Quantifying Bone Marrow Fat Fraction and Iron by MRI for Distinguishing Aplastic Anemia from Myelodysplastic Syndromes

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Background: Bone marrow of patients with aplastic anemia (AA) is different from that of patients with myelodysplastic syndrome (MDS) and is difficult to identify by blood examination. IDEAL-IQ (iterative decomposition of water and fat with echo asymmetry and least-squares estimation) imaging might be able to quantify fat fraction (FF) and iron content in bone tissues. **Purpose:** To determine if IDEAL-IQ measurements of bone marrow FF and iron content can distinguish between patients with AA and MDS.

Study Type: Retrospective.

Population: Fifty-seven patients with AA, 21 patients with MDS, and 24 healthy controls.

Field Strength/Sequence: 3.0 T, IDEAL-IQ sequence.

Assessment: Three independent observers evaluated the IDEAL-IQ images and measured FF and R2* in the left posterior superior iliac spine.

Statistical Tests: Kruskal–Wallis test, linear correlations, and Bland–Altman analysis were used. A P-value of <0.05 was considered statistically significant.

Results: The FF in patients with AA (79.46% \pm 15.00%) was significantly higher than that in patients with MDS (42.78% \pm 30.09%) and control subjects (65.50% \pm 14.73%). However, there was no significant difference in FF between control subjects and patients with MDS (P = 0.439). The R2* value of AA, MDS, and controls was 145.38 \pm 53.33, (171.13 \pm 100.89, and 135.99 \pm 32.41/second, respectively, with no significant difference between the three groups (P = 0.553).

Data Conclusion: Quantitative IDEAL-IQ magnetic resonance imaging may facilitate the diagnosis of AA and distinguish it from MDS.

Level of Evidence: 3 Technical Efficacy Stage: 2

J. MAGN. RESON. IMAGING 2021;54:1754-1760.

Introduction

Aplastic anemia (AA) is characterized by microenvironmental changes and bone marrow hypocellularity, resulting in severe pancytopenia and bone marrow failure.¹ In terms of pathophysiology, the hematopoietic cells in AA are replaced by adipose tissue.² Mesenchymal stem cells from patients with AA are more readily induced to differentiate from adipocytes as

opposed to marrow tissue.^{3,4} Bone marrow biopsy and histology of AA have shown hypocellularity, with increased fat content.⁵ The basic diagnostic feature of AA is extensive fatty bone marrow.⁶

On the other hand, myelodysplastic syndromes (MDS) are myeloid neoplasms characterized by clonal proliferation of hematopoietic stem cells, recurrent genetic abnormalities,

View this article online at wileyonlinelibrary.com. DOI: 10.1002/jmri.27769

Received Mar 23, 2021, Accepted for publication May 21, 2021.

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Contract grant sponsor: The study was partly supported by Zhejiang Medical Science and Technology Project (2018Ky135 and 2020Ky661) and Zhejiang TCM Science and Technology Program (2018ZA043 and 2021ZB114).

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myelodysplasia, ineffective hematopoiesis, and low count of the peripheral blood cell.⁷ Clinical diagnosis is based on an examination of blood and bone marrow showing low count of the blood cell in at least one hematologic cell line and hypercellular marrow with dysplasia, without an excess of fat cells.⁸ The differential diagnosis of the nonsevere subtype of AA and hypocellular MDS is difficult according to clinical findings or examination of blood.⁹ Routine diagnosis is mostly invasive including bone marrow aspiration to detect morphologic dysplasia and blasts, bone marrow biopsy to assess marrow cellularity and fibrosis, and conventional cytogenetics to detect nonrandom chromosomal abnormalities.¹⁰

Iterative decomposition of water and fat with echo asymmetry and least-squares estimation quantitation (IDEAL-IQ) of complex-based fat-water R2* magnetic resonance imaging (MRI) has been used to estimate fat fraction (FF).¹¹ In IDEAL-IQ, images are acquired at multiple echo times (TE), and an iterative least-squares decomposition algorithm is employed to simultaneous solve for FF, water fraction, and R2*.^{11,12} IDEAL-IQ imaging enables adjustment for common biases in the measurement of tissue fat, including T1 and T2* effects, as well as main magnetic field inhomogeneity.^{13,14} Recently, it has been used in many diagnostic studies. It has been an effective method for noninvasive assessment of pancreatic fat infiltration in diabetic pigs, showing that pancreatic fat infiltration is significantly correlated with diabetes.¹⁵ IDEAL-IQ imaging has also been used for quantitative evaluation of changes in vertebral microvascular permeability and vertebral fat deposition in sacroiliac alloxan-induced diabetic rabbits, which are significantly higher than that of the normal rabbits.¹⁶ Furthermore, it has also shown that the FF of inactive sacroiliitis was joint or of active sacroiliac arthritis. IDEAL-IQ imaging has also been used to quantitatively evaluate sacroiliitis in patients with ankylosing spondylitis.¹⁷

In addition to investigating FF, some studies have used the iron (R2*) images of IDEAL-IQ to accurately measure the hepatic iron concentration.^{18–20} R2* can also reflect iron deposition in bone marrow.^{21,22} IDEAL-IQ imaging allows for quantification of the FF and simultaneous R2* estimation in one acquisition. Furthermore, it also provides anatomical evaluation of the bone within a very short imaging time^{23,24} and it has been shown that FF and R2* of vertebrae and femur are significantly different.²⁵

Thus, the aim of this study was to determine if IDEAL-IQ MRI measurements of bone marrow FF and iron content can distinguish between patients with AA and MDS.

Materials and Methods

Study Population

Our institutional review board approved this retrospective study and the need for written informed consent was waived. From January 2016 to November 2020, patients diagnosed with AA or MDS by pathological bone marrow biopsy of the right posterior superior iliac spine in our hospital were examined using the IDEAL-IQ sequence. All patients included were older than 18 years. Patients were excluded if they had undergone bone marrow transplant or had other malignant tumors. A control group of 24 healthy individuals were examined with the same MRI protocol. They had no history of hemopathy or related symptoms and MRI showed normal bone marrow.

MR Imaging

All MRI examinations were performed on a 3-T MRI system (Discovery MR750, GE Healthcare) using a 32-channel phased-array surface coil. After a conventional three-plane localizer, transverse T2-weighted (repeat time [TR] = 2400 msec, TE = 56 msec, field of view [FOV] = $400 \text{ mm} \times 400 \text{ mm}$, slice thickness = 5 mm, matrix = 320×256 , number of excitations [NEX] = 2), transverse T1-weighted (TR = 420 msec, TE = 10.3 msec, FOV = 400 mm \times 400 mm, slice thickness = 5 mm, matrix = 320×256 , NEX = 2), and coronal T2-weighted (TR = 3000 msec, TE = 68 msec, $FOV = 400 \text{ mm} \times 400 \text{ mm}$, slice thickness = 4 mm, matrix = 320×224 , NEX = 2) images were acquired using fast spin-echo sequences for clinical interpretation. IDEAL-IQ imaging was then performed with the following scan parameters: transverse orientation, TR = 8.3 msec, TE = 3.9 msec, FOV = 360 mm × 360 mm, slice thickness = 5 mm, turning angle = 3° , echo train length = 3, matrix = 224×224 , NEX = 1. The scanning time was 1 minute and 31 seconds.

Image Analysis

All MR images were sent to AW4.6 workstation (GE Healthcare). Three observers (two radiologists and a clinician) evaluated the images. Reader 1 is Z.Z., a junior radiologist with 3 years of experience in musculoskeletal MRI. Reader 2 is W.W., a senior radiologist with 22 years of experience in musculoskeletal MRI. Reader 3 is B.Y., a hematologist with no experience in musculoskeletal MRI. The image datasets of patients and controls were anonymized and presented to the observers in a random order. The gender, age, and patient information were all blinded to the readers. Each reader performed the following evaluations independently. T1- and T2-weighted images were used as references for FF and R2* quantification. Regions of interest (ROIs) were manually drawn in the IDEAL-IQ sequence FF images and R2* images of the left posterior superior iliac spine in the largest level. Red bone marrow and puncture holes were excluded (Fig. 1). The system automatically calculated the FF and R2* mean values for the drawn regions.

Statistical Analysis

SPSS 25 software was employed for statistical analysis. Continuous variables were tested for normality and homoscedasticity. Continuous data were tested for normality with the Shapiro–Wilk test. To compare differences in FF and iron content among the three groups, the Kruskal–Wallis test was applied to non-normally distributed data. Interobserver agreement between the three observers on parameter measurements was analyzed by calculating the interclass correlation coefficient (ICC). ICCs were interpreted as follows: 0–0.20, poor agreement; 0.21–0.40, fair agreement; 0.41–0.60, moderate agreement; 0.61–0.80, good agreement; and 0.81–1.00, excellent agreement. Area under the receiver operating characteristic (ROC) curve (AUC) analysis was performed to identify the optimal FF threshold to differentiate AA from MDS combined controls.

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FIGURE 1: ROIs were manually drawn at the level containing the largest section of the left posterior superior ilium (A, B, D, E). The zoomed version of the ROIs showed in the upper left corner. (A, D) FF value of AA and MDS is 86.98% and 25.84%, respectively. (B, E) Iron content from R2*image is 117.91 and 147.98/second. (C, F) Histologic sections images of AA and MDS. Compared with MDS group (F), the number of fat cells (black arrow) in the AA group (C) was increased.



FIGURE 2: Bland–Altman analysis of three observers for FF and R2* values.

Specificity and sensitivity were calculated according to the cut-off value that maximized the Youden index. A *P*-value of <0.05 indicated a statistically significant result for all tests.

Results

A total of 118 patients were recruited, including 22 patients with MDS, 72 patients with AA, and 24 patients in the control group. Sixteen patients were excluded due to prior bone marrow transplantation, including 15 patients with AA and 1 patient with MDS. Finally, the study included 21 patients with MDS (9 males, age range: 38–77 years, median: 56 years), 57 patients

with AA (29 males, age range: 20–69 years, median: 42 years), and 24 control subjects (15 males, age range: 26–68 years, median: 51 years). The age of AA patients was significantly lower than that of MDS patients and control subjects. The MDS and control groups were not significantly different in terms of age (P = 0.542). There were no significant differences in sex ratio (P = 0.250) and body mass index (BMI) (P = 0.776) between the AA and MDS groups.

Image acquisition and data analysis were successful in all participants. The ICC of FF values were 0.978 (95% confidence interval [CI]: 0.968–0.985) between reader 1 and reader

TABLE 1. Comparison FF and iron content of AA, MDS, and control subjects						
	AA (N = 57)	MDS (N = 21)	Control (<i>N</i> = 24)	<i>P/t</i> (AA-MDS)	<i>P\t</i> (AA-control)	<i>P/t</i> (MDS-control)
FF (%)	79.46 ± 15.00	42.78 ± 30.09	65.50 ± 14.73	<0.001/5.258	0.001/3.733	0.439/-1.452
Age (years)	42.25 ± 14.39	58.05 ± 12.99	51.67 ± 13.24	< 0.001/-4.002	0.032/-2.554	0.542/1.339
R2* (/second)	171.13 ± 100.89	145.38 ± 53.33	135.99 ± 32.41	0.553ª		
^a <i>P</i> -values for comparison between the AA_MDS_and control						

^aP-values for comparison between the AA, MDS, and control.



FIGURE 3: Scatterplots of FF against age for AA, MDS, and control groups. The line represents best-fit regression trend. The shaded area is CI. The FF values in the AA group were higher than in the MDS and control groups.

2, 0.967 (95% CI: 0.951–0.977) between reader 1 and reader 3, and 0.977 (95% CI: 0.966–0.985) between reader 2 and reader 3, indicating near-perfect interobserver agreement (all P < 0.05). The ICC of R2* values was 0.978 (95% CI: 0.968– 0.985) between reader 1 and reader 2, 0.980 (95% CI: 0.970– 0.986) between reader 1 and reader 3, and 0.970 (95% CI: 0.956–0.980) between reader 2 and reader 3, indicating nearperfect interobserver agreement. Applying Bland–Altman statistics, it indicated a reliable interobserver agreement between observers. The corresponding Bland–Altman plots for three observers are shown in Fig. 2.

The FF of patients with AA (79.46% \pm 15.00%) was significantly higher than that of patients with MDS (42.78% \pm 30.09%) and of control subjects (65.50% \pm 14.73%). The FF in control subjects was not significantly different to that in patients with MDS (P = 0.439). There was no significant difference (P = 0.553) in the R2* values of patients with MDS (171.13 \pm 100.89/second), AA (145.38 \pm 53.33/second), and control groups (135.99 \pm 32.41/second; table 1). Scatterplots of FF against age for AA, MDS, and control groups are shown in Fig. 3.

Using ROC analysis, the area under the curve value of FF was 0.822, the sensitivity was 0.719, and the specificity was 0.867. The critical value of FF for AA was 78.67. AUC value of age was 0.266 (Fig. 4).

Discussion

This study used IDEAL-IQ imaging to measure FF and R2* for hemopathy. We found a significantly elevated ilium FF in AA compared to MDS and normal bone marrow. MDS showed no significant difference in FF from control subjects. This result is consistent with the current clinical diagnosis of AA, which mainly relies on bone marrow biopsy to detect the fat content. However, the IDEAL-IQ method has the potential to assess this noninvasively. There was a significant difference between the age of patients with AA and MDS. However, through ROC curve analysis, age did not affect the diagnosis of AA and MDS. Differentiation of these two diseases also needs to be combined with blood examination. Peripheral blood smears of controls would be expected to be normal, while those of MDS patients would not. The iron



FIGURE 4: ROC curve of FF for differentiating AA with MDS combined control group.

content of the bone marrow, as reflected by the R2* values, is no different among AA patients, MDS patients, and control subjects. AA and MDS patients with severe hemocytopenia often need blood transfusion, and multiple blood transfusions lead to increased iron deposition in various tissues.²⁶ Blood transfusion can cause iron deposition in organs, but not in the bone marrow. IDEAL-IQ imaging can also quantify iron deposition in other tissues^{21,22} and has promise in monitoring the occurrence of adverse reactions.

In our study, the ICCs of our independent readers indicated near-perfect interobserver agreement, regardless of years' experience or medical specialty (radiologist/clinician). These results suggest that the determination of FF and R2* appears to be reader-independent and that it does not require extensive training.

T1- and T2-weighted image could not quantify FF. MR spectroscopy assessed fat content is impractical in some clinical settings due to long scan time, small imaging range, and a substantial amount of postprocessing.¹⁴ Positron emission tomography/computed tomography (PET/CT) examination has shown low bone metabolism in AA patients, which could be used for differential diagnosis from atypical MDS.²⁷ However, PET/CT is expensive and requires injections of radioactive agents. Quantitative analysis of bone marrow fat (BMF) content through IDEAL-IQ imaging allows for the detection of abnormal changes in the bone marrow. In combination with the clinical manifestations and relevant laboratory tests, it has the potential to improve the diagnostic accuracy of AA and MDS. A correct diagnosis based on noninvasive examination may avoid the need for invasive procedures. In addition to monitoring AA, IDEAL-IQ imaging may also be useful for monitoring disease progression of MDS and acute myelocytic leukemia, which typically is induced by genetic mutations leading to cloned hematopoiesis.^{28–30} Other predisposing factors for MDS and AA include apoptosis induced by DNA damage from cytotoxic chemotherapy, radiotherapy, chemical or physical drugs, and clinical drugs (chloramphenicol, nonsteroidal anti-inflammatory drugs, antiepileptic drugs, and antithyroid drugs).³¹ IDEAL-IQ may have potential for monitoring BMF change during and after treatment to prevent the occurrence of AA or MDS.

Bone marrow perfusion is correlated to BMI in adults. The intramedullary blood flow and the exchanges between bone marrow and bone vessels increase with BMI.³² In our study, there was no statistically significant difference in BMI between the three groups in this study. The effect of BMI on measuring bone marrow FF was excluded. The technique using standard T1-weighted images was less sensitive to variations in fat concentration in the bone marrow.³³ However, IDEAL-IQ can sensitively detect variations in fat concentration in the bone marrow. The IDEAL-IQ technique has a shorter scan time and can provide much greater coverage. The IDEAL method may therefore be a better choice than MR spectroscopy and the standard T1-weighted method when assessing BMF for clinical and research purposes.^{33,34} More recent work has revealed that BMF plays an important role in many diseases. BMF accumulation is thought to be correlated with endocrine and metabolic diseases, such as obesity, osteoporosis, aging, and type 1 diabetes.^{35,36} It has also been associated with bone metastases in cancer.³⁷⁻⁴⁰ In addition, bone marrow is closely related with hematopoietic function.41 The decrease of hematopoietic activity in bone marrow with age may be related to the accumulation of BMF.41,42 IDEAL-IQ imaging can be used for quantitative measurement of BMF, and may be of value for the assessment and diagnosis of diseases, such as iron deposition in liver after blood transfusion, sacroiliitis, and diabetes.¹⁵⁻¹⁸ Although BMF content can be accurately measured, more studies are needed with comparisons to pathological results to demonstrate increased applications of IDEAL-IQ.

Limitations

This study was performed at a single center on a small number of subjects. Studies including larger patient cohorts in multicentric trials will be necessary to further demonstrate the robustness of IDEAL-IQ results. The bone marrow can also be affected by various factors and individual differences. This leads to the discrete curve of FF in patients with MDS in the experiment. In addition, to keep ROIs consistent with the bone marrow biopsy, only one level of the left posterior superior ilium was selected in this experiment, not the whole pelvis.

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Conclusion

IDEAL-IQ technology can efficiently quantify the content of fat and iron in bone tissue. The values of FF determined by IDEAL-IQ were able to differentiate between AA and MDS without the need for an invasive procedure.

Conflict of Interest

The authors have no conflict of interest to declare.

References

- Gonzaga VF, Wenceslau CV, Lisboa GS, Frare EO, Kerkis I. Mesenchymal stem cell benefits observed in bone marrow failure and acquired aplastic anemia. Stem Cells Int 2017;2017:8076529.
- Luzzatto L, Risitano AM. Advances in understanding the pathogenesis of acquired aplastic anaemia. Br J Haematol 2018;182(6):758-776.
- Medinger M, Drexler B, Lengerke C, Passweg J. Pathogenesis of acquired aplastic anemia and the role of the bone marrow microenvironment. Front Oncol 2018;8:587.
- Zhao J, Chen J, Huang F, et al. Human gingiva tissue-derived MSC ameliorates immune-mediated bone marrow failure of aplastic anemia via suppression of Th1 and Th17 cells and enhancement of CD4 +Foxp3+ regulatory T cells differentiation. Am J Transl Res 2019;11 (12):7627-7643.
- Gaman A, Gaman G, Bold A. Acquired aplastic anemia: Correlation between etiology, pathophysiology, bone marrow histology and prognosis factors. Rom J Morphol Embryol 2009;50(4):669-674.
- 6. Young NS. Aplastic anemia. N Engl J Med 2018;379(17):1643-1656.
- Arber DA, Orazi A, Hasserjian R, et al. The 2016 revision to the World Health Organization classification of myeloid neoplasms and acute leukemia. Blood 2016;127(20):2391-2405.
- Cazzola M. Myelodysplastic syndromes. N Engl J Med 2020;383(14): 1358-1374.
- Kulasekararaj AG, Jiang J, Smith AE, et al. Somatic mutations identify a subgroup of aplastic anemia patients who progress to myelodysplastic syndrome. Blood 2014;124(17):2698-2704.
- Ades L, Itzykson R, Fenaux P. Myelodysplastic syndromes. Lancet 2014; 383(9936):2239-2252.
- Reeder SB, Wen Z, Yu H, et al. Multicoil Dixon chemical species separation with an iterative least-squares estimation method. Magn Reson Med 2004;51(1):35-45.
- Yu H, Shimakawa A, McKenzie CA, Brodsky E, Brittain JH, Reeder SB. Multiecho water-fat separation and simultaneous R2* estimation with multifrequency fat spectrum modeling. Magn Reson Med 2008;60(5): 1122-1134.
- Eskreis-Winkler S, Corrias G, Monti S, et al. IDEAL-IQ in an oncologic population: Meeting the challenge of concomitant liver fat and liver iron. Cancer Imaging 2018;18(1):51.
- Aoki T, Yamaguchi S, Kinoshita S, Hayashida Y, Korogi Y. Quantification of bone marrow fat content using iterative decomposition of water and fat with echo asymmetry and least-squares estimation (IDEAL): Reproducibility, site variation and correlation with age and menopause. Br J Radiol 2016;89(1065):20150538.
- Chen Y, Long L, Jiang Z, Zhang L, Zhong D, Huang X. Quantification of pancreatic proton density fat fraction in diabetic pigs using MR imaging and IDEAL-IQ sequence. BMC Med Imaging 2019;19(1):38.
- Hu L, Zha YF, Wang L, et al. Quantitative evaluation of vertebral microvascular permeability and fat fraction in alloxan-induced diabetic rabbits. Radiology 2018;287(1):128-136.
- Ren C, Zhu Q, Yuan H. Mono-exponential and bi-exponential modelbased diffusion-weighted MR imaging and IDEAL-IQ sequence for quantitative evaluation of sacroiliitis in patients with ankylosing spondylitis. Clin Rheumatol 2018;37(11):3069-3076.

- Obrzut M, Atamaniuk V, Glaser KJ, et al. Value of liver iron concentration in healthy volunteers assessed by MRI. Sci Rep 2020;10(1):17887.
- Wood JC, Enriquez C, Ghugre N, et al. MRI R2 and R2* mapping accurately estimates hepatic iron concentration in transfusion-dependent thalassemia and sickle cell disease patients. Blood 2005;106(4):1460-1465.
- Kuhn JP, Meffert P, Heske C, et al. Prevalence of fatty liver disease and hepatic iron overload in a northeastern German population by using quantitative MR imaging. Radiology 2017;284(3):706-716.
- Franca M, Marti-Bonmati L, Porto G, et al. Tissue iron quantification in chronic liver diseases using MRI shows a relationship between iron accumulation in liver, spleen, and bone marrow. Clin Radiol 2018;73(2): 215.e1-215.e9.
- Tsujikawa T, Oikawa H, Tasaki T, et al. Integrated [(18)F]FDG PET/MRI demonstrates the iron-related bone-marrow physiology. Sci Rep 2020; 10(1):13878.
- Regis-Arnaud A, Guiu B, Walker PM, Krause D, Ricolfi F, Ben Salem D. Bone marrow fat quantification of osteoporotic vertebral compression fractures: Comparison of multi-voxel proton MR spectroscopy and chemical-shift gradient-echo MR imaging. Acta Radiol 2011;52(9):1032-1036.
- Kuhn JP, Hernando D, Meffert PJ, et al. Proton-density fat fraction and simultaneous R2* estimation as an MRI tool for assessment of osteoporosis. Eur Radiol 2013;23(12):3432-3439.
- Li D, Tao X, Zhang N, et al. Do magnetic resonance imaging manifestations of skeletal system improve after treatment of Gaucher disease? Eur J Radiol 2020;125:108851.
- Hod EA, Zhang N, Sokol SA, et al. Transfusion of red blood cells after prolonged storage produces harmful effects that are mediated by iron and inflammation. Blood 2010;115(21):4284-4292.
- Chen M, Lu L, Li J, et al. Value of systemic PET/CT in the diagnosis and differential diagnosis of aplastic anemia. Oncol Lett 2018;16(3):3215-3222.
- Yoshizato T, Dumitriu B, Hosokawa K, et al. Somatic mutations and clonal hematopoiesis in aplastic anemia. N Engl J Med 2015;373(1): 35-47.
- Ogawa S. Clonal hematopoiesis in acquired aplastic anemia. Blood 2016;128(3):337-347.
- Negoro E, Nagata Y, Clemente MJ, et al. Origins of myelodysplastic syndromes after aplastic anemia. Blood 2017;130(17):1953-1957.
- Furlong E, Carter T. Aplastic anaemia: Current concepts in diagnosis and management. J Paediatr Child Health 2020;56(7):1023-1028.
- Budzik JF, Lefebvre G, Behal H, et al. Bone marrow perfusion measured with dynamic contrast enhanced magnetic resonance imaging is correlated to body mass index in adults. Bone 2017;99:47-52.
- Zhang C, Slade JM, Miller F, Modlesky CM. Quantifying bone marrow fat using standard T1-weighted magnetic resonance images in children with typical development and in children with cerebral palsy. Sci Rep 2020;10(1):4284.
- Baum T, Yap SP, Dieckmeyer M, et al. Assessment of whole spine vertebral bone marrow fat using chemical shift-encoding based water-fat MRI. J Magn Reson Imaging 2015;42(4):1018-1023.
- Scheller EL, Cawthorn WP, Burr AA, Horowitz MC, MacDougald OA. Marrow adipose tissue: Trimming the fat. Trends Endocrinol Metab 2016;27(6):392-403.
- Botolin S, McCabe LR. Bone loss and increased bone adiposity in spontaneous and pharmacologically induced diabetic mice. Endocrinology 2007;148(1):198-205.
- Morris EV, Edwards CM. Bone marrow adipose tissue: A new player in cancer metastasis to bone. Front Endocrinol (Lausanne) 2016; 7:90.
- Kim TY, Schafer AL. Diabetes and bone marrow adiposity. Curr Osteoporos Rep 2016;14(6):337-344.

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- Templeton ZS, Lie WR, Wang W, et al. Breast cancer cell colonization of the human bone marrow adipose tissue niche. Neoplasia 2015;17(12):849-861.
- Patsch JM, Li X, Baum T, et al. Bone marrow fat composition as a novel imaging biomarker in postmenopausal women with prevalent fragility fractures. J Bone Miner Res 2013;28(8):1721-1728.
- Ambrosi TH, Scialdone A, Graja A, et al. Adipocyte accumulation in the bone marrow during obesity and aging impairs stem cell-based hematopoietic and bone regeneration. Cell Stem Cell 2017;20(6):771-784.e6.
- 42. Wang H, Leng Y, Gong Y. Bone marrow fat and hematopoiesis. Front Endocrinol (Lausanne) 2018;9:694.