

Monitoring of tumor vascular normalization: the key points from basic research to clinical application

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Abstract: Tumor vascular normalization alleviates hypoxia in the tumor microenvironment, reduces the degree of malignancy, and increases the efficacy of traditional therapy. However, the time window for vascular normalization is narrow; therefore, how to determine the initial and final points of the time window accurately is a key factor in combination therapy. At present, the gold standard for detecting the normalization of tumor blood vessels is histological staining, including tumor perfusion, microvessel density (MVD), vascular morphology, and permeability. However, this detection method is almost unrepeatable in the same individual and does not dynamically monitor the trend of the time window; therefore, finding a relatively simple and specific monitoring index has important clinical significance. Imaging has long been used to assess changes in tumor blood vessels and tumor changes caused by the oxygen environment in clinical practice; some preclinical and clinical research studies demonstrate the feasibility to assess vascular changes, and some new methods were in preclinical research. In this review, we update the most recent insights of evaluating tumor vascular normalization.

Keywords: angiogenesis, vascular normalization, time window

Background

The growth of solid tumors is closely related to active recruitment of blood vessel network – the so-called tumor angiogenesis. The tumor cells away from vessels experience hypoxia due to deficiency of blood and oxygen when the tumor is larger than 1–2 mm; as a result, tumor cells initiate the process of angiogenesis by generating excessive pro-angiogenic factors as an adaptive adjustment.^{1,2} Various molecules and genes have been identified to play a critical role in angiogenesis,^{3,4} under these circumstances, the equilibrium between angiogenic promoters and angiogenic inhibitors tilts in favor of the pro-angiogenic factors,^{3–6} which breaks the existing vascular silence and elicits the angiogenesis of tumor vessels.^{7,8} Professor Judah Folkman first proposed the theory of tumor angiogenesis in 1971,^{1,5} and a new therapy method that aimed to starve tumors by blocking their blood vessels was established. The first clinical trial of anti-angiogenesis was of interferon alpha for life-threatening hemangioma,⁹ and the first anti-angiogenesis agent approved for clinical use is bevacizumab, which is used for treating colon cancer, lung cancer, kidney cancer, and brain cancer. However, some clinical trials showed that the efficacy of anti-angiogenesis monotherapy is limited,^{10–12} and antivascular endothelial growth factor (anti-VEGF) therapy cannot produce sustained shrinkage in certain tumors, such as colorectal and breast cancer tumors.¹³ It is noteworthy that the combination of anti-angiogenesis therapy with

systemic chemotherapy has often proven to be an effective strategy, with outcomes better than those of chemotherapy alone,^{13–19} which means that anti-angiogenesis in some way enhances the activity of cytotoxins. Why is this happening?

In response, Jain et al^{7,20,21} proposed the “normalization of tumor blood vessels” hypothesis in 2001. In tumors, uncontrolled angiogenesis is associated with damage of the tumor vascular maturation process, leading to a heterogeneous structure with tortuous, dilated, increased endothelial cell gap, and scarcity of pericyte coverage.^{22,23} These structural abnormalities contribute to dysfunction in tumor vessels, characterized by hypoperfusion, hyperpermeability, increased interstitial fluid pressure, and severe hypoxia.^{7,22,24} As a result, blood supply deficiency and interstitial hypertension impede the delivery of cytotoxic agents to solid tumors,^{4,22,25} and hypoxia favors tumor progression and acquired resistance both in radiotherapy and chemotherapy.^{26–28} The hypothesis of tumor vascular normalization posits that judicious use of anti-angiogenic therapy restores the abnormal structure and function of the tumor vasculature toward a more normal state²² and tumor blood flow (BF) and oxygenation transiently increase, thus providing an opportunity to improve radiotherapy, chemotherapy, and immunotherapy^{13,21,25–30} (Figure 1).

However, limitations exist in the clinical application of tumor vascular normalization – one of which is how to detect the time window simply and repeatedly. Tumor vascular normalization manifested as reduced blood vessel density, more regular vascular distribution, integrated pericyte coverage, and increased tumor perfusion. All these changes can be determined by histological detection. Vascular

endothelial cells can be marked by CD 31 and CD 34,^{14,15,25,31} and markers for tumor pericytes include NG2, PDGFR- β , and α -SMA,^{15,25,30} which are readily detected in pericytes in tumor angiogenesis. Tumor perfusion was determined by intravenous injection of fluorescein-labeled lectin or Evans blue,²⁶ and vascular permeability was measured by fluorescein-labeled dextran.¹⁵ However, the above-mentioned methods are difficult to carry out in the clinic because it is almost unrepeatable in the same individual; thus, it is difficult to dynamically monitor the process of tumor vascular normalization, which limits the ability of guiding traditional therapy. Therefore, establishing a more convenient and repeatable detection method of vascular normalization is of great significance. In this review, we summarized the novel insights of detecting tumor vascular normalization from studies and discussed the questions that must be faced in the clinic (Table 1).

Computed tomography (CT)

Tumor vascular normalization is often manifested as changes in the vascular network architecture and perfusion. CT can visualize the vascular density, bifurcation, perfusion, and oxygen content of a tumor. CT for detecting tumor vessels has been proposed as early as the tumor vascular normalization proposed.²⁰ CT perfusion imaging is used to obtain the time–density curve of the region of interest (ROI) through a continuous scan after the contrast medium of bolus injection, and the hemodynamic parameters are calculated by software using mathematical models. Perfusion CT parameters of blood volume (BV), which may be related to vascular

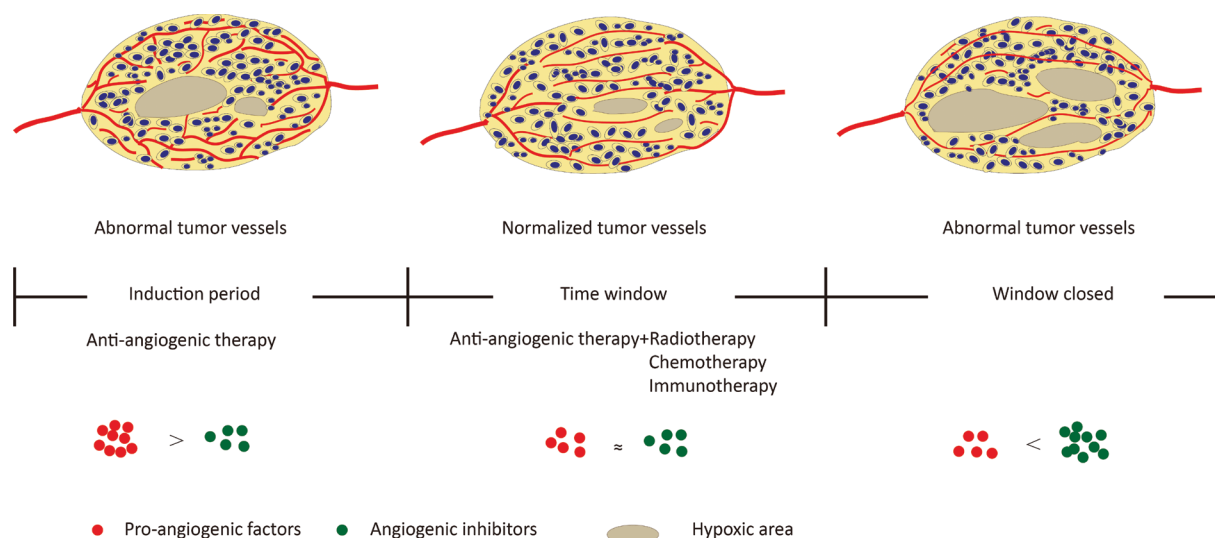


Figure 1 Proangiogenic factors and angiogenic inhibitors tend to be in a state of equilibrium after moderate anti-angiogenesis therapy, forming a tumor vascular normalization time window; vascular structure and function are normalized, resulting in a remission of hypoxia, and increase radiotherapy, chemotherapy, and immunotherapy efficacy.

Table 1 Summary of techniques with the advantages and limitations

Methods	Parameters	Agents	References	Advantages	Limitations
Perfusion CT/ Dynamic CT	BV, PE, TTP, SLOPE, ΔH, TBR, AUC, MTT, and PSAP	Iodine Iomeprol Iopromide Iopamidol	31, 32, 33, 35–38, 51	Fast speed of image acquisition Easily repeatable Widespread availability Morphological evaluation and physiological evaluation can be made in single scan	High ionizing radiation Lack of uniform standard
Spectral CT	IC	Iohexol	34	Provide more image information than conventional CT Provide material decomposed images with a single CT scan	High demands of clinical systems Low resolution Spectral variations of the X-ray beam may result in artifacts
DCE-MRI/MRA	BV, VD, K^{trans} , RSI, AUC, Vp, Ve, PS, peak, slope, $iAUC_{60}$, and ΔSO_2	Gadolinium Gadodiamide Gadoterate meglumine Gadobutrol	32, 42, 44–50, 52, 54–57	No ionizing radiation Daily or weekly repeats Without the depth limitations of optical techniques Achieve the same spatial resolution and higher contrast-to-noise ratio with a shorter imaging time Provide information of interstitial oxygen state Deoxyhemoglobin as a natural contrast agent No contrast agent	Cannot resolve vessels at the capillary level Lack of consensus Easily be affected by various methodological and technological issues Slow speed of image acquisition Indirectly reflects rather than directly displaying vascular changes
BOLD-MRI	R2* value	—	58		
ECT	BF, BV, HV, metabolism, and SUVmax	^{18}F -FMISO ^{18}F -FDG $[^{15}O]H_2O$ Arg-Gly-Asp	60, 62, 68, 72	Provide information about metabolism and function Display angiogenesis based on the expression and functional activity of proteins	Need to improve the stability, target affinity, and specificity Tracers' accumulation in tumors is slow, and tracers have short half-life of the isotopes and a considerable amount of radioactive metabolites
DCE-US	AUC, I_{pk} , T_{pk} , WIR, WOR, BV, σ_f , PI, MTT, VM, VT, PE, and RT	Microbubble	78, 79, 82, 84–87, 90, 91, 93–95	Easily repeatable without risk and with low cost Simultaneously display the morphology and function of blood vessels	Influenced by intestine gas Unable to accurately monitor the BF of abdominal and pelvic foci
Plasma/serum	PIGF, VEGF, sVEGFR-1, Ang2, sTie2, MMP-10, bFGF, sVEGFR2, SDF1 α , and collagen IV	—	39, 44, 54, 56, 100	More convenient Simultaneously predicts prognosis and recurrence Display changes in body metabolism and mechanisms	Has not yet formed a unified standard Different agents or types of tumors may have effects on serum proteins

Notes: σ_f , shape parameter; ΔH , density difference before and after tissue enhancement; $iAUC_{60}$, initial area under the curve for 60 seconds after injection; I_{pk} , peak intensity; K^{trans} , volume transfer constant between extracellular extravascular space and blood plasma; PS, vascular permeability; R2* value, transverse relaxation rate of water; ΔSO_2 , oxygen saturation levels and tissue oxygen consumption before and after treatment; SLOPE, slope of the time–density curve; SUVmax, standardized uptake values; T_{pk} , time-to-peak intensity; Ve, fractional extravascular volume; and Vp, fractional plasma volume.

Abbreviations: AUC, area under the contrast enhancement curve; BF, blood flow; BOLD-MRI, blood oxygenation level-dependent MRI; BV, blood volume; DCE-MRI, dynamic contrast-enhanced magnetic resonance imaging; DCE-US, dynamic contrast-enhanced ultrasonography; ECT, emission computed tomography; HV, hypoxic volume; IC, iodine concentration; MRA, magnetic resonance angiography; MTT, mean transit time; PE, peak enhancement; PI, peak intensity; PSAP, permeability surface-area product; ROI, region of interest; RSI, relative signal intensity; RT, retention time; soluble vascular endothelial growth factor receptor 2; TBR, tissue–blood ratio; TTP, time to peak enhancement; VD, vessel diameter; VM, vascular morphology; VT, vascular tortuous; WIR, wash-in rate; WOR, wash-out rate.

normalization, were positively correlated with microvessel density (MVD) in gastric adenocarcinoma.³² BV and peak enhancement index (PEI) were positively correlated with MVD in lung tumor measured by pathology and CT.³¹ Iodine concentration (IC) was widely used in clinical diagnosis of vascular imaging and various diseases; quantitative IC value detected by spectral CT correlated with the MVD and reflected angiogenesis in advanced gastric cancer.³³

With the development of functional imaging, tumor vessel assessment by contrast-enhanced CT makes the detection more comprehensive; the contrast agent provides indirect evidence for morphological and hemodynamic indices and extravasation in different tumor regions.^{7,34} Studies have revealed that the peak enhancement (PE) of the tumor and the enhancement ratio measured by dynamic multidetector CT correlate positively with the extent of angiogenesis, and dynamic-enhanced CT images may reflect the heterogeneity of tumor angiogenesis in view of the correlation between enhancement parameters and MVD.^{35–37} BV and permeability surface-area product (PSAP, measures of capillary leakage and functional vascular density) other than BF and transit time evaluated by multidetector CT correlated positively with MVD; however, there was no significant correlation between the imaging vascular parameters and the histological parameters pericyte coverage, vascular endothelial growth factor (VEGF) expression, and GLUT-1 expression.³⁸

An open-label Phase II study evaluated dynamic CT-based vascular parameters in patients with advanced non-small-cell lung cancer, and results showed that BF, BV, and permeability-surface area were significantly decreased after the induction dose of bevacizumab, but the change in mean transit time was more heterogeneous between patients.³⁹ Dynamic contrast-enhanced CT (DCE-CT) is a noninvasive technique to image vascular and interstitial tumor characteristics, which are used to observe tumor neo-angiogenesis and other vascular parameters. Early activity of cetuximab induced changes in tumor vascular, and interstitial characteristics were detected by DCE-CT.⁴⁰ More research is needed to verify the relationship between vascularization parameters and vascular normalization.

The ability of CT to detect tumor perfusion, vessel morphology, and response to anti-angiogenic therapy has been clinically validated; however, CT perfusion imaging is influenced by many factors, such as scanning solutions, image analysis software, and personal bias; thus, the sensitivity and reliability of perfusion CT need to be verified. At present, the normalization of tumor blood vessels by CT has not been clinically confirmed, and more data are needed to support this.

Magnetic resonance imaging (MRI)

MRI is a versatile tool to noninvasively evaluate changes in tumor angiogenesis over time. MRI can be performed repeatedly to measure morphology and function of the target dynamically in the short term;⁴¹ therefore, it is an ideal platform for assessing changes in blood vessels.⁴² Dynamic contrast-enhanced MRI (DCE-MRI) is a functional imaging, which has been used in clinical trials to assess the role of anti-angiogenic agents.⁴³

The MRI parameter K_{trans} is a key factor displaying volume transfer coefficient of the contrast agent between plasma and extravascular space. K_{trans} is used for characterizing vascular function and influenced by flow, permeability, or both.^{44–47} Changes in vascular heterogeneity quantified by K_{trans} distribution have been shown in patients with primary rectal cancer and breast cancer.^{48–50} Tumor blood perfusion, which is another predictor of normalization, can also be detected using DCE-MRI by pharmacokinetic behavior of gadolinium (Gd)-based contrast agents.⁵¹ Patients with an increase in tumor perfusion measured by MRI showed significantly higher vascular normalization index (three parameters: K_{trans} , microvessel volume, and plasma collagen IV) compared with patients with stable or decreased perfusion.^{44,45} This result offers direct clinical evidence in support of the hypothesis that vascular normalization benefits outcomes, and the vascular normalization index is a potential indicator for progression-free survival and overall survival.⁵² Advanced MRI showed that treatment with cediranib increased tumor blood perfusion in some patients with recurrent glioblastoma undergoing VEGF treatment, and these patients survived longer than patients whose tumor blood perfusion did not increase.⁴⁵ In patients with breast cancer, doxorubicin/cyclophosphamide plus sunitinib induced functional changes in tumor vasculature. The DCE-MRI functional parameters, including K_{trans} , Vp (fractional plasma volume), Ve (fractional extravascular volume), and PS (vascular permeability), were significantly increased after one cycle of combined treatment except for perfusion and the increase in K_{trans} with good histological response compared with decline subset.⁵³

In another prospective study, physiological MRI showed vascular integrity, and perfusion improved in patients with newly diagnosed glioblastoma who underwent cediranib plus chemoradiation therapy compared with those who underwent conventional chemoradiation alone.⁵⁴ The relative difference in the oxygen saturation levels – one of the indicators of tumor blood vessel normalization as measured by MRI – was linked with increased perfusion. T1- and T2-weighted MRI with the cerebra BV from the DSC-MRI modality to study

tumor perfusion in glioblastoma showing parameter variations predict tumor perfusion normalization.⁵⁵ An intuitive description of the tumor vascular normalization by MRI in clinical practice demonstrates that relative tumor vascular size decreased in 1 day after cediranib treatment, and it remained decreased at day 28. At day 56, the relative vessel size reversed toward abnormal, suggesting the beginning of the closure of the vascular structural normalization window; at the same time, MRI detected a reduction in vascular permeability (as measured by the transfer constant K_{trans} of Gd) at days 1 and 28, and vascular permeability remained decreased until day 112, indicating that vascular function normalized.⁵⁶ One study determined the appropriate time of chemotherapy administration after bevacizumab therapy in metastatic brain tumors in patients with breast cancer. The result showed reductions in the mean percentage change in MRI parameters peak, slope, $iAUC_{60}$, and K_{trans} at 1 hour and 24 hours, and the reductions in all parameters were significantly higher at 24 hours than at 1 hour, which suggested that the appropriate time frame of vascular normalization of bevacizumab was 24 hours.⁵⁷

Another hallmark of tumor vascular normalization is the alleviation of hypoxia in tumor tissue, and this change could be detected by MRI. Blood oxygenation level-dependent MRI (BOLD-MRI) is a functional MRI technique using the paramagnetic properties of deoxyhemoglobin, which can be seen as a natural contrast agent to map the local oxygen concentration. $R2^*$ values positively correlated with the level of CA IX, and HIF-1 α demonstrates BOLD-MRI as a reliable predictor to reflect oxygen content.^{58,59} Using MRI to accurately monitor the changes in tumor tissue oxygen content can indirectly reflect the changes in vascular function.⁶⁰

Overall, MRI provides a very comprehensive and versatile platform to analyze the morphology and function of vascular normalization. However, the quality of a DCE-MRI vascular normalized study can easily be affected by various methodological and technological issues, such as treatment schedule, contrast medium, analysis performed, and types of tumors; therefore, further research and a unified standard need to be developed.

Emission computed tomography (ECT)

ECT is a computer imaging method that includes positron emission tomography (PET) and single-photon emission computed tomography (SPECT). PET is a molecular imaging technology that provides information about function and metabolism, including biomolecule metabolism, cell proliferation, receptors, and nerve mediators in vivo.⁶¹ This

technique is based on the high glucose metabolism in malignancies that have more accumulation of tracers labeled with radionuclides (such as ^{18}F , ^{15}O , and ^{11}C). SPECT is a nuclear medicine tomographic imaging technique that uses gamma rays; it can be freely reformatted or manipulate images as required to provide true three-dimensional (3D) information.

PET with [^{15}O]H₂O/[^{18}F] fluorodeoxyglucose (FDG) was used to analyze tumor BF and metabolism response to different doses of endostatin in clinical practice and display a biphasic concentration–BF curve.⁶² Using [^{15}O]H₂O/[^{18}F] FLT PET imaging demonstrated that transient antiangiogenic treatment improves tumor BF corresponding to a transient tumor vessel normalization time window, which improved delivery of erlotinib into the tumor.⁶³ Perfusion and metabolism changes after anti-angiogenesis treatment can be detected by dynamic [^{18}F]-FDG PET, and the time frame of potential tumor vasculature renormalization was monitored to allow optimal timing of follow-up treatment.⁶⁴ In preclinical studies, ^{18}F -fluoromisonidazole (^{18}F -FMISO) accumulation levels in renal cell carcinoma were significantly increased compared with the control group after sorafenib treatments, and this increase was dose-dependent, which is consistent with decreasing microvessels.⁶⁵

Like BOLD-MRI, ^{18}F -FMISO PET provides information of changes in interstitial oxygen state, a surrogate parameter of vascular normalization, and might help track the normalization time window.^{7,60,66–70} In addition, PET has the potential to display angiogenesis on a molecular level based on the expression and functional activity of proteins.⁷¹ One study used PET and ^{68}Ga -NODAGA-c(RGDfK) imaging $\alpha v\beta 3$ integrin – one of the most extensively examined targets of angiogenesis – to monitor tumor angiogenesis after bevacizumab treatment of squamous cell carcinoma xenografts. The result showed that ^{68}Ga -NODAGA-c(RGDfK) uptake was significantly increased at day 7 of treatment and maintained until 3 weeks, accompanied with a transient normalization of blood vessel morphology and reduction of MVD and $\alpha v\beta 3$ integrin expression.⁷¹ Arg-Gly-Asp (RGD) peptides have a high affinity and selectivity for $\alpha v\beta 3$; RGD-based PET tracers can measure the changes in neovascular density and integrin expression during antiangiogenic therapy.^{72–74} Similarly, PET also accurately traced vascular normalization and improved interstitial chemotherapy delivery; when [^{18}F]-FMISO-PET signal decreased, the tissue hypoxia reduction and the vascular structures are normalized; thus, it could be a potential biomarker in anti-angiogenic therapy.^{66,67}

Using (99m)Tc-RGD on SPECT/CT to evaluate the tumor vessels determined the optimal dose regimen for

bevacizumab and radiotherapy alone. Scintigraphic imaging showed a significantly increased RGD tumor uptake 2 hours after bevacizumab treatment compared with those 24 hours after bevacizumab treatment and controls, which identified the vascular normalization window and showed the effect of bevacizumab when administered 2 hours before radiotherapy.⁷⁵ $^{99m}\text{Tc}-(\text{CO})_3$ His-Annexin A5 SPECT probes a significant antitumor efficacy of irinotecan during normalization of tumor blood vessels caused by bevacizumab.⁷⁶

PET has been clinically used to detect the lesions of tumor metastasis and guide the staging and treatment program of the tumor. However, it failed to gain wider acceptance for routine clinical application for detecting tumor vasculature because of several limitations, for instance, the tracers' accumulation in hypoxic tumors is slow, tracers have short half-life of the isotopes,⁶⁴ and a considerable amount of radioactive metabolites.⁷⁷ Data regarding SPECT in the clinical setting in response to antiangiogenic treatment are scarce. As a new advanced versatile detection platform, a large amount of clinical data and preclinical studies need to be collected and analyzed comprehensively to evaluate its value in detecting tumor vascular normalization.

Dynamic contrast-enhanced ultrasonography (DCE-US)

DCE-US is a functional technique using Doppler ultrasound with contrast medium and perfusion software, using a mathematical model to quantitatively evaluate BF and vascular morphological characteristics.^{78–80} For example, DCE-US has been introduced to improve the diagnosis of thyroid nodules, given the abundant vasculature of the thyroid gland.⁸¹ In solid tumors, changes in tumor vascularization can be detected earlier than changes in tumor volume, and DCE-US has been proposed as an alternative method to evaluate vascular response to anti-angiogenic therapy and targeted therapy.^{82–87}

Microvascular morphology can be delineated by contrast-enhanced ultrasound angiography (CEUA). Cannula centerlines extracted from ultrasound images can be more conveniently acquired vascular morphology parameters, such as vascular length, density, bifurcations, junction points, and other topologic features,⁸⁸ thus CEUA provides a quantitative basis for distinguishing malignant from normal tissue due to vascular heterogeneity.⁸⁹ 3D contrast-enhanced ultrasonography could identify benign and malignant breast tumors and correlates with MVD and VEGF expression.⁹⁰ Combined analysis of quantitative vasculature, vascular morphology, and tortuosity by 3D power Doppler ultrasound can potentially serve as imaging biomarkers to predict the

early response to anti-angiogenesis therapy.⁹¹ DCE-US-based vascular morphology parameters exhibit a marked reduction in tumor vessels, bifurcations, and tortuosity, which are manifestations of tumor blood vessel normalization.⁷⁸

DCE-US imaging was used to estimate tissue perfusion, which is another index for tumor vascular normalization. Microbubble contrast agents (MCAs) will disintegrate and dissolve under ultrasound. The MCA reperfusion rate into the microvasculature will reflect BF. This technique has been used to map BF rate in many organs and tumors.⁹² DCE-US could detect considerable changes in intratumoral BV through the functional parameters of area under the curve and peak intensity (PI), BF rate by time-to-peak intensity, wash-in rate (WIR), and wash-out rate (WOR), all of which may prove useful in determining tumor response to anti-angiogenesis or chemotherapy.⁷⁸ An earlier study used dynamic US to quantify dynamic changes in tumor blood vessels' early response to bevacizumab treatment in patients with hepatocellular carcinoma, although there is no direct description of the alleviation in hypoxia and interstitial pressure due to the vascular normalization; however, the total area under the time–intensity curve that corresponds to BV and is probably the best indicator of tissue necrosis.⁹³ A clinical trial enrolled 539 patients in which DCE-US was carried out at baseline and 7 days after anti-angiogenic treatment. The trial identified the mean transit time of at least 12 seconds was the only criterion that correlated with freedom from progression of patients treated with bevacizumab at day 7, and this criterion might be linked to vascular normalization.⁹⁴ The hemodynamics of liver metastasis in patients with colorectal cancer who received anti-angiogenesis therapy was quantitatively evaluated by DCE-US. Dynamic monitoring showed that retention time (RT) increased continuously in the bevacizumab-sensitive tumors and transient reduction in bevacizumab-resistant tumor vessels. This heterogeneity might be related to the normalization of vasculature.⁹⁵ A recent study provided direct evidence by 3D power Doppler ultrasound that the possible timing of the normalization window was 20–24 hours after the administration of bevacizumab in human breast cancer.⁹⁶

In conclusion, tumor vascular parameters could be analyzed using various techniques. Among them, DCE-US has been proven to be safe, easily repeatable, low cost, and with reproducible results, which make it a feasible tool that can be relatively easy to implement to monitor tumor vascular normalization; however, the detection is influenced by intestine gas and is limited in its accuracy to monitor the BF of abdominal and pelvic tumors. Furthermore, in some tumors, the guidelines for evaluating the quality of results need to be established.

Plasma or serum marker

Since various proteins released by tumors are identified in the plasma or serum, blood is an ideal biological sample to predict disease progression, and blood proteomics have gained considerable interest in identification of novel reliable disease biomarkers.

Soluble vascular endothelial growth factor receptor-1 (sVEGFR-1) is an endogenous antagonist of VEGF and placenta growth factor (PlGF) and is related to tumor vascular normalization. The plasma sVEGFR-1 correlates with antitumor and systemic efficacy of bevacizumab-based chemoradiation.⁹⁷ A transient decrease in plasma sVEGFR1 was measured at day 7 after the induction of bevacizumab,³⁹ which can be used as a candidate biomarker for predicting normalization of tumor blood vessels. Angiopoietin-1/2 (Ang1/2) plays a dynamic role in vessel formation, permeability, maturation, and maintenance.⁹⁸ Serum Ang2 is emerging as an endothelium activation marker in certain diseases, such as acute lung injury, hypertension-related myocardial infarction, sepsis, and many cancers,⁹⁹ and it has been reported to be overexpressed in tumors after anti-angiogenic therapies;⁹⁸ however, cediranib treatment induced transient decreases in Ang2 in plasma.¹⁰⁰ In tumor tissue, the Ang1/Ang2 ratio correlated with the degree of vascular normalization and with the survival of patients with glioblastoma.¹⁰¹ Cediranib treatment led to transient normalization of the vasculature and was associated with a transient increase in plasma collagen IV at day 2, which reflects basement membrane thinning.¹⁰² In clinical practice, circulating collagen IV level is one of the parameters to identify the tumor vascular normalization index with MRI.⁴⁴

Apelin/APJ signaling regulates pathological angiogenesis, and the secretion level of apelin was increased under hypoxic environment, which was mediated by HIF-1 α ;^{103,104} furthermore, apelin expression is upregulated in the process of new vascular formation but downregulated following vascular stabilization.^{105,106} A preclinical study found that apelin expression both in tumor tissue and in plasma would be transiently decreased during the vessel normalization window induced by bevacizumab and restored with the regression of vascular normalization.¹⁰⁷ Considering the relationship between hypoxia and apelin, this change is thought to be due to a temporary alleviation of hypoxia in the time window; however, the clinical usefulness of apelin to identify the tumor vascular normalization needs to be analyzed.

In addition, a series of factors, genes, or cells that exist in both blood and tumor tissue have been demonstrated as a remarkable marker in tumor tissue. Type 1 T helper (T_H1) cells are associated with vessel normalization by secreting

interferon- γ , and there is a positive feedback loop between T_H1 and vascular normalization, accompanied with a decrease in the expression of *Angpt2* and other *VEGF*-signature genes.¹⁰⁸ Moreover, Tian et al¹⁰⁸ identified that various angiogenesis-related genes positively or negatively correlate with survival, and they defined these genes as good- and poor-prognosis angiogenesis genes (GPAGs and PPAGs). The inversion of GPAGs and PPAGs correlates with “invasive vasculature”, and thus, these genes can be used as vessel normalization indicators.

Easy accessibility and sensitivity to changes in tumor vasculature make plasma and serum as promising markers for monitoring tumor vascular normalization during anti-angiogenic treatment. These markers suggest that potential combination regimens improve the effectiveness of chemotherapy drugs, and some of them may be applicable to other tumor types and warrant further testing.

Conclusion and outlook

Preclinical or clinical studies have shown that normalization of tumor blood vessels can improve the comprehensive therapy efficacy, including radiotherapy, chemotherapy, and immunotherapy. To ensure drug administration precisely within normalized time window, it is necessary to monitor the time window accurately; however, how to conduct effective clinical monitoring of vascular normalization time window is a key constraint. Although PET, MRI, and CT perfusion imaging have been used to evaluate the therapeutic efficacy of anti-angiogenesis therapy, no consensus has yet been reached. To date, no single method has been validated for detecting the complex process of normalization. At present, MRI and ultrasound are the most reported in the clinical literature, and their reliability and stability deserve more observation. PET and CT as the platform for the observation method have been widely used. Recently, we and other researchers have been gradually looking for serum or plasma markers of interest in monitoring, combining imaging methods to establish a more effective evaluation system that deserves further study.

Disclosure

The authors report no conflicts of interest in this work.

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