Data in brief 26 (2019) 104485

Contents lists available at ScienceDirect

Data in brief

journal homepage: www.elsevier.com/locate/dib



Data Article

Experimental data on the characterization of hydroxyapatite synthesized from biowastes



J.K. Abifarin ^a, D.O. Obada ^{a, *}, E.T. Dauda ^b, D. Dodoo-Arhin ^{c, d, **}

^a Department of Mechanical Engineering, Ahmadu Bello University, Zaria, Nigeria

^b Department of Metallurgical and Materials Engineering, Ahmadu Bello University, Zaria, Nigeria

^c Department of Materials Science and Engineering, University of Ghana, Legon, Ghana

^d Institute of Applied Science and Technology, University of Ghana, Legon, Ghana

ARTICLE INFO

Article history: Received 13 July 2019 Received in revised form 15 August 2019 Accepted 29 August 2019 Available online 11 September 2019

Keywords: Animal bones Calcination Microstructure Infrared region

ABSTRACT

The purpose of the dataset is to present the morphological features, elemental composition and functional groups of hydroxyapatite (HAp) synthesized from non-separated biowastes (animal bones) by a modified facile heat treatment method up to a maximum temperature of 1100 °C. The synthesized powders were characterized using scanning electron microscopy (SEM) equipped with electron dispersive X-ray analysis (EDX) and Fourier transform infrared spectroscopy (FTIR). These evaluations were to reveal the surface features, elemental composition and identify the functional groups of the synthesized powders. After heat treatment of the raw biowastes to 900 °C, 1000 °C, and 1100 °C (regime of heat treatment), the morphological features of the samples exhibited a more densely packed microstructure at the highest sintering temperature (1100 °C). The elemental composition as evaluated by EDX on a weight and atomic basis for all samples provided information on the calcium to phosphate transforms into apatite with a Ca/P ratio of 3.60, 2.04, 2.50 and 2.32 wt % and 2.79, 1.58, 1.94 and 1.78 at. % respectively for raw biowastes (RB) to sintered samples (HA-900, HA-1000 and, HA-1100 °C). The FTIR data showed phosphate and hydroxyl peaks in the thermally treated samples and all the samples produced characteristic

* Corresponding author.

** Corresponding author. Department of Materials Science and Engineering, University of Ghana, Legon, Ghana. *E-mail addresses:* doobada@abu.edu.ng (D.O. Obada), d.dodoo-arhin@ug.edu.gh (D. Dodoo-Arhin).

https://doi.org/10.1016/j.dib.2019.104485



^{2352-3409/© 2019} The Authors. Published by Elsevier Inc. This is an open access article under the CC BY license (http:// creativecommons.org/licenses/by/4.0/).

stretching modes of O–H bands at about 3417 $\rm cm^{-1}$ which are noticed in all FTIR spectra of HAp.

© 2019 The Authors. Published by Elsevier Inc. This is an open access article under the CC BY license (http://creativecommons. org/licenses/by/4.0/).

Specifications Table

a.1.1.	- · · ·
Subject	Engineering
Specific subject area	Biomedical Materials: synthesis and characterization
Type of data	Table
	Image
	Chart
	Graph
	Figure
How data were acquired	SEM/EDX and FTIR techniques
Data format	Raw
	Analysed
	Images
	Tables
	Plots
Parameters for data collection	Hydroxyapatite was produced from the calcination of clean animal bones at 900 °C, 1000 °C, 1100 °C for a dwell time of 2 h.
Experimental features	1. The animal bones were thoroughly cleaned to remove the protein externally by soaking for 24 h, washing with pure water and boiling for 3 h
	2. The cleaned bones were rinsed in warm water, and dried at 150 °C in an electric oven
	for 8 h.
	3. Calcination was conducted under atmospheric condition using an electric furnace at
	900 °C at a ramp rate of 5 °C/min with 2 h of soaking time
	4. The calcined powders were crushed with a metallic mortar and pestle and sieved
	through a 300 μ m mesh sieve to obtain a fine powder prior to characterization.
Data source location	Department of Mechanical Engineering, Ahmadu Bello University, Zaria, Nigeria
	With the article
Data accessibility	

Value of the data

- The dataset can be used to monitor changes in the properties of hydroxyapatite derived biomaterials at the microscale
- Researchers working on biomaterials and biowaste valorization can benefit hugely from the data
- The FTIR data provided in this article provides an indirect evaluation of the synthesized hydroxyapatite, showing the most characteristic chemical groups in the FTIR spectrum of synthesized HAp such as PO₄⁻⁷, OH-, CO₂⁻⁷.
- Data obtained in this study would be useful for future investigation on the industrial applicability of biowastes derived hydroxyapatite

1. Data

The dataset presented in this article for SEM and FTIR analyses as shown in Figs. 1 and 2 are for synthesized hydroxyapatite subjected to various sintering temperatures (900 °C, 1000 °C, 1100 °C). The morphology of samples in Fig. 2 is at a magnification of 10.0 and 15.0 kx. The elemental composition and FTIR summary tables (Tables 1a and 1b and Table 2) show Ca/P ratios and obtained functional groups which provides useful information about the composition of samples and the location of peaks, their intensities, width and shape in the required wave number range. Raw data for FTIR spectrogram is presented as supplementary files.

The surface morphology of the samples after sintering at 900 °C, 1000 °C and 1100 °C at different magnifications (10.0 and 15.0 kx) is shown in Fig. 1 and the corresponding EDS spectra is shown in



Fig. 1. SEM micrographs of RB, HA-900, HA-1000 and HA-1100 at different magnifications.

Fig. 2. Close observation of the SEM images reveal increasingly dense microstructure as a function of increased sintering temperature. The densification of hydroxyapatite particles as revealed by SEM increases as sintering temperature increase. Samples sintered at 900 °C reveal fine grains which are not closely packed. Samples sintered at 1000 °C show some grain growth tendencies which can be attributed to re-crystallization phase with porosities embedded between the large grains. The sample sintered at 1100 °C show grain growth, closely packed particles as well as decreasing pore sizes and density. In addition, the micrographs in Fig. 1 show morphologies for all samples with fine particles and



Fig. 2. EDS spectra of RB, HA-900, HA-1000 and HA-1100.

culcium/i nospinate ratio (irit	,0).			
Sample Code	RB	HA-900	HA-1000	HA-1100
Calcium (Wt %)	44.98	38.28	45.11	40.76
Phosphorus (Wt %)	12.47	18.71	18.00	17.55
Ca/P (Wt %)	3.60	2.04	2.50	2.32

ladie la		
Calcium/Phosphate ratio	(Wt	%).

Table 1b

....

Calcium/Phosphate ratio (At%).

Sample Code	RB	HA-900	HA-1000	HA-1100
Calcium (At%)	25.21	21.95	27.57	23.78
Phosphorus (At%)	9.04	13.88	14.23	13.25
Ca/P (At %)	2.79	1.58	1.94	1.79

reduced pore size details (magnification 10.0 kx). With an increase to 15.0 kx (b), it is observed that the particles are clustered with more pore size details reavealed. From the EDX spectra as depicted in Fig. 2, the characteristic peaks of Ca, P and O are present with the atomic and weight percentages which provides the mean relative calcium to phosphate ratios as shown in Tables 1a and 1b.

Tables 1a and 1b represents the elemental composition of the raw biowastes and synthesized hydroxyapatite with their corresponding calcium to phosphate (Ca/P) ratios obtained by energy dispersive X-ray analysis (EDX). Weight percentage (wt%) and atomic percentage (at%) were considered to give Ca/P approximations. From the data (Tables 1a and 1b), calculated Ca/P ratios for sample HA-900 were 2.04 and 1.58 for weight and atomic percentages respectively. Comparatively, the atomic Ca/P ratio (1.58) of HA-900 was the closest to stoichiometric Ca/P ratio of hydroxyapatite (1.67) amongst all the hydroxyapatite samples investigated in this study.

Fig. 3 shows the Fourier Transform Infrared (FT-IR) spectrogram of synthesized HAp before and after sintering at different temperatures with further description in Table 2. Typical characteristic bands corresponding to the carbonate groups of the CaCO₃ component of hydroxyapatite are located around 1411 cm⁻¹ and 1465 cm⁻¹. The sintered samples showed small frequency bands around 2345 cm⁻¹ and 2353 cm⁻¹ ascribed to the release of CO₂ during heat treatment [10]. The initial formative indicator of hydroxyapatite at all point of sintering (900 °C, 1000 °C, 1100 °C) was in the form of a pronounced broad band around 1000 cm⁻¹ –1100 cm⁻¹ which can be ascribed to asymmetric stretching mode of vibration of PO₄ group. However, as noticed for the raw biowastes bone, a small band noticed at 1033 cm⁻¹ indicates a deficient asymmetric stretching mode of vibration of PO₄ group that was made pronounced by heat treatment. Also, the band between 570 cm⁻¹ – 565 cm⁻¹ for all the samples

Table 2	
Wavenumbers, chemical groups and description of the FT-IR spectrum of RB, HA-900, HA-1000 and HA-1100.	

Sample code and Wavenumber (cm ⁻¹)			Chemical	Description	References		
RB	HA-900	HA-1000	HA-1100	group			
563, 601	570, 601	570, 601	570, 601	PO ₄ ³⁻	bending mode	[3-5,12 -14]	
671, 3417	632, 3417	632, 3417	632, 3417	OH-	OH [−] ions prove presence of HA	[3,4,7,12 -14]	
1033, 1134	1049, 1095	1049, 1095	1049, 1095	PO_{4}^{3-}	Antisymmetric stretching mode	[1,3 -5,9,12 -14]	
1412, 1466, 1643,	1411, 1465, 1550, 1643, 2152, 2345	1411, 1465, 1643, 2152, 2345	1411, 1465, 1643, 2553	CO ₃ ²⁻	Substitutes phosphate ion, B-type HA (i.e. $\rm CO_3$ substituting for $\rm PO_4$) is formed	[2,6–9,12 –14]	
2862, 2924	2931	2924	2924	Adsorbed water	Under influence of thermal treatment, absorption band becomes narrower	[2,8,9,12 -14]	



Fig. 3. FT-IR spectrogram of RB, HA-900, HA-1000 and HA-1100.

corresponds to symmetric P–O stretching vibration of PO₄ group [11]. The prominent bands at 3417 $\rm cm^{-1}$ for all samples is due to the vibratory stretching of OH group of HAp while the bands at 1643 $\rm cm^{-1}$ for all samples were attributed to adsorbed water molecules [1]. All the samples produced typical stretching modes of O–H bands at about 3417 cm⁻¹ characteristic of FT-IR spectrogram of HAp. From the FT-IR spectrogram, differences between the spectrum of the raw and heat treated hydroxyapatite samples can be noticed for the bands at 1411 and 1465 cm⁻¹ for HA-1000 and HA-1100 samples as compared to the bands ascribed to RB and HA-900 samples. These differences are indicative of the degree of carbonate ion substitution. The bands at 1643 and 3417 cm⁻¹ for all samples with broader bands for RB and HA-900 samples correspond to the disappearance of absorbed water after sintering [15,16].

2. Experimental design, materials, and methods

The biowastes (animal bones) were obtained from an Abattoir in Zaria, Nigeria. The as-received bones were cleaned thoroughly to remove the protein externally by soaking for 24 h, washing with tap water and boiling for 3 h. This was followed by rinsing in warm water before drying at 150 °C in an electric oven for 8 h. The as-produced powders were calcined under atmospheric condition using an electric furnace at 900 °C at a ramp rate of 5 °C/min with 2 h of soaking time. The calcined powders were crushed with a metallic mortar and pestle and sieved through a 300 μ m mesh sieve to obtain a fine powder prior to characterization. Fig. 4 shows a schematic of the experimental procedure for the synthesized hydroxyapatite. The produced hydroxyapatite powders were further sintered at 1000 °C and 1100 °C to investigate the effects of sintering temperature on the morphological features and retention of functional groups relating to produced hydroxyapatite. The nomenclature of samples synthesized and analysed are: RB (raw biowaste), HA-900 (samples sintered at 900 °C), HA-1000 (samples sintered at 1000 °C) and HA-1100 (samples sintered at 1100 °C).

The morphology of the samples was carried out on an ultra-high vacuum and high resolution MAIA3 TESCAN scanning electron microscopic—energy dispersive X-ray analysis (SEM-EDX) operated at 5 kV. The samples were prepared by gold sputtering the surface of the samples using a low deposition rate. The functional groups present in the samples have been identified by FT-IR equipped with UATR sampling accessory in the range of 500–4000 cm⁻¹. Samples were grinded and mixed with dried KBr using ceramic mortar and loaded into a sample holder mounted in the instrument.



Fig. 4. Schematic of hydroxyapatite preparation and characterization techniques.

Acknowledgments

Authors acknowledge the Department of Mechanical Engineering and Materials and Metallurgical Engineering, Ahmadu Bello University, Zaria, Nigeria for technical support. In addition, DDA acknowledges the support of the University of Ghana BANGA-Africa programme.

Conflict of interest

The authors declare that they have no known competing financial interests or personal relationships that could have appeared to influence the work reported in this paper.

Appendix A. Supplementary data

Supplementary data to this article can be found online at https://doi.org/10.1016/j.dib.2019.104485.

References

- A.I. Adeogun, A.E. Ofudje, M.A. Idowu, S.O. Kareem, Facile development of nano size calcium hydroxyapatite based ceramic from eggshells: synthesis and characterization, Waste and Biomass Valorization 9 (8) (2018) 1469–1473.
- [2] Y.M.Z. Ähmed, S.M. El-Sheikh, Z.I. Zaki, Changes in hydroxyapatite powder properties via heat treatment, Bull. Mater. Sci. 38 (7) (2015) 1807–1819.
- [3] A. Destainville, E. Champion, D. Bernache-Assollant, E. Laborde, Synthesis, characterization and thermal behavior of apatitic tricalcium phosphate, Mater. Chem. Phys. 80 (1) (2003) 269–277.
- [4] J.K. Han, H.Y. Song, F. Saito, B.T. Lee, Synthesis of high purity nano-sized hydroxyapatite powder by microwavehydrothermal method, Mater. Chem. Phys. 99 (2–3) (2006) 235–239.
- [5] I. Mobasherpour, M. Heshajin, Synthesis of nanocrystalline hydroxyapatite by using precipitation method, J. Alloy. Comp. 430 (2007) 330–333.
- [6] B. Ratner, A. Hoffman, F. Schoen, et al., Characterisation and thermal stability of powders, Biomaterials (23) (2004) 1065–1072. Biomaterials Scienc. An Introduction to Materials in Medicine, Second Edition//Academic Press, p. 851.
- [7] S. Raynaud, E. Champion, D. Bernache-Assollant, P. Thomas, Calcium phosphate apatites with variable Ca/P atomic ratio I. Synthesis, characterisation and thermal stability of powders, Biomaterials 23 (4) (2002) 1065–1072.
- [8] S. Meejoo, W. Maneeprakorn, P. Winotai, Phase and thermal stability of nanocrystalline hydroxyapatite prepared via microwave heating, Thermochim. Acta (447) (2006) 115–120.
- [9] L. Berzina-Cimdina, N. Borodajenko, Research of calcium phosphates using Fourier transform infrared spectroscopy, in: Infrared Spectroscopy-Materials Science, Engineering and Technology, IntechOpen, 2012.

- [10] S. Ummartyotin, B. Tangnorawich, Utilization of eggshell waste as raw material for synthesis of hydroxyapatite, Colloid Polym. Sci. 293 (9) (2015) 2477–2483.
- [11] H.K. Varma, S.S. Babu, Synthesis of calcium phosphate bioceramics by citrate gel pyrolysis method, Ceram. Int. 31 (1) (2005) 109–114.
- [12] G.A. Mekhemer, H. Bongard, A.A. Shahin, M.I. Zaki, FTIR and electron microscopy observed consequences of HCl and CO₂ interfacial interactions with synthetic and biological apatites: influence of hydroxyapatite maturity, Mater. Chem. Phys. 221 (2019) 332–341.
- [13] C.C. Coelho, L. Grenho, P.S. Gomes, P.A. Quadros, M.H. Fernandes, nano-hydroxyapatite in oral care cosmetics: characterization and cytotoxicity assessment, Sci. Rep. 9 (1) (2019) 11050.
- [14] J.J. Malpica-Maldonado, J.A. Melo-Banda, A.L. Martínez-Salazar, M. Garcia-Hernández, Synthesis and characterization of Ni-Mo₂C particles supported over hydroxyapatite for potential application as a catalyst for hydrogen production, Int. J. Hydrogen Energy 44 (24) (2019) 12446–12454.
- [15] A. Almirall, G. Larrecq, J.A. Delgado, S. Martınez, J.A. Planell, M.P. Ginebra, Fabrication of low temperature macroporous hydroxyapatite scaffolds by foaming and hydrolysis of an α-TCP paste, Biomaterials 25 (17) (2004) 3671–3680.
- [16] H.R. Ramay, M. Zhang, Preparation of porous hydroxyapatite scaffolds by combination of the gel-casting and polymer sponge methods, Biomaterials 24 (19) (2003) 3293–3302.