, $D_{1\text{ cc}}$, $D_{2\text{ cc}}$, $D_{5\text{ cc}}$, and $D_{10\text{ cc}}$ (maximal doses received by 0.1, 1, 2, 5, and 10 cc volumes, respectively). The fractionation for the high-dose rate brachytherapy was 24 Gy in 4 fractions.

Chemotherapy

Weekly cisplatin (40 mg/m²) or nedaplatin (30 mg/m²) was injected intravenously for 5 weeks. Antiemetic and acid-inhibitor were administered prior to the use of cisplatin.

Pelvic DCE-MRI

Imaging Acquisition of DCE-MRI

Pelvic DCE-MRI scans were performed before RT, in the middle of RT (at third week of RT), and at the end of RT, separately. Conventional high-resolution MRI images were acquired by using 3T superconducting magnetic resonance imager (Tim Trio Siemens 3.0 T) equipped with an eight-channel phased array coil, including sagittal T2WI, axial T2WI, and axial T1WI. Multi-flip angle approach is utilized for a T1 map. DCE-MRI scans were performed after the injection of the contrast. Three-dimensional volumetric interpolated breath-hold sequence was used for quantitative DCE-MRI examination. Scan parameters were as the following: TR, 3.5 ms; TE, 1.06 ms; array, 256×256; FOV, 24 cm×24 cm; slice thickness, 3.0 mm; slice interval, 0 mm; NEX, 1; parallel acquisition, 2 times. Initially, three unenhanced sequences at 5°, 10°, and 15° flip angles were obtained. After the scan was taken to the fifth phase in quantitative DCE-MRI, Gd-DTPA-BMA (Omniscan, Shanghai GE Health, Shanghai, China) was injected at a dosage of 0.1 mmol/kg by a high-pressure spring and retention needle at a speed of 2 mL/s through a previously inserted catheter placed into the antecubital vein and followed by saline flush at a dosage of 0.2 mL/kg at the same speed. Then, 30 phases of consecutive scans were taken, with 22 images and 7.2 seconds each phase. There were 770 images in 35 phases in total.

Image Analysis

The acquired images were measured by using a commercial post-processing software (Siemens Syngo MMWP, Siemens Healthcare, Berlin, Germany). The first step was to align the images in order to minimize the artifacts caused by respiratory motion. Then, the three flip angle images and the aligned images were imported.

The third step was to measure arterial input function (AIF) at the internal iliac artery by using Extended Tofts two-compartment model. Finally, regions of interest (ROI) were drawn by hand by a senior radiologist. T1 map was used to calculate the T1 value for ROI. Parameters in this study included volume transfer constant (K^{trans}), flux rate constant (K_{ep}), and extravascular extracellular space volume fraction (V_e).

ROI Drawing

A maximum section of lesions was selected as the central slice. ROI included the central slice and its nearest upper one and lower one slice. Care was taken to avoid large vessels, cystic or necrotic regions, and regions with bleeding.

Assessment of Treatment Response

Calculations of tumor volume were as the following:¹⁰

The maximum left–right diameter measured on the largest slice in axial T2-weighted MR images was denoted as d1, and the maximum caudo-cranial and anterior-posterior diameters measured on the largest slice in sagittal T2-weighted MR images were denoted as d2 and d3, respectively. Tumor volume was calculated according to the formula: $V = d1 \times d2 \times d3 \times \pi / 6$. The change rate of tumor volume at a certain time point was calculated as the following equation: [(volume prior to treatment-volume at this time point)/volume prior to treatment] $\times 100\%$.

Short-term treatment response was evaluated according to Response Evaluation Criteria in Solid Tumors (RECIST), Version 1.1. Complete response (CR) is defined as disappearance of all target lesions; partial response (PR) is defined as at least a 30% decrease in the sum of diameters of target lesions taking as reference the baseline sum diameters; progressive disease (PD) is defined as at least a 20% increase in the sum of diameters of target lesions or presence of new lesions; and stable disease (SD) is defined as neither sufficient shrinkage to qualify for PR nor sufficient increase to qualify for PD.

Observational Variants

The observational variants were as the following: K^{trans} , K_{ep} , and V_e prior to RT (pre-RT), in the middle of RT (mid-RT), and at the end of RT (post-RT); dynamic changes of the above three parameters; pre-, mid-, and post-RT K^{trans} were denoted as $K^{\text{trans}}\text{-preTx}$, $K^{\text{trans}}\text{-midTx}$, and $K^{\text{trans}}\text{-postTx}$, respectively. Likewise, K_{ep} and V_e were denoted as $K_{\text{ep}}\text{-preTx}$, $K_{\text{ep}}\text{-midTx}$, $K_{\text{ep}}\text{-postTx}$, $V_e\text{-preTx}$, $V_e\text{-midTx}$, and $V_e\text{-postTx}$, respectively.

Difference for the same parameter such as K^{trans} measured between two consecutive time points was calculated as second K^{trans} value-first K^{trans} value. The differences in K^{trans} between pre-RT and post-RT, between pre-RT and mid-RT, and between mid-RT and post-RT were denoted as $\Delta K^{\text{trans}}\text{-post-preTx}$, $\Delta K^{\text{trans}}\text{-mid-preTx}$, and $\Delta K^{\text{trans}}\text{-post-midTx}$, respectively. Likewise, the differences in K_{ep} were denoted as $\Delta K_{\text{ep}}\text{-post-preTx}$, $\Delta K_{\text{ep}}\text{-mid-preTx}$, and $\Delta K_{\text{ep}}\text{-post-midTx}$, respectively, and the differences in V_e were denoted as $\Delta V_e\text{-post-preTx}$, $\Delta V_e\text{-mid-preTx}$, and $\Delta V_e\text{-post-midTx}$, respectively.

Statistical Analysis

SPSS 22 software was used for statistical analysis and a probability value less than 0.05 was considered significant. A paired sample *t* test or Wilcoxon rank sum test was chosen based on the data types. Comparisons of the DCE-MRI parameters at different time points were performed through paired sample *t* test. One-Way ANOVA was used for the comparison of baseline characteristics and the DCE-MRI parameters for patients in the same group. Potential predictors for early treatment response were screened by the binary logistic regression model and their discriminatory power was calculated by Receiver Operating Characteristic Curve (ROC).

Results

Patient Characteristics

Between January 2017 and September 2019, a total of 57 patients were enrolled in the study. The median age was 56 years old, ranging from 36 to 75 years old. After the treatment, 31 patients had CR and those patients were included in the CR group. The remaining 26 patients had PR and those patients were included in the NCR group. The detailed information about patient characteristics is shown in Table 1.

Tumor Volume and Volume Change

The pre-RT tumor volume for all patients was $43.2 \pm 7.5 \text{ cm}^3$. As the treatment proceeded, dramatical volume changes were observed. The mid-RT and post-RT tumor volumes were $23.5 \pm 5.8 \text{ cm}^3$ and $5.7 \pm 4.8 \text{ cm}^3$, respectively. The mid-RT volume was remarkably smaller than the pre-RT volume ($19.7 \pm 6.3 \text{ cm}^3$, 95% CI: 18.0–21.4, $t=23.5$, $p=0.000$). Compared with the pre-RT volume, the post-

Table I Baseline Characteristics of Patients

Parameters	All Pts	CR Group	NCR Group	p value
No. of pts	57	31	26	
Age (yrs) Median (range)	56 (36–75)	57 (38–70)	57 (36–75)	0.458
Histological type (n, %) Squamous cell Adenocarcinoma	51 (89.5) 6 (0.5)	28 (90.3) 3 (9.7)	23 (88.5) 3 (11.5)	0.820
FIGO Stage (n, %) IB2 IIA-IIIB IIIA-IIIB IVA	3 (5.3) 35 (61.4) 17 (29.8) 2 (3.5)	2 (6.4) 23 (74.2) 5 (16.2) 1 (3.2)	1 (3.9) 12 (46.1) 12 (46.1) 1 (3.9)	0.099
Cycles of Chemo (n, %) ≤3 4 5	5 (8.8) 22 (38.6) 30 (52.6)	2 (6.5) 12 (38.7) 17 (54.8)	3 (11.5) 10 (38.5) 13 (50.0)	0.854
PS Score (n, %) 0 I	5 (8.8) 52 (91.2)	3 (9.7) 28 (90.3)	2 (7.7) 24 (92.3)	1.000

RT volume shrank significantly ($38.3 \pm 8.9 \text{ cm}^3$, 95% CI: 35.9–40.7, $t=32.3$, $p=0.000$). Similarly, the post-RT volume was significantly smaller than the mid-RT volume ($18.6 \pm 6.3 \text{ cm}^3$, 95% CI: 16.8–20.4, $t=20.7$, $p=0.000$). Significant differences were also found in the change rate of volume between the two groups. Change rate in mid-RT in the CR group was significantly larger than that in the NCR group ($48.7 \pm 13.7\%$ vs $41.4 \pm 7.4\%$; $p=0.019$; inter-group difference = $7.2 \pm 3.0\%$, 95% CI: 1.2–13.3%). Patients in the CR group had significantly higher change rate of tumor volume after RT than those in the NCR group ($100.0 \pm 0.0\%$ vs $75.4 \pm 5.1\%$; $p=0.000$; inter-group difference = $24.6 \pm 1.0\%$, 95% CI: 22.6–26.7%) **Figure 1** illustrates the tumor volume changes at different time points.

Before RT, patients in both the CR and NCR groups had a similar tumor volume, with values of $43.2 \pm 8.9 \text{ cm}^3$ and $43.2 \pm 5.7 \text{ cm}^3$, respectively ($p=0.975$, 95% CI: -3.99 – 4.12). In mid-RT, a significantly smaller tumor volume was found in patients in the CR group, compared with the NCR group ($22.1 \pm 6.9 \text{ cm}^3$ vs $25.2 \pm 3.7 \text{ cm}^3$; $p=0.046$, 95% CI: -6.11 – 0.58). The difference in tumor volume between the two groups became more evident after RT (0.0 vs $10.7 \pm 2.7 \text{ cm}^3$; $p=0.000$, 95% CI: -11.82 – 9.58).

Changes in DCE-MRI Parameters

The overall changing tendency for K^{trans} and K_{ep} was an increase at first and then a decline to a level that was lower than that before RT. The maximum values were found in mid-RT, but K_{ep} had a larger reduction range than K^{trans} . As for V_e , the overall change pattern was a consistently escalating trend, with a peak occurring in post-RT (**Figure 2**).

For patients in the CR group, $K^{\text{trans}}\text{-preTx}$, $K^{\text{trans}}\text{-midTx}$, and $K^{\text{trans}}\text{-postTx}$ were $0.203 \pm 0.105 \text{ min}^{-1}$, $0.348 \pm 0.282 \text{ min}^{-1}$, and $0.177 \pm 0.166 \text{ min}^{-1}$, respectively. Significant differences were found between pre-RT and mid-RT, and between mid-RT and post-RT; $K_{\text{ep}}\text{-preTx}$, $K_{\text{ep}}\text{-midTx}$, and $K_{\text{ep}}\text{-postTx}$ were $0.549 \pm 0.256 \text{ min}^{-1}$, $0.706 \pm 0.370 \text{ min}^{-1}$ and $0.232 \pm 0.114 \text{ min}^{-1}$, respectively. $V_e\text{-preTx}$, $V_e\text{-midTx}$, and $V_e\text{-postTx}$ were 0.378 ± 0.149 , 0.524 ± 0.214 and 0.695 ± 0.134 , respectively. For both K_{ep} and V_e , significant differences were observed between each time point. **Figure 3** represents the dynamic changes of these parameters through time in a responder.

For patients in the NCR group, $K^{\text{trans}}\text{-preTx}$, $K^{\text{trans}}\text{-midTx}$, and $K^{\text{trans}}\text{-postTx}$ were $0.244 \pm 0.168 \text{ min}^{-1}$, $0.365 \pm 0.234 \text{ min}^{-1}$ and $0.340 \pm 0.173 \text{ min}^{-1}$, respectively. Significant differences were found between pre-RT and

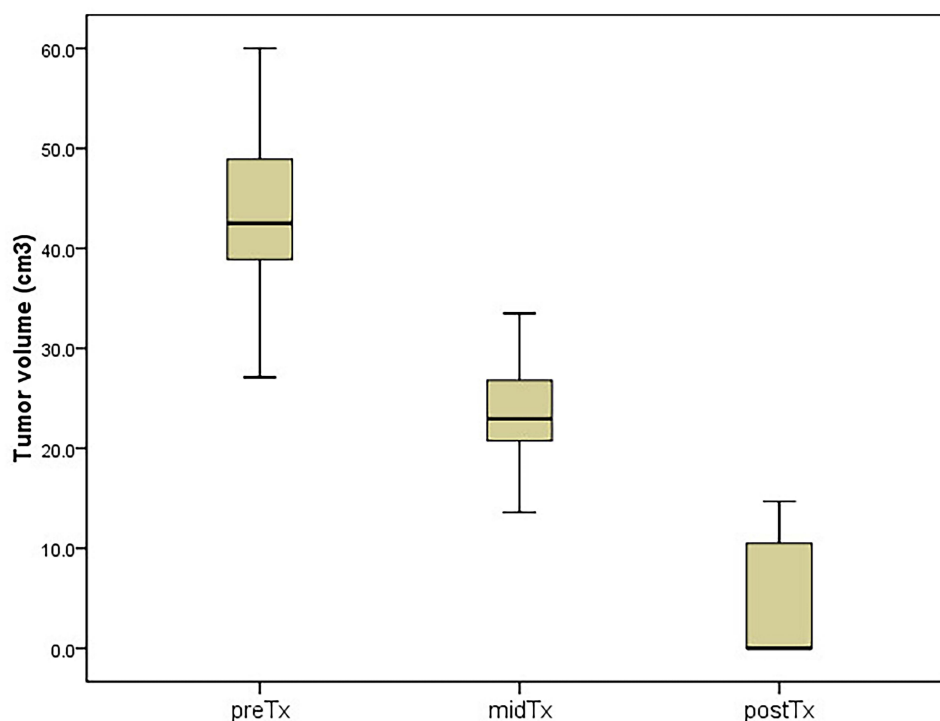


Figure 1 Pre-, mid-, and post-RT tumor volume changes.

mid-RT, and between mid-RT and post-RT; K_{ep} -preTx, K_{ep} -midTx, and K_{ep} -postTx were $0.603 \pm 0.393 \text{ min}^{-1}$, $0.622 \pm 0.410 \text{ min}^{-1}$ and $0.462 \pm 0.205 \text{ min}^{-1}$, respectively. Significant difference was found between mid-RT and post-RT; V_e -preTx, V_e -midTx, and V_e -postTx were 0.409 ± 0.182 , 0.645 ± 0.184 and 0.740 ± 0.169 , respectively. Significant differences were observed between each time point (Table 2). Figure 4 represents the dynamic changes of these parameters through time in a non-responder.

There were significant differences in K^{trans} -postTx, K_{ep} -postTx, V_e -midTx, ΔK^{trans} -mid-preTx, ΔK^{trans} -post-midTx, ΔK_{ep} -post-preTx, ΔK_{ep} -mid-preTx and ΔK_{ep} -post-midTx between the two groups. However, no significant differences were found in K^{trans} -preTx, K^{trans} -midTx, K_{ep} -preTx, K_{ep} -midTx, V_e -preTx, V_e -postTx, ΔK^{trans} -post-preTx, ΔV_e -post-preTx, ΔV_e -mid-preTx and ΔV_e -post-midTx between the two groups (Table 3).

Correlation Between DCE-MRI Parameters and Tumor Volume/Change in Tumor Volume

For all patients, no correlations were found between the pre-RT tumor volume and any DCE-MRI parameter. There was a significant correlation between K^{trans} -preTx and the mid-RT tumor volume ($r=0.277$, $p<0.05$). The

post-RT tumor volume was significantly related to K^{trans} -postTx, K_{ep} -postTx, V_e -midTx, ΔK^{trans} -post-preTx, ΔK^{trans} -post-midTx, ΔK_{ep} -post-preTx, and ΔK_{ep} -post-midTx ($r=0.425$, 0.525 , 0.272 , 0.276 , 0.343 , 0.329 , and 0.412 , respectively; all p values <0.05). The change rates of tumor volumes in the middle of RT (compared with pre-RT tumor volume) were significantly correlated with K^{trans} -preTx, K^{trans} -postTx, K_{ep} -postTx, and V_e -preTx ($r=-0.265$, -0.346 , and -0.267 , respectively; all p values <0.05). The change rates of tumor volumes after RT (compared with pre-RT tumor volume) were significantly correlated with K^{trans} -preTx, K^{trans} -postTx, K_{ep} -postTx, V_e -midTx, ΔK^{trans} -post-preTx, ΔK^{trans} -post-midTx, ΔK_{ep} -post-preTx, and ΔK_{ep} -post-midTx ($r=1.000$, -0.443 , -0.540 , -0.301 , -0.322 , -0.373 , -0.359 , and -0.475 ; all p values <0.05) (Table 4).

Predictive Role of DCE-MRI Parameters and Their Changes in Early Treatment Response

Mann-Whitney test was performed for DCE-MRI parameters at different time points. There were significant differences in K^{trans} -postTx, K_{ep} -postTx, and V_e -midTx between the two groups ($p=0.000$, 0.000 , and 0.039 , respectively), suggesting that the abovementioned

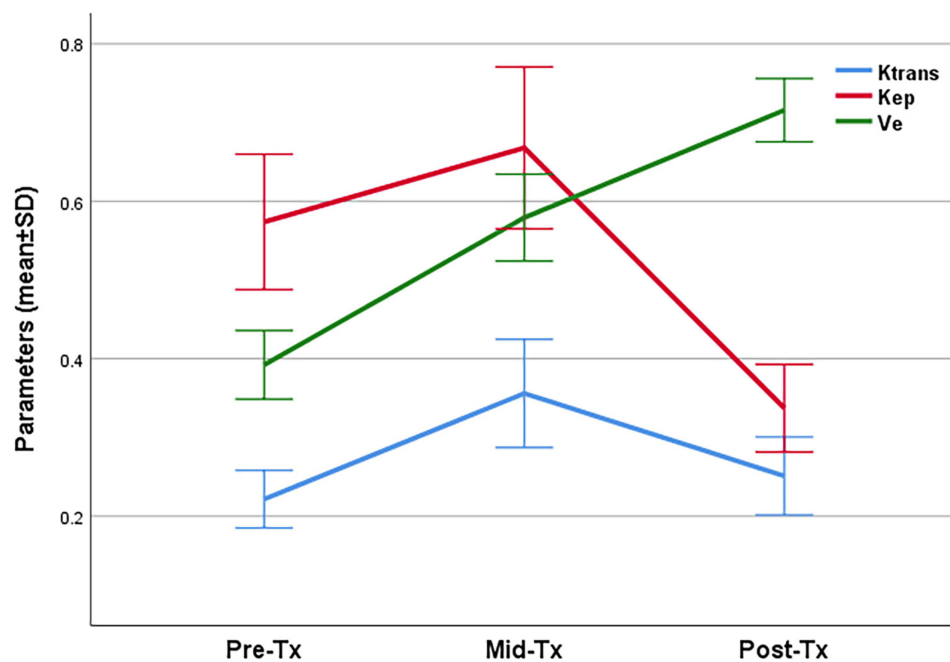


Figure 2 Changes in K^{trans} , K_{ep} , and V_e at different time points.

parameters may have a predictive role in early treatment response. Whereas no significant differences were observed in other parameters, including K^{trans} -preTx, K^{trans} -midTx, K_{ep} -preTx, K_{ep} -midTx, V_e -preTx, and V_e -postTx, between the two groups (Table 3). The performances of K^{trans} -postTx, K_{ep} -postTx, and V_e -midTx in predicting treatment response were assessed by ROC analysis. K^{trans} -postTx showed an area under curve (AUC) of 0.839 (95% CI: 0.718–0.823), with a cutoff value of 0.256, sensitivity of 93.5% (95% CI: 78.6–99.2%), specificity of 73.1% (95% CI: 52.2–88.4%), and maximal Youden Index of 66.6; K_{ep} -postTx showed an AUC of 0.849 (95% CI: 0.729–0.930), with a cutoff value of 0.341, sensitivity of 87.1% (95% CI: 70.2–96.4%), specificity of 73.1% (95% CI: 52.2–88.4%), and maximal Youden Index of 60.2; V_e -midTx showed an AUC of 0.660 (95% CI: 0.523–0.780), with a cutoff value of 0.557, sensitivity of 61.3% (95% CI: 42.2–78.2%), specificity of 76.9% (95% CI: 56.4–91.0%), and maximal Youden Index of 38.2 (Figure 5, Table 5).

There were significant differences in ΔK^{trans} -post-preTx, ΔK^{trans} -post-midTx, ΔK_{ep} -post-preTx, ΔK_{ep} -mid-preTx, and ΔK_{ep} -post-midTx between the two groups ($p=0.004$, 0.011 , 0.044 , 0.014 , and 0.001 , respectively), suggesting that the abovementioned parameters may have a predictive role in early treatment response,

whereas no significant differences were observed in other parameters, including ΔK^{trans} -mid-preTx, ΔV_e -post-preTx, ΔV_e -mid-preTx, and ΔV_e -post-midTx, between the two groups (Table 3). The performances of ΔK^{trans} -post-preTx, ΔK^{trans} -post-midTx, ΔK_{ep} -post-preTx, ΔK_{ep} -mid-preTx, and ΔK_{ep} -post-midTx in predicting treatment response were assessed by ROC analysis. ΔK^{trans} -post-preTx showed an AUC of 0.722 (95% CI: 0.588–0.833), with a cutoff value of -0.016 , sensitivity of 64.5% (95% CI: 45.4–80.8%), specificity of 73.1% (95% CI: 52.2–88.4%), and maximal Youden Index of 37.6; ΔK^{trans} -post-midTx showed an AUC of 0.698 (95% CI: 0.562–0.812), with a cutoff value of 0.003, sensitivity of 90.3% (95% CI: 74.2–98.0%), specificity of 46.1% (95% CI: 26.6–66.6%), and maximal Youden Index of 36.5; ΔK_{ep} -post-preTx showed an AUC of 0.690 (95% CI: 0.553–0.806), with a cutoff value of -0.039 , sensitivity of 83.9% (95% CI: 66.3–94.5%), specificity of 57.7% (95% CI: 36.9–76.6%), and maximal Youden Index of 41.6; ΔK_{ep} -mid-preTx showed an AUC of 0.656 (95% CI: 0.518–0.777), with a cutoff value of 0.044, sensitivity of 74.2% (95% CI: 55.4–88.1%), specificity of 65.4% (95% CI: 44.3–82.8%), and maximal Youden Index of 39.6; ΔK_{ep} -post-midTx showed an AUC of 0.763 (95% CI: 0.632–0.866), with a cutoff value of -0.196 , sensitivity of 80.6% (95% CI:

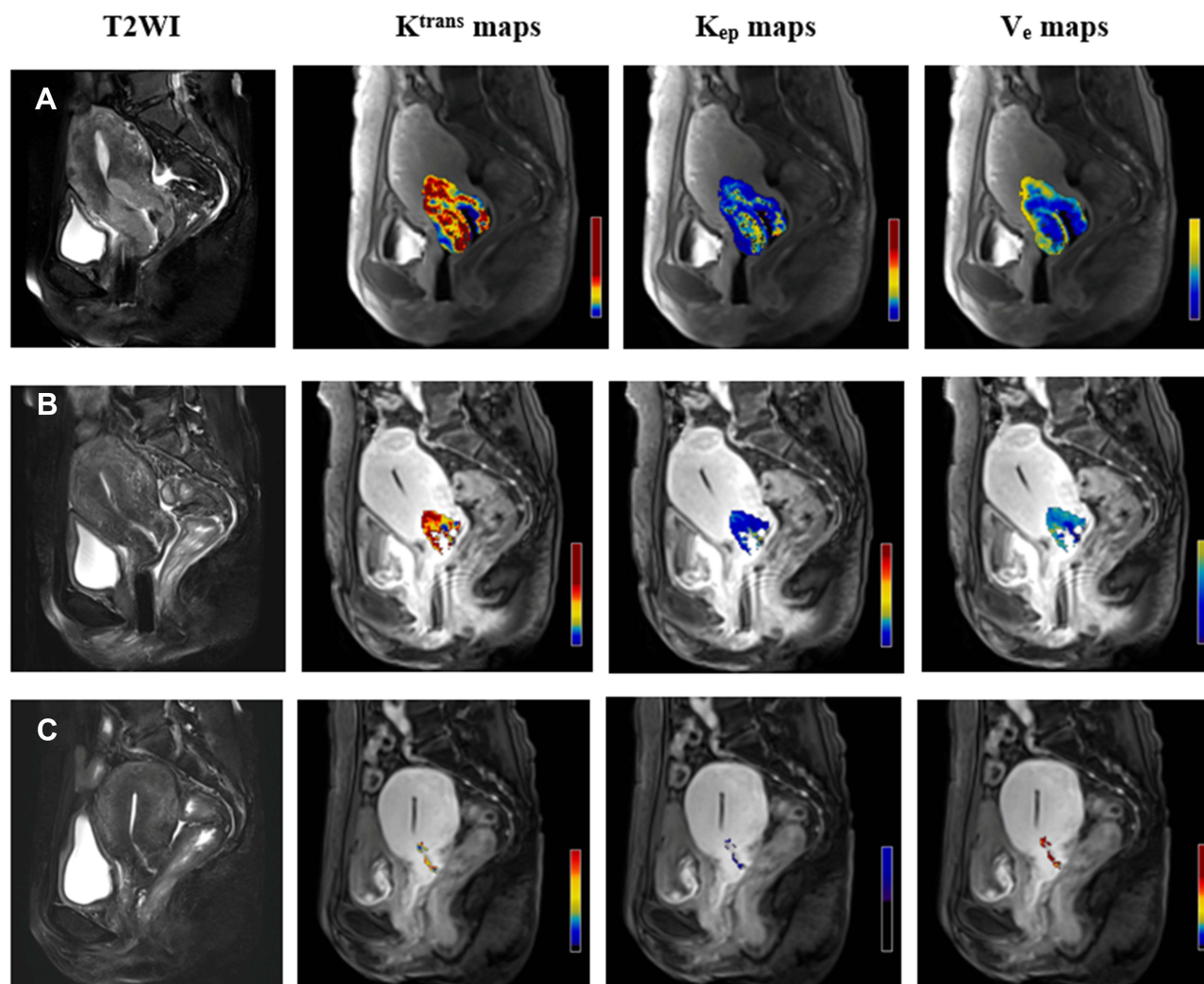


Figure 3 Dynamic changes of DCE-MRI parameters in a responder. Images in each row are representative images from three different timepoints (**A**=pre-RT; **B**=mid-RT; **C**=post-RT) from a 68-year old patient with IIB disease. The images of the primary tumor from T2WI are presented to show volume changes in mid- and post-RT in comparison with the baseline. Corresponding kinetic parameters (K^{trans} , K_{ep} , and V_e maps) of the primary tumor are presented to show permeability changes from the three given timepoints (Pre-, mid-, and post-RT). K^{trans} in pre-, mid-, and post-RT were 1.157 min^{-1} , 1.978 min^{-1} , and 0.367 min^{-1} , respectively; K_{ep} in pre-, mid-, and post-RT were 3.302 min^{-1} , 3.713 min^{-1} , and 0.482 min^{-1} , respectively; V_e in pre-, mid-, and post-RT were 0.411, 0.577, and 0.763, respectively. This patient achieved a complete response after the treatment.

62.5–92.5%), specificity of 61.5% (95% CI: 40.6–79.8%), and maximal Youden Index of 42.2 (Figure 6, Table 5). Logistic regression model was performed to analyze the predictive role of the combined parameters including K^{trans} -postTx, K_{ep} -postTx, V_e -midTx, ΔK^{trans} -post-preTx, ΔK^{trans} -post-midTx, ΔK_{ep} -post-preTx, ΔK_{ep} -mid-preTx, and ΔK_{ep} -post-midTx. It showed an AUC of 0.952 (95% CI: 0.860–0.991), with sensitivity of 87.1% (95% CI: 70.2–96.4%), specificity of 96.1% (95% CI: 80.4–99.9%), and maximal Youden Index of 83.3 (Table 5, Figure 7).

Discussion

CCRT is an effective treatment combination for locally advanced cervical cancer. In the present study, the tumor volume continuously shrank as the treatment proceeded. The volume after RT was significantly smaller than that in mid-RT or pre-RT. Even in mid-RT, the tumor volume remained quite smaller than that in pre-RT. However, for patients who obtained different treatment response, the absolute tumor volumes and their change rates may vary significantly. Both the CR and NCR groups had similar tumor volume in pre-RT. In mid-RT, however, the CR

Table 2 Comparison of DCE-MRI Parameters Within Each Group at Different Time Points

Parameters	CR Group				NCR Group			
	Pre-Tx	Mid-Tx	Post-Tx	p	Pre-Tx	Mid-Tx	Post-Tx	p
K^{trans}	0.203±0.105	0.348±0.282		0.002	0.244±0.168	0.365±0.234		0.014
	0.203±0.105		0.177±0.166	0.398	0.244±0.168		0.340±0.173	0.028
		0.348±0.282	0.177±0.166	0.000		0.365±0.234	0.340±0.173	0.578
K_{ep}	0.549±0.256	0.706±0.370		0.011	0.603±0.393	0.622±0.410		0.826
	0.549±0.256		0.232±0.148	0.000	0.603±0.393		0.462±0.205	0.075
		0.706±0.370	0.232±0.148	0.000		0.622±0.410	0.462±0.205	0.024
V_e	0.378±0.149	0.524±0.214		0.001	0.409±0.182	0.645±0.184		0.000
	0.378±0.149		0.695±0.134	0.000	0.409±0.182		0.740±0.169	0.000
		0.524±0.214	0.695±0.134	0.000		0.645±0.184	0.740±0.169	0.045

group had a significantly smaller volume, compared with the NCR group, and this difference in tumor volume became even more apparent in post-RT. The regression rate of the tumor volume in the CR group was notably higher than that in the NCR group. These findings suggest that patients with CR are more sensitive to chemoradiotherapy. Therefore, they are more likely to achieve a better short-term local/regional tumor control or even a long-term survival benefit. In fact, studies on cervical cancer,^{11,12} small-cell lung cancer,¹³ and gastric cancer¹⁴ have found that patients' prognosis are closely related to the size of residual tumor and the tumor regression rate. Those with less tumor residuals or higher tumor regression rate benefit most in the short-term or long-term outcomes.

The tumor volume and its change were associated with DCE-MRI parameters. K^{trans} -preTx was closely correlated with the tumor regression rates in pre-, mid-, and post-RT; K_{ep} -postTx was closely correlated with the tumor volume in mid-RT, and regression rates in mid- and post-RT; V_e -preTx was closely correlated with the tumor regression rate in mid-RT; V_e -midTx, K^{trans} -postTx, ΔK^{trans} -post-preTx, ΔK^{trans} -post-midTx, ΔK_{ep} -post-preTx, and ΔK_{ep} -post-midTx were closely correlated with the tumor volume in post-RT and the tumor regression rate in post-RT.

So far, numerous studies on DCE-MRI have suggested that its quantitative parameters could be served as potential markers to predict treatment response and long-term survival.^{15,16} K^{trans} is an indicator for tumor blood flow and permeability of the microvasculature and is often used to monitor anti-tumor treatment response. Other

pharmacokinetic parameters such as K_{ep} , and V_e are sometimes used to describe the absorption of low molecular weight gadolinium. V_e is defined as the volume of extravascular extracellular space (EES) per unit volume of tissue, and EES consists of interstitial fluid and connective tissues.¹⁷ It is commonly believed that a higher K^{trans} value is an indicator for increased vascular leakage, whereas an increased vascular leakage represents active angiogenesis. As these parameters can provide different physiological information, when they are combined with other quantified or qualified parameters, they may play a complementary role in assessing treatment response. Since the effectiveness of anti-tumor treatment is often closely related to local blood flow perfusion and angiogenesis, and tumors with higher perfusion and active angiogenesis are more sensitive to chemoradiotherapy. Theoretically, tumors with higher K^{trans} and K_{ep} may have a better prognosis. Several studies on rectal cancer,^{18,19} head-and-neck cancer,^{15,16,20–22} breast cancer,²³ and esophagus cancer²⁴ have found that patients with higher K^{trans} prior to chemoradiotherapy have a favorable prognosis, including pathological response rate, clinical response rate, a long-term survival. However, other studies drew inconsistent or even opposite conclusions.²⁵

Studies specifically focused on the application of DCE-MRI to cervical cancer is rare and often with small sample size. Semple et al²⁶ performed DCE-MRI scans for 20 cervical cancer patients with locally advanced disease undergoing chemoradiotherapy before treatment, 2 weeks

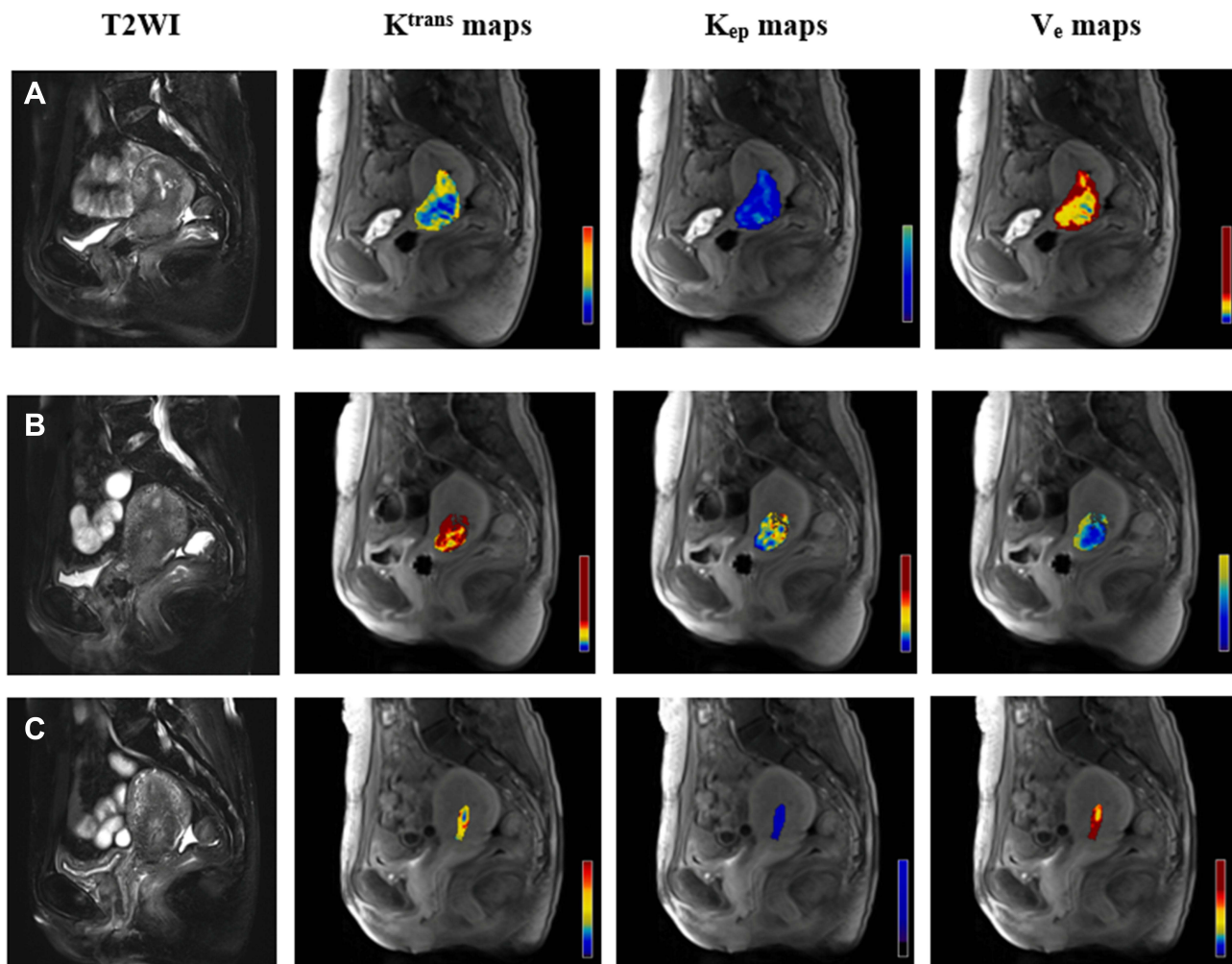


Figure 4 Dynamic changes of DCE-MRI parameters in a non-responder. Images in each row are representative images from three different timepoints (**A**=pre-RT; **B**=mid-RT; **C**=post-RT) from a 46-year old patient with IIB disease. The images of the primary tumor from T2WI are presented to show volume changes in mid- and post-RT in comparison with the baseline. Corresponding kinetic parameters (K^{trans} , K_{ep} , and V_e maps) of the primary tumor are presented to show permeability changes from the three given timepoints (Pre-, mid-, and post-RT). K^{trans} in pre-, mid-, and post-RT were 0.097 min^{-1} , 1.601 min^{-1} , and 0.306 min^{-1} , respectively; K_{ep} in pre-, mid-, and post-RT were 0.422 min^{-1} , 4.958 min^{-1} , and 0.544 min^{-1} , respectively; V_e in pre-, mid-, and post-RT were 0.263, 0.335, and 0.565, respectively. This patient achieved a partial response after the treatment.

after the initiation of treatment, and at the end of treatment. They found that pretreatment imaging parameters and K^{trans} were closely correlated with anti-tumor response. Another study with a small subject demonstrated that tumor regression rate was positively related to K^{trans} and K_{ep} .²⁷ However, their predictive role in cervical cancer treated with chemoradiotherapy is still controversial. Pretreatment K_{ep} was not correlated with treatment outcome, shown by a study of pharmacokinetic model.²⁸ In the present study, changes in the CR and NCR groups were not totally the same. In the CR group, K^{trans} in mid-RT was significantly higher than that in pre-RT, and K^{trans} in post-RT was significantly higher than that in mid-RT. However, when comparing pre- and post-RT, no

significant difference was found in K^{trans} . While in the NCR group, K^{trans} in mid-RT was significantly higher than that in pre-RT. Significant difference was found in K^{trans} between pre- and post-RT, but the changing direction was opposite to the CR group. Compared with K^{trans} in mid-RT, no substantial change in K^{trans} was found in post-RT, but it was higher than that in pre-RT. As for K_{ep} , significant differences were observed in the CR group between every two time points, but in the NCR group, significant differences existed only between pre- and post-RT. With respect to V_e , the CR and NCR groups had the same changing pattern. Significant differences were observed between every two time points. This may be explained by the following: After anti-tumor therapy,

Table 3 Comparison of Each DCE-MRI Parameter Between the CR and NCR Group

Parameter	CR Group	NCR Group	p value
K^{trans} (min^{-1})			
$K^{trans}_{\text{-preTx}}$	0.203±0.105	0.244±0.168	0.559
$K^{trans}_{\text{-midTx}}$	0.348±0.282	0.365±0.234	0.516
$K^{trans}_{\text{-postTx}}$	0.177±0.166	0.340±0.173	0.000
K_{ep} (min^{-1})			
$K_{ep,\text{preTx}}$	0.549±0.256	0.603±0.393	0.968
$K_{ep,\text{midTx}}$	0.706±0.370	0.622±0.410	0.259
$K_{ep,\text{postTx}}$	0.232±0.148	0.462±0.205	0.000
V_e			
$V_{e,\text{preTx}}$	0.378±0.149	0.409±0.182	0.614
$V_{e,\text{midTx}}$	0.524±0.214	0.645±0.184	0.039
$V_{e,\text{postTx}}$	0.695±0.134	0.740±0.169	0.159
ΔK^{trans} (min^{-1})			
$\Delta K^{trans}_{\text{-post-preTx}}$	0.146±0.234	0.120±0.231	0.695
$\Delta K^{trans}_{\text{-mid-preTx}}$	-0.026±0.169	0.095±0.208	0.004
$\Delta K^{trans}_{\text{-post-midTx}}$	-0.172±0.204	-0.025±0.226	0.011
ΔK_{ep} (min^{-1})			
$\Delta K_{ep,\text{post-preTx}}$	0.156±0.320	0.019±0.446	0.044
$\Delta K_{ep,\text{mid-preTx}}$	-0.317±0.287	-0.140±0.385	0.014
$\Delta K_{ep,\text{post-midTx}}$	-0.473±0.313	-0.160±0.339	0.001
ΔV_e			
$\Delta V_{e,\text{post-preTx}}$	0.145±0.222	0.236±0.277	0.062
$\Delta V_{e,\text{mid-preTx}}$	0.316±0.179	0.331±0.273	0.511
$\Delta V_{e,\text{post-midTx}}$	0.171±0.171	0.095±0.230	0.603

Notes: $K^{trans}_{\text{-preTx}}$, $K^{trans}_{\text{-midTx}}$, and $K^{trans}_{\text{-postTx}}$ represent the values of K^{trans} prior to RT, in the middle of RT, and at the end of RT, respectively, and the same denoting rule also goes for K_{ep} and V_e ; $\Delta K^{trans}_{\text{-post-preTx}}$, $\Delta K^{trans}_{\text{-mid-preTx}}$, and $\Delta K^{trans}_{\text{-post-midTx}}$ represent the differences in K^{trans} between pre-RT and post-RT, between pre-RT and mid-RT, and between mid-RT and post-RT, respectively, and the same denoting rule is also applied to K_{ep} and V_e .

patients in the CR group had a larger area containing fibrillation and a significantly lower vascular permeability, comparing with those in the PR group who had substantial tumor residuals. This phenomenon took place not only in chemoradiotherapy, but also in anti-angiogenesis agents.^{29,30} In fact, it might be more meaningful to compare the magnitudes of decrease for every parameter in both groups. Several studies indicated that tumors with higher K^{trans} and K_{ep} before treatment but lower K^{trans} and K_{ep} after treatment, or a higher reduction range in K^{trans} and K_{ep} after treatment were more responsive to treatment.^{19,24,31} Consistent with the findings mentioned above, significant differences were observed in $K^{trans}_{\text{-postTx}}$, $K_{ep,\text{postTx}}$, $V_{e,\text{midTx}}$, $\Delta K^{trans}_{\text{-post-preTx}}$,

Table 4 Correlation Between DCE-MRI Parameters and Tumor Volume/Volume Change (n=57, r Value)

Parameter	Tumor Volume (cm^3)			Volume Response Rate (%)	
	Pre-Tx	Mid-Tx	Post-Tx	Pre-midTx	Post-preTx
$K^{trans}_{\text{-preTx}}$	0.074	0.277	0.184	-0.265	1.000
$K^{trans}_{\text{-midTx}}$	0.045	0.249	0.009	-0.248	0.004
$K^{trans}_{\text{-postTx}}$	-0.089	0.063	0.425	-0.149	-0.443
$K_{ep,\text{preTx}}$	0.093	0.089	-0.010	-0.028	0.032
$K_{ep,\text{midTx}}$	0.025	0.138	-0.097	-0.188	0.147
$K_{ep,\text{postTx}}$	-0.196	0.120	0.525	-0.346	-0.540
$V_{e,\text{preTx}}$	-0.111	0.160	0.179	-0.267	-0.152
$V_{e,\text{midTx}}$	-0.113	0.049	0.272	-0.110	-0.301
$V_{e,\text{postTx}}$	-0.079	0.118	0.155	-0.219	-0.140
$\Delta K^{trans}_{\text{-post-preTx}}$	0.006	-0.135	0.276	0.044	-0.322
$\Delta K^{trans}_{\text{-mid-preTx}}$	-0.137	0.113	-0.100	-0.121	0.089
$\Delta K^{trans}_{\text{-post-midTx}}$	-0.126	-0.234	0.343	0.163	-0.373
$\Delta K_{ep,\text{post-preTx}}$	-0.053	-0.011	0.329	-0.184	-0.359
$\Delta K_{ep,\text{mid-preTx}}$	-0.207	-0.064	-0.090	-0.165	0.121
$\Delta K_{ep,\text{post-midTx}}$	-0.142	-0.079	0.412	0.001	-0.475
$\Delta V_{e,\text{post-preTx}}$	-0.022	-0.038	-0.026	0.048	0.017
$\Delta V_{e,\text{mid-preTx}}$	0.028	-0.064	0.109	0.084	-0.150
$\Delta V_{e,\text{post-midTx}}$	0.058	-0.079	-0.164	-0.051	0.205

Notes: $K^{trans}_{\text{-preTx}}$, $K^{trans}_{\text{-midTx}}$, and $K^{trans}_{\text{-postTx}}$ represent the values of K^{trans} prior to RT, in the middle of RT, and at the end of RT, respectively, and the same denoting rule also goes for K_{ep} and V_e ; $\Delta K^{trans}_{\text{-post-preTx}}$, $\Delta K^{trans}_{\text{-mid-preTx}}$, and $\Delta K^{trans}_{\text{-post-midTx}}$ represent the differences in K^{trans} between pre-RT and post-RT, between pre-RT and mid-RT, and between mid-RT and post-RT, respectively, and the same denoting rule is also applied to K_{ep} and V_e .

$\Delta K^{trans}_{\text{-post-midTx}}$, $\Delta K_{ep,\text{post-preTx}}$, $\Delta K_{ep,\text{mid-preTx}}$, and $\Delta K_{ep,\text{post-midTx}}$ between the two groups.

There are a number of studies that were focused on the role of DCE-MRI parameters in predicting treatment outcome. For example, findings from a study of esophagus cancer patients who underwent CCRT showed that a number of parameters, including pre-treatment K^{trans} , post-treatment K^{trans} and change rate of K^{trans} , difference in K^{trans} between pre- and post-treatment and change rate of K^{trans} , post-treatment K_{ep} , and difference in K_{ep}

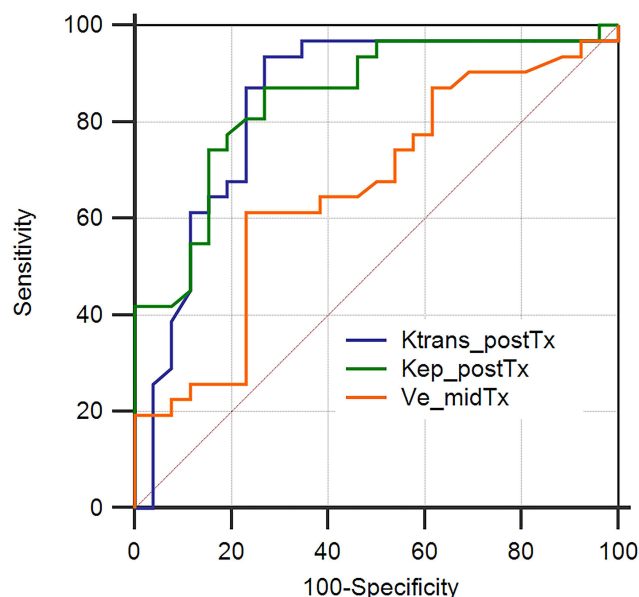


Figure 5 ROC for K^{trans} -postTx, K_{ep} -postTx, and V_e -midTx.

between pre- and post-treatment and change rate of K_{ep} , were all predictive of early treatment response. Among these parameters, change rate of K^{trans} was most potent predictor, with an AUC of 0.840, sensitivity of 89.5%, and specificity of 61.9%.²⁴ In our study, significant differences were found in K^{trans} -postTx, K_{ep} -postTx, V_e -midTx, ΔK^{trans} -post-preTx, ΔK^{trans} -post-midTx, ΔK_{ep} -post-preTx,

ΔK_{ep} -mid-preTx, and ΔK_{ep} -post-midTx between the two groups. A ROC analysis showed an AUC of 0.656–0.849, sensitivity of 61.3–93.5%, specificity of 46.1–73.1%, and maximal Youden Index of 36.5–66.6. Among those parameters, K_{ep} -postTx was the best, and its AUC, sensitivity, specificity, maximal Youden Index, and cutoff value were 0.849, 87.1%, 73.1%, 60.2, and 0.341, respectively. The combination of these parameters showed an AUC of 0.952, with sensitivity of 87.1%, specificity of 96.1%, and maximal Youden Index of 83.2.

There are several limitations in the present study. First, only early treatment response was predicted through DCE-MRI parameters, and the assessment of early treatment response was clinically based. An ideal tool to assess the early response should be post-treatment pathological findings. However, for patients in this study, it is almost impossible to obtain tissue samples after definitive chemoradiotherapy unless patients were initially treated with surgery. In order to assess whether the early response determined at the end of RT would be reliably representative of the status of tumor control, we compared the images obtained at the end of RT with those obtained 6 months after RT and found the two findings were consistent. An ideal predictor should be the one capable of predicting long-term outcome, survival in particular. However, in the present study, the follow-up time was

Table 5 Diagnostic Efficiency of Kinetic Parameters in Differentiating Responders from Non-Responders

Parameter	AUC	Sensitivity (%)	Specificity (%)	Cutoff Value	Maximal Youden Index	p
K^{trans} -preTx	0.545 (0.408–0.678)	64.5 (45.4–80.8)	53.8 (33.4–73.4)	0.229	18.4	0.567
K^{trans} -midTx	0.550 (0.413–0.682)	58.1 (39.1–75.5)	61.5 (40.6–79.8)	0.278	19.6	0.518
K^{trans} -postTx	0.839 (0.718–0.923)	93.5 (78.6–99.2)	73.1 (52.2–88.4)	0.256	66.6	<0.001
K_{ep} -preTx	0.503 (0.368–0.638)	12.9 (3.6–29.8)	73.1 (52.2–88.4)	0.317	14.0	0.969
K_{ep} -midTx	0.587 (0.449–0.716)	83.9 (66.3–94.5)	38.5 (20.2–59.4)	0.442	22.3	0.261
K_{ep} -postTx	0.849 (0.729–0.930)	87.1 (70.2–96.4)	73.1 (52.2–88.4)	0.341	60.2	<0.001
V_e -preTx	0.539 (0.402–0.672)	96.8 (83.3–99.9)	15.4 (4.4–34.9)	0.656	12.2	0.619
V_e -midTx	0.660 (0.523–0.780)	61.3 (42.2–78.2)	76.9 (56.4–91.0)	0.557	38.2	0.030
V_e -postTx	0.609 (0.471–0.736)	80.6 (62.5–92.5)	50.0 (29.9–70.1)	0.802	30.6	0.179
ΔK^{trans} -post-preTx	0.722 (0.588–0.833)	64.5 (45.4–80.8)	73.1 (52.2–88.4)	−0.016	37.6	0.001
ΔK^{trans} -mid-preTx	0.530 (0.394–0.664)	87.1 (70.2–96.4)	30.8 (14.3–51.8)	0.252	17.8	0.703
ΔK^{trans} -post-midTx	0.698 (0.562–0.812)	90.3 (74.2–98.0)	46.1 (26.6–66.6)	0.003	36.5	<0.001
ΔK_{ep} -post-preTx	0.690 (0.553–0.806)	83.9 (66.3–94.5)	57.7 (36.9–76.6)	−0.039	41.6	0.010
ΔK_{ep} -mid-preTx	0.656 (0.518–0.777)	74.2 (55.4–88.1)	65.4 (44.3–82.8)	0.044	39.6	0.042
ΔK_{ep} -post-midTx	0.763 (0.632–0.866)	80.6 (62.5–92.5)	61.5 (40.6–79.8)	−0.196	42.2	<0.001
ΔV_e -post-preTx	0.551 (0.413–0.683)	87.1 (70.2–96.4)	38.5 (20.2–59.4)	0.494	25.6	0.543
ΔV_e -mid-preTx	0.645 (0.507–0.767)	83.9 (66.3–94.5)	46.1 (26.6–66.6)	0.348	30.0	0.058
ΔV_e -post-midTx	0.540 (0.403–0.673)	16.1 (5.5–33.7)	100.0 (86.8–100.0)	0.423	16.1	0.609

Notes: K^{trans} -preTx, K^{trans} -midTx, and K^{trans} -postTx represent the values of K^{trans} prior to RT, in the middle of RT, and at the end of RT, respectively, and the same denoting rule also goes for K_{ep} and V_e ; ΔK^{trans} -post-preTx, ΔK^{trans} -mid-preTx, and ΔK^{trans} -post-midTx represent the differences in K^{trans} between pre-RT and post-RT, between pre-RT and mid-RT, and between mid-RT and post-RT, respectively, and the same denoting rule is also applied to K_{ep} and V_e .

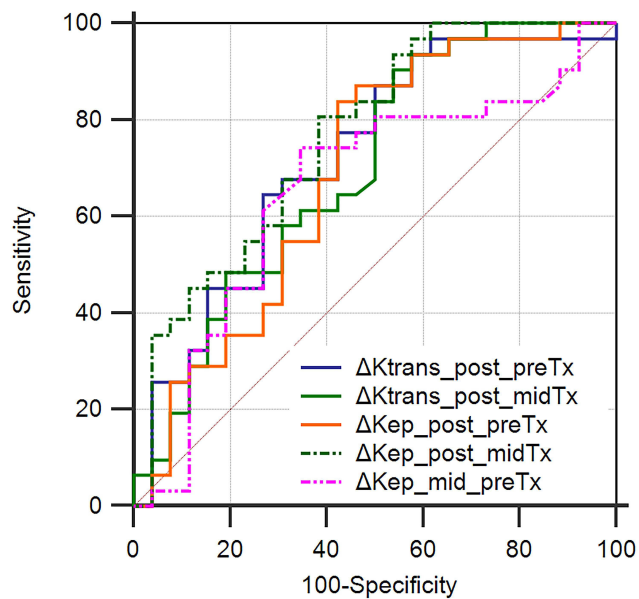


Figure 6 ROC for $\Delta K^{\text{trans}}_{\text{post-preTx}}$, $\Delta K^{\text{trans}}_{\text{post-midTx}}$, $\Delta K_{\text{ep,post-preTx}}$, $\Delta K_{\text{ep,post-midTx}}$, and $\Delta K_{\text{ep,mid-preTx}}$.

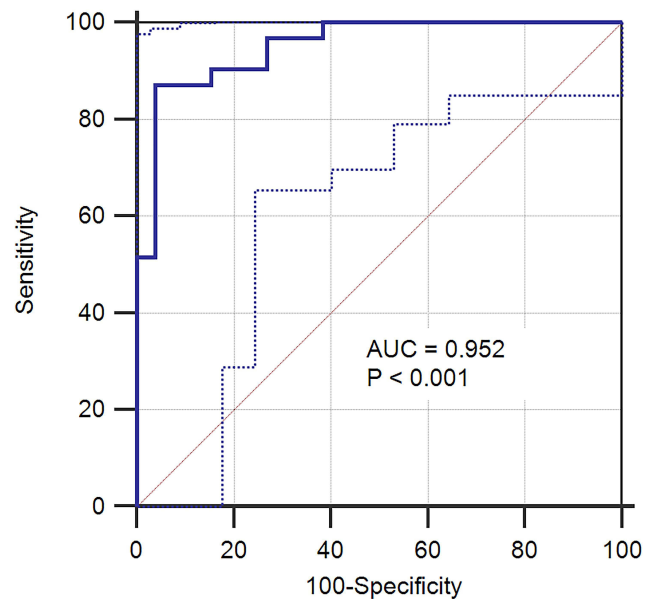


Figure 7 ROC for the combined DCE-MRI parameters.

relatively short, and only a few endpoint events took place. Therefore, it was difficult to assess and predict the long-term outcomes.

In a word, the potentials of DCE-MRI in assessing and predicting treatment outcome have been shown in a variety of tumor types and anti-tumor therapies. The combination of anatomic and functional images could overcome the drawback of mono-imaging technique. However, a lot of difficulties need to be solved, including appropriate selection of pharmacokinetic model, reproducibility of research findings, and selection of optimal parameter. Meanwhile, prospective studies with large sample size are warranted to confirm those findings.

Conclusion

For LACC patients who undergo definitive CCRT, DCE-MRI parameters can predict the early treatment response. Among those parameters, $K_{\text{ep,postTx}}$ is the best predictor for early treatment response. The combination of multi-parameters can increase the predictive potency.

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Disclosure

The authors report no conflicts of interest in this work.

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