Ranolazine inhibits shear sensitivity of endogenous Na⁺ current and spontaneous action potentials in HL-1 cells

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 $Ta_v 1.5$ is a mechanosensitive voltage-gated Na⁺ channel encoded by the gene SCN5A, expressed in cardiac myocytes and required for phase 0 of the cardiac action potential (AP). In the cardiomyocyte, ranolazine inhibits depolarizing Na⁺ current and delayed rectifier (I_K) currents. Recently, ranolazine was also shown to be an inhibitor of Na, 1.5 mechanosensitivity. Stretch also accelerates the firing frequency of the SA node, and fluid shear stress increases the beating rate of cultured cardiomyocytes in vitro. However, no cultured cell platform exists currently for examination of spontaneous electrical activity in response to mechanical stimulation. In the present study, flow of solution over atrial myocyte-derived HL-1 cultured cells was used to study shear stress mechanosensitivity of Na⁺ current and spontaneous, endogenous rhythmic action potentials. In voltageclamped HL-1 cells, bath flow increased peak Na⁺ current by 14 ± 5%. In current-clamped cells, bath flow increased the frequency and decay rate of AP by $27 \pm 12\%$ and $18 \pm 4\%$, respectively. Ranolazine blocked both responses to shear stress. This study suggests that cultured HL-1 cells are a viable in vitro model for detailed study of the effects of mechanical stimulation on spontaneous cardiac action potentials. Inhibition of the frequency and decay rate of action potentials in HL-1 cells are potential mechanisms behind the antiarrhythmic effect of ranolazine.

Introduction

 $Na_v 1.5$ is a sodium-selective voltage-gated ion channel present in various mechanically active cells, such as cardiac myocytes, human intestinal smooth muscle cells, and interstitial cells of Cajal. Mutations in *SCN5A*, the gene encoding Na_v1.5, are known to cause cardiac arrhythmias such as long QT 3 (LQT3) and Brugada syndromes.¹ Na_v1.5 has a well-defined role in the cardiac action potential, and electrophysiologic pathologies that result from Na_v1.5 abnormalities have solid molecular and physiological foundations.^{1,2}

Ion channel mechanosensitivity has been well documented, but most studies focus on non-voltage gated ion channel mechanosensitivity. Not until recently has evidence emerged to suggest that mammalian voltage-gated ion channels such as Na_v1.5,^{3,4} shaker⁵ and the L-type Ca²⁺ channel are mechanosensitive.6-8 While the actin cytoskeleton contributes to Nav1.5 mechanosensitivity,9 the Nav1.5 a-subunit is mechanosensitive as a standalone unit.¹⁰ We have recently shown that ranolazine inhibits the excitatory component of Nav1.5 mechanosensitivity.11 However, the roles of voltage-gated ion channel mechanosensitivity in physiology and ranolazine-mediated inhibition of Na, 1.5 in the heart are unclear.

Mutations in *SCN5A* and dysfunction of Na_v1.5 are associated with clinical pathologies rooted in cardiac mechano-electrical feedback (MEF) dysfunction. For example, in both familial



Figure 1. Voltage dependent sodium current contributes to spontaneous, rhythmic action potentials in untransfected HL-1 cultured atrial myocytes. (**A**) Representative family of current traces from a voltage-clamped cell dialyzed with Cs⁺ rich solution and elicited by the voltage protocol shown (inset). (**B**) Current-voltage relationship of the traces shown in (**A**). (**C**) Spontaneous rhythmic action potentials recorded sequentially in current-clamp mode from a cell which produced Na⁺ current similar to (**A**). Extracellular solution contained the principal charge carrier Na⁺ (Control, t = set as 0 min, baseline = -32 mV), NMDG⁺ (NMDG⁺ substitution, t = 2 min, resting potential = 44 mV), then Na⁺ (Wash out, t = 40 min, resting potential = -31 mV).

and idiopathic-dilated cardiomyopathy, SCN5A mutations are the only α -subunit channelopathies described;¹² all other mutations implicated in idiopathicdilated cardiomyopathy lie in genes that code for structural proteins. Several of these structural proteins associate with or are important in Na, 1.5 mechanosensitivity, including telethonin,¹³ dystrophin¹⁴ and syntrophin.¹⁵ In addition to inhibiting the excitatory aspects of Na₂1.5 mechanosensitivity,¹¹ ranolazine has shown promise for the treatment of abnormalities leading to heart failure.¹⁶ These studies provide rationale and a potential mechanism for structural or mechanical abnormalities

in cardiac disease. Another potential example involves stretch of the pulmonary veins, which may serve to trigger and/or propagate atrial fibrillation.¹⁷ Pulmonary veins contain interstitial cells of Cajallike cells. Interstitial cells of Cajal of the human gut express Na_v1.5 and are mechanosensitive.^{18,19} Interestingly, ranolazine was effective in suppression of excitatory Na⁺ channel activity in pulmonary vein sleeves.²⁰

In our recent study, ranolazine was found to abolish pressure- and flowinduced mechanical activation of voltage shifts or increased peak current, respectively.¹¹ The correlation of these changes, as seen by voltage clamp electrophysiology, with spontaneous action potentials has been limited. Ranolazine was reported to reduce action potential frequency and TTX-resistant and -sensitive currents in rat DRG neurons.²¹ Furthermore, optical mapping of ventricular myocytes under intermittent shear stress^{22,23} lacks accompanying electrophysiological data. These studies on mechanosensitivity have utilized either dissociated native cells or transfected cultured cells that generally lack required components.

There were two aims in this study. First, we sought to determine whether HL-1 cultured cells, derived from murine atrial myocytes and known to exhibit spontaneous electro-mechanical rhythmic activity, would be sensitive to mechanical stimulation. Second, to determine whether this mechanical sensitivity would be responsive to ranolazine, we examined the sensitivity of spontaneous action potentials to flow of extracellular solution in current-clamp mode and correlated this shear stressmediated sensitivity with that of voltageclamped Na⁺ currents in the same cells. We found rhythmic action potentials and whole cell Na⁺ currents to be mechanosensitive and mechanosensitivity of either to be inhibited by ranolazine.

Results

Na⁺ current is required for action potentials in HL-1 cultured atrial myocytes. Sodium current contributes to action potentials (AP) in cardiac smooth muscle. Additionally, the currents in the murine atrial myocyte cell line HL-1 have been shown previously to have genotypic, phenotypic, and electrophysiologic properties similar to adult atrial cardiomyocytes.24 Inward currents recorded from a voltageclamped HL-1 cell dialyzed with Cs⁺- rich solution resembled the sodium current prevalent in native cardiomyocytes with a similar voltage-dependence of activation¹¹ (Fig. 1A and B). HL-1 cells plated on coverslips formed networks, and a majority of cells exhibited rhythmic contractions. Replacement of extracellular Na⁺ with N-methyl-D-glucamine (NMDG⁺) abolished action potential spikes in HL-1 (Fig. 1C), an effect partially reversible but persistent after 40 min, suggesting the Na⁺ current was a prerequisite for action potential oscillations.

Ranolazine inhibits the mechanical activation of peak Na⁺ current induced by bath flow in HL-1 cells. Ranolazine can inhibit peak and persistent Na⁺ current of Na, 1.5.25 Having tested the effect of ranolazine on the mechanosensitivity of Na⁺ channels in dissociated murine cardiomyocytes and SCN5A-transfected HEK293 cells,11 we confirmed its effect on HL-1 cells. Shear stress by flow of control solution at 10 mL/min led to a 14 ± 5% increase in peak Na⁺ current (control, $-9.8 \pm 2.0 \text{ pA/pF}$; flow, $-11.2 \pm 2.4 \text{ pA/pF}$; n = 5, p < 0.05, Fig. 2). In the same cells, 50 µM ranolazine blocked peak Na⁺ current by 47 ± 3% (control, -9.8 ± 2.0 pA/pF; ranolazine, -5.0 ± 0.9 pA/pF; n = 5, p < 0.05) and inhibited the peak current activated by flow (ranolazine, -5.0 ± 0.9 pA/pF; flow with ranolazine, $-4.9 \pm$ 0.9 pA; n = 5, p > 0.05, Fig. 2), suggesting that ranolazine inhibits shear-induced mechanosensitivity of endogenous Na⁺ current in HL-1 as in dissociated myocytes or SCN5A-transfected HEK cells.

Ranolazine inhibits mechanical activation of rhythmic action potentials in HL-1 cells. We tested the effect of ranolazine on AP using current-clamp wholecell electrophysiology. Flow of drug-free solution significantly increased the rate of AP decay by $27 \pm 12\%$ (control, -37.6 \pm 0.8; flow, -46.9 \pm 0.8 mV/s; n = 4, p < 0.05) and increased AP frequency by $18 \pm 4\%$ (control, 0.43 ± 0.03 ; flow, 0.50± 0.03 Hz; n = 4, p < 0.05, Fig. 3). After incubation with ranolazine (50 μ M) for 4.2 ± 0.8 min, the slope of decay decreased $32 \pm 12\%$ to -25.1 ± 0.6 mV/s, and frequency slowed 16 \pm 5% to 0.35 Hz (n = 4, p < 0.05 to control). However, myocytes exposed to ranolazine were less responsive to mechanical stimulus, as decay slope increased only 17 ± 6% (ranolazine, -25.1 \pm 0.6 mV/s; flow with ranolazine, -28.6 \pm 0.6 mV/s; n = 4, p > 0.05), and frequencyincreased only 10 ± 2% (ranolazine, 0.35 \pm 0.01 Hz; flow with ranolazine, 0.38 \pm 0.01 Hz; n = 4, p > 0.05 to no drug with flow or p < 0.05 to drug without flow by two-way repeated-measures ANOVA with Bonferroni multiple comparisons posttest). No significant changes to peak amplitude, area, rise slope, or baseline



Figure 2. Ranolazine blocks the mechanosensitive response and peak currents of endogenous Na⁺ channels in HL-1 cells. (**A**) Single Na⁺ current traces recorded by whole cell voltage-clamp from HL-1 cells, elicited by stepping to -30 from -120 mV before (black traces, Flow OFF) or during (gray traces, Flow ON) bath flow, produced by rinsing solution through the recording chamber at 10 mL/min in the absence (Control, 0 μ mol/L) or presence (Ranolazine, 50 μ M) of drug. (**B**) Mean parameters of HL-1 Na⁺ current in response to solution flow with or without ranolazine. From top left to bottom right, peak current density, time constant (τ) of activation, V_{1/2} of steady-state activation, slow time constant of inactivation (τ_1), fast time constant of inactivation (τ_2), and V_{1/2} of steady-state inactivation. (n = 5; *p < 0.05 compared with 0 mL/min flow, †p < 0.05 compared with 0 μ M ranolazine, and p > 0.05 interaction between bath flow and ranolazine blockade by two-way ANOVA with Bonferroni multiple comparisons posttest).

(Fig. 3C) nor to antipeak amplitude (data not shown) were observed in response to flow and/or drug.

Discussion

In this study, we report the following: first, the HL-1 cultured cell line, derived from murine atrial caridiomyocytes, express robust spontaneous rhythmic action potentials; second, shear stress by flow increases peak Na⁺ currents and action potential frequency, and it also accelerates the repolarization phase of the action potential; third, both the baseline current and flow-induced changes to the action potential were blocked by ranolazine.

Ranolazine prolongs repolarization and decreases frequency of the HL-1 **spontaneous action potentials.** The HL-1 cell line is a robust in vitro model for studying atrial myocyte electrophysiology. In the absence of shear stress, ranolazine extended the AP length via delayed repolarization, as demonstrated previously in dissociated myocytes.^{26,27} Rather than by block of late Na⁺ current which would shorten repolarization, AP extension due to prolongation of the repolarization phase is more likely due to block of I_{Kr} and/or NCX, two other known targets for ranolazine (IC₅₀ ~10 and ~100 uM for ranolazine²⁸).

Shear flow shortens repolarization and increases frequency of the HL-1 spontaneous action potentials. Faster AP frequency evoked by flow in HL-1 cells is similar to what has been reported on rat



ventricular cardiomyocytes with optical mapping under intermittent parallelplate shear stress.^{22,23} The effects of shear stress on HL-1 AP are not uniform across all AP parameters, such as resting potential, upstroke, plateau, or repolarization. Thus, it is less likely that non-selective cation stretch-sensitive channels (SACs) are involved in the shear response.²⁹ Instead, voltage-gated ion channels may be responsible for shear sensitivity of HL-1 AP.

Figure 3. Ranolazine inhibits the flow-induced response of rhythmic action potentials in HL-1 atrial myocytes. (A) Rhythmic action potentials recorded sequentially from a single HL-1 atrial myocyte before (OFF) or during (ON) flow of extracellular solution without (0 μ M) or with drug (50 μ M ranolazine). From top to bottom, time elapsed was 0, 2, 12 and 14 min, and resting potential was -42, -40, -32 and -31 mV. (B) Action potentials from (A) were both normalized to and centered at peak. (C) Mean parameters of HL-1 action potentials in response to solution flow without (0 µM, filled circles) or with drug (50 μM ranolazine, empty circles). From top left to bottom right, peak amplitude, frequency, area between peak and baseline, rate of rise, rate of decay, baseline. (n = 4; *p < 0.05 compared with Flow OFF, †p < 0.05 compared with 0 μ M Ranolazine, and p > 0.05 interaction between bath flow and ranolazine blockade by two-way ANOVA with Bonferroni multiple comparisons posttest).

Ranolazine decreases the effects of shear flow on HL-1 spontaneous action potentials. Shortened repolarization and increased frequency, the responses of HL-1 AP to shear stress that were decreased by ranolazine, support the notion that ranolazine modulates cardiomyocyte mechanosensitivity.11 The voltage clamp data presented here show that Na_v currents are present in HL-1 cells (Fig. 1) and that shear stress increases their peak currents (Fig. 2). These results agree with previous findings in Na_v1.5-transfected HEK293 and freshly dissociated murine cardiomyocytes.11 However, under shear stress without ranolazine, we would have predicted that sodium channel mechanoactivation should depolarize the membrane, accelerate the early part of the upstroke, accelerate the initial part of the repolarization, and have a mixed effect on frequency (i.e., slower recovery from inactivation vs. a left-shifted window). Our results do not support this prediction; instead, the upstroke and early part of repolarization both overlap while frequency changes. We offer two potential explanations. First, the lack of depolarization with shear stress could be due to low availability of Na_v current in resting HL-1 cells. While the resting membrane potential of HL-1 cells is -15 mV (Fig. 3C), the half-point of Na⁺ channel availability is -100 mV, and the window current is -70 mV (Fig. 1B). Therefore, we expect the availability of $Na_v 1.5$ at the resting potential to be small, which would limit the effects of mechanosensitivity on Na_v channels at baseline. Second, we have shown previously that recovery from inactivation is delayed with stretch in the patch, possibly explaining the lack of effect on the AP upstroke as Na^* channel availability is decreased.³

While ranolazine and shear stress affect the same parameters of HL-1 AP, their effects are opposite. Furthermore, when ranolazine and shear stress are combined, ranolazine diminishes the effects of the latter on HL-1 AP. These data support the role of ranolazine as a blocker of mechanosensitivity and suggest that other targets of ranolazine may be involved in mechanosensitivity. Aside from $Na_v1.5$, ranolazine is known to affect several other ion channels and transporters, including some possibly involved in the effects of shear stress.²⁸

In summary, we show that the HL-1 cell line is a viable model for the study of atrial myocyte mechanosensitivity, that ranolazine and shear stress have opposite effects on spontaneous action potentials, and that ranolazine diminishes the effects of shear stress. We also show that Na⁺ currents in HL-1 cells are responsive to both ranolazine and shear stress and suggest other potential ranolazine targets of mechanosensitivity.

Methods

HL-1 cell culture. The HL-1 murine atrial myocyte cell line was maintained in accordance with established protocol.²⁴ HL-1 cells grown on coverslips were transferred directly to a recording chamber filled with extracellular solution (below) without resuspension.

Data acquisition. Electrodes (Kimble KG12 glass) were pulled by a Sutter P97 puller (Sutter Instruments), fire polished to 2–5 M Ω resistance and coated with R6101 heat-cured compound. Whole cell data from HL-1 cells dialyzed with intracellular solution were recorded with an Axopatch200B patch clamp, CyberAmp320, Digidata 1322A, and pClamp9.2 software (Molecular Devices).

Voltage-clamp protocol. A single 18 sweep, 90 sec pulse protocol was designed to measure peak current, voltage dependence, and kinetics of activation and inactivation as described previously.¹¹ Cells were held at -120 mV, stepped to test pulses from -130 to 30 mV at 5 or 10 mV intervals for 3 sec, then to -120 mV for 0.1 msec, and finally to a second test pulse at -30 mV for 100 ms. The sampling rate was 20 kHz, and intersweep time was 5 sec.

Current-clamp protocol. Currentclamp data were acquired in gap-free mode with no current injected. Data were sampled at 100 Hz and filtered at 40 Hz.

Solutions. The extracellular solution contained (in mM): 160 Cl⁻, 150 Na⁺ or NMDG⁺, 5 K⁺, 2.5 Ca²⁺, 10 HEPES, 5.5 glucose, and 0 or 0.05 ranolazine. pH was adjusted to 7.4 with NaOH. The intracellular solution contained (in mM): 125 CH₃SO₃⁻, 35 Cl⁻, 145 Cs⁺, 5 Na⁺, 5 Mg²⁺, 5 HEPES, 2 EGTA. pH was adjusted to 7.0 with CsOH. Osmolality was 290 mmol/kg. The predicted liquid junction potential of -12.7 mV was subtracted during analysis. All chemicals were purchased from Sigma-Aldrich.

Mechanical stimulation. Flow of solution through the bath chamber at 10 mL/min served as the mechanical stimulus as previously described.9,11 For voltage-clamp experiments, control currents were recorded in ranolazine-free solution after seal and access until a stable baseline was established. Next, the 0.7 mL elliptical chamber was flushed with ranolazine-free solution at 10 mL/min for the duration of the 90 sec recording to obtain bath flow data as a paired control. Upon the conclusion of the flow recording, extracellular solution plus ranolazine premixed to 50 µM was immediately washed into the chamber then allowed to incubate on cells for 4 min before the ranolazine data were recorded. Finally, the cells were perfused with ranolazine solution at 10 mL/min to determine the effect of ranolazine on mechanosensitivity of Na_v1.5. For current-clamp experiments, continuous recordings were taken under stagnant control or flowing conditions for 4 or 1 min, respectively, alternately without or with ranolazine (50 μ M) present.

Analysis. Data were analyzed with pClamp 10 (Molecular Devices), Microsoft Excel 2010, and SigmaPlot 12 (Systat Software). Spontaneous action potentials were analyzed by template search event detection in pClamp 10. Peak currents are expressed as a fraction of cell capacitance (pA/pF). Peak currents at test pulses 1 or 2 vs. the voltages of test pulse 1 determined the voltage dependence of activation or inactivation, respectively. Peak currents normalized to the equation

$$I_{NORM} = \frac{100 \left(I_{V} \right)}{I}$$

I PEAK were fit with a sigmoid 3-parameter curve:

$$y = \frac{1}{1 + e^{\left(\frac{x_0 - x}{b}\right)}}$$
 where

, where x_0 is $V_{1/2}$, the voltage of half-activation or -inactivation. Currents that activated during the first 50 ms of test pulse 1 were fitted with a three-term weighted exponential equation:

$$f(t) = K_0 \left(\sum_{1}^{3} f_i e^{-t/\tau_i} \right) + C$$

three time constants represent one activation and two inactivation states of $Na_v 1.5$. Significance was assigned when p < 0.05by two-way repeated measures ANOVA with Bonferroni multiple comparisons posttest (Prism 5, GraphPad Software).

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