OPEN

Heart Rate Detrended Fluctuation Indexes as Estimate of Obstructive Sleep Apnea Severity

Eduardo Luiz Pereira da Silva, MSc, Rafael Pereira, PhD, Luciano Neves Reis, MD, Valter Luis Pereira Jr., MD, Luciana Aparecida Campos, PhD, Niels Wessel, PhD, and Ovidiu Constantin Baltatu, MD, PhD

Abstract: In the present study, we aimed at investigating a heart rate variability (HRV) biomarker that could be associated with the severity of the apnea–hypopnea index (AHI), which could be used for an early diagnosis of obstructive sleep apnea (OSA).

This was a cross-sectional observational study on 47 patients (age 36 ± 9.2 standard deviation) diagnosed with mild (23.4%), moderate (34%), or severe (42.6%) OSA. HRV was studied by linear measures of fast Fourier transform, nonlinear Poincaré analysis, and detrended fluctuation analysis (DFA)—DFA α 1 characterizes short-term fluctuations, DFA α 2 characterizes long-term fluctuations. Associations between polysomnography indexes (AHI, arousal index [AI], and oxygen desaturation index [ODI]) and HRV indexes were studied.

Patients with different grades of AHI had similar sympathovagal balance levels as indicated by the frequency-domain and Poincaré HRV indexes. The DFA α 2 index was significantly positive correlated with AHI, AI, and ODI (Pearson *r*: 0.55, 0.59, and 0.59, respectively, with P < 0.0001). The ROC analysis revealed that DFA α 2 index predicted moderate and severe OSA with a sensitivity/specificity/area under the curve of 0.86/0.64/0.8 (P = 0.005) and 0.6/0.89/0.76 (P = 0.003), respectively.

Our data indicate that the DFA α 2 index may be used as a reliable index for the detection of OSA severity.

(Medicine 94(4):e516)

Abbreviations: AHI = apnea-hypopnea index, AI = arousal index, ANS = autonomic nervous system, DFA = detrended fluctuation

Editor: Bernhard Schaller.

- Correspondence: Ovidiu Constantin Baltatu, MD, PhD, Center of Innovation, Technology, and Education—(CITE), Camilo Castelo Branco University (UNICASTELO), Av. Dr Altino Bondensan 500, Eugenio de Melo, São José dos Campos-SP 12247-016, Brazil (e-mail: ocbaltatu@gmail.com).
- OCB, ELPS: study conception and design; LNR, ELPS: acquisition of data; RP, VLP, LAC, ELPS, LNR, NW, OCB: analysis and interpretation of data; OCB, LAC: drafting of manuscript; and NW, ELPS, RP, LNR, VLP: critical revision.
- This study was supported by the State of São Paulo Research Foundation (FAPESP 13/14724-0, 13/06698-0) and the National Council for Scientific and Technological Development (CNPq 301706/2013-1).
- The authors have no conflicts of interest to disclose.

Copyright © 2015 Wolters Kluwer Health, Inc. All rights reserved.

This is an open access article distributed under the Creative Commons Attribution License 4.0, which permits unrestricted use, distribution, and reproduction in any medium, provided the original work is properly cited. ISSN: 0025-7974

DOI: 10.1097/MD.000000000000516

analysis, ECG = electrocardiogram, HF = high frequency, HRV = heart rate variability, LF = low frequency, ODI = oxygen desaturation index, OSA = obstructive sleep apnea, PSG = polysomnography, ROC = receiver–operator characteristic.

INTRODUCTION

bstructive sleep apnea (OSA) is the most common form of sleep apnea and it is characterized by partial or complete blockage of the upper airway during sleep. According to the frequency of apnea/hypopnea events per hour (ie, apneahypopnea index [AHI]) determined through polysomnography (PSG), OSA has been categorized to mild, moderate, or severe level of breathing and sleep disturbance.¹ OSA is considered as a considerable risk factor for cardiovascular morbidity.^{2,3} Major pathophysiologic mechanisms responsible for cardiovascular complications associated to OSA include activation of the autonomic nervous system (ANS).² The impact of OSA on ANS has been extensively studied and continues to be a subject of actual interest. The alterations of the cardiovascular ANS arise subsequently to the upper airway collapse-induced apneic and hyperventilation phases during sleep. Heart rate variability (HRV) algorithms have been used to study the cardiac ANS under various pathophysiological conditions for potential early diagnosis, prognosis, or risk stratification of diseases.^{4,5} These HRV algorithms were employed to investigate the ANS responses to different types of sleep apnea in normal and sleep apnea subjects^{6,7} and detect abnormal breathing events.⁸ Most of these studies analyzed the heart rate extracted from specific sleep segments (or time windows) associated with apnea/hypopnea events or different sleep stages. In the present study, we aimed at identifying a HRV biomarker that could be correlated with the severity of OSA, which could be directly detected from a full-length of sleep electrocardiogram (ECG) without the need of preliminary detection and segmentation in sleep apnea time windows. For this, besides linear algorithms, we employed nonlinear analyses of HR dynamics that are able to detect long-range correlations in noisy, nonstationary time series. Those included Poincaré plots and detrended fluctuation analysis (DFA) that may detect pathophysiologic information that is not achieved by conventional HR variability analysis.¹³

MATERIALS AND METHODS

Study Design and Setting

All subjects were referred to the Sleep Institute of Itaperuna, Rio de Janeiro, Brazil, for the investigation of possible sleep-disordered breathing. This was a cross-sectional observational study on 47 patients (age 36 ± 9.2 standard deviation [SD]) diagnosed through PSG with mild (23.4%), moderate (34%), or severe (42.6%) OSA between August 2012 and April

Received: December 9, 2014; revised: January 6, 2015; accepted: January 7, 2015.

From the Center of Innovation, Technology, and Education—CITE (ELPS, VLP, LAC, OCB), Camilo Castelo Branco University (UNICASTELO), Sao Jose dos Campos Technology Park, Sao Jose dos Campos; University Iguaçu Campus—V (ELPS), Itaperuna, Rio de Janeiro; Department of Biological Sciences (RP), State University of Southwest Bahia—UESB, Jequie, Bahia; Sleep Institute of Itaperuna (LNR), Rio de Janeiro, Brazil; and Humboldt-Universität zu Berlin (NW), Berlin, Germany.

2013. Patient-level data were anonymized by removing all patient-identifying details and allocating a unique study code to each PSG recording. The study was approved by the Research Ethics Committee of the Faculty of Medical Sciences in accordance with resolution 196/96 and 340/2004 of the National Health Council (Ministry of Health) for research on human beings (CAAE: 01328712.0.0000.5244, permit no. 18326). The study is registered in ClinicalTrials.gov with the registration number: NCT02044900.

Inclusion and Exclusion Criteria

Criteria of selection from the PSG database were males over 18 years of age diagnosed with OSA. Subjects with a history or clinical examination suggestive of hypertension, neuromuscular disease, or any surgical treatment were not considered in the study.

Study Measurements: PSG

PSG monitoring and diagnosis was in accordance with the American Society of Sleep Medicine standards.¹⁴ Standard baseline PSG was performed using a computerized system (iBlue 42; iCelera - Celera Tecnologia em Equipamentos Médicos, Sao Paulo, Brazil). The following extracted signals were measured: 2 electroencephalogram channels (O1-A2, O2-A1, C3-A2, C4-A1), 2 electrooculogram channels, electromyography (EMG; bilateral anterior tibialis), pulse oximetry (arterial oxygen saturation), nasal-oral airflow (thermistors), and ECG derivation DII. The polysomnograms were scored according to the criteria of Rechtschaffen and Kales.¹ Respiratory signals were scored automatically in accordance with current, internationally accepted guidelines.¹⁵ Obstructive apnea was defined as the complete cessation of or a >50%reduction in airflow lasting >10 seconds, accompanied by persistent respiratory effort, with or without oxygen desaturation or arousal. The AHI was defined as the number of obstructive hypopneas and apneas per hour of sleep. Hypopnea was defined as a reduction in airflow of <50% for >10 seconds, detected by thermistor or nasal cannula, accompanied by oxygen desaturation of $\geq 4\%$ or an arousal of ≥ 1.5 seconds. Apnea was defined as an airflow reduction of ≥80% for at least 10 seconds. The oxygen desaturation index (ODI) was defined as the number of events per hour in which oxygen saturation decreased by $\geq 4\%$. Arousal was defined as any electroencephalography frequency shift lasting 3 to 15 seconds during nonrapid eye movement sleep; during rapid eye movement sleep, an increase in EMG was required as well. Arousal index (AI) was defined as the number of arousals per hour of sleep.

Study Measurements: HRV Analysis

Single-lead DII ECG recordings were extracted from polysomnogram measurements. The duration of the recordings was 412 ± 12 minutes. HRV was assessed with the Kubios HRV analysis software (Department of Applied Physics, University of Eastern Finland).¹⁶ HRV was assessed in frequency domain by using a fast Fourier transform spectral analysis; the parameters included were as follows: low frequency (LF; 0.04–0.15 Hz), high frequency (HF; 0.15–0.4 Hz), and LF/ HF ratio. We normalized LFnu and HFnu for analysis so as to minimize the effect on these 2 values by changes in the total power considering them as equivalent carriers of information about sympathovagal balance.¹⁷ The nonlinear properties of HRV were analyzed by Poincaré plots and DFA. In the Poincaré plots, an ellipse was fitted and 2 indexes were calculated: SD1 (the standard deviation of the points perpendicular to the line of identity) and SD2 (the standard deviation along the line of identity). In the DFA method, long-range correlations between interbeat intervals separated by several beats were detected by investigating the scaling behavior of the heartbeat fluctuations on different time scales disregarding trends and nonstationarities in the data.¹⁸ A detailed description of the DFA algorithm and its underlying theory for the analysis of neuronal oscillations was pertinently presented by Hardstone et al¹³ in their recent methods article. We quantified the fractal structure of heart rate by estimating a short-term (α 1, short-term fluctuations, obtained from the range $4 \le n \le 16$) and a long-term (α 2, long-term fluctuations, obtained from the range $16 \le n \le 64$) scaling exponent by DFA.

Statistical Analysis

Data were tested for normality using the D'Agostino and Pearson omnibus normality test. Data normally distributed are represented by mean (standard error), and data that are not normally distributed are represented by median (interquartile range). Differences between 3 distinctive populations were tested using analysis of variance followed by Tukey's multiple comparisons test (P < 0.05 was regarded as being statistically significant). Pearson's correlation coefficient r was used to quantify a relationship between ≥ 2 variables; a 2-tailed *P* value <0.05 was considered statistically significant. A receiveroperator characteristic (ROC) analysis for the HRV index that correlated best with the AHI was performed. To evaluate the efficacy of the HRV index that correlated best with the AHI as a potential tool for diagnosing different grades of obstructive apnea, 2 ROC curves based on a threshold of AHI = 15 (for moderate obstructive apnea) and AHI = 30 (for severe obstructive apnea) were plotted and their areas under the curve were calculated as a measure of the overall efficacy of the diagnostic score. Data were analyzed using statistical software (Prism 6, GraphPad Software, Inc., La Jolla, USA for Mac OS X).

RESULTS

Significant Positive Correlation Between AHI and the Other PSG Indexes

The mild, moderate, or severe OSA was defined according to the AHI (Figure 1A–C). Multiple comparisons revealed significant differences between the severe group and the other 2 groups (mild and moderate) for all PSG indexes AHI, AI, and ODI. The AHI was significantly correlated with AI and ODI (Figure 1D, the Pearson correlation coefficients had values of 0.86 (95% confidence interval [CI]: 0.77 to 0.92) for the AHI to AI correlation and 0.75 (95% CI: 0.60 to 0.85) for the AHI to ODI correlation).

Patients With Different Severity Levels of AHI Have Similar Basal Sympathovagal Balance Levels

Patients with different grades of AHI had similar sympathovagal balance levels, as indicated by the HRV frequency and time-domain indexes. The LFnu, Hfnu, and LF/HF values among the different severity apnea groups were statistically not different (Figure 2A and B). The time-domain indexes SD1 (representing the dispersion of points perpendicular to the line of identity) and SD2 (representing the dispersion of points along



FIGURE 1. (A) AHI, (B) AI, and (C) ODI in obstructive sleep apnea across different degrees of severity according to the AHI: mild (AHI < 15), moderate (15 < AHI < 30), and severe (AHI > 30); #, P < 0.001. (D) Correlations between AHI and the other polysomnography indexes, AI, and ODI. Values are Pearson *r* and 95% CI. AHI = apnea–hypopnea index, AI = arousal index, CI = confidence interval, ODI = oxygen desaturation index.



FIGURE 2. Basal sympathovagal balance levels indicated by (A) and (B) the frequency-domain HRV indexes, and the (C) and (D) timedomain HRV indexes in obstructive sleep apnea across different degrees of severity according to the AHI: mild (AHI < 15), moderate (15 < AHI < 30), and severe (AHI > 30). AHI = apnea–hypopnea index, HF = high frequency, HRV = heart rate variability, LF = low frequency, SD = standard deviation.

the line of identity) were also not statistically different among the different severity apnea groups (Figure 2C and D).

Heart Rate DFA Indexes Correlates in OSA

DFA α 1 values were close to 1.0 (Figure 3A) indicating persistent long-range power-law correlations and suggesting that the fluctuations are generated by complex systems with multiple feedback regulations.^{16,19} The DFA α 1 index was not significantly altered across different OSA severity categories (Figure 3A) and did not correlate with the AHI or with other PSG indexes (Figure 3B). DFA α 2 values were close to 0.5 (Figure 3C) suggesting random dynamics (no correlation) of the R–R interval time series. There was a significant positive correlation of the DFA α 2 index with the AHI and the other PSG indexes (Figure 3D).

Heart Rate DFA α 2 Index Prediction Value for the Severity of OSA

ROC curves were examined to identify the optimal DFA $\alpha 2$ index thresholds that maximize sensitivity and specificity for predicting moderate or severe OSA. Thus, for moderate OSA, the threshold was set to AHI > 15 as dependent variable (Figure 4), using a cutoff for DFA $\alpha 2$ index > 0.32; sensitivity for moderate OSA prediction was 86.11% (95% CI: 70.50 to 95.33) and specificity was 63.64% (95% CI: 30.79 to 89.07). The calculated area under a ROC curve was 0.8 (95% CI: 63 to 94) with significance value of P = 0.005. Setting the threshold to AHI > 30 as dependent variable for severe OSA (Figure 4), the cutoff value for identifying severe OSA patients with DFA $\alpha 2$ index > 0.47 and yielded a sensitivity prediction of 60% (95% CI: 36.05 to 80.88) and specificity 88.89% (95% CI: 70.84 to 97.65). The calculated area under a ROC curve was 0.76 (95% CI: 60 to 90) with significance value of P = 0.003.

DISCUSSION

The major finding of this study is that the heart ratederived DFA $\alpha 2$ index from the full length of sleep ECG can accurately predict moderate or severe OSA. Also, there are significant positive correlations between AHI and the other PSG indexes, ODI and AI.

Agreements between AHI, ODI, and AI were found in our as well as in other studies.²⁰ OSA is defined by episodes of partial or complete collapse of upper airway during sleep (ie, AHI). This causes a decrease or complete cessation of airflow. Consequently, a defective alveolar ventilation results and arterial oxygen saturation may drop (ie, ODI). These events are commonly terminated by arousals (ie, AI). Therefore, it makes sense to detect a statistical correlation between these PSG indexes that may be useful in standardizing PSG equipment and specific scoring approaches for quantifying sleep-related breathing disorders.^{21,22}

In the present study, the frequency (LFnu, HFnu, and LF/HF ratio) and time-domain (SD1 and SD2) HRV indexes from the full length of sleep ECG were not different among the groups with different severity OSA. The normalized LFnu and HFnu frequency-domain indexes and their LF/HF ratio are considered to carry information about sympathovagal balance.¹⁷ The time-domain SD1 appears to be an index of instantaneous beat-to beat variability and SD2 index that characterizes long-term HRV is thought to reflect global autonomic variability.⁴ Although we did not find significant differences among the OSA groups in the frequency (LFnu, HFnu,



FIGURE 3. HRV DFA indexes in different degrees of obstructive sleep apnea and their correlations with polysomnography indexes. (A) and (B) DFA α 1 index has no correlation with the AHI and the other polysomnography indexes. (C) and (D) DFA α 2 index is significant positive correlated with the AHI and the other polysomnography indexes. AHI = apnea-hypopnea index, a.u. = arbitrary units, DFA = detrended fluctuation analysis, HRV = heart rate variability.

and LF/HF ratio) and time-domain (SD1 and SD2) HRV indexes, these data do not disagree with several indications of activated sympathetic activity in specific narrow time windows when apnea/hypopnea episodes occur. In the present study, analyzing the HRV of a full-length sleep through linear analyses may give information on the baseline levels of the

Copyright © 2015 Wolters Kluwer Health, Inc. All rights reserved.



FIGURE 4. Diagnostic yield for DFA α 2 index cutoff values compared with AHI cutoff values (reference values) obtained by polysomnography. ROC curve for identifying patients with (A) moderate (AHI threshold = 15) or (B) severe obstructive sleep apnea (AHI threshold = 30). AHI = apnea–hypopnea index, AUC = area under the curve, CI = confidence interval, DFA = detrended fluctuation analysis, ROC = receiver–operator characteristic.

sympathovagal balance and may not have the power to detect short-term apnea/hypopnea events.

DFA measures the fractal-like correlation properties of the R–R interval time series.²³ The long-term $\alpha 2$ exponent provides a relatively good approximation of the multiscale structure of beat-by-beat series of HR dynamics.²⁴ As such, DFA $\alpha 2$ alterations, indicating loss of fractal HR dynamics, were significantly associated with the risk of cardiac death.²⁵ Patients with OSA have increased risk of cardiovascular disease.²⁵ In these patients, significant relationships between the risk of cardiac death and AHI were reported.²⁶ In the present study, the significant positive correlation detected between DFA $\alpha 2$ and AHI may indicate that the alteration of fractal HR dynamics might represent the linkage of AHI on the prognosis of OSA. In a study with hemodialysis patients, DFA $\alpha 2$ was significantly positive correlated with OSA and a possible independent cardiovascular risk factor.

The ROC sensitivity analysis of α 2 index indicated that the fraction of people with OSA at which the test correctly identifies as positive was 86.11% for moderate and 60% for severe OSA. The fraction of people without the disease at which the test correctly identifies as negative was 63.64% for moderate and 88.89% for severe OSA, as indicated by ROC specificity. Although the ROC analysis indicated a significant prognostic power of DFA α 2 index for the severity of OSA, our study's drawback is not having a control group without OSA (ie, AHI < 5). The present study was limited by the data available in the patient sleep institute record. Further studies shall include volunteers without sleep apnea to further characterize the DFA α 2 index as a prognostic biomarker for OSA and also for other types of apnea.

OSA is a common disease. Community-based studies using screening questionnaires tend to overestimate indications for PSG raising the legitimate question "When Does This Patient Have Obstructive Sleep Apnea?"²⁸ Moreover, it is recommended that clinical examination for likelihood of OSA should be established prior to referring patients for definitive testing. Our study indicates that DFA α^2 index derived from an overnight heart rate recording can be a good predictive biomarker of OSA. Prescreening of patients suspected with OSA with heart rate DFA α^2 index may improve discrimination of sleep apnea. Advances in health self-monitoring technologies including heart rate monitoring through ECG or photoplethysmography methods offer a promising choice to provide a simplified technique for screening of OSA and possibly of sleep apnea, in general, in cardiologists' daily practice.

REFERENCES

- Hori T, Sugita Y, Koga E, et al. Proposed supplements and amendments to 'A Manual of Standardized Terminology, Techniques and Scoring System for Sleep Stages of Human Subjects', the Rechtschaffen & Kales (1968) standard. *Psychiatry Clin Neurosci*. 2001;55:305–310.
- Vrints H, Shivalkar B, Hilde H, et al. Cardiovascular mechanisms and consequences of obstructive sleep apnoea. *Acta Clin Belg.* 2013;68:169–178.
- Wang X, Ouyang Y, Wang Z, et al. Obstructive sleep apnea and risk of cardiovascular disease and all-cause mortality: a meta-analysis of prospective cohort studies. *Int J Cardiol.* 2013;169:207–214.
- Campos LA, Pereira VL Jr, Muralikrishna A, et al. Mathematical biomarkers for the autonomic regulation of cardiovascular system. *Front Physiol.* 2013;4:279.
- Gunther A, Witte OW, Hoyer D. Autonomic dysfunction and risk stratification assessed from heart rate pattern. *Open Neurol J.* 2010;4:39–49.
- Stein PK, Pu Y. Heart rate variability, sleep and sleep disorders. Sleep Med Rev. 2012;16:47–66.
- 7. Tobaldini E, Nobili L, Strada S, et al. Heart rate variability in normal and pathological sleep. *Front Physiol.* 2013;4:294.
- Marcos JV, Hornero R, Alvarez D, et al. Automated prediction of the apnea-hypopnea index from nocturnal oximetry recordings. *IEEE Trans Bio-med Eng.* 2012;59:141–149.
- Otero A, Felix P, Alvarez MR, et al. Fuzzy structural algorithms to identify and characterize apnea and hypopnea episodes. *Conf Proc IEEE Eng Med Biol Soc.* 2008;2008:5242–5245.
- Penzel T, McNames J, Murray A, et al. Systematic comparison of different algorithms for apnoea detection based on electrocardiogram recordings. *Med Biol Eng Comp.* 2002;40:402–407.
- Polat K, Yosunkaya S, Gunes S. Comparison of different classifier algorithms on the automated detection of obstructive sleep apnea syndrome. J Med Syst. 2008;32:243–250.
- Waxman JA, Graupe D, Carley DW. Automated prediction of apnea and hypopnea, using a LAMSTAR artificial neural network. *Am J Respir Crit Care Med.* 2010;181:727–733.

- Hardstone R, Poil SS, Schiavone G, et al. Detrended fluctuation analysis: a scale-free view on neuronal oscillations. *Front Physiol.* 2012;3:450.
- The Report of an American Academy of Sleep Medicine Task Force. Sleep-related breathing disorders in adults: recommendations for syndrome definition and measurement techniques in clinical research. *Sleep.* 1999;22:667–689.
- Kushida CA, Littner MR, Morgenthaler T, et al. Practice parameters for the indications for polysomnography and related procedures: an update for 2005. *Sleep.* 2005;28:499–521.
- Tarvainen MP, Niskanen JP, Lipponen JA, et al. Kubios HRV: heart rate variability analysis software. *Comput Methods Programs Biomed.* 2014;113:210–220.
- Burr RL. Interpretation of normalized spectral heart rate variability indices in sleep research: a critical review. *Sleep.* 2007;30:913–919.
- Bunde A, Havlin S, Kantelhardt JW, et al. Correlated and uncorrelated regions in heart-rate fluctuations during sleep. *Phys Rev Lett.* 2000;85:3736–3739.
- Iyengar N, Peng CK, Morin R, et al. Age-related alterations in the fractal scaling of cardiac interbeat interval dynamics. *Am J Physiol.* 1996;271 (4 Pt 2):R1078–R1084.
- Torre-Bouscoulet L, Castorena-Maldonado A, Banos-Flores R, et al. Agreement between oxygen desaturation index and apnea-hypopnea index in adults with suspected obstructive sleep apnea at an altitude of 2240 m. Arch Bronconeumol. 2007;43:649–654.

- De Backer W. Obstructive sleep apnea/hypopnea syndrome. Panminerva Med. 2013;55:191–195.
- Redline S, Budhiraja R, Kapur V, et al. The scoring of respiratory events in sleep: reliability and validity. *J Clin Sleep Med.* 2007;3:169–200.
- Peng CK, Havlin S, Stanley HE, et al. Quantification of scaling exponents and crossover phenomena in nonstationary heartbeat time series. *Chaos.* 1995;5:82–87.
- Castiglioni P, Quintin L, Civijian A, et al. Local-scale analysis of cardiovascular signals by detrended fluctuations analysis: effects of posture and exercise. *Conf Proc IEEE Eng Med Biol Soc.* 2007;2007:5035–5038.
- Dong JY, Zhang YH, Qin LQ. Obstructive sleep apnea and cardiovascular risk: meta-analysis of prospective cohort studies. *Atherosclerosis.* 2013;229:489–495.
- Kendzerska T, Mollayeva T, Gershon AS, et al. Untreated obstructive sleep apnea and the risk for serious long-term adverse outcomes: A systematic review. *Sleep Med Rev.* 2014;18:49–59.
- Kojima M, Hayano J, Fukuta H, et al. Loss of fractal heart rate dynamics in depressive hemodialysis patients. *Psychosom Med.* 2008;70:177–185.
- Myers KA, Mrkobrada M, Simel DL. Does this patient have obstructive sleep apnea? The Rational Clinical Examination systematic review. J Am Med Assoc. 2013;310:731–741.