A Pilot Study with Randomised Controlled Design Comparing TiZr Alloy Dental Implants to Ti Implants

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ABSTRACT

Objectives: Evidence on the clinical performance of recently introduced dental implants in titanium-zirconium alloy is sparse. The aim of the present pilot study with randomized controlled design is to compare changes in supporting structures around dental titanium-zirconium alloy implants to commercially pure titanium implants.

Material and Methods: The present material includes consecutive patients referred to a specialist clinic in Sweden. Two patient groups treated with dental implants in two different materials - titanium (Ti) and titanium-zirconium (TiZr) - were defined after block randomisation for smoking. In total, 40 implants installed in 21 patients were available for one-year follow-up. Marginal bone level, soft tissue height and width of keratinised mucosa were registered at baseline and at one-year follow-up.

Results: At implant level, the test group (TiZr) yielded significant marginal bone loss (P < 0.001) after one year. Additionally, marginal bone loss after one year was significantly higher for TiZr implants (P < 0.001) as compared to traditional Ti implants. Soft tissue dimensions were stable throughout the evaluation time for both implant materials.

Conclusions: One-year results indicate more pronounced initial marginal bone loss for dental implants in titanium-zirconium alloy as compared to implants made of commercially pure titanium.

Keywords: bone resorption; dental implants; dental materials; titanium; zirconium.

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INTRODUCTION

In the 1960s, Brånemark and co-workers [1] first presented dental implants and osseointegration as a reliable concept in treatment of edentulous patients. Since the introduction of dental implants titanium (Ti) grade 1 and gradually grade 4, also known as commercially pure Ti (cp-Ti), has been the golden standard when it comes to implant materials suitable for dental use. Properties as high strength, high resistance to corrosion, easy processing and favourable integration with surrounding tissue, contributes to its common use both in general medicine and in dental implantology [2]. Research has shown that treatment with dental implants made from Ti are predictable in terms of implant survival although the challenge is to keep patients enrolled in follow-up programs and to deal with technical and biological complications [3-5]. Nevertheless, the accumulated knowledge about Ti implants, as seen from 15- and 20-year followups, has been based on prerequisites that are not always followed today. One of them is that dental implants are not always made from cp-Ti. New materials have been studied as alternatives to the well-documented implant material Ti [6,7], with a focus on finding a material with increased mechanical combined with improved biological characteristics. Unfortunately, the mechanical strength can be insufficient and narrow diameter Ti implants have been associated with increased risk of fatigue fractures especially in areas with high load or in patients with parafunctional habits [8-10].

Alloys including Ti, incorporating non-toxic elements such as zirconium (Zr), niobium (Nb), tantalum (Ta), palladium (Pd) and indium (In), are being explored for their ability to match or increase the mechanical strength and corrosion resistance of Ti, with improved biocompatibility [11]. Ti alloys including aluminium (Al) (Ti6Al4V) which present better mechanical properties under cyclic loading relative to cp-Ti [12]. However, creating sufficient surface roughness on Ti6Al4V implants has been challenging leading to concerns regarding material biocompatibility [13,14]. Ti and Zr are both transition metals in the same group of the periodic table and have similar chemical properties. An insoluble oxide layer is formed on the surface of both materials upon contact with oxygen, thereby enhancing their anticorrosive properties [15] thereby making them interesting for dental implant

The aim of the present randomized controlled pilot

study is to compare the clinical performance of titanium-zirconium alloy implants to commercially pure titanium implants with emphasis on hard and soft tissue-oriented outcomes after 1 year.

MATERIAL AND METHODS

The study was registered in online clinical trials register system <u>www.clinicaltrials.gov</u> and can be accessed with number NCT02681250.

Ethical approval has been acquired by the National Board of Review, Gothenburg, Western Sweden (reference number 216-15).

Patient recruitment

The present material represents a pilot study including 23 consecutive patients in need of dental implant treatment referred to the Department of Prosthodontics in Borås, Sweden from October 2015 to November 2016. In order to increase the study relevance for everyday clinical practice, several prosthetic protocols were included. No patients with history of periodontitis were included in the study. Patients belonging to the American Society of Anesthesiologists (ASA) class 4 (e.g., myocardial infarction or thrombotic episode within the last three months) [16]. Before entering the study, every patient had to sign a document of informed consent. If needed, hygiene instructions cooperation control on individual performed before starting the treatment. were The following patient-related variables were assessed:

- Gender (male/female);
- Age (years);
- Smoking habits (yes/no);
- Number of cigarettes/day (0 to 10, 0 to 20 and > 20).

General health status and medication were also reported (Table 1).

The patients underwent block randomisation for smoking (K.H.) since smoking is a known risk factor for implant treatment [17,18]. Tissue level implants (Institute Straumann® AG; Basel, Switzerland) with sandblasted and acid-etched surface (Straumann® SLA®) were installed. The test group received TiZr alloy with 13 - 17% Zr (TiZr1317) implants (Straumann® Tissue Level Standard Plus SLA® Roxolid®) and the control group dental cp-Ti implants (Straumann® Tissue Level Standard Plus SLA®).

Table 1. Distribution of implant characteristics

Implant characteristics		Implant material		Total
		Ti (n)	TiZr (n)	(n)
Position in jaw	Anterior maxilla (#13-23)	1	4	5
	Posterior maxilla (#14-17, #24-27)	4	7	11
	Anterior mandible (#33-43)	0	2	2
	Posterior mandible (#34-37, #44-47)	11	11	22
Implant length	8 mm	3	2	5
	10 mm	11	16	27
	12 mm	2	6	8
Implant diameter	3.3 mm	1	6	7
	4.1 mm	15	15	30
	4.8 mm	0	3	3
Abutment use	Abutment	13	24	37
	No abutment	3	0	3
Anchorage	Screw retained	15	24	39
	Cemented	0	1	1
Type of restoration	Single crown	6	9	15
	Partial bridge	10	11	21
	Full arch bridge	0	4	4

n = number.

Clinical procedures

Surgery was performed by two experienced surgeons (C.B., U.J.), at the Department of Oral and Maxillofacial Surgery in Borås, Sweden. Implant installation was performed according to the standard surgical protocol recommended from the manufacturer. Delayed loading protocol was employed in all cases. Impressions were made in polyether impression material (ImpregumTM DuoSoftTM, 3MTM ESPETM, for single crowns and partial dentures and ImpregumTM, 3MTM ESPETM, for full arch impressions). All abutments were made in Ti. Prosthesis material varied and was either metal ceramic (cobalt-chromium with veneering porcelain), yttrium-stabilised tetragonal zirconium dioxide (with or without veneering porcelain) or (for the full arch prosthesis) Ti framework with acrylic veneering. Prosthesis screw torque was set according to manufacturer's instruction. Individually tailored oral hygiene instructions were given by a dental hygienist and the patients were recalled after 1 year.

Radiographic examination

Postoperative radiographic examinations were

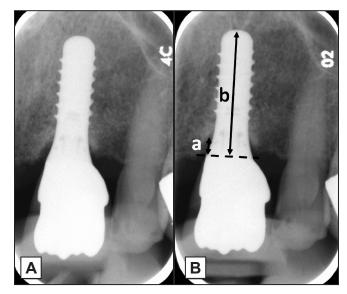


Figure 1. Postoperative standardised periapical radiographs: A = baseline X-ray; B = follow-up X-ray (a = marginal bone level; b = calibration measure).

performed upon delivery of the permanent restoration (baseline) and at follow-up examinations at 1 year. Standardised periapical radiographs were taken using film holders (Have-Super-BiteTM - Hawe-Neos Dental; Genilino, Switzerland) and digital imaging plate system (Vistascan® - Dürr Dental AG; Bietigheim-Bissingen, Germany) with the X-ray beam perpendicular to the implant. The film holder device was attached to the occlusal surface of the supraconstruction using a putty silicone impression material (Flexitime® Easy Putty - Heraeus Kulzer; Hanau, Germany) to ensure that the film holder position can be repeated at the follow-up visit [19,20].

The radiographs were evaluated regarding marginal bone level. Interexaminer reliability (KH, AE) was performed in terms of calibration at 10 randomly selected implants. All measurements were made in Romexis® software (Planmeca Romexis®, Helsinki, Finland). Before measurements were made, implants were calibrated in the software according to the known length of the individual implant. The distance between the implant reference point (implant shoulder) to the marginal bone was recorded (Figure 1). The mean value of the two interproximal aspects of the implant was reported as primary outcome.

Clinical examination

At baseline and after 1 year in function, the following parameters were recorded:

- Type of implant material (TiZr/Ti);
- Position of the implant;
- Type of prosthodontics (single crown/partial bridge/full arch bridge);
- Number of implants included in the prostheses;

- Use of abutment (yes/no);
- Connection type of the prosthesis (screw retained/ cemented);
- Implant length (mm);
- Implant diameter (mm).

The vertical dimension of the mucosa was registered with a periodontal probe (Hu-Friedy Mfg. Co., LLC; Frankfurt, Germany) and was assessed from the bottom of pocket to the mucosal margin at the mesial, distal, palatal/lingual and buccal site (mm) [21]. The width of the keratinised mucosa (mm) was registered with the periodontal probe from the mucosal margin to the most apical part of keratinised mucosa at the buccal side of the implant. Clinical measurements were performed by the same clinician (KH) at all follow-ups.

Statistical analysis

The statistical analysis was performed with SPSS Statistics version 22 (SPSS Inc.; Chicago, Illinois, USA). The primary outcome was alteration in marginal bone level from baseline to the one-year examination. Alterations in marginal bone level, soft tissue height and width of the keratinised mucosa were assessed. An overview of the present patient material and alterations in marginal bone level is presented with descriptive statistics at patient-

and implant level (Figure 2 and 3). Two-way mixed model was used for estimating inter-examiner reliability resulting to a correlation coefficient of 0.95. Paired samples t-test was used to compare alterations in marginal bone levels, vertical dimension peri-implant mucosa and the width of the keratinised mucosa within each implant group. The intergroup alterations in marginal bone level were compared by using t-test. Pearson correlations test was used for testing of correlation between width of keratinised mucosa and marginal bone loss. P-values \leq 0.05 were considered statistically significant. Parametric data were expressed as mean and standard deviation (M [SD]).

RESULTS

In total, 23 patients were included in the study and randomized into two groups (Ti = 11, TiZr = 12). Two patients, one from each group were considered as drop outs; one patient received another implant design due to aesthetic considerations and one patient did not attend the follow-up visit. In total, 21 patients (Ti = 10, TiZr = 11) completed the 1-year follow-up rendering a drop-out rate of 8.7%. Given the low and equally distributed dropout rate, a per-protocol analysis was implemented.

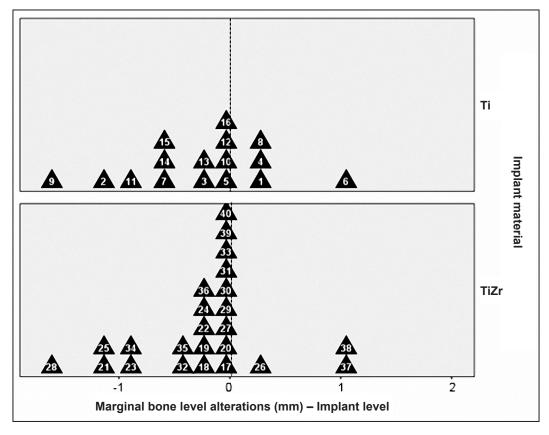


Figure 2. Marginal bone level alterations (numbers displaying implant).

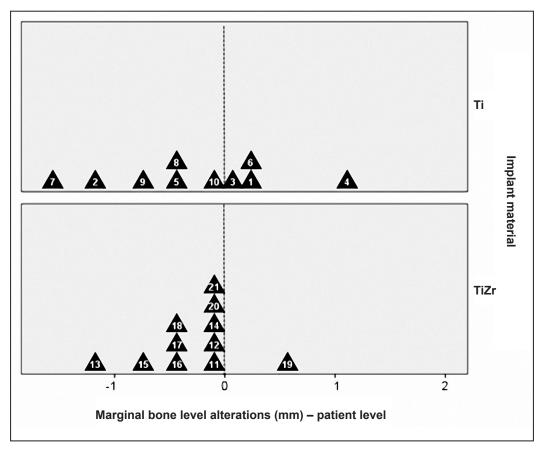


Figure 3. Marginal bone level alterations (numbers displaying patient).

Forty implants (Ti = 16, TiZr = 24) were installed in 13 males and 8 females (Ti = 5 males/5 females, TiZr = 8 males/3 females). The mean age was 42.5 (23.8) years in the control group and 54.6 (19.2) years in the test group. Five patients (Ti = 2, TiZr = 3) were smokers at the time of surgery, all in group "0 - 10 cigarettes/day", no patients reported more than 10 cigarettes/day. Patient related characteristics are presented in Table 2.

Fifteen implants supported single crowns (Ti = 6, TiZr = 9), 21 implants supported partial bridges (Ti = 10, TiZr = 11), and four implants supported one full arch bridge (Ti = 0, TiZr = 4). Only one restoration (single crown) in the test group (TiZr) was cemented, all other restorations were screw retained. Implant related characteristics are presented in Table 2. The mean diameter in the test and control group was 3.99 mm and 4.05 respectively. The mean implant length was 10.33 mm and 9.88 mm respectively.

Marginal bone level

Paired samples t-test for the control group (Ti) revealed no significant alterations in marginal bone level at implant level (P = 0.12) (Table 3, Figure 2). However, the test group (TiZr) demonstrated significant bone loss (P < 0.001)

Table 2. Distribution of patient characteristics

Patient characteristics		Im _I	Total	
		Ti	TiZr	
		10	11	21
Age (years)	Meana	42.5	54.6	48.8
	SD	23.8	19.2	21.8
	Male	5	8	13
	Female	5	3	8
Health/ diseases (n)	Cardiovascular	2 ^b	3°	5
	Diabetes	0	1	1
	Other	3	4	7
	Healthy	6	5	11
Cigarettes/ day (n)	0	8	8	16
	0 to 10	2	3	5
	10 to 20	0	0	0
	> 20	0	0	0

^aStatistically non-significant difference between the two age groups (P = 0.22).

^bOne subject with "cardiovascular" and "other" diseases.

^eOne subject with "cardiovascular" and "other" diseases and one subject with "cardiovascular" and "diabetes".

n = number; SD = standard deviation.

Paired differences SD P-value^a Mean Alterations in marginal bone level, MBL (mm) - implant level Ti MBL. Baseline - Ti MBL 1 year -0.270.64 0.12 TiZr MBL. Baseline - TiZr MBL 1 year -0.981.01 < 0.001 Alterations in marginal bone level, MBL (mm) - patient level Ti MBL. Baseline - Ti MBL 1 year -0.270.63 0.21 TiZr MBL. Baseline - TiZr MBL 1 year -0.190.61 0.32 Alterations in vertical dimension of the soft tissue (mm) - implant level Ti. Baseline - Ti 1 year -0.310.6 0.06 TiZr. Baseline - TiZr 1 year 0.020.57 0.86 Alterations in keratinized mucosa (mm) - implant level Both groups. Baseline - 1 year -0.15 0.87 0.28

Table 3. Alterations in marginal bone level, vertical dimensions of the soft tissue and keratinized mucosa

between baseline and one year (Table 3, Figure 2) on implant level. The marginal bone loss for TiZr implants was significantly higher as compared to the control group (P < 0.001). At patient level, the alterations in marginal bone level were not significant (TiZr: P = 0.32, Ti: P = 0.21), (Figure 3, Table 3). It was concluded that the change in marginal bone level was independent of the width of the keratinised

Soft tissue

mucosa at baseline (P = 0.81).

The vertical dimension of the soft tissue surrounding the implants was stable throughout the evaluation time for both implant materials (Ti: P = 0.06, TiZr: P = 0.86) (Table 3). The amount of keratinised mucosa surrounding the implants did not change significantly in neither of groups during the evaluation period (P = 0.28) (Table 3).

DISCUSSION

The results of the present pilot study suggest that sandblasted and acid-etched TiZr alloy implants present more pronounced initial marginal bone loss as compared to implants in cp-Ti with corresponding surface modification. The vertical dimensions of the soft tissues surrounding the implants seem to be stable over the follow-up period regardless the implant material. Additionally, the initial marginal bone loss seems to be independent of the width of keratinised mucosa at baseline.

Currently, research on dental implants in TiZr alloy is limited [22] and consists mainly of animal studies and a few clinical studies [23,24] by which only a few have comparative design [25-27]. Although the first study in humans was published in 2011 [28], no results are available with more than five years of clinical follow-up [25].

The objective of the present study was to compare two core materials having been subjected to the same surface treatment modality, i.e. large grit blasting and acid-etching. It is evident that surface topography and chemistry affect the osseointegration process [29-31]. It has been demonstrated that due to the monophasic alphastructure of TiZr1317, microtopography is developed by acid-etching and sandblasting [32,33]. However, some differences in microtopography have been observed between cp-Ti and TiZr after acid-etching and sandblasting. An in vitro study by Frank et al. [33] comparing sandblasted and acid-etched discs in cp-Ti and TiZr demonstrated significant differences on micro- and nanotopography. Wennerberg et al. [34] concluded in vitro that hydrophilic, sandblasted and acid-etched (SLA-active modified) Ti discs presented higher mean surface roughness (Sa), lower density of surface summit (Sds) and higher total surface exposed to bone (Sdr) as compared to TiZr. Similar results were presented in an animal study by Jimbo et al. [35] The authors compared the surface topography of cp-Ti SLActive® and TiZr SLActive® implants and found that average height deviation was similar, but the TiZr implants were overall less rough, as the Sds and the Sdr were significantly smaller compared to the cp-Ti implants [35].

aStatistically significant at level P < 0.05 (Paired samples t-test). MBL = marginal bone level; SD = standard deviation.

A proposed explanation model for the different clinical outcomes may be found in a study by Lotz et al. [36]. In this in vitro study it was concluded that human osteoblasts cultured on SLActive® modified TiZr discs presented lower gene expressions of IL-6 and BMP-4 as compared to Ti discs. IL-6 is a proinflammatory marker considered to be important in bone formation in conditions of high bone turnover [37]. Since inflammation is proved to be concomitant to bone formation [38], it is reasonable to assume that lower levels of IL-6 imply lower rate of bone formation. Furthermore, lower expression of BMP-4 may denote lower osteogenic capacity for TiZr surfaces as compared to Ti. Our study revealed a significant difference in marginal bone loss at implant level from baseline to one year follow-up in the TiZr group but not in the Ti group which can be interpreted as the core material might have an impact on the osseointegration process.

Gottlow et al. [39] presented results from an animal study comparing TiZr implants to implants made from commercially pure Ti in 12 mini pigs. Although similar osteoconductive properties in terms of bone-to-implant-contact were demonstrated, TiZr-implants were associated with significantly higher stability compared to implants made from cp-Ti [39]. However, other animal studies have failed to demonstrate improved biological and mechanical properties of dental implants made from TiZr1317 as compared to cp-Ti [40,41].

Benic et al. [42] presented one-year results from a human randomized controlled clinical study on 40 single implants in anterior and premolar region comparing 3.3 mm Straumann® TiZr SLActive® to 4.1 mm Straumann® Ti SLActive® implants. No differences between the two core materials regarding change in marginal bone loss, clinical parameters and the occurrence of adverse events were evident [42]. Three-year results from the same patient material no significant differences in either change in marginal bone level, change in mucosa levels or occurrence of complications could be proved [26]. In another randomized multicenter clinical trial on implant supported overdentures with split mouth design, narrow diameter implants in TiZr and cp-Ti were compared [25]. The study had high dropout rate since 49 of 91 patients fulfilled the study to the five-year follow-up. No differences in terms of marginal bone loss or mucosal health could be concluded from that study. Tolentino et al. [27] presented the results from a small randomized study in split mouth design on narrow diameter implants in TiZr compared to cp-Ti supporting single crowns in molar region in a one year follow-up. The surface treatment on the TiZr implant was not reported. No differences in marginal bone loss or mucosal health were concluded [27].

The current study presents unfavourable results for TiZr implants in terms of increased marginal bone loss over the one year follow-up. Since soft tissue integration has gained increasing attention as a tentative factor influencing implant success, it is reasonable to assume that implant core material may affect soft tissue healing and integration. In the present study, the one-piece implant design contributes with a study model exposing the same implant core material against both hard and soft tissues. However, the results of the current study yield no significant changes in the vertical soft tissue dimension in neither the Ti nor the TiZr implant group over the one year observation period. These results are in agreement with five year clinical results comparing implants in cp-Ti and TiZr [25,27]. The penetrating mucosal part of the Straumann® Tissue Level implants has a machined/polished surface with no additional surface modification. Since the machining process gives raise to similar surface characteristics for both cp-Ti and TiZr [33], it may be speculated that both implant materials may result to similar soft tissue responses. Zhang et al. [11] could not reveal any differences in growth of human fibroblasts on machined TiZr alloy discs as compared to machined cp-Ti discs in a laboratory study [43]. Similar results could be concluded in a comparable study by Gomez-Florit et al. [44]. These results are in line with the results from this current clinical study.

Since the participants of the current study were recruited in a consecutive basis, some general conditions may have affected the study outcome. Smoking and poorly controlled diabetes are known patient-related factors that may influence the long-term stability of peri-implant tissues [17,45]. However, a recent 5-year follow-up [46] concluded that smoking had no effect on peri-implant tissues surrounding Ti- or TiZr-implants, concomitantly highlighting the role of routine oral hygiene maintenance. Also, when it comes to patients with well-controlled diabetes mellitus type 2, the prognosis for TiZr-implants seems to be equally good as for subjects with normal glycemic level [47]. Although it has been suggested that dental implants require a soft tissue barrier to prevent bacterial penetration [48], the need for keratinised mucosa surrounding dental implants in order to guarantee long term success is still unclear [49,50]. Chung et al. [51] found no correlation between the presence of keratinised mucosa and annual bone loss. Nevertheless, the findings supported a correlation between absence of keratinised mucosa and higher plaque accumulation and gingival inflammation [51].

In a long term follow-up of 58 implant patients treated with guided bone regeneration no evidence was found that the width of keratinised mucosa is a predictor for bone loss [52]. Correlation analysis in our study suggested no significant correlation between the width of keratinised mucosa at baseline and the alterations of marginal bone level.

CONCLUSIONS

Despite the limitations of this pilot study in terms of mixed implants diameters and prosthetic protocols, the one-year results indicate more pronounced initial marginal bone loss for titanium zirconium alloy with 13 - 17% zirconium implants as compared to implants made from commercially pure titanium. These results, in combination with the absence of other large scale studies in this narrow scientific field, advocate the need for larger scale studies in order to be able

to clarify any differences in maintaining a stable marginal bone level around the two implant types. However, the vertical dimensions of the peri-implant soft tissue seem to be stable over the follow-up period regardless of the implant material. Additionally, the width of keratinised mucosa at baseline seems not to influence marginal bone level.

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