

# Evaluation of the calculation formulas of the cardio-ankle vascular index used in the Japanese apparatus

This article was published in the following Dove Press journal:  
*Vascular Health and Risk Management*

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**Background:** Recently, coefficients in the equation of cardio-ankle vascular index (CAVI) used in VaSera<sup>®</sup> device were disclosed. This study aimed to simulate the influence of adjusting the coefficients in the equation of CAVI and also aimed to validate the equation.

**Methods:** The CAVI displayed by VaSera (CAVIs) and the CAVI estimated (CAVIEs) with fixing the coefficients of the middle range of the heart-ankle stiffness parameter  $\beta$  ( $ha\beta$ ) in the equation were compared. Moreover, the heart-ankle pulse wave velocity ( $haPWV$ ) which corresponds to the low cutoff  $ha\beta$  of 7.348 was estimated in various blood pressure patterns to validate the formula.

**Results:** The CAVIs was clearly lower than CAVIEs in the low and the high range of CAVIs. Moreover, it was virtually impossible to obtain the low cutoff  $ha\beta$  of 7.348 by using typical values of  $haPWV$ .

**Conclusion:** The CAVIs in the high-range of VaSera underestimates the original property of stiffness parameter  $\beta$ . Moreover, there will be also a missing information in the equations introduced in the corresponding article, especially in the calculation formula of CAVIs from  $ha\beta$ . Therefore, in order to make the best use of the nature of the stiffness parameter  $\beta$  to be used in VaSera, fixing the coefficients or termination of its use should be considered.

**Keywords:** brachial-ankle pulse wave velocity, arterial stiffness, arterial compliance, vascular function, peripheral arterial disease, ankle-brachial index

In a recent article published in the *Journal of Atherosclerosis and Thrombosis*, Takahashi et al disclosed the values of coefficients “a” and “b”, which are used to calculate the cardio-ankle vascular index (CAVI) using the VaSera<sup>®</sup> (VS) device.<sup>1</sup> CAVI estimated using VS (CAVIs) is a blood pressure-adjusted product of heart-ankle ( $ha$ ) pulse wave velocity ( $PWV$ ); the concept of CAVI is derived from the stiffness parameter  $\beta$ .

The  $\beta$  value for  $haPWV$  ( $ha\beta$ ) is calculated using the following equation:<sup>1</sup>

$$ha\beta = 2\rho \times haPWV^2 \times \text{Ln}[SBP/DBP] \div (SBP - DBP)$$

where  $\rho$  is blood density (fixed value of 1.05 in VS devices),  $\text{Ln}$  is natural logarithm, SBP is systolic blood pressure (SBP), and DBP is diastolic blood pressure (DBP).

CAVIs is calculated using the following equation:<sup>1</sup>

$$CAVIs = a \times ha\beta + b$$

Regarding this equation, Takahashi et al disclosed that the coefficients “a” and “b” were changed by the  $ha\beta$  level (Table 1) to adjust  $ha\beta$  to Hasegawa-PWV ( $H-PWV$ ). They explained the reason as follows:

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**Table 1** The coefficients of a and b according to  $ha\beta$  and CAVIvs

$ha\beta$	Low range	Middle range	High range
	$<7.34875$	$7.34875 \leq to < 10.30372$	$10.30372 \leq$
a	0.85	0.658	0.432
b	0.695	2.103	4.441
CAVIvs	$<6.9414375$	$6.9384775 \leq to < 8.88284776$	$8.89220704 \leq$

**Note:**  $CAVIvs = a \times ha\beta + b$ .

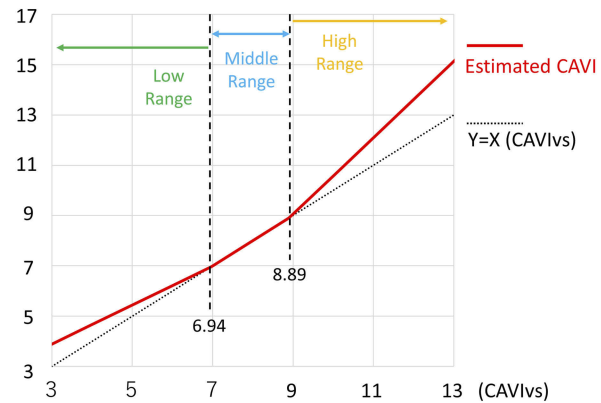
**Abbreviations:** ha, heart-ankle; CAVIvs, cardio-ankle vascular index measured by VaSera®.

Because  $ha\beta$  is based on PWV squared, whereas H-PWV is based solely on PWV, it is difficult to maintain a high correlation in a wide range of values with one approximate adjustment. For this reason, the portion that coincides with the correlation equation of  $ha\beta$  and H-PWV was defined as the middle range. For the upper and lower ranges that were outside the middle range, the coefficients were adjusted so that the difference between H-PWV and CAVI was small throughout the clinical range.<sup>1</sup>

Here, a fundamental issue arises. Generally, the logic of the blood pressure (BP) independency of the stiffness parameter  $\beta$  is considered appropriate. However, originally, this hypothesis is to be applied on one arterial location. No logical explanation exists as to why this method is also perfectly valid in the evaluation of the long distant arteries with multiple segments. Nevertheless, we suppose that  $ha\beta$  is also BP independent. If we fix the coefficients of “a” and “b”, we can suppose that the characteristics of  $ha\beta$  is also reserved in all of the CAVIvs range. However, if coefficients “a” and “b” change according to the  $ha\beta$  value, the change in CAVIvs cannot properly reflect the original change in  $ha\beta$  when CAVIvs fluctuates across the points where the coefficients change (Figure 1). Therefore, the whole range of CAVIvs can never maintain the property of  $ha\beta$  nor stiffness parameter  $\beta$ . In fact, Lim et al demonstrated the difference between CAVIvs and the stiffness parameter  $\beta$  in a BP perturbation study.<sup>2</sup> In this study, the change in CAVIvs correlated with that in BP, whereas the change in stiffness parameter  $\beta$  measured at the carotid segment did not. This indicates the BP dependency of CAVIvs and the difference between CAVIvs and “real” stiffness parameter  $\beta$ , although direct comparison was impossible due to different segments.

Regarding BP dependency of CAVI, Steppan et al demonstrated the BP dependency of CAVI in a rat model.<sup>3</sup> Furthermore, Spronck et al and Segers elegantly proved the residual BP dependency of CAVI.<sup>4-6</sup> Moreover, the author pointed out a fundamental discrepancy in BP

Presented CAVI



Abbreviations: CAVI, cardio-ankle vascular index; CAVIvs, cardio-ankle vascular index measured by VaSera®

**Figure 1** CAVIvs and estimated CAVI if the coefficients in the middle range of  $ha\beta$  were fixed in the whole range.

**Notes:** The horizontal axis means the value of CAVIvs. The vertical axis means the CAVI value according to the methods. The red line shows the CAVI estimated by the coefficients of the middle range fixed.

measured using an oscillometric method from the internal arterial pressure measured with the catheter method.<sup>7</sup>

In addition, there will be also a fault in the equations introduced in the corresponding article.<sup>1</sup> If we calculate  $ha\beta$  using typical  $haPWV$  value of 7 m/s (and SBP; 115 mmHg, DBP; 75 mmHg), the  $ha\beta$  is 1.10. The required  $haPWV$  to obtain the low cutoff  $ha\beta$  of 7.348 in several BP patterns is summarized in Table 2. The required  $haPWV$  values are considered too high for the middle-aged subjects with low cutoff  $ha\beta$  and CAVIvs because  $haPWV$  is inevitably much lower than  $baPWV$  due to the measurement process.<sup>8</sup> Moreover, according to the study which adopted the same method using  $baPWV$  and central BP on the  $ha\beta$  equation,<sup>9</sup> the central SBP was  $115 \pm 1.0$  mmHg (mean  $\pm$  standard error (SEM)), the central DBP was  $75 \pm 1.0$  mmHg (SEM), and the  $baPWV$  was  $16 \pm 0.2$  m/s (SEM). However, the “brachial-ankle  $\beta$ ” was  $5.6 \pm 0.1$  (SEM), which is much lower than the low cutoff  $ha\beta$  of 7.348.

In reality, the SI units should be used for the calculation,  $\rho$  should be  $1500 \text{ kg/m}^3$  (not  $1.05 \text{ g/cm}^3$  or  $1.05 \text{ kg/L}$ ), and the unit of BP should be Pa (using the conversion value of  $1 \text{ mmHg} = 133.32 \text{ kg/[m s}^2]$ ).<sup>10</sup> Table 3 shows the revision of Table 2 using SI units. The results are plausible for  $haPWV$ . Therefore, Takahashi et al should have clarified these points.<sup>1</sup>

Tabara et al recently found the so-called regression-to-the-mean phenomenon after multivariate adjustment of the longitudinal change in CAVIvs (in about 5 years) in the general population.<sup>11</sup> In this study, the most powerful

**Table 2** The haPWV to obtain ha $\beta$  of 7.348 in various BP patterns

SBP (mmHg)	80	100	120	130	140	160	180
DBP (mmHg)	50	60	70	80	90	100	110
haPWV (m/s)	14.945	16.553	18.016	18.983	19.899	21.135	22.301

**Abbreviations:** ha, heart-ankle; PWV, pulse wave velocity; BP, blood pressure; SBP, systolic blood pressure; DBP, diastolic blood pressure.

**Table 3** The haPWV to obtain ha $\beta$  of 7.348 in various BP patterns using SI units

SBP (mmHg)	80	100	120	130	140	160	180
DBP (mmHg)	50	60	70	80	90	100	110
↓	↓	↓	↓	↓	↓	↓	↓
SBP (Pa)	10,665.6	13,332	15,998.4	17,331.6	18,664.8	21,331.2	23,997.6
DBP (Pa)	6666	7999.2	9332.4	10,665.6	11,998.8	13,332	14,665.2
haPWV (m/s)	5.457	6.044	6.578	6.931	7.266	7.717	8.143

**Notes:** 1 mmHg is converted to 133.32 Pa.  $\rho$  is 1050 kg/m<sup>3</sup>.

**Abbreviations:** ha, heart-ankle; PWV, pulse wave velocity; BP, blood pressure; SBP, systolic blood pressure; DBP, diastolic blood pressure.

independent determinant of the change in CAVIvs ( $\Delta$ CAVIvs) was the baseline CAVIvs (standardized coefficient,  $-0.590$ ;  $P < 0.001$ ). Moreover,  $\Delta$ CAVIvs was approximately  $-0.3$  in the subjects with a baseline CAVIvs of  $\geq 9.5$ , which indicated a decrease in CAVIvs in the multivariate adjusted model. The reason for these phenomena may be partly explained by the decrease in the coefficient “a” in the high range of ha $\beta$  compared with that in the middle range of ha $\beta$ .

Therefore, if we continue to use CAVIvs, we must be aware of the difference in CAVIvs from that of ha $\beta$  when CAVIvs changes across the designated low and high points of CAVIvs (6.94 and 8.89, respectively). We must also recognize the substantial underestimation of the significance of high CAVIvs ( $> 8.89$ ) in regard to the original significance of the stiffness parameter  $\beta$ . Moreover, any fault in the corresponding article<sup>1</sup> as pointed out above must be immediately amended.

Finally, if the original nature of stiffness  $\beta$  is to be properly adopted for haPWV in the VS device, the author suggests revalidation of the previous and upcoming data by fixing the coefficients or terminating the use of coefficients “a” and “b”. This will be the best way to use the concept of stiffness parameter  $\beta$  on PWV indices not only for ourselves but also for the researchers and the patients in the future. Grillo et al suggest that the calculation of  $\beta$ -stiffness index from PWV and BP-values is an interesting evolution that could overcome limitations and ambiguities derived from the BP dependency of the properties of the arterial wall, although the way of calculating this parameter is still debated.<sup>12</sup> Combined use of the CAVI-0

method can be considered as well.<sup>4-7</sup> Recently, Spronck et al presented an easy and useful method (using simple software, either Microsoft<sup>®</sup> Excel or PDF) to convert CAVIvs to CAVI0, which will greatly help in the simultaneous research on CAVIvs and CAVI0.<sup>13</sup> The use of CAVIvs has spread widely. However, around 15 years have passed since it was produced, and it is used as a parameter only in VaSera. Conversely, adaptation of the stiffness  $\beta$  method on PWVs without using coefficients is the simplest method and will be available for the foreseeable future. In this situation, some difficulty is expected to emerge in the compatibility between CAVIvs and other PWV-derived stiffness  $\beta$ . As adequate data have been accumulated using VS, estimation of CAVI no longer has to rely on H-PWV data with deteriorating the nature of stiffness parameter  $\beta$ .

## Acknowledgment

The author appreciates the researchers and participants of the preceding studies.

## Disclosure

Dai Ato is a former employee of Fukuda Colin (formerly Omron Colin, Nippon Colin) Co., Ltd., a distributor of Vascular Profiler<sup>®</sup> (form PWV/ABI, BP-203RPE series). Dai Ato is an independent researcher and wrote this article as an academic activity based on the guaranteed right of freedom in academia for the Japanese (Article 23) and on the supreme law provided in Article 98 of the Constitution of Japan. Dai Ato reports no other conflicts of interest in this work.

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