

Advancements and challenges in mRNA and ribonucleoprotein-based therapies: From delivery systems to clinical applications

Zohre Eftekhari,^{1,4} Horieh Zohrabi,^{1,4} Akbar Oghalaie,¹ Tahereh Ebrahimi,² Fatemeh Sadat Shariati,³ Mahdi Behdani,¹ and Fatemeh Kazemi-Lomedasht¹

¹Venom and Biotherapeutics Molecules Laboratory, Biotechnology Department, Biotechnology Research Center, Pasteur Institute of Iran, Tehran 1316943551, Iran; ²Department of Nanobiotechnology, New Technologies Research Group, Pasteur Institute of Iran, Tehran 1316943551, Iran; ³Department of Influenza and other Respiratory Viruses, Pasteur Institute of Iran, Tehran 1316943551, Iran

The use of mRNA and ribonucleoproteins (RNPs) as therapeutic agents is a promising strategy for treating diseases such as cancer and infectious diseases. This review provides recent advancements and challenges in mRNA- and RNP-based therapies, focusing on delivery systems such as lipid nanoparticles (LNPs), which ensure efficient delivery to target cells. Strategies such as microfluidic devices are employed to prepare LNPs loaded with mRNA and RNPs, demonstrating effective genome editing and protein expression *in vitro* and *in vivo*. These applications extend to cancer treatment and infectious disease management, with promising results in genome editing for cancer therapy using LNPs encapsulating Cas9 mRNA and single-guide RNA. In addition, tissue-specific targeting strategies offer potential for improved therapeutic outcomes and reduced off-target effects. Despite progress, challenges such as optimizing delivery efficiency and targeting remain. Future research should enhance delivery efficiency, explore tissue-specific targeting, investigate combination therapies, and advance clinical translation. In conclusion, mRNA- and RNP-based therapies offer a promising avenue for treating various diseases and have the potential to revolutionize medicine, providing new hope for patients worldwide.

INTRODUCTION

Background on mRNA and ribonucleoprotein therapies

In vitro transcription (IVT) of mRNA involves utilizing linearized plasmid DNA or PCR templates, which necessitate a promoter and the corresponding mRNA construct sequence.^{1–3} Polymerases such as T7, T3, or SP6 are added to facilitate IVT, but additional capping is necessary to prevent rapid degradation of uncapped mRNA by RNase, which contains a 5'-ppp group causing heightened immune stimulation.^{4,5} Capping can be achieved through two methods: co-transcriptional and post-transcriptional capping.⁶ Co-transcriptional capping involves incorporating cap dinucleotide mixtures at the 5' end of RNA during transcription, allowing coordinated transcription with mRNA capping.⁷ However, this method encounters challenges such as the competitive incorporation of GTP nucleosides, which can impact capping efficiency. Initially, GTP binds to RNA chains through a 5'-5'

triphosphate bond and undergoes 7-methylation at the 5' terminal guanosine during post-transcriptional capping.⁸ Capping enzymes derived from vaccinia virus are efficient in capping mRNA, producing cap 0, while cap-specific 2'-O methyltransferase can further modify cap 0 to cap 1 or cap 2, reducing mRNA immunogenicity.^{9,10} However, capping can lead to the formation of m7GpppGpG in a reversed linkage, hindering mRNA translation. Anti-reverse cap analogs are synthesized to enhance translation efficiency by modifying the m7G part of caps.^{11,12} Poly(A) tails in IVT mRNAs can be encoded in the DNA template or added enzymatically, with the former method providing more precise control.^{8,13,14} Linearization of plasmid templates using type II restriction enzymes can lead to overhangs at the 3' end of poly(A) tails, affecting translational efficacy, necessitating the use of type IIS restriction enzymes to avoid this issue.^{1,15}

In-vitro-transcribed mRNAs necessitate purification to eliminate immunostimulatory contaminants, free ribonucleotides, as well as short mRNA and DNA templates.^{16–19} DNase is typically used to degrade excess DNA templates, followed by commercial purification kits and precipitation methods using ethanol or isopropanol to obtain high-purity mRNA. Chromatographic methods such as molecular exclusion chromatography, ion-exchange chromatography, or affinity chromatography can further purify mRNA, while reversed-phase HPLC is effective in removing dsRNA contaminants but may not be scalable for large-scale production.^{18,19} Alternatively, RNase III has been proposed for the removal of dsRNA contaminants, and cellulose chromatography has shown promise in purifying IVT mRNAs efficiently and on a larger scale. Gel electrophoresis can also be employed to remove short RNAs and separate long RNAs. Ultimately, the choice of purification method depends on the specific purity requirements and scale of production, with stringent quality control being essential for maximizing the benefits of mRNA therapeutics.¹⁸

<https://doi.org/10.1016/j.omtn.2024.102313>

⁴These authors contributed equally

Correspondence: Fatemeh Kazemi-Lomedasht, Biotechnology Research Center, Pasteur Institute of Iran, Tehran, Iran.

E-mail: fa_kazemi@pasteur.ac.ir



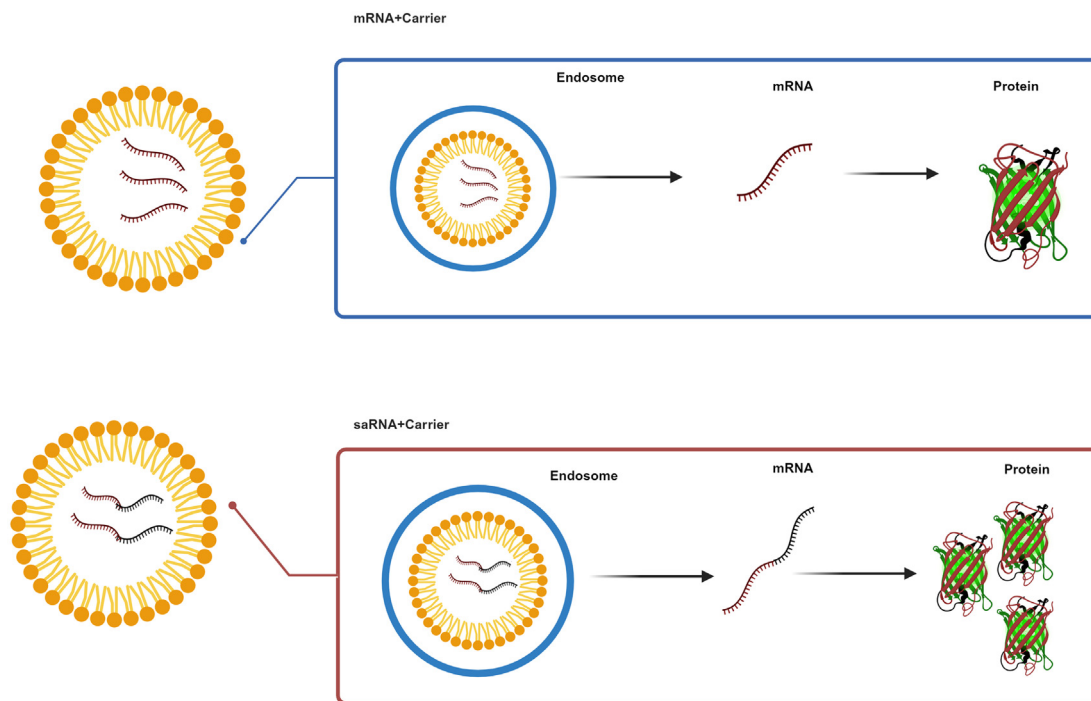


Figure 1. The differences between conventional mRNA and self-amplifying mRNA

saRNA, derived from alphaviruses, self amplifies for efficient protein expression, promising high antibody titers against pathogens.³²

Different formats of mRNA, such as self-amplifying mRNA (saRNA),²⁰ unmodified mRNA with codon usage optimization,²¹ nucleoside-modified mRNA,²² and trans-amplifying mRNA (taRNA),²³ offer distinct advantages and challenges in therapeutic applications. saRNA, derived from alphaviruses, contains a replicase sequence enabling self-amplification and efficient protein expression²⁴ (Figure 1). Despite its longer sequence compared with conventional mRNA, saRNA shows promising results in inducing high antibody titers against pathogens.^{25–28} Unmodified mRNA with codon optimization promotes immunogenicity by augmenting antigen presentation, acting as an adjuvant in mRNA vaccines.²⁹ Nucleoside-modified mRNA, incorporating modified nucleosides such as 2'-O methyl nucleoside, suppresses immune response by inhibiting TLR-mediated dendritic cell activation, potentially improving safety and efficacy.³⁰ taRNA, an advanced version of saRNA, separates the replicase from multiple target mRNAs, allowing simultaneous amplification of various proteins.³¹ This flexibility simplifies transfection protocols and offers potential in infectious disease vaccines. Each mRNA format has its advantages and limitations, highlighting the importance of selecting the appropriate format based on specific therapeutic needs and challenges.

Importance and potential impact on modern medicine

Efficient intracellular delivery of mRNA remains a significant challenge due to its large molecular weight, high negative charge density, and inherent instability. Various strategies, including microinjections, gene gun-based administration, and encapsulation in nanopar-

ticles, have been explored to improve RNA delivery.^{33–37} Formulating mRNA with delivery systems protects it against degradation and facilitates cellular uptake. Mechanisms for mRNA loading include electrostatic interactions, hydrogen bonds, or coordination interactions. Vectors such as lipid nanoparticles (LNPs), polymeric nanoparticles, and cationic nanoemulsions have been engineered to augment mRNA delivery.^{38–40} Optimization of these delivery systems holds promise for enhancing mRNA transfection efficiency, thereby advancing mRNA therapeutics. Examples include LNPs modified with cationic peptides,⁴¹ graphene oxide, and polyethylenimine (PEI) hydrogels carrying mRNA vaccines,⁴² and mesoporous silica nanoparticles encapsulating mRNA and RNA-activated protein kinase inhibitors.⁴³

OBJECTIVES OF THE REVIEW

This review provides a comprehensive overview of the advancements and challenges in mRNA and ribonucleoprotein (RNP)-based therapies, focusing on delivery systems, mechanisms of action, therapeutic applications, and future directions.

Overview of mRNA- and RNP-based therapies

mRNA therapies involve the delivery of mRNA molecules into cells, where they are translated into proteins that can perform therapeutic functions.⁴⁴ The mRNA is designed to encode specific proteins needed to treat or prevent diseases.⁴⁵ RNP therapies involve the use of RNPs, complexes of RNA and proteins, to achieve therapeutic effects.⁴⁶ These therapies often utilize CRISPR-Cas9 technology for

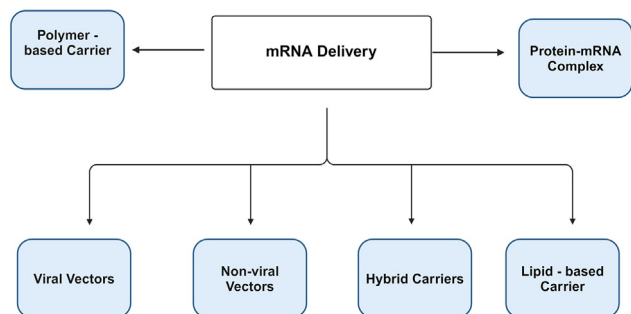


Figure 2. mRNA delivery systems

Efficient mRNA delivery is challenging due to its size and charge.⁴⁸

genome editing, where RNPs can precisely target and modify specific genetic sequences.⁴⁷ While both mRNA and RNP therapies aim to treat diseases at the molecular level, mRNA therapies focus on protein production, whereas RNP therapies primarily involve gene editing. Both approaches offer unique advantages and face specific challenges in terms of delivery, efficiency, and safety.

Advancements in delivery systems

An overview of various delivery systems (different vectors and carriers employed to deliver mRNA effectively into target cells) used for mRNA-based therapies are shown in Figure 2. It includes sections on viral vectors, which utilize modified viruses to deliver genetic material; hybrid carriers, which combine multiple delivery mechanisms; polymer-based carriers, which use synthetic polymers to encapsulate and protect mRNA; lipid-based carriers, such as LNPs, which are commonly used for their efficiency in protecting and delivering mRNA into cells; protein-mRNA complexes, which involve the use of proteins to stabilize and transport mRNA; and non-viral vectors, which include a range of synthetic and natural materials designed to facilitate mRNA delivery without using viral components. These varied approaches are crucial for optimizing the stability, efficiency, and targeting of mRNA-based treatments.

LNPs

Lipid-based carriers, including LNPs and lipoplexes, are extensively utilized for delivering nucleic acids.⁴⁹ Proper engineering allows effective encapsulation of mRNA into LNPs and lipoplexes, protecting it from degradation and facilitating cellular uptake and endosomal escape. Components such as cationic or ionizable lipids, cholesterol, poly(ethylene) glycol (PEG)-lipid, and phospholipids are crucial for mRNA encapsulation and stability.⁵⁰ Precise molar ratios of these components generate LNPs with desired functionalities for mRNA delivery. Optimization studies have focused on factors such as lipid-to-mRNA weight ratio, phospholipid identity, and molar ratios of lipid components to enhance transfection efficiency. Novel cationic or ionizable lipids with modified head or tail groups have been explored to improve delivery efficacy.⁵⁰ In addition, various components such as proteins, vitamins, and aminoglycosides have been utilized to construct effective LNPs for mRNA delivery. For example, mechanism of action of mRNA-LNP vaccines are shown in Figure 3.

Zwitterionic phospholipids have also gained attention for their involvement in endosomal escape membrane via membrane fusion.^{51,52} pH-switchable ionizable phospholipids with multi tails have shown promise in mRNA delivery, exhibiting organ selectivity *in vivo*.⁵³ However, concerns regarding their toxicity, especially those composed of polycationic and pegylated lipids, have been raised in several studies.⁵⁴ Polycationic lipids, known for their ability to encapsulate nucleic acids effectively, can also induce cytotoxic effects due to their positive charge, which may disrupt cellular membranes and lead to cell death.^{55,56} This is particularly relevant in the context of therapeutic applications, where the balance between effective delivery and cellular safety is critical.^{57,58} Pegylated lipids, while enhancing the stability and circulation time of LNPs in the bloodstream, can also elicit immune responses that may lead to adverse effects.⁵⁹ Studies have shown that pegylation can alter the pharmacokinetics of nanoparticles, potentially resulting in unexpected toxicity.⁶⁰ For instance, the formation of anti-PEG antibodies has been documented, which can lead to accelerated clearance of pegylated nanoparticles and reduced therapeutic efficacy.⁶⁰ Furthermore, the accumulation of these nanoparticles in various tissues can provoke inflammatory responses, highlighting the need for careful design and optimization of lipid formulations.⁶⁰

Polymer-based delivery systems

Polymeric nanoparticles are a promising delivery system for mRNA-based therapeutics⁶² (Figure 4). Cationic polymers can complex with mRNA to form nanoparticles called mRNA polyplexes.⁶³ While early materials such as PEI and poly(l-lysine) showed limited *in vivo* efficacy and toxicity, recent attention has turned to functional and biodegradable polymers for better outcomes.⁶⁴ Charge-altering releasable transport (CART) systems, capable of changing charge properties in different pH environments, aid in mRNA release in the cytoplasm, enhancing transfection efficacy.⁶⁵ Several chemical structures of CARTs have been explored successfully. In addition, poly(β -amino esters) (PBAEs) and their derivatives, such as polycaprolactone-based PBAEs and oligopeptide end-modified PBAEs, have shown promise in mRNA delivery by facilitating complex formation and enhancing endosomal escape.⁶⁶ Hyperbranched PBAEs, synthesized with a trifunctional amine, have demonstrated superior stability and transfection efficiency compared with linear PBAEs, particularly in delivering mRNA to the lung epithelium.⁶⁷ Libraries of biodegradable polymers such as poly(amine-co-ester)s have been developed to quantitate endosomal escape, with high encapsulation efficiency identified as a crucial step in mRNA transfection.⁶⁸ Ionizable amphiphilic Janus dendrimers (IAJDs) have emerged as a simple yet effective one-component system for mRNA delivery.⁶⁹ Various IAJDs have been synthesized and evaluated, with some showing high transfection efficacy, while the cation- π interaction has been identified as a potential avenue for further design optimization.⁶⁹

Viral vectors and non-viral delivery methods

Delivery of mRNA can be accomplished using both viral and non-viral vectors.^{71,72} Viral vectors, such as adeno-associated viruses and genetically modified viruses, offer the advantage of local

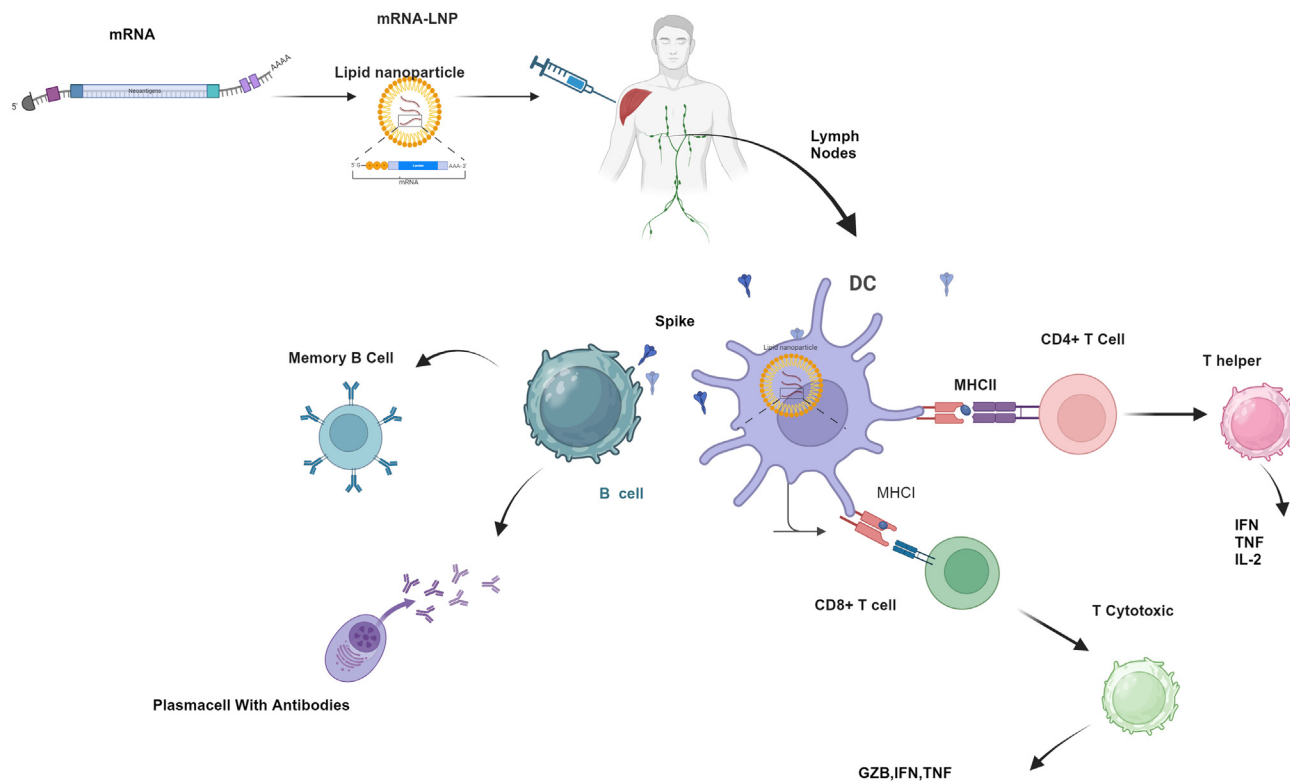


Figure 3. Mechanism of action of mRNA-LNP vaccines

This schematic diagram illustrates the process of how mRNA-LNP (messenger RNA-lipid nanoparticle) vaccines elicit an immune response. (1) mRNA packaging: mRNA encoding the pathogen's spike protein is encapsulated in LNPs to protect it from degradation and aid its delivery into human cells. (2) Delivery and translation: LNPs transport mRNA into dendritic cells (DCs), mainly in the lymph nodes, where it is translated into the spike protein. (3) Antigen presentation: the spike protein is displayed on DCs via MHC molecules, activating CD4+ and CD8+ T cells. (4) T cell activation: CD4+ T cells recognize MHCII-bound spike proteins, secreting cytokines to stimulate immune responses, while CD8+ T cells recognize MHCI-bound proteins and release cytotoxic molecules to kill infected cells. (5) B cell activation and memory: B cells recognize the spike protein, producing antibodies via plasma cells and forming memory B cells for long-term immunity against future infections.⁶¹

replication and expression in the cytoplasm.^{73,74} However, cytotoxic effects and potential host rejection pose challenges for viral vectors. Non-viral vectors include naked mRNA, which can be administered intramuscularly, subcutaneously, or intradermally, bypassing obstacles associated with systemic administration.^{71,75,76} Naked mRNA has demonstrated efficient translation and immune response induction, particularly when administered subcutaneously. Various physical and active methods have been employed to enhance skin penetration and mRNA delivery, including electroporation, microporation, and microneedle-based delivery.⁷⁷ These approaches offer advantages such as reduced cost and potential risk, although naked mRNA faces challenges such as short plasma half-life and susceptibility to degradation. Delivery systems have been developed to protect mRNA and promote cellular uptake, addressing these challenges.⁷⁸

Protein-mRNA complex

Natural positively charged proteins can form complexes with negatively charged mRNA via electrostatic interactions, facilitating the self-assembly of protein-mRNA complexes.⁷⁹ Protamine, a positively charged protein abundant in arginine, has been utilized to complex

with mRNA vaccines, enhancing immune stimulation by activating the TLR7 receptor.⁸⁰ Studies have demonstrated that protamine-complexed mRNA encoding tumor-associated antigens can induce a strong antitumor immune response in mice and metastatic melanoma patients with minimal toxicity.⁸¹ In addition, mammalian retrovirus-like protein PEG10 has been reported as a promising vehicle for mRNA delivery, capable of binding, stabilizing, and delivering mRNA efficiently in human cells, including both single-guide RNA and *Streptococcus pyogenes* Cas9 (SpCas9).^{82–84}

INNOVATIONS IN TARGETED DELIVERY AND TISSUE-SPECIFIC TARGETING

Advancements in targeted delivery, such as tissue-specific ligands and hybrid carriers, aim to improve the precision and efficacy of mRNA and RNP therapies.

Hybrid carriers

Hybrid carriers, combining both lipid and polymer components, offer advantages in mRNA delivery.⁸⁵ These carriers can enhance stability and pharmacokinetics, particularly when decorated with lipid to

prolong circulation time by evading uptake by the reticuloendothelial system.⁸⁵ Organic/inorganic hybrid nanoparticles, including metal-organic frameworks, gold nanoparticles, and graphene oxide-PEI complexes, have shown promise in mRNA delivery.⁸⁶ A study by Choi et al. demonstrated the efficacy of PEI-conjugated graphene oxide in mRNA delivery.⁸⁷ This hybrid nanoparticle increased loading capacity, protected mRNA against degradation, and significantly enhanced transfection efficacy compared with conventional materials.⁸⁷ Wang et al. utilized PEI-modified mesoporous organosilica for mRNA delivery, achieving high transfection efficacy by incorporating large-pore structures and tetrasulfide to activate the mTORC1 pathway.⁸⁸ Lipid/polymer hybrid nanoparticles are also promising mRNA carriers. Islam et al. combined cationic lipid, PLGA, and DSPE-PEG to construct robust hybrid nanoparticles, exhibiting superior transfection efficacy compared with conventional lipids.⁸⁹

MECHANISMS OF ACTION AND THERAPEUTIC TARGETS

Current therapeutic targets (e.g., infectious diseases, cancer, genetic disorders)

mRNA-based therapeutics show great potential for treating a diverse range of challenging diseases, such as infectious diseases, metabolic genetic disorders, cancer, cardiovascular ailments, and others.¹ Multiple studies have illustrated mRNA's advantages over traditional protein and DNA drugs, including enhanced transfection efficiency, prolonged protein expression, and reduced risk of genomic integration.^{90,91} Moreover, mRNA can be synthesized rapidly through IVT, facilitating quick adaptation to various therapies. Chemical modifications of specific nucleotides address concerns regarding immunogenicity and stability, further enhancing the appeal of mRNA therapy.⁹² The burgeoning interest in mRNA has attracted substantial investment, contributing to the establishment of well-funded biotechnology companies such as Moderna, CureVac, BioNTech, and others. These companies are actively engaged in advancing mRNA-based drug technologies, underscoring the significant potential of mRNA in drug development.⁹³

Hematologic diseases

Preclinical studies have investigated mRNA-based protein replacement therapy for hematologic diseases, particularly hemophilia.^{94,95} Hemophilia, characterized by deficiencies in blood coagulation factors, such as factor VIII (hemophilia A) and factor IX (hemophilia B), has been targeted for correction using mRNA technology.⁹⁵ LNPs encapsulating mRNAs encoding different variants of factor VIII (F8) induced rapid and sustained expression of FVIII in hemophilia A mice.⁹⁵ In hemophilia B, mRNA encoding factor IX (FIX) was delivered using lipidoids called TTs, leading to restoration of FIX function in FIX-knockout mice.⁹⁶ In addition, lipid-enabled LUNAR LNPs encapsulating hFIX mRNA showed promising results in treating hemophilia B mice, with a rapid onset of FIX expression lasting up to several days.⁹⁶

Metabolic diseases

mRNA-based therapies offer promise for treating metabolic diseases that currently lack effective treatments. Conditions such as hepatore-

nal tyrosinemia, acute intermittent porphyria, Fabry disease, glycogen storage disease type 1 A, Crigler-Najjar syndrome type 1, and ornithine transcarboxylase deficiency could potentially benefit from mRNA therapies.^{97–103} For instance, in hepatorenal tyrosinemia, dendrimer LNPs loaded with mRNA encoding fumarylacetoacetate-hydrolase were designed to restore liver function in mice models.¹⁰⁴ In acute intermittent porphyria, LNP-encapsulated mRNA induced expression of porphobilinogen deaminase, normalizing urine porphyrin precursor excretion and mitigating porphyria attacks.¹⁰⁵ Methylmalonic acidemia, another metabolic disorder, showed reduction in plasma methylmalonic acid levels with systemic expression of functional mitochondrial methylmalonyl-CoA mutase delivered via LNPs.¹⁰⁶ Hybrid mRNA technology was utilized to deliver ornithine transcarboxylase mRNA, improving plasma ammonia levels and survival in deficient mice.^{103,107} In addition, mRNA therapies have shown promise in treating diseases such as Fabry disease and alpha 1-antitrypsin deficiency.^{108,109} Moreover, mRNA-based therapies have been explored for tumor treatment, with PTEN mRNA delivery inhibiting tumor growth in PTEN-null mice, and p53 mRNA delivery inducing growth inhibition and apoptosis in tumor cells.¹¹⁰ Furthermore, mRNA encoding anti-angiogenic proteins has shown efficacy in inhibiting tumors.¹¹¹

mRNA-based stem cell therapeutics

RNA-based genome editing has emerged as a potent tool for treating a variety of diseases, particularly in stem cell therapy.¹¹² Retroviral vectors have been utilized to deliver ZFN protein, mRNA, and DNA to disrupt targeted genes with high efficiency.¹¹³ ZFN mRNA has demonstrated superior specificity compared with TALEN mRNA and CRISPR-Cas9 mRNA when delivered via electroporation into primary human hematopoietic stem and progenitor cells.¹¹³ Plasmid-derived gRNA and Cas9 mRNA exhibited comparable acute cytotoxicity, emphasizing the need for optimization in CRISPR-Cas9 delivery to these cells. Innovative strategies involving macaque-specific CCR5 ZFN mRNA have enabled successful *ex vivo* modification of hematopoietic stem and progenitor cells in large animal models.^{114–116}

mRNA-based monoclonal antibodies

Nucleic acid-encoded monoclonal antibodies (mAbs), particularly mRNA-based mAbs, hold promise for improving therapy efficacy and reducing production costs compared with traditional mAbs.¹¹⁷ mRNA-mAbs are mainly applied in treating infections and tumors.¹¹⁷ For instance, mRNA encoding the broadly neutralizing anti-HIV-1 antibody VRC01 successfully produced the antibody in mice and protected them from HIV-1 infection.¹¹⁸ Similarly, mRNA encoding neutralizing antibodies against respiratory syncytial virus (RSV) and chikungunya virus (CHKV-24) demonstrated efficacy in inhibiting virus replication and protecting against disease in animal models.^{119,120} In tumor treatment, mRNA-based antibodies induced rapid and sustained serum antibody levels, allowing mice to survive tumor challenges. Delivery methods such as LNPs have been employed to efficiently transfer mRNA-encoding antibodies. Moreover, mRNA-based bispecific T cell-engaging antibodies (bsAbs) showed promising results in inhibiting tumor growth.¹²¹

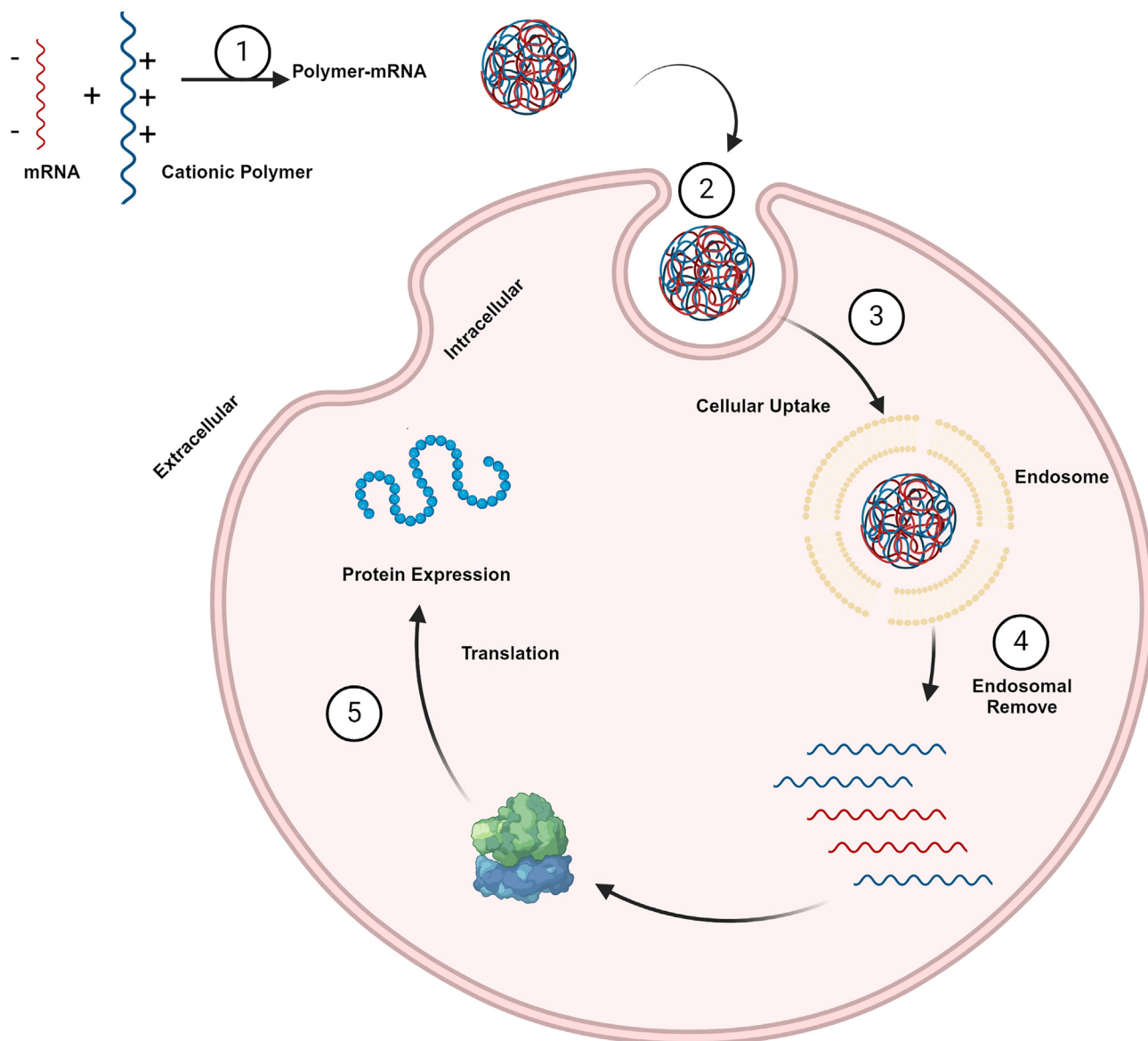


Figure 4. Polymer-mRNA delivery system for protein expression

This schematic diagram illustrates the process of mRNA delivery using a cationic polymer carrier, highlighting the key steps involved in cellular uptake and protein expression. (1) Complex formation: the mRNA (depicted as a red strand) is complexed with a cationic polymer (depicted as a blue strand) to form a polymer-mRNA complex. The cationic polymer protects the mRNA and facilitates its delivery into the cell. (2) Cellular uptake: the polymer-mRNA complex is taken up by the cell through endocytosis, a process where the cell membrane engulfs the complex and brings it into the intracellular environment. (3) Endosomal encapsulation: once inside the cell, the polymer-mRNA complex is encapsulated within an endosome, a membrane-bound vesicle. (4) Endosomal escape: the mRNA is released from the endosome into the cytoplasm. (5) Translation and protein expression: the released mRNA is translated by the cellular machinery to produce the target protein, completing the process of gene expression.⁷⁰

However, some challenges remain, such as safety concerns with certain delivery vectors like those that viral vectors used for SARS-CoV-2 mRNA vaccine development.

Non-formulated mRNA vaccine

Non-formulated mRNA, administered intradermally or intranodally, has proven effective in initiating T cell responses in both mice and hu-

mans.^{21,122–124} Intranodal injection specifically targets dendritic cells in the area of T cell activation, utilizing macropinocytosis for uptake.¹²⁴ Clinical trials with metastatic melanoma patients have demonstrated the safety and feasibility of naked mRNA vaccines, stimulating antigen-specific T cell responses.¹²³ For instance, in melanoma patients, intradermal injection of autologous tumor mRNA combined with GM-CSF enhanced T cell responses. Similarly, in

renal cell carcinoma (RCC) patients, intradermal administration of non-formulated mRNA encoding various antigens along with GM-CSF led to stable disease and partial responses, with a majority of patients showing antigen-specific T cell responses.¹²³

CHALLENGES AND LIMITATIONS

Stability and degradation of mRNA

RNA is inherently unstable and can trigger immune responses, necessitating delivery vehicles for efficient transport to target cells.¹²⁵ Natural RNAs are prone to degradation by native nucleases, but stability can be significantly enhanced through synthetic modifications.¹²⁶ Developing effective carriers to protect RNA from the harsh physiological environment is crucial due to RNA's substantial negative charges and chemical alterations.¹²⁷ These challenges have impeded the clinical advancement of some RNA-based therapies, resulting in varied outcomes in trials. However, recent promising trial results indicate that these obstacles can be surmounted with improved synthetic delivery carriers and chemical modifications of RNA therapeutics. Encapsulating RNA within various carriers protects it from nuclease degradation after systemic administration, thereby enhancing its stability and longevity.^{128–131}

Immunogenicity and immune response

RNA therapy, utilizing RNA-based molecules to influence biological pathways, represents a versatile and specific therapeutic approach with significant potential for treating a diverse array of diseases.¹³² One of major hurdles to advancing RNA therapy is immunogenicity; injected or administered RNAs can be recognized by the immune system as foreign entities, triggering an innate immune response that might reduce the therapeutic efficacy, and possibly cause side effects.¹³³ There have been efforts to address this by modifying the structure or sequence of RNA nucleotides, coding sequence optimization, suppressing the immune system, and packaging RNA within a shielding delivery system.¹³⁴ In a study, researchers have identified a novel method to mitigate the immunogenicity problem. They used an acylating reagent to add acyl groups to the 2'-hydroxyl (OH) groups on RNAs.¹³⁵ Studies have shown that local delivery of naked small interfering RNAs (siRNAs) or aptamers, often preferred for lung, eye, and skin applications, can trigger a proinflammatory response due to the activation of TLRs and suffer from poor cellular uptake and nuclease sensitivity.¹³⁵ In some cases, these issues can be mitigated by encapsulating the nucleic acid with a synthetic carrier or introducing chemical modifications. These strategies are expected to enhance the specificity, stability, and immunoresistance of RNA-based drugs.¹³⁶ Modified ribonucleotides, such as N1-methylpseudouridine, are incorporated into therapeutic mRNAs primarily to reduce their innate immunogenicity.¹³⁷ The reduction of immune recognition is crucial for avoiding hyperinflammatory responses, ensuring that therapeutic mRNA reaches its target cells without being prematurely degraded by the body's innate immune system. These modifications have been essential to the success of mRNA vaccines, allowing them to deliver genetic instructions effectively and with fewer side effects.¹³⁷ However, incorporating N1-methylpseudouridine can lead to +1 ribosomal frameshifting during the translation

of mRNA. These +1 frameshifted products may initiate immune responses, as demonstrated by cellular immunity to these abnormal proteins after vaccination with mRNA vaccines containing N1-methylpseudouridine. This response involves T cells and possibly B cells, indicating the potential for unintended immunogenic effects.^{137,138} Frameshifting is mainly attributed to ribosomal stalling at particular slippery sequences, potentially leading to the synthesis of abnormal proteins. This phenomenon has been observed in both lab-based studies and cultured cells, possibly due to disruptions in aminoacyl-tRNA binding that slow down the translation process.^{139–141} Despite evidence that N1-methylpseudouridine can induce frameshifting, it is important to note that no adverse reactions have been reported in humans who have received mRNA-based SARS-CoV-2 vaccines. The safety of these vaccines has been thoroughly assessed, and frameshifting has not been linked to any major clinical consequences.^{142–144} To reduce the risks associated with frameshifting, researchers have pinpointed synonymous targeting of slippery sequences as an effective method. Optimizing mRNA sequences can reduce the occurrence of frameshifting events, thereby decreasing the production of aberrant proteins. This approach is crucial for enhancing the safety and efficacy of future mRNA-based therapies.¹⁴⁵ Further investigation into alternative ribonucleotide modifications is needed. For instance, using 5-methoxyU has shown to decrease translation efficiency, which could limit its clinical application.¹⁴⁶ Researching various modifications may lead to strategies that maintain low immunogenicity without affecting translation fidelity.¹⁴⁶

Efficiency of delivery and cellular uptake

Recent advancements in nanotechnology and materials science offer promising solutions to the intricate challenges of delivering oligonucleotide drugs, especially for achieving effective intracellular penetration across biological barriers and membranes.¹⁴⁷ Nanoparticle-based drug delivery systems provide several advantages, including the ability to finely tune biophysical parameters such as size, shape, and chemical composition, alongside optimizing biological properties through targeted ligand functionalization.¹⁴⁸ Ensuring efficient RNA delivery into the cytoplasm is critical for successful RNA therapy, as RNA's large size, hydrophilicity, and negative charge hinder its passive diffusion across lipid bilayers.¹⁴⁹ Overcoming extracellular and intracellular barriers involves evading serum nucleases, bypassing macrophage scavenging in the reticuloendothelial system, and navigating through the extracellular matrix via receptor-mediated endocytosis.¹⁵⁰ Effective endosomal escape and non-toxic release of RNAs into the cytoplasm remain significant technical hurdles.¹⁵¹ To address these challenges, researchers are exploring various chemical modifications and engineered delivery formulations to optimize pharmacodynamic and pharmacokinetic profiles. The complexity of delivering RNA-based drugs, due to their larger size compared with traditional therapeutics, underscores the need for precise targeting strategies within the body.

Off-target effects and specificity

Jackson and Linsley reported the first instances of off-target effects using genome-wide microarray profiling.¹⁵² They observed modest alterations (1.5- to 3-fold changes) in the expression of numerous genes

upon transfecting individual siRNA molecules.¹⁵² The degree of complementarity between the siRNA's sense or antisense strand and off-target genes varied widely, resulting in distinct off-target expression profiles for each siRNA sequence.¹⁵³ Off-target effects occur when siRNA is processed by the RNA-induced silencing complex, inadvertently suppressing unintended gene targets.¹⁵⁴ These unintended changes in gene expression can lead to observable phenotypic variations, such as false positives, underscoring the need to elucidate the underlying mechanisms of off-targeting.¹⁵⁵ Understanding these mechanisms is crucial for developing strategies to mitigate off-target effects. Similarly, ribozymes and aptamers encounter challenges related to delivery and off-target toxicity, akin to those faced by siRNAs.^{156,157}

Risks associated with mRNA therapies

Continuous positive PCR tests for SARS-CoV-2 have been observed in patients long after recovery, raising questions about the cause.^{158–160} While reinfection is possible, some studies suggest that these cases are not due to new infections, as no active virus has been isolated from such individuals.^{161–163} One theory is that viral RNA might integrate into the host genome via a reverse transcription mechanism, leading to persistent RNA detection.¹⁶⁴ SARS-CoV-2, an RNA virus, replicates its RNA using an RNA-dependent RNA polymerase. However, nonretroviral RNA viruses such as SARS-CoV-2 could potentially be reverse-transcribed and integrated into host DNA by endogenous reverse transcriptase, such as those from LINE-1 elements.¹⁶⁵ These elements, prevalent in the human genome, can be activated by viral infections, including SARS-CoV-2, potentially explaining the persistent detection of viral RNA. This mechanism might also account for why some patients test positive long after recovery, as integrated viral DNA could lead to RNA expression, mimicking active infection.¹⁶⁶ Zhang et al. provide evidence that SARS-CoV-2 sequences can be reverse-transcribed and integrated into human cell DNA, primarily through endogenous LINE-1 elements. Such integration results in the expression of chimeric virus-host RNAs, possibly affecting clinical outcomes by continuously stimulating immune responses without producing infectious virus. While only a small fraction of cells may express viral sequences, this process could potentially influence the disease course or even trigger autoimmunity. This discovery also highlights potential challenges in using PCR tests to monitor antiviral treatment effectiveness, as they may detect integrated viral sequences rather than active infections.¹⁶⁶ The mRNA vaccines from Moderna and Pfizer-BioNTech use LNPs to deliver synthetic mRNA into human cells. This mRNA encodes the spike protein of SARS-CoV-2, facilitating the immune system's ability to recognize and fight the virus. Importantly, this mRNA does not enter the cell nucleus and thus does not interact with or integrate into human DNA.^{167–169} The cellular machinery translates the mRNA into the spike protein in the cytoplasm, after which the mRNA is naturally degraded by normal cellular processes.¹⁷⁰

CLINICAL APPLICATIONS AND TRIALS

Various RNA-based strategies have been explored extensively in both experimental and clinical settings. There is significant interest in

exploring the synergistic effects of combining mRNA- and RNP-based therapies with other treatments such as immunotherapy or chemotherapy, potentially enhancing patient outcomes. Moving forward from preclinical investigations to clinical trials is crucial to establish the safety and effectiveness of mRNA- and RNP-based therapies in human patients. This progression is essential to pave the way for broader adoption and application of these therapies in clinical practice.¹⁷¹ RNA-based therapeutics have gained initial traction in addressing diseases with clear pathological mechanisms, such as oncology, neurological disorders, and infectious diseases (Table 1)^{172–175}. These therapies are particularly aimed at conditions where conventional treatments have limited efficacy. Ongoing clinical studies are exploring RNA-based approaches for a wide range of incurable diseases. The specific RNA sequence plays a pivotal role in modulating the expression or activity of target molecules. Notably, a significant portion of phase I trials involving antisense oligonucleotide (ASO)-based therapies has progressed to phase II/III trials over the past 5 years, focusing on rare and common diseases, including orphan genetic disorders and cancer. The US FDA has approved several ASO drugs, such as mipomersen and inotersen (notably identified by the -rsen suffix), underscoring their clinical relevance and potential impact.¹⁷⁶ In 2013, the FDA-approved mipomersen as the second ASO drug, targeting homozygous familial hypercholesterolemia. Mipomersen functions by binding to the mRNA sequence of apolipoprotein B-100 (ApoB-100) and cleaving it to reduce cholesterol levels. Other FDA-approved ASO drugs, such as nusinersen, eteplirsen, and golodirsen, modulate target pre-mRNAs' splicing processes. In addition, the FDA has approved three siRNA-based drugs: patisiran, givosiran, and lumasiran, identified by the -siran suffix. Patisiran, approved in 2018, addresses hereditary transthyretin-mediated amyloidosis by targeting transthyretin mRNA to inhibit protein synthesis. Givosiran, the second approved siRNA-based drug, treats acute hepatic porphyria by reducing levels of aminolevulinic acid (ALA) and porphobilinogen, metabolic intermediates in heme biosynthesis pathway, thus alleviating symptoms associated with the disease.^{177,178} Givosiran functions by targeting ALA synthase 1, thereby suppressing its expression and restoring normal heme biosynthesis.¹⁷⁹ Its delivery involves a trivalent N-acetylgalactosamine conjugate attached to the 3' end of its passenger strand, enabling subcutaneous administration and specific targeting of hepatocytes via the asialoglycoprotein receptor. This delivery approach, effective for liver-targeting siRNAs, is widely employed for similar therapeutics. In 2021, the US FDA-approved inclisiran for the treatment of primary hypercholesterolemia or mixed dyslipidemia.^{171,180}

SAFETY AND REGULATORY CONSIDERATIONS

RNA therapy involves using RNA-based molecules to treat or prevent diseases. Unlike DNA therapy, RNA therapy does not pose significant genotoxic effects. In DNA-based therapies, the DNA molecule is introduced into cells using a viral vector, which can integrate into the genome and potentially cause mutations. This risk is mitigated with RNA therapy, as RNA is used instead of DNA. Despite its promise, RNA therapy faces challenges, including poor pharmacological properties, difficulties in intracellular delivery, and immune-related

toxicity. Issues such as off-target binding, sequence-induced toxicity, and oversaturation of the endogenous RNA processing pathway also impact the effectiveness of RNA-based approaches.^{171,181,182}

Innovations in delivery systems and formulation

Effective delivery of RNA-based drugs poses a formidable hurdle in their therapeutic application. Current strategies include integrating targeting elements, encapsulating in lipid-based nanoparticles, or direct administration to specific organs with minimal alteration. Kim et al. emphasize the urgent need for advancing RNA drug delivery techniques as a cornerstone of future research efforts.¹⁸³ RNA therapeutics operate by modulating the expression and function of precise target molecules, offering a novel approach to treating diseases resistant to traditional pharmaceuticals. These therapies hold promise for customization across diverse RNA and protein formats, potentially revolutionizing personalized medicine and addressing unmet needs in rare disease treatments.¹³² Stephenson and Zamecnik's pioneering work in 1978 marked the first therapeutic use of RNA base-pairing, employing an ASO to target the 35S RNA of the Rous sarcoma virus and inhibit viral replication.¹⁸⁴ Nearly two decades later, the US FDA approved the first ASO drug for treating cytomegalovirus retinitis, illustrating a significant milestone in RNA-based therapy.^{185,186} RNA splicing, crucial for removing introns and joining exons in RNA transcripts, was first elucidated in 1977.¹⁸⁷ Variations in splicing are implicated in various human diseases, challenging conventional drug treatments but offering potential targets for RNA-based therapies such as ASOs.^{188,189}

In contrast to the extended development timeline of ASO drugs, the progress from discovery to clinical application of siRNAs was notably swift. RNA interference (RNAi) was initially characterized in 1998, demonstrating potent and specific inhibition of targeted mRNAs in *Caenorhabditis elegans* embryos treated with sense and antisense RNAs.¹⁹⁰ The simplicity and effectiveness of RNAi quickly gained traction in scientific research and applications.¹⁹¹ In 2002, RNAi was shown to inhibit hepatitis C virus replication in mice, prompting widespread exploration of its therapeutic potential.¹⁹² Clinical trials employing RNAi technologies began in 2010, with a notable study using an siRNA targeting the M2 subunit of ribonucleotide reductase to treat melanoma, achieving successful mRNA cleavage via targeted nanoparticle delivery.¹⁹³ Subsequent evaluations led to the approval of the first siRNA-based drug for hereditary transthyretin-mediated amyloidosis in 2018, highlighting the transformative impact of RNA-based therapies in modern medicine.¹³² Chemical modification represents a promising approach for enhancing the delivery of RNA-based drugs. By altering the nucleic acid backbone, ribose ring, and nucleobase, researchers can optimize these molecules to exhibit more favorable drug-like properties. For instance, extensive chemical modifications enable gapmer ASOs to reach various tissues effectively without requiring additional delivery agents. Currently, 8 out of the 10 approved oligonucleotide treatments are administered without the need for supplemental delivery vehicles. However, caution is warranted as certain synthetic nucleotides, such as LNA-modified nucleic acids, have been associated with significant hepatotoxicity risks. In

response, bioengineered RNAi agents have emerged as a promising new class of *in vivo* RNA agents designed with minimal post-transcriptional modifications, offering exciting prospects for future applications.^{132,171}

NEW THERAPEUTIC TARGETS AND APPLICATIONS

Targeting undruggable targets

RNA-based therapeutics offer a significant advantage in their ability to target virtually any genetic component within a cell, including those traditionally considered undruggable by small molecules and antibodies.^{194,195} Noncoding RNAs, particularly small RNAs, are distinguished by their specific RNA sequences, enabling drugs such as antisense RNA and siRNA to bind selectively to their targets.¹⁹⁶ This sequence specificity suggests that these therapies can effectively target noncoding RNAs, which play crucial roles in disease pathogenesis.¹⁹⁷ Given the prevalence of noncoding RNAs in the human genome and their documented significance in various diseases, RNA-based treatments are increasingly recognized for their potential impact and therapeutic relevance.^{198,199}

Less than one-third of human proteins are thought to be suitable targets for small-molecule drugs.^{200–202} This limitation arises from the structural similarities shared among many proteins, which complicates the direct targeting of specific ones.²⁰³ Membrane-integrated proteins pose an additional challenge because their interaction sites within the cytoplasm are limited, making them difficult targets for small molecules or antibodies.²⁰⁴ In contrast, RNA-based drugs offer a different approach by targeting the biogenesis of these proteins. By inhibiting their production, RNA-based therapies have the potential to enhance therapeutic effectiveness in cases where direct protein targeting is challenging.^{205,206} This strategy represents a promising avenue for developing treatments that can address conditions associated with membrane-integrated proteins and other challenging therapeutic targets.^{205,206} Developing new small-molecule- or antibody-based drugs usually involves a lengthy timeline.²⁰⁶ In contrast, once the chemical structure of RNA and its delivery method are determined, RNA-based drugs can be swiftly designed and synthesized for clinical trials.²⁰² For example, an siRNA drug designed to target a disease caused by excessive gene expression in a specific organ can easily be modified to treat other diseases affecting the same organ by adjusting the siRNA sequence.²⁰⁷ This adaptability is evident in the extensive development of siRNA drugs using liver cell-specific conjugates to address various liver metabolism-related disorders.²⁰⁷ This rapid adaptability underscores the potential of RNA-based therapies to quickly respond to emerging medical needs and expand treatment options within specific organs.²⁰⁷

LONG-TERM OUTLOOK AND FUTURE RESEARCH DIRECTIONS

Despite facing substantial hurdles in clinical testing, RNA-based therapeutics have gleaned invaluable insights from previous trials. These efforts have shown early potential in treating cancers, viral infections, and genetic disorders. However, fully realizing the capabilities of RNAi- and RNA-based therapies necessitates advanced delivery

Table 1. Approved and clinical trials for RNA therapeutics

Trade name	Approved and clinical trials	Disease type	Administration route	Delivery system
mRNA: (elasomeran) <i>Moderna</i>	2021 FDA approved	infectious	intramuscular	LNP
mRNA: Comirnaty (tozinameran) <i>Pfizer-BioNTech</i>	2021 FDA approved	infectious	intramuscular	LNP
siRNA: Givlaari (givosiran) <i>Alnylam</i>	2019 FDA approved	genetics	subcutaneous	conjugate (GalNAc)
siRNA: Onpattro (patisiran) <i>Alnylam</i>	2018 FDA approved	genetics	intravenous	LNP
siRNA: Oxlumo (lumasiran) <i>Alnylam</i>	2020 FDA approved	genetics	subcutaneous	conjugate (GalNAc)
siRNA: Leqvio (inclisiran) <i>Novartis</i>	2021 FDA approved	genetic and physiological	subcutaneous	conjugate (GalNAc)
ASO: Vitravene (fomivirsen) <i>Isis Pharmaceuticals</i> —discontinued	1998 FDA approved	infectious	intravitreal	Mod/Sub (PS)
Spinraza (nusinersen) <i>Biogen</i>	2016 FDA approved	genetic	intrathecal	Mod/Subs (2'-MOE, PS, 5-methyl cytosine)
Kynamro (mipomersen) <i>Genzyme</i> —discontinued	2013 FDA approved	genetic	subcutaneous	Mod/Subs (2'-MOE, PS, 5-methyl cytosine)
Tegsedi (inotersen) <i>Akcea</i>	2018 FDA approved	genetic	subcutaneous	Mod/Subs (2'-MOE, PS)
Vyondys 53 (golodisen) <i>Sarepta</i>	2019 FDA approved	genetic	intravenous	Mod/Subs (PMO)
Exondys 51 (eteplirsen) <i>Sarepta</i>	2016 FDA approved	genetic	intravenous	Mod/Subs (PMO)
Milasen <i>Brammer Bio</i>	2018 FDA approved	genetic	intrathecal	Mod/Subs (2'-MOE, PS, 5-methyl cytosine)
Viltepso (viltolarsen) <i>NS Pharma</i>	2020 FDA approved	genetic	intravenous	Mod/Subs (PMO)
Waylivra (volanesorsen) <i>Akcea</i>	2019 EMA	genetic	subcutaneous	Mod/Subs (2'-MOE)
Aptamer: Macugen (pegaptanib) <i>Gilead</i> —discontinued	2004 FDA approved	physiological	intravitreal	conjugate (PEG)
NCT04573140	phase I	cancer	intravenous	liposome
NCT02316457	phase I	cancer	intravenous	liposome
NCT02872025	early phase I	cancer	intralesional	LNP
NCT03897881	phase II	cancer	intravenous	LNP
NCT03871348	phase I	cancer	intratumoral	LNP
NCT03164772	phase I/II	cancer	intradermal	LNP
NCT03948763	phase I	cancer	intradermal	LNP
NCT04163094	phase I	cancer	intravenous	liposome
NCT03313778	phase I	cancer	intramuscular	LNP
NCT04534205	phase II	cancer	intravenous	liposome
NCT05043181	phase I	genetic	intravenous	other (exosome)
NCT04990388	phase I/II	genetic	intravenous	LNP
NCT04442347	phase I	genetic	intravenous	LNP
NCT05130437	phase I/II	genetic	intravenous	LNP
NCT04652102	phase II/III	infectious	intramuscular	LNP
NCT05085366	phase III	infectious	intramuscular	LNP
NCT05001373	phase I	infectious	intramuscular	LNP
NCT04144348	phase I	infectious	intramuscular	LNP

strategies. Innovations such as aptamer-siRNA chimeras and transferrin-decorated nanoparticles are poised to significantly enhance the precision and efficacy of RNA drug delivery. These engineered designs represent crucial advancements in targeting specific tissues and cells, thereby paving the way for broader applications of RNA-based treatments in clinical settings.^{171,172} The future of RNA-based drugs hinges on refining their biochemical properties to optimize potency while reducing off-target toxicity and immunogenicity. Specifically,

siRNAs will require precise chemical modifications to mitigate nonspecific inflammatory responses, alongside the use of natural or synthetic carriers to achieve efficient and targeted delivery to tissues. These considerations have played a pivotal role in yielding promising clinical outcomes for various siRNA drugs such as CALAA-01, TD101, ALN-VSP02, and ALN-RSV01. While these successes highlight the potential of siRNA therapeutics, they also underscore the critical importance of developing tailored carriers that can selectively

target specific cells and tissues, thereby maximizing therapeutic efficacy while minimizing adverse effects. Continued advancements in carrier design and chemical modification strategies are essential for advancing RNA-based therapies into broader clinical applications.¹⁷²

FUTURE DIRECTIONS AND EMERGING TRENDS

Continued research should focus on improving the efficiency of mRNA and RNP delivery systems, particularly addressing challenges such as off-target effects, RNP denaturation during production, and encapsulation efficiency. Developing strategies for precise tissue-specific targeting of mRNA- and RNP-loaded LNPs will be crucial for enhancing therapeutic outcomes while minimizing off-target effects.²⁰⁸ The field of mRNA- and RNP-based therapies holds immense promise for revolutionizing disease treatment, ranging from cancer therapy to infectious diseases. Significant progress has been made in developing delivery systems, such as LNPs, to efficiently transport mRNA and RNPs into target cells, enabling precise genome editing and protein expression. Despite remaining challenges, including optimization of delivery efficiency and tissue-specific targeting, ongoing research efforts continue to drive innovation in this rapidly evolving field.²⁰⁸ With continued advancements and translation into clinical practice, mRNA- and RNP-based therapies have the potential to significantly impact the landscape of modern medicine, offering new hope for patients with a wide range of diseases.¹³²

CONCLUSION

RNA-based approaches encompass a diverse array of techniques applied in both experimental settings and clinical trials. Widely utilized methods include commoditized ASOs, siRNAs, antagomirs, and aptamers, which are instrumental in manipulating mRNA expression levels and inhibiting noncoding RNA functions through specific RNA targeting. Several ASOs, siRNAs, aptamers, and mRNA vaccines have received clinical approval, underscoring their therapeutic potential. Despite these advancements, the primary challenge hindering broader adoption of RNA-based therapies lies in effectively delivering these drugs to target organs and tissues beyond the liver. Issues such as off-target binding, sequence-induced toxicity, and saturation of endogenous RNA processing pathways can also impact treatment efficacy. To address these challenges, enhancing RNA drug delivery efficiency through chemical modifications and conjugation with nanocarrier systems holds promise. Continued research into RNA-based therapeutics, including the exploration of RNA molecules as therapeutic agents and their targeting with small molecules, will drive advancements toward more effective treatments for patients.

ACKNOWLEDGMENTS

The authors would like to thank the Pasteur Institute of Iran for supporting this study.

AUTHOR CONTRIBUTIONS

Writing – review & editing, Z.E., H.Z., A.O., T.E., F.S.S., M.B., and F.K.-L.; conceptualization, F.K.-L.; supervision, F.K.-L.

DECLARATION OF INTERESTS

The authors declare no competing interests.

REFERENCES

- Sahin, U., Karikó, K., and Türeci, Ö. (2014). mRNA-based therapeutics—developing a new class of drugs. *Nat. Rev. Drug Discov.* 13, 759–780.
- Caruthers, M.H. (2011). A brief review of DNA and RNA chemical synthesis. *Biochem. Soc. Trans.* 39, 575–580.
- Kang, D.D., Li, H., and Dong, Y. (2023). Advancements of *in vitro* transcribed mRNA (IVT mRNA) to enable translation into the clinics. *Adv. Drug Deliv. Rev.* 199, 114961.
- Tabor, S., and Richardson, C.C. (1985). A bacteriophage T7 RNA polymerase/promoter system for controlled exclusive expression of specific genes. *Proc. Natl. Acad. Sci. USA* 82, 1074–1078.
- Thiel, V., Herold, J., Schelle, B., and Siddell, S.G. (2001). Infectious RNA transcribed *in vitro* from a cDNA copy of the human coronavirus genome cloned in vaccinia virus. *J. Gen. Virol.* 82, 1273–1281.
- Fabrega, C., Hausmann, S., Shen, V., Shuman, S., and Lima, C.D. (2004). Structure and mechanism of mRNA cap (guanine-N7) methyltransferase. *Mol. Cell* 13, 77–89.
- Stepinski, J., Waddell, C., Stolarski, R., Darzynkiewicz, E., and Rhoads, R.E. (2001). Synthesis and properties of mRNAs containing the novel “anti-reverse” cap analogs 7-methyl (3'-O-methyl) GpppG and 7-methyl (3'-deoxy) GpppG. *Rna* 7, 1486–1495.
- Mockey, M., Gonçalves, C., Dupuy, F.P., Lemoine, F.M., Pichon, C., and Midoux, P. (2006). mRNA transfection of dendritic cells: synergistic effect of ARCA mRNA capping with Poly (A) chains in cis and in trans for a high protein expression level. *Biochem. Biophys. Res. Commun.* 340, 1062–1068.
- Kuhn, A.N., Diken, M., Kreiter, S., Selmi, A., Kowalska, J., Jemielity, J., Darzynkiewicz, E., Huber, C., Türeci, O., and Sahin, U. (2010). Phosphorothioate cap analogs increase stability and translational efficiency of RNA vaccines in immature dendritic cells and induce superior immune responses *in vivo*. *Gene Ther.* 17, 961–971.
- Williams, G.D., Gokhale, N.S., Snider, D.L., and Horner, S.M. (2020). The mRNA cap 2'-O-methyltransferase CMTR1 regulates the expression of certain interferon-stimulated genes. *mSphere* 5, e00202-20. <https://doi.org/10.1128/msphere.00202-00220>.
- Henderson, J.M., Ujita, A., Hill, E., Yousif-Rosales, S., Smith, C., Ko, N., McReynolds, T., Cabral, C.R., Escamilla-Powers, J.R., and Houston, M.E. (2021). Cap 1 messenger RNA synthesis with co-transcriptional cleancap® analog by *in vitro* transcription. *Curr. Protoc.* 1, e39.
- Egloff, M.P., Benarroch, D., Selisko, B., Romette, J.L., and Canard, B. (2002). An RNA cap (nucleoside-2'-O-)methyltransferase in the flavivirus RNA polymerase NS5: crystal structure and functional characterization. *EMBO J.*
- Meijer, H.A., Bushell, M., Hill, K., Gant, T.W., Willis, A.E., Jones, P., and de Moor, C.H. (2007). A novel method for poly (A) fractionation reveals a large population of mRNAs with a short poly (A) tail in mammalian cells. *Nucleic Acids Res.* 35, e132.
- Park, J., Kim, M., Yi, H., Baeg, K., Choi, Y., Lee, Y.-S., Lim, J., and Kim, V.N. (2023). Short poly (A) tails are protected from deadenylation by the LARP1–PABP complex. *Nat. Struct. Mol. Biol.* 30, 330–338.
- Zhao, J., Hyman, L., and Moore, C. (1999). Formation of mRNA 3' ends in eukaryotes: mechanism, regulation, and interrelationships with other steps in mRNA synthesis. *Microbiol. Mol. Biol. Rev.* 63, 405–445.
- Pardi, N., Hogan, M.J., Porter, F.W., and Weissman, D. (2018). mRNA vaccines—a new era in vaccinology. *Nat. Rev. Drug Discov.* 17, 261–279.
- Plotkin, S., Robinson, J.M., Cunningham, G., Iqbal, R., and Larsen, S. (2017). The complexity and cost of vaccine manufacturing—an overview. *Vaccine* 35, 4064–4071.
- Rosa, S.S., Prazeres, D.M.F., Azevedo, A.M., and Marques, M.P.C. (2021). mRNA vaccines manufacturing: Challenges and bottlenecks. *Vaccine* 39, 2190–2200.
- Karikó, K., Muramatsu, H., Ludwig, J., and Weissman, D. (2011). Generating the optimal mRNA for therapy: HPLC purification eliminates immune activation and improves translation of nucleoside-modified, protein-encoding mRNA. *Nucleic Acids Res.* 39, e142.

20. Fuller, D.H., and Berglund, P. (2020). Amplifying RNA vaccine development. *N. Engl. J. Med.* *382*, 2469–2471.
21. Lutz, J., Lazzaro, S., Habbedine, M., Schmidt, K.E., Baumhof, P., Mui, B.L., Tam, Y.K., Madden, T.D., Hope, M.J., Heidenreich, R., and Fotin-Mlecsek, M. (2017). Unmodified mRNA in LNPs constitutes a competitive technology for prophylactic vaccines. *NPJ Vaccines* *2*, 29.
22. Pardi, N., and Weissman, D. (2017). Nucleoside modified mRNA vaccines for infectious diseases. *Methods Mol. Biol.* *1499*, 109–121.
23. Lundstrom, K. (2023). Trans-amplifying RNA: Translational application in gene therapy. *Mol. Ther.* *31*, 1507–1508.
24. Li, Y., Teague, B., Zhang, Y., Su, Z., Porter, E., Dobosh, B., Wagner, T., Irvine, D.J., and Weiss, R. (2019). In vitro evolution of enhanced RNA replicons for immunotherapy. *Sci. Rep.* *9*, 6932.
25. Maruggi, G., Ulmer, J.B., Rappuoli, R., and Yu, D. (2021). Self-amplifying mRNA-based Vaccine Technology and its Mode of Action. *Curr. Top. Microbiol. Immunol.* *440*, 31–70.
26. Geall, A.J., Verma, A., Otten, G.R., Shaw, C.A., Hekele, A., Banerjee, K., Cu, Y., Beard, C.W., Brito, L.A., Krucker, T., et al. (2012). Nonviral delivery of self-amplifying RNA vaccines. *Proc. Natl. Acad. Sci. USA* *109*, 14604–14609.
27. Mandl, C.W., Aberle, J.H., Aberle, S.W., Holzmann, H., Allison, S.L., and Heinz, F.X. (1998). In vitro-synthesized infectious RNA as an attenuated live vaccine in a flavivirus model. *Nat. Med.* *4*, 1438–1440.
28. Blakney, A.K., McKay, P.F., Bouton, C.R., Hu, K., Samnuan, K., and Shattock, R.J. (2021). Innate inhibiting proteins enhance expression and immunogenicity of self-amplifying RNA. *Mol. Ther.* *29*, 1174–1185.
29. Kauffman, K.J., Mir, F.F., Jhunjhunwala, S., Kaczmarek, J.C., Hurtado, J.E., Yang, J.H., Webber, M.J., Kowalski, P.S., Heartlein, M.W., DeRosa, F., and Anderson, D.G. (2016). Efficacy and immunogenicity of unmodified and pseudouridine-modified mRNA delivered systemically with lipid nanoparticles *in vivo*. *Biomaterials* *109*, 78–87.
30. Kariko, K., and Weissman, D. (2007). Naturally occurring nucleoside modifications suppress the immunostimulatory activity of RNA: implication for therapeutic RNA development. *Curr. Opin. Drug Discov. Dev* *10*, 523.
31. Beissert, T., Perkovic, M., Vogel, A., Erbar, S., Walzer, K.C., Hempel, T., Brill, S., Haefner, E., Becker, R., Türeci, Ö., and Sahin, U. (2020). A trans-amplifying RNA vaccine strategy for induction of potent protective immunity. *Mol. Ther.* *28*, 119–128.
32. Maruggi, G., Zhang, C., Li, J., Ulmer, J.B., and Yu, D. (2019). mRNA as a transformative technology for vaccine development to control infectious diseases. *Mol. Ther.* *27*, 757–772.
33. Moody, S.A. (2018). Microinjection of mRNAs and Oligonucleotides. *Cold Spring Harbor Protoc.* *2018*, Pdb.Prot097261.
34. Golombek, S., Pilz, M., Steine, H., Kochba, E., Levin, Y., Lunter, D., Schlensak, C., Wendel, H.P., and Avci-Adali, M. (2018). Intradermal delivery of synthetic mRNA using hollow microneedles for efficient and rapid production of exogenous proteins in skin. *Mol. Ther. Nucleic Acids* *11*, 382–392.
35. Jones, V.A.S., Bucher, M., Hambleton, E.A., and Guse, A. (2018). Microinjection to deliver protein, mRNA, and DNA into zygotes of the cnidarian endosymbiosis model *Aiptasia* sp. *Sci. Rep.* *8*, 16437.
36. Wang, S., Zhang, C., Zhang, L., Li, J., Huang, Z., and Lu, S. (2008). The relative immunogenicity of DNA vaccines delivered by the intramuscular needle injection, electroporation and gene gun methods. *Vaccine* *26*, 2100–2110.
37. Hou, X., Zaks, T., Langer, R., and Dong, Y. (2021). Lipid nanoparticles for mRNA delivery. *Nat. Rev. Mater.* *6*, 1078–1094.
38. Su, X., Fricke, J., Kavanagh, D.G., and Irvine, D.J. (2011). In vitro and *in vivo* mRNA delivery using lipid-enveloped pH-responsive polymer nanoparticles. *Mol. Pharm.* *8*, 774–787.
39. Park, Y., Moses, A.S., Demessie, A.A., Singh, P., Lee, H., Korzun, T., Taratula, O.R., Alani, A.W.G., and Taratula, O. (2022). Poly (aspartic acid)-Based polymeric nanoparticle for local and systemic mRNA delivery. *Mol. Pharm.* *19*, 4696–4704.
40. Brito, L.A., Chan, M., Shaw, C.A., Hekele, A., Carsillo, T., Schaefer, M., Archer, J., Seubert, A., Otten, G.R., Beard, C.W., et al. (2014). A cationic nanoemulsion for the delivery of next-generation RNA vaccines. *Mol. Ther.* *22*, 2118–2129.
41. Lou, G., Anderluzzi, G., Schmidt, S.T., Woods, S., Gallorini, S., Brazzoli, M., Giusti, F., Ferlenghi, I., Johnson, R.N., Roberts, C.W., et al. (2020). Delivery of self-amplifying mRNA vaccines by cationic lipid nanoparticles: The impact of cationic lipid selection. *J. Control. Release* *325*, 370–379.
42. Jiao, L., Wang, Z., Song, Z., Zhang, T., Yu, L., Yu, R., Gao, Q., Peng, S., Jin, H., Wang, D., and Liu, Z. (2023). Lentinan-functionalized graphene oxide hydrogel as a sustained antigen delivery system for vaccines. *Int. J. Biol. Macromol.* *253*, 126629.
43. Khaliq, N.U., Lee, J., Kim, J., Kim, Y., Yu, S., Kim, J., Kim, S., Sung, D., and Kim, H. (2023). Mesoporous Silica Nanoparticles as a Gene Delivery Platform for Cancer Therapy. *Pharmaceutics* *15*, 1432.
44. Kowalski, P.S., Rudra, A., Miao, L., and Anderson, D.G. (2019). Delivering the messenger: advances in technologies for therapeutic mRNA delivery. *Mol. Ther.* *27*, 710–728.
45. Gu, Y., Duan, J., Yang, N., Yang, Y., and Zhao, X. (2022). mRNA vaccines in the prevention and treatment of diseases. *MedComm* *3*, e167.
46. Bloomer, H., Khirallah, J., Li, Y., and Xu, Q. (2022). CRISPR/Cas9 ribonucleoprotein-mediated genome and epigenome editing in mammalian cells. *Adv. Drug Deliv. Rev.* *181*, 114087.
47. Campbell, L.A., Richie, C.T., Maggirwar, N.S., and Harvey, B.K. (2019). Cas9 ribonucleoprotein complex delivery: methods and applications for neuroinflammation. *J. Neuroimmune Pharmacol.* *14*, 565–577.
48. Hameed, S.A., Paul, S., Dellosa, G.K.Y., Jaraquemada, D., and Bello, M.B. (2022). Towards the future exploration of mucosal mRNA vaccines against emerging viral diseases; lessons from existing next-generation mucosal vaccine strategies. *NPJ Vaccines* *7*, 71.
49. Zhang, W., Jiang, Y., He, Y., Boucetta, H., Wu, J., Chen, Z., and He, W. (2023). Lipid carriers for mRNA delivery. *Acta Pharm. Sin. B* *13*, 4105–4126.
50. Sun, D., and Lu, Z.-R. (2023). Structure and function of cationic and ionizable lipids for nucleic acid delivery. *Pharm. Res. (N. Y.)* *40*, 27–46.
51. Khunsuk, P.-O., Pongma, C., Palaga, T., and Hoven, V.P. (2023). Zwitterionic Polymer-Decorated Lipid Nanoparticles for mRNA Delivery in Mammalian Cells. *Biomacromolecules* *24*, 5654–5665.
52. Liu, S., Wang, X., Yu, X., Cheng, Q., Johnson, L.T., Chatterjee, S., Zhang, D., Lee, S.M., Sun, Y., Lin, T.C., et al. (2021). Zwitterionic phospholipidation of cationic polymers facilitates systemic mRNA delivery to spleen and lymph nodes. *J. Am. Chem. Soc.* *143*, 21321–21330.
53. Liu, S., Cheng, Q., Wei, T., Yu, X., Johnson, L.T., Farbiak, L., and Siegwart, D.J. (2021). Membrane-destabilizing ionizable phospholipids for organ-selective mRNA delivery and CRISPR–Cas gene editing. *Nat. Mater.* *20*, 701–710.
54. Lv, H., Zhang, S., Wang, B., Cui, S., and Yan, J. (2006). Toxicity of cationic lipids and cationic polymers in gene delivery. *J. Control. Release* *114*, 100–109.
55. Kedmi, R., Ben-Arie, N., and Peer, D. (2010). The systemic toxicity of positively charged lipid nanoparticles and the role of Toll-like receptor 4 in immune activation. *Biomaterials* *31*, 6867–6875.
56. Xue, H.Y., Narvikar, M., Zhao, J.-B., and Wong, H.L. (2013). Lipid encapsulation of cationic polymers in hybrid nanocarriers reduces their non-specific toxicity to breast epithelial cells. *Pharm. Res. (N. Y.)* *30*, 572–583.
57. Campos, J., Severino, P., Santini, A., Silva, A., Shegokar, R., Souto, S., and Souto, E.B. (2020). Solid lipid nanoparticles (SLN): prediction of toxicity, metabolism, fate and physicochemical properties. *Nanopharmaceutics* *1*, 1–15.
58. Reichmuth, A.M., Oberli, M.A., Jaklenec, A., Langer, R., and Blankschtein, D. (2016). mRNA vaccine delivery using lipid nanoparticles. *Ther. Deliv.* *7*, 319–334.
59. Sharma, A., Madhunapantula, S.V., and Robertson, G.P. (2012). Toxicological considerations when creating nanoparticle-based drugs and drug delivery systems. *Expert Opin. Drug Metab. Toxicol.* *8*, 47–69.
60. Tenchov, R., Sasso, J.M., and Zhou, Q.A. (2023). PEGylated lipid nanoparticle formulations: immunological safety and efficiency perspective. *Bioconjug. Chem.* *34*, 941–960.

61. Lee, J., Woodruff, M.C., Kim, E.H., and Nam, J.-H. (2023). Knife's edge: Balancing immunogenicity and reactogenicity in mRNA vaccines. *Exp. Mol. Med.* 55, 1305–1313.
62. Yang, W., Mixich, L., Boonstra, E., and Cabral, H. (2023). Polymer-based mRNA delivery strategies for advanced therapies. *Adv. Healthc. Mater.* 12, 2202688.
63. Uchida, S., and Kataoka, K. (2019). Design concepts of polyplex micelles for *in vivo* therapeutic delivery of plasmid DNA and messenger RNA. *J. Biomed. Mater. Res.* 107, 978–990.
64. Nimesh, S., Gupta, N., and Chandra, R. (2011). Cationic polymer based nanocarriers for delivery of therapeutic nucleic acids. *J. Biomed. Nanotechnol.* 7, 504–520.
65. McKinlay, C.J., Benner, N.L., Haabeth, O.A., Waymouth, R.M., and Wender, P.A. (2018). Enhanced mRNA delivery into lymphocytes enabled by lipid-varied libraries of charge-altering releasable transporters. *Proc. Natl. Acad. Sci. USA* 115, E5859–E5866.
66. Karlsson, J., Rhodes, K.R., Green, J.J., and Tzeng, S.Y. (2020). Poly (beta-amino ester)s as gene delivery vehicles: challenges and opportunities. *Expert Opin. Drug Deliv.* 17, 1395–1410.
67. Patel, A.K., Kaczmarek, J.C., Bose, S., Kauffman, K.J., Mir, F., Heartlein, M.W., DeRosa, F., Langer, R., and Anderson, D.G. (2019). Inhaled nanoformulated mRNA polyplexes for protein production in lung epithelium. *Adv. Mater.* 31, 1805116.
68. Cui, J. (2017). Poly (Amine-co-ester) Nanoparticles for the Delivery of siRNA Therapeutics (Yale University).
69. Chen, J., Zhu, D., Liu, X., and Peng, L. (2022). Amphiphilic dendrimer vectors for RNA delivery: State-of-the-art and future perspective. *Acc. Mater. Res.* 3, 484–497.
70. Huang, P., Deng, H., Zhou, Y., and Chen, X. (2022). The roles of polymers in mRNA delivery. *Matter* 5, 1670–1699.
71. Guan, S., and Rosenecker, J. (2017). Nanotechnologies in delivery of mRNA therapeutics using nonviral vector-based delivery systems. *Gene Ther.* 24, 133–143.
72. Schott, J.W., Galla, M., Godinho, T., Baum, C., and Schambach, A. (2011). Viral and non-viral approaches for transient delivery of mRNA and proteins. *Curr. Gene Ther.* 11, 382–398.
73. Wang, D., Tai, P.W.L., and Gao, G. (2019). Adeno-associated virus vector as a platform for gene therapy delivery. *Nat. Rev. Drug Discov.* 18, 358–378.
74. Ballesteros-Briones, M.C., Silva-Pilipich, N., Herrador-Cañete, G., Vanrell, L., and Smerdou, C. (2020). A new generation of vaccines based on alphavirus self-amplifying RNA. *Curr. Opin. Virol.* 44, 145–153.
75. Ibba, M.L., Ciccone, G., Esposito, C.L., Catuogno, S., and Giangrande, P.H. (2021). Advances in mRNA non-viral delivery approaches. *Adv. Drug Deliv. Rev.* 177, 113930.
76. Yan, Y., Liu, X.-Y., Lu, A., Wang, X.-Y., Jiang, L.-X., and Wang, J.-C. (2022). Non-viral vectors for RNA delivery. *J. Control. Release* 342, 241–279.
77. Chakraborty, C., Bhattacharya, M., and Lee, S.-S. (2023). Current Status of Microneedle Array Technology for Therapeutic Delivery: From Bench to Clinic. *Mol. Biotechnol.* 65, 1–23.
78. Wadhwa, A., Aljabbari, A., Lokras, A., Foged, C., and Thakur, A. (2020). Opportunities and challenges in the delivery of mRNA-based vaccines. *Pharmaceutics* 12, 102.
79. Rissland, O.S. (2017). The organization and regulation of mRNA–protein complexes. *Wiley Interdiscip. Rev. RNA* 8, e1369.
80. Jarzebska, N.T., Lauchli, S., Iselin, C., French, L.E., Johansen, P., Guenova, E., Kündig, T.M., and Pascolo, S. (2020). Functional differences between protamine preparations for the transfection of mRNA. *Drug Deliv.* 27, 1231–1235.
81. Mai, Y., Guo, J., Zhao, Y., Ma, S., Hou, Y., and Yang, J. (2020). Intranasal delivery of cationic liposome-protamine complex mRNA vaccine elicits effective anti-tumor immunity. *Cell. Immunol.* 354, 104143.
82. Segel, M., Lash, B., Song, J., Ladha, A., Liu, C.C., Jin, X., Mekhedov, S.L., Macrae, R.K., Koonin, E.V., and Zhang, F. (2021). Mammalian retrovirus-like protein PEG10 packages its own mRNA and can be pseudotyped for mRNA delivery. *Science* 373, 882–889.
83. Asencio, C., Hervé, P., Morand, P., Oliveres, Q., Morel, C.A., Prouzet-Mauleon, V., Biran, M., Monic, S., Bonhivers, M., Robinson, D.R., et al. (2023). Streptococcus pyogenes Cas9 ribonucleoprotein delivery for efficient, rapid and marker-free gene editing in *Trypanosoma* and *Leishmania*. *Mol. Microbiol.* 121, 1079–1094.
84. Yadav, M., Atala, A., and Lu, B. (2022). Developing all-in-one virus-like particles for Cas9 mRNA/single guide RNA co-delivery and aptamer-containing lentiviral vectors for improved gene expression. *Int. J. Biol. Macromol.* 209, 1260–1270.
85. Zhao, W., Zhang, C., Li, B., Zhang, X., Luo, X., Zeng, C., Li, W., Gao, M., and Dong, Y. (2018). Lipid polymer hybrid nanomaterials for mRNA delivery. *Cell. Mol. Bioeng.* 11, 397–406.
86. Kashapov, R., Ibragimova, A., Pavlov, R., Gabdrakhmanov, D., Kashapova, N., Burilova, E., Zakharova, L., and Sinyashin, O. (2021). Nanocarriers for biomedicine: From lipid formulations to inorganic and hybrid nanoparticles. *Int. J. Mol. Sci.* 22, 7055.
87. Choi, H.Y., Lee, T.-J., Yang, G.-M., Oh, J., Won, J., Han, J., Jeong, G.J., Kim, J., Kim, J.H., Kim, B.S., and Cho, S.G. (2016). Efficient mRNA delivery with graphene oxide-polyethylenimine for generation of footprint-free human induced pluripotent stem cells. *J. Control. Release* 235, 222–235.
88. Wang, Y., Song, H., Liu, C., Zhang, Y., Kong, Y., Tang, J., Yang, Y., and Yu, C. (2021). Confined growth of ZIF-8 in dendritic mesoporous organosilica nanoparticles as bioregulators for enhanced mRNA delivery *in vivo*. *Natl. Sci. Rev.* 8, nwa268.
89. Islam, M.A., Xu, Y., Tao, W., Ubellacker, J.M., Lim, M., Aum, D., Lee, G.Y., Zhou, K., Zope, H., Yu, M., et al. (2018). Restoration of tumour-growth suppression *in vivo* via systemic nanoparticle-mediated delivery of PTEN mRNA. *Nat. Biomed. Eng.* 2, 850–864.
90. Kallen, K.-J., and Theß, A. (2014). A development that may evolve into a revolution in medicine: mRNA as the basis for novel, nucleotide-based vaccines and drugs. *Ther. Adv. Vaccines* 2, 10–31.
91. Tavernier, G., Andries, O., Demeester, J., Sanders, N.N., De Smedt, S.C., and Rejman, J. (2011). mRNA as gene therapeutic: how to control protein expression. *J. Control. Release* 150, 238–247.
92. Franco, M.K., and Koutmou, K.S. (2022). Chemical modifications to mRNA nucleobases impact translation elongation and termination. *Biophys. Chem.* 285, 106780.
93. Webb, C., Ip, S., Bathula, N.V., Popova, P., Soriano, S.K.V., Ly, H.H., Eryilmaz, B., Nguyen Huu, V.A., Broadhead, R., Rabel, M., et al. (2022). Current status and future perspectives on mRNA drug manufacturing. *Mol. Pharm.* 19, 1047–1058.
94. DeRosa, F., Guild, B., Karve, S., Smith, L., Love, K., Dorkin, J.R., Kauffman, K.J., Zhang, J., Yahalom, B., Anderson, D.G., and Heartlein, M.W. (2016). Therapeutic efficacy in a hemophilia B model using a biosynthetic mRNA liver depot system. *Gene Ther.* 23, 699–707.
95. Chen, C.-Y., Tran, D.M., Cavedon, A., Cai, X., Rajendran, R., Lyle, M.J., Martini, P.G.V., and Miao, C.H. (2020). Treatment of hemophilia A using factor VIII messenger RNA lipid nanoparticles. *Mol. Ther. Nucleic Acids* 20, 534–544.
96. Russick, J., Delignat, S., Milanov, P., Christophe, O., Boros, G., Denis, C.V., Lenting, P.J., Kaveri, S.V., and Lacroix-Desmazes, S. (2020). Correction of bleeding in experimental severe hemophilia A by systemic delivery of factor VIII-encoding mRNA. *Haematologica* 105, 1129–1137.
97. Miliotou, A.N., Pappas, I.S., Spyroulias, G., Vlachaki, E., Tsiftoglou, A.S., Vizirianakis, I.S., and Papadopoulou, L.C. (2021). Development of a novel PTD-mediated IVT-mRNA delivery platform for potential protein replacement therapy of metabolic/genetic disorders. *Mol. Ther. Nucleic Acids* 26, 694–710.
98. Cacicedo, M.L., Weindl-Tenbruck, C., Frank, D., Wirsching, S., Straub, B.K., Hauke, J., Okun, J.G., Horscroft, N., Hennermann, J.B., Zepp, F., et al. (2022). mRNA-based therapy proves superior to the standard of care for treating hereditary tyrosinemia 1 in a mouse model. *Mol. Ther. Methods Clin. Dev.* 26, 294–308.
99. Jiang, L., Berraondo, P., Jericó, D., Guey, L.T., Sampedro, A., Frassetto, A., Benenato, K.E., Burke, K., Santamaría, E., Alegre, M., et al. (2018). Systemic messenger RNA as an etiological treatment for acute intermittent porphyria. *Nat. Med.* 24, 1899–1909.
100. Zhu, X., Yin, L., Theisen, M., Zhuo, J., Siddiqui, S., Levy, B., Presnyak, V., Frassetto, A., Milton, J., Salerno, T., et al. (2019). Systemic mRNA therapy for the treatment of Fabry disease: preclinical studies in wild-type mice, Fabry mouse model, and wild-type non-human primates. *Am. J. Hum. Genet.* 104, 625–637.

101. Cao, J., Choi, M., Guadagnin, E., Soty, M., Silva, M., Verzieux, V., Weisser, E., Markel, A., Zhuo, J., Liang, S., et al. (2021). mRNA therapy restores euglycemia and prevents liver tumors in murine model of glycogen storage disease. *Nat. Commun.* *12*, 3090.
102. Greig, J.A., Chorazeczewski, J.K., Chowdhary, V., Smith, M.K., Jennis, M., Tarrant, J.C., Buza, E.L., Coughlan, K., Martini, P.G.V., and Wilson, J.M. (2023). Lipid nanoparticle-encapsulated mRNA therapy corrects serum total bilirubin level in Crigler-Najjar syndrome mouse model. *Mol. Ther. Methods Clin. Dev.* *29*, 32–39.
103. Yamazaki, K., Kubara, K., Ishii, S., Kondo, K., Suzuki, Y., Miyazaki, T., Mitsuhashi, K., Ito, M., and Tsukahara, K. (2023). Lipid nanoparticle-targeted mRNA formulation as a treatment for ornithine-transcarbamylase deficiency model mice. *Mol. Ther. Nucleic Acids* *33*, 210–226.
104. Cheng, Q., Wei, T., Jia, Y., Farbiak, L., Zhou, K., Zhang, S., Wei, Y., Zhu, H., and Siegwart, D.J. (2018). Dendrimer-based lipid nanoparticles deliver therapeutic FAH mRNA to normalize liver function and extend survival in a mouse model of hepatorenal tyrosinemia type I. *Adv. Mater.* *30*, 1805308.
105. Parra-Guillen, Z.P., Fontanellas, A., Jiang, L., Jericó, D., Martini, P., Vera-Yunca, D., Hard, M., Guey, L.T., and Troconiz, I.F. (2020). Disease pharmacokinetic-pharmacodynamic modelling in acute intermittent porphyria to support the development of mRNA-based therapies. *Br. J. Pharmacol.* *177*, 3168–3182.
106. An, D., Frassetto, A., Jacquinet, E., Eybye, M., Milano, J., DeAntonis, C., Nguyen, V., Laureano, R., Milton, J., Sabnis, S., et al. (2019). Long-term efficacy and safety of mRNA therapy in two murine models of methylmalonic acidemia. *EBioMedicine* *45*, 519–528.
107. Prieve, M.G., Harvie, P., Monahan, S.D., Roy, D., Li, A.G., Blevins, T.L., Paschal, A.E., Waldheim, M., Bell, E.C., Galperin, A., et al. (2018). Targeted mRNA therapy for ornithine transcarbamylase deficiency. *Mol. Ther.* *26*, 801–813.
108. Karadagi, A., Cavedon, A.G., Zemack, H., Nowak, G., Eybye, M.E., Zhu, X., Guadagnin, E., White, R.A., Rice, L.M., Frassetto, A.L., et al. (2020). Systemic modified messenger RNA for replacement therapy in alpha 1-antitrypsin deficiency. *Sci. Rep.* *10*, 7052.
109. Michel, T., Kankura, A., Salinas Medina, M.L., Kurz, J., Behring, A., Avci-Adali, M., Nolte, A., Schlensak, C., Wendel, H.P., and Krajewski, S. (2015). In vitro evaluation of a novel mRNA-based therapeutic strategy for the treatment of patients suffering from alpha-1-antitrypsin deficiency. *Nucleic Acid Ther.* *25*, 235–244.
110. Lin, Y.-X., Wang, Y., Ding, J., Jiang, A., Wang, J., Yu, M., Blake, S., Liu, S., Bieberich, C.J., Farokhzad, O.C., et al. (2021). Reactivation of the tumor suppressor PTEN by mRNA nanoparticles enhances antitumor immunity in preclinical models. *Sci. Transl. Med.* *13*, eaba9772.
111. Steinle, H., Golombek, S., Behring, A., Schlensak, C., Wendel, H.P., and Avci-Adali, M. (2018). Improving the angiogenic potential of EPCs via engineering with synthetic modified mRNAs. *Mol. Ther. Nucleic Acids* *13*, 387–398.
112. Breda, L., Papp, T.E., Triebwasser, M.P., Yadegari, A., Fedorky, M.T., Tanaka, N., Abdulmalik, O., Pavani, G., Wang, Y., Grupp, S.A., et al. (2023). In vivo hematopoietic stem cell modification by mRNA delivery. *Science* *381*, 436–443.
113. Bobis-Wozowicz, S., Galla, M., Alzubi, J., Kuehle, J., Baum, C., Schambach, A., and Cathomen, T. (2014). Non-integrating gamma-retroviral vectors as a versatile tool for transient zinc-finger nuclease delivery. *Sci. Rep.* *4*, 4656.
114. Zhang, H.-X., Zhang, Y., and Yin, H. (2019). Genome editing with mRNA encoding ZFN, TALEN, and Cas9. *Mol. Ther.* *27*, 735–746.
115. Okee, M., Baiyana, A., Musubika, C., Joloba, M.L., Ashaba-Katabazi, F., Bagaya, B., and Wayengera, M. (2018). In vitro transduction and target-Mutagenesis efficiency of HIV-1 pol gene targeting ZFN and CRISPR/Cas9 delivered by various plasmids and/or vectors: toward an HIV cure. *AIDS Res. Hum. Retroviruses* *34*, 88–102.
116. Lyu, P., Wang, L., and Lu, B. (2020). Virus-like particle mediated CRISPR/Cas9 delivery for efficient and safe genome editing. *Life* *10*, 366.
117. Ouranidis, A., Choli-Papadopoulou, T., Papachristou, E.T., Papi, R., and Kostomitsopoulos, N. (2021). Biopharmaceutics 4.0, advanced pre-clinical development of mRNA-encoded monoclonal antibodies to immunosuppressed murine models. *Vaccines* *9*, 890.
118. Pardi, N., Secreto, A.J., Shan, X., Debonera, F., Glover, J., Yi, Y., Muramatsu, H., Ni, H., Mui, B.L., Tam, Y.K., et al. (2017). Administration of nucleoside-modified mRNA encoding broadly neutralizing antibody protects humanized mice from HIV-1 challenge. *Nat. Commun.* *8*, 14630.
119. August, A., Attarwala, H.Z., Himansu, S., Kalidindi, S., Lu, S., Pajon, R., Han, S., Lecerf, J.M., Tomassini, J.E., Hard, M., et al. (2021). A phase 1 trial of lipid-encapsulated mRNA encoding a monoclonal antibody with neutralizing activity against Chikungunya virus. *Nat. Med.* *27*, 2224–2233.
120. Schultheis, K., Pugh, H.M., Oh, J., Nguyen, J., Yung, B., Reed, C., Cooch, N., Chen, J., Yan, J., Muthumani, K., et al. (2020). Active immunoprophylaxis with a synthetic DNA-encoded monoclonal anti-respiratory syncytial virus scFv-Fc fusion protein confers protection against infection and durable activity. *Hum. Vaccin. Immunother.* *16*, 2165–2175.
121. Alsajjan, R., and Mason, W.P. (2023). Bispecific T-cell engagers and chimeric antigen receptor T-cell therapies in glioblastoma: an update. *Curr. Oncol.* *30*, 8501–8549.
122. Hussein, R.A., Abe, N., Hara, T., Abe, H., and Kogure, K. (2023). Use of iontophoresis technology for transdermal delivery of a minimal mRNA vaccine as a potential melanoma therapeutic. *Biol. Pharm. Bull.* *46*, 301–308.
123. Hasan, M., Khatun, A., and Kogure, K. (2023). Intradermal Delivery of Naked mRNA Vaccines via Iontophoresis. *Pharmaceutics* *15*, 2678.
124. Joe, P.T., Christopoulou, I., Van Hoecke, L., Schepens, B., Ysenbaert, T., Heirman, C., Thielemans, K., Saelens, X., and Aerts, J.L. (2019). Intranasal administration of mRNA encoding nucleoprotein provides cross-strain immunity against influenza in mice. *J. Transl. Med.* *17*, 242.
125. Minnaert, A.-K., Vanluchene, H., Verbeke, R., Lentacker, I., De Smedt, S.C., Raemdonck, K., Sanders, N.N., and Remaut, K. (2021). Strategies for controlling the innate immune activity of conventional and self-amplifying mRNA therapeutics: Getting the message across. *Adv. Drug Deliv. Rev.* *176*, 113900.
126. Zhang, H., Vandesompele, J., Braeckmans, K., De Smedt, S.C., and Remaut, K. (2024). Nucleic acid degradation as barrier to gene delivery: a guide to understand and overcome nuclease activity. *Chem. Soc. Rev.*
127. Shin, H., Park, S.J., Yim, Y., Kim, J., Choi, C., Won, C., and Min, D.H. (2018). Recent advances in RNA therapeutics and RNA delivery systems based on nanoparticles. *Adv. Ther.* *1*, 1800065.
128. Ross, J. (1995). mRNA stability in mammalian cells. *Microbiol. Rev.* *59*, 423–450.
129. Hargrove, J.L., and Schmidt, F.H. (1989). The role of mRNA and protein stability in gene expression. *FASEB J.* *3*, 2360–2370.
130. Deutscher, M.P. (2006). Degradation of RNA in bacteria: comparison of mRNA and stable RNA. *Nucleic Acids Res.* *34*, 659–666.
131. Guhaniyogi, J., and Brewer, G. (2001). Regulation of mRNA stability in mammalian cells. *Gene* *265*, 11–23.
132. Kim, Y.-K. (2022). RNA therapy: rich history, various applications and unlimited future prospects. *Exp. Mol. Med.* *54*, 455–465.
133. Nelson, J., Sorensen, E.W., Mintri, S., Rabideau, A.E., Zheng, W., Besin, G., Khatwani, N., Su, S.V., Miracco, E.J., Issa, W.J., et al. (2020). Impact of mRNA chemistry and manufacturing process on innate immune activation. *Sci. Adv.* *6*, eaaz6893.
134. Muslimov, A., Tereshchenko, V., Shevryev, D., Rogova, A., Lepik, K., Reshetnikov, V., and Ivanov, R. (2023). The dual role of the innate immune system in the effectiveness of mRNA therapeutics. *Int. J. Mol. Sci.* *24*, 14820.
135. Delehedde, C., Even, L., Midoux, P., Pichon, C., and Perche, F. (2021). Intracellular routing and recognition of lipid-based mRNA nanoparticles. *Pharmaceutics* *13*, 945.
136. Paunovska, K., Loughrey, D., and Dahlman, J.E. (2022). Drug delivery systems for RNA therapeutics. *Nat. Rev. Genet.* *23*, 265–280.
137. Mulrone, T.E., Pöyry, T., Yam-Puc, J.C., Rust, M., Harvey, R.F., Kalmar, L., Horner, E., Booth, L., Ferreira, A.P., Stoneley, M., et al. (2024). N1-methylpseudouridylation of mRNA causes +1 ribosomal frameshifting. *Nature* *625*, 189–194.
138. Salleh, M.Z., Norazmi, M.N., and Deris, Z.Z. (2022). Immunogenicity mechanism of mRNA vaccines and their limitations in promoting adaptive protection against SARS-CoV-2. *PeerJ* *10*, e13083.
139. Champagne, J., Mordente, K., Nagel, R., and Agami, R. (2022). Slippy-Sloppy translation: a tale of programmed and induced-ribosomal frameshifting. *Trends Genet.* *38*, 1123–1133.

140. Dinman, J.D. (2012). Mechanisms and implications of programmed translational frameshifting. *Wiley Interdiscip. Rev. RNA* 3, 661–673.
141. Hong, S., Sunita, S., Maehigashi, T., Hoffer, E.D., Dunkle, J.A., and Dunham, C.M. (2018). Mechanism of tRNA-mediated +1 ribosomal frameshifting. *Proc. Natl. Acad. Sci. USA* 115, 11226–11231.
142. Baden, L.R., El Sahly, H.M., Essink, B., Kotloff, K., Frey, S., Novak, R., Diemert, D., Spector, S.A., Rouphael, N., Creech, C.B., et al. (2021). Efficacy and safety of the mRNA-1273 SARS-CoV-2 vaccine. *N. Engl. J. Med. Overseas. Ed.* 384, 403–416.
143. Polack, F.P., Thomas, S.J., Kitchin, N., Absalon, J., Gurtman, A., Lockhart, S., Perez, J.L., Pérez Marc, G., Moreira, E.D., Zerbini, C., et al. (2020). Safety and efficacy of the BNT162b2 mRNA Covid-19 vaccine. *N. Engl. J. Med.* 383, 2603–2615.
144. Sadoff, J., Gray, G., Vandebosch, A., Cárdenas, V., Shukarev, G., Grinsztejn, B., Goepfert, P.A., Truyers, C., Fennema, H., Spiessens, B., et al. (2021). Safety and efficacy of single-dose Ad26. COV2. S vaccine against Covid-19. *N. Engl. J. Med.* 384, 2187–2201.
145. de la Torre, D., and Chin, J.W. (2021). Reprogramming the genetic code. *Nat. Rev. Genet.* 22, 169–184.
146. Liu, A., and Wang, X. (2022). The pivotal role of chemical modifications in mRNA therapeutics. *Front. Cell Dev. Biol.* 10, 901510.
147. Chen, S., Huang, X., Xue, Y., Álvarez-Benedicto, E., Shi, Y., Chen, W., Koo, S., Siegwart, D.J., Dong, Y., and Tao, W. (2023). Nanotechnology-based mRNA vaccines. *Nat. Rev. Methods Primers* 3, 63.
148. Huang, P., Deng, H., Wang, C., Zhou, Y., and Chen, X. (2024). Cellular Trafficking of Nanotechnology-Mediated mRNA Delivery. *Adv. Mater.* 36, 2307822.
149. Tenchov, R., Bird, R., Curtze, A.E., and Zhou, Q. (2021). Lipid nanoparticles— from liposomes to mRNA vaccine delivery, a landscape of research diversity and advancement. *ACS Nano* 15, 16982–17015.
150. Van de Vyver, T., De Smedt, S.C., and Raemdonck, K. (2022). Modulating intracellular pathways to improve non-viral delivery of RNA therapeutics. *Adv. Drug Deliv. Rev.* 181, 114041.
151. Durymanov, M., and Reineke, J. (2018). Non-viral delivery of nucleic acids: insight into mechanisms of overcoming intracellular barriers. *Front. Pharmacol.* 9, 971.
152. Jackson, A.L., and Linsley, P.S. (2004). Noise amidst the silence: off-target effects of siRNAs? *Trends Genet.* 20, 521–524.
153. Jackson, A.L., and Linsley, P.S. (2010). Recognizing and avoiding siRNA off-target effects for target identification and therapeutic application. *Nat. Rev. Drug Discov.* 9, 57–67.
154. Fedorov, Y., Anderson, E.M., Birmingham, A., Reynolds, A., Karpilow, J., Robinson, K., Leake, D., Marshall, W.S., and Khvorova, A. (2006). Off-target effects by siRNA can induce toxic phenotype. *RNA* 12, 1188–1196.
155. Singh, S., Narang, A.S., and Mahato, R.I. (2011). Subcellular fate and off-target effects of siRNA, shRNA, and miRNA. *Pharm. Res. (N. Y.)* 28, 2996–3015.
156. Brown, K., and Samarsky, D. (2006). RNAi off-targeting: Light at the end of the tunnel. *J. RNAi Gene Silencing* 2, 175–177.
157. Scientific, T (2006). Off-Target Effects: Disturbing the silence of RNA interference (RNAi). *Dharmacon Technol. Rev.* 82, 1.
158. Bullard, J., Dust, K., Funk, D., Strong, J.E., Alexander, D., Garnett, L., Boodman, C., Bello, A., Hedley, A., Schiffman, Z., et al. (2020). Predicting infectious severe acute respiratory syndrome coronavirus 2 from diagnostic samples. *Clin. Infect. Dis.* 71, 2663–2666.
159. He, X., Lau, E.H.Y., Wu, P., Deng, X., Wang, J., Hao, X., Lau, Y.C., Wong, J.Y., Guan, Y., Tan, X., et al. (2020). Temporal dynamics in viral shedding and transmissibility of COVID-19. *Nat. Med.* 26, 672–675.
160. Li, N., Wang, X., and Lv, T. (2020). Prolonged SARS-CoV-2 RNA shedding: not a rare phenomenon. *J. Med. Virol.* 92, 2286–2287.
161. To, K., Hung, I., Ip, J.D., Chu, A., Chan, W.-M., Tam, A.R., Fong, C.H., Yuan, S., Tsoi, H.W., Ng, A.C., et al. (2020). COVID-19 re-infection by a phylogenetically distinct SARS-coronavirus-2 strain confirmed by whole genome sequencing. *Clin. Infect. Dis.* 10, ciaa1275.
162. Huang, J., Zheng, L., Li, Z., Hao, S., Ye, F., Chen, J., Yao, X., Liao, J., Wang, S., Zeng, M., et al. (2020). Recurrence of SARS-CoV-2 PCR positivity in COVID-19 patients: a single center experience and potential implications. Preprint at medRxiv. <https://doi.org/10.1101/2020.05.06.20089573>.
163. Yuan, B., Liu, H.-Q., Yang, Z.-R., Chen, Y.-X., Liu, Z.-Y., Zhang, K., Wang, C., Li, W.X., An, Y.W., Wang, J.C., and Song, S. (2020). Recurrence of positive SARS-CoV-2 viral RNA in recovered COVID-19 patients during medical isolation observation. *Sci. Rep.* 10, 11887.
164. Belyi, V.A., Levine, A.J., and Skalka, A.M. (2010). Unexpected inheritance: multiple integrations of ancient bornavirus and ebolavirus/marburgvirus sequences in vertebrate genomes. *PLoS Pathog.* 6, e1001030.
165. Horie, M., Honda, T., Suzuki, Y., Kobayashi, Y., Daito, T., Oshida, T., Ikuta, K., Jern, P., Gojobori, T., Coffin, J.M., and Tomonaga, K. (2010). Endogenous non-retroviral RNA virus elements in mammalian genomes. *Nature* 463, 84–87.
166. Zhang, L., Richards, A., Barrasa, M.I., Hughes, S.H., Young, R.A., and Jaenisch, R. (2021). Reverse-transcribed SARS-CoV-2 RNA can integrate into the genome of cultured human cells and can be expressed in patient-derived tissues. *Proc. Natl. Acad. Sci. USA* 118, e2105968118.
167. Khurana, A., Allawadhi, P., Khurana, I., Allwadh, S., Weiskirchen, R., Banothu, A.K., Chhabra, D., Joshi, K., and Bharani, K.K. (2021). Role of nanotechnology behind the success of mRNA vaccines for COVID-19. *Nano Today* 38, 101142.
168. Zhang, L., More, K.R., Ojha, A., Jackson, C.B., Quinlan, B.D., Li, H., He, W., Farzan, M., Pardi, N., and Choe, H. (2023). Effect of mRNA-LNP components of two globally-marketed COVID-19 vaccines on efficacy and stability. *NPJ Vaccines* 8, 156.
169. Wilson, B., and Geetha, K.M. (2022). Lipid nanoparticles in the development of mRNA vaccines for COVID-19. *J. Drug Deliv. Sci. Technol.* 74, 103553.
170. Wang, M.M., Wappelhorst, C.N., Jensen, E.L., Chi, Y.-C.T., Rouse, J.C., and Zou, Q. (2023). Elucidation of lipid nanoparticle surface structure in mRNA vaccines. *Sci. Rep.* 13, 16744.
171. Zhu, Y., Zhu, L., Wang, X., and Jin, H. (2022). RNA-based therapeutics: an overview and prospectus. *Cell Death Dis.* 13, 644.
172. Burnett, J.C., and Rossi, J.J. (2012). RNA-based therapeutics: current progress and future prospects. *Chem. Biol.* 19, 60–71.
173. Lucas, T., Bonauer, A., and Dimmeler, S. (2018). RNA therapeutics in cardiovascular disease. *Circ. Res.* 123, 205–220.
174. Kim, Y.-K. (2020). RNA therapy: current status and future potential. *Chonnam Med. J.* 56, 87–93.
175. Xue, H., Guo, P., Wen, W.-C., and Wong, H. (2015). Lipid-based nanocarriers for RNA delivery. *Curr. Pharm. Des.* 21, 3140–3147.
176. Collotta, D., Bertocchi, I., Chiapello, E., and Collino, M. (2023). Antisense oligonucleotides: a novel Frontier in pharmacological strategy. *Front. Pharmacol.* 14, 1304342.
177. Cejka, D., Losert, D., and Wacheck, V. (2006). Short interfering RNA (siRNA): tool or therapeutic? *Clin. Sci.* 110, 47–58.
178. Rizk, M., and Tüzmen, Ş. (2017). Update on the clinical utility of an RNA interference-based treatment: focus on Patisiran. *Pharmgenomics. Pers. Med.* 10, 267–278.
179. Sardh, E., Harper, P., Balwani, M., Stein, P., Rees, D., Bissell, D.M., Desnick, R., Parker, C., Phillips, J., Bonkovsky, H.L., et al. (2019). Phase 1 trial of an RNA interference therapy for acute intermittent porphyria. *N. Engl. J. Med.* 380, 549–558.
180. Springer, A.D., and Dowdy, S.F. (2018). GalNAc-siRNA conjugates: leading the way for delivery of RNAi therapeutics. *Nucleic Acid Ther.* 28, 109–118.
181. Dowdy, S.F. (2017). Overcoming cellular barriers for RNA therapeutics. *Nat. Biotechnol.* 35, 222–229.
182. Zamecnik, P.C., and Stephenson, M.L. (1978). Inhibition of Rous sarcoma virus replication and cell transformation by a specific oligodeoxynucleotide. *Proc. Natl. Acad. Sci. USA* 75, 280–284.
183. Kim, M., Jeong, M., Hur, S., Cho, Y., Park, J., Jung, H., Seo, Y., Woo, H.A., Nam, K.T., Lee, K., and Lee, H. (2021). Engineered ionizable lipid nanoparticles for targeted delivery of RNA therapeutics into different types of cells in the liver. *Sci. Adv.* 7, eabf4398.
184. Stephenson, M.L., and Zamecnik, P.C. (1978). Inhibition of Rous sarcoma viral RNA translation by a specific oligodeoxyribonucleotide. *Proc. Natl. Acad. Sci. USA* 75, 285–288.

185. Hoffman, V.F., and Skiest, D.J. (2000). Therapeutic developments in cytomegalovirus retinitis. *Expert Opin. Investig. Drugs* 9, 207–220.
186. Dunn, J.P. (2014). An overview of current and future treatment options for patients with cytomegalovirus retinitis. *Exp. Opin. Orphan Drugs* 2, 999–1013.
187. Hamer, D.H., and Leder, P. (1979). Splicing and the formation of stable RNA. *Cell* 18, 1299–1302.
188. Murray, V., and Holliday, R. (1979). A mechanism for RNA–RNA splicing and a model for the control of gene expression. *Genet. Res.* 34, 173–188.
189. Sharp, P.A. (1994). Split genes and RNA splicing. *Cell* 77, 805–815.
190. Sharp, P.A. (2001). RNA interference—2001. *Genes Dev.* 15, 485–490.
191. Sharp, P.A. (1999). RNAi and double-strand RNA. *Genes Dev.* 13, 139–141.
192. Randall, G., and Rice, C.M. (2004). Interfering with hepatitis C virus RNA replication. *Virus Res.* 102, 19–25.
193. Li, H.-C., and Lo, S.-Y. (2015). Hepatitis C virus: Virology, diagnosis and treatment. *World J. Hepatol.* 7, 1377–1389.
194. Bartolucci, D., Pession, A., Hrelia, P., and Tonelli, R. (2022). Precision anti-cancer medicines by oligonucleotide therapeutics in clinical research targeting undruggable proteins and non-coding RNAs. *Pharmaceutics* 14, 1453.
195. Kaur, J., Sharma, A., Mundlia, P., Sood, V., Pandey, A., Singh, G., and Barnwal, R.P. (2024). RNA–Small-Molecule Interaction: Challenging the “Undruggable” Tag. *J. Med. Chem.* 67, 4259–4297.
196. Coleman, N., and Rodon, J. (2021). Taking aim at the undruggable. *Am. Soc. Clin. Oncol. Educ. Book.* 41, 1–8.
197. Esteller, M. (2011). Non-coding RNAs in human disease. *Nat. Rev. Genet.* 12, 861–874.
198. Saw, P.E., and Song, E. (2024). Advancements in clinical RNA therapeutics: Present developments and prospective outlooks. *Cell Rep. Med.* 5, 101555.
199. Zhang, G., Zhang, J., Gao, Y., Li, Y., and Li, Y. (2022). Strategies for targeting undruggable targets. *Expert Opin. Drug Discov.* 17, 55–69.
200. Scott, D.E., Bayly, A.R., Abell, C., and Skidmore, J. (2016). Small molecules, big targets: drug discovery faces the protein–protein interaction challenge. *Nat. Rev. Drug Discov.* 15, 533–550.
201. Buchwald, P. (2010). Small-molecule protein–protein interaction inhibitors: Therapeutic potential in light of molecular size, chemical space, and ligand binding efficiency considerations. *IUBMB Life* 62, 724–731.
202. Warner, K.D., Hajdin, C.E., and Weeks, K.M. (2018). Principles for targeting RNA with drug-like small molecules. *Nat. Rev. Drug Discov.* 17, 547–558.
203. Lomenick, B., Olsen, R.W., and Huang, J. (2011). Identification of direct protein targets of small molecules. *ACS Chem. Biol.* 6, 34–46.
204. Gallego, J., and Varani, G. (2001). Targeting RNA with small-molecule drugs: therapeutic promise and chemical challenges. *Acc. Chem. Res.* 34, 836–843.
205. Hermann, T. (2000). Strategies for the design of drugs targeting RNA and RNA–protein complexes. *Angew. Chem. Int. Ed. Engl.* 39, 1890–1904.
206. Thomas, J.R., and Hergenrother, P.J. (2008). Targeting RNA with small molecules. *Chem. Rev.* 108, 1171–1224.
207. Wilson, W.D., and Li, K. (2000). Targeting RNA with small molecules. *Curr. Med. Chem.* 7, 73–98.
208. Xu, X., and Xia, T. (2023). Recent advances in site-specific lipid nanoparticles for mRNA delivery. *ACS Nanosci. Au* 3, 192–203.