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Dependence of Work on the Pulling Speed in Mechanical Ligand Unbinding

Hong An Pham, Duc Toan Truong, and Mai Suan Li*



speed V and, in the linear Bell–Evans regime, $F_{\text{max}} \sim \ln(V)$. Recently, it has been found that non-equilibrium work W is better than F_{max} in describing relative ligand binding affinity, but the dependence of W on V remains unknown. In this paper, we developed an analytical theory showing that in the linear regime, W $\sim c_1 \ln(V) + c_2 \ln^2(V)$, where c_1 and c_2 are constants. This quadratic dependence was also confirmed by all-atom steered molecular dynamics simulations of protein–ligand complexes. Although our theory was developed for ligand unbinding, it is also



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In recent decades, single-molecule force spectroscopy (AFM, laser optical tweezers, and magnetic tweezers) has been widely used to understand biomolecular processes such as protein, RNA, and DNA unfolding, ligand unbinding, and so forth. In experiments, where the external force is ramped up at a constant speed V, the force-displacement/time profile contains the maximum or rupture force F_{max} that can be used to characterize mechanical stability of the biomolecule or binding affinity of the ligand.

The question of the dependence of the rupture force on the puling speed attracts the attention of many researchers because such a dependence can be used to extract the parameters characterizing the free energy landscape. In the linear or Bell–Evans regime, ^{1,2} where V is small enough and it is assumed that the transition state is not shifted under an external force, Evans and Ritchie showed that² $F_{max} \sim \ln(V)$, and this dependence has been confirmed by numerous experimental and simulation works (see ref 3 and references therein). To go beyond the linear regime, different scenarios of the dependence of the rupture force on the pulling speed were proposed.^{4,5}

From a computational point of view, the steered molecular dynamics $(SMD)^{6-8}$ can be used to mimic the results obtained by using single-molecule force spectroscopy. In particular, several groups have shown⁹⁻¹⁴ that this method is effective in predicting the relative binding affinity of small ligands to proteins based on the fact that the greater the rupture force, the higher the binding affinity. SMD can provide results as accurate as other standard methods for estimation of the binding free energy like MM-PBSA but computationally much faster¹¹ as it deals with a non-equilibrium process related with fast pulling. Therefore, the use of this method is becoming

more and more popular in computer-aided drug design.^{9,11,13,15}

It was shown¹⁶ that non-equilibrium work, defined as

$$W = \int \vec{F} \cdot d\vec{r} \tag{1}$$

where r is the ligand displacement, has a better correlation with the experiment on binding affinity than the rupture force because W is defined for the entire process, while F_{max} is calculated in only one state. This result indicates that W can be used as a good score for the ligand binding affinity. Despite this important fact, the dependence of the non-equilibrium work on pulling speed has not been obtained. Moreover, knowledge of this dependence should be useful for a deeper understanding of the free energy landscape of biomolecular systems, especially ligand-receptor complexes. The dependence of the average dissipated work on the displacement in the DNA hairpin pulling experiment was obtained numerically, but the analytical formula was missing.¹⁷ This prompted us to develop a theory by exactly solving a one-dimensional problem, which shows that at sufficiently low pulling speeds, the dependence of W on *V* is determined using the quadratic function of $\ln(V)$. We also

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Figure 1. (A) Schematic description of the SMD method and single-molecule experiment. (B) Force-displacement profile: $F = k_m x$, $k'_m (L_0 - x)$, and 0 for $x \le x^{\ddagger}$, $x^{\ddagger} < x \le L_0$, and $x > L_0$, respectively. (C) Dependence of potential energy $V_0(x)$ given using eq 3 on position. For simplicity, the constant in eq 3 is set to 0. (D) Conceptual graph of free energy *vs x*. The TS, which appears at x^{\ddagger} , separates the bound state from the unbound one.

performed all-atom simulations of protein-ligand complexes in explicit water, which confirmed our theory.

ONE-DIMENSIONAL MODEL WITH HARMONIC POTENTIAL

Following Hummer and Szabo,¹⁸ we consider a one-dimensional motion of a ligand interacting with the receptor through potential $V_0(x)$. In order to mimic the single-molecule force experiment, an external force is applied to a dummy atom which is connected with the ligand using a spring with a spring constant k_s (Figure 1A). Assuming that the external force is increased at a constant speed V, the motion of ligand in the viscous environment is described by the following equation

$$m\ddot{x} = -\frac{\delta}{\delta x}V_0(x) - \overline{\gamma}\dot{x} - k_s(x - Vt) + \xi(t)$$
⁽²⁾

here $x \equiv x(t)$ is the time-dependent displacement, $\overline{\gamma}$ is the Stokes friction coefficient, and $\xi(t)$ is a Gaussian random force with $\langle \xi(t) \rangle = 0$ and $\langle \xi(t)\xi(t') \rangle = 2\overline{\gamma}k_{\rm B}T\delta(t-t')$.

To choose an analytical expression for potential $V_0(x)$, we analyze a typical force-extension profile, obtained for a ligand pulled from the binding site of the protein by using all-atom SMD simulations in explicit water (Figure S1A in the Supporting Information). The ligand motion can be divided into three regimes: $x \le x^{\ddagger}, x^{\ddagger} < x \le L_0$, and $x > L_0$, where x^{\ddagger} corresponds to the position of the rupture force F_{max} and it is the distance from the bound sate and transition state (TS).^{18,19} Note that x^{\ddagger} corresponds to the TS because, as was clearly shown in our previous work,¹⁹ this is the maximum of the binding free energy (see also Figure S1B) obtained by using the Jarzynski's identity.^{20,21} For $x \le x^{\ddagger}$ and $x^{\ddagger} < x \le L_0$, the dependence of the force experienced by the ligand on the displacement can be approximated using a linear function (Figure S1A), that is, $F = k_m x$ and $F = k'_m (L_0 - x)$, respectively

(Figure 1B), where k_m and k'_m are spring constants. Above L_0 , the force and the receptor-ligand interaction disappear. Thus, $V_0(x)$ can be approximated using a harmonic potential as follows

$$V_{0}(x) = \begin{cases} \frac{1}{2}k_{m}x^{2} + \text{const} & (x \le x^{\ddagger}) \\ -\frac{1}{2}k'_{m}(x - L_{0})^{2} & (x^{\ddagger} < x \le L_{0}) \\ 0 & (x > L_{0}) \end{cases}$$
(3)

The constant in eq 3 can be obtained from the condition that the potential must be continuous at the rupture point x^{\ddagger} . In general, the spring constants k_m and k'_m differ from k_s of the cantilever.¹⁸ $V_0(x)$ given by eq 3 correctly describes the fact that in the first regime $(x \le x^{\ddagger})$, the force experienced by the ligand increases and then it decreases in the second regime (x^{\ddagger} $\langle x \leq L_0 \rangle$ before vanishing at $x > L_0$ (Figure 1C). In addition, the dependence of $V_0(x)$ on x (Figure 1C) is similar to that obtained from the SMD simulations (Figure S1C), which implies that our choice of potential energy is reasonable as it is supported by all-atom simulations. Based on the SMD results (Figure S1B), we can schematically describe free energy as a function of displacement (Figure 1D), which shows that ligand binding/unbinding is a barrier-crossing process. Bound and unbound states are separated by the TS, which occurs at the rupture position x^{\ddagger} . Our free energy profile differs, for example, from Hummer and Szabo,¹⁸ who were interested in the behavior of the rupture force without caring about the second regime $x^{\ddagger} < x \le L_0$. By contrast, we must take this regime into account because it contributes to the work. As in the protein folding problem, x^{\ddagger} depends on the external force, but in this work, we assume it to be constant, which means that we adopt the Bell-Evans approximation.

Equation 2 with the harmonic potential (eq 3) was solved exactly, and then, using eq 1, we can obtain W. Because in the third region ($x > L_0$), the work is zero, $W = W_1 + W_2$, where W_1 and W_2 correspond to the first and second intervals, respectively.

Work in the First Region $x \le x^{\ddagger}$. In this region, the ligand is located in the binding site and the viscosity term in eq 2 is neglected as it is much smaller than the ligand-protein interaction term.¹⁸ Then, eq 2 is replaced by eq S1 in the Supporting Information with initial conditions x(0) = 0 and $\dot{x}(0) = v_0$. This equation can be written as eq S2 using the Fourier transformations (eqs S3-S5) and has the exact solution for $x(\omega)$ (eq S6) and velocity $v(\omega)$ (eq S7).

The work in the first region, W_1 , was calculated using the definition given by eq 1 (see also eq S8 in the Supporting Information) and the expression for F (eq S9). After several steps (eqs S10 and S11), we obtained the work which depends on the random force (eq S12). Averaging over the random force (eqs S13–S14) and using rupture time $t_{\text{max}} \approx F_{\text{max}}/k_s V$, we obtained W_1 (eq S15) for one MD trajectory with a given F_{max} .

Work in the Second Region $x^{\ddagger} \le x \le L_0$. In this region, we have to keep the viscosity term and solve full eq 2. Similar to the first case, the motion equation was exactly solved (eqs S16–S19). Details of derivation of the work in the second region, W_2 , are described in the Supporting Information (eqs S20–S22). After averaging over the random force, we obtained the expression for W_2 (eq S24).

Dependence of the Average Total Work on the Pulling Speed. Using eqs S15 and S24, we obtain the total work

$$W = W_{1} + W_{2}$$

$$= \frac{1}{2} \frac{k_{m}}{(k_{s} + k_{m})^{2}} F_{max}^{2} + \frac{\gamma_{0}(\gamma_{0} - 1)}{2k_{s}} F_{max}^{2}$$

$$- \frac{\gamma_{0}^{2}}{k_{s}} (k'_{m}(L_{0} - x^{\ddagger}) + \gamma_{0}V\overline{\gamma})F_{max} - \frac{\gamma_{0}(\gamma_{0} - 1)\overline{\gamma}^{2}}{2k_{s}}V^{2}$$

$$+ \frac{\gamma_{0}^{3}}{k_{s}}\overline{\gamma}^{2}V^{2} - \gamma_{0}^{3}\overline{\gamma}x^{\ddagger}V - \gamma_{0}(\gamma_{0} - 1)L_{0}\overline{\gamma}V$$

$$+ \frac{\gamma_{0}^{2}}{k_{s}}\overline{\gamma}L_{0}(k_{s}\gamma_{0} + k'_{m})V - \gamma_{0}^{2}k'_{m}L_{0}x^{\ddagger}$$

$$+ \frac{\gamma_{0}(\gamma_{0} - 1)}{2}k_{s}(x^{\ddagger})^{2} - \frac{\gamma_{0}(\gamma_{0} - 1)}{2}k_{s}L_{0}^{2} + \gamma_{0}^{2}k'_{m}L_{0}^{2}$$
(4)

where $\gamma_0 = k_s/k_s - k'_m$.

In order to obtain the experimentally measurable work, we have to average W over the distribution of $F_{\text{max}} < W > = \int P(F_{\text{max}})W(F_{\text{max}}) \, dF_{\text{max}}$, where in the Bell–Evans approximation, the distribution of the rupture force is given by the following expression¹⁸

$$P(F_{\max}) = \frac{k_0}{k_s V} e^{\beta F_{\max} x^{\dagger}} \exp\left[\frac{k_0}{\beta x^{\dagger} k_s V} (1 - e^{\beta F_{\max} x^{\dagger}})\right]$$
(5)

where k_0 is the intrinsic rate constant. Using the distribution given by eq 5, one can exactly calculate $\langle F_{max} \rangle$ and $\langle F_{max}^2 \rangle^{18}$

$$\langle F_{\rm max} \rangle = \frac{1}{\beta x^{\ddagger}} \ln \frac{\beta k_s x^{\ddagger} V}{k_0 e^{\gamma}}$$
(6a)

.

$$\langle F_{\max}^2 \rangle = \langle F_{\max} \rangle^2 + \sigma_{F_{\max}}^2 = \left(\frac{1}{\beta x^{\ddagger}}\right)^2 \ln^2 \frac{\beta k_s x^{\ddagger} V}{k_0 e^{\gamma}} + \frac{1}{6} \left(\frac{\pi}{\beta x^{\ddagger}}\right)^2$$
(6b)

with Euler constant $\gamma = 0.577$. Equation 6a describes the wellknown dependence $F_{\text{max}} \sim \ln V^2$, which has been widely used in interpretation of results obtained by single-molecule force spectroscopy for protein unfolding under an external force.^{22,23} This relationship is also valid for the ligand unbinding from the receptor at low loading rates.³

Using eq 6a to calculate the average work eq 4, we obtain

$$W = \frac{1}{2\beta^{2}(x^{\ddagger})^{2}} \left(\frac{\gamma_{0}(\gamma_{0}-1)}{k_{s}} + \frac{k_{m}}{(k_{s}+k_{m})^{2}} \right) \ln^{2}(aV) - \frac{\gamma_{0}^{2}}{k\beta x^{\ddagger}} k'_{m}(L_{0}-x^{\ddagger}) \ln(aV) - \frac{\gamma_{0}^{3}\overline{\gamma}}{ak\beta x^{\ddagger}}(aV) \ln(aV) + \left(\frac{\gamma_{0}^{3}}{a^{2}k_{s}} \overline{\gamma}^{2} - \frac{\gamma_{0}(\gamma_{0}-1)\overline{\gamma}^{2}}{2a^{2}k_{s}} \right) (aV)^{2} + \left(\frac{\gamma_{0}^{2}}{k_{s}} \overline{\gamma} L_{0}(k_{s}\gamma_{0}+k'_{m})}{a} - \frac{\gamma_{0}^{3}\overline{\gamma}x^{\ddagger}}{a} - \frac{\gamma_{0}(\gamma_{0}-1)L_{0}\overline{\gamma}}{a} \right) (aV) + \gamma_{0}^{2}k'_{m}L_{0}^{2} + \frac{\pi^{2}\gamma_{0}(\gamma_{0}-1)}{12k\beta^{2}(x^{\ddagger})^{2}} - \gamma_{0}^{2}k'_{m}L_{0}x^{\ddagger} + \frac{\gamma_{0}(\gamma_{0}-1)}{2}k_{s}(x^{\ddagger})^{2} - \frac{\gamma_{0}(\gamma_{0}-1)}{2}k_{s}L_{0}^{2}$$
(7)

where aV is the dimensionless speed with $a = \beta k_s x^{\ddagger}/k_0 e^{\gamma}$.

In the Jarzynski identity $\exp(-\Delta F/k_{\rm B}T) = \langle \exp(-W/k_{\rm B}T) \rangle$,²⁰ we must calculate the exponential average of work over all possible trajectories connecting the states A and B. The free energy difference $\Delta F = F_{\rm B} - F_{\rm A}$, which is obtained in equilibrium, does not depend on the pulling speed, and the exponential average of work is also independent of *V*, despite the fact that work distribution depends on the pulling speed. This can be explained by the fact that trajectories with small *W* (rare events) make the largest contribution to the exponential average. Because the process with small *W* is very close to equilibrium, $\langle \exp(-W/k_{\rm B}T) \rangle$ does not depend on the pulling speed. In our case, we calculated the linear average of work, $\langle W \rangle$, where the contribution from trajectories with large *W* (far from equilibrium) is important, and therefore, the result depends on the pulling speed.

To estimate the contribution of each term in eq 7, we rewrite the mechanical work as follows

$$W = a_1 \ln^2(aV) - a_2 \ln(aV) - a_3(aV) \ln(aV) + a_4(aV)^2 + a_5(aV) + a_6$$
(8)

where a_1 , ..., and a_6 , which have a unit of energy, are shown in the Supporting Information (eq S25). To estimate these coefficients, we took the typical value of the spring constant of the cantilever in the AFM experiment ~1 $N m^{-1}$,²⁴ the friction coefficient $\overline{\gamma} \sim 10^{-14} \text{ kg s}^{-1}$,²⁵ and rate constant $k_0 \approx 10^7 \text{ s}^{-1}$.²⁶ The rupture position and rupture force depend on the system and pulling speed (see Figure S1B and ref 19), but we can set $x^{\ddagger} \approx 10^{-10}$ m and $F_{\text{max}} \approx 1000$ pN. Then, the spring constant $k_m \approx F_{\text{max}}/x^{\ddagger} \approx 1000$ pN/ $(10^{-10} \text{ m}) \approx 10$ Nm⁻¹. The spring constant k'_m can be obtained from the condition that the first derivative of $V_0(x)$ with respect to x should be continuous at x^{\ddagger} , which implies that $k_m x^{\ddagger} = k'_m (L_0 - x^{\ddagger})$. Using $L_0 \approx 2$ nm (Figure S1A) and the values of k_m and x^{\ddagger} given here, we obtain $k'_m \approx 0.5$ Nm⁻¹. For clarity, all parameters which will be used for estimation of $a_1 - a_6$ are shown in eq S26 in the Supporting Information. Using eq S25 and these parameters, we obtained $a_1 \sim 10^{-21}$, $a_2 \sim 10^{-21}$, $a_3 \sim 10^{-27}$, $a_4 \sim 10^{-34}$, $a_5 \sim 10^{-25}$, and $a_6 \sim 10^{-18}$ J (Table S1). We tested a few different sets of parameters, but the results did not change qualitatively.

It can be shown that for low pulling speeds $V < 10^2$ nm/ns, the third, fourth, and fifth terms in eq 8 can be neglected, resulting in the following expression of the average work

$$W = \frac{1}{2\beta^{2}(x^{\ddagger})^{2}} \left(\frac{\gamma_{0}(\gamma_{0}-1)}{k_{s}} + \frac{k_{m}}{(k_{s}+k_{m})^{2}} \right) \ln^{2}(aV)$$

$$- \frac{\gamma_{0}^{2}}{k_{s}\beta x^{\ddagger}} k'_{m}(L_{0}-x^{\ddagger}) \ln(aV) + \gamma_{0}^{2}k'_{m}L_{0}^{2}$$

$$+ \frac{\pi^{2}\gamma_{0}(\gamma_{0}-1)}{12k_{s}\beta^{2}(x^{\ddagger})^{2}} - \gamma_{0}^{2}k'_{m}L_{0}x^{\ddagger} + \frac{\gamma_{0}(\gamma_{0}-1)}{2}k_{s}(x^{\ddagger})^{2}$$

$$- \frac{\gamma_{0}(\gamma_{0}-1)}{2}k_{s}L_{0}^{2}$$
(9)

Because the experiment is conducted at low $V \sim nm/s$, this dependence must be valid for its interpretation. Thus, in the Bell–Evans approximation, contrary to the rupture force case, the dependence of work on the pulling speed contains not only the ln(V) term but also the quadratic term $ln^2(V)$. At high pulling speeds $V > 10^2$ nm/ns, the terms $\sim V$ and V^2 in eq 8 prevail over logarithmic terms, but this area is not interesting from an experimental point of view.

SMD Simulations. To support our analytical theory (eq 9), we performed all-atom SMD simulations with explicit water for two protein–ligand complexes: the SBX small compound bound with the FKBP12 protein (PDB ID: 1FKH) and ZB6 carboxylic acid, a small compound, in complex with the AmpC beta-lactamase protein(PDB ID: 4KZ6) (Figure S2). The FKBP12 protein, consisting of 107 amino acids,²⁷ is a cytosolic protein that is abundantly expressed in all tissues. It binds to FK506 and rapamycin, mediating the immunosuppressive action of drugs.²⁸ Beta-lactamase,²⁹ a well-known enzyme produced by bacteria,³⁰ is responsible for bacterial resistance to many beta-lactam antibiotics. For clarity, the two protein–ligand complexes will hereinafter be referred as 1FKH and 4KZ6 after their PDB code.

We used the CHARMM27 force field 33^{31} and the TIP3P³² water model for molecular modeling. SMD simulations were carried out for a pulling speed V in the range 0.025-54 nm/ns, where eq 9 is applicable. Simulations below this range are beyond our computational capabilities. The number of trajectories was from 10 to 200 depending on the system and V (Table S2 in the Supporting Information). To mimic the AFM experiment, we chose the typical spring constant $k_s = 600$ kJ/(mol nm²) of the spring that connects the center of mass of the ligand to the dummy atom. To prevent the receptor from drifting under the influence of an external force, its C α -atoms were restrained but the side chains were allowed to fluctuate. The details on SMD simulations are given in Supporting

Information. The results obtained for F_{max} and W of two complexes with various pulling speeds are shown in Table S3. At low pulling speeds, the rupture force is linear with $\ln(V)$ (Figure 2) for both systems, but for 1FKH (the first nine

1400 u = 1**1FPK** u = 2Rupture force (pN) 1200 1000 800 600 400<u>-</u>6 Ln(V)1400 u = 1/21200 4KZ6 u = 2/3Rupture force (pN) 1000 800 600 400 200 Ln(V)

Figure 2. Dependence of the rupture force F_{max} on the logarithm of the pulling speed for complexes 1FKH (top) and 4KZ6 (bottom). The blue line is a linear fit for the first nine data points of 1FPK (R = 0.983) and the first seven points of 4KZ6 (R = 0.955). The correlation level R is shown in parentheses. The arrow indicates the point below which the Bell–Evans theory applies. The red and green curves are nonlinear fits using Dudko–Hummer–Szabo theory with $\nu = 1/2$ and 2/3 for the whole data set ($\nu = 1$ corresponds to Bell–Evans theory). For 1FPK, R = 0.994 and 0.992 for $\nu = 1/2$ and 2/3, respectively, and for 4KZ6, R = 0.991 for both values of ν .

points), the linear theory works over a wider range than 4KZ6 (the first seven points). The correlation level of the fit is high with R = 0.98 and 0.96 for 1FPK and 4KZ6, respectively. Dudko-Hummer-Szabo nonlinear theory with $\nu = 1/2$ and $2/3^4$ is applicable to the entire region (Figure 2).

Because our theory was developed in the Bell–Evans approximation, we first applied the quadratic fit (eq 9) to the region where the rupture force linearly depends on $\ln(V)$, confining ourselves to the data points on the left side of the arrow in Figure 3. This fit (green curve) works perfectly for 1FPK (R = 0.996) and 4KZ6 (R = 0.997), which fully supports our theory. The blue curve in Figure 3 is a quadratic fit for the entire data set. Because the fit is good with R = 0.983 and 0.988 for 1FPK and 4KZ6, respectively, within error bars, our theory works for a wider range than linear. This may be due to the fact that compared with the Bell–Evans theory, we have one more fitting parameter associated with the term $\ln^2(V)$. Additional protein–ligand complexes should be studied to clarify this issue.



Figure 3. Dependence of *W* on $\ln(V)$ for 1FKH (top) and 4KZ6 (bottom). The arrow refers to the point below which the rupture F_{max} is linear with $\ln(V)$. The green curve is a quadratic fit for the first nine data points of 1FPK (R = 0.996) and the first 7 points of 4KZ6 (R = 0.997), which is the area where Bell–Evans theory is valid. The correlation level is indicated in parentheses. The blue curve is also the quadratic fit but for the entire data set with R = 0.983 and 0.988 for 4FPK and 4KZ6, respectively.

Ln(V)

CONCLUSIONS

We developed a theory for the dependence of the mechanical work performed by the ligand during the escape from the receptor binding site on the pulling speed. Our exactly solvable one-dimensional model was based on the results obtained using all-atom MD simulations with explicit water. Assuming that the position of the transition state does not depend on the external force and that the receptor-ligand interaction can be described using a harmonic potential, we obtained the exact expression of *W* as a quadratic function of $\ln(V)$ at low enough pulling speeds. It would be interesting to confirm our theory experimentally. Although our theory was developed for ligand unbinding, it should be applied to the mechanical unfolding of proteins, RNA, and DNA and, presumably, to other more complex processes in cells.³³ In general, the quadratic dependence (eq 9) works for the case when the forceextension profile is similar to the one shown in Figure 1B, that is, unbinding/unfolding occurs without intermediates.

Agmon and Hopfield³⁴ developed a two-dimensional model of CO binding to heme proteins, in which the conceptual protein coordinate is included in addition to the CO-iron distance. This model can be used³⁵ to understand recent experiments on enzyme-catalyzed reduction of disulfide bonds in proteins using the mechanical force applied to the ends of the protein.³⁶ Thus, it would be interesting to extend our theory to the case where the ligand binding reaction coordinate is coupled to the protein coordinate that is responsible for the disulfide bond cleavage.³⁵ This problem is challenging due to the biphasic force dependence of the bond breaking rate.

Single-molecule force spectroscopy is an effective tool for studying the breaking and formation of non-covalent protein—protein bonds, which are critical for the functions of cell adhesion complexes. It is generally believed that the external force reduces the free energy barrier to break the bond and thus shortens the bond lifetime.² In contrast, Dembo *et al.*^{37,38} hypothesized that force can also increase the bond lifetime by transforming the adhesive complexes into a bound state.

These two different ways of responding to external force, known as slip and grip tricks.^{37,38} By developing a phenomenological theory, Barsegov and Thirumalai showed³⁹ that the dependence of the rupture force on $\ln(V)$ is linear in the slip regime, while it becomes more complicated (almost linear but with two different slopes) in the catch bond regime. Because our theory was developed for the case when $F_{\rm max} \sim \ln(V)$, it is applicable to the slip mode. Extension to the case, where catch–slip transition occurs, requires further investigation. Then, instead of one bound state in the energy landscape, one has to deal with two bound states or two pathways.³⁹

In general, extension of our theory beyond the Bell–Evans approximation is of great interest. Work in this direction is in progress.

ASSOCIATED CONTENT

Supporting Information

The Supporting Information is available free of charge at https://pubs.acs.org/doi/10.1021/acs.jpcb.1c01818.

Typical force-displacement profiles, binding free energy and potential energy obtained by using all-atom SMD simulations at a pulling speed V = 5 nm/ns; derivation of the analytical expression for the pulling work; SMD simulations of 1FPK and 4KZ6 in complex with different ligands; number of trajectories used for various pulling speeds; and average rupture force and pulling work obtained by using SMD simulations for systems 1FPK and 4KZ6 (PDF)

AUTHOR INFORMATION

Corresponding Author

Mai Suan Li – Institute of Physics, Polish Academy Science, Warsaw 02-668, Poland; Occid.org/0000-0001-7021-7916; Phone: +48 886813018; Email: masli@ifpan.edu.pl

Authors

- Hong An Pham Institute for Computational Science and Technology, Ho Chi Minh City 700000, Vietnam
- **Duc Toan Truong** Institute for Computational Science and Technology, Ho Chi Minh City 700000, Vietnam

Complete contact information is available at: https://pubs.acs.org/10.1021/acs.jpcb.1c01818

Author Contributions

MSL designed the research. HAP and DTT conducted the experiment. HAP, DTT, and MSL analyzed the results. All authors wrote and reviewed the article.

Notes

The authors declare no competing financial interest.

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REFERENCES

(1) Bell, G. Models for the specific adhesion of cells to cells. *Science* **1978**, 200, 618–627.

(2) Evans, E.; Ritchie, K. Dynamic strength of molecular adhesion bonds. *Biophys. J.* **1997**, *72*, 1541–1555.

(3) Rico, F.; Russek, A.; González, L.; Grubmüller, H.; Scheuring, S. Heterogeneous and rate-dependent streptavidin—biotin unbinding revealed by high-speed force spectroscopy and atomistic simulations. *Proc. Natl. Acad. Sci. U.S.A.* **2019**, *116*, 6594–6601.

(4) Dudko, O.; Hummer, G.; Szabo, A. Intrinsic rates and activation free energies from single-molecule pulling experiments. *Phys. Rev. Lett.* **2006**, *96*, 108101–108104.

(5) Friddle, R. W.; Noy, A.; De Yoreo, J. J. Interpreting the widespread nonlinear force spectra of intermolecular bonds. *Proc. Natl. Acad. Sci. U.S.A.* **2012**, *109*, 13573–13578.

(6) Grubmüller, H.; Heymann, B.; Tavan, P. Ligand binding: molecular mechanics calculation of the streptavidin-biotin rupture force. *Science* **1996**, *271*, 997–999.

(7) Izrailev, S.; Stepaniants, S.; Balsera, M.; Oono, Y.; Schulten, K. Molecular dynamics study of unbinding of the avidin-biotin complex. *Biophys. J.* **1997**, *72*, 1568–1581.

(8) Isralewitz, B.; Izrailev, S.; Schulten, K. Binding pathway of retinal to bacterio-opsin: a prediction by molecular dynamics simulations. *Biophys. J.* **1997**, *73*, 2972–2979.

(9) Colizzi, F.; Perozzo, R.; Scapozza, L.; Recanatini, M.; Cavalli, A. Single-molecule pulling simulations can discern active from inactive enzyme inhibitors. *J. Am. Chem. Soc.* **2010**, *132*, 7361–7371.

(10) Mai, B. K.; Viet, M. H.; Li, M. S. Top leads for swine influenza A/H1N1 virus revealed by steered molecular dynamics approach. *J. Chem. Inf. Model.* **2010**, *50*, 2236–2247.

(11) Suan Li, M.; Khanh Mai, B. Steered molecular dynamics-a promising tool for drug design. *Curr. Bioinf.* **2012**, *7*, 342–351.

(12) Villarreal, O. D.; Yu, L.; Rodriguez, R. A.; Chen, L. Y. Computing the binding affinity of a ligand buried deep inside a protein with the hybrid steered molecular dynamics. *Biochem. Biophys. Res. Commun.* **2017**, 483, 203–208.

(13) Chen, L. Y. Hybrid Steered Molecular Dynamics Approach to Computing Absolute Binding Free Energy of Ligand-Protein Complexes: A Brute Force Approach That Is Fast and Accurate. *J. Chem. Theory Comput.* **2015**, *11*, 1928–1938.

(14) Ytreberg, F. M. Absolute FKBP binding affinities obtained via nonequilibrium unbinding simulations. *J Chem Phys* **2009**, *130*, 164906.

(15) Ho, K.; Truong, D. T.; Li, M. S. How Good is Jarzynski's Equality for Computer-Aided Drug Design? *J. Phys. Chem. B* 2020, 124, 5338–5349.

(16) Vuong, Q. V.; Nguyen, T. T.; Li, M. S. A new method for navigating optimal direction for pulling ligand from binding pocket: application to ranking binding affinity by steered molecular dynamics. *J. Chem. Inf. Model.* **2015**, *55*, 2731–2738.

(17) Monge, A. M.; Manosas, M.; Ritort, F. Experimental test of ensemble inequivalence and the fluctuation theorem in the force ensemble in DNA pulling experiments. *Phys. Rev. E* **2018**, *98*, 032146.

(18) Hummer, G.; Szabo, A. Kinetics from nonequilibrium singlemolecule pulling experiments. *Biophys. J.* **2003**, *85*, 5–15.

(19) Truong, D. T.; Li, M. S. Probing the Binding Affinity by Jarzynski's Nonequilibrium Binding Free Energy and Rupture Time. *J. Phys. Chem. B* **2018**, *122*, 4693–4699.

(20) Jarzynski, C. Nonequilibrium equality for free energy differences. *Phys. Rev. Lett.* **1997**, *78*, 2690–2693.

(21) Hummer, G.; Szabo, A. Free energy reconstruction from nonequilibrium single-molecule pulling experiments. *Proc. Natl. Acad. Sci. U.S.A.* **2001**, *98*, 3658–3661.

(22) Williams, P. M.; Fowler, S. B.; Best, R. B.; Luis Toca-Herrera, J.; Scott, K. A.; Steward, A.; Clarke, J. Hidden complexity in the mechanical properties of titin. *Nature* **2003**, *422*, 446–449.

(23) Kumar, S.; Li, M. S. Biomolecules under mechanical force. *Phys. Rep.* **2010**, 486, 1–74.

(24) Binnig, G.; Quate, C. F.; Gerber, C. Atomic Force Microscope. *Phys. Rev. Lett.* **1986**, *56*, 930–933.

(25) Veitshans, T.; Klimov, D.; Thirumalai, D. Protein folding kinetics: timescales, pathways and energy landscapes in terms of sequence-dependent properties. *Folding Des.* **1997**, *2*, 1–22.

(26) Bruce, N. J.; Ganotra, G. K.; Kokh, D. B.; Sadiq, S. K.; Wade, R. C. New approaches for computing ligand-receptor binding kinetics. *Curr. Opin. Struct. Biol.* **2018**, *49*, 1–10.

(27) Clackson, T.; Yang, W.; Rozamus, L. W.; Hatada, M.; Amara, J. F.; Rollins, C. T.; Stevenson, L. F.; Magari, S. R.; Wood, S. A.; Courage, N. L.; Lu, X.; Cerasoli, F.; Gilman, M.; Holt, D. A. Redesigning an FKBP-ligand interface to generate chemical dimerizers with novel specificity. *Proc. Natl. Acad. Sci. U.S.A.* 1998, 95, 10437-10442.

(28) Ivery, M. T. G. Immunophilins: switched on protein binding domains? *Med. Res. Rev.* 2000, 20, 452-484.

(29) Majiduddin, F. K.; Materon, I. C.; Palzkill, T. G. Molecular analysis of beta-lactamase structure and function. *IJMM Int. J. Med. Microbiol.* **2002**, 292, 127.

(30) Jameel, N.-u.-A.; Ejaz, H.; Zafar, A.; Amin, H. Multidrug resistant AmpC β -lactamase producing Escherichia coli isolated from a paediatric hospital. *Pakistan J. Med. Sci.* **2014**, *30*, 181.

(31) MacKerell, A. D., Jr; Banavali, N.; Foloppe, N. Development and current status of the CHARMM force field for nucleic acids. *Biopolymers* **2000**, *56*, 257–265.

(32) Sun, Y.; Kollman, P. A. Hydrophobic solvation of methane and nonbond parameters of the TIP3P water model. *J. Comput. Chem.* **1995**, *16*, 1164–1169.

(33) Müller, D. J.; Dumitru, A. C.; Lo Giudice, C.; Gaub, H. E.; Hinterdorfer, P.; Hummer, G.; De Yoreo, J. J.; Dufrêne, Y. F.; Alsteens, D. Atomic Force Microscopy-Based Force Spectroscopy and Multiparametric Imaging of Biomolecular and Cellular Systems. *Chem Rev.* **2020**, DOI: 10.1021/acs.chemrev.0c00617.

(34) Agmon, N.; Hopfield, J. J. CO binding to heme proteins: A model for barrier height distributions and slow conformational changes. *J. Chem. Phys.* **1983**, *79*, 2042–2053.

(35) Roy, M.; Grazioli, G.; Andricioaei, I. Rate turnover in mechanocatalytic coupling: A model and its microscopic origin. *J. Chem. Phys.* **2015**, *143*, 045105.

(36) Liang, J.; Fernández, J. M. Kinetic Measurements on Single-Molecule Disulfide Bond Cleavage. J. Am. Chem. Soc. 2011, 133, 3528–3534.

(37) Dembo, M.; Torney, D. C.; Saxman, K.; Hammer, D.; Murray, J. D. The reaction-limited kinetics of membrane-to-surface adhesion and detachment. *Proc. R. Soc. Lond. Ser. B Biol. Sci.* **1988**, 234, 55–83.

(38) Dembo, M. Lectures on Mathematics in the Life Sciences. Some Mathematical Problems in Biology; American Mathematical Society: Providence, RI, 1994; Vol. 24, pp 51–77.

(39) Barsegov, V.; Thirumalai, D. Dynamics of unbinding of cell adhesion molecules: transition from catch to slip bonds. *Proc. Natl. Acad. Sci. U. S. A.* **2005**, *102*, 1835–1839.