



Influence of Synthesis Conditions on Gadolinium-Substituted Tricalcium Phosphate Ceramics and Its Physicochemical, Biological, and Antibacterial Properties

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Abstract: Gadolinium-containing calcium phosphates are promising contrast agents for various bioimaging modalities. Gadolinium-substituted tricalcium phosphate (TCP) powders with 0.51 wt% of gadolinium (0.01Gd-TCP) and 5.06 wt% of (0.1Gd-TCP) were synthesized by two methods: precipitation from aqueous solutions of salts (1) (Gd-TCP-pc) and mechano-chemical activation (2) (Gd-TCP-ma). The phase composition of the product depends on the synthesis method. The product of synthesis (1) was composed of β -TCP (main phase, 96%), apatite/chlorapatite (2%), and calcium pyrophosphate (2%), after heat treatment at 900 °C. The product of synthesis (2) was represented by β -TCP (main phase, 73%), apatite/chlorapatite (20%), and calcium pyrophosphate (7%), after heat treatment at 900 °C. The substitution of Ca²⁺ ions by Gd³⁺ in both β -TCP (main phase) and apatite (admixture) phases was proved by the electron paramagnetic resonance technique. The thermal stability and specific surface area of the Gd-TCP powders synthesized by two methods were significantly different. The method of synthesis also influenced the size and morphology of the prepared Gd-TCP powders. In the case of synthesis route (1), powders with particle sizes of tens of nanometers were obtained, while in the case of synthesis (2), the particle size was hundreds of nanometers, as revealed by transmission electron microscopy. The Gd-TCP ceramics microstructure investigated by scanning electron microscopy was different depending on the synthesis route. In the case of (1), ceramics with grains of 1–50 µm, pore sizes of 1–10 µm, and a bending strength of about 30 MPa were obtained; in the case of (2), the ceramics grain size was $0.4-1.4 \mu m$, the pore size was 2 µm, and a bending strength of about 39 MPa was prepared. The antimicrobial activity of powders was tested for four bacteria (S. aureus, E. coli, S. typhimurium, and E. faecalis) and one fungus (C. albicans), and there was roughly 30% of inhibition of the micro-organism's growth. The metabolic activity of the NCTC L929 cell and viability of the human dental pulp stem cell study



Citation: Fadeeva, I.V.; Deyneko, D.V.; Barbaro, K.; Davydova, G.A.; Sadovnikova, M.A.; Murzakhanov, F.F.; Fomin, A.S.; Yankova, V.G.; Antoniac, I.V.; Barinov, S.M.; et al. Influence of Synthesis Conditions on Gadolinium-Substituted Tricalcium Phosphate Ceramics and Its Physicochemical, Biological, and Antibacterial Properties. *Nanomaterials* 2022, *12*, 852. https:// doi.org/10.3390/nano12050852

Academic Editor: Csaba Balázsi

Received: 1 February 2022 Accepted: 1 March 2022 Published: 3 March 2022

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Copyright: © 2022 by the authors. Licensee MDPI, Basel, Switzerland. This article is an open access article distributed under the terms and conditions of the Creative Commons Attribution (CC BY) license (https:// creativecommons.org/licenses/by/ 4.0/). demonstrated the absence of toxic effects for all the prepared ceramic materials doped with Gd ions, with no difference for the synthesis route.

Keywords: gadolinium; tricalcium phosphate; gadolinium-substituted tricalcium phosphate; gadolinium tricalcium phosphate powder; gadolinium tricalcium phosphate ceramics; gadolinium doped tricalcium phosphate

1. Introduction

Nowadays, a rapid increase in the aging of the population has been observed. Worldwide, about 20% of the population (around 2 billion) is foreseen to be over 60 years old by 2050 [1]. According to the World Health Organization, around 40% of people over 60 years old experience musculoskeletal disorders [1,2]. The aging of a population is characterized by a progressive bone loss of individuals. Osteopenia is associated with several outcomes, including functional decline, high risk of fractures, and frailty. Musculoskeletal disorders are among the key causes of morbidity in elderly people. For all these reasons, there is an enormous demand for synthetic bone substitutes and new tissue regeneration strategies. Various synthetic bone grafts have been developed over the past few decades, a part of them being based on calcium phosphates similar to those present in the human body, such as hydroxyapatite (HA, $Ca_{10}(PO_4)_6(OH)_2)$) and tricalcium phosphate (β -TCP, β -Ca₃(PO₄)₂) [3–5].

 β -TCP is one of the most used and promising synthetic bone graft substitutes, being osteoconductive and osteoinductive. Such properties combined with resorption mediated by cells result in the complete bone defect regeneration [4]. β -TCP has a higher solubility and, accordingly, rate of resorption in comparison with HA. In the case of β -TCP, the period of replacement of the majority of artificial material with natural bone is about 6-24 months [6-8]. It is possible to regulate the rate of resorption, physical features, and biological performance by cationic or anionic substitutions in the β -TCP structure [9–11]. For example, doping the β -TCP structure with various metal cations, such as copper (II), manganese (II), iron (III), and zinc (II) [12–15], leads to its destabilization and, consequently, to the increase in the rate of dissolution of these cations in the body fluid. In addition to the modulation of physicochemical characteristics of β -TCP, metal-substituted TCPs provide new advanced properties to the materials. Antibacterial characteristics can be imparted by Cu²⁺, Fe³⁺, Zn²⁺, and Ag⁺ ions [12,14–16], and the biocompatibility properties and, namely, cell proliferation on the materials surface can be improved by Fe³⁺ and Sr²⁺ ions substitution [5,14,17–19]. Mg-doped β -TCP biomaterials are able to enhance the cell proliferation and viability of human bone marrow-derived mesenchymal stem cells [20] and the differentiation of hBMSCs into osteoblasts [21].

For tissue regeneration, each step of bone healing needs to be optimized followed by imaging techniques, such as X-ray radiography, computed tomography (CT), singlephoton emission computerized tomography (SPECT), and magnetic resonance imaging (MRI). However, even when using these methods, it is difficult to follow the processes of bone tissue regeneration and to control the degradation of synthetic bone substitutes without any contrast-providing substances. This problem can be solved by adding contrast agents to β -TCP bone substitute materials [22]. Calcium phosphate nanoparticles were employed as contrast agents by doping with europium (Eu³⁺), gadolinium (Gd³⁺), iron (Fe³⁺), neodymium (Nd³⁺), terbium (Tb³⁺), dysprosium (Dy³⁺), etc., for such imaging modalities as fluorescence, CT, MR, and nuclear imaging [23]. The synthesis of Gd³⁺-doped HA for a dual-modal probe for SPECT and MRI was developed in [24,25]. Gd-doped nanocomposites with enhanced MRI and X-ray dual imaging were developed in [26] to simulate the electrical properties of bone.

A number of studies have been devoted to Gd^{3+} -substituted β -TCP materials [27,28]. It was demonstrated that Gd^{3+} -doped β -Ca₃(PO₄)₂ exhibited nontoxic behavior toward

MG-63 cells and paramagnetic behavior [27]. In [28], the Gd, Ce, and Tb co-doped β -TCP porous nanospheres exhibited excellent cytocompatibility and were found to be promising for bioimaging guidance.

The present study was aimed at the investigation of the influence of two synthesis routes of the Gd-substituted β -TCP: precipitation from aqueous solutions of salts [9] (1) and mechano-chemical activation (2), and of gadolinium concentration on the phase composition, morphology, and sintering behavior of Gd-TCP powders, and the microstructure and properties of the corresponding Gd-substituted tricalcium phosphate ceramics for possible use as contrast agents in bioimaging techniques. The prepared powder samples were characterized by the Fourier-transform infrared spectroscopy (FT-IR), X-ray diffraction (XRD), electron paramagnetic resonance spectroscopy (EPR), thermogravimetric analysis (TGA), specific surface area, scanning electrons microscopy (SEM), and transmission electron microscopy (TEM) methods. Antimicrobial in vitro tests using four bacteria (*S. aureus*, *E. coli*, *S. typhimurium*, and *E. faecalis*) and one fungus (*C. albicans*) were performed. The fibroblast cell line NCTC clone L929 was used for cytotoxicity studies, and the viability of postnatal human dental pulp stem cells (DPSCs) was investigated.

2. Materials and Methods

Gadolinium-substituted tricalcium phosphates with 0.51 wt% (0.01Gd-TCP) and 5.06 wt% (0.1Gd-TCP) of gadolinium were synthesized by two methods: precipitation from aqueous solutions of salts (1) [9] and mechano-chemical activation (2) [29].

The raw materials for precipitation from aqueous solutions of salts were calcium nitrate (chemical grade, Chimmed, Moscow, Russia), diammonium phosphate (analytical grade, Chimmed, Moscow, Russia), gadolinium chloride (chemical grade, Chimmed, Moscow, Russia), and 25% aqueous ammonia solution (analytical grade, Chimmed, Moscow, Russia). Synthesis of Gd-substituted TCP was performed according to reactions (1) and (2):

 $2.9 \text{ Ca}(\text{NO}_3)_2 + 0.067 \text{ GdCl}_3 + 2 (\text{NH}_4)_2 \text{HPO}_4 + 2 \text{ NH}_4 \text{OH} \rightarrow \text{Ca}_{2.9} \text{Gd}_{0.067} (\text{PO}_4)_2 + 0.2 \text{ NH}_4 \text{Cl} + 5.8 \text{ NH}_4 \text{NO}_3 + 2 \text{ H}_2 \text{O}$ (1)

 $2.99 Ca(NO_3)_2 + 0.0067 GdCl_3 + 2 (NH_4)_2 HPO_4 + 2 NH_4 OH \rightarrow Ca_{2.99}Gd_{0.0067} (PO_4)_2 + 0.02 NH_4 Cl + 5.98 NH_4 NO_3 + 2 H_2 O$

The samples obtained by the precipitation method were named 0.1-Gd-TCP-pc (Reaction (1)) and 0.01Gd-TCP-pc (Reaction (2)).

The mechano-chemical activation was carried out in the planetary mill container PM-1, (Vibrotechnik, St. Petersburg, Russia) at a 1500 min⁻¹ rotation rate. The ratio between materials mixture: zirconium oxide balls was 1:5 and the activation time was 30 min. The amounts of the reagents were calculated according to Reactions (3) and (4):

$$2.9 \text{ CaO} + 0.067 \text{ GdCl}_3 + 2 (\text{NH}_4)_2 \text{HPO}_4 \rightarrow \text{Ca}_{2.9} \text{Gd}_{0.067} (\text{PO}_4)_2 + 3.8 \text{ NH}_3 + 0.2 \text{ NH}_4 \text{Cl} + 2.9 \text{ H}_2 \text{O}$$
(3)

$2.99 \text{ CaO} + 0.0067 \text{ GdCl}_3 + 2 \text{ (NH}_4)_2 \text{HPO}_4 \rightarrow \text{Ca}_{2.9} \text{Gd}_{0.0067} \text{(PO}_4)_2 + 3.8 \text{ NH}_3 + 0.02 \text{ NH}_4 \text{Cl} + 2.9 \text{ H}_2 \text{O}$ (4)

Immediately after the synthesis, 200 mL of water was added to the reagents, and grinding was continued for 30 min. The precipitate was filtered out using the Buchner funnel and dried at 110 °C for 12–15 h. The samples obtained by the mechano-chemical activation method were named 0.1Gd-TCP-ma (Reaction (3)) and 0.01Gd-TCP-ma (Reaction (4)).

The powders obtained by synthesis methods (1) and (2) were heat-treated at 900 $^{\circ}$ C for 1 h. The corresponding ceramics were prepared by uniaxial pressing of the powders in a steel mold under pressure of 100 MPa, followed by the sintering of compacts in air atmosphere in the muffle furnace at 1100 $^{\circ}$ C for 2 h.

Fourier-transform infrared spectroscopy absorption spectra of the synthesized powders mixed with KBr were recorded in the range of 400–4000 cm⁻¹ with a resolution of 0.9 cm⁻¹ by means of the Thermo Nicolet Avatar 330 FTIR spectrometer (Thermo Fisher Scientific, Waltham, MA, USA). Powder X-ray diffraction patterns were collected on a Rigaku D/MAX 2500 (Niradiation filter Cu K α , $\theta/2\theta$ geometry). XRD data were obtained at room temperature in the 2 θ range between 10° and 60° with a step interval of 0.02° and 3°/min scan rate. The LeBail decomposition [30] was applied using the JANA2006 software for unit cell parameters and volume determination. Phase analysis was carried out by means of the Crystallographica Search-March program (version 2.0.3.1) and the JCPDS PDF-2 and PDF-4 databases. The Rietveld method was applied for quantitative phase analysis using the JANA2006 software [31]. Crystallographic data of the space group (SG), unit cell, and atomic coordinates of β -Ca₃(PO₄)₂ (PDF#4 No. 70-2065) [32], Ca₁₀(PO₄)₆(OH)₂ (ICDD 183744) [33], and Ca₂P₂O₇ (PDF#4 No. 04-009-3876) [34] were applied as initial parameters. The fifteenth-order polynomial was applied to refine the background and modified pseudo-Voigt function-peak profiles. The unit cell parameters were refined, but the atomic coordinates were taken without refinement. After the last refinement procedure, a good agreement was found between the experimental and calculated patterns.

Electron paramagnetic resonance spectra in pulse mode were recorded using a Bruker Elexsys E580 spectrometer in the X-band microwave range ($v_{MW} = 9.61$ GHz) at the temperatures of 12 and 25 K. The duration of the microwave $\pi/2$ pulse in the pulse sequences was 16 ns. The technique for detecting the integral intensity of the electron spin echo during the sweep of the magnetic field B₀ was used to measure the EPR spectra. The relaxation processes were measured using a Hahn sequence with a time variation between the first and second pulses from 180 to 4276 ns. The electron-nuclear interaction spectra were recorded using the HYSCORE sequence (hyperfine sublevel correlation) with a change in both distances (τ and T) from 180 to 1204 ns. Gadolinium-substituted TCP-0.001Gd-TCP with a gadolinium content of 0.0067 wt% was synthesized for the EPR spectroscopic studies by the precipitation method.

Thermogravimetric analysis was carried out by a thermogravimetric analyzer Model: Q-1500 D (Paulik and Erdei, Hungary) in the temperature range of 20–1200 $^{\circ}$ C with a heating rate of 5 $^{\circ}$ /min.

The specific surface area of powders was measured by low-temperature nitrogen adsorption by the Brunauer–Emmett–Teller (BET) method. The samples were preheated in vacuum to remove the adsorbed water. Afterward, the samples placed in an ampoule filled with helium were immersed in a Dewar vessel filled with liquid nitrogen. The ampoule was evacuated and cooled to a temperature of 77 K. The external pressure corresponded to the pressure of saturated nitrogen vapor at T = 77 K. As a next step, nitrogen gas was dosed until the desired pressure was reached in the ampoule (0.30 atm), and the volume of injected nitrogen was measured.

Scanning electron microscopy observations of Gd-substituted TCP were performed to study the microstructure of the ceramic materials by a Tescan Vega II scanning electron microscope. The grain size was calculated by the random secant method from SEM data. The method consists of calculating the intersection of grain boundaries of a random secant, which is the middle line of the eyepiece–micrometer. This method determines the average diameter in the case of equiaxial grains.

Transmission electron microscopy images of pure β -TCP-pc, β -TCP-ma, and Gd-substituted TCP—0.1Gd-TCP-pc and 0.01Gd-TCP-pc—were obtained by using a LEO 912 AB OMEGA microscope (Carl Zeiss, Oberckochen, Germany).

The antimicrobial activity was evaluated for 0.1Gd-TCP-pc and 0.1Gd-TCP-ma powder samples using four bacteria (*S. aureus*, *E. coli*, *S. typhimurium*, and *E. faecalis*) and one fungus (*C. albicans*). First, the tested samples were autoclaved at 121 °C for 20 min at a pressure of 1.1 bar and diluted to 1:1000 (w/v) in Brain Heart Infusion (BHI, DIFCO, Sparks, NV, USA). Each microorganism was grown in the presence of the tested powder samples for 24 h, under slow stirring. The temperature for the bacteria was 37 °C, while that for the fungus was 28 °C. The growth of microorganisms was assessed by reading the OD600_{nm} (optical density at 600 nm (λ adsorption)) of the growth medium with a Biophotometer

D30 (Eppendorf, Hamburg, Germany). The experiments were carried out in triplicate, and the results are expressed as the mean value \pm standard deviation (SD).

Cytotoxicity was investigated using extracts prepared according to the requirements of GOST R ISO 10993.5-2011 and GOST ISO 10993-12-2015 (Russian Federation) on fibroblast cell line NCTC clone L929 in the culture medium DMEM/F12 using the MTT test.

To study the viability of cells on the surface of ceramic materials, we used postnatal human dental pulp stem cells (DPSCs) isolated from molar rudiment extracted in accordance with the orthodontic indications [35], supported by the voluntary consent of donors. For investigations, the cell culture at the 5th passage was applied.

Sterilized samples were placed in the wells of a 24-well plate and DPSC cells were seeded at a concentration of 30,000 cells/cm² in DMEM/F12 medium (1:1) supplemented with 10% fetal bovine serum (FBS), 100 U/mL penicillin/streptomycin, and 2 mL glutamine, and cultured at 37 °C in an atmosphere of 5% CO₂.

Cell viability was assessed by differential fluorescent staining of living and dead cells using the SYTO 9 fluorescent dyes, propidium iodide and Hoechst 33342. Microphotographies were carried out by means of an Axiovert 200 inverted microscope (Zeiss Oberckochen, Germany). In the modes $\lambda_{exc} = 450-490$ nm and $\lambda_{em} = 515-565$ nm, fluorescent dye SYTO 9 stained green DNA and RNA of living and dead cells. In the study modes $\lambda_{exc} = 546$ nm and $\lambda_{em} = 575-640$ nm, the intercalating reagent propidium iodide (PI) stained the nuclei of dead cells red. In the study modes $\lambda_{exc} = 355$ nm and $\lambda_{em} = 460$ nm, fluorescent dye Hoechst 33,342 stained DNA of living and dead cells blue.

The percentage of viable cells was calculated on a fixed surface area (in the micrographs) by the number of cell nuclei stained with Hoechst 33,342 (all cells) and PI (dead cells).

To obtain cell viability and survivability results, 8 repetitions were made for each point. The calculation of standard deviation was performed for each point in all the sections. The statistical analysis of the reliability was carried out according to the Mann–Whitney U-test ($p \le 0.01$).

3. Results

3.1. FT-IR Study

FT-IR spectra of the Gd-substituted TCP powders prepared by methods (1) and (2) are shown in Figure 1. The spectra are characterized by the distinctive features of the substituted β -TCP-type structure compounds (Figure 1). Assignment of the vibration bands from the FT-IR spectrum of Gd-TCP is provided in Table 1. According to the FT-IR results, the formation of the impurity $Ca_2P_2O_7$ phase is confirmed, which is consistent with the XRD data shown in the next section. Vibrations of hydroxyl groups appear only in samples obtained by the mechano-chemical activation method (2). The position of the OH⁻ bands, the absence of a band at 633 cm⁻¹, as well as the splitting of the vibrations of the hydroxyl group (3644 cm⁻¹, 3544 cm⁻¹) for the 0.1Gd-TCP-ma sample (Figure 1) may indicate that Cl⁻ ions enter the structure of the apatite phase. The presence of bands assigned to the carbonate group should also be noted, and it indicates partial replacement of the groups $PO_4^{3-} \rightarrow CO_3^{2-}$. It is known that the size of powder particles can also affect the shape of the FTIR spectra of samples [36]. However, according to the TEM data, the particle size of the powder obtained by wet precipitation is close to each other, and the differences in the spectra can be attributed to the content of Gd in the samples. Samples obtained by the mechano-chemical activation are multi-phase samples and contain the TCP phase, as well as the apatite phase. Therefore, it is difficult to isolate the effect of dispersion on the nature and shape of the IR spectra.



Figure 1. FT-IR spectra of Gd-substituted TCP powders obtained by precipitation: 0.1Gd-TCP-pc (1) and 0.01Gd-TCP-pc (2), and mechano-chemical activation: 0.1Gd-TCP-ma (3) and 0.01Gd-TCP-ma (4).

Assignment	Wavenumber, cm ⁻¹	Vibration Mode	Sample
OH-(Cl-)	3644, 3544	Valence	(4); weak: (3)
PO4 ³⁻	973	ν_1	(1), (2), (3), (4)
PO4 ³⁻	493, 432	ν_2	(1), (2); weak: (3) (4)
PO4 ³⁻	1123, 1044	ν_3	(1), (2), (3), (4)
PO4 ³⁻	607, 574, 556	ν_4	(1), (2), (3), (4)
$P_2O_7^{4-}$	1212, 727	Valence P-O-P	(1), (2); weak: (3), (4)
CO3 ²⁻	1490	ν_3	(1), (2), (3), (4)
CO3 ²⁻	875	ν_2	(1), (2), (3), (4)

Table 1. Vibration modes in the FT-IR spectrum of Gd-substituted TCP powders.

3.2. X-Ray Diffraction Study

Figure 2 shows the XRD patterns of 0.1 Gd-TCP samples obtained by two methods. According to the XRD data, β -TCP is the main crystalline phase in the synthesized samples, after calcination at 900 °C. In addition, two impurity phases are found: chlorapatite (Ca₁₀(PO₄)₆Cl₂, Cl-AP-phase) and β -calcium pyrophosphate (β -Ca₂P₂O₇). The formation of the chlorapatite phase is associated with the use of GdCl₃ as a precursor. Thus, the presence of Cl⁻ ions in the reaction mixture promotes the formation of a thermodynamically stable chlorapatite phase [33]. Ca₂P₂O₇ is formed during the annealing from a by-product of the reaction of dicalcium phosphate dihydrate (CaHPO₄·2H₂O), according to Reaction (5):

$$2 \operatorname{CaHPO}_4 \cdot 2 \operatorname{H}_2 O \to \operatorname{Ca}_2 P_2 O_7 + 5 \operatorname{H}_2 O \tag{5}$$

The quantitative phase analysis of all the synthesized samples is shown in Table 2 along with the reference data for the pure TCP, chlorapatite, HA, and pyrophosphate phases. The phase composition of 0.1Gd-TCP-ma is the most inhomogeneous compared to other samples (Figure 2). The main phase is β -TCP (73 wt%), and the content of apatite is significant (20 wt%), compared to 0.1Gd-TCP-pc (2 wt%). The pyrophosphate phase is detected in all synthesized samples, with an average content in the range of 2–7%. The scheme of the substitution is $3Ca^{2+} \rightarrow 2R^{3+} + \Upsilon$ (Υ -vacancy), with the formation of a vacancy, and no additional charge compensators are required. The values of the ionic radii of calcium ($r_{VI} = 1.00$ Å, $r_{VIII} = 1.12$ Å) and gadolinium ($r_{VI} = 0.94$ Å, $r_{VIII} = 1.05$ Å) [37] ions in this substitution should have an impact on the unit cell parameters and volume.

Previously [38], it was shown that Gd³⁺ ions occupy only *M*1–*M*3 sites in the β -TCP-type structure. There are no reported data on the unit cell changes in the Ca_{3-x}Gd_{2x/3}(PO₄)₂ solid solutions. However, such data are available for Ca_{3-x}Eu_{2x/3}(PO₄)₂ solid solutions [39]. When Ca²⁺ ions are replaced by Eu³⁺, the parameter *a* and the unit cell volume *V* increase. As the radii of Gd³⁺ (*r*_{VIII} = 1.05 Å) and Eu³⁺ (*r*_{VIII} = 1.07 Å) [37] slightly differ, it can be assumed that the unit cell parameters will change similarly when Ca²⁺ is replaced by Gd³⁺. If we assume that all the Gd³⁺ ions during the synthesis enter the β -TCP lattice, then the composition of this phase is described by the formula Ca_{2.9}Gd_{0.067}(PO₄)₂ (0.1Gd-TCP-pc). Comparing the unit cell parameters of Ca_{2.9}Gd_{0.067}(PO₄)₂, Ca_{2.928}Eu_{0.048}(PO₄)₂, and Ca_{2.858}Eu_{0.095}(PO₄)₂ with a similar composition (see Table 2), one can observe that most of the Gd³⁺ ions are included in the β -TCP structure upon its preparation by the precipitation method. In this case, the unit cell volume of 0.1Gd-TCP-ma obtained by mechano-chemical activation is smaller than that of pure β -TCP (Table 2). These data indicate the existence of impurity amounts of Gd³⁺ in the 0.1Gd-TCP-ma sample.



Figure 2. XRD pattern of Gd-TCP powders prepared by precipitation and mechano-chemical activation methods: 0.01-Gd-TCP-pc (1), 0.01-Gd-TCP-ma (2), 0.1-Gd-TCP-pc (3), and 0.1-Gd-TCP-ma (4).

The calculated unit cell parameters for the impurity apatite phase are noticeably smaller compared to the pure Cl-AP (apatite) phase (Table 2). Therefore, we made an assumption on the existence of a mixture of phases: Cl-AP and HA in the synthesized samples (this assumption is in agreement with the obtained FT-IR results). In the impurity HA phase, some Ca^{2+} ions might be substituted by the Gd^{3+} ions with the formation of oxyapatite according to (6) [40]:

$$OH^{-} + Ca^{2+} \to Gd^{3+} + O^{2-}$$
 (6)

	Phase, SG	wt% (JANA 2006)	a, Å	c, Å	<i>V</i> , Å ³
0.1Gd-TCP-ma	β-TCP, R3c	73	10.423(6)	37.391(3)	3518.3(8)
Ca _{2.9} Gd _{0.067} (PO ₄) ₂	Cl-AP, P6 ₃ /m	20	9.435(8)	6.867(4)	529.5(8)
	Ca ₂ P ₂ O ₇ , P4 ₁	7	6.686(5)	24.148(6)	1081.0(4)
0.1Gd-TCP-pc	β-TCP, R3c	96	10.443(5)	37.438(9)	3536.3(8)
Ca _{2.9} Gd _{0.067} (PO ₄) ₂	Cl-AP, P63/m	2	9.339(7)	6.918(6)	522.7(8)
	Ca ₂ P ₂ O ₇ , P4 ₁	2	6.684(2)	24.149(4)	1080.5(4)
0.01Gd-TCP-ma	β-TCP, R3c	87	10.437(4)	37.403(2)	3529.1(9)
Ca _{2.9} Gd _{0.0067} (PO ₄) ₂	Cl-AP, P6 ₃ /m	7			
	Ca ₂ P ₂ O ₇ , P4 ₁	6	6.685(9)	24.148(4)	1082.1(6)
0.01Gd-TCP-pc	β - TCP, R3c	96	10.438(1)	37.406(2)	3526.4(8)
Ca _{2.9} Gd _{0.0067} (PO ₄) ₂	Cl-AP, <i>P</i> 6 ₃ / <i>m</i>	0	-	-	-
	Ca ₂ P ₂ O ₇ , P4 ₁	4			
β -Ca ₃ (PO ₄) ₂ [32]	R3c (Z = 21)		10.435(2)	37.402(9)	3527.2(6)
Ca _{2.928} Eu _{0.048} (PO ₄) ₂ [39]	R3c (Z = 21)		10.440(1)	37.380(1)	3528.0(9)
Ca _{2.858} Eu _{0.095} (PO ₄) ₂ [39]	R3c (Z = 21)		10.440(1)	37.39(1)	3529
Ca ₁₀ (PO ₄) ₆ Cl ₂ [41]	$P6_3/m (Z = 1)$		9.590(2)	6.766(6)	538.96
Ca ₁₀ (PO ₄) ₆ (OH) ₂ [42]	$P6_3/m (Z = 1)$		9.4207(1)	6.8817(1)	528.92
(Ca _{4.87} Gd _{0.11}) ₂ (PO ₄) ₆ (OH) ₂ [43]	$P6_3/m (Z = 1)$		9.41284(6)	6.8815(1)	528.03(9)
Ca ₂ P ₂ O ₇ [34]	$P4_1 (Z = 8)$		6.6858(8)	24.147(5)	1081.1(3)

Table 2. The results of the quantitative phase analysis for $Ca_{2.9}Gd_{0.067}(PO_4)_2$ (0.1Gd-TCP) and $Ca_{2.9}Gd_{0.0067}(PO_4)_2$ (0.01Gd-TCP) synthesized by precipitation and mechano-chemical activation methods.

The decrease in the unit cell parameters and volume is a result of the partial substitution of Ca²⁺ with smaller Gd³⁺ ions at both cation sites in the apatite-type structure [44]. The calculated data are in good agreement with previously reported Gd³⁺-doped hydroxyapatite [43]. Thus, it can be concluded that the impurity apatite phases are also doped by the Gd³⁺ ions. The Ca₂P₂O₇ phase is not doped by Gd³⁺ ions, as the unit cell parameters do not change significantly, accounting the possible error range (Table 2). The schematic representation of substitution of Ca²⁺ by Gd³⁺ ions in apatite (Figure 3a) and whitlockite (Figure 3b) phases is shown.



Figure 3. The schematic representation of substitution of Ca^{2+} by Gd^{3+} ions in apatite (**a**) and β -TCP (**b**) phases.

3.3. EPR Study

For EPR studies, only the Gd-TCP-pc (i.e., the sample obtained by precipitation from aqueous solutions of salts) powder was used, as it is more phase-pure with respect to the product obtained by mechano-chemical activation, i.e., 96% of β -TCP phase vs. 73%, respectively. The sample with a small concentration of Gd—0.001-Gd-TCP—was

chosen because higher concentrations of Gd in EPR might result in peaks' conglomerating and broadening.

The EPR spectra were measured at 25 K. In Figure 4a (black line, powder sample), the spectrum recorded at a minimum time between $\pi/2$ and π pulses, $\tau = 0.18 \ \mu$ s, is shown. It does not contain clearly distinguished individual lines. Measurements of the decay curves of the transverse magnetization revealed two exponential processes with $T_2 = 0.19 \pm 0.01 \ \mu$ s and $1.0 \pm 0.05 \ \mu$ s characteristic times. To check the nature of the appearance of the two processes, the EPR spectrum was recorded for a longer time of $\tau = 0.54 \ \mu$ s between $\pi/2$ and π pulses (Figure 4a, red line). In the case of the existence of two types of centers with different relaxation times, with increasing time, a strong decrease in the spectrum component with a longer time. This transforms the shape of the EPR spectrum (redistribution of intensities), which can be seen in Figure 4a as the difference between the black and red lines. The simplest mathematical processing separates the spectrum into two components with fast $T_2 = 0.19 \pm 0.01 \ \mu$ s and slow $T_2 = 1.0 \pm 0.05 \ \mu$ s transverse relaxation, shown in Figure 4b as blue and red lines, respectively.



Figure 4. (a) EPR spectra of 0.001 Gd-TCP-pc. The black line corresponds to the time between pulses $\tau = 0.18 \ \mu$ s, and the red line corresponds to $\tau = 0.54 \ \mu$ s (increased in amplitude by a factor of 4); (b) EPR spectrum components differing in decay times T₂ of transverse magnetization. The component indicated by the blue line corresponds to T₂ = 0.19 ± 0.01 \ \mus, and that indicated by the red line corresponds to T₂ = 1.0 ± 0.05 \ \mus.

Rare earth gadolinium Gd³⁺ ion with the 4f⁷ configuration in the ${}^{8}S_{7/2}$ ground state is paramagnetic and has electron spin S = 7/2 with zero orbital angular momentum L = 0. For this spin system, the spectrum should contain 2 * S = 7 different transitions, which give 7 lines in the EPR spectrum. The intensity of each of these lines will be proportional to the square of the matrix element $S_x = \sqrt{S(S+1) - M_S(1)M_S(2)}$, i.e., maximum for the transition $M_S = -\frac{1}{2} \leftrightarrow \frac{1}{2}$ and minimum for $M_S = \pm 7/2 \leftrightarrow \pm 5/2$. It makes it possible to compare the transitions to the lines based on their intensities, even when the spectrum is averaged by different orientations of the powder grains in the sample under study.

Center 2 has long relaxation times and an expressed structure of seven almost equidistant lines (the structure is shown by arrows in Figure 4b). The intensities of these lines increase toward the center of the spectrum, which indicates a pronounced axiality of the crystal structure corresponding to TCP crystals [45,46]. Center 1 with short relaxation times does not have such a structure and its linewidth is much higher than that of Center 2. Therefore, it can be attributed to the impurity of Gd³⁺ in the admixture phases, the low crystallinity of which leads to an additional broadening of the EPR lines.

The spin-lattice relaxation rate was measured for both centers at 25 K. The values of the magnetic field were $B_0 = 344.3 \text{ mT}$ (contributions are made by both types of centers) and

B₀ = 118.2 mT (there is only a contribution from the center 2). The spin-lattice relaxation rate of Gd³⁺ for both centers turned out to be short, $T_1 = 30 \pm 2 \mu s$, which is comparable to the relaxation of gadolinium in other crystals [47]. The electron-nuclear interactions were measured at 12 K. For this temperature, $T_1 = 160 \pm 8 \mu s$, which is sufficient for the HYSCORE sequence. The electron-nuclear interactions were detected at two values 118.2 mT and 344.3 mT of the magnetic field induction B₀, which allowed the observation to be made of the total spectrum HYSCORE (Figure 5a) and the spectrum only from Center 2 (Figure 5b). A strong interaction with the phosphorus nucleus was observed for Center 2 (Figure 5b). The peak corresponding to this interaction was narrow, which indicates the absence of a significant distribution in the Gd–P distances and a small distortion of the crystal structure. In the case of the sum of two HYSCORE spectra (Figure 5a), the electron-nuclear interaction with phosphorus was blurred, and it was much stronger than it should be for the transition $M_S = -1/2 \leftrightarrow 1/2$, which also indicates the localization of Gd³⁺ in a low crystalline phase.



Figure 5. 2D spectrum of electron-nuclear interactions measured using the HYSCORE sequence at magnetic field induction $B_0 = 344.3 \text{ mT}$ (**a**) and 118.2 mT (**b**). Dashed lines show the regions of expected interactions with ¹H, ³¹P nuclei, and ¹⁵⁵Gd and ¹⁵⁷Gd isotopes.

As it follows from the EPR experiments, two types of paramagnetic Gd³⁺ ions are found in the investigated materials, which differ in their electronic spin–spin relaxation (dephasing) times with $T_2 = 0.19 \pm 0.01 \ \mu$ s (type 1, fast relaxing) and $T_2 = 1.0 \pm 0.05 \ \mu$ s (type 2, slow relaxing), correspondingly. This suggests that gadolinium is present in two different phases.

The type 1 Gd does not reveal a resolved fine structure in the EPR spectrum. It can be caused by a wide distance distribution of ions (which creates a crystal field on the Gd^{3+}) in the neighborhood of the paramagnetic ion environment. In the HYSCORE spectrum, no interaction with nuclei is observed, likely also due to the distribution of the Gd^{3+} -nucleus distance, causing a strong broadening of the HYSCORE peaks. It can be speculated that the type 1 center is in the amorphous phase or in the phase containing a number of dislocations.

The type 2 Gd has a resolved fine structure in the EPR spectrum and reveals a hyperfine interaction with the ³¹P nuclei in the HYSCORE experiments, meaning that the spread of the distances between the paramagnetic ion and the nearest nuclei is small (quite modest). Therefore, it can be suggested that this type of Gd is detected in a crystal phase characterized by a low number of defects.

3.4. Thermogravimetric Analysis

To investigate the thermal behavior of powders, 0.1Gd-TCP samples obtained by precipitation and mechano-chemical activation methods were taken, in order to better investigate the effect of Gd³⁺. The thermal behavior of the 0.1Gd-TCP-pc and 0.1Gd-TCP-

ma samples differs significantly (Table 3). The thermal decomposition of 0.1Gd-TCP-pc proceeds in several steps and is accompanied by a strong endothermic effect at 250 °C, corresponding to the removal of chemically bonded water molecules. During the thermal decomposition of 0.1Gd-TCP-ma, two overlapping endo-effects are observed in the range of 80–200 °C, accompanied by a mass loss of 15%, which can be attributed to the removal of chemically coordinated water molecules.

Table 3. Thermogravimetric analysis data for 0.1Gd-TCP samples obtained by precipitation and mechano-chemical activation methods.

Sample	Temperature, °C	Thermal Effect Type	Mass Loss, wt%	Mass Loss Corresponds to
0.1Gd-TCP-pc	80	endothermic	5	physically adsorbed H ₂ O
	250	endothermic	45	chemically coordinated H ₂ O
0.1Gd-TCP-ma	110–250	endothermic	20	two-stage H ₂ O elimination

From the results presented in Table 3, it can be seen that the 0.1Gd-TCP-ma powder is more thermally stable: in this case, the mass loss is two times lower and starts at a higher temperature.

3.5. Specific Surface Area of Powders

Specific surface area experimental data for all the samples obtained by the BET method are presented in Table 4. As one can see from the table, the specific surface area of powders obtained by precipitation from aqueous solutions is more than twice higher compared to the specific surface area of powders obtained by mechano-chemical activation. The different specific surface area of the powders is related to the methods of their preparation. Powders obtained by precipitation follow the so-called "bottom up" path, i.e., individual ions interact with each other in the solution volume with the formation of a large number of crystallization centers. As a result of such crystallization, the concentration of ions in solution rapidly decreases and the growth of particles stops. This leads to the formation of nanoparticles with a size of tens of nanometers (see Section 3.6). Powders obtained by mechanochemical activation pass the so-called "top down" path, i.e., the initial oxides with certain particle sizes reduce their size as a result of grinding. The interaction takes place between these small particles and leads to the formation of larger particles compared to those obtained by the precipitation method. The incorporation of Gd^{3+} into the TCP structure leads to a decrease in the specific surface area of the powders, which is equivalent to an increase in the particle size. An increase in the particle size of the Gd-TCP-pc samples compared to TCP-ma can be associated with the formation of a smaller number of crystallization centers in the solution with gadolinium. A smaller number of crystallization centers is due to the fact that the formation of Gd-TCP-pc requires the combination of three particles (the Ca²⁺, Gd³⁺ cations, and the PO_4^{3-} anion), whereas the formation of TCP-pc requires a combination of two particles Ca^{2+} and PO_4^{3-} .

Table 4. BET data for TCP and Gd-TCP, synthesized by precipitations and mechano-activation methods.

Ν	Sample	Surface Area, m ² /g
1	TCP-pc	77.07 ± 0.09
2	0.01Gd-TCP-pc	72.49 ± 0.07
3	0.1Gd-TCP-pc	66.41 ± 0.13
4	TCP-ma	30.09 ± 0.01
5	0.01Gd-TCP-ma	35.88 ± 0.04
6	0.1Gd-TCP-ma	32.73 ± 0.03

3.6. TEM Studies of Powders

For TEM studies, β -TCP-pc, β -TCP-ma, 0.01Gd-TCP-pc, and 0.1Gd-TCP-pc powder samples were selected. The β -TCP-pc and β -TCP-ma samples were chosen in order to observe the particle differences prepared by precipitation (1) and mechano-chemical activation (2). As one can see from Figure 6a,b, small particles of tens of nanometers are prepared by synthesis route (1), while in the case of synthesis route (2), the particle size is in the range of hundreds of nanometers. For the Gd-TCP-pc with different substitution amounts, no significant differences are observed with respect to the pure β -TCP-pc sample, as expected.



Figure 6. TEM images of TCP-pc (a), TCP-ma (b), 0.01Gd-TCP-pc (c), and 0.1Gd-TCP-pc (d).

3.7. SEM Observations of Ceramics

For SEM investigation, 0.1Gd-TCP-pc and 0.1Gd-TCP-ma ceramic samples with the highest concentration of Gd were used, in order to better observe the influence of Gd on the samples' morphology and microstructure. The SEM images of the synthesized 0.1Gd-TCP ceramic samples after sintering at 1100 °C are presented in Figure 7. The microstructure of ceramic sample obtained from the powder synthesized by precipitation from solutions is inhomogeneous: there are both large conglomerates, consisting of small grains, and smaller grains, ranging in size from 1 up to about 50 μ m (Figure 7 and Table 4). The ceramics obtained from powder synthesized using mechano-chemical activation look more uniform; the grain size varies from 0.4 to 1.4 μ m (Figure 7 and Table 4). The comparison of the grain sizes of Gd-TCP, obtained using two methods, shows that larger grains and conglomerates of grains are formed in the case of using the precipitation method. This can be explained by the fact that, as a result of the synthesis by precipitation from aqueous solutions, more dispersed (nanoscale) powders are obtained (see TEM results, Section 3.6), compared to powders synthesized by mechano-chemical activation (see TEM results, Section 3.6). During the drying process, agglomeration of nanopowders occurs, accompanied by a decrease in surface energy. When removing water having a high surface tension ($\sigma = 72.7 \text{ MJ/m}^2$), aggregation of nanoparticles dispersed in an aqueous suspension occurs, accompanied by the formation of micro-scale aggregates. During further sintering at a higher temperature of 1100 °C, the particles inside the aggregate unit are tightly sintered, and, therefore, after sintering, initial nanoparticles are transformed into particles of 5–10 μ m. Thus, as a result of the sintering of powders synthesized by precipitation from aqueous solutions, ceramics with a large grain size spread are obtained (Figure 7 and Table 4).



Figure 7. SEM images of 0.1Gd-TCP-pc (a,b) and 0.1Gd-TCP-ma (c,d) followed by sintering at 1100 °C.

In the case of sintering of the 0.1Gd-TCP-ma powder, ceramics with a more uniform grain size are obtained. When using the 0.1Gd-TCP-pc powders, ceramics are composed by grains of dissimilar size (Figure 7a): larger grains are composed of smaller, joined grains. This is due to the fact that smaller crystallites obtained by the precipitation method from aqueous solutions agglomerate during drying, and at 1100 °C, their sintering occurs inside the agglomerates. This fact is confirmed by the size of the ceramic grains (Table 5): the average grain size of ceramics from the 0.1Gd-TCP-pc powder is 2.2 μ m. It is almost three times larger than the grain size of ceramics from the 0.1Gd-TCP-ma powder. The grain size presented in Table 5 was determined from the SEM data by means of the random secant method.

Table 5. Average grain size of 0.1Gd-TCP ceramics.

Grain Size, μm	0.1Gd-TCP-pc	0.1Gd-TCP-ma
minimal	1.2	0.4
maximal	49.1	1.4
median	2.2	0.8

The pore size, calculated from the SEM data by the random secant method for the 0.1Gd-TCP-pc ceramics (Figure 7a,b), varies from 1–2 μ m up to 5–10 μ m. The sintering process was carried out at 1100 °C, and the porosity at this temperature is maintained, following from the SEM data described above. In connection with this, the bending strength of ceramics is low—about 30 MPa, and the fracture curve corresponds to the brittle fracture characteristic for ceramic samples [48]. In contrast, the 0.1Gd-TCP-ma ceramics are characterized by a more homogeneous structure (see Figure 7c,d), and its bending strength of 38.6 MPa is higher, which is connected to the fact that the pore size, in this case, does not exceed 2 μ m.

3.8. Antibacterial Activity Study

The results obtained by applying the microorganisms (*S. aureus, E. coli, S. typhimurium, E. faecalis,* and *C. albicans*) grown in the presence of 0.1Gd-TCP-pc and 0.1Gd-TCP-ma powders demonstrate a good inhibition of growth for all the microorganism species. The

values of the mean OD, standard deviation, %growth, and %inhibition for each microorganism for two tested samples, after 24 h of incubation, are detailed in Table 6 and Figure 8. For all the microorganisms, there is a good inhibition of growth (a minimum of 12.2% and a maximum of 30.4%). As can be observed, the 0.1Gd-TCP-pc inhibits the growth of *S. aureus, E. coli, E. faecalis*, and *C. albicans* better than the 0.1Gd-TCP-ma. Only for the *S. typhimurium*, the inhibition of growth is slightly higher for the 0.1Gd-TCP-ma compared to the 0.1-Gd-TCP-pc.

Table 6. Mean values of OD_{600} , SD, and percentage of growth and inhibition of the different microorganisms by 0.1Gd-TCP-pc and 0.1Gd-TCP-ma powders, derived from three independent experiments.

		C. albicans				
	OD ₆₀₀	SD	% Growth	% Inhibition		
ctr + (control sample)	0.711	0.008	100	0		
0.1Gd-TCP-pc	0.495	0.020	69.7	30.3		
0.1Gd-TCP-ma	0.519	0.007	73.1	26.9		
		E. coli				
	OD ₆₀₀	SD	% Growth	% Inhibition		
ctr + (control sample)	0.845	0.025	100	0		
0.1Gd-TCP-pc	0.638	0.054	75.5	24.5		
0.1Gd-TCP-ma	0.741	0.015	87.8	12.2		
		E. faecalis				
	OD ₆₀₀	SD	% Growth	% Inhibition		
ctr + (control sample)	0.570	0.021	100	0		
0.1Gd-TCP-pc	0.443	0.011	77.8	22.2		
0.1Gd-TCP-ma	0.445	0.032	78.1	21.9		
S. aureus						
	OD ₆₀₀	SD	% Growth	% Inhibition		
ctr + (control sample)	0.951	0.021	100	0.		
0.1Gd-TCP-pc	0.723	0.072	76.1	23.9		
0.1Gd-TCP-ma	0.744	0.016	78.3	21.7		
S. typhimurium						
	OD ₆₀₀	SD	% Growth	% Inhibition		
ctr + (control sample)	0.906	0.076	100	0		
0.1Gd-TCP-pc	0.634	0.040	70.0	30.0		
0.1Gd-TCP-ma	0.648	0.043	71.6	28.4		

3.9. Metabolic Activity Study

The metabolic activity study of the NCTC L929 cells performed by the MTT test (Figure 9) showed the absence of significant differences between the experiment and control in the ceramic samples of pure β -TCP, 0.1Gd-TCP-pc, and 0.01Gd-TCP-pc obtained from powders synthesized by the precipitation method, indicating the absence of toxic effects for three-day extracts (Figure 9). The extracts from the 0.1Gd-TCP-ma sample have an inhibitory effect on the NCTC L929 fibroblasts (reliability according to the Mann–Whitney *U*-test *p* < 0.01) (see Figure 8).



Figure 8. Results of the growth rate of *S. aureus, E. coli, S. typhimurium, E. faecalis,* and *C. albicans* in the presence and absence (positive control, ctr +) of 0.1Gd-TCP-pc and 0.1Gd-TCP-ma. The %growth was calculated from three independent experiments.



Figure 9. Metabolic activity of the NCTC L929 cells after 24 h of incubation with 3 day extracts of pure β -TCP (1), 0.01Gd-TCP (2), and 0.1Gd-TCP (3) synthesized by precipitation and mechanochemical activation.

However, the inoculation of cells onto the surface of the tested materials and the study of their viability (by the direct contact method) allowed us to establish the absence of toxic effects in the Gd-TCP samples. Images of cells cultured on the surface of materials are shown in Figure 10.

The DPSC test study showed that there is a decrease in the total number of cells on ceramic samples doped with Gd³⁺ ions, obtained by mechano-chemical activation synthesis, in comparison with the control (see Figure 11). However, the number of dead cells on the surface of all studied ceramic materials is insignificant, which indicates the absence of cytotoxicity of these ceramic materials. Thus, the decrease in cellular activity is not associated with cell death. Therefore, the 0.01Gd-TCP and 0.1Gd-TCP ceramic samples obtained from powders synthesized by both the precipitation and the mechano-chemical activation can be recognized as biocompatible.



Figure 10. Images of the DPSC cells during incubation on the surface of tested ceramic materials during the first day after inoculation. Dyeing propidium iodide (**A**), Hoechst 33,342 (**B**), and SYTO 9 (**C**) (scale 100 μm).



Figure 11. Number of DPSC cells seeded on the surface of ceramics: TCP-pc (1), TCP-ma (2), 0.01Gd-TCP-pc (3), 0.01Gd-TCP-ma (4), 0.1Gd-TCP-pc (5), 0.1Gd-TCP-ma (6), and control sample (7). The error bars show the standard deviation.

4. Conclusions

It was established that the synthesis method influenced the phase composition of the prepared Gd-substituted TCP powders: the precipitation from solutions method resulted in a more homogeneous phase composition of β -TCP-type. In particular, the 0.1Gd-TCP-pc and 0.01Gd-TCP-pc powders contained 96 wt% of β -TCP, whereas the 0.1Gd-TCP-ma and 0.01Gd-TCP-ma contained 73 and 87 wt% of β -TCP, respectively, as confirmed by the XRD and FT-IR methods. Both synthesis routes, the precipitation from solutions and mechanochemical activation, led to the effective substitution of Ca²⁺ ions by Gd³⁺ in both β -TCP (main phase) and apatite (admixture) phases. These results were revealed by the EPR method, which also confirmed the oxidation state of the Gd³⁺ ions. It was shown that Gd³⁺ ions were localized directly in the crystal lattice, with a small scattering of Ca–P distances and a slight distortion in the EPR spectra of the investigated materials was associated with the presence of gadolinium in two different phases, the main β -TCP phase and impurity phases (apatite/pyrophosphate), or a secondary amorphous phase, in agreement with the XRD results.

The 0.1Gd-TCP-ma powder was more thermally stable with respect to the 0.1Gd-TCP-pc: its mass loss was two times lower and started at a higher temperature. The specific surface area of the prepared powders obtained by precipitation from aqueous solutions was more than twice higher compared to the specific surface area of powders obtained by mechano-chemical activation. In particular, the specific surface area value obtained for 0.01Gd-TCP-pc was 72.4 m²/g, that for 0.1Gd-TCP-pc was 66.4 m²/g, that for 0.01Gd-TCP-ma was 35.8 m²/g, and that for 0.1Gd-TCP-ma was 32.7 m²/g.

The method of synthesis also affected the size and morphology of the obtained powders. TEM observations revealed that, in the case of the precipitation synthesis, the powders particle size was tens of nanometers, while, in the case of mechano-chemical activation, particles of hundreds of nanometers were obtained.

The SEM microstructure of ceramics obtained from the powder synthesized by precipitation was inhomogeneous, consisting of grains of 1–50 μ m. The ceramics obtained from powder synthesized using mechano-chemical activation were more uniform, with grain sizes of 0.4–1.4 μ m. The pore size for 0.1Gd-TCP-pc ceramics varied from 1–2 μ m up to 5–10 μ m with a bending strength of about 30 MPa. The 0.1Gd-TCP-ma ceramics were more homogeneous, with a pore size of 2 μ m and a bending strength of about 39 MPa.

The results of the antimicrobial activity tests showed that 0.1Gd-TCP-pc and 0.1Gd-TCP-ma materials were able to inhibit the growth of the four tested bacteria (*S. aureus*, *E. coli*, *S. typhimurium*, and *E. faecalis*) and one tested fungus (*C albicans*) with respect to the relative controls: about 30% of inhibition for 0.1Gd-TCP-pc and about 28% for 0.1Gd-TCP-ma were detected. In particular, the 0.1Gd-TCP-pc inhibited *S. aureus*, *E. coli*, *E. faecalis*, and *C. albicans* more effectively than the 0.1Gd-TCP-ma. The growth of *S. typhimurium* was inhibited slightly better by the 0.1Gd-TCP-ma with respect to the 0.1Gd-TCP-pc.

According to the results of the in vitro testing, all the prepared ceramics can be recognized as biocompatible. The MTT test results on the metabolic activity of the NCTC L929 cells evidenced the absence of toxic effects. The DPSC viability study showed the absence of cytotoxicity of the prepared ceramic materials doped with Gd ions with no difference for the synthesis route.

Author Contributions: Conceptualization, I.V.F. and J.V.R.; methodology, I.V.F., D.V.D., K.B., G.A.D., M.A.S., F.F.M., A.S.F., V.G.Y., I.V.A., B.I.L. and J.V.R.; validation, I.V.F., D.V.D., K.B., G.A.D., F.F.M., V.G.Y., I.V.A., S.M.B., B.I.L. and J.V.R.; formal analysis, D.V.D., K.B., G.A.D., M.A.S., F.F.M. and A.S.F.; investigation, I.V.F., D.V.D., K.B., G.A.D., M.A.S., F.F.M. and A.S.F.; resources, I.V.F., G.A.D., K.B., F.F.M., V.G.Y., S.M.B., B.I.L. and J.V.R.; data curation, D.V.D., K.B., G.A.D., M.A.S. and F.F.M.; writing—original draft preparation, I.V.F., D.V.D., K.B., A.S.F., M.A.S., F.F.M., B.I.L. and J.V.R.; writing—review and editing, J.V.R.; visualization, D.V.D.; supervision, I.V.F. and J.V.R.; funding acquisition, I.V.F. and F.F.M. All authors have read and agreed to the published version of the manuscript.

Funding: The work was supported by the Russian Science Foundation (Project No. 22-23-00278). The EPR studies were supported by the Russian Federation State Task No. 0671-2020-0051. The X-ray study was carried out in accordance with the state of the Russian Federation, state registration number 122011300125-2.

Institutional Review Board Statement: All the experiments were conducted in agreement with the good clinical practice and ethical principles of the current edition of the Declaration of Helsinki, after the permission of the Ethics Committee of Institute of Theoretical and Experimental Biophysics of the Russian Academy of Sciences (Moscow, Russian Federation), protocol Nº 31 from 9 February 2021.

Informed Consent Statement: Informed consent was obtained from all subjects involved in the study.

Data Availability Statement: The data are available upon an official and reasonable request.

Acknowledgments: The technical support of Massimo Di Menno Di Bucchianico, Luca Imperatori, and Marco Ortenzi is gratefully acknowledged.

Conflicts of Interest: The authors declare no conflict of interest.

Ethics Statement: Postnatal human dental pulp stem cells were extracted from the 3rd molar tooth of a donor. The tooth was removed according to the orthodontic indications at the Central Research Institute of Dentistry and Maxillofacial Surgery of the Ministry of Health (Moscow, Russian Federation), in accordance with the ethics committee requirements, after the consent signed by the patient's parents. All the experiments were conducted in agreement with the good clinical practice and ethical principles of the current edition of the Declaration of Helsinki.

References

- 1. Ageing and Health. Available online: https://www.who.int/news-room/fact-sheets/detail/ageing-and-health (accessed on 4 October 2021).
- 2. Woolf, A.D.; Pfleger, B. Burden of major musculoskeletal conditions. Bull. World Health Organ. 2003, 81, 646–656.
- Ratnayake, J.T.B.; Mucalo, M.; Dias, G.J. Substituted hydroxyapatites for bone regeneration: A review of current trends. J. Biomed. Mater. Res. Part B Appl. Biomater. 2017, 105, 1285–1299. [CrossRef] [PubMed]
- Bohner, M.; Santoni, B.L.G.; Döbelin, N. β-tricalcium phosphate for bone substitution: Synthesis and properties. *Acta Biomater*. 2020, 113, 23–41. [CrossRef] [PubMed]
- 5. Wang, W.; Yeung, K.W.K. Bone grafts and biomaterials substitutes for bone defect repair: A review. *Bioact. Mater.* **2017**, *2*, 224–247. [CrossRef]
- 6. Sohn, H.-S.; Oh, J.-K. Review of bone graft and bone substitutes with an emphasis on fracture surgeries. *Biomater. Res.* **2019**, *23*, 9. [CrossRef] [PubMed]

- Zyman, Z.; Glushko, V.; Dedukh, N.; Malyshkina, S.; Ashukina, N. Porous calcium phosphate ceramic granules and their behaviour in differently loaded areas of skeleton. *J. Mater. Sci. Mater. Med.* 2008, 19, 2197–2205. [CrossRef]
- 8. Bohner, M. Physical and chemical aspects of calcium phosphates used in spinal surgery. *Eur. Spine J.* **2001**, *10*, S114–S121. [CrossRef]
- Fadeeva, I.V.; Gafurov, M.R.; Kiiaeva, I.A.; Orlinskii, S.B.; Kuznetsova, L.M.; Filippov, Y.Y.; Fomin, A.S.; Davydova, G.A.; Selezneva, I.I.; Barinov, S.M. Tricalcium Phosphate Ceramics Doped with Silver, Copper, Zinc, and Iron (III) Ions in Concentrations of Less Than 0.5 wt.% for Bone Tissue Regeneration. *Bionanoscience* 2017, 7, 434–438. [CrossRef]
- 10. Laskus, A.; Kolmas, J. Ionic Substitutions in Non-Apatitic Calcium Phosphates. Int. J. Mol. Sci. 2017, 18, 2542. [CrossRef]
- 11. Lu, H.; Zhou, Y.; Ma, Y.; Xiao, L.; Ji, W.; Zhang, Y.; Wang, X. Current Application of Beta-Tricalcium Phosphate in Bone Repair and Its Mechanism to Regulate Osteogenesis. *Front. Mater.* **2021**, *8*, 277. [CrossRef]
- Fadeeva, I.V.; Lazoryak, B.I.; Davidova, G.A.; Murzakhanov, F.F.; Gabbasov, B.F.; Petrakova, N.V.; Fosca, M.; Barinov, S.M.; Vadalà, G.; Uskoković, V.; et al. Antibacterial and cell-friendly copper-substituted tricalcium phosphate ceramics for biomedical implant applications. *Mater. Sci. Eng. C* 2021, 129, 112410. [CrossRef] [PubMed]
- Rau, J.V.; Fadeeva, I.V.; Fomin, A.S.; Barbaro, K.; Galvano, E.; Ryzhov, A.P.; Murzakhanov, F.; Gafurov, M.; Orlinskii, S.; Antoniac, I.; et al. Sic Parvis Magna: Manganese-Substituted Tricalcium Phosphate and Its Biophysical Properties. *ACS Biomater. Sci. Eng.* 2019, *5*, 6632–6644. [CrossRef] [PubMed]
- Uskoković, V.; Graziani, V.; Wu, V.M.; Fadeeva, I.V.; Fomin, A.S.; Presniakov, I.A.; Fosca, M.; Ortenzi, M.; Caminiti, R.; Rau, J.V. Gold is for the mistress, silver for the maid: Enhanced mechanical properties, osteoinduction and antibacterial activity due to iron doping of tricalcium phosphate bone cements. *Mater. Sci. Eng. C* 2019, *94*, 798–810. [CrossRef]
- Fadeeva, I.V.; Goldberg, M.A.; Preobrazhensky, I.I.; Mamin, G.V.; Davidova, G.A.; Agafonova, N.V.; Fosca, M.; Russo, F.; Barinov, S.M.; Cavalu, S.; et al. Improved cytocompatibility and antibacterial properties of zinc-substituted brushite bone cement based on β-tricalcium phosphate. *J. Mater. Sci. Mater. Med.* 2021, 32, 99. [CrossRef] [PubMed]
- Graziani, G.; Barbaro, K.; Fadeeva, I.V.; Ghezzi, D.; Fosca, M.; Sassoni, E.; Vadalà, G.; Cappelletti, M.; Valle, F.; Baldini, N.; et al. Ionized jet deposition of antimicrobial and stem cell friendly silver-substituted tricalcium phosphate nanocoatings on titanium alloy. *Bioact. Mater.* 2021, *6*, 2629–2642. [CrossRef]
- Kannan, S.; Pina, S.; Ferreira, J.M.F. Formation of Strontium-Stabilized β-Tricalcium Phosphate from Calcium-Deficient Apatite. J. Am. Ceram. Soc. 2006, 89, 3277–3280. [CrossRef]
- Singh, R.K.; Srivastava, M.; Prasad, N.K.; Awasthi, S.; Dhayalan, A.; Kannan, S. Iron doped β-Tricalcium phosphate: Synthesis, characterization, hyperthermia effect, biocompatibility and mechanical evaluation. *Mater. Sci. Eng. C* 2017, *78*, 715–726. [CrossRef]
- De Bonis, A.; Uskoković, V.; Barbaro, K.; Fadeeva, I.; Curcio, M.; Imperatori, L.; Teghil, R.; Rau, J.V. Pulsed laser deposition temperature effects on strontium-substituted hydroxyapatite thin films for biomedical implants. *Cell Biol. Toxicol.* 2020, 36, 537–551. [CrossRef]
- Gu, Y.; Zhang, J.; Zhang, X.; Liang, G.; Xu, T.; Niu, W. Three-dimensional Printed Mg-Doped β-TCP Bone Tissue Engineering Scaffolds: Effects of Magnesium Ion Concentration on Osteogenesis and Angiogenesis In Vitro. *Tissue Eng. Regen. Med.* 2019, 16, 415–429. [CrossRef] [PubMed]
- Wang, Z.; Liu, Q.; Liu, C.; Tan, W.; Tang, M.; Zhou, X.; Sun, T.; Deng, Y. Mg²⁺ in β-TCP/Mg–Zn composite enhances the differentiation of human bone marrow stromal cells into osteoblasts through MAPK-regulated Runx2/Osx. *J. Cell. Physiol.* 2020, 235, 5182–5191. [CrossRef]
- Kalidoss, M.; Yunus Basha, R.; Doble, M.; Sampath Kumar, T.S. Theranostic Calcium Phosphate Nanoparticles With Potential for Multimodal Imaging and Drug Delivery. Front. Bioeng. Biotechnol. 2019, 7, 7. [CrossRef]
- 23. Qi, C.; Lin, J.; Fu, L.-H.; Huang, P. Calcium-based biomaterials for diagnosis, treatment, and theranostics. *Chem. Soc. Rev.* 2018, 47, 357–403. [CrossRef]
- Ashokan, A.; Gowd, G.S.; Somasundaram, V.H.; Bhupathi, A.; Peethambaran, R.; Unni, A.K.K.; Palaniswamy, S.; Nair, S.V.; Koyakutty, M. Multifunctional calcium phosphate nano-contrast agent for combined nuclear, magnetic and near-infrared in vivo imaging. *Biomaterials* 2013, 34, 7143–7157. [CrossRef]
- Liu, Y.; Sun, Y.; Cao, C.; Yang, Y.; Wu, Y.; Ju, D.; Li, F. Long-term biodistribution in vivo and toxicity of radioactive/magnetic hydroxyapatite nanorods. *Biomaterials* 2014, 35, 3348–3355. [CrossRef]
- 26. Wang, P.; Hao, L.; Wang, Z.; Wang, Y.; Guo, M.; Zhang, P. Gadolinium-Doped BTO-Functionalized Nanocomposites with Enhanced MRI and X-ray Dual Imaging to Simulate the Electrical Properties of Bone. *ACS Appl. Mater. Interfaces* **2020**, *12*, 49464–49479. [CrossRef]
- Meenambal, R.; Poojar, P.; Geethanath, S.; Kannan, S. Substitutional limit of gadolinium in β-tricalcium phosphate and its magnetic resonance imaging characteristics. J. Biomed. Mater. Res. Part B Appl. Biomater. 2017, 105, 2545–2552. [CrossRef]
- Zhu, G.; Zhao, R.; Li, Y.; Tang, R. Multifunctional Gd,Ce,Tb co-doped β-tricalcium phosphate porous nanospheres for sustained drug release and bioimaging. *J. Mater. Chem. B* 2016, *4*, 3903–3910. [CrossRef]
- Bulina, N.V.; Chaikina, M.V.; Prosanov, I.Y.; Dudina, D.V. Strontium and silicate co-substituted hydroxyapatite: Mechanochemical synthesis and structural characterization. *Mater. Sci. Eng. B* 2020, 262, 114719. [CrossRef]
- Le Bail, A.; Duroy, H.; Fourquet, J.L. Ab-initio structure determination of LiSbWO₆ by X-ray powder diffraction. *Mater. Res. Bull.* 1988, 23, 447–452. [CrossRef]

- 31. Petricek, V.; Dusek, M.; Palatinus, L.; Petrícek, V.; Dušek, M.; Palatinus, L. Crystallographic computing system JANA2006: General features. *Z. Für Krist.* 2014, 229, 345–352. [CrossRef]
- Yashima, M.; Sakai, A.; Kamiyama, T.; Hoshikawa, A. Crystal structure analysis of β-tricalcium phosphate Ca₃(PO₄)₂ by neutron powder diffraction. *J. Solid State Chem.* 2003, 175, 272–277. [CrossRef]
- 33. Ruszala, F.; Kostiner, E. Preparation and characterization of single crystals in the apatite system Ca₁₀(PO₄)₆(Cl,OH)₂. *J. Cryst. Growth* **1975**, *30*, 93–95. [CrossRef]
- 34. Boudin, S.; Grandin, A.; Borel, M.M.; Leclaire, A.; Raveau, B. Redetermination of the β-Ca₂P₂O₇ structure. *Acta Crystallogr. Sect. C Cryst. Struct. Commun.* **1993**, 49, 2062–2064. [CrossRef]
- Poltavtseva, R.A.; Nikonova, Y.A.; Selezneva, I.I.; Yaroslavtseva, A.K.; Stepanenko, V.N.; Esipov, R.S.; Pavlovich, S.V.; Klimantsev, I.V.; Tyutyunnik, N.V.; Grebennik, T.K.; et al. Mesenchymal Stem Cells from Human Dental Pulp: Isolation, Characteristics, and Potencies of Targeted Differentiation. *Bull. Exp. Biol. Med.* 2014, *158*, 164–169. [CrossRef]
- Savchyn, P.; Karbovnyk, I.; Vistovskyy, V.; Voloshinovskii, A.; Pankratov, V.; Cestelli Guidi, M.; Mirri, C.; Myahkota, O.; Riabtseva, A.; Mitina, N.; et al. Vibrational properties of LaPO₄ nanoparticles in mid- and far-infrared domain. *J. Appl. Phys.* 2012, 112, 124309. [CrossRef]
- 37. Shannon, R.D. Revised effective ionic radii and systematic studies of interatomic distances in halides and chalcogenides. *Acta Crystallogr. Sect. A* **1976**, *32*, 751–767. [CrossRef]
- 38. Bessière, A.; Aı⁻⁻t, R.; Benhamou, A.; Wallez, G.; Lecointre, A.; Viana, B. Site occupancy and mechanisms of thermally stimulated luminescence in Ca₉Ln(PO₄)₇ (Ln = lanthanide). *Acta Mater.* **2012**, *60*, 6641–6649. [CrossRef]
- 39. Lazoriak, B.I.; Golubev, V.N.; Salmon, R.; Parent, C.; Hagenmuller, P. Distribution of Eu³⁺ ions in whitlockite-type Ca_{3-x}Eu_{2x/3}(PO₄)₂ orthophosphates. *Eur. J. Solid State Inorg. Chem.* **1989**, *26*, 455–463.
- 40. Demirel, B.; Saban, E.; Yaras, A.; Akkurt, F. Synthesis of Gd+3 doped hydroxyapatite ceramics: Optical, thermal and electrical properties. *J. Asian Ceram. Soc.* 2021, *9*, 865–873. [CrossRef]
- 41. Kim, J.Y.; Fenton, R.R.; Hunter, B.A.; Kennedy, B.J. Powder diffraction studies of synthetic calcium and lead apatites. *Aust. J. Chem.* 2000, *53*, 679–686. [CrossRef]
- Gomes, S.; Nedelec, J.-M.; Jallot, E.; Sheptyakov, D.; Renaudin, G. Unexpected Mechanism of Zn²⁺ Insertion in Calcium Phosphate Bioceramics. *Chem. Mater.* 2011, 23, 3072–3085. [CrossRef]
- Paterlini, V.; Bettinelli, M.; Rizzi, R.; El Khouri, A.; Rossi, M.; Della Ventura, G.; Capitelli, F. Characterization and Luminescence of Eu³⁺- and Gd³⁺-Doped Hydroxyapatite Ca₁₀(PO₄)₆(OH)₂. *Crystals* 2020, *10*, 806. [CrossRef]
- Ignjatović, N.L.; Mančić, L.; Vuković, M.; Stojanović, Z.; Nikolić, M.G.; Škapin, S.; Jovanović, S.; Veselinović, L.; Uskoković, V.; Lazić, S.; et al. Rare-earth (Gd³⁺,Yb³⁺/Tm³⁺, Eu³⁺) co-doped hydroxyapatite as magnetic, up-conversion and down-conversion materials for multimodal imaging. *Sci. Rep.* 2019, *9*, 16305. [CrossRef]
- Clayton, J.A.; Keller, K.; Qi, M.; Wegner, J.; Koch, V.; Hintz, H.; Godt, A.; Han, S.; Jeschke, G.; Sherwin, M.S.; et al. Quantitative analysis of zero-field splitting parameter distributions in Gd(III) complexes. *Phys. Chem. Chem. Phys.* 2018, 20, 10470–10492. [CrossRef] [PubMed]
- Nakashima, K.; Yamauchi, J. Magnetic properties of gadolinium-doped β-tricalcium phosphate. J. Alloy. Compd. 2006, 408–412, 761–765. [CrossRef]
- 47. Maron, S.; Dantelle, G.; Gacoin, T.; Devreux, F. NMR and ESR relaxation in Nd- and Gd-doped LaPO₄: Towards the accurate determination of the doping concentration. *Phys. Chem. Chem. Phys.* **2014**, *16*, 18788–18798. [CrossRef]
- 48. Barinov, S.M. Calcium phosphate-based ceramic and composite materials for medicine. *Russ. Chem. Rev.* **2010**, *79*, 13–29. [CrossRef]