

# **ARTICLE**



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# Plasmonic nano-aperture label-free imaging (PANORAMA)

Label-free optical imaging of nanoscale objects faces fundamental challenges. Techniques based on propagating surface plasmon resonance (SPR) and localized surface plasmon resonance (LSPR) have shown promises. However, challenges remain to achieve diffraction-limited resolution and better surface localization in SPR imaging. LSPR imaging with dark-field microscopy on metallic nanostructures suffers from low light throughput and insufficient imaging capacity. Here we show ultra-near-field index modulated PlAsmonic NanO-apeRture lAbel-free iMAging (PANORAMA) which uniquely relies on unscattered light to detect sub-100 nm dielectric nanoparticles. PANORAMA provides diffraction-limited resolution, higher surface sensitivity, and wide-field imaging with dense spatial sampling. Its system is identical to a standard bright-field microscope with a lamp and a camera – no laser or interferometry is needed. In a parallel fashion, PANORAMA can detect, count and size individual dielectric nanoparticles beyond 25 nm, and dynamically monitor their distance to the plasmonic surface at millisecond timescale.

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ielectric nanoparticles are considered transparent "phase" objects in optical physics, i.e., they contribute a slight variation to the local refractive index. Unlike plasmonic nanoparticles consisting of noble metal such as Au and Ag, dielectric nanoparticles scatter far less light. Owing to their minute physical dimension, there are two fundamental issues preventing their facile characterization at single-particle level by optical microscopy. First, because their scattering cross-section is extremely small, they can hardly stand out from the background, representing a detection challenge. Second, because of their size being much smaller than the optical diffraction limit, resolving individual units among a group of nanoparticles within close proximity is difficult, posing a resolution challenge<sup>1</sup>. To overcome the detection challenge, dark-field illumination has been employed while suffering low light throughput thus slow imaging speed<sup>2,3</sup>. To circumvent the resolution challenge, recent advances in superresolution imaging have gained considerable ground, but are limited to fluorescence microscopy<sup>4</sup>. Non-fluorescent nanoparticles can flow through one by one in flow cytometry so there is no need to resolve<sup>5</sup>. This type of serial measurement is usually in the dark-field mode with limited throughput. To increase throughput, intense light illumination has to be employed which could introduce adverse effects. Using a single-pixel detector, they cannot take advantage of the rapid advances in camera technology for high-throughput, high-information content (HIC) imaging. In addition, any flow-through technology can only measure the nanoparticle as it travels by the detection area. This prevents timelapse monitoring of the same nanoparticles. Besides, once a nanoparticle is measured, it is difficult to retrieve it for any additional measurement or processing. For label-free measurements, e.g., darkfield scattering, there is a lack of molecular information—only particle count and size distribution can be obtained<sup>6</sup>. Label-free optical techniques also include interferometric scattering microscopy (iSCAT)<sup>7,8</sup> and Interferometric Reflectance Imaging Sensor (IRIS)<sup>9</sup>. Although iSCAT has been shown to detect single molecules and gold particles as small as 2 nm<sup>10</sup>, it generally does not provide size information and thus has been primarily employed for tracking applications. IRIS is based on traditional interference technique so the surface sensitivity is lower than plasmonic techniques. Nevertheless, both iSCAT and IRIS require an interferometry setup and a high-quality laser or LED. Labeled techniques require additional labeling and washing procedures of reporter labels such as fluorescent dyes, quantum dots, and gold nanoparticles, which increases complexity and cost<sup>11</sup>. Fluorescence imaging, a commonly used labeled technique in biology, still faces challenges in imaging biological nanoparticles such as extracellular nanovesicles and viruses detection due to insufficient fluorescent photons and photobleaching.

Light excited surface plasmons (SP) have become the basis of many optical imaging and sensing techniques<sup>12</sup>. Relying on propagating surface plasmon polariton (SPP), surface plasmon resonance (SPR) is a highly effective mechanism to detect minute refractive index (RI) changes on a gold thin film<sup>13</sup>. Because most detection targets have a RI higher than that of the ambient medium (e.g., air or water), SPR can detect surface binding without "labeling" with reporters such as fluorescent dyes, bypassing many potential labeling associated issues. Surface plasmon resonance imaging (SPRI) broadens the repertoire of SPR sensing by incorporating an imaging component<sup>14-16</sup>. However, SPRI typically cannot achieve diffraction-limited lateral resolution with respect to the excitation wavelength due to the wave propagating nature of SPP that "smears" the point spread function. Recently, improved spatial resolution has been demonstrated by interferometric SPRI with image processing 17. The concept of digital holography has also been implemented to image single nanoparticles by SPR with near-field optics<sup>18</sup>. Longitudinally, the evanescent field of SPP extends into the medium with

a 1/e distance ~240 nm, which can be considered as the first-order approximation of its sensing range above the gold film<sup>16,19–21</sup>. A predominant SPRI instrument configuration is based on the Kretschmann design where a prism is employed to provide total internal reflection (TIR) excitation, a required condition for momentum matching. It is worth noting that SPRI can only sense a few hundreds of nanometers above the gold surface, so it requires another imaging modality for the parts of specimen outside of this distance. For example, a standard SRPI system constructed based on an inverted microscope requires two light sources, one to provide the bottom-up TIR excitation, and the other a top-down transmission illumination<sup>21</sup>. If a single camera is employed for detection, it must be time-shared by the two imaging modalities.

Localized surface plasmons (LSP), in contrast, refers to nonpropagating SPs localized in metallic nanostructures and nanoparticles with a size comparable or smaller than the excitation wavelength<sup>12</sup>. Similar to SPR, LSPR is also sensitive to the surface RI changes and has been heavily pursued in optical sensing of surface molecular binding<sup>22,23</sup>. Due to the non-propagating nature of LSP, LSPR imaging (LSPRI) would address a key drawback in SPRI by eliminating the smearing effect, thus making diffraction-limited lateral resolution possible<sup>24</sup>. Longitudinally, LSPRI also features shorter sensing distance from the surface, which can provide better sensitivity toward the surface compared to SPRI<sup>19,25</sup>. Nevertheless, these tantalizing capabilities have not been fully realized. To date, LSPRI embodiments utilize colloidal nanoparticles or nanostructured substrates as sparse sensing units in the form of dark-field scattering microscopy 25,26. In the former case where colloidal nanoparticles are employed, their distribution is not pre-arranged nor controllable 27,28. In the latter case, arrays of sparsely distributed nanostructures such as pillars, posts, spikes, etc., have prevented continuous lateral (i.e., in the x-yplane) sampling<sup>29,30</sup>. Compared to how SPRI is employed, where the gold substrate surface can be 100-percent utilized for continuous sampling, the existing LSPRI can only yield laterally sparse images with small imaging fill factor. Failure to supply continuous sampling has several drawbacks such as lower efficiency, missing spatial context, and "blind" to anything outside the sensing near-field both laterally and longitudinally.

In this paper, we demonstrate ultra-near-field index modulated plasmonic nano-aperture label-free imaging (PANORAMA) that addresses existing issues for present SPRI and LSPRI techniques. On one hand, PANORAMA can produce diffraction-limited lateral resolution free of the previously mentioned smearing effect in SPRI. PANORAMA also has higher surface sensitivity due to the LSPR decay length being shorter than that of SPR. Its system configuration is identical to a standard bright-field microscope using a transillumination tungsten-halogen lamp. Therefore, PANORAMA simultaneously images everything within the microscope objective's depth of focus with a single lamp source and a single camera. However, the intensity ratio increases as the target becomes closer to the imaging substrate. Furthermore, PANORAMA addresses the sparse sampling issue in dark-field LSPRI and provides dense sampling with a large imaging fill factor. In other words, our technique can provide a panoramic view of both laterally and longitudinally—overcoming the lack of imaging depth for both SPRI and LSPRI, and the insufficient lateral sampling for LSPRI. PANORAMA is demonstrated on a high-density Arrayed Gold Nanodisk on Invisible Substrate (AGNIS) measuring 360 nm in diameter, 50 nm in thickness, and 100 nm in edge-to-edge distance. AGNIS has been fabricated using nanosphere lithography followed by a self-aligned substrate undercut. Partial substrate removal to alter LSPR was demonstrated in the literature<sup>31,32</sup>. However, given the relatively large nanodisk dimensions, our AGNIS (Supplementary Fig. 1a-d) features significantly blue-shifted LSPR extinction peak due to

both far-field plasmonic coupling and substrate undercut<sup>31–34</sup>. The blue-shifted LSPR peak provides better diffraction-limited resolution and utilization of high quantum yield in silicon-based cameras. We demonstrate the ability of PANORAMA to image dielectric nanoparticles as small as 25 nm by a standard transmission bright-field microscope with a tungsten-halogen lamp. In addition to ultrahigh sensitivity to deep sub-100 nanoparticles, PANORAMA can also provide their size information. Furthermore, using the arrival time difference in a dynamic imaging mode, individual nanoparticles in a cluster with interparticle distance well below the diffraction limit of the current optical

system (330 nm) can be counted. Moreover, the longitudinal distance between a nanoparticle and AGNIS can be monitored using the dynamic imaging mode.

# Results

**Principle of PANORAMA**. The light scattering cross-section ( $\sigma_{\rm scatt}$ ) of a spherical particle is proportional to the 6th power of the particle diameter (d) given by  $\sigma_{\rm scatt} = (2\pi^5 d^6 n_{\rm med}^4/3 \lambda_{\rm inc}^4)^* |(m^2-1)/(m^2+2)|^2$ , where  $n_{\rm med}$  is the refractive index of the medium surrounding the particle, and

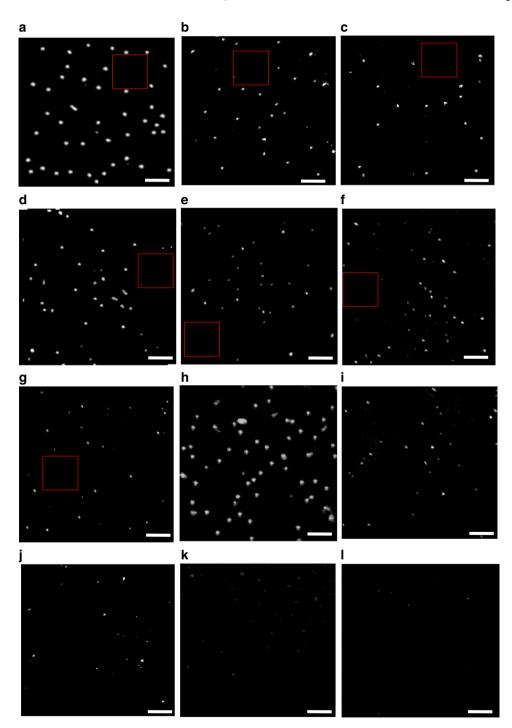
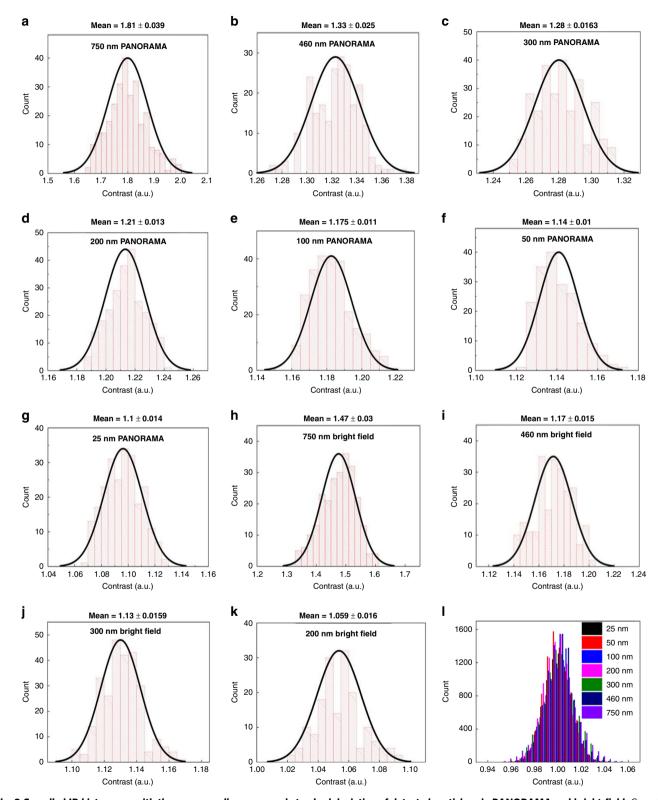


Fig. 1 Images of detected particles via PANORAMA and bright-field. PANORAMA images of PS beads: a 750 nm, b 460 nm, c 300 nm, d 200 nm, e 100 nm, f 50 nm, and g 25 nm. Bright-field images of PS beads: h 750 nm, i 460 nm, j 300 nm, k 200 nm, and l 100 nm. The squared regions are where the background IR was calculated in Fig. 2I. Scale bar: 5 μm.

m is the ratio of the refractive indices of the particle and medium<sup>1,5,17</sup>. Unlike most light scattering techniques, PANORAMA does not solely rely on scattered light to detect nanoparticles.

With the transillumination geometry, the camera receives transmitted light passing through the AGNIS after a bandpass filter. The bandpass filter is located near the half-max wavelength on



**Fig. 2** Compiled IR histograms with the corresponding mean and standard deviation of detected particles via PANORAMA and bright-field. Compiled IR histograms of detected PS beads by PANORAMA: a 750 nm (n = 10), b 460 nm (n = 5), c 300 nm (n = 5), d 200 nm (n = 5), e 100 nm (n = 10), f 50 nm (n = 5), and g 25 nm (n = 10). Compiled IR histograms of detected particles by bright-field: h 750 nm (n = 10), i 460 nm (n = 5), j 300 nm (n = 5), and k 200 nm (n = 5). I Corresponding IR histogram of the background from the squared regions in Fig. 1. Each particle size detection was repeated n times. All particles detected from all experiments (n) are used to plot the IR histogram and calculate the mean and standard deviation.

the left shoulder of the AGNIS's LSPR extinction curve (Supplementary Fig. 1c). When an imaging target resides outside the AGNIS's longitudinal sensing range, i.e., too far away from the surface, it will show up as a standard light scattering object with its intensity reduced when transmitted through the AGNIS. However, as the imaging target approaches AGNIS, the elevated local RI causes the LSPR extinction curve to redshift. The LSPR redshift causes increased light transmission within the imaging wavelength range and acts as if a virtual nano-aperture is formed right beneath the target. We emphasize that the nano-aperture allows higher transmission for both the nanoparticle scattered light and the unscattered incidence light. In other words, unlike most scattering-based imaging techniques, PANORAMA relies on unscattered light to detect nanoparticles smaller than 100 nm. A quantitative study can be found in Supplementary Fig. 3, where differential light transmission via PANORAMA is compared to the LSPR shift for different particle sizes. However, it is critically important to recognize that the increased transmission of the unscattered incidence light is crucial for detecting weakly scattering nanoparticles (sizes < 200 nm).

Nanoparticle detection. Polystyrene (PS) bead sizes of 750, 460, 300, 200, 100, 50, and 25 nm were used to show PANORAMA's

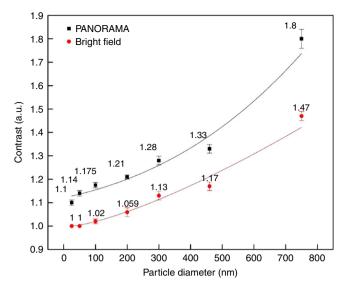


Fig. 3 IR vs. nanoparticle diameter via PANORAMA (black squares) and by bright-field microscopy (red circles). The curves are provided for visual guidance. The averages and error bars were calculated from the points used to plot histograms in Fig. 2.

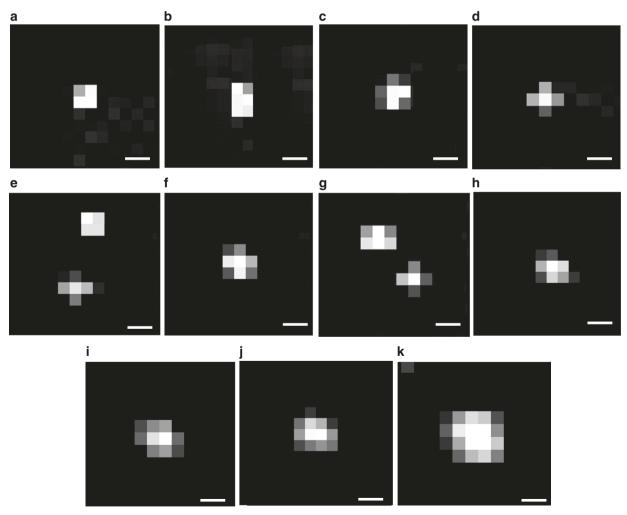


Fig. 4 Detected particle pixel illumination grid via PANORAMA. a-d 25 nm, e 50 nm, f 100 nm, g 200 nm, h, i 300 nm, j 460 nm, and k 750 nm PS bead particle size. Scale bar: 390 nm.

performance in detecting tiny phase objects. A ratiometric image ("intensity ratio") is obtained by dividing the image after nanoparticle settlement by the image without nanoparticles. For a control experiment where a ratiometric image is obtained by dividing two images without nanoparticles, resulting in an image histogram with a mean of 1 and a standard deviation of 0.013, which is used as a baseline intensity ratio (IR) image. A threshold IR value is selected to be  $1 + 3 \times 0.013 \sim 1.04$ . Assuming Gaussian statistics, an IR value larger than 1.04 indicates particle detection with a p-value < 0.001. Figure 1a-g shows PANOMARA images of nanoparticles of all sizes after the thresholding process. To compare PANORAMA's performance with standard bright-field microscopy, all PS bead sizes were imaged on a glass coverslip using the same setup (Fig. 1h-l). PANORAMA provides images of detected beads of all sizes (Fig. 1a-g). In contrast, bright-field images (Fig. 1h-l) show a gradual decrease in intensity toward smaller bead size, and no detection can be made for 100 nm (Fig. 11) and smaller beads (not shown).

Figure 2 shows a histogram analysis constructed from IR values recorded from all detected nanoparticles in Fig. 1 and control experiments. By applying a gaussian fit, the mean IR values by PANORAMA were 1.81, 1.33, 1.28, 1.22, 1.175, 1.14, and 1.1 for decreasing nanoparticle size (Fig. 2a–g), while the values from bright-field microscopy were 1.47, 1.17, 1.13, 1.06, 1.02, 1, and 1 (Fig. 2h–k). As mentioned earlier, an IR value smaller than 1.04 is considered not detectable. Considering the smallest PS bead size

of 25 nm, PANORAMA provides an IR of 1.1 with sigma 0.014, which is well separated from the background histograms which centers at 1 with sigma 0.0131 (Fig. 2l), suggesting the potential of detecting even smaller particles or single molecules. Overall, PANORAMA has been shown to detect PS bead sizes down to 25 nm, whereas bright-field microscopy cannot detect beads equal or smaller than 100 nm.

Considering the ability of PANORAMA to detect sizes reaching 25 nm, it cannot spatially resolve nanoparticle sizes below the diffraction limit. However, the mean and standard deviation of the histograms shows a correlation between nanoparticle size and IR where increasing nanoparticle size registers larger IR. Figure 3 illustrates the image IR vs. nanoparticle size extracted from Fig. 2 for both PANORAMA (black squares) and bright-field microscopy (red circles). It is observed that PANORAMA maintains a larger IR from 11 to 22% among various nanoparticles size. It is remarkable to note that PANAROMA's IR continues to decrease for nanoparticle smaller than 300 nm, suggesting that PANORAMA can provide size information beyond the diffraction-limited resolution.

It is worth noting that PANORAMA has better contrast over IRIS for nanoparticle smaller than about 120 nm. For example, PANORAMA provides a contrast of ~14% for 50 nm PS nanoparticles while IRIS has a contrast ~2%. In addition, PANORAMA maintains ~10% contrast for 25 nm PS nanoparticles but IRIS has already reached the noise floor<sup>35</sup>. These results should not be too surprising. It is well-known that LSPR has

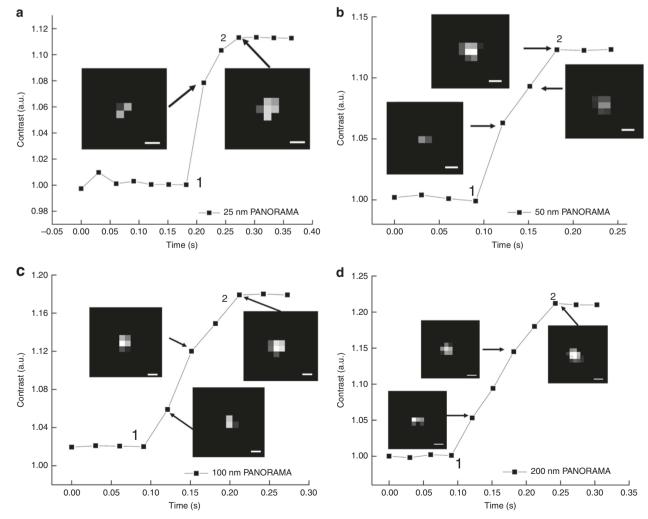


Fig. 5 Continued

much better surface sensitivity than SPR and traditional interferometry.

PANORAMA nano-aperture size dependence on nanoparticle size. An interesting property of PANORAMA lies in the nanoaperture size dependence on the nanoparticle size. The smallest achievable aperture size is roughly the gold disk diameter of 360 nm, which is comparable to the diffraction-limited resolution (330 nm) and larger than the equivalent EMCCD pixel size (195 nm) at the sample plane. We note that the gold disks can be made smaller than both the diffraction-limited resolution and the camera pixel size. Figure 4a-d shows images of detected 25 nm PS beads, where a single pixel with the highest IR can be found to be accompanied with several surrounding lower IR pixels. The pattern varies according to the specific positions of the gold disk with respect to the EMCCD pixel grid, and to a certain degree the relative position of the PS bead on the gold disk. The minimum pattern size is equivalent to a patch of 2 × 2 pixels (Fig. 4a), but most detected nanoparticles appear in a patch of  $3 \times 3$  pixels (Fig. 4c, d). PS bead sizes of 50, 100, 200, and 300 nm show similar patterns as 25 nm PS beads (Fig. 4e-h), suggesting the nanoparticle caused the LSPR of a single gold disk to red-shift in most cases. When the nanoparticle size becomes comparable to the gold disk, e.g., 300 nm PS beads, the pattern can occasionally

appear as a slightly larger patch (Fig. 4i). A plausible explanation is as the nanoparticles become larger, the probability increases for a single nanoparticle to causes LSPR shift for the adjacent disk(s). Nano-aperture across multiple gold disks becomes more apparent for larger nanoparticles as shown in Fig. 4j for 460 nm and Fig. 4k for 750 nm, respectively. The sampling density can be improved by higher magnification and smaller camera pixels, which will be investigated in the future.

Interpreting nanoparticle to surface distance by dynamic monitoring. A key strength of PANORAMA is its outstanding light throughput, which enables dynamic imaging at millisecond timescale. To demonstrate this experimentally, we performed dynamic imaging at 33 Hz frame rate and 10 ms integration time per frame during nanoparticle settling. We note that the frame rate is limited by preventing the camera from overheating. Similar IR values have been obtained from 25 nm PS beads with as little as 1 ms integration time, suggesting the potential of reaching kHz frame rate. Figure 5a–g shows the IR values of various size PS beads as they settle on the AGNIS. Nanoparticle settling time ( $\tau$ ) can be defined as the travel time between the nanoparticle is first detected and IR plateau (complete settlement) as shown in Fig. 5a–g, suggesting a trend of increased  $\tau$  with increased nanoparticle size (Fig. 5h). Assuming the settling speed does not

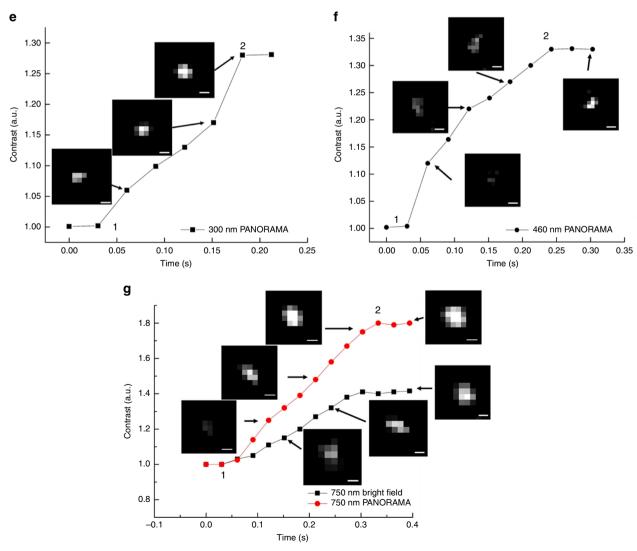
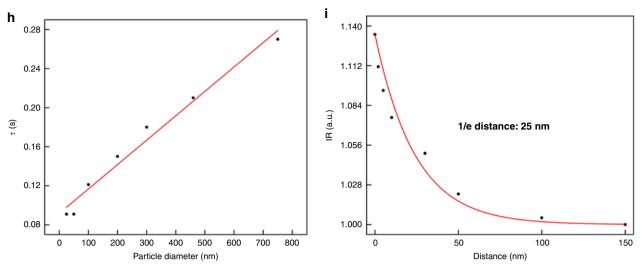
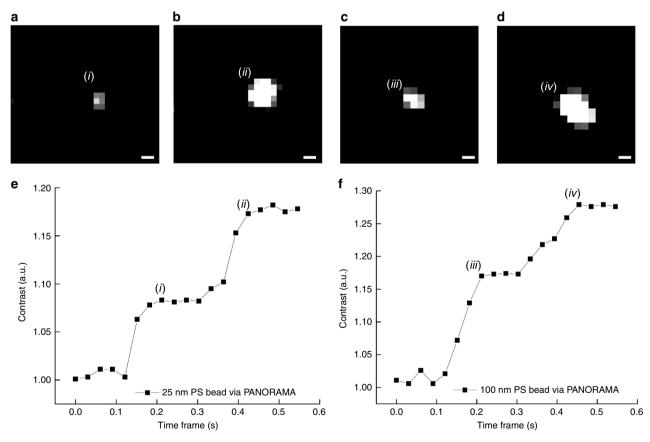


Fig. 5 Continued

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**Fig. 5 Particle size vs. settlement time on AGNIS.** PANORAMA IR change of **a** 25 nm, **b** 50 nm, **c** 100 nm, **d** 200 nm, **e** 300 nm, and **f** 460 nm PS beads as it settles on AGNIS. **g** The IR change of 750 nm PS bead as it settles on the surface via PANORAMA (red) and via bright-field imaging (black). **h** Particle settlement time ( $\tau$ ) vs. particle size.  $\tau$  was calculated from the points labeled 1 to 2 for all particle sizes in (**a-g**). **i** FDTD simulation of IR vs. distance between a 50 nm particle and AGNIS. Scale bar: 390 nm.



**Fig. 6 Particle differentiation in a cluster. a**, **b** Detected 25 nm PS bead at time frame i and ii in (**e**). **c**, **d** Detected 100 nm PS bead at time frame iii and iv in (**f**). Dynamic monitoring of IR vs. time where two **e** 25 nm and **f** 100 nm PS beads settle at the same location. Scale bar: 390 nm.

strongly depend on size, the larger  $\tau$  for larger nanoparticles suggests that they can be detected farther away from the AGNIS surface. The plateau IR values for all particle sizes agree well with the previously established values after nanoparticle settlement (Fig. 3). To gain more insight on the surface sensitivity of

PANORAMA, we performed finite difference time domain (FDTD) simulations where a 50 nm PS nanoparticle was placed at various distances from the AGNIS. As shown in Fig. 5i, the IR of the particle increases as the nanoparticle becomes closer to AGNIS with a 1/e distance of 25 nm. Interpreting the 50 nm

nanoparticle results in Fig. 5b in the light of the simulated results, the nanoparticle was outside the detectable distance (~100 nm) from the AGNIS surface prior to  $t \sim 99$  ms, after which it moved toward the AGNIS and arrived at the surface at  $t \sim 190$  ms. As shown previously, 50 nm PS nanoparticle does not provide detectable light scattering in the bright-field imaging mode, suggesting the settling process was imaged entirely by PANAR-OMA. In contrast, larger nanoparticle (e.g., >100 nm) can provide detectable light scattering as long as the nanoparticle enters the imaging system depth of focus (DOF)  $\sim +-413$  nm. In other words, larger nanoparticles can be first detected when they are significantly farther away from the AGNIS surface entirely due to its own light scattering. In the case of 750 nm nanoparticles (Fig. 5g), it first entered the DOF at  $t \sim 66$  ms, then moved toward the AGNIS surface and arrived at  $t \sim 333$  ms. It is remarkable that PANORAMA contributes additional IR even for larger nanoparticles as shown in Fig. 5g. The time for the 750 nm PS bead to settle on both the glass coverslip and AGNIS's surface is the same, however, the slope of the IR vs. time curve for PANORAMA is significantly higher than that of the standard bright-field image, indicating higher distance sensitivity.

These results suggest that the  $\tau$  during nanoparticle settlement can provide an additional means for nanoparticle sizing. They also suggest that it is possible to monitor the distance between the nanoparticle and AGNIS and obtain velocity with a resolution far better than the diffraction limit provided careful calibration and higher imaging speed.

The dynamic imaging capability can be further exploited to count nanoparticle clusters with interparticle distance smaller than the diffraction limit. Counting is achieved by monitoring the IR fluctuations over time. As shown in Fig. 6a where a 25 nm PS bead was initially settled on the surface at time *i*, followed by a second bead settling into the same region at time *ii* and formed a cluster (Fig. 6b). The process is evident by monitoring the IR over time in Fig. 6e where the first bead shows a typical IR value for a single 25 nm PS bead. At time *ii*, the IR jump indicates the settlement of a second particle. The same behavior can be seen for 100 nm PS bead in Fig. 6c, d, and f.

# **Discussion**

Plasmonic nano-aperture label-free imaging (PANORAMA) has been demonstrated as a novel nanoparticle imaging technique. Its basic principle stems from virtual nano-apertures modulated by ultra-near-field refractive index. Instead of measuring the light scattered by the nanoparticle, which diminishes dramatically with reducing size, PANORAMA detects both the scattered and unscattered light modulated by the nano-aperture, thus enjoys unprecedented sensitivity. PANORAMA addresses several limitations in existing SPR and LSPR imaging techniques by providing a large lateral imaging fill factor and extended longitudinal imaging range while achieving diffraction-limited imaging resolution. Its system configuration is identical to a standard brightfield microscope using a transillumination tungsten-halogen lamp instead of lasers or other high-intensity light sources, and a single camera. The bright-field approach provides much higher light throughput for dynamic imaging at the millisecond timescale compared to dark-field microscopy that suffers low light throughput. We have demonstrated that PANORAMA can size single nanoparticle down to 25 nm which exceeds the 100 nm dielectric particle detection limit achieved via dark-field microscopy<sup>3</sup>, dynamically monitor single nanoparticle approaching the plasmonic surface, and count individual nanoparticles in a cluster. PANORAMA would provide new capabilities in label-free imaging and single nanoparticle analysis. More importantly, molecular imaging can be envisioned with a functionalized

AGNIS surface for single biological nanoparticle analysis including extracellular vesicles such as exosomes<sup>36</sup> and viruses.

#### Methods

**Materials.** Polystyrene beads of sizes 25, 50, 100, 200, 300, 460, and 750 nm were purchased from Sigma-Aldrich. Ethanol (200 proof) was purchased from Decon Laboratories, Inc. Gold sputtering target was purchased from ACI Alloys, Inc. Argon gas (99.999%) was used for RF-sputter etching.

**Fabrication of AGNIS**. Fabrication steps involve deposition of 2 nm of Titanium as an adhesion layer and then 80 nm of the gold film using electron-beam evaporation. A monolayer of polystyrene beads of average diameter 460 nm was assembled over the gold film. The substrate was exposed to oxygen plasma etching to shrink the size of the polystyrene beads, followed by Argon Ion milling to etch away the uncovered part of the gold. The polystyrene beads were washed away via sonication. This generated a two-dimensional polycrystalline array of gold nanodisks with an average diameter of 360 nm with a pitch size (center-to-center distance) of 460 nm. This gold nanodisk array was immersed in a buffer HF to undercut the glass substrate beneath the disks (Supplementary Fig. 1a, b). The LSPR extinction peak of AGNIS is at 620 nm in air and 690 nm in water (Supplementary Fig. 1c). The gold nanodisks occupy ~55% of the total substrate footprint. However, this is a conservative estimate because the LSPR electromagnetic field extends further away from the edges of nanodisk. As shown in Fig. 5i, the 1/e distance for lateral electric field decay is ~30 nm, which brings the effective lateral imaging fill factor to ~75%.

**Optical setup.** White light from a tungsten-halogen lamp passes through a condenser (IX-LWUCD, Olympus) and illuminates the sample on an inverted microscope (IX71, Olympus). The transmitted light passes through an infinity-corrected 60X water immersion lens with a 1.2 numerical aperture (UPLSA-PO60XW, Olympus). The light exiting the side-port is relayed to an electron-multiplied charge-coupled device (EMCCD; ProEM 1024, Princeton Instruments) via a 4f system, where a bandpass filter with 650-670 nm passband (FB660-10, Thorlabs) at its Fourier plane (Supplementary Fig. 2).

### **Data availability**

The data that support the findings of this study are available from the corresponding authors upon request.

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#### References

- Bohren, C. F. & Huffman, D. R. Absorption and Scattering of Light by Small Particles (John Wiley & Sons, 2008).
- Fu, Y. H., Kuznetsov, A. I., Miroshnichenko, A. E., Yu, Y. F. & Luk'yanchuk, B. Directional visible light scattering by silicon nanoparticles. *Nat. Commun.* 4, 1–6 (2013).
- Wagner, T., Lipinski, H.-G. & Wiemann, M. Dark field nanoparticle tracking analysis for size characterization of plasmonic and non-plasmonic particles. *J. Nanopart. Res.* 16, 2419 (2014).
- Betzig, E. et al. Imaging intracellular fluorescent proteins at nanometer resolution. Science 313, 1642–1645 (2006).
- Zhu, S. et al. Light-scattering detection below the level of single fluorescent molecules for high-resolution characterization of functional nanoparticles. ACS Nano 8, 10998–11006 (2014).
- Wang, F. et al. Scattered light imaging enables real-time monitoring of labelfree nanoparticles and fluorescent biomolecules in live cells. *J. Am. Chem. Soc.* 141, 14043–14047 (2019).
- Arroyo, J. O., Cole, D. & Kukura, P. Interferometric scattering microscopy and its combination with single-molecule fluorescence imaging. *Nat. Protoc.* 11, 617–633 (2016).
- Piliarik, M. & Sandoghdar, V. Direct optical sensing of single unlabelled proteins and super-resolution imaging of their binding sites. *Nat. Commun.* 5, 1–8 (2014).
- Daaboul, G. G. et al. Digital detection of exosomes by interferometric imaging. Sci. Rep. 6, 37246 (2016).
- Taylor, R. W. & Sandoghdar, V. in Label-Free Super-Resolution Microscopy 25–65 (Springer, 2019).
- Jin, D. et al. Nanoparticles for super-resolution microscopy and singlemolecule tracking. Nat. Methods 15, 415–423 (2018).
- Maier, S. A. Plasmonics: Fundamentals and Applications (Springer Science & Business Media, 2007).
- 13. Raether, H. Surface plasmons. Springe. Tracts Mod. Phys. 111, 1 (1988).

- Maley, A. M., Lu, G. J., Shapiro, M. G. & Corn, R. M. Characterizing single polymeric and protein nanoparticles with surface plasmon resonance imaging measurements. ACS Nano 11, 7447–7456 (2017).
- Shan, X. et al. Imaging the electrocatalytic activity of single nanoparticles. Nat. Nanotechnol. 7, 668–672 (2012).
- 16. Brolo, A. G. Plasmonics for future biosensors. Nat. Photonics 6, 709 (2012).
- Yang, Y. et al. Interferometric plasmonic imaging and detection of single exosomes. Proc. Natl Acad. Sci. USA 115, 10275–10280 (2018).
- 18. Nelson, J. W., Knefelkamp, G. R., Brolo, A. G. & Lindquist, N. C. Digital plasmonic holography. *Light.: Sci. Appl.* 7, 1–11 (2018).
- Otte, M. A. et al. Identification of the optimal spectral region for plasmonic and nanoplasmonic sensing. ACS Nano 4, 349–357 (2010).
- Shan, X. et al. Measuring surface charge density and particle height using surface plasmon resonance technique. Anal. Chem. 82, 234–240 (2010).
- Shan, X., Patel, U., Wang, S., Iglesias, R. & Tao, N. Imaging local electrochemical current via surface plasmon resonance. *Science* 327, 1363–1366 (2010).
- Willets, K. A. & Van Duyne, R. P. Localized surface plasmon resonance spectroscopy and sensing. Annu. Rev. Phys. Chem. 58, 267–297 (2007).
- Sepúlveda, B., Angelomé, P. C., Lechuga, L. M. & Liz-Marzán, L. M. LSPR-based nanobiosensors. Nano Today 4, 244–251 (2009).
- 24. Fritzsche, J. et al. Single particle nanoplasmonic sensing in individual nanofluidic channels. *Nano Lett.* **16**, 7857–7864 (2016).
- Chen, P. et al. Multiplex serum cytokine immunoassay using nanoplasmonic biosensor microarrays. ACS Nano 9, 4173–4181 (2015).
- Liang, K. et al. Nanoplasmonic quantification of tumour-derived extracellular vesicles in plasma microsamples for diagnosis and treatment monitoring. *Nat. Biomed. Eng.* 1, 1–11 (2017).
- Kawawaki, T., Zhang, H., Nishi, H., Mulvaney, P. & Tatsuma, T. Potential-scanning localized plasmon sensing with single and coupled gold nanorods. *J. Phys. Chem. Lett.* 8, 3637–3641 (2017).
- Howes, P. D., Chandrawati, R. & Stevens, M. M. Colloidal nanoparticles as advanced biological sensors. Science 346, 1247390 (2014).
- Raghu, D. et al. Nanoplasmonic pillars engineered for single exosome detection. PLoS ONE 13, e0202773 (2018).
- Shen, B. et al. Plasmonic nanostructures through DNA-assisted lithography. Sci. Adv. 4, eaap8978 (2018).
- Zhao, F., Arnob, M. M. P., Zenasni, O., Li, J. & Shih, W.-C. Far-field plasmonic coupling in 2-dimensional polycrystalline plasmonic arrays enables wide tunability with low-cost nanofabrication. *Nanoscale Horiz.* 2, 267–276 (2017).
- 32. Dmitriev, A. et al. Enhanced nanoplasmonic optical sensors with reduced substrate effect. *Nano Lett.* **8**, 3893–3898 (2008).
- Aćimović, S. S. et al. Superior LSPR substrates based on electromagnetic decoupling for on-a-chip high-throughput label-free biosensing. *Light.: Sci. Appl.* 6, e17042–e17042 (2017).
- Misbah, I. & Shih, W.-C. in Bio-Optics: Design and Application. DW2B. 2 (Optical Society of America, 2019).

- Daaboul, G. G. et al. Enhanced light microscopy visualization of virus particles from Zika virus to filamentous ebolaviruses. PLoS ONE 12, e0179728 (2017).
- Ohannesian, N. et al. Commercial and emerging technologies for cancer diagnosis and prognosis based on exosomal biomarkers. J. Phys. Photon. 2, 032002 (2020).

#### Author contributions

W.-C.S. conceived the idea and directed the study. N.O. and W.-C.S. designed the experiment and analyzed the data. N.O. performed the experiment and produced the figures. I.M. fabricated the AGNIS and performed FDTD simulations. N.O., S.H.L., and W.-C.S. provided substantial input to the project and to the writing of the manuscript.

# **Competing interests**

The authors declare no competing interests.

#### **Additional information**

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