Contents lists available at ScienceDirect

HardwareX

journal homepage: www.elsevier.com/locate/ohx

Open source timed pressure control hardware and software for delivery of air mediated distensions in animal models

Trishna Patel^{a,b}, Jamie Hendren^a, Nathan Lee^a, Aaron D. Mickle^{a,b,c,*}

^a Department of Physiological Sciences, College of Veterinary Medicine, University of Florida, Gainesville, FL, United States

^b Department of Biomedical Engineering, Herbert Wertheim College of Engineering, University of Florida, Gainesville, FL, United States

^c Deparment of Neuroscience, College of Medicine, University Florida, Gainesville, FL, United States

A R T I C L E I N F O

Article history: Received 15 March 2021 Received in revised form 20 January 2022 Accepted 27 January 2022

Keywords: Visceromotor response Visceral pain Arduino Solenoid

ABSTRACT

Studying the visceral sensory component of peripheral nervous systems can be challenging due to limited options for consistent and controlled stimulation. One method for mechanical stimulation of hollow organs, including the colon and bladder, is controlled distensions mediated by compressed air. For example, distension of the bladder can be used as an assay for bladder nociception. Bladder distension causes a corresponding increase in abdominal electromyography, which increases with distension pressure and is attenuated with analgesics. However, the hardware used to control these distensions are primarily all one-off custom builds, without clear directions on how to build your own. This has made it difficult for these methods to be fully utilized and replicated as not everyone has the access, knowledge, and resources required to build this controller. Here we show an open-source Arduino-based system for controlling a solenoid valve to deliver timed pressure distensions in the experimental model. This device can be controlled by one of two methods through direct TTL pulses from the experimenter's data acquisition software (ex. CED Spike2) or by a graphical user interface, where the user can set the time before, during, and after distension as well as the number of cycles. This system's low cost and relative ease to build will allow more groups to utilize timed pressure distensions in their experiments.

© 2022 The Author(s). Published by Elsevier Ltd. This is an open access article under the CC BY-NC-ND license (http://creativecommons.org/licenses/by-nc-nd/4.0/).

Specifications table:

| Hardware name | Timed Distension Controller | | |
|------------------------|--|--|--|
| Subject area | Neuroscience | | |
| | • General | | |
| Hardware type | Electrical engineering and computer science | | |
| Open Source License | CC-BY-SA 4.0 | | |
| Cost of Hardware | \sim \$215 + \$180 for peripheral components for complete system | | |
| Source File Repository | https://doi.org/10.17605/OSF.IO/RS5P4 | | |

* Corresponding author at: Department of Physiological Sciences, College of Veterinary Medicine, University of Florida, Gainesville, FL, United States. *E-mail address:* amickle@ufl.edu (A.D. Mickle).

https://doi.org/10.1016/j.ohx.2022.e00271

2468-0672/© 2022 The Author(s). Published by Elsevier Ltd. This is an open access article under the CC BY-NC-ND license (http://creativecommons.org/licenses/by-nc-nd/4.0/).







1. Hardware in context

Normally we have very little perception of our bladder, intestine, and stomach as they function to extract nutrients and remove the body's waste. However, for greater than 20% of the world's population, discomfort and/or pain accompany these normal physiological activities [1]. Unfortunately, the mechanisms surrounding these diseases, like irritable bowel syndrome, interstitial cystitis, and bladder pain syndrome, have yet to be elucidated. One tool neuroscientists use to assess the sensory function of visceral structures is hollow organ distension which is a validated and widely used technique in both animal models [2–5] and human studies [6–8]. Graded distension directly with air or via a balloon can provide organ-specific stimuli critical for studying these structures under normal and disease conditions.

These experimental distensions are typically controlled either by the manual opening of a valve or via an electronic control system [7,9]. Using an electronic control system has a number of advantages, including consistent timing of distention series, almost immediate on and off times, as well as alignment with other stimuli or experimental interventions. However, the use of these control systems has been limited as the devices described in the literature are all custom built with no published designs and usually custom made by various university machine shops. There are two methods for controlling the timed pressure controller published by Andersen, Ness, and Gebhart (1987) [9]. Building this system requires expertise and skill with electronics normally not found in neuroscience or biology labs. Outsourcing the build increases the cost and thus limits the number of groups who can build their own controller. With the increased availability and decreased cost of off-the-shelf microcontroller boards, like the Arduino Uno, there are now simpler and cheaper ways of building and using a time-distension controller.

The second was a recently published visceral pain stimulator [10]. This device takes advantage of new microprocessors and microcontrollers to increase the flexibility and accessibility of previously published devices. There are several similarities between the visceral pain stimulator and the timed pressure controller we described here. 1) They both use modern microcontrollers to offer flexibility and reduced cost compared to older systems. 2) Both have open-source software to control the duration and frequency of distension. 3) They send digital signals to data acquisition systems so that measured physiologic responses can be time-locked to stimulation.

Each device also offers some advantages over the other. The visceral pain stimulator sends a digital pressure reading to the data acquisition system. Similar data can be collected with our system, but it requires an external pressure sensor and amplifier. As a result, our device has the advantage of a more simplified design resulting in a slightly cheaper raw material cost (~\$200 here compared to ~\$500; estimated from the published parts list [10]). Further, our system can be controlled directly with experimental software/hardware that many labs already use (Spike 2, LabView, etc.), allowing for coordination with other types of stimulation physiologic recordings. The visceral pain stimulator has the flexibility to be programmed for this type of control, but this is not currently available. Finally, our device has detailed build instructions that someone with little electronics background can complete.

Here we describe an easy to build, low-cost timed distension control device and peripheral components needed to fully use the system to study visceral sensory systems on rodents. This system can be assembled with limited tools and technical knowledge. This system will make it easier to utilize controlled distension stimulation in labs that study visceral organ physiology. We have designed two different ways to operate the Arduino-controlled solenoid. The first is a standalone user interface that uses Python's open-source programming language to control distention (variables duration, time between distensions, and the number of trials). The second mode of operation uses transistor-transistor logic (TTL) to control the solenoid with other lab software/hardware, which allows precise coordination of distension with commonly used lab equipment and other experimental interventions.

2. Hardware description

Our timed distension controller uses an Arduino microcontroller to control a relay module that opens and closes a solenoid valve. The electronics and solenoid are contained within a 3D printed case with a removable lid (Fig. 1). Opening the solenoid allows pressurized air to flow to the target/animal and distend the hollow organ or balloon (Fig. 2). The pressure of distension is controlled by a flowmeter regulator and is changed manually for different distension pressures (Fig. 2). The timing of the distension can be controlled using the Python-based user interface (Fig. 3), or if precise coordination with other software/stimuli is needed, it can be triggered using a TTL pulse. Three LEDs on the outside of the case illuminate during each stage of the distension; yellow in the pre-distension time period, red during distension, and blue during the postdistension time.

The primary advantages of using the system described here over other systems are the availability, cost, and ability to control distention with a TTL interface. The only other published system is more than 30 years old and would be challenging for a non-electrical engineer to reproduce [9]. Newer systems have been used, but the designs have not been published [11,12]. If you can find someone to build one of these previously used systems, the cost is significantly higher than this system, with quotes in the \$2000 to \$3000 range. In some previously described timed distension control devices, the stimulus is timed with direct inputs [11,12], and in others, it can be triggered by TTL input [13–15]. For this device, we have the option of either direct input control or triggering valve opening with TTL pulses for controlling distension with other software and/or to coordinate with other experimental interventions.



Fig. 1. Timed Distension Controller and User Interface. The timed distension controller uses an Arduino microcontroller to control a relay module that opens and closes a solenoid valve. We have designed a 3D printable box to mount the electronics and solenoid. Three LEDs indicate what distension phase the device is in, closed before valve opening (yellow), time open (red), and time closed (blue) (A). There are two connectors on the left side of the box for sending TTL pulses to the timed pressure controller and from the devices to a data acquisition system (**B**). On the right side of the box, there are cutouts for the Arduino USB and power adaptors. Additionally, there is a power adaptor for the solenoid (**C**). Inside the 3D-printed box, the main components are the Arduino Uno, relay board, and solenoid controlling air release to the animal (**D**). (For interpretation of the references to colour in this figure legend, the reader is referred to the web version of this article.)

- This device is easy to build, and with basic soldering skills, any lab should be able to build its own.
- This device is cost-effective, with all the components costing around ~\$200 compared to ~\$2000–3000 obtained quotes to build something similar by a university machine shop core, where the plans are not publicly available.
- The design and components are easily accessible and can be modified to fit specific experimental needs.
- Operation modes are flexible for multiple applications with or without additional equipment.

3. Design files

3.1. Design files summary

| Design file name | File type | Open source license | Location of the file | | |
|---|---|--|--|--|--|
| Wiring Diagram TPC-Case TPC-Case TPC-Lid TPC-Lid TCP_GUIv1.2 TPC_TTL_Trigggring | .PDF .STEP .STL .STEP .STL .PY | CC-BY-SA 4.0 CC-BY-SA 4.0 CC-BY-SA 4.0 CC-BY-SA 4.0 CC-BY-SA 4.0 CC-BY-SA 4.0 CC-BY-SA 4.0 | https://10.17605/OSF.IO/RS5P4 https://10.17605/OSF.IO/RS5P4 https://10.17605/OSF.IO/RS5P4 https://10.17605/OSF.IO/RS5P4 https://10.17605/OSF.IO/RS5P4 https://10.17605/OSF.IO/RS5P4 | | |
| Air Flow Diagram | .PDF | CC-BY-SA 4.0 | https://10.17605/OSF.IO/RS5P4 | | |



Fig. 2. Complete Assembly and Flow Diagram. (**A**) A labeled picture of the whole working system with the timed pressure controller. (**B**) This experimental diagram demonstrates how the timed distension controller fits in the entire distension workflow from the compressed air tank to the animal. Blueline indicates the path the compressed air takes.



Fig. 3. User Interface for Timed Distension Controller. A screenshot of the user interface shows the input parameters, time closed before stimulus (predistension time), time open (stimulus time), time off (post-distension time), and cycles (the number of times it is repeated).

3.2. Description of each file

- Wiring Diagram PDF file with a wiring diagram to aid in the assembly of the device.
- 3D Case and Lid Files The STL files for 3D printing the timed distension controller case. The CAD file (.STEP format) has also been included if you want to make modifications.
- TCP_GUI_v1.2- Python code for the user interface to control the timed pressure controller.
- TCP_TTL_Triggering Arduino code for the timed pressure controller TTL mode of operation.

4. Bill of materials

Please see attached editable spreadsheet file with links.

| Designator | Component | Number | Cost per unit - currency | Total cost - currency | Source of materials | Material type |
|--|----------------------|--------|--------------------------------|-----------------------------|-----------------------------------|---------------------------------|
| Arduino Uno | DEV-11021 | 1 | \$22.95 | \$22.95 | Sparkfun | Other |
| 2-Channel 5 V Relay Module | 101-70-100 | 1 | \$5.99 | \$5.99 | SainSmart | Other |
| Solenoid Valve | 61245 K84 | 1 | \$143.49 | \$143.49 | McMaster Carr | Other |
| M3 Screws | | 9 | \$0.03 | \$0.27 | Amazon | Stainless Steel |
| USB 2.0 A-Male to B-Male Cord | 7HUA | 1 | \$8.74 | \$8.74 | Amazon | Other |
| 1 N5819 Diode | COM-10926 | 1 | \$0.15 | \$0.15 | Sparkfun | Other |
| 8-32 7/16" Phillips Flat Head Screws | 91500A319 | 2 | \$0.16 | \$0.32 | McMaster Carr | 316 Stainless Steel |
| Hook-Up Wire (Solid Core, 22 AWG) | PRT-11367 | 1 | \$16.95 | Small amount | SparkFun | Other |
| Resistor $- 1/4W$ | COM-10969 | 3 | \$0.02 | \$0.06 | SparkFun | Other |
| Barbed Hose Fitting $3/16$ in $\times 1/8$ in | 6AFP5 | 2 | \$4.62 | \$9.24 | Grainger | Brass |
| Male/Male Jumper Wires | 758 | 3 | \$0.10 | \$0.30 | Adafuit | Other |
| Diffused 5 mm LED | 4203 | 3 | \$0.20 | \$0.60 | Adafruit | Other |
| 5 mm Chromed Metal Narrow Bevel LED Holder | 2176 | 3 | \$0.59 | \$1.77 | Adafruit | Chromed Metal and Plastic |
| DC Power Cord | AFP2FA_A5 | 1 | \$7.99 | \$7 99 | Amazon | Other |
| Plumbers Tane | 21TF19 | 5 | \$7.33 \$0.002/in | \$0.01 | Crainger | PTFF |
| Pre-Cut Multi-Colored Heat Shrink Pack Kit – 280 pcs | 4559 | 18 | \$0.03 | \$0.54 | Adafruit | Plastic |
| RF/Coaxial Connector | 523-31-10- RFXG1 | 2 | \$2.57 | \$5.14 | Mouser | Nickel Plated Brass |
| 5.5mmx2.1 mm 2 Pins DC Power Jack Female Panel Mounting Connector Socket | B01N8VV78D | 1 | \$0.58 | \$0.58 | Amazon | Metal and Plastic |
| 3D Printed Case - PLA | PRM-PLA- GLX-1000 | 1 | \$24.99/kg | \$5.74 | Prusa Research | PLA |
| 3D Printed Lid -PLA | PRM-PLA- GLX-1000 | 1 | \$24.99/kg | \$1.76 | Prusa Research | PLA |
| | | | Total | \$215.64 | | |
| Associated Peripherals Tubing, 3/16 in Inside Dia., 3/8 in | 742 T67 | 4 | \$1.47/ft | \$5.88 | Grainger | PVC |
| Outside Dia. | | | | | | |
| Prestige Medical -Model 79-G | B073G97XSP | 2 | \$15.75 | \$31.50 | Amazon | Other |
| Masterflex Variable-Area Flowmeter Regulator | EW-03216– 28 | 1 | \$138.00 | \$138.00 | Cole Parmer | Other |
| Tubing, 3/32 in Inside Dia., 5/32 in Outside Dia. | 22XH31 | 4 | \$0.35/ft | \$1.40 | Grainger | PVC |
| Assorted Tubing connectors | B08D8PVHCG | 5 | \$0.15 | \$0.75 | Amazon | Plastic |
| Elite 2-Way Air Control Valve | B0002AQIAY | 1 | \$3.49 Total | \$3.49 \$181.02 | Amazon | Plastic |
| Optional | | | | | | |
| Blood Pressure Transducer and Cable | BLPR2 | 1 | \$184.00 | \$184.00 | World Precision Instruments | Other |

Additional notes on component Selection:

The electrical air directional control solenoid valve was chosen because it operates on 12 V, is normally closed, can operate at low pressure (0 PSI) and has a vent to release air pressure from the OUT tubing allowing the distension to quickly end after the value closes. When we originally purchased the valve, it was cheaper than the listed price on the bill of materials. There may be other more cost-effective options now available.

Additional parts from this list could be designed and 3D printed to reduce cost and waste of having to buy more parts than you need, this includes all the tubing connectors and the LED holders. Versions of these parts can be found on many 3D printing repositories, which could be modified for this use case. Our lab these parts already for other builds, which eliminated the need to design and print these parts.

Tools needed that are not included on the bill of materials list:

- Soldering iron, Teflon tape, crescent wrench, screwdrivers, scissors, wire strippers, and heat gun.
- 3D printer Parts could be ordered from a commercial 3D part printer
 - o All parts were printed on a Prusa MK3s, STL file was prepared for printing using Prusa Slicer 2.3, the standard 0.30 mm Draft setting was used (with a layer height of 0.3 mm, infill density of 20%, a print temperature of 210 °C, and a bed temperature of 60 °C).

5. Build instructions

5.1. Assembly of timed distension controller hardware

All circuit components are detailed in the bill of materials. Use the wiring diagram to aid (Fig. 4) in the wiring and assembly of the timed distension controller. Print the case and lid prior to starting assembly.

- 1. Attach Arduino Uno and relay module to case mounts using 6 mm M3 screws (Fig. 5a).
- 2. Prepare solenoid before mounting in case (Fig. 5b).
 - a. Wrap both barbed hose fittings in the plumber's Teflon tape.
 - b. Screw-in each barbed hose fitting onto solenoid outlets.
 - c. Attach 3/16 in. inner diameter tubing onto the barbed portion of each fitting.
- 3. Mount solenoid to the case.
 - a. Feed tubes through case openings. The tube on the wiring side should go through the round opening and the other tube through the rectangular opening. There is also a flow arrow on the solenoid. The "in tube" should enter through the smaller hole on the case, and the exit tube will go out the larger rectangular hole. It is important to mount the solenoid in the correct direction as the OUT side of the value has a value to release air when the solenoid is closed. This will dissipate distension when the stimulus is removed.
 - b. Line up solenoid over mounting holes.
 - c. Holding the solenoid in place with one hand, flip the case over and insert an 8–32 screw into each hole, and tighten the screws to attach the solenoid.



Fig. 4. Times Distension Controller Wiring Diagram. A wiring diagram to aid in the assembly of the device.



Fig. 5. Assembly Photos of Timed Distension Controller Hardware. The timed distension controller hardware consists of an Arduino Uno microcontroller and a 2-channel relay wired together, and a solenoid mounted to the base of a 3D printed case (**A**, **B**, **and C**). The hardware also includes mounted RF/coaxial connectors and LEDs, all wired to the Arduino (**D**, **E**, **F**, **G**, **and H**). Lastly, there is a DC power and diode connected to the two solenoid wires, the output of which are then plugged into the relay module (**I**, **J**, **and K**). Labels are added to the outside of the box to distinguish the two RF/coaxial connectors based on their Arduino wiring (**L**).

- 4. Insert the LED holders, threaded side first, into each of the three LED holes (three uniform holes on the long side of the case). Secure the LED holder in its designated hole with its washer.
- 5. Wire together Arduino and relay module using male-to-male jumper wires.
 - a. Connect relay GND to Arduino GND, relay IN1 to Arduino 13, and relay VCC to Arduino 5 V (Fig. 5c).
 - b. Use a jumper to connect VSS to JD-VCC on the relay module to power the relay with the Arduino.
- 6. Prepare RF/coaxial connector for mounting (Fig. 5d).
 - a. Cut one 3-inch segment and one 5-inch segment of the solid core wire and strip ~ 1 cm off each end of both wires. Choose two different colors to aid in identifying the different pin outputs after the RF connector is prepared.
 - b. Solder the 3-inch wire to the ground (flat) pin on the connector and the 5-inch wire to the positive (roundcenter) pin. Black wire was used for ground and red for positive in the images.
 - c. Cover soldered connection and any exposed portion of the pins with heat shrink, using the smallest size that will fit over the solder. Apply hot air to secure the heat shrink. Heat shrink is used to prevent any exposed metal/wire/solder from touching and to support any brittle soldering connections.
 - d. Repeat steps 6a-c with a second RF connector.
- 7. Mount and install RF/coaxial connectors.
 - a. Insert RF/coaxial connectors into the two slots on the short side of the case, feeding the wires in first. Secure using the associated washer.
 - b. Insert positive wire for the right RF/coaxial connector into Arduino pin 2 and the positive wire for the left RF connector into Arduino pin A0.
 - c. Twist the ground wires for the RF/coaxial connector together. Cut another 3-inch segment of the solid core wire and strip \sim 1 cm from each end. Twist this 3rd wire around the other 2 (Fig. 5e). Solder this connection together, and cover with heat shrink, applying hot air to secure. The end of this wire should then be connected to an Arduino GND pin (Fig. 5f).

- 8. Prepare red, yellow, and blue LEDs for mounting (Fig. 5g).
 - a. For one LED, feed LED legs through the plastic portion of the LED holder.
 - b. Bend ground (short) leg of the LED, cut a 3-inch segment of solid core wire, and strip \sim 1 cm from each end. Twist one end of the wire with the LED ground leg.
 - c. Solder that connection and cover with heat shrink, applying hot air to secure.
 - d. Repeat steps 8 a-c. with the other two LEDs.
 - e. For each LED, connect the positive (long) leg to its respective resistor by twisting the LED's positive leg and one of the resistor's legs together and soldering that connection. The LEDs in our circuit require resistors to limit current flow to each LED. This ensures that the LEDs will not burn out. The red and yellow LEDs have similar voltage requirements and need one 220 Ω resistor each. The blue LED has a higher voltage requirement and will need one 100 Ω resistor. Cover soldered connections with heat shrink and secure using hot air.
 - f. Next, gather the three ground wires from each LED and twist them together. Cut a 3-inch segment of the solid core wire and strip \sim 1 cm off each end, then twist one end of this wire together with the other three wires. Solder this connection and cover with heat shrink, applying hot air to secure.
 - g. Next, cut three 3-inch pieces of solid core wire, stripping ~ 1 cm off each of all three wires. For each LED, twist the free leg of their respective resistor together with one piece of solid core wire, solder the connection, cover with heat shrink, and apply hot air to secure.
- 9. Mount and install the LEDs.
 - a. Mount the LEDs into their holders in the case from the inside, arranged so that the yellow LED is on the left, red in the middle, and blue on the right.
 - b. Connect the LED's ground wire to Arduino GND pin, the yellow LED's positive wire to Arduino pin 6, the red LED's positive leg to Arduino pin 8, and the blue LED's positive leg to Arduino pin 10 (Fig. 5h).
- 10. Prepare solenoid wires to be connected to the relay unit.
 - a. Solder short (8–10 cm) wires to the DC power jack connector socket. For this connector the short pin is the center connection (positive pole for our power adapter) and the long pin is the ground. Guide wires through designated hole and secure the power jack to the case by pressing it into the hole.
 - b. Place heat shrink on the ground wire for later use. Twist the black ground wire together with the ground leg of a diode and solder the connection, making sure to keep the heat shrink away from the connection; otherwise, the heat shrink will pre-emptively shrink. The diode prevents current discharge from coming back through the circuit and damaging the circuit.
 - c. Pick one of the solenoid wires and place a piece of heat shrink on it. Then, wrap the wire around the soldered DC power ground-diode connection. (Fig. 5i). Solder the solenoid wire into place. Push the two pieces of heat shrink, one on the solenoid wire and the other on the ground wire, together to cover as much of the soldered connection as possible. Cover the rest of the solder with heat shrink cut to diode leg size and slid over the diode. Apply hot air to shrink all the wrap.
 - d. Put ½ of a piece of heat shrink over the diode, push as far down the diode as possible, and another full piece down the second solenoid wire. Twist the positive leg of the diode together with the second solenoid wire. Then, cut a 3-inch piece of the solid core wire, stripping ~ 1 cm from each end, and twist one of the wire ends together with the diode and solenoid wire. Solder this connection together, then push the two pieces of heat shrink together to cover as much solder as possible. Put a third piece of heat shrink over the solid core wire and push it down to cover the rest of the exposed solder. Apply hot air to shrink all the wrap (Fig. 5j).
 - e. Bend the exposed metal of the power cord's positive wire and the free end of the solid core wire at a 90-degree angle. Loosen the screws on the COM (middle) port and the NO (normally open; right) ports of the K1 channel. Insert the solid core wire into the COM port, tighten the Port's screw down, and tug gently to ensure it is securely connected. Insert the positive power wire into the NO (normally open) port, tighten the Port's screw down, and tug gently to ensure it is securely connected (Fig. 5k).
- 11. Label the left (going to pin A0) RF/coaxial connector with "IN" and the right (going to pin 2) RF/coaxial connector with "OUT" (Fig. 21).
- 12. Slide the case lid on and use a 16 mm M3 screw to secure the lid into place.

5.2. Assembly of the completed timed distension controller system with peripherals.

- 1. The airflow diagram in Fig. 1c shows how to connect the tubing from the compressed air source to the animal. There is an additional 'air flow diagram' file in the build files.
- 2. Connect the air cylinder regulator to the flowmeter regulator using appropriate tubing.
- 3. Then using 3/16 in. interior diameter tubing, connect the flow meter to the leak valve. This allows for a small amount of leak, making it easier to adjust the pressures and limiting the pressure that can go to the animal.
- 4. Add another piece of 3/16 in. inner diameter tubing to the other side of the leak valve and connect it to a T connector. One side of the T goes to the first aneroid gauge. The other side of the T goes into the IN inlet of the solenoid valve in the time distension controller.
- 5. From the OUT of the solenoid valve, run the 3/16 in. interior diameter tubing to the barbed 3/16 to 3/32 reducer.

- 6. From the other side of the reducer, now using the smaller 3/32 in. inside diameter tubing, run to a T connector where one side will go to the second android gauge, and the other will go either to the optional pressure sensor.
- 7. The pressure sensory we used here was a Blood Pressure Transducer and Cable (World Precision Instruments, listed on Bill of Materials). It has Luer lock adaptors on both sides, so it can fit in line with the 3/32 with barbed to Leur lock adaptors. The signal from the pressure transducer is transmitted to an amplifier (4-channel transducer amplifier, SYS-TBM4M, World Precision Instruments; Working pressure –50 to + 300 mmHg) and then to our data acquisition system. This component is optional as the aneroid gauges will read the current pressure being delivered. However, this is one way to keep electronic records of the distension waveform. Pressure can be calibrated using the aneroid gauges prior to the experiment.
- 8. Coming out of the optional pressure sensor, we run the tubing to the animal. The final adaptor will depend on what you are using to distend. In our case, we used a barbed to slip Luer lock adaptor to connect to a catheter.

5.3. Arduino software installation

There are two modes of operation independent control, through graphical user interface (GUI)-based or TTL triggered software. These require different software to be loaded on the Arduino, so either follow 5.3.1 or 5.3.2. The mode of operation can be changed later if needed.

5.3.1. Installation of independent GUI-based control

- 1. Download the Arduino IDE desktop app from arduino.cc (https://www.arduino.cc/).
- a. Follow the directions for download options based on computer specs.
- 2. Install and open the Arduino IDE.
- 3. Connect the Arduino hardware to the PC via USB cable.
- 4. Arduino Startup
 - a. Configure the board
 - i. Tools > Board
 - ii. Select which Arduino board is being used
 - b. Select appropriate Port
 - i. Tools > Port
 - ii. Select the Port indicating the Arduino Uno
- 5. In the Arduino IDE, run "Standard Firmata".
 - a. File > Examples > Firmata > Standard Firmata
 - b. Verify and Upload
 - c. This file must always be running for the python scripts to run,
- 6. Install Python
 - a. Go to python.org (https://www.python.org/downloads/)
 - b. Download the latest version (we are using version 3.8)
 - c. Open Software
- 7. In Python, install the pyFirmata package.
 - a. Go to pypi.org (https://pypi.org/project/pyFirmata/)
 - b. Copy "pip install pyFirmata"
 - c. Open Python and in the IPython console, paste and run the code
 - d. Restart Python to use the added package
- 8. Upload the "TCP_GUIv1.2" to Python terminal.
 - a. Open code in python terminal, we used Spyder 2.8 IDE.
 - b. In line 23 of the code, change the Port from 'COM3' to whichever Port the user is working with, i.e., the Port that was selected in the Arduino IDE.
- 9. Save and run the code (Section 6.1.1)
- 5.3.2. Installation of TTL triggered operation
- Download the Arduino IDE desktop app from arduino.cc (https://www.arduino.cc/).
 a. Follow the directions for download options based on computer specs.
- 2. Install and open the Arduino IDE.
- 3. Connect the Arduino hardware to the PC via USB cable.
- 4. Arduino Startup
 - a. Configure the board
 - i. Tools > Board

- ii. Select which Arduino board is being used
- b. Select appropriate Port
- i. Tools > Port
- ii. Select the Port indicating the Arduino Uno
- 5. In the Arduino IDE, run "TPC_TTL_Triggering"
 - a. Verify and Upload

6. Operation instructions

6.1.1. Operation of timed distension controller with GUI -based control

- 1. After running the code (Step 5.3.1). A pop-up labeled "Distension Cycles" will appear (Fig. 1d). This window contains the four different input variables, Time Pre-Distension, Distension Time, Time Post-Distension, and Cycles.
- 2. When operating the program, the "Start" button will begin to run the software, and the "Time Left:" and "Cycles Left:" fields in the bottom left corner of the pop-up will auto-populate to allow you to keep track of the hardware status and cycle information
- 3. The "Restart" button can be used if the cycle set needs to be stopped or reset. This will return the valve to the closed state.
- 4. When finished, use the "Close" button to exit out of the software.

6.1.2. Operation of timed distension controller with TTL triggering

- 1. After uploading the "TPC_TTL_Triggering" the hardware will be set up to receive TTL signals to open the solenoid.
- 2. Opening of the valve and distension can be triggered by a TTL pulse greater than 4 V. This can be changed in the "TPC_TTL_Triggering file if your system delivers a different voltage level.
- 3. When a pulse (greater than4 V) is delivered, the solenoid will open. Programing the TTL pulses will depend on the software and hardware being used. If you need a simple TTL triggering device to coordinate multiple TTL pulses, we suggest the Arduino TTL Pulse Generator and Controller from the Optogenetics and Neural Engineering Core at the University of Colorado Anschutz Medical Campus. This can coordinate multiple TTL pulses as we used in the validation (section 7).

6.2.1. Safety considerations

There are no major safety concerns with the operation of this device. However, we do test the device every time we use it on a small balloon (glove finger) to make sure the valve is opening and closing when it should be. We do this because we do not want to accidentally distend the animal when not intending to, which can lead to organ damage or cause undue harm to the animal. The leak valve will also help reduce the chances of accidentally distending at high pressures. We recommend unplugging the solenoid and Arduino when not in use.

7. Validation and characterization

In order to validate the timed pressure controller, we performed bladder distension evoked visceral motor response assay [3,11,12,16]. This experiment is an assay of bladder nociception in mice [3,12]. Increasing bladder distension pressures result in a corresponding increase in electromyography (EMG) activity in the superior oblique abdominal muscles. This reflex is termed a visceral motor response. This visceromotor response can be attenuated with the use of analgesics, suggesting it can be used as an indirect measure of bladder nociception in mice [3]. A detailed explanation and descriptive methods have been published in the Journal of Visualized Experiments [12].

Here we used wild-type C57Bl/6J mice to demonstrate the functionality of the timed distention controller and associated software to increases in pressure (20, 30, 40, 50, 60, 70 mmHg). After a transurethral catheter is inserted, EMG electrodes are placed in the superior oblique abdominal muscles, and the correct anesthesia plane is maintained; we then proceeded with a distension protocol [12]. We started by adjusting the distension pressure using the flowmeter regulator and the pre-solenoid aneroid gauge to 20 mmHg. Once the pressure is set, we entered our input parameters in the user interface (Time closed before stimulus = 20, Time on/open = 20, Time off/closed = 60 and Cycles = 18) (Fig. 3). After clicking 'start', we observed the animal and the post-solenoid aneroid gauge, and once the distension started, we adjusted the pressure with the flowmeter regulator if necessary so that the post-solenoid aneroid gauge indicated 20 mmHg. After three cycles, we then increased by 10 mmHg and repeated the same process up to 70 mmHg. Using an amplifier (Grass P511), Micro 1404 digitizer (CED) and Spike2 (CED) software, and a pressure transducer, we recorded EMG responses from the superior oblique abdominal muscles, solenoid pressure output, and the coaxial voltage output from the timed pressure controller, which indicates that the valve is open (Fig. 3a).



Fig. 6. Validation of the Timed Distension Controller Using Mouse Bladder Distension to Evoke a Visceral Motor Response. A) An example screenshot of data acquisition software (Spike2, CED) used to acquire abdominal EMG responses evoked by bladder distension. The timed pressure controller is controlled using the user interface set 18 cycles of 20 sec off, 20 sec open, 60 s closed. The 5 V pulse from the time pressure controller indicates the valve is open, which correlates with the inline pressure transducer measurement (distension pressure) and physiologic EMG response. B) Representative examples of 20, 40, and 60 mmHg distensions demonstrate a tight correlation between solenoid valve opening, downstream pressure, and physiologic EMG response. C) Quantification of one mouse responses to all distensions. D Example of TTL activation of the time distension controller and LED optogenetic stimulation using Spike2 software and a Micro1401 data acquisition system.

Our results indicate that the timed distension controller operates as designed, opening the solenoid at the indicated time and performing the input number of cycles (Fig. 6a). The inline pressure transducer indicates the pressure increases at the same time the voltage pulse is sent. The distensions also correlate with increased physiologic EMG responses (Fig. 6b and c), as has been demonstrated in numerous other publications [3,12,16]. These results indicate that the timed pressure delivery is working as intended, delivering air to distend the bladder and evoke abdominal EMG responses.

Next, we tested the TTL triggered mode of operation using Spike2 software to program the TTL pulses and a Micro 1404 to deliver the voltage stimulus to the timed pressure controller. As a proof in concept, we also paired programmed a TTL pulse

to activate a blue laser prior to distension (Fig. 6d). This can be used in optogenetic experiments to activate opsins, lightactivated proteins, in a population of cells prior to delivering the distension stimulus [11,16–18]. Here we show a TTL pulse sent to the laser 5 s prior to sending the triggering stimulus to the timed distension controller. The timed distension controller opens the valve, which correlates to an increase in distension pressure (Fig. 6d). When the valve closes (after 10 s), the distension quickly dissipates. Together these results show that by using the user interface, we were able to control the solenoid valve and that delivery of bladder distension was able to replicate the capabilities of previous work.

CRediT authorship contribution statement

Trishna Patel: Software, Methodology, Investigation, Formal analysis, Writing – original draft, Writing – review & editing, Visualization. **Jamie Hendren:** Software. **Nathan Lee:** Software. **Aaron D. Mickle:** Conceptualization, Methodology, Investigation, Formal analysis, Resources, Writing – original draft, Writing – review & editing, Visualization, Supervision, Project administration.

Declaration of Competing Interest

The authors declare that they have no known competing financial interests or personal relationships that could have appeared to influence the work reported in this paper.

Acknowledgements

We would like to acknowledge Alex Toney and Al Amin Hadis for their assistance with early hardware iterations. We would also like to thank Gabriella Robilotto for her technical support and logistical help for the project.

Funding

This work was supported by startup funds from the University of Florida.

Data availability

All design files and software are published and available at: https://doi.org/10.17605/OSF.IO/RS5P4. None to declare.

Human and animal rights

All experiments were performed using adult (8-12 weeks old) female mice (C57Bl/6J; Jackson # 000664) housed in a facility on a 12-hour light/dark cycle with access to food and water ad libitum. All the procedures involving mice were approved by the University of Florida Institutional Animal Care and Use Committees (Protocol # 201910733), and in strict accordance with the US National Institute of Health (NIH) Guide for the Care and Use of Laboratory Animals (NIH Publications No. 8023, revised 1978).

References

- [1] L. Grundy, A. Erickson, S.M. Brierley, Visceral Pain, Annu. Rev. Physiol. 81 (1) (2019) 261–284.
- [2] T.J. Ness, G.F. Gebhart, Colorectal distension as a noxious visceral stimulus: physiologic and pharmacologic characterization of pseudaffective reflexes in the rat, Brain Res 450 (1-2) (1988) 153–169.
- [3] T.J. Ness, H. Elhefni, Reliable visceromotor responses are evoked by noxious bladder distention in mice, J. Urol. 171 (4) (2004) 1704–1708.
- [4] T.J. Ness, G.F. Gebhart, Visceral pain: a review of experimental studies, Pain 41 (2) (1990) 167–234.
- [5] K. Lamb, G.F. Gebhart, K. Bielefeldt, Luminal stimuli acutely sensitize visceromotor responses to distension of the rat stomach, Dig. Dis. Sci. 52 (2) (2007) 488–494.
- [6] T.J. Ness, H.E. Richter, E.R. Varner, R.B. Fillingim, A psychophysical study of discomfort produced by repeated filling of the urinary bladder, Pain 76 (1) (1998) 61–69.
- [7] M. Karpefors, L.M.A. Akkermans, A. Bayati, A new intelligent distension system for hollow organs, Med. Biol. Eng. Comput. 45 (3) (2007) 275–281.
- [8] M.P. FitzGerald, D. Koch, J. Senka, Visceral and cutaneous sensory testing in patients with painful bladder syndrome, Neurourol. Urodyn. 24 (7) (2005) 627–632.
- [9] R.H. Anderson, T.J. Ness, G.F. Gebhart, A distension control device useful for quantitative studies of hollow organ sensation, Physiol. Behav. 41 (6) (1987) 635–638.
- [10] M. DeLong, M. Gil-Silva, V.M. Hong, O. Babyok, B.J. Kolber, Visceral pressure stimulator for exploring hollow organ pain: a pilot study, Biomed. Eng. Online 20 (1) (2021), https://doi.org/10.1186/s12938-021-00870-y.
- [11] J.J. DeBerry et al, Differential regulation of bladder pain and voiding function by sensory afferent populations revealed by selective optogenetic activation, Front. Integr. Neurosci. 12 (2018) 5.
- [12] K.E. Sadler, J.M. Stratton, B.J. Kolber, Urinary bladder distention evoked visceromotor responses as a model for bladder pain in mice, J. Vis Exp. 86 (2014).
- [13] A. Miranda, E. Nordstrom, A. Mannem, C. Smith, B. Banerjee, J.N. Sengupta, The role of transient receptor potential vanilloid 1 in mechanical and chemical visceral hyperalgesia following experimental colitis, Neuroscience 148 (4) (2007) 1021–1032.

T. Patel, J. Hendren, N. Lee et al.

- [14] A. Mickle, M. Sood, Z. Zhang, G. Shahmohammadi, J.N. Sengupta, A. Miranda, Antinociceptive effects of melatonin in a rat model of post-inflammatory visceral hyperalgesia: A centrally mediated process, Pain 149 (3) (2010) 555–564.
- [15] E.H. Kamp, R.C.W. Jones, S.R. Tillman, G.F. Gebhart, Quantitative assessment and characterization of visceral nociception and hyperalgesia in mice, Am. J. Physiol. Gastrointest Liver Physiol. 284 (3) (2003) G434–G444.
- [16] V.K. Samineni, A.D. Mickle, J. Yoon, J.G. Grajales-Reyes, M.Y. Pullen, K.E. Crawford, K.N. Noh, G.B. Gereau, S.K. Vogt, H.H. Lai, J.A. Rogers, R.W. Gereau, Optogenetic silencing of nociceptive primary afferents reduces evoked and ongoing bladder pain, Sci. Rep. 7 (1) (2017), https://doi.org/10.1038/ s41598-017-16129-3.
- [17] K.E. Sadler, N.A. McQuaid, A.C. Cox, M.N. Behun, A.M. Trouten, B.J. Kolber, Divergent functions of the left and right central amygdala in visceral nociception, Pain 158 (4) (2017) 747–759.
- [18] L.W. Crock, B.J. Kolber, C.D. Morgan, K.E. Sadler, S.K. Vogt, M.R. Bruchas, R.W. Gereau, Central amygdala metabotropic glutamate receptor 5 in the modulation of visceral pain, J. Neurosci. 32 (41) (2012) 14217–14226.



Trishna Patel graduated from the University of Florida in 2021 with a Bachelor's of Science in Biomedical Engineering (cum laude). Under the supervision of Dr. Aaron Mickle, Trishna's undergraduate research focused on studying the visceral sensory component of the peripheral nervous system through the mechanical and optical stimulation of the bladder. She is currently working as a Device Engineer at Regenzbio.



Jamie Hendren is a Power Distribution Engineer at Georgia Power Company in Savannah, Georgia. In 2020 she obtained her Bachelor of Science Degree in Chemical Engineering from the University of Florida. While at the University of Florida, her undergraduate research included projects that focused on the development of bench scale heat exchangers, fluidized bed experimental modules, and software to control prototype pressure-delivery devices. In her current role at Georgia Power, she designs electrical distribution systems to serve power to GPC customers.



Nathan Lee is a Computer Science undergraduate at the Wertheim Herbert School of Engineering at the University of Florida from Tampa, Florida. He has worked under the supervision of Prof. A. Mickle for 2 years. His undergraduate research focused on software for graph analysis, controlling prototype pressure-delivery devices, and software for image processing. After graduation, he plans on entering the Computer Science industry as a software engineer, focusing on becoming a backend developer.



Aaron Mickle is an Assistant Professor in the Department of Physiological Sciences, in the college of Veterinary Medicine at the University of Florida. He received my PhD in pharmacology from the University of Iowa under the mentorship of Dr. DP Mohapatra studying nociceptor sensitization in the context of metastasized cancer pain. He then completed his postdoctoral fellowship at Washington University in Saint Louis with Dr. Robert Gereau where he collaborated with material, electrical, and biomedical engineers to develop closed-loop optogenetic based neuromodulatory technologies targeting the lower urinary tract. In August of 2019, he joined the department of Physiological Sciences to establish his own lab. His current research focuses on the develop of neuromodulation technology and studying mechanisms of bladder pain and dysfunction using both cellular and systems approaches.