

Application of nanoparticles for oral delivery of acid-labile lansoprazole in the treatment of gastric ulcer: in vitro and in vivo evaluations

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Abstract: The aim of this study was to develop nanoparticles for oral delivery of an acid-labile drug, lansoprazole (LPZ), for gastric ulcer therapy. LPZ-loaded positively charged Eudragit® RS100 nanoparticles (ERSNPs-LPZ) and negatively charged poly(lactic-co-glycolic acid) nanoparticles (PLGANPs-LPZ) were prepared. The effect of charge on nanoparticle deposition in ulcerated and non-ulcerated regions of the stomach was investigated. The cellular uptake of nanoparticles in the intestine was evaluated in a Caco-2 cell model. The pharmacokinetic performance and ulcer healing response of LPZ-loaded nanoparticles following oral administration were evaluated in Wistar rats with induced ulcers. The prepared drug-loaded ERSNPs-LPZ and PLGANPs-LPZ possessed opposite surface charge ($+38.5 \pm 0.3$ mV versus -27.3 ± 0.3 mV, respectively) and the particle size was around 200 nm with a narrow size distribution. The negatively charged PLGANPs adhered more readily to the ulcerated region ($7.22 \pm 1.21\%$ per cm^2), whereas the positively charged ERSNPs preferentially distributed in the non-ulcerated region ($8.29 \pm 0.35\%$ per cm^2). Both ERSNPs and PLGANPs were prominent uptake in Caco-2 cells, too. The nanoparticles sustained and prolonged LPZ concentrations up to 24 hours, and the half-life and mean residence time of LPZ were prolonged by 3.5-fold and 4.5-fold, respectively, as compared with LPZ solution. Oral administration of LPZ-loaded nanoparticles healed 92.6%–95.7% of gastric ulcers in Wistar rats within 7 days.

Keywords: nanoparticles, lansoprazole, Eudragit® RS100, PLGA

Introduction

Acid-related disorders, such as peptic ulcer and gastroesophageal reflux disease, frequently occur in elderly people and are associated with morbidity.¹ Proton pump inhibitors are the most effective drugs for ulcer healing and achieve greater symptomatic relief in patients. The mechanism of action of proton pump inhibitors is via selective inhibition of H^+/K^+ ATPase (also known as the proton pump), an enzyme system present in gastric parietal cells, to suppress secretion of gastric acid and promote ulcer healing activity in patients.² Lansoprazole (LPZ) is a proton pump inhibitor. It is metabolized in the parietal cells to form an active sulfonamide metabolite that inactivates the sulfhydryl group of the proton pump, thereby reducing hydrogen ion secretion.³ LPZ induces onset of maximal acid suppression more rapidly than its analogs and provides earlier and better symptom relief.⁴

LPZ is an acid-labile and poorly water-soluble drug.⁵ It is necessary to protect LPZ from degradation in gastric acid when orally administered. The commercial available solid dosage forms of LPZ include enteric-coated granules, tablets, and capsules. The enteric delayed-release dosage form of LPZ has been reported to be unable

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to efficiently suppress nocturnal acid secretion in the event of gastroesophageal reflux disease.^{6,7} Nocturnal acid breakthrough frequently occurs in patients with gastroesophageal reflux disease during the first half of the sleeping period, and affects sleep quality and daytime functioning.

Eudragit® RS100 and poly(lactic-co-glycolic acid) (PLGA) polymers have been used as drug carriers. Eudragit RS100 is insoluble but swellable at physiological pH. It contains 4.5%–6.8% quaternary ammonium groups that impart a positive charge to the polymer and is responsible for the bioadhesive properties of this polymer.⁸ Eudragit RS100 has been used to prepare sustained-release nanoparticulate dosage forms. Adibkia et al developed Eudragit nanoparticles to sustain delivery of naproxen via ocular and intra-articular administration.⁹ Devarajan and Sonavane reported that Eudragit nanoparticles enabled a sustained-release profile for gliclazide after oral administration,¹⁰ and Dai et al used Eudragit nanoparticles as a carrier to enhance the oral bioavailability of cyclosporine.¹¹

PLGA is a biocompatible and biodegradable copolymer. It contains carboxyl groups that impart a negative charge to the polymer. PLGA is approved by the US Food and Drug Administration as a biomedical material.^{12,13} An emulsification/solvent evaporation method is generally used to prepare PLGA microparticles and nanoparticles, which are used widely to control drug delivery.⁸

Nanoparticles are colloidal carriers with a size range of 10–200 nm and have the potential for uptake in inflamed tissues.¹⁴ It has been reported that the particle size and surface charge on polystyrene nanoparticles play a vital role in efficient uptake of these nanoparticles in stomach tissue.¹⁵ In a previous study, we combined the nanoparticle dosage form with an enteric-coating technique to protect LPZ from degradation in the stomach, and achieved a reliable gastric ulcer healing response in an animal model of induced ulcers.

In this study, we aimed to develop a non-enteric-coated nanoparticulate delivery system for acid-labile LPZ. Up until now, no non-enteric-coated nanoparticulate dosage form containing LPZ has been available. Such a formulation would be expected to provide reliable long-term acid suppression when administered orally once daily. LPZ-loaded positively charged Eudragit RS100 nanoparticles (ERSNPs-LPZ) and negatively charged PLGA nanoparticles (PLGANPs-LPZ) were prepared using a solvent evaporation method. The effect of charge on deposition of the nanoparticles in ulcerated and non-ulcerated regions of the stomach was investigated using fluorescent nanoparticles, and cellular uptake of the nanoparticles in the intestine was further evaluated in a monolayer

of Caco-2 cells. Finally, the pharmacokinetic performance and ulcer healing response were demonstrated in Wistar rats with induced ulcers after oral administration of ERSNPs-LPZ and PLGANPs.

Materials and methods

Materials

LPZ was obtained from Alcon Biosciences Private Ltd (Mumbai, India). Eudragit RS100 (Degussa, Darmstadt, Germany) and PLGA (molecular weight 28,000 Da, copolymer ratio 50:50, Boehringer Ingelheim, Ingelheim, Germany) were also used. Coumarin-6 (Sigma-Aldrich, St Louis, MO, USA) was used as a fluorescence marker. A human colon adenocarcinoma (Caco-2) cell line was a gift from Li-Juan Shen (Graduate Institute of Pharmaceutical Sciences, National Taiwan University, Taipei, Taiwan) and originated from the American Type Culture Collection (Manassas, VA, USA). Dulbecco Modified Eagle's Medium (with 4.5 g/L D-glucose and L-glutamine, without sodium pyruvate and sodium bicarbonate), non-essential amino acids, and mycoserum-tested fetal bovine serum were purchased from Biological Industries (Beit-Haemek, Israel). Hank's balanced salt solution buffer (HBSS) and propidium iodide were purchased from Invitrogen Corporation (Carlsbad, CA, USA).

Preparation of LPZ-loaded Eudragit nanoparticles

The ERSNPs-LPZ were prepared by an oil-in-water (o/w) emulsion solvent evaporation/extraction method. Eudragit RS100 (200 mg) and LPZ (200 mg) were dissolved in 10 mL of a dichloromethane/methanol mixture (5/5, v/v). The organic phase was added to 100 mL of aqueous poly(vinyl alcohol) solution (0.25% w/v, pH 9.0) under sonication at 4°C for 20 minutes. The organic solvent was evaporated by magnetic stirring at room temperature for 3 hours followed by a rotavapor under reduced pressure at 35°C for 5 minutes. The nanoparticles were recovered after centrifugation at 17,000 rpm for 30 minutes (Avanti J26 XP centrifuge, Beckman Coulter, Miami, USA). The collected nanoparticles were washed with deionized water three times and resuspended in 1 mL of deionized water containing 5% w/v sucrose, and then freeze-dried.

Preparation of LPZ-loaded PLGA nanoparticles

PLGANPs-LPZ were prepared using a water-in-oil-in-water (w/o/w) emulsion method. PLGA (200 mg) and LPZ (100 mg) were dissolved in 10 mL of a dichloromethane/acetone

mixture (5/5 v/v). An aqueous solution of NaHCO_3 (1 mL, 0.2%) was added to PLGA solution and emulsified to obtain a primary water-in-oil emulsion using an ultrasonic probe at 4°C for 2 minutes. The primary emulsion was then added to 100 mL of aqueous poly(vinyl alcohol) solution (0.25% w/v, pH 9.0) and followed the same procedures as for preparation of ERSNPs-LPZ.

Characterization of nanoparticles

The particle size and zeta potential of the nanoparticles were determined by a Zetasizer (Nano ZS, Malvern Co Ltd, Malvern, UK). The morphology of the nanoparticles was examined using an H7100 transmission electron microscope (Hitachi High-technologies Corporation, Tokyo, Japan) where the freeze-dried nanoparticles were dispersed in deionized water and stained with 2% phosphotungstic acid for 30 seconds, then placed on copper grids for observation. For determination of LPZ content, about 5 mg each of ERSNPs-LPZ and PLGANPs-LPZ were dissolved in 5 mL of methanol and acetonitrile, respectively. Each sample was centrifuged at 14,000 rpm for 10 minutes, and 20 μL of the supernatant was injected into a high-performance liquid chromatography (HPLC) system (Jasco International Company Ltd, Tokyo, Japan). The HPLC system consisted of a pump (PU-2089) and an MD-2010 photo diode array detector at 285 nm. A reversed phase silica column (C-18, 4.6×250 mm, $5 \mu\text{m}$, Phenomenex Inc, Torrance, CA, USA) was used. The mobile phase comprised water, acetonitrile, and triethylamine in a volume ratio of 50:50:0.1 (pH 7) at a flow rate of 1 mL per minute. The HPLC analytical method was validated prior to sample analysis. Drug loading (DL) and encapsulation efficiency (EE) were calculated using equations (1) and (2).

$$\text{DL (\%)} = \frac{\text{Determined amount of drug in nanoparticles}}{\text{Total amount of nanoparticles}} \times 100\% \quad (1)$$

$$\text{EE (\%)} = \frac{\text{Determined amount of drug in nanoparticles}}{\text{Total amount of drug used for nanoparticles preparation}} \times 100\% \quad (2)$$

In vitro drug release

LPZ-loaded nanoparticles were suspended in 5 mL of phosphate-buffered solution (pH 7.4) which was placed in a dialysis bag (molecular weight cutoff 6,000–8,000 Da) followed by immersion in 100 mL of the same release medium at $37^\circ\text{C} \pm 0.5^\circ\text{C}$ in a shaker bath at 75 rpm. Samples

(1 mL) were collected at time intervals of 0.5, 1, 2, 4, 6, 8, 12, and 24 hours, and the same volume of fresh release medium was replaced. The amount of LPZ in each release sample was analyzed by the HPLC method. Release of LPZ from the nanoparticles was analyzed by equation (3) based on the Korsmeyer–Peppas model.¹⁶

$$M_t/M_\infty = kt^n \quad (3)$$

where M_t/M_∞ is the percentage of drug released, k is the release rate constant, n is the release exponent, and t is the release time. The n value of the Korsmeyer–Peppas equation was used to indicate the release mechanism.¹⁷ In addition, the similarity factor (f_2) was calculated to compare the release profiles of ERSNPs-LPZ and PLGANPs-LPZ.¹⁸

$$f_2 = 50 \times \log \left\{ \left[1 + \left(\frac{1}{n} \right) \sum_{i=1}^n (R_i - T_i)^2 \right]^{-0.5} \times 100 \right\} \quad (4)$$

where n is the number of time points, R_i and T_i are the mean percent of drug released from the reference and test dissolution profiles, respectively, at each time point (t). Generally, an f_2 value in the range of 50–100 indicates similarity between two comparative release profiles.

Preparation of coumarin-6-loaded fluorescence nanoparticles

Coumarin-6-loaded Eudragit RS100 (ERSNPs-C6) and PLGA (PLGANPs-C6) fluorescence nanoparticles were prepared by an o/w solvent evaporation method. Eudragit RS100 or PLGA (200 mg) and coumarin-6 (1 mg) were dissolved in 10 mL of dichloromethane/acetone mixture (5/5 v/v). The preparation procedures that followed were the same as those described for preparation of the LPZ nanoparticles. The amounts of coumarin-6 entrapped in ERSNPs-C6 and PLGANPs-C6 were determined using a fluorescence spectrophotometer (F4500, Hitachi Ltd, Tokyo, Japan). The nanoparticles were dissolved in acetone for measurement of fluorescence at an excitation wavelength of 430 nm and an emission wavelength of 490 nm. Leaching of coumarin-6 from the nanoparticles was also evaluated. ERSNPs-C6 and PLGANPs-C6 (10 mg) were dispersed in 1 mL of HBSS (pH 7.4) and then placed in the dialysis bag (molecular weight cutoff 6,000–8,000 Da) which was immersed in 10 mL of HBSS at $37^\circ\text{C} \pm 0.5^\circ\text{C}$ in a mechanical shaker at 50 rpm for 24 hours. The sample was collected and diluted with acetone followed by fluorescence measurement.

Biodistribution of nanoparticles in stomach tissue

Male Wistar rats (250–300 g) were used in this study, and were obtained from the National Laboratory Animal Center (Taipei, Taiwan). All animal experiments were carried out in accordance with the Guide for the Care and Use of Laboratory Animals published by the National Institutes of Health, and all procedures were examined by the ethics committee on animal experimentation at National Taiwan University (Taipei, Taiwan). The rats were fasted but allowed free access to water overnight. Gastric ulceration was induced by oral administration of absolute ethanol (5 mL/kg).¹⁹ The ulcer-induced rats were divided into three groups (one control group and two treatment groups), and each group included four rats. Each treatment group received a hard gelatin capsule (#9, Torpac Inc, Fairfield, NJ, USA) filled with ERSNPs-C6 or PLGANPs-C6, and the control group received saline solution only. The formulations were administered orally 1 hour after administration of ethanol. The rats were sacrificed 4 hours after dose administration. The stomach was opened longitudinally and rinsed with saline solution. The ulcerated and non-ulcerated regions of stomach tissue were cut and the freshly excised tissues were cryofixed using Tissue-Tek®. The molded tissue sample was sectioned using a CM3050 S Cryostat (Leica Microsystems, Wetzlar, Germany) and observed under a fluorescence microscope combined with a digitally integrated photomicrography system (AxioPhot 2, Carl Zeiss, Hamburg, Germany). In addition, the sectioned stomach tissues were stained with hematoxylin and eosin to illustrate the morphology of the healthy and ulcerated tissues. For quantitative determination, the total mucosal area and the ulcerated area were measured using Axio Vision software (version 4.8, Carl Zeiss International, New York, NY, USA). The ulcerated and non-ulcerated tissues were lyophilized separately in the dark. Acetone was added to each tissue sample followed by sonication for 15 minutes. The tissue samples were centrifuged at 2,000 rpm for 5 minutes and the supernatant was collected. The extraction procedure was repeated three times. Finally, the supernatant was diluted with acetone and analyzed using a fluorescence spectrophotometer (F4500, Hitachi Ltd) at an excitation wavelength of 430 nm and an emission wavelength of 490 nm. Uptake of the nanoparticles by stomach tissues was expressed as a percentage of nanoparticle uptake per cm² of ulcerated or non-ulcerated stomach tissue.

Uptake of nanoparticles by Caco-2 cells

The Caco-2 cell monolayer was washed with HBSS (pH 7.4) twice followed by preincubation with HBSS at

37°C for 30 minutes. The HBSS (control), free coumarin-6 solution, ERSNPs-C6, and PLGANPs-C6 suspension in HBSS equivalent to 200 ng/mL of coumarin-6 were added in the apical side while 3 mL of HBSS was added in the basolateral side. The Caco-2 cell monolayer was incubated for 0.5 hours and 1 hour at 37°C in an atmosphere of 5% CO₂ and 90% relative humidity. The cell monolayer was then washed with phosphate-buffered saline (PBS, pH 7.4) followed by trypsinization for 5 minutes (0.25% trypsin ethylenediaminetetraacetic acid). Cold PBS was added and the cells were centrifuged at 1,000 rpm for 5 minutes, resuspended in 2 mL of PBS, and analyzed using a fluorescence activated flow cytometer (FACSCalibur, BD Biosciences, Franklin Lakes, NJ, USA). For confocal microscopic observation, the cell monolayer was incubated at 37°C for 0.5 hours, washed with PBS, and then fixed with 3.7% paraformaldehyde solution in PBS for 30 minutes. The cells were washed again, then treated with RNase solution for 30 minutes. The nuclei were then stained with propidium iodide for 30 minutes. The cell monolayer was then mounted on a glass slide with Fluoromount™ medium (Sigma-Aldrich). The images were captured using a confocal laser scanning microscopy imaging system (TCS SP5, Leica).

Pharmacokinetic study

The Wistar rats (250–300 g) with induced ulcers were divided into three groups, with each group including four rats. The LPZ-NaHCO₃ solution (5 mg LPZ/kg) and the hard gelatin capsules (#9, Torpac Inc) filled with sodium bicarbonate (20 mg/kg) and either ERSNPs-LPZ or PLGANPs-LPZ (5 mg LPZ/kg) were orally administered to the Wistar rats. The LPZ solution (1 mg/mL) was prepared by dissolving LPZ in a mixture of PEG 400 and 1% NaHCO₃ (2:3 v/v).²⁰ Blood samples were collected from the tail vein of each rat prior to drug administration and at time intervals of 0.5, 1, 1.5, 2, 3, 4, 5, 6, 8, 10, 12, and 24 hours after dosing. The blood samples were centrifuged at 12,000 rpm for 10 minutes at 4°C and the supernatant was collected. The LPZ in each sample was extracted using acetonitrile followed by centrifugation. The supernatant was collected, air-dried, and reconstituted with mobile phase for HPLC analysis. The recovery of LPZ from serum samples was in the range of 98.60%–101.78%. The pharmacokinetic parameters were obtained based on a non-compartmental pharmacokinetic analysis model (WinNonlin software, version 5.3, Pharsight Corporation, Mountain View, CA, USA). The statistical analysis was performed using the Student's *t*-test, and a *P*-value of *P*<0.05 was considered to be statistically significant.

Pharmacodynamic study

The Wistar rats with induced ulcers were divided into four groups (n=4 each) to receive saline solution (control group), LPZ solution, or a capsule filled with ERSNPs-LPZ or PLGANPs-LPZ. The formulations were orally administered once daily for 7 days. The rats were euthanized 24 hours after the last dose. The stomach was cut along the greater curvature, and the mucosal surface of the stomach was washed with saline solution. Photographic images (Nikon E5000, Nikon Corporation, Tokyo, Japan) of the mucosal surface of the stomach were obtained, and the total mucosal area and the ulcerated area were measured using Axio Vision software (version 4.8, Carl Zeiss International). The ulcer index (UI) was calculated using equation (5).²¹

$$\text{Ulcer index (UI)} = \frac{\text{The ulcerated area}}{\text{Total mucosal area}} \times 100 \quad (5)$$

Results and discussion

Characterization of ERSNPs-LPZ and PLGANPs-LPZ

Figure 1A and 1B show a transmission electron micrograph of the ERSNPs-LPZ and PLGANPs-LPZ, indicating that these nanoparticles have a spherical shape and smooth surface. The mean particle size of ERSNPs-LPZ was 203.9 ± 4.9 nm and the polydispersity index was 0.09 ± 0.04 , indicating a narrow size distribution (Figure 1C). The EE and DL were $79.3\% \pm 1.0\%$ and $43.7\% \pm 0.5\%$, respectively. The ERSNPs-LPZ showed a zeta potential of $+38.5 \pm 0.3$ mV due to the quaternary ammonium groups of Eudragit RS100. The mean particle size of PLGANPs-LPZ was 219.2 ± 2.9 nm and the polydispersity index was 0.13 ± 0.07 (Figure 1D). The carboxyl end groups of the PLGA copolymer form an acidic microenvironment which may affect the stability of LPZ, so sodium bicarbonate was added as an alkaline stabilizer during preparation of PLGANPs-LPZ in order to maintain the stability of LPZ in

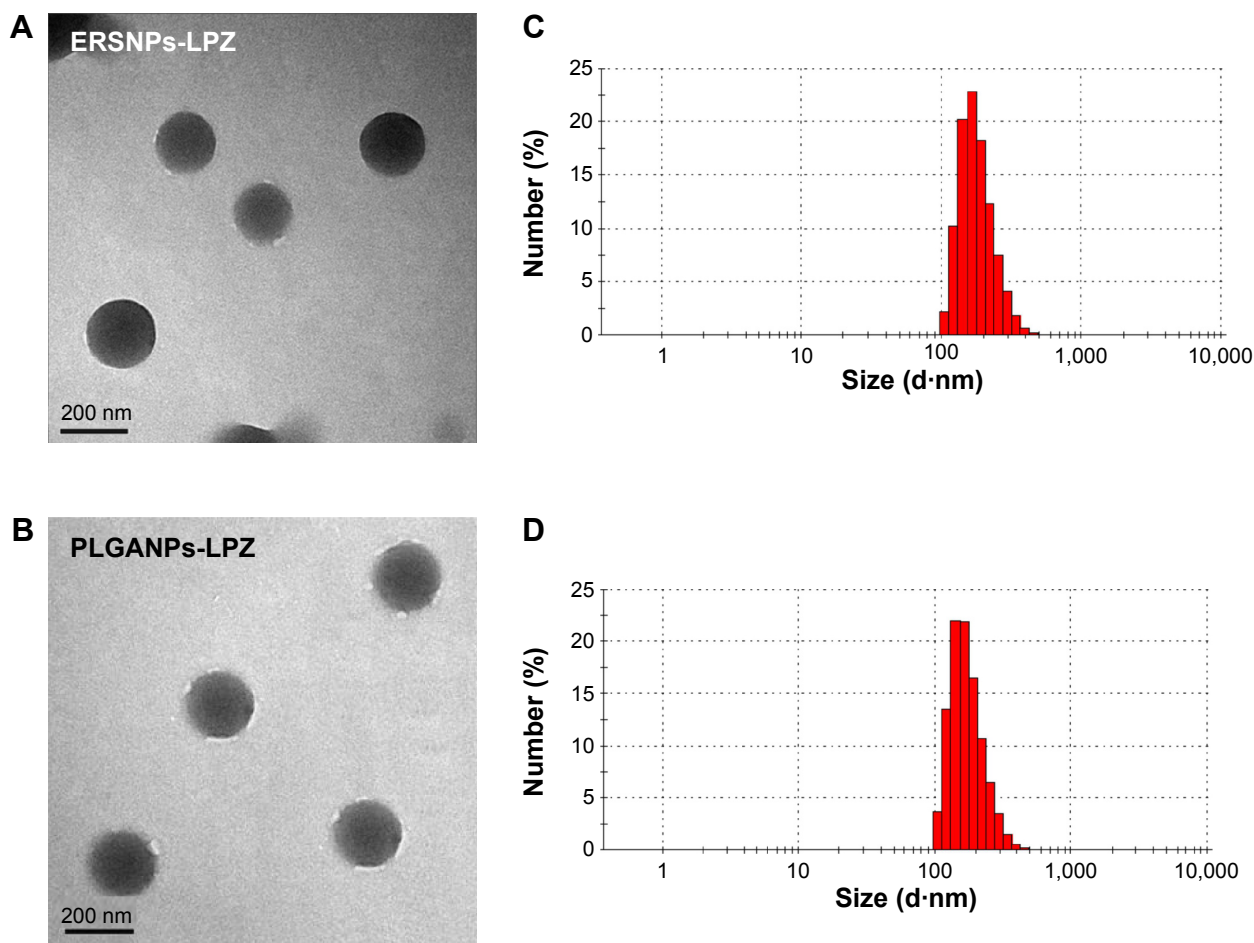


Figure 1 Transmission electron micrographs (50,000 \times) and particle size distribution of ERSNPs-LPZ (A, C) and PLGANPs-LPZ (B, D).

Abbreviations: LPZ, lansoprazole; ERSNPs-LPZ, LPZ-loaded Eudragit[®] RS100 nanoparticles; PLGANPs-LPZ, LPZ-loaded poly(lactic-co-glycolic acid) nanoparticles.

the PLGA nanoparticles.²² The EE and DL of PLGANPs-LPZ were $79.6\% \pm 2.2\%$ and $28.7\% \pm 1.2\%$, respectively. PLGANPs-LPZ showed a zeta potential of -27.3 ± 0.3 mV due to the carboxyl end groups of PLGA.

In vitro drug release

Figure 2 shows the in vitro release of LPZ from ERSNPs-LPZ and PLGANPs-LPZ in pH 7.4 release medium. ERSNPs-LPZ and PLGANPs-LPZ showed sustained-release behavior for up to 24 hours. The similarity factor, f_2 , was calculated to be 58, indicating no difference in drug release profile between ERSNPs-LPZ and PLGANPs-LPZ. Release of LPZ from the nanoparticles was analyzed using the Korsmeyer–Peppas model. The release rate constants (k) for ERSNPs-LPZ and PLGANPs-LPZ were $10.6\% \pm 0.4\% \text{ h}^{-n}$ ($R^2=0.9305 \pm 0.015$) and $11.0\% \pm 1.2\% \text{ h}^{-n}$ ($R^2=0.9609 \pm 0.008$), respectively, and the corresponding release exponent values (n) were 0.77 ± 0.01 and 0.69 ± 0.02 , implying that the release of LPZ from both types of nanoparticles was dominated by non-Fickian diffusion. Eudragit RS100 is a water-insoluble but swellable polymer that behaves as a rate-limiting matrix to control drug release from ERSNPs-LPZ via a non-Fickian diffusion mechanism.^{23,24} The same release mechanism has been demonstrated for ERSNPs loaded with gatifloxacin or amphotericin B.^{25,26} PLGA is a water-insoluble and biodegradable polymer. Release of LPZ from PLGANPs-LPZ was dominated by polymer degradation and drug diffusion in terms of an n value in the range of 0.5–1.0. The same release mechanism has been demonstrated for bupivacaine-loaded PLGA nanoparticles.²⁷

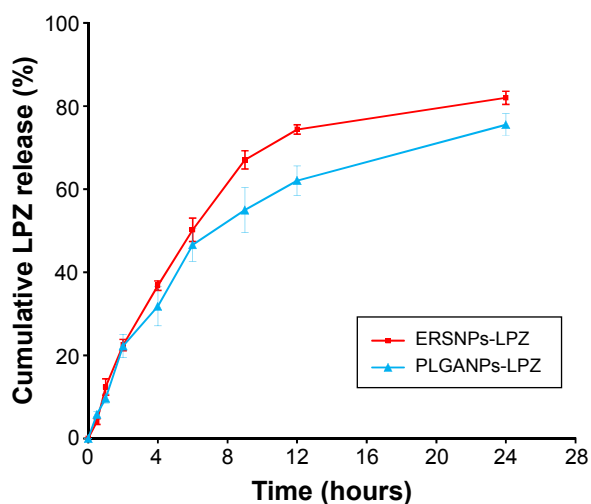


Figure 2 Release of LPZ from (■) ERSNPs-LPZ and (▲) PLGANPs-LPZ in pH 7.4 phosphate-buffered solution ($n=3$).

Abbreviations: LPZ, lansoprazole; ERSNPs-LPZ, LPZ-loaded Eudragit® RS100 nanoparticles; PLGANPs-LPZ, LPZ-loaded poly(lactic-co-glycolic acid) nanoparticles.

Characterization of coumarin-6-loaded fluorescence nanoparticles

Coumarin-6 is widely used as a fluorescence marker for confocal microscopic investigation due to its high fluorescence sensitivity. It has been reported that about 0.05% w/w dye loading is sufficient to produce bright fluorescence nanoparticles for visualization.²⁸ Coumarin-6-loaded fluorescence nanoparticles were prepared to demonstrate the biodistribution and cellular uptake of nanoparticles in the gastrointestinal tract. The mean particle size of ERSNPs-C6 and PLGANPs-C6 was 188.9 ± 8.7 nm and 193.4 ± 2.9 nm, respectively, and the zeta potential was $+39.4 \pm 0.6$ mV and -24.5 ± 0.7 mV. The dye loadings of ERSNPs-C6 and PLGANPs-C6 were $0.35\% \pm 0.03\%$ and $0.088\% \pm 0.003\%$, respectively. Use of a fluorescence marker for visualization of nanoparticles may lead to misinterpretation of results in the event of leaching or release of fluorescence marker into the release medium and subsequently into the cells.²⁹ Less than 0.05% of the coumarin-6 was released from our ERSNPs-C6 and PLGANPs-C6 in the release medium within 24 hours, which was considered negligible. It was thus reasonable to assume that the coumarin-6 was stably retained in the nanoparticles ready for biodistribution and cellular uptake studies.

Biodistribution of fluorescence nanoparticles

Figure 3A illustrates the fluorescence microscopic images of ulcerated and non-ulcerated regions of the stomach after 4 hours of oral administration of ERSNPs-C6 and PLGANPs-C6 in Wistar rats with induced ulcers. Figure 3Ai and 3Aii show the pathology of the ulcerated and non-ulcerated regions of stomach tissue stained with hematoxylin and eosin before treatment with the nanoparticles. The nanoparticles were localized in both ulcerated (Figure 3Aiii and 3Av) and non-ulcerated (Figure 3Aiv and 3Avi) regions after oral administration of the nanoparticles, and the corresponding values are shown in Figure 3B. The PLGANPs-C6 ($7.22\% \pm 1.21\%$ per cm^2) was deposited in the ulcerated region more than ERSNPs-C6 ($4.28\% \pm 0.39\%$ per cm^2). In contrast, ERSNPs-C6 ($8.29\% \pm 0.35\%$ per cm^2) was distributed more than PLGANPs-C6 ($5.77\% \pm 0.66\%$ per cm^2) in the non-ulcerated region. These results indicate that the negatively charged PLGANPs-C6 adhered more readily to the ulcerated region, whereas the positively charged ERSNPs-C6 preferred localization in the non-ulcerated region of the stomach.

Different biodistribution of ERSNPs-C6 and PLGANPs-C6 in ulcerated and non-ulcerated regions of the stomach was observed. It has been reported that ulcerated tissue contains

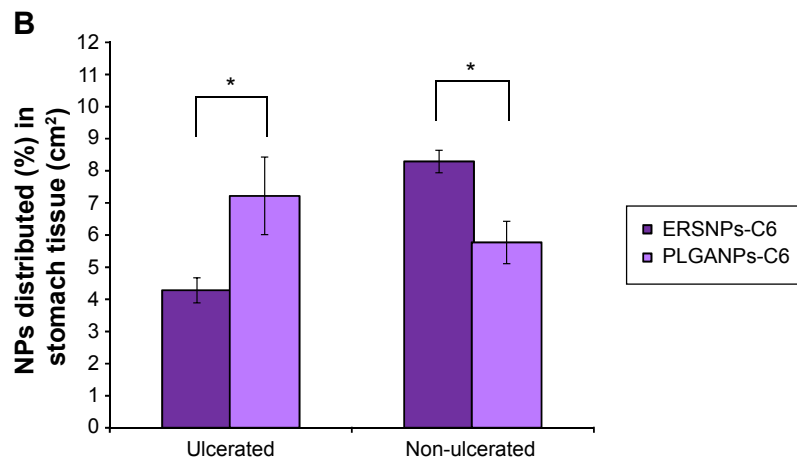
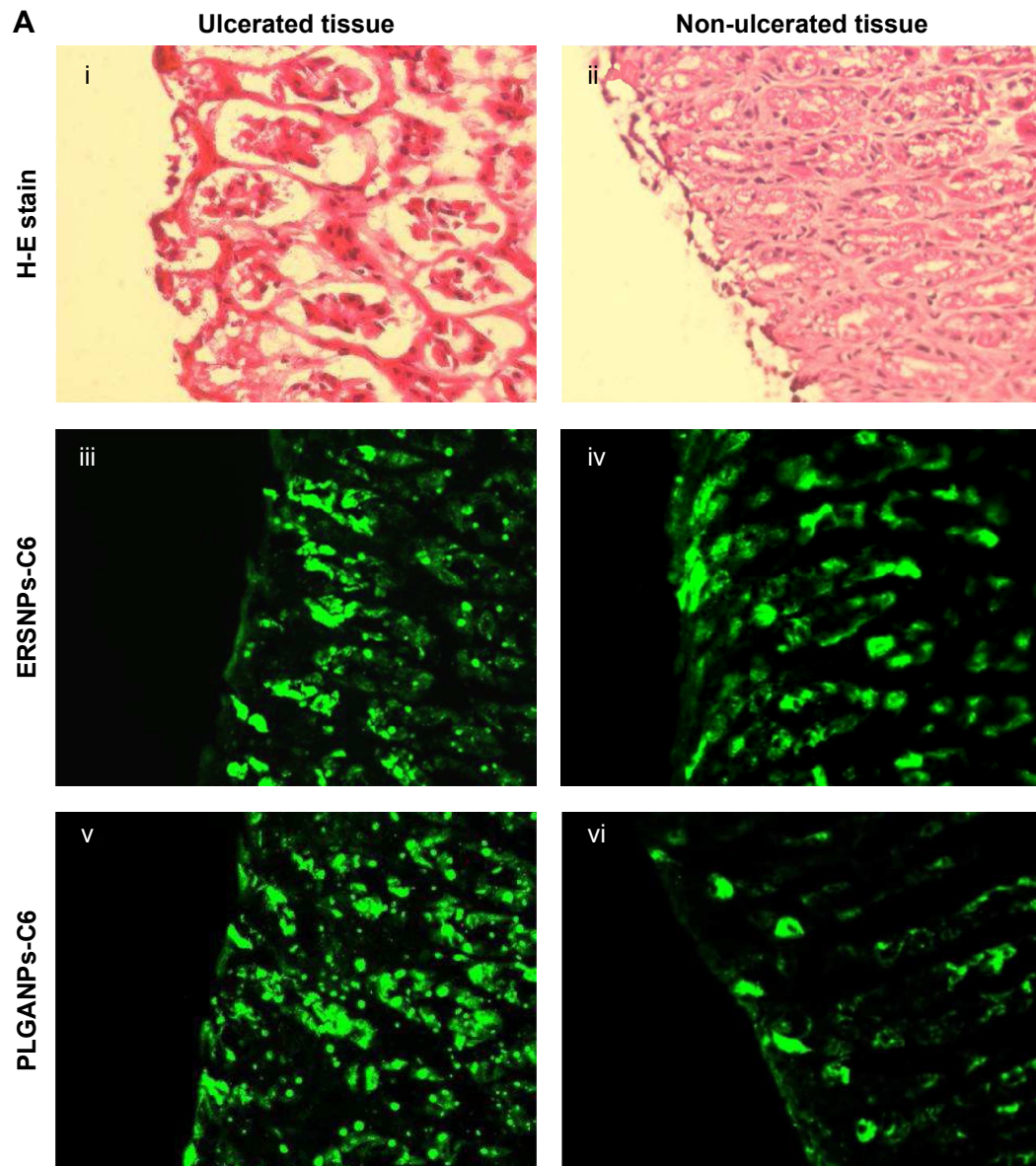


Figure 3 Fluorescence microscopic images and biodistribution of nanoparticles.

Notes: Fluorescence microscopic images (40x) (A) and biodistribution of nanoparticles (B) in ulcerated (i, iii, and v) and non-ulcerated (ii, iv, and vi) stomach tissue in Wistar rats with induced ulcers, after oral administration of ERSNPs-C6 and PLGANPs-C6 for 4 hours (n=4). *P<0.001.

Abbreviations: ERSNPs-C6, coumarin-6-loaded Eudragit RS100 nanoparticles; H-E, hematoxylin and eosin; NP, nanoparticle; PLGANPs-C6, coumarin-6-loaded poly(lactic-co-glycolic acid) nanoparticles.

high concentrations of positively charged proteins which have a high affinity for negatively charged PLGANPs-C6 in terms of bioadhesion of these nanoparticles in the ulcerated region.¹⁵ In contrast, positively charged ERSNPs-C6 had a high affinity for the negatively charged cell membrane, resulting in bioadhesion in the non-ulcerated region. A similar result has been observed in negatively charged polystyrene nanoparticles which were taken up in the ulcerated region of stomach tissue more than in healthy stomach tissue.¹⁵

Cellular uptake of fluorescence nanoparticles

The uptake of coumarin-6-loaded ERSNPs-C6 and PLGANPs-C6 in the Caco-2 cell monolayer was monitored

by flow cytometry, and the result is shown in Figure 4A. The cellular uptake of free coumarin-6 ($1.27\% \pm 0.3\%$) was comparable with that in the control group ($1.00\% \pm 0.03\%$). It has been suggested that it is not feasible for coumarin-6 to internalize into Caco-2 cells.³⁰ However, a significant increase of fluorescence intensity in Caco-2 cells was observed when these cells were incubated with ERSNPs-C6 ($78.4\% \pm 0.8\%$) and PLGANPs-C6 ($45.3\% \pm 4.6\%$). The positively charged ERSNPs-C6 enhanced cellular uptake more prominently than negatively charged PLGANPs-C6 ($P < 0.05$). The strong affinity of positively charged nanoparticles for negatively charged cell membranes accounted for this result. Figure 4B shows the confocal microscopic images of the Caco-2 cell monolayer after incubation with

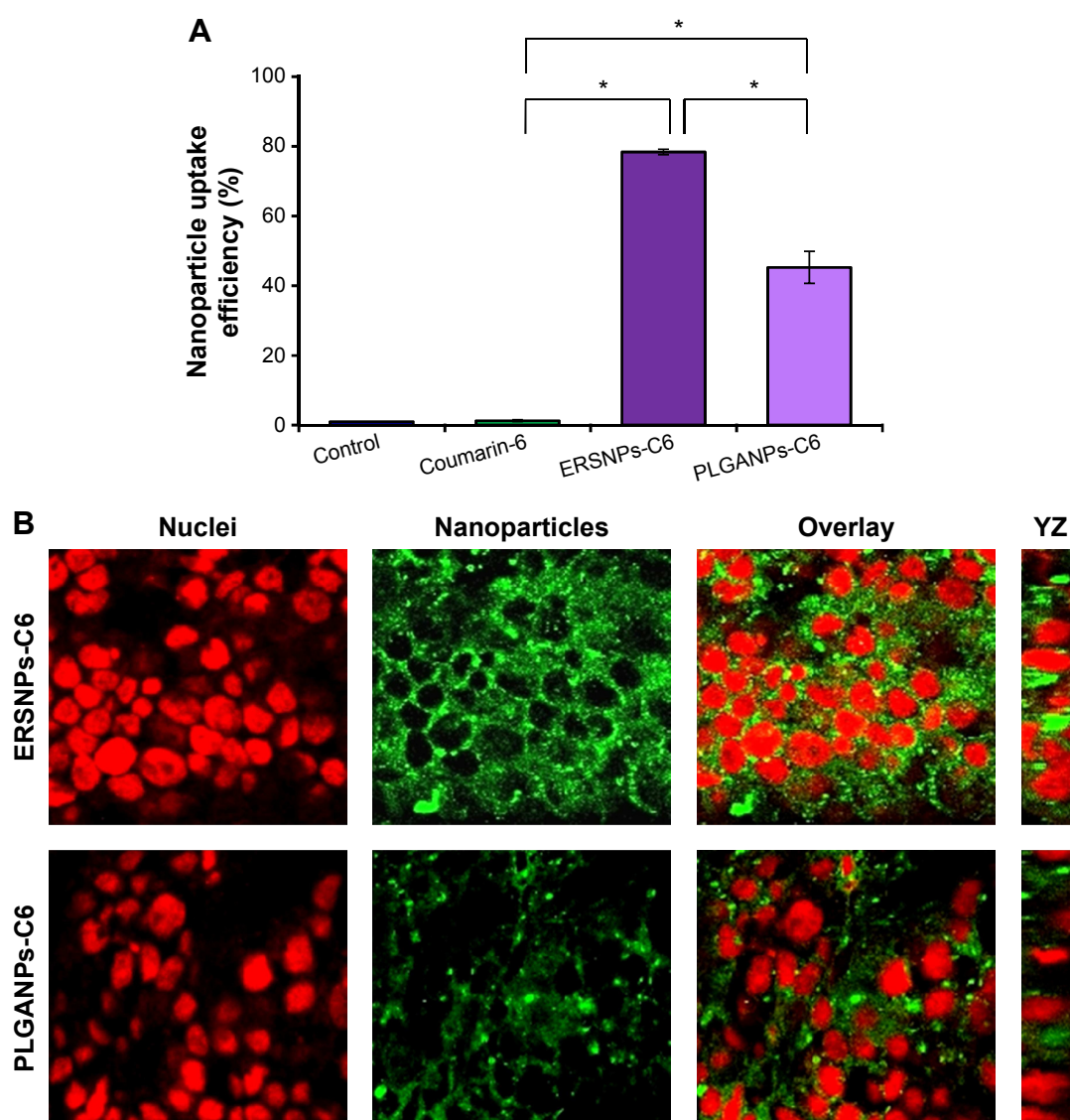


Figure 4 Cellular uptake efficiency (%) and confocal microscopic images of Caco-2 cells.

Notes: Cellular uptake efficiency (%), (n=3) (**A**) and confocal microscopic images (**B**) of Caco-2 cells after incubation with ERSNPs-C6 and PLGANPs-C6 fluorescence nanoparticles at 37°C for 0.5 hours. * $P < 0.001$. Green denotes nanoparticles and red denotes nuclei.

Abbreviations: ERSNPs-C6, coumarin-6-loaded Eudragit RS100 nanoparticles; PLGANPs-C6, coumarin-6-loaded poly(lactic-co-glycolic acid) nanoparticles.

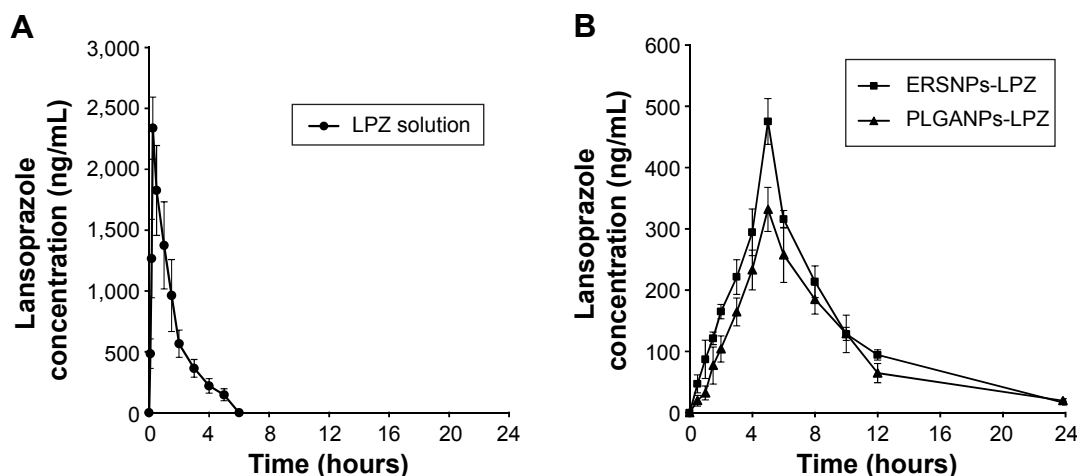


Figure 5 LPZ concentration versus time profiles in Wistar rats with induced ulcers, after oral administration of (A) LPZ solution (●), (B) ERSNPs-LPZ (■), and PLGANPs-LPZ (▲) (LPZ 5 mg/kg), respectively (n=4).

Abbreviations: LPZ, lansoprazole; ERSNPs-LPZ, LPZ-loaded Eudragit® RS100 nanoparticles; PLGANPs-LPZ, LPZ-loaded poly(lactic-co-glycolic acid) nanoparticles.

ERSNPs-C6 and PLGANPs-C6 for 0.5 hours. The strong green fluorescence in the cytoplasm indicated localization of nanoparticles in the cells. A similar charge effect has been reported by He et al whereby positively charged chitosan nanoparticles showed higher phagocytic uptake in LO2 and SMMC-7721 cells than negatively charged carboxymethyl-grafted chitosan nanoparticles.⁵ The uptake of nanoparticles into Caco-2 cells was further confirmed by three-dimensional analysis, where the fluorescence signal clearly appeared in the YZ plane, as shown in Figure 4B. All of these results confirm that both ERSNPs and PLGANPs were able to internalize into Caco-2 cells in a charge-dependent manner. This finding explored the possibility of nanoparticles being absorbed in the intestinal tract.

Pharmacokinetic study

Figure 5 shows the LPZ concentration versus time profiles after oral administration of ERSNPs-LPZ, PLGANPs-LPZ, and LPZ solution in Wistar rats with induced ulcers. The pharmacokinetic parameters are listed in Table 1. All LPZ was eliminated within 6 hours after oral administration of LPZ solution, while the nanoparticle formulations showed sustained and prolonged LPZ concentrations up to 24 hours. The elimination half-life and mean residence time for ERSNPs-LPZ (4.60 ± 0.45 hours and 8.19 ± 0.28 hours, respectively) and PLGANPs-LPZ (4.71 ± 0.41 hours and 9.07 ± 0.83 hours) were significantly longer than those for LPZ solution (1.36 ± 0.24 hours and 1.94 ± 0.44 hours; $P < 0.05$). Meanwhile, both types of nanoparticles markedly

Table 1 Pharmacokinetic parameters of LPZ after oral administrations of ERSNPs-LPZ, PLGANPs-LPZ and LPZ solution in Wistar rats with induced ulcers, at an LPZ dose of 5 mg/kg (n=4)

PK parameters	ERSNPs-LPZ	PLGANPs-LPZ	LPZ solution
AUC ₀₋₂₄ (ng [*] h/mL)	3,151.8±107.7 ^b	2,449.8±270.1 ^a	3,472.6±644.6
AUC _{0-∞} (ng [*] h/mL)	3,253.6±129.4 ^b	2,579.7±254.9 ^a	3,772.4±537.2
C _{max} (ng/mL)	475.3±37.5 ^{a,b}	331.7±36.0 ^a	2,338.3±255.3
T _{max} (hours)	5.0±0.0 ^a	5.0±0.0 ^a	0.25±0.00
k (per hour)	0.15±0.02 ^a	0.15±0.01 ^a	0.52±0.08
k _a (per hour)	0.13±0.01 ^a	0.12±0.01 ^a	0.76±0.19
T _{1/2} (hours)	4.60±0.45 ^a	4.71±0.41 ^a	1.36±0.24
V _d /F (mL/kg)	10,180.5±796.1 ^{a,b}	13,326.6±2,264.2 ^a	2,674.1±846.0
CL/F (mL/hour/kg)	1,538.6±62.8 ^b	1,951.9±185.6 ^a	1,346.7±199.5
MRT (hours)	8.19±0.28 ^{a,b}	9.07±0.44 ^a	1.94±0.44

Notes: ^aStatistical significance of LPZ nanoparticles and solution ($P < 0.05$); ^bstatistical significance between nanoparticles ($P < 0.05$). The data is presented as mean ± SD.

Abbreviations: AUC_{0-∞}, area under the serum concentration versus time curve from zero to infinity; C_{max}, maximum drug concentration; T_{max}, time to reach the C_{max}; k, elimination rate constant; k_a, absorption rate constant; T_{1/2}, elimination half-life; V_d/F, relative apparent volume of distribution; CL/F, relative clearance; MRT, mean residence time; PK, pharmacokinetic; LPZ, lansoprazole; ERSNPs-LPZ, LPZ-loaded Eudragit® RS100 nanoparticles; PLGANPs-LPZ, LPZ-loaded poly(lactic-co-glycolic acid) nanoparticles.

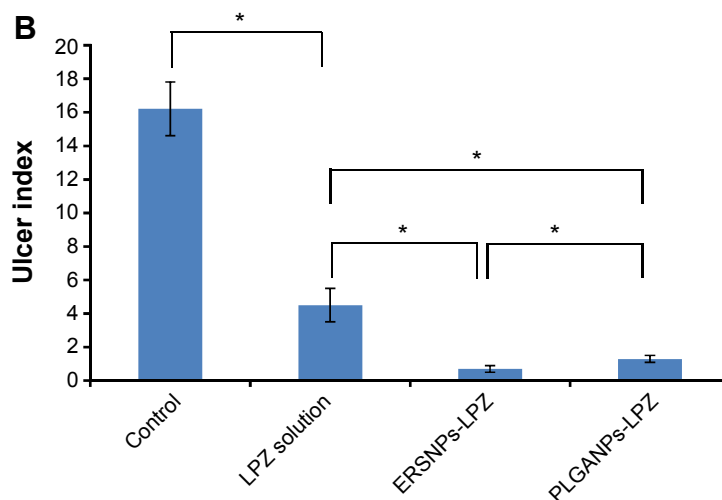
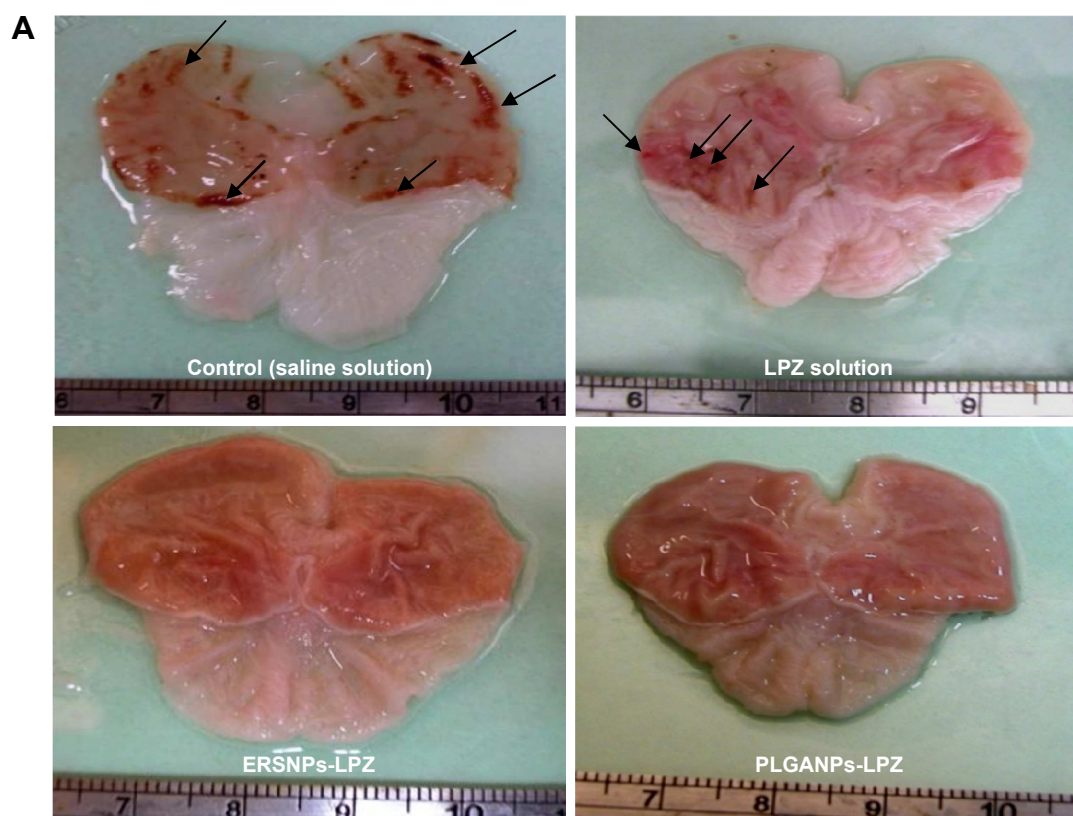


Figure 6 Photographs of stomach and ulcer index.

Notes: Photographs of stomach (A) and ulcer index (B) in Wistar rats with induced ulcers after oral administration of saline solution (control), LPZ solution, ERSNPs-LPZ, and PLGANPs-LPZ (LPZ 5 mg/kg/day) for 7 days (n=4). The arrows indicate the ulcerated region. * $P < 0.05$.

Abbreviations: LPZ, lansoprazole; ERSNPs-LPZ, LPZ-loaded Eudragit® RS100 nanoparticles; PLGANPs-LPZ, LPZ-loaded poly(lactic-co-glycolic acid) nanoparticles.

reduced the peak plasma concentration of LPZ (475.3 ± 37.5 ng/mL and 331.7 ± 36.0 ng/mL) as compared with LPZ solution ($2,338.3 \pm 255.3$ ng/mL; $P < 0.05$). Herein, ERSNPs-LPZ produced a comparable area under the curve from time zero to infinity ($AUC_{0-\infty}$) with LPZ solution. However, the $AUC_{0-\infty}$ of PLGANPs-LPZ was significantly lower than for LPZ solution and ERSNPs-LPZ ($P < 0.05$). There were

significant differences in $AUC_{0-\infty}$, peak plasma concentration, relative apparent volume of distribution (Vd/F), and relative clearance (CL/F) between the two types of nanoparticles ($P < 0.05$). Since the $AUC_{0-\infty}$ of ERSNPs-LPZ was higher than that of PLGANPs-LPZ, the higher relative bioavailability of ERSNPs-LPZ resulted in the Vd/F and CL/F being significantly lower than for PLGANPs-LPZ.

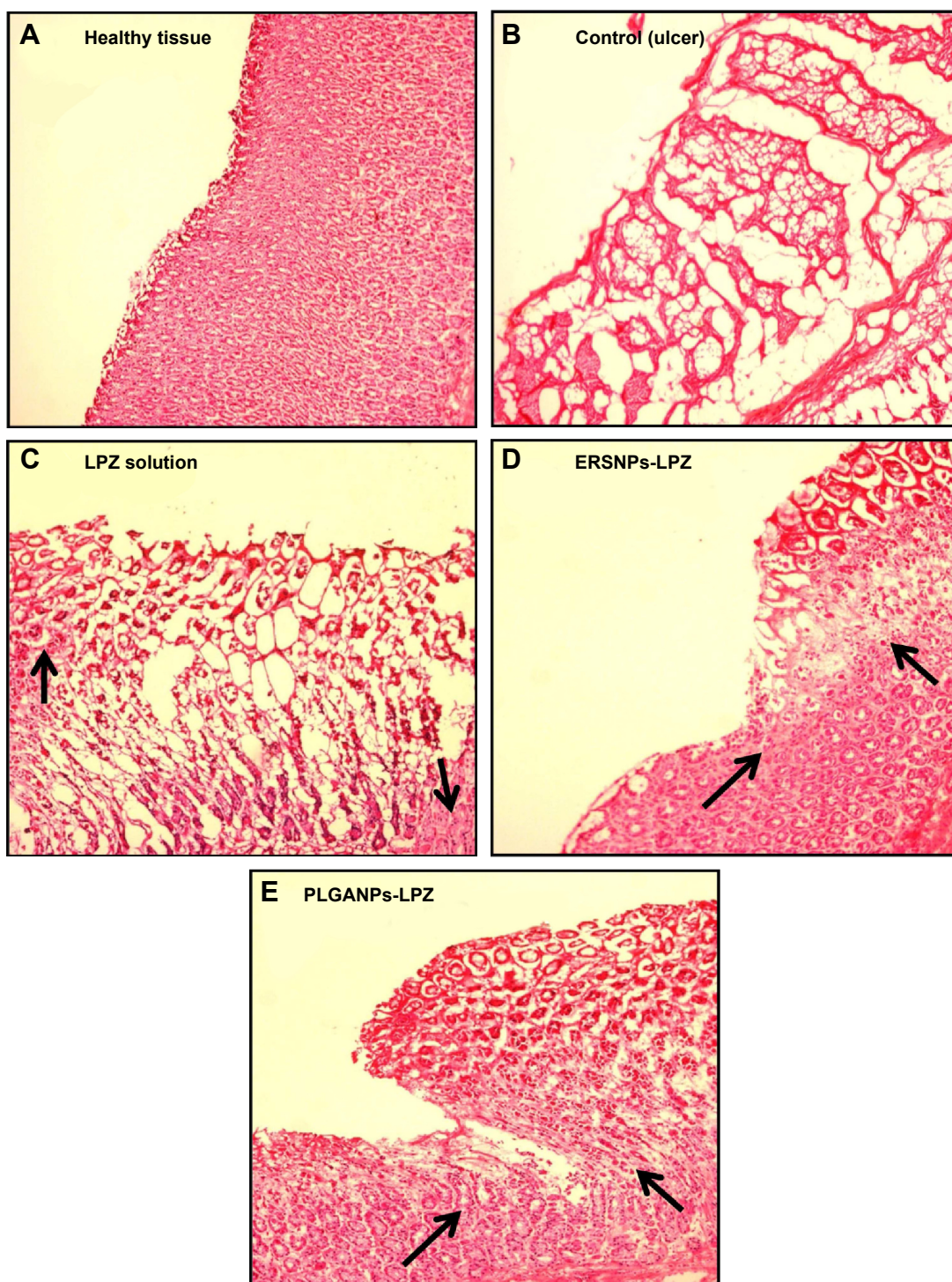


Figure 7 Histopathological images of healthy tissue and healing ulcer tissues.

Notes: Histopathological images of healthy tissue (A) and healing ulcer tissues after oral administration of saline solution (control) (B), LPZ solution (C), ERSNPs-LPZ (D), and PLGANPs-LPZ (E) (LPZ 5 mg/kg/day) for 7 days. The arrows indicate granulation tissue developed during the ulcer healing process (100 \times).

Abbreviations: LPZ, lansoprazole; ERSNPs-LPZ, LPZ-loaded Eudragit[®] RS100 nanoparticles; PLGANPs-LPZ, LPZ-loaded poly(lactic-co-glycolic acid) nanoparticles.

It was reported that oral administration of Levant[™] (an enteric-coated capsule containing LPZ 30 mg, Ranbaxy Ltd, London, UK) in healthy male subjects resulted in rapid LPZ absorption (mean peak plasma concentration 817 \pm 284 ng/mL; time taken to reach peak plasma

concentration 2.72 \pm 0.87 hours; mean residence time 4.00 \pm 0.79 hours).³¹ A similar result was obtained following oral administration of the capsule filled with enteric-coated LPZ pellets in healthy Chinese male volunteers (peak plasma concentration 1,047 \pm 344 ng/mL; time taken to reach peak

plasma concentration 2.0 ± 0.7 hours; mean residence time 3.62 ± 0.87 hours).³² Stefanič et al reported that oral absorption of dispersible tablets composed of enteric-coated LPZ pellets was completed in 6 hours in healthy subjects.³³ Our nanoparticles provided sustained release of LPZ for up to 24 hours with a long mean residence time as compared with LPZ solution in an ulcer-induced Wistar rat model. In contrast with conventional enteric-coated LPZ formulations, the current nanoparticles have the potential to provide effective acid suppression, especially late in the day and throughout the night. It has been reported that higher LPZ blood levels are usually associated with a higher incidence of diarrhea as a side effect.³⁴ The constant LPZ blood level delivered by these nanoparticles could also be of benefit in reducing such side effects.

Ulcer healing response

The ulcer healing efficacy of LPZ nanoparticles was further evaluated. Figure 6A shows photographic images of the stomach after oral administration of saline solution (control group), LPZ solution, ERSNPs-LPZ, and PLGANPs-LPZ, respectively, for 7 days in ulcer-induced Wistar rats. The corresponding gastric UI was 16.2 ± 1.6 , 4.5 ± 1.0 , 0.7 ± 0.2 , and 1.2 ± 0.2 (Figure 6B). This result shows that the gastric ulceration gradually healed within 1 week after oral administration of LPZ solution and LPZ nanoparticles. Oral administration of LPZ solution for 7 days healed 72.2% of gastric ulcers as compared with the control group, while oral administration of ERSNPs-LPZ and PLGANPs-LPZ for 7 days healed 95.7% and 92.6% of gastric ulcers, respectively. The better ulcer healing efficacy of LPZ nanoparticles when compared to LPZ solution could be due to sustained release properties and the prolonged in vivo absorption characteristics of the nanoparticles which continuously suppressed acid secretion. Figure 7 shows the histopathology of healing ulcer tissue after oral administration of the four formulations. In the control group, the mucosal surface of the gastric ulcer was damaged and dilated gastric glands were spread across a large region of the ulcer. After oral administration of LPZ solution, granulation tissue developed during the ulcer healing process. Granulation tissue is an important component of healing which supplies connective tissue and microvessels in the ulcer scar.³⁵ Oral administration of LPZ nanoparticles induced much more growth of granulation tissue than LPZ solution. All results confirmed the efficient ulcer healing effect of LPZ-loaded nanoparticles in an ulcer-induced animal model after 7 days of treatment. However, the possible absorption pathway(s) for oral administration of LPZ-loaded

nanoparticles was/were not elucidated in this study, and should be investigated further.

Conclusion

Eudragit RS100 and PLGA nanoparticles were designed for oral delivery of LPZ as gastric ulcer therapy. The prepared LPZ-loaded nanoparticles had opposite surface charge and the particle size was around 200 nm with a narrow size distribution. The nanoparticles adhered and deposited in the stomach tissue were charge-dependent. The negatively charged PLGANPs adhered more readily to the ulcerated region whereas the positively charged ERSNPs preferred distribution in the non-ulcerated region of the stomach. Furthermore, the nanoparticles were able to internalize and localize in Caco-2 cells, where the positively charged ERSNPs enhanced cellular uptake more prominently than negatively charged PLGANPs. The nanoparticles allowed sustained and prolonged release of LPZ for up to 24 hours. Oral administration of LPZ-loaded nanoparticles for 7 days healed 92.6%–95.7% of gastric ulcers. Our results indicate that the nanoparticles developed in this study have the potential to release LPZ in a sustained manner and heal gastric ulcer effectively following oral administration.

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Disclosure

The authors report no conflicts of interest in this work.

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