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Gait asymmetry, and bilateral coordination of gait during a six-minute walk test in persons with multiple sclerosis

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Gait impairments in persons with multiple sclerosis (pwMS) leading to decreased ambulation and reduced walking endurance remain poorly understood. Our objective was to assess gait asymmetry (GA) and bilateral coordination of gait (BCG), among pwMS during the six-minute walk test (6MWT), and determine their association with disease severity. We recruited 92 pwMS (age: 46.6 ± 7.9 ; 83% females) with a range of clinical disability, who completed the 6MWT wearing gait analysis system. GA was assessed by comparing left and right swing times, and BCG was assessed by the phase coordination index (PCI). Several functional and subjective gait assessments were performed. Results show that gait is more asymmetric and less coordinated as the disease progresses ($p < 0.0001$). Participants with mild MS showed significantly better BCG as reflected by lower PCI values in comparison to the other two MS severity groups (severe: $p = 0.001$, moderate: $p = 0.02$). GA and PCI also deteriorated significantly each minute during the 6MWT ($p < 0.0001$). GA and PCI (i.e., BCG) show weaker associations with clinical MS status than associations observed between functional and subjective gait assessments and MS status. Similar to other neurological cohorts, GA and PCI may be important parameters to assess and target in interventions among pwMS.

Multiple sclerosis (MS) is a degenerative, progressive, autoimmune disease of the central nervous system, often resulting in a continuous deterioration of walking¹. Hence, gait parameters, e.g. cadence, step-length, step-time, are impaired as compared to those measured in abled bodied individuals¹⁻⁴. This gait deterioration has been demonstrated as a decline in the ability to walk long distances, based on the 6-min or 500-m walk tests^{5,6}. One critical component of walking impairment is gait variability. Gait variability tends to change throughout the MS disease course, with greater variability in the higher levels of disability^{7,8}. Furthermore, gait variability is associated with increased fall risk⁹.

Human gait requires a high degree of symmetry and coordination. Gait asymmetry is associated with reduced walking velocity¹⁰⁻¹² and increased energy expenditure¹³. Spinal cord injury is frequent in persons with multiple sclerosis (pwMS), noted in 83% by MRI and up to 99% at autopsy^{14,15}. Spinal cord injury is associated with lower extremity sensorimotor deficits and impaired ambulation. It was previously reported that walking velocity in pwMS was reduced when in vivo diffusion tensor imaging (DTI) of the cervical spinal cord reveals myelin and tissue injury within posterior columns (PC) and lateral corticospinal tracts (CST)¹⁶. Since CST injury in pwMS is asymmetric¹⁷, we hypothesize that MS will be associated with increased gait asymmetry, since asymmetric lesions in the spinal white matter lesions have been shown to correspond to asymmetric motor function¹⁸.

Gait coordination is the ability to maintain a consistent phase-dependent cyclical relationship between different body segments or joints in both spatial and temporal domains¹⁹. In humans, the control of right-left stepping, or bilateral coordination of gait (BCG), is hypothesized to be mediated by central pattern generators (CPGs) within lumbrosacral spinal locomotor centers¹³. CPGs are local neuronal circuits that generate rhythmic stepping

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movements by alternating activity between groups of flexor and extensor muscles. CPGs are modulated by large fiber sensory afferents, along with supraspinal input²⁰. Damage within the spinal cord may limit afferent (PC) and efferent (CST) input to the CPGs and thus, contributes to impaired BCG^{21,22}. Thus, it is also hypothesized that MS is characterized by impaired BCG.

In the present study we assess GA by the evaluating how leg movements differ while walking (comparing swing times between the legs and symmetry of swing duration)²³. Left–right stepping coordination is assessed by the phase coordination index (PCI), a measure of the accuracy and consistency of the phase relationship between the step timing of the left and right legs²³. Only three reports directly assessed PCI or GA among pwMS. Gianfrancesco et al. compared between cane users (n = 6) with non-users (n = 5) and attributed lower values of PCI and GA (i.e., better coordination and lower asymmetry) to the former group²⁴. Kasser et al. compared PCI values before and after an acute aerobic exercise in pwMS and reported no significant change²⁵. However, the relation to other clinical parameters, such as disease severity, was not assessed in these papers. Recently, Shema-Shiratzky et al.²⁶ measured GA among pwMS during the 6-min walk test (6MWT) and reported its relation to disease severity, however, only mild and moderate pwMS were assessed and PCI values were not measured in their study. Thus, gait difficulties in left–right stepping coordination and GA in PwMS, measured by temporal gait metrics (cycle to cycle performance), has not yet been fully described. In the present work we study these gait features using the 6MWT which is widely accepted as a valid outcome to assess fitness and endurance in a clinical context^{5,27}.

Study rationale. Characterizing GA and coordination impairments in MS, and their relations with functional (and subjective) gait assessments and with disease severity, would provide a more comprehensive picture about gait impairments in this cohort. GA and coordination impairments may prove useful in defining treatment targets and efficacy assessments for improving gait in MS. Assessing the relation of these parameters with disease severity could shed light on the progression of the MS and its effect on gait and risk of falls.

The objective of this study was to characterize GA and BCG in pwMS, during a long-distance walk (i.e., the 6MWT), and to assess their relationship with established gait assessments and other clinical parameters for pwMS. The study is driven by two hypotheses: (1) Human gait requires a high degree of symmetry and coordination, both of which are potentially altered in MS. (2) The type of gait patterns in pwMS (as reflected by gait asymmetry, coordination and variability outcomes) will be correlated with the level of impairment on key MS clinical outcomes, such as walking endurance as reflected by the distance covered during the 6MWT, and self-reported walking limitations.

Methods

Participants. A total of 92 pwMS were recruited through the John L. Trotter MS Center at Washington University School of Medicine. This cross-sectional study was approved by the local Human Research Protection Office/Institutional Review Board of the Washington University in St. Louis. All participants signed an informed consent prior to entering the study and all methods were performed in accordance with the relevant guidelines and regulations. Inclusion criteria were: > 18 years of age; relapsing–remitting MS (RRMS), secondary-progressive MS (SPMS), or primary-progressive MS (PPMS); evidence of cervical spinal cord disease by symptoms or signs (e.g. Lhermitte’s sign, upper extremity weakness, upper extremity sensory symptoms), T2 lesions on clinical cervical MRI, and > 180 days post-relapse. Exclusion criteria: confounders which could affect ambulation outside the spinal cord (e.g. poor vision) pregnancy, lower extremity orthopedic conditions that limit ambulation, morbid obesity, cardiac pacemaker, metallic implant, and claustrophobia. Participants were then grouped by disease severity, i.e. mild (EDSS 0–2.5, n = 60), moderate (EDSS 3–4, n = 26) and severe (EDSS 4.5–6.5, n = 6).

Experimental protocol. The participants wore a six Opal motion sensor-based gait analysis system (APDM, Portland, Oregon, USA). The 6MWT⁵ was performed along a 50 foot walkway (i.e., participants turned around cones at each end of the 50 foot walkway). Spatiotemporal parameters of gait were collected by sensors worn on the ankles, wrists, lower back and chest, and transmitted to a wireless access device for storage on a mobile computer. Additional assessments included the Timed 25-foot Walk Test (T25FWT)²⁸, self-perceived walking limitation [12-item MS walking scale (MSWS-12v2)]²⁹ and balance confidence (Activities-specific balance confidence scale (ABC))³⁰.

Gait cycle timing related outcome measures. Outcomes were calculated based on ‘heel strike’ and ‘toe off’ timing obtained from the straight-line walking segments (180° turns at end of walkway were omitted):

- (1) Gait variability [%]: was defined by Stride time variability^{7,23}: coefficient of variation (CV) of the mean value of the stride time (multiplied by 100 to obtain percentage). We termed this parameter stride CV. Stride CV was calculated separately for the left and the right legs and since values of the right and left legs were highly correlated ($r = 0.989$; $p < 0.001$), we present data only for the right leg.
- (2) GA[%] = $100 \cdot |\ln(R_SW/L_SW)|$, where R_SW and L_SW stand for the mean value of right and left leg swing time, respectively²³.
- (3) Phase coordination index (PCI; [%])—for the quantification of BCG): A full description and derivation of the PCI metric is detailed elsewhere²³. Briefly, PCI is a metric that combines the accuracy and consistency of stepping phases generation with respect to the value of 180°, which represents the ideal anti-phased left–right stepping. Lower PCI values (also transformed to percentile unit; %) reflect a more consistent and more accurate phase generation, while higher values indicate a more impaired BCG^{23,31,32}.

	Total (n = 92)	Mild (n = 60)	Moderate (n = 26)	Severe (n = 6)
Age in years, mean \pm SD (range)	46.6 \pm 10.9 (22–66)	43.2 \pm 10.4 (22–66)	53.0 \pm 8.1 (33–65)	54.1 \pm 11.2 (34–63)
EDSS, median (range)	2.0 (2.0–6.5)	2.0 (0–2.5)	3.0 (3–4)	5.5 (5.0–6.5)
Female, n (%)	76 (83%)	49 (82%)	21 (81%)	6 (100%)
Race (Caucasian, African–American, Asian), n (%)	83/8/1 (90, 9, 1)	53/6/1 (88, 10, 2)	24/2/0 (92, 8, 0)	6/0/0 (100, 0, 0)
Type of MS (RR/SP/PP), n (%)	88/2/2 (96%, 2%, 2%)	59/0/1 (98%, 0%, 2%)	23/2/1 (88%, 8%, 4%)	6/0/0 (100%, 0%, 0%)
Years since diagnosis, mean \pm SD (range)	10.7 \pm 7.9 (1–37)	9.2 \pm 7.0 (1–30)	13.8 \pm 7.8 (2–31)	12.3 \pm 12.6 (2–37)

Table 1. Demographic and clinical data of the cohort. *EDSS* expanded disability status scale, *RR* relapsing remitting, *SP* secondary progressive, *PP* primary progressive.

Functional and objective outcome measures.

Distance covered during the 6MWT (ft) (reflective of gait speed).

Time (sec) to complete the T25FWT.

Transformed Score on the MSWS-12v2³³ (higher score reflect perception of being more limited).

Transformed Score on the ABC (higher scores reflect more confidence in performing balance capabilities related activities).

Gait variability, GA, PCI and distance covered were calculated and measured for each minute of the 6MWT trail.

Statistical analysis. For Gait variability, GA, PCI and distance covered, we performed a Repeated measures ANOVA treating each 1-min interval ('time' effect) as a within subject level during the 6MWT, and the three severity subgroups ('group' effect) as a between-subject factor. When violations of the assumption of sphericity were observed, Greenhouse–Geisser estimates were used to correct the degrees of freedom. The Bonferroni method was used to correct for the post-hoc comparisons.

One-way between-groups ANOVAs and Bonferroni's post-hoc tests compared the functional and objective outcome measures (apart of distance covered) among the MS severity subgroups.

Demographic and clinical factors which differed significantly between these groups (i.e. Age, Disease duration) were added as covariates in both of these analyses.

Effect sizes were reported as Eta squared and Cohen's d.

Correlation analyses between distance covered, stride CV, GA and PCI and the functional and subjective gait assessments were performed (Pearson) for the entire cohort and within each severity group. For the correlation analysis, we used the distance covered, stride CV, GA and PCI values measures and calculated over the entire 6MWT.

Results

Demographic and clinical data of the sample appear in Table 1. Of the 92 participants, 60 were classified as having mild disability, 26 as moderate disability, and 6 as severe disability. As expected, significant group differences were found for age ($F_{(2,89)} = 10.8$, $p < 0.001$, $\eta^2 = 0.19$) and disease duration ($F_{(2,89)} = 3.39$, $p < 0.03$, $\eta^2 = 0.07$). Post-hoc comparisons indicate younger age and shorter disease duration associated with mild disability. In light of these group differences, in the following analyses, we entered age and disease duration as covariates.

Group (MS severity) and time effects on distance covered, gait variability, coordination and asymmetry. Significant group differences were found for distance covered ($F_{(2,87)} = 20.7$, $p < 0.0001$, $\eta^2 = 0.32$), gait variability (i.e., Stride CV, $F_{(2,86)} = 13.9$, $p < 0.0001$, $\eta^2 = 0.24$), PCI ($F_{(2,86)} = 9.3$, $p < 0.0001$, $\eta^2 = 0.17$), and GA ($F_{(2,86)} = 12.0$, $p < 0.0001$, $\eta^2 = 0.21$; see Fig. 1 for post-hoc group to group comparisons).

Figure 2 depicts three examples of data sets from three participants, one from each severity level group. These examples are representative of the group differences described above. Stride-to-stride time variability is larger for the more severely affected participants, as expressed by the larger range of values of the stride times in the participants with moderate and severe MS. Left–right stepping coordination (i.e., BCG) as expressed by the large variability in ϕ values (i.e., reduced consistency), and with values fairly 'distant' from the 'ideal' value of 180° is impaired in the participant with moderate MS ($\phi = 173.0 \pm 4.2^\circ$) as compared to the participant with mild MS ($\phi = 179.4 \pm 2.7^\circ$), and even worse in the participant with the severe MS ($\phi = 187.3 \pm 11.3^\circ$; see PCI values for all participants in Fig. 2). Similarly, the increased GA exhibited by the participants with moderate and severe MS is clearly demonstrated by the separation in the scatter of right (red) and left (green) swing times.

Significant time (i.e., potential fatigue) effects were found for PCI ($F_{(5,430)} = 5.6$, $p < 0.0001$, $\eta^2 = 0.06$, due to a general decrease in coordination (i.e., larger PCI values) over time, in addition to a significant interaction between severity group and time, $F_{(10,430)} = 4.9$, $p < 0.0001$, $\eta^2 = 0.1$, due to a larger increase in PCI values among the severe MS group. Further, significant time effects were also found for GA ($F_{(5,430)} = 4.9$, $p < 0.0001$, $\eta^2 = 0.05$, due to a general increase in asymmetry across groups, and in this case as well, a significant interaction was yielded between severity group and time, $F_{(10,430)} = 5.3$, $p < 0.0001$, $\eta^2 = 0.11$, due to a larger increase in asymmetry among the severe MS group. Unexpectedly, time effect was not demonstrated with regards to distance covered, $F_{(5,435)} = 0.7$, $p = 0.6$, $\eta^2 = 0.008$, or Gait variability (i.e., Stride CV, $F_{(5,430)} = 1.8$, $p = 0.09$, $\eta^2 = 0.02$) nor interactions between fatigue (i.e., time effect) and severity group regarding these measures.

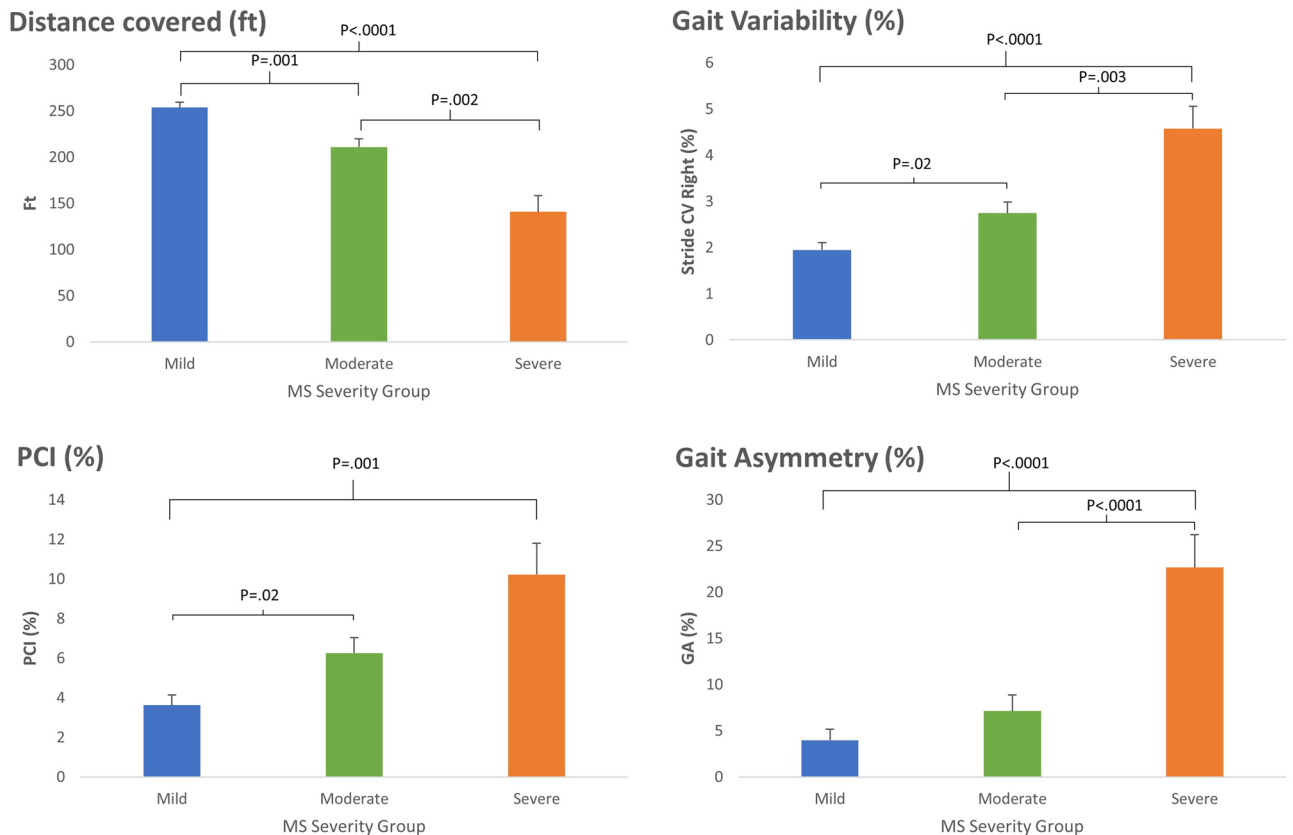


Figure 1. Mean values of distance covered, Stride time CV, GA and PCI during 6MWT in pwMS with different disease severity (see key). Bars represent mean values calculated based on the per-minute measures (see “Methods”). Statistically significant differences in post-hoc group-to-group comparisons are marked above with horizontal brackets. Means and standard deviations are as followed: The severe disability group had greater asymmetry (GA: 22.6 ± 3.5) than the mild (GA: 3.9 ± 1.1) or moderate (GA: 7.1 ± 1.7) disability groups, and more impaired PCI (10.2 ± 1.5) than the mild disability group (3.6 ± 0.5). The moderate disability group had worse PCI (6.2 ± 0.5) compared to the mild disability group, and better PCI than the severe disability group. Gait Asymmetry did not significantly differ between the mild vs. moderate disability groups ($p = 0.47$). Distance covered significantly differed among all three MS severity groups (Severe: 141.6 ± 17.2 , Moderate: 211.3 ± 8.3 , Mild: 253.4 ± 5.4) and Gait Variability also significantly differed among all three MS severity groups (Severe: 4.5 ± 0.4 , Moderate: 2.7 ± 0.2 , Mild: 1.9 ± 0.1). Upper limit of the abscissa is 360 s.

The role of gait speed: post hoc analyses. Since significant correlations were found between walking speed (distance covered) and PCI, GA and stride CV (see Table 2 below), we performed three additional repeated measures analyses to test for PCI, GA and stride CV group differences while adding the distance covered (i.e., walking speed) as a covariate. While time effects remained significant for all three analyses, the analyses also revealed that for both gait variability and PCI, the group effect did not remain statistically significant (Stride CV, $F_{(2,85)} = 1.5$, $p = 0.21$, $\eta^2 = 0.03$, PCI ($F_{(2,85)} = 0.9$, $p = 0.38$, $\eta^2 = 0.02$), and the group effect for GA remained statistically significant ($F_{(2,85)} = 4.2$, $p = 0.01$, $\eta^2 = 0.09$).

We also performed additional analyses to determine the relationship within a subject between variability in walking speed and variability in gait parameters. Stride CV, GA and PCI were analyzed, for each minute in the 6MWT, expressed by the Pearson correlation coefficient (r_p , see Fig. 3). See full account on r_p analyses in the Supplementary material 1).

To control for the effects of these intrinsic associations, we performed three additional repeated measures analyses to test group effects for PCI, GA and stride CV while adding the relevant r_p (i.e., for PCI, GA and Stride CV). The new analyses revealed that for Stride CV, PCI, and GA, the group effects remained significant (Stride CV, $F_{(2,85)} = 14.0$, $p < 0.0001$, $\eta^2 = 0.24$, PCI ($F_{(2,85)} = 9.5$, $p < 0.0001$, $\eta^2 = 0.18$, GA ($F_{(2,85)} = 10.3$, $p < 0.0001$, $\eta^2 = 0.19$).

Functional and subjective gait assessments. Figure 4 depicts groups’ performance on the functional and subjective gait assessments. Eighty-one participants completed the T25FWT (52 from the mild group, 23 from the moderate group and six from the severe group). Group effect was statistically significant ($F_{(4,76)} = 13.86$, $p < 0.001$, $\eta^2 = 0.42$), demonstrating that participants with milder MS severity walk faster.

Self-perceived walking limitations and balance confidence worsened with disease severity. Group effect was statistically significant for the MSWS-12v2 ($F_{(4,87)} = 14.48$, $p < 0.001$, $\eta^2 = 0.40$) and for the ABC test ($F_{(4,87)} = 7.49$,

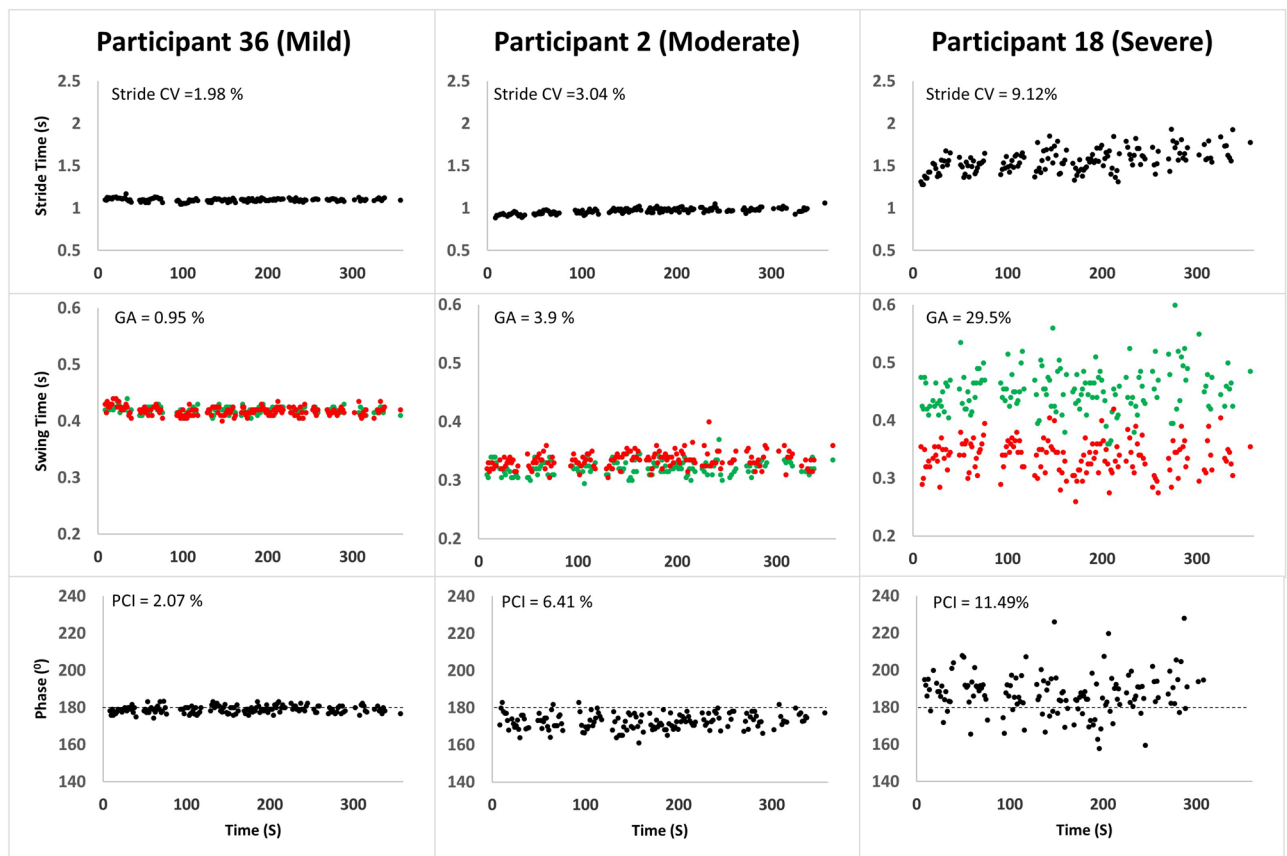


Figure 2. Three examples of data sets from three participants. Series of stride times (Top), left–right stepping phases (Middle), and swing times, (Bottom) are plotted for a 42 year old female patient with mild disease severity (left: EDSS = 2; 6MWT distance = 1,514 ft; MSWWS-12v2 = 12; ABC = 98), a 59 year old female patient with moderate disease severity (middle: EDSS = 3.0, 6MWT distance = 1,319 ft; MSWWS-12v2 = 38; ABC = 66), and a 48 year old female with severe disease severity (right: EDSS 6.5; 6MWT distance = 406 ft; MSWWS12v2 = 76; ABC = 49). Red and green dots at the lower panels represent right and left swing times, respectively.

	EDSS	Distance covered	MSWS-12v2	ABC	T25FWT
Stride CV	0.44**	−0.57**	0.53**	−0.47**	0.60**
PCI	0.42**	−0.54**	0.43**	−0.39**	0.50**
GA	0.35**	−0.42**	0.29**	−0.31**	0.46**
Distance covered	−0.59**		−0.60**	0.56**	−0.84**
MSWS-12v2	−0.59**			−0.72**	0.61**
ABC	−0.49**				−0.53**
T25FWT	0.60**				

Clinical status	Gait parameters	Functional and subjective measures
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Table 2. Pearson correlations between clinical status, gait parameters and functional and subjective gait assessments. EDSS Expanded Disability Status Scale, CV coefficient of variation, PCI phase coordination index, GA gait asymmetry, MSWS-12v2 12-item multiple sclerosis walking scale, ABC activities-specific balance confidence scale, T25FWT Timed 25-Foot Walk Test. ** $p \leq 0.01$.

$p < 0.001$, $\eta^2 = 0.25$), as participants with milder MS severity reporting lower self-perceived gait limitations and higher balance confidence. Group to group post-hoc comparisons are detailed in Fig. 4.

Correlation analyses. Statistically significant correlations were found between distance covered, PCI, GA and stride CV and clinical, functional and subjective outcomes (i.e., EDSS score, distance covered, MSWS12, T25WT and ABC) for the whole cohort ($r_p = |0.29| - |0.60|$, $p < 0.01$; see Table 2 for details). PCI, GA and stride CV showed stronger correlations when evaluating data from pwMS participants with more severe disease (see

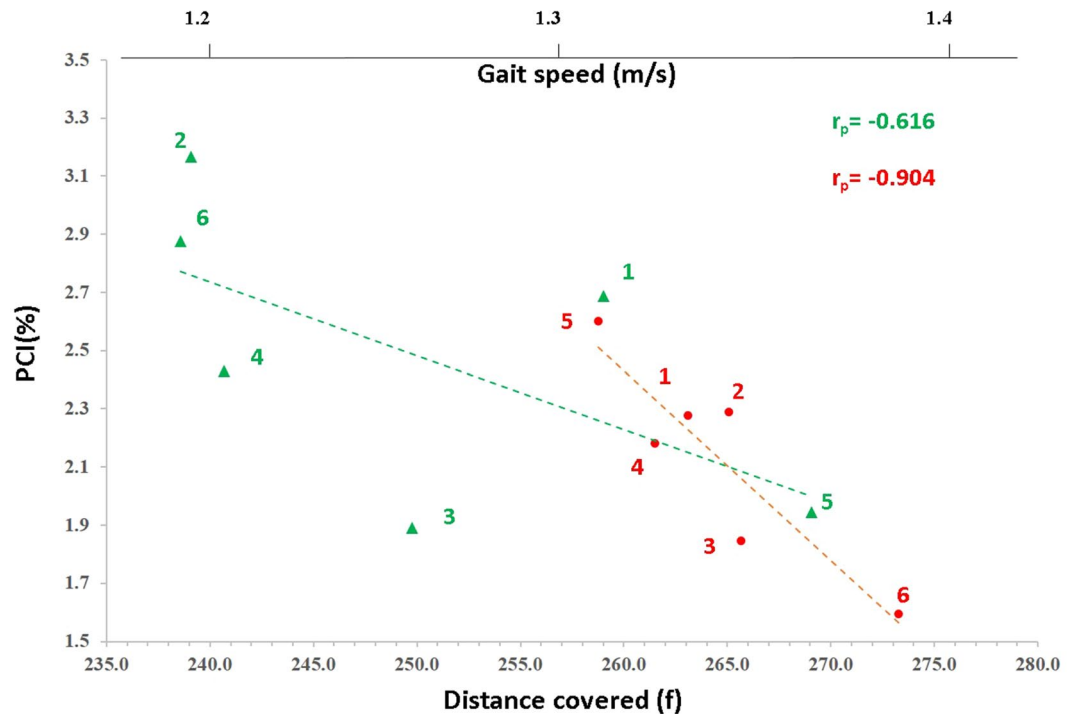


Figure 3. Examples of Intrinsic relations between gait coordination and gait speed. PCI values calculated for each minute of the 6MWT plotted against distance covered (equivalent to gait speed as shown on the top horizontal axis) for 24 years old male person with MS with EDDS score 2 (green triangles), and 55 years old female person with MS with EDDS score 1 (red circles). The numbers indicate the minute number of the 6MWT from which data were extracted to calculate the values for this point. The Pearson correlation coefficients are indicated for both cases (top right) and linear trend lines (dashed) are plotted (see more details in the Supplementary material 1).

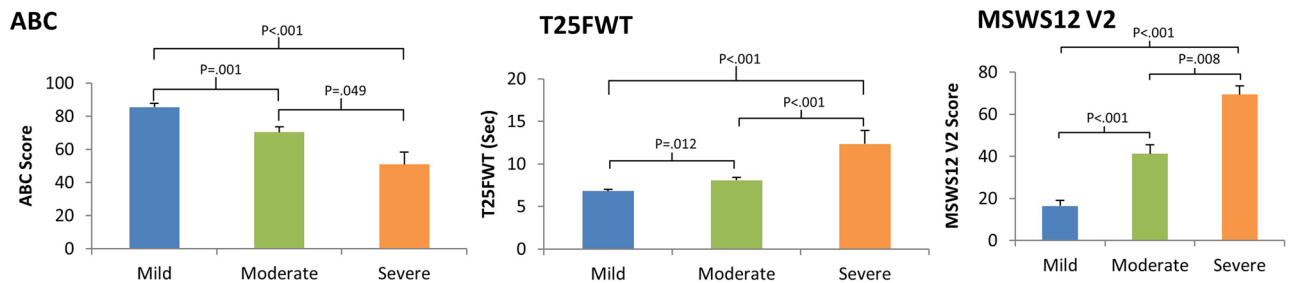


Figure 4. Mean values of ABC scores, MSWS12 V2 scores, and T25FWT seconds to complete in pwMS with different disease severity (see key). Statistically significant differences in post hoc group to group comparisons are marked above the horizontal brackets. Means, standard deviations and effect sizes are as followed: The severe disability group reported less balance confidence (ABC score: 50.9 ± 18.0), more self-perceived walking limitation (MSWS12 V2 score: 69.4 ± 9.9), and performed worse on the T25FWT seconds to complete (7.5 ± 2.2) than the moderate group (ABC score: 70.3 ± 16.3 , $d = 1.12$; MSWS12 V2 score: 41.2 ± 22.5 , $d = 1.6$; T25FWT seconds to complete: 12.3 ± 3.8 , $d = 1.45$) and compared to the mild group (ABC score: 85.4 ± 18.2 , $d = 1.9$; MSWS12 V2 score: 16.4 ± 20.4 , $d = 3.29$; T25FWT seconds to complete: 6.8 ± 1.4 , $d = 1.9$). Furthermore, the moderate severity group also reported less balance confidence, more self-perceived walking limitation, and performed worse on the T25FWT than the mild group (ABC, a).

Table 3 for details). For example, PCI was strongly correlated with GA within the group with moderate MS ($r_p = 0.86$; $p < 0.01$) and severe MS ($r_p = 0.99$; $p < 0.01$), but not as strongly correlated within the group with mild MS ($r_p = 0.36$; $p < 0.01$).

	Stride CV			PCI		
PCI	0.70**					
	0.57**	0.61**	0.84**			
GA	0.62**			0.83**		
	0.32*	0.50**	0.83**	0.36**	0.86**	0.99**
	Gait parameters	Mild MS group	Moderate MS group	Severe MS group		

Table 3. General and severity group Pearson correlations between the gait parameters. CV coefficient of variation, PCI phase coordination index, GA gait asymmetry. * $p \leq 0.05$. ** $p \leq 0.01$.

Discussion

Summary of findings. This study which assessed gait asymmetry and impaired BCG among pwMS with spinal cord injury (i.e., excluding those with clear brainstem or cerebellar signs, see “Methods”) during relatively long-distance walk (i.e., 6MWT) observed a relationship with disease severity and functional and subjective gait assessments. In this cohort, gait was more asymmetric and less coordinated as the disease progressed. While impairments in these functions are probably related to loss of spinal structures affecting CPGs outcomes (see below), potential impacted supra spinal regions (e.g., cortex, basal ganglia) may also contribute to deficits in GA and BCG (e.g.³¹).

Participants with severe MS had larger GA values as compared to participants from the moderate and mild groups. Participants with mild MS showed significantly better BCG as reflected by lower PCI values in comparison to the other two MS severity groups.

Significant time effect (i.e., minute by minute evaluation of parameters) was observed for PCI and GA, indicating within testing deteriorations in bilateral coordination and in gait symmetry. This deterioration was more evident in participants with more severe symptomology (i.e., significant group \times time interaction). Time was not a statistically significant effect for distance covered (i.e., gait speed) and stride CV. A possible interpretation is that maintaining gait coordination (PCI) and symmetry (GA) is not maintained as well as maintaining gait rhythmicity (i.e., low gait variability—stride CV) and speed among pwMS when walking without stopping for several minutes.

Cross-subjects analyses show that PCI and GA measured in participants with MS were highly inter-correlated, and correlated with gait variability, functional gait performance and subjective gait and balance assessments.

The role of gait speed. The 6MWT measures average gait speed by distance covered over a period of six minutes. When using overall distance covered (i.e. averaged walking speed) as a covariate, MS severity level (i.e., ‘group’ effect) was not statistically significant for stride CV and PCI. However, using this parameter as covariate was too robust as it is based on the overall distance covered (and not per each minute).

Notably, our measurement methodologies allowed us to partition the data to sub-segments, 1 min long each, and to assess the effect of time. This analyses revealed the potential intrinsic (i.e., within subject) association between gait speed and gait parameters (e.g., Fig. 3, and Supplementary material 1) by calculating correlation coefficients based on six data points sets. We used these correlation coefficients as covariates and determined that after controlling for how gait speed is related with gait parameters (stride CV, PCI and GA) for each individual, ‘group’ effect remain significant (i.e., CV, PCI and GA are affected by disease severity in pwMS).

The literature lacks consensus with regards to the association between gait speed and GA, PCI or Gait Variability. Studies report conflicting findings regarding each association with the literature supporting positive, negative and no correlations between gait speed and GA³⁴, gait speed and PCI^{35,36}, and gait speed and gait variability^{37–39}. Within subject effects were seen on PCI but not on GA when gait was deliberately slowed⁴⁰.

Relation to previous findings. PCI and GA values in the current study observed in the severe group were consistent with the PCI and GA values reported in Gianfrancesco et al.²⁴ measured among pwMS with severe MS (EDSS 4–5.5) while walking unassisted at a preferred walking speed. Despite the use of a different gait analysis system by these investigators, GA and PCI appear to be robust measures characterizing the gait of pwMS.

Recently, Shema-Shiratzky et al.²⁶ reported the results of a study in which various gait domains (e.g., pace, rhythm, variability, symmetry, and complexity) were measured and compared among mild- and moderate pwMS who performed the 6MWT while wearing body-fixed sensors. They did not recruit participants with severe MS nor reported on PCI values. In addition, they did not use gait speed as a covariate in their analysis of the gait domains. Their results show, similarly to the current findings, an association between gait deterioration, patient-reported gait disability and disease severity. However, in our study, symmetry had worsened during the 6MWT and variability did not while in Shema-Shiratzky et al.’s study, variability had worsened, and symmetry did not change. Since we included participants with EDSS score lower than 2 and above 6, (not included by Shema-Shiratzky et al.) it might be the case that trends were missed or enhanced as a result of this truncation. Future studies may clarify this possibility.

While a control group was not included in the present study, prior studies^{32,33} suggest gait parameters in healthy individuals to be similar to our mild pwMS cohort. PCI values calculated using a similar gait analysis system were comparable ($3.9 \pm 13\%$) to able-bodied controls with an age range similar to the age range of the mild

pwMS cohort (45.4 ± 3.6 years; $n = 20$ vs 43.2 ± 10.4 ; $n = 60$, respectively). GA values were not reported on that study. Despite similar PCI values, the total distance covered by the present mild cohort ($\sim 1,520$ ft) was smaller than an able-bodied control group with similar age range ($\sim 2,300$ ft⁴¹). This suggests that PCI may not be the most sensitive or earliest parameters to coincide with walking impairment, and that deficits in walking endurance may precede impairment in the bilateral coordination of gait. In our study, pwMS with moderate disease severity exhibited PCI values of $\sim 6.2\%$ (Fig. 1), larger than the PCI values observed in able-bodied participants from a comparable age group (PCI = 4.3% ⁴²). Thus, the PCI may differentiate pwMS from able-bodied persons as the disease progresses.

PCI values observed among participants from the severe MS group were similar to an elderly population. One study of healthy individuals in their eighth decade of life demonstrated that their PCI was approximately 10%, comparable to the severe MS cohort PCI of 10.2% at a median age of 54 years³⁵. This observation illustrates the high degree of impaired coordination of gait in ambulatory pwMS with severe clinical disability. These data, taken together with a previous report of lower PCI and GA values (i.e., better coordination and lower asymmetry) in pwMS using a cane vs no cane²⁴, suggest the use of an assistive device may improve the BCG in similar pwMS.

PCI and GA were documented in other cohorts: stroke patients³¹, persons with Parkinson's disease (PD)^{23,43} and elderly fallers⁴³. Similar to the results of the present study, PCI and GA were found to be associated with severity of the PD symptoms. Specifically, patients who suffer from the freezing of gait symptom exhibited higher values of GA⁴⁴ and PCI³², indications for asymmetric gait, and impaired BCG.

Gait variability in pwMS has been assessed in many studies (see⁴⁵ for review). This gait parameter was found to be associated to disease severity, in agreement with the present results. It is worth noting that not all studies use the same parameter to describe gait variability. For instance, Kalron⁷ and Socie et al.³ used Step Length, Time and Width CV, Kaipust et al.⁴⁶ used Stride Length and Step Width CV.

Few studies have reported upon correlations between clinical, functional and subjective measures among pwMS. Goldman et al.⁵ reported high correlation between the 6MWT and subjective quality of life and walking quality. Socie et al.³ reported high correlations between disease severity and three measures of gait variability (e.g., $r = 0.51$ between step length and EDSS values). Learmonth et al.⁴⁷ reported high correlations ($r > |0.62|$) between EDSS and 6MWT distance, time to complete the T25FW and subjective walking quality. All these findings point to a positive relation between objective gait measures and subjective assessments of performance and quality of life.

Relation between GA, BCG and MS. We found a strong correlation between GA and PCI (c.f., Table 3). However, BCG differs from gait symmetry. BCG reflects the level of coordination between the ongoing stepping movements of both legs (i.e. the phase-dependent relationship between right and left heel strike over a number of steps)^{23,31}. Because people can have different swing durations for each leg with preservation of the phase relationship between the legs, an asymmetrical gait is not necessarily an uncoordinated gait^{23,48}. We propose that the PCI-GA correlation found in the present study may reflect the global impact of the pathogenicity on the ability to generate symmetric as well as coordinated gait.

The symmetrical gait commonly observed during normal walking can be attributed to the symmetric function of the central pattern generators (CPGs—the assumed neuronal substrate underlying rhythmical stepping movement of the lower limbs). Anti-phased stepping is an expression of the coordination between CPGs on both sides of the spine, most likely connected by commissural fibers²¹. Damage to the CST in pwMS¹⁶ most likely impact these neuronal substrates⁴⁹. Thus, we hypothesize that pwMS with asymmetrical CST are more likely to have an asymmetrical and less coordinated gait compared to pwMS with symmetrical CST, PC, or no injury. These hypotheses, and how spinal pathophysiological pathways are interacting with effects of supra spinal lesions to alter BCG and GA functions may be tested in future studies also involving imaging, including assessments of spinal gray matter integrity.

Limitations, implications of findings and future directions. While providing data from relatively large cohort of pwMS, the small number of participants ($n = 6$, $\sim 7\%$) in the severe group should be acknowledged as it poses limitation on the external validity of our findings. According to the literature of gait studies with the participation of pwMS, the relative portion of participants with more severe symptomatology varies. In some studies it is relatively small or absent (e.g.^{2,3}), in few others the proportion of this sub group was higher than in the presents study ($\sim 15\%$ ⁵). Noteworthy, while we used EDSS score 4.5–6 as a criteria for the sever group, different studies set different criteria (e.g.^{7,24}). Future studies should investigate a larger cohort of pwMS with severe disability.

We propose that stride CV, GA and PCI are important parameters to assess among pwMS, since they seem to deteriorate with disease progression. Stride CV, GA and PCI can be objectively assessed during home monitoring. While functional tests and subjective questionnaires require trained personnel, current light wearable sensors technologies (e.g.^{50,51}) allow an objective assessment of gait parameters like those at the focus of the present study. Longitudinal studies will be required to determine whether changes over time in these (and other gait parameters) have predictive diagnostic value regarding the progression of MS. Subtle impairments in gait performances have been demonstrated as prodromal signs for worsening due to PD^{42,52}. Further, gait coordination and gait asymmetry can be defined as targets for interventions aiming to improve gait performance^{53–55}. The efficacy of similar interventions in the context of fall prevention in MS⁵⁶ is still to be determined.

In conclusion, GA and BCG are worse in pwMS who have more disability and disease progression, compared to those with mild to moderate disability. Longitudinal studies would help determine the rate of change in these parameters, and whether early changes have a predictive ability on disability and quality of life. Studies of physical therapy programs designed to target GA and BCG in pwMS may have potential to improve ambulation and falls.

Data availability

The datasets generated during and/or analysed during the current study are available from the corresponding author on reasonable request.

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Author contributions

M.P., J.M.W., G.A., and R.T.N. designed and performed the study. AG and MP did the data analysis, interpreted the data, prepared the figures and drafted the main manuscript text. J.M.W. and R.T.N. substantively revised the manuscript.

Competing interests

RTN has received honorarium for speaking/consulting from Alexion, Alkermes, Biogen, Celgene, EMD Serono, Genentech, Genzyme, Novartis, Alexion, TG Therapeutics, Viela Bio. All other authors declare no competing interests.

Additional information

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