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Legomedicine—A Versatile Chemo-Enzymatic Approach for the Preparation of Targeted Dual-Labeled Llama Antibody–Nanoparticle Conjugates

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Supporting Information

ABSTRACT: Conjugation of llama single domain antibody fragments (Variable Heavy chain domains of Heavy chain antibodies, VHHs) to diagnostic or therapeutic nanoparticles, peptides, proteins, or drugs offers many opportunities for optimized targeted cancer treatment. Currently, mostly nonspecific conjugation strategies or genetic fusions are used that may compromise VHH functionality. In this paper we present a versatile modular approach for bioorthogonal VHH modification and conjugation. First, sortase A mediated transPEGylation is used for introduction of a chemical click moiety. The resulting clickable VHHs are then used for conjugation to other groups employing the Cu⁺-independent strain-promoted alkyne–azide cycloadition (SPAAC) reaction.



Using this approach, tail-to-tail bispecific VHHs and VHH-targeted nanoparticles are generated without affecting VHH functionality. Furthermore, this approach allows the bioconjugation of multiple moieties to VHHs for simple and convenient production of VHH-based theranostics.

INTRODUCTION

The challenge in cancer therapy is to specifically deliver therapeutic agents to tumor cells with minimal delivery to and effects on healthy tissues. Targeted delivery of drugs with antibody drug conjugates (ADCs) has received a lot of attention in the last decades. Also, nanoparticles have been used for drug delivery. Liposomes can carry hydrophilic drugs in the lumen^{1,2} while micelles are suited for carrying hydrophobic drugs.³ Liposomes and micelles, however, distribute relatively randomly in the body after intravenous injection,¹ and introduction of tumor specificity in these nanoparticles could greatly increase local delivery and efficacy of cancer therapeutics.^{4–6}

A number of therapeutic antibodies with relative tumor specificity are now applied clinically (e.g., trastuzumab and cetuximab against HER2 and EGFR^{7,8}). Effects of treatments with these targeted drugs are often limited because of recurrences of drug-resistant tumors.^{9–12} The challenge should therefore be to develop a multispecific tumor-targeting nanoparticle platform that can deliver cytotoxic payload to all cancer cells in a tumor, resulting in specific and acute death of all cells in a tumor.

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Figure 1. (A) CBB stained SDS-PAGE gel of samples obtained during 7D12-C-LPETG-8xHis-Vsv production. 1 = bacterial lysate, 2 = flow-through Ni-NTA purification, 3 = pre-eluate Ni-NTA purification, 4 = eluate post Ni-NTA purification and dialysis. (B) LC-MS characterization of 7D12-C-LPETG-8xHis-Vsv (with an expected mass of 17837 Da, observed 17962 and 18137 Da) before TCEP reduction. (C) LC-MS characterization of 7D12-C-LPETG-8xHis-Vsv after 20 min incubation with 20 mM TCEP. A pure product of 17831 Da was detected, suggesting that the thiol before TCEP reduction was oxidized by small molecules, among which was presumably glutathione. The left graphs show the ultraviolet absorbance chromatograms (at 215 nm) and the middle and right graphs show the total mass spectra and deconvoluted spectra of the UV-peaks bracketed by the arrowheads, respectively.

Conventional protein conjugation strategies mostly use relatively nonspecific methods, e.g., N-hydroxysuccinimide (NHS) chemistry utilizing ε -NH₂ groups from lysines. Depending on the number and distribution of lysines in the active binding domain of the targeting agent, these conjugation protocols may compromise functionality. This specifically applies to single domain antibody fragments (VHHs, Nanobodies) due to their small size. VHHs are recombinant antigenbinding domains that are derived from cameloid heavy chainonly antibodies and receive increasing interest as therapeutic or diagnostic compounds.^{13,14} VHHs typically have a molecular weight of 15-20 kDa and may bind target antigens with pM to nM affinity, similar to conventional antibodies. The ease of genetic engineering and handling of VHHs, combined with a number of other advantages such as high water solubility, low production cost, small size, low immunogenicity in humans, and high thermo- and pH stability,¹⁵ makes this class of antibodies a highly interesting alternative to conventional antibodies.

A number of VHHs with high specificity and affinity against tumor targets (e.g., EGFR, HER2, MET) have been developed.^{16–18} Approaches to conjugate VHHs without compromising functionality include the site specific introduction of a carboxyterminal cysteine allowing maleimide chemistry¹⁹ and introduction of a carboxyterminal five-amino-acid sequence (LPXTG) allowing sortase A transpeptidation.²⁰

Here we present a versatile modular approach for bioorthogonal VHH conjugations, using sortase A mediated transPEGylation to introduce a carboxyterminal click moiety, and subsequent Cu⁺-independent strain-promoted alkyne-azide cycloadition (SPAAC) for conjugation of a functional group that may be connected to another VHH and/or polymeric micelles. Furthermore, introduction of a cysteine before the LPXTG tag allows maleimide chemistry to introduce a second diagnostic or therapeutic compound. This method allows the production of highly uniform VHH-based conjugates that can consist of multiple modular moieties, examples being labeled bispecific VHHs, bivalent VHHs, and VHH-targeted nanoparticles. Because all chemistry occurs at the carboxyterminus, this method does not affect VHH functionality. Furthermore, concomitant with conjugation, carboxy-terminal tags that allow purification of the VHHs after bacterial expression are removed, a prerequisite for future clinical applications.

RESULTS AND DISCUSSION

VHHs were successfully expressed and purified as VHH-C-LPETG-8xHis-Vsv or VHH-LPETG-8xHis-Vsv fusion proteins with yields of 5-10 mg/L *E. coli* culture (see Figure 1A for a



Figure 2. (A) Fluorescent image and (B) CBB staining of an SDS-PAGE gel of samples obtained during the procedure of sortagging. $1 = 7D12^{[Fluo]}$, $2 = 7D12^{[Fluo]}$, sortase A/H₂N-PEG₃-N₃ reaction mixture after overnight reaction, $3 = purified 7D12^{[Fluo]}$ -N₃. Note the molecular shift between lanes 1 and 2, 3 that is a result of removal of the G-8xHis-Vsv tag and simultaneous addition of the small PEG₃-N₃ group. (C) LC-MS characterization of $7D12^{[Fluo]}$ (expected 18265 Da, observed 18278 Da). (D) LC-MS characterization of $7D12^{[Fluo]}$ -N₃ (expected 15790 Da, observed 15806 Da). The left graphs show the ultraviolet absorbance chromatograms (at 215 nm) and the middle and right graphs show the total mass spectra and the deconvoluted spectra of the UV-peaks bracketed by the arrowheads, respectively.

representative Coomassie Brilliant Blue (CBB) stained SDS-PAGE gel of 7D12-C-LPETG-8xHis-Vsv, the anti-EGFR VHH that was used as a prototype in this study). Since the 8xHis-Vsv tags are substituted by compounds of interest during the sortase A reaction, loss of these tags was compensated for by introducing a cysteine residue directly upstream of the LPETG-8xHis-Vsv sequence, allowing maleimide-based labeling with alternative tags for detection. Liquid chromatography mass spectrometry (LC-MS) indicated the correct mass for expressed 7D12-C-LPETG-8xHis-Vsv and it showed that the free thiol group of this cysteine was oxidized, presumably by glutathione based on its molecular weight of 307 Da (Figure 1B). After a mild TCEP reduction, the thiol was available for conjugation (Figure 1C). The reaction of the 7D12-C-LPETG-8xHis-Vsv protein (from now on referred to as 7D12) with fluorescein-5-maleimide was efficient, resulting in a pure preparation of 7D12-C^[Fluo]-LPETG-8xHis-Vsv (from now on referred to as 7D12^[Fluo]) (Figure 2A +B, lane 1). LC-MS confirmed the conjugation of one fluorescein residue per VHH in 7D12^[Fluo] (Figure 2C), demonstrating that the two native framework cysteine residues involved in an intramolecular disulfide bridge²¹ were not reactive toward fluorescein-5-maleimide under the conditions used. This was further confirmed in additional experiments that showed an absence of maleimide reaction with multiple VHHs lacking the C terminal cysteine (Figure S1).

The LPETG-8xHis-Vsv tag in $7D12^{[Fluo]}$ allows sortase A mediated transpeptidation which releases the G-8xHis-Vsv tag in exchange for an H₂N-GGG-containing peptide (the prototypical

substrate of sortase A). This allows rapid and easy purification of the reaction product to homogeneity, because the G-8xHis-Vsv cleavage product and the 6xHis-tagged sortase A enzyme can be removed from the reaction mixture by Ni-bead depletion. Because a wide variety of chemically modified monodisperse PEG compounds is nowadays available, sortase A mediated conjugation of such compounds to the carboxyterminus is a highly attractive approach.

Using H₂N-PEG_x-X as a nucleophile for sortase A mediated PEGylation, a range of VHH-PEG_x-X constructs can be generated in which X represents a drug or a reactive group. In this work we used the combination of H2N-PEG3-N3 and H2N-PEG₃-DBCO in the SPAAC reaction.²² In an attempt to improve the reaction with H_2N -PEG_x-X, we tested recently described mutants of sortase A with optimized LPETG cleavage activity,²³ and compared them to the variants with a N-terminal deletion of either 25 or 59 amino acids (Supporting Information Figure S8). These optimizations were performed using the anti-PlexinD1 VHH A12.²⁴ Sortase A Δ 59 was ultimately selected as most optimal, since despite increased LPETG cleavage rates, the low affinity of the mutant sortases for H2N-GGG or H2N-PEGx-X resulted in high levels of hydrolysis at the threonine. Furthermore, we found that the sortase A $\Delta 25$ variant, that contains an N-terminal 6xHis-tag, experienced unexplained proteolysis just downstream of the His-tag during the sortase A reaction (Supporting Information Figure S8D). Since this precluded complete removal of sortase A activity, we discarded this variant.

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Further experimentation using different molar ratios of H₂N-PEG_x-X or H₂N-GGG revealed that H₂N-PEG_x-X was incorporated less efficiently than H₂N-GGG, requiring a 200fold molar excess of H₂N-PEG_x-X over VHH-(C)LPETG-8xHis-Vsv as compared to a 25-fold excess of H₂N-GGG (under conditions of 4 h reaction at 30 °C with sortase A Δ 59). Lower concentrations of both nucleophiles in the reaction resulted in the formation of VHH-LPET-OH hydrolysis products, as observed with LC-MS (Supporting Information Figure S9A). These results were in line with those of Parthasarathy et al., who showed that conjugation of H₂N-PEG, to EGFP in a ratio of 1:1 by sortase A Δ 59 was highly inefficient.²⁵ Yet, the use of H₂N-PEG.-X nucleophiles instead of triglycine-containing substrates would have an important advantage: conjugation of H₂N-PEG₂-X yields VHH-(C)LPET-PEG_x-X in a one-way reaction, unlike conjugation of H₂N-GGG-X that reconstitutes a sortase A substrate site in the VHH-(C)LPET-GGG-X reaction product. Indeed we could show that VHH-LPET-PEG_x-X is not a substrate for sortase A, in contrast to VHH-LPETGGG-peptide (see Figure S2).

Using the optimized conditions, $7D12^{[Fluo]}$ was conjugated to H_2N -PEG₃-N₃ with sortase A Δ 59 to yield $7D12^{[Fluo]}$ -N₃ (Figure 2A+B). After removal of sortase A Δ 59, G-8xHis-Vsv, and unreacted $7D12^{[Fluo]}$ by Ni-NTA depletion, $7D12^{[Fluo]}$ -N₃ was obtained in a 66% yield with a >95% purity based on LC-MS (Figure 2D). Similar results were obtained when H_2N -PEG₃-DBCO was used in the reaction with sortase A Δ 59 (Figure S3). Furthermore, the methodology has been successfully tested and validated for three more VHHs in our lab (Supporting Information Figure S10) demonstrating the versatility of this approach.

Bispecific or bivalent antibody conjugates are valuable compounds for targeted cancer therapy.^{26,27} Current approaches to make bispecific or bivalent VHHs often involve genetic fusion of VHH open reading frames, allowing production only in head-to-tail fusion format. It has already been shown that the affinity of the second VHH in such bispecific constructs may be dramatically affected by the presence of the first VHH.²⁸ Sortase A technology allows the generation of tail-to-tail dimers, leaving antigen binding sites of the individual composing VHHs intact²⁰ (Figures 3 and 4A). We tested the validity of this hypothesis by



Figure 3. Schematic representation of the monomeric VHH, head-totail bispecific VHH, and tail-to-tail bispecific VHH and their nomenclature in this report.

using sortase A Δ 59 in combination with H₂N-PEG₃-X linkers to generate 7D12^[Fluo]-N₃ and 4E4-DBCO, 4E4 being a low-affinity Transferrin receptor (TfR)-binding VHH (unpublished results) that is used here as a control. After the click reaction (see Figure 4B+C for analysis of the reaction products), heterodimer ^N7D12^{C[Fluo]_C}4E4^N could be readily purified from residual monomers by size exclusion chromatography, resulting in >90% pure product of 36 kDa (Figure S4). In parallel, we generated



Figure 4. (A) Schematic overview of bispecific tail-to-tail (Structure 1) or head-to-tail (Structure 2) VHH constructs. In panels B and C, SDS-PAGE is shown (fluorescence signal and CBB staining, respectively) depicting the products of the sortase A reaction to produce bispecific $^{N}7D12^{C[Fluo]}_{-}C4E4^{N}$. 1 = $7D12^{[Fluo]}$, 2 = 4E4, 3 = $7D12^{[Fluo]}_{-}DBCO$, 4 = $4E4-N_3$, 5 = $^{N}7D12^{C[Fluo]}_{-}C4E4^{N}$ before sephadex G75 purification. In panels D and E, the expression of bispecific head-to-tail VHHs is depicted with (D) fluorescence signal and (E) CBB staining of an SDS-PAGE gel. 1 = $^{N}7D12^{C}_{-}[G_4S]_{10}^{-N}4E4^{C}_{-}[Fluo]$, 2 = $^{N}4E4^{C}_{-}[G_4S]_{10}^{-N}7D12^{C}_{-}[Fluo]$, 3 = $^{N}7D12^{C}_{-}[G_4S]_{20}^{-N}4E4^{C}_{-}[Fluo]$, 4 = $^{N}4E4^{C}_{-}[G_4S]_{20}^{-N}7D12^{C}_{-}[Fluo]$. (F) Flow cytometry histogram derived from A431 cells incubated with the various bispecific constructs and controls.

conventional head-to-tail bispecific VHHs, with 7D12 and 4E4 separated by a $[G_4S]_{10}$ linker or a $[G_4S]_{20}$ linker and a C-terminal C-Flag-6xHis (compounds ^N7D12^C- $[G_4S]_n$ -^N4E4^C and ^N4E4^C- $[G_4S]_n$ -^N7D12^C; Figures 3 and 4A). *E. coli* expression of these bispecific VHHs was successful as shown with SDS-PAGE analysis (Figure 4D+E). Yields were 2–4 mg/L *E. coli* culture. The bispecifics were labeled on the C-terminal cysteine with fluorescein-5-maleimide as described for monomeric VHHs, and the correct mass was confirmed with LC-MS (Figure S5).

Importantly, in this context both the head-to-tail and tail-totail bispecific VHHs contain only one fluorescein molecule, allowing quantitative comparison of the EGFR-binding capacity of these formats with 7D12^[Fluo]. Constructs were tested in flow cytometry analyses using the high EGFR expressing squamous carcinoma cell line A431 (Figure 4F). Compounds ^N7D12^C- $[G_4S]_n$ -^N4E4^{C[Fluo]} with both G_4S linker lengths and

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Figure 5. Chemical structures and corresponding ¹H NMR-spectra of (A) Ben-PCL₇-mPEG₂₀₀₀ and (B) Ben-PCL₇-PEG₂₀₀₀-DBCO measured in CDCl₃.



Figure 6. (A) Cartoon of VHH^[Fluo]-decorated mTHPC loaded micelles. (B) Fluorescein visualization. (C) CBB staining of the SDS-PAGE analysis of SPAAC reaction between 7D12^[Fluo]-N₃ and DBCO-micelles. $1 = 7D12^{[Fluo]}$, $2 = 7D12^{[Fluo]}$ -N₃, 3 = 10% DBCO-micelles with 5% mTHPC, and 4 = 10% DBCO-micelles with 5% mTHPC and 5% 7D12^[Fluo]. (D) Median values of fluorescence intensity as measured in flow cytometry. Left bar graph = fluorescein total signal on A431 (EGFR⁺) and E98 (EGFR⁻) cells after incubation with $7D12^{[Fluo]}$ as a positive control and $7D12^{[Fluo]}$ -micelles. Right bar graph = mTHPC total signal on both A431 and E98 cells after incubation with targeted or nontargeted micelles. * indicates significance with p < 0.05. (E) Fluorescence microscopy of A431 cells immediately after incubation with $1 = 7D12^{[Fluo]}$, $2 = 7D12^{[Fluo]}$ -micelles, and 3 = nontargeted micelles. Cyan depicts mTHPC, incorporated in the micelles; green depicts fluorescein. The scale bar depicts 20μ M.

 $^{\rm N}7D12^{\rm C[Fluo]_C}4E4^{\rm N}$ were equally effective as $7D12^{\rm [Fluo]}$ in binding to A431 cells. In contrast, binding to EGFR was reduced with a factor of 10 for compounds $^{\rm N}4E4^{\rm C}\text{-}[G_4S]_{\rm n}\text{-}^{\rm N}7D12^{\rm C[Fluo]}$ with both G_4S linker lengths, confirming that, at least for VHH 7D12, epitope binding is hindered by the presence of a VHH at the amino-terminus. Thus, bispecific VHHs generated via tail-to-tail click fusion are more robust than head-to-tail bispecific VHHs.

PEGylation is an important modification of nanoparticles that is applied to increase half-life in the circulation by avoiding rapid clearance by spleen, liver, and kidney.²⁹ PEGylation of VHHs, accomplished by clicking DBCO-PEG to VHH-N₃, indeed results in better in vivo characteristics.³⁰ Sortase A mediated conjugation of H₂N-PEG_x yields the interesting option to decorate PEGylated nanoparticles with functionally active VHHs. To test this hypothesis we applied click chemistry to conjugate 7D12^[Fluo]- N_3 to benzoyl-poly(ε -caprolactone)methoxypoly(ethylene glycol) (ben-PCL₇-mPEG₂₀₀₀) diblockbased micelles, equipped with a small percentage of DBCO groups. Ben-PCL7-mPEG2000 diblock-based micelles are biocompatible and biodegradable, and can be used as carriers of hydrophobic drugs that can be incorporated in the micellar The decoration of micelles with VHHs may increase core.3 affinity of the nanoparticles to targets by an avidity effect. Also, this approach allows the generation of multispecific drug-loaded targeting nanoparticles by simply decorating these with different tumor-targeting VHHs.

¹H NMR spectra showed that synthesis of intermediate products (Figure S6) and end products ben-PCL₇-mPEG₂₀₀₀ and ben-PCL₇-mPEG₂₀₀₀-DBCO (Figure 5A+B) was successful. Micelles were prepared by film-hydration of a mixture of 90% ben-PCL₇-mPEG₂₀₀₀ diblock polymers and 10% ben-PCL₇-mPEG₂₀₀₀-DBCO, resulting in micelles that contain a calculated 20–30 DBCO click groups per particle. Dynamic light scattering (DLS) experiments of the resulting micelles revealed a mean particle size of 28 ± 2 nm and a polydispersity index (PDI) of 0.32 ± 0.02.

DBCO-micelles were decorated with 7D12 via a click chemistry reaction with 7D12^[Fluo]-N₃ in a 2:1 DBCO:N₃ ratio, to minimize amounts of residual unconjugated $7D12^{[Fluo]}$ -N₃ after the click reaction. To confirm that during handling and experimentation micelles remained intact, we included the hydrophobic photosensitizer meta-tetra(hydroxyphenyl)chlorin (mTHPC) during micelle formation, equipping the micelles with a fluorescent signal that is readily distinguishable from 7D12associated fluorescein (Figure 6A). SDS-PAGE of the 7D12 conjugated micelles revealed a shift of ~3 kDa as compared to the starting material 7D12^[Fluo]-N₃, indicating successful conjugation of 7D12^[Fluo]-N₃ to the DBCO-block-copolymer with a conjugation yield of >85% (Figure 6B,C). Again this conjugation method was verified for other available VHHs in our lab (Supporting Information, Figure S11A+B), showing its versatility.

We next tested whether 7D12 on the decorated micelles had retained EGFR affinity by performing flow cytometry after incubation with EGFR-positive A431 squamous cell carcinoma or EGFR-negative E98 glioma cells,³² using 7D12^[Fluo] as reference. 7D12^[Fluo]-micelles showed efficient binding to A431 cells but negligible binding to E98 cells (Figure 6D). Importantly, binding of 7D12^[Fluo]-micelles led to 70% higher cell-associated fluorescein-fluorescence than binding of monomeric 7D12^[Fluo]. This may reflect the loading of individual micelles with multiple fluorescein-labeled 7D12 moieties or may be due to cooperative binding and an avidity effect. Increased binding of $7D12^{[Fluo]}$ micelles to A431 cells was confirmed with fluorescence microscopy, using the fluorescein signal as readout (Figure 6E, green signal in panel 2, compare to $7D12^{[Fluo]}$ in panel 1). The increase in fluorescein signal was accompanied by an increased association of mTHPC fluorescence in $7D12^{[Fluo]}$ -micelles as compared to nondecorated micelles (Figure 6D, right graph, and Figure 6E, cyan signal). There was no difference in binding of $7D12^{[Fluo]}$ -micelles and nondecorated micelles to E98 cells, suggesting that $7D12^{[Fluo]}$ -micelles bound as intact particles to A431 cells in an EGFR-dependent manner. It must however be noted that there was also some nonspecific association of mTHPC with both A431 cells and E98 cells. Whether this reflects nonspecific binding of micelles or of free mTHPC that is released from micelles is difficult to discriminate.

These results indicate that the multivalency induced by coupling multiple VHHs to a micelle, increased uptake of these particles and their payload in target positive cells. Although we restricted ourselves in this study to micelles, this conjugation approach is predicted to work with many other types of proteinor PEG-based nanoparticles (e.g., liposomes, polymersomes) once a controlled percentage of the building blocks is equipped with a chemical click group. Interestingly, this procedure will also allow the controlled synthesis of multispecific targeting nanoparticles, e.g., by preparing nanoparticles with a defined number of noncompatible clickable agents such as DBCO and tetrazine moieties, allowing simultaneous conjugation of VHH-PEG₃-N₃ and VHH-PEG_x-TCO (trans-cyclooctene). Whereas the free thiol group in VHH-C-LPET-PEG_x-X may be used for maleimide-based conjugation of hydrophilic drugs, micelles may be used to simultaneously carry hydrophobic drugs, making this to a versatile approach.

CONCLUSION

Conjugations of VHHs to diagnostic or therapeutic compounds should involve the VHH's carboxy-terminus, distant from the antigen binding site, in order to retain full VHH functionality. Here, a bioorthogonal site-specific conjugation approach is presented based on sortase A and click chemistry, combined with cysteine—maleimide conjugation. This approach allows the preparation of molecularly defined targeted nanoparticles, preserving targeting potential and concomitantly removing unwanted tags from VHHs, a prerequisite for potential clinical applications. The potential to perform controlled dual labeling of proteins without the loss of protein function is an important next step to the preparation of optimized theranostics.

EXPERIMENTAL PROCEDURES

VHH Production and Purification. VHH 4E4 is a low affinity VHH ($K_d \sim 500$ nM) directed against transferrin receptor (TfR) and was used as an inert VHH in this study. VHH 7D12 against EGFR has been described in detail before.^{17,33} The VHH coding sequences were cloned in frame behind the pelB leader sequence in modified pHEN-IX vectors in which the sortase A recognition sequence LPETG, either or not preceded by a cysteine, was inserted just upstream of the 8xHis-Vsv tags, resulting in pHENIX-VHH-LPETG-8xHis-Vsv and pHENIX-VHH-C-LPETG-8xHis-Vsv. Plasmids were transformed in *E. coli* strain ER2566 for standard protein expression. Cells were grown in 2xTY medium containing 3.5% (w/v) glycerol and 50 μ g/mL ampicillin at 37 °C. At an OD₆₀₀ between 0.6 and 0.8, recombinant protein expression was induced with 1.0 mM

isopropyl β -D-thiogalactoside (IPTG, Serva, Heidelberg, Germany) at 30 °C for 2.5 h. Cells were harvested by centrifugation at 2830 g for 20 min at 4 °C and the periplasmic protein fraction was isolated via osmotic lysis. Cells were resuspended in ice cold TES buffer (200 mM Tris pH 8.0, 0.5 mM EDTA, 20% w/v sucrose, protease inhibitors (Complete cocktail, Roche, Basel, Switzerland)) and incubated for 20 min on ice, followed by centrifugation (4424 g, 20 min, 4 °C). After collection of the supernatant the bacterial pellet was resuspended in TES buffer containing 15 mM MgSO4 and incubated on ice for 20 min. After centrifuging, both supernatants were pooled and incubated with Ni-NTA sepharose (IBA, Goettingen, Germany), pre-equilibrated with 50 mM phosphate pH 7.4, 500 mM NaCl, for 1 h at 4 °C. After washing of the beads with 50 mM phosphate pH 7.4, 500 mM NaCl, and 10 mM imidazole, 8xHis-tagged proteins were eluted with 500 mM imidazole in 50 mM phosphate pH 7.4 and 500 mM NaCl. The eluate was dialyzed against 50 mM TRIS pH 7.5 and 150 mM NaCl in a 3.5 kDa dialysis membrane (Spectrum laboratories, Los Angeles, CA, USA). VHHs were analyzed by SDS-PAGE under reducing conditions (Coomassie brilliant blue (CBB) staining), followed by analysis on the Odyssey CLx infrared imaging system (LI-COR, Lincoln, NE, USA)) and liquid chromatography and mass spectrometry (LC-MS, Shimadzu HPLC and Thermo Finnigan LCQ Fleet) on a C4 column. Protein concentrations were determined by absorbance at 280 nm using a Nanodrop spectrophotometer (Thermo Fisher Scientific, Waltham, MA, USA).

Generation and Production of In Tandem VHH Dimers. In tandem bispecific $^{N}7D12^{C_N}4E4^{C}$ and the converse orientation $^{N}4\dot{E4}^{C_{-}N}7D12^{C}$ VHHs connected by $[G_{4}S]_{10}$ of [G₄S]₂₀ linkers and one C-terminal cysteine and Flag-8xHis-tags were synthesized as described before.³² In short, reading frames encoding 7D12 and 4E4 were PCR amplified with primer sets that allowed fusion of the two VHHs, separated by $[G_4S]_{10}$ or $[G_4S]_{20}$ linkers. The N-terminal VHH was amplified with M13rev and primer (Rev10GS agtaGGATCCGCCACCTCCA-CTGCCACCGCCACCtgaggagaccgtgacctgggtccc) annealing to the VTVSS sequence of the VHH thereby introducing the linker including a BamHI site. The C-terminal VHH was amplified with M13 and a primer (Forw10GS tcttGGATCCGGCGGGGGGAG-GTAGTGGGGGGGGGGGGGGCTCAgaggtgcagctgggggtctggg) annealing to EVQLV of the VHH introducing the rest of the linker and also including a BamHI site. The resulting fragments were respectively cut with SfiI/BamHI and BamHI/Eco91I and subsequently ligated into the vector (SffiI/Eco91I) in a three point ligation. Plasmids were validated by Sanger sequencing, and proteins expressed in E. coli strain TG1 and purified as described above. VHHs were analyzed by SDS-PAGE under reducing conditions.

Sortase A Production and Purification. Plasmid pGBMCS-SortA (Addgene, Cambridge, MA, USA, plasmid #21931), encoding sortase A with a deletion of amino acids 1–59 and an N-terminal Gb1 domain was transformed into *E. coli* ER2566 and protein expression induced using standard conditions as used for VHHs. After harvesting cells by centrifugation and resuspension in 50 mM TRIS pH 8.0, 150 mM NaCl, and Cocktail protease inhibitor (Roche), cells were lysed by sonication at 4 °C using a Bandalin Sonopuls HD2070 sonicator. The bacterial extracts were cleared by centrifugation and the 6xHis-tagged sortase A Δ 59 was purified with Ni-NTA sepharose as described for VHHs. The purified sortase A Δ 59 was dialyzed in a 3.5 kDa membrane against 50 mM TRIS pH 7.5 and 150 mM NaCl. The protein was analyzed by SDS-PAGE

under reducing conditions (CBB staining) and LC-MS. Protein concentration was determined by absorbance at 280 nm using a Nanodrop spectrophotometer.

Fluorescein-5-Maleimide Conjugation. Monomeric VHH-C-LPETG-8xHis-Vsv and in tandem bispecific ^NVHH₂^C- $[G_4S]_n$ -^NVHH_b^C-C-Flag-6xHis (typically ~50-250 μ M) were incubated for 15 min at RT with 20 mM tris(2-carboxyethyl)phosphine (TCEP, Thermo Fisher Scientific, Waltham, MA, USA) to reduce the free thiol group. TCEP was removed by filtration over a 10 kDa MWCO centrifugal unit (Amicon, Millipore, Billerica, MS, USA) employing 5 washing cycles with 20 mM phosphate pH 7.0, 150 mM NaCl, and 5 mM EDTA. Fluorescein-5-maleimide (Thermo Fisher Scientific, Waltham, MA, USA) from a 10 mM stock in dimethylformamide was reacted with the reduced VHH construct in a 3:1 molar ratio, shielded from light and at RT for 2 h to yield VHH^[Fluo] or ^NVHH_A^C-[G₄S]_{10/20}^NVHH_B^{C[Fluo]}. Excess fluorescein-5-maleimide was removed by filtration in a 10 kDa MWCO centrifugal unit employing 4 washing cycles with 50 mM Tris pH 7.5 and 150 mM NaCl. Reaction products were analyzed by SDS-PAGE under reducing conditions and/or LC-MS. Fluorescein signal was visualized on a Chromato-vue TM-20 Transilluminator (UVP) after which the gel was stained with CBB. Protein concentration was determined by ultraviolet absorbance at 494 nm ($\varepsilon_{494,7D12\text{-}FLUO}$ = 70 000 M⁻¹ cm⁻¹) using a Nanodrop spectrophotometer.

Sortase A Mediated Conjugation of Click Moieties. To produce clickable fluorescent VHHs, 50 µM VHH^[Fluo] was incubated overnight at RT in the dark with 50 μ M sortase A Δ 59 and 4.0 mM H₂N-PEG₃-N₃ or H₂N-PEG₃-DBCO (Jena Biosciences, Jena, Germany) in 50 mM Tris pH 7.5, 150 mM NaCl supplemented with 10 mM CaCl₂. This reaction induces the covalent linkage of PEG linkers via the amine group to the threonine in the LPETG tag, releasing G-8xHis-Vsv. Sortase A Δ 59, the cleaved G-8xHis-Vsv tag from the reacted VHH, and residual intact VHH were removed by adsorption to Ni-NTA sepharose, pre-equilibrated with 50 mM phosphate pH 7.4 and 500 mM NaCl, for 1 h at 4 °C. Then, the excess of unreacted PEG linkers was removed by filtration in a 10 kDa MWCO centrifugal unit. The reaction product was washed three times with 50 mM phosphate pH 7.4 and 500 mM NaCl, and two times with 50 mM phosphate pH 7.4 and 500 mM NaCl containing 20% w/v glycerol. The protein constructs were analyzed by SDS-PAGE under reducing conditions and LC-MS, and protein concentration was determined by ultraviolet absorbance at 494 nm.

To check if LPET-PEG-X is a substrate for sortase A, 20 μ M 7D12^[Fluo], 20 μ M 7D12^[Fluo]-N₃-DBCO-biotin, and 7D12-GGG-peptide were incubated with 50 μ M sortase A Δ 59 for 4 h at 30 °C. Reaction products were analyzed on a CBB stained SDS-PAGE gel and a Western blot stained with 1:10.000 Avidin-Alexa680 (Invitrogen).

Generation of VHH Dimers via C-to-C Conjugation. Tail to tail coupled bispecific VHHs were produced by incubating 4E4-N₃ with 7D12^[Fluo]-DBCO in a 1:1 molar ratio o/n at RT. Bispecific ^N7D12^{C[Fluo]-C}4E4^N was separated from single VHHs by separation on a G75 Sephadex (Pharmacia fine chemicals, Uppsala, Sweden) column. Fractions were analyzed on a SDS-PAGE gel under reducing conditions (CBB staining).

Synthesis of Diblock Copolymers. *Ben-PCL₇-PEG*₂₀₀₀*methoxy*. The amphiphilic diblock copolymer consisting of the hydrophobic poly(ε -caprolactone) (PCL) and the hydrophilic methoxy-polyethylene glycol (mPEG) were synthesized using a method described by Wennink et al. (submitted for publication).



Figure 7. Synthesis routes for ben-PCL₇-mPEG₂₀₀₀ and ben-PCL₇-mPEG₂₀₀₀-DBCO. Synthesis of both molecules starts with (A) ring opening polymerization of ε -caprolactone with benzyl alcohol which affords ben-PCL₇-OH and (B) activation of the hydroxyl end group with *p*-nitrophenylchloroformate. Then for synthesis of amphiphilic ben-PCL₇-mPEG₂₀₀₀, (C) mPEG₂₀₀₀-NH₂ is coupled to the activated ben-PCL₇-PNC. For synthesis of clickable ben-PCL₇-mPEG₂₀₀₀-DBCO, (D) NH₂-PEG₂₀₀₀-NHBoc is coupled to the activated ben-PCL₇-PNC, (E) the Boc protection group is removed with HCl gas, and (F) NHS-DBCO is conjugated to ben-PCL₇-mPEG₂₀₀₀-NH₂.

Briefly, Ben-PCL-OH macromers were prepared using benzyl alcohol as the initiator in the Tin(II) ethylhexanoate $(Sn(Oct)_2)$ catalyzed ring opening polymerization of ε -caprolactone (CL) (Figure 7A). The monomer to initiator ratio was chosen such that the average degree of polymerization was 7 CL units. The hydroxyl end groups of ben-PCL₇-OH were subsequently reacted with *p*-nitrophenyl chloroformate to form *p*-nitrophenyl carbonate substituted polymers (PNC) (Figure 7B). The diblock copolymers were obtained by reacting ben-PCL₇-PNC and mPEG2000-NH₂ at 1:1 ratio in toluene at RT (Figure 7C). Average molecular weights of the polymers were determined by NMR.

Ben-PCL₇-PEG₂₀₀₀-DBCO. NH₂-PEG2000-NH-Boc (1.00 g, 0.5 mmol) (Layson Bio, Arab, AL, USA) was added to a solution of ben-PCL₇-PNC (0.707 g, 0.5 mmol) in 20 mL dry toluene. This mixture was stirred for 1 h at RT under nitrogen atmosphere (Figure 7D). The mixture was washed at least 6 times with diethyl ether to remove *p*-nitrophenol. The product was dried in a vacuum oven and obtained as a white powder (yield: 97%). Subsequently, 0.2 g of the powder was dissolved in 20 mL of DCM and the Boc group was removed by bubbling HCL gas through the solution for 15 min (Figure 7E). The product, ben-PCL₇-PEG₂₀₀₀-NH₂ (0.187 g, 0.063 mmol), was purified by precipitation in diethyl ether and subsequently dissolved in 20 mL of dry DCM. To produce clickable copolymers, dibenzocyclooctyne (DBCO)-NHS (0.025 g, 0.063 mmol) (Jena Biosciences, Jena, Germany) was added to this ben-PCL₇-PEG₂₀₀₀-NH₂ solution, and the reaction mixture was

stirred for 24 h at RT under a nitrogen atmosphere (Figure 7F). The mixture was carefully washed with diethyl ether to remove unreacted DBCO-NHS. The product was dried in a vacuum oven and obtained as a white powder (yield: 61%).

¹H (300 MHz) NMR spectra were recorded using a Gemini NMR spectrometer (Varian Associates Inc. NMR instruments, Palo Alto, CA). Polymers were dissolved in $CDCl_3$ at a concentration of 0.015 g mL⁻¹.

Dynamic Light Scattering. The size and the size distribution of empty particles were measured by dynamic light scattering (DLS) using a Malvern CGS-3 multiangle goniometer (Malvern ltd., Malvern), consisting of a HeNe laser source ($\lambda = 632.8 \text{ nm}, 22 \text{ mW}$ output power), temperature controller (Julabo water bath) and a digital correlator ALV-5000/EPP. Time correlation functions were analyzed using the ALV-60X0 Software v 3.X provided by Malvern, to obtain the *Z*-average hydrodynamic diameter of the particles (Zave) and the particle size distribution (polydispersity index, PDI). The samples were analyzed at 25 °C.

7D12 Functionalized mTHPC Loaded Micelle Preparation. Micelles were formed by film-hydration. To prepare micelles with 10% functional groups on the surface, ben-PCL₇-PEG₂₀₀₀ and ben-PCL₇-PEG₂₀₀₀-DBCO were dissolved in dichloromethane (DCM, Sigma-Aldrich, Saint Louis, MS, USA) and mixed in a 9:1 weight ratio in a 5 mL glass vial (VWR, Radnor, PA, USA). To this mixture, the hydrophobic photosensitizer mTHPC (*meta*-tetra(hydroxyphenyl) chlorine, Biolitec AG, Jena, Germany) in tetrahydrofuran (THF, Sigma-

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Aldrich, Saint Louis, MS, USA) was added at a 5% w/w mTHPC/polymer ratio. DCM and THF were evaporated under vacuum. The obtained polymer film was hydrated to a 20 mg/mL solution in PBS for 2 h at RT, gently heated to 60 °C, and filtered through a 0.22 μ m filter. To obtain micelles with 5% surface coverage with VHH 7D12^[Fluo], the DBCO-micelles were reacted with 7D12^[Fluo]-N₃ in a 2:1 molar DBCO:N₃ ratio. To ensure efficient click reaction kinetics, we kept the N₃ and DBCO concentration >100 μ M. Reactions were allowed to proceed overnight in the dark at 4 °C with continuous shaking at 450 rpm. The final product was analyzed by SDS-PAGE under reducing conditions (Fluorescein signal and CBB staining). Nontargeted mTHPC-ben-PCL₇-PEG₂₀₀₀ micelles were prepared according to the same procedure, but without incubation with 7D12^[Fluo]-N₃.

Cell Culture. The EGFR-overexpressing squamous carcinoma cell line A431 and the EGFR-negative glioma cell line E98³⁴ were cultured in DMEM (Lonza, Basel, Switzerland) supplemented with 10% fetal calf serum (FCS, Gibco, Thermo Fisher Scientific, Waltham, MA, USA) and 40 μ g/mL gentamycin (Centrafarm, Etten-Leur, The Netherlands). Cells were incubated at 37 °C in 5% CO₂ in a humidified atmosphere.

Flow Cytometry and Confocal Fluorescence Microscopy Analysis. Cells were dissociated from culture flasks with 10 mM EDTA, counted, and transferred to V-bottom-shaped 96well microplates (BD Biosciences, Franklin Lakes, NJ, USA) at 5 \times 10⁵ cells/well. All subsequent steps were done on ice and all washing steps were executed by centrifugation of the plates at 1,500xg for 2 min. Cells were washed twice with PBS and aspecific binding sites were blocked by preincubating cells for 10 min with PBA (PBS, 0.5%BSA, 2% FCS). Subsequently cells were incubated with 1 μ M fluorescein-labeled VHHs in PBA for 20 min, washed and resuspended in PBA, and analyzed using the CyAn ADP analyzer (Beckman Coulter, Fullerton, CA, USA).

To analyze uptake of VHH-micelles with flow cytometry, cells were grown to 80% confluency in 8-well chambered glass slides (NUNC, Thermo Fisher Scientific, Waltham, MA, USA) and incubated with 20 μ M (=0.6 mg/mL) targeted or nontargeted mTHPC-micelles or equimolar VHH concentrations at 37 °C for 30 min. Cells were washed twice with warm DMEM and dissociated with trypsin at 37 °C. Then, cells were taken up in PBA and analyzed using the CyAn flow cytometer. mTHPC was quantified with parameter FL-8, fluorescein was quantified with parameter FL-1. To visualize binding and uptake with confocal microscopy A431 and E98 cells were grown in 8 wells Lab-Tek borosilicate coverglass chambers (Nunc, ThermoFisher Scientific, Waltham, MA, USA), and incubated with the micelles and controls as described for flow cytometry. After washing, cells were kept in phenol red free DMEM supplemented with 20 mM HEPES, and imaged on a TCS SP8 microscope (Leica Microsystems, Mannheim, Germany) equipped with a HC PL APO C5 40×/0.85 dry objective. During imaging, cells were maintained at 37 °C. The UV405 laser was used for excitation, and emission was collected between 500 and 600 nm for fluorescein and 630 and 730 nm for mTHPC.

ASSOCIATED CONTENT

Supporting Information

The Supporting Information is available free of charge on the ACS Publications website at DOI: 10.1021/acs.bioconj-chem.6b00638.

Site specificity of maleimide labeling; reconstitution of the sortase A substrate site when conjugating with either H_2N -PEG₃-X or H2N-GGG; sephadex G75 purification of tail-to-tail dimers; LC-MS characterization of head-to-tail dimers and ¹H NMR spectra of intermediate products of micellar building blocks; comparison of sortase A variants; comparison of H_2N -PEG- N_3 to H_2N -GGG incorporation by sortase A; applicability of sortase A conjugations to other VHHs (PDF)

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Notes

The authors declare no competing financial interest.

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REFERENCES

(1) Barenholz, Y. C. (2012) Doxil(R) - The first FDA-approved nanodrug: Lessons learned. *J. Controlled Release* 160 (2), 117–34.

(2) Dawidczyk, C. M., Kim, C., Park, J. H., Russell, L. M., Lee, K. H., Pomper, M. G., and Searson, P. C. (2014) State-of-the-art in design rules for drug delivery platforms: lessons learned from FDA-approved nanomedicines. *J. Controlled Release 187*, 133–44.

(3) Gou, M., Zheng, X., Men, K., Zhang, J., Wang, B., Lv, L., Wang, X., Zhao, Y., Luo, F., Chen, L., et al. (2009) Self-assembled hydrophobic honokiol loaded MPEG-PCL diblock copolymer micelles. *Pharm. Res.* 26 (9), 2164–73.

(4) Molavi, O., Xiong, X. B., Douglas, D., Kneteman, N., Nagata, S., Pastan, I., Chu, Q., Lavasanifar, A., and Lai, R. (2013) Anti-CD30 antibody conjugated liposomal doxorubicin with significantly improved therapeutic efficacy against anaplastic large cell lymphoma. *Biomaterials* 34 (34), 8718–25.

(5) Arachchige, M. C., Reshetnyak, Y. K., and Andreev, O. A. (2015) Advanced targeted nanomedicine. J. Biotechnol. 202, 88–97.

(6) Fan, M., Liang, X., Yang, D., Pan, X., Li, Z., Wang, H., and Shi, B. (2016) Epidermal growth factor receptor-targeted peptide conjugated phospholipid micelles for doxorubicin delivery. *J. Drug Targeting 24*, 111.

(7) Stemmler, H. J., Kahlert, S., Siekiera, W., Untch, M., Heinrich, B., and Heinemann, V. (2005) Prolonged survival of patients receiving trastuzumab beyond disease progression for HER2 overexpressing metastatic breast cancer (MBC). *Oncol. Res. Treat.* 28 (11), 582–6.

(8) Grigorean, V. T., Ciuhu, A. N., Rahnea Nita, G., Strambu, V., Straja, D. N., Popescu, M., Sandu, A. M., and Rahnea Nita, R. A. (2014) Efficacy of cetuximab in metastatic colon cancer - case report. *Chirurgia (Bucur)* 109 (3), 383–9.

(9) de Paula Costa Monteiro, I., Madureira, P., de Vasconscelos, A., Pozza, D. H., and de Mello, R. A. (2015) Targeting HER family in HER2-positive metastatic breast cancer: potential biomarkers and novel targeted therapies. *Pharmacogenomics* 16 (3), 257–71.

(10) Xie, C., Jin, J., Bao, X., Zhan, W. H., Han, T. Y., Gan, M., Zhang, C., and Wang, J. (2010) Inhibition of mitochondrial glutaminase activity reverses acquired erlotinib resistance in non-small cell lung cancer. *Oncotarget* 1 (1), 610–21.

(11) Soucheray, M., Capelletti, M., Pulido, I., Kuang, Y., Paweletz, C. P., Becker, J. H., Kikuchi, E., Xu, C., Patel, T. B., Al-Shahrour, F., et al. (2015) Intratumoral Heterogeneity in EGFR-Mutant NSCLC Results in Divergent Resistance Mechanisms in Response to EGFR Tyrosine Kinase Inhibition. *Cancer Res.* 75 (20), 4372–83.

(12) Lee, Y., Wang, Y., James, M., Jeong, J. H., and You, M. (2016) Inhibition of IGF1R signaling abrogates resistance to afatinib (BIBW2992) in EGFR T790M mutant lung cancer cells. *Mol. Carcinog.* 55 (5), 991–1001.

(13) Kijanka, M., Dorresteijn, B., Oliveira, S., and van Bergen en Henegouwen, P. M. (2015) Nanobody-based cancer therapy of solid tumors. *Nanomedicine (London, U. K.)* 10 (1), 161–74.

(14) Chakravarty, R., Goel, S., and Cai, W. (2014) Nanobody: the "magic bullet" for molecular imaging? *Theranostics* 4 (4), 386–98.

(15) Harmsen, M. M., and De Haard, H. J. (2007) Properties, production, and applications of camelid single-domain antibody fragments. *Appl. Microbiol. Biotechnol.* 77 (1), 13–22.

(16) Moghimi, S. M., Rahbarizadeh, F., Ahmadvand, D., and Parhamifar, L. (2013) Heavy Chain Only Antibodies: A New Paradigm in Personalized HER2+ Breast Cancer Therapy. *Bioimpacts* 3 (1), 1–4.

(17) Roovers, R. C., Laeremans, T., Huang, L., De Taeye, S., Verkleij, A. J., Revets, H., de Haard, H. J., and van Bergen en Henegouwen, P. M. (2007) Efficient inhibition of EGFR signaling and of tumour growth by antagonistic anti-EFGR Nanobodies. *Cancer Immunol. Immunother.* 56 (3), 303–317.

(18) Heukers, R., Altintas, I., Raghoenath, S., De Zan, E., Pepermans, R., Roovers, R. C., Haselberg, R., Hennink, W. E., Schiffelers, R. M., Kok, R. J., et al. (2014) Targeting hepatocyte growth factor receptor (Met) positive tumor cells using internalizing nanobody-decorated albumin nanoparticles. *Biomaterials* 35 (1), 601–10.

(19) Massa, S., Xavier, C., De Vos, J., Caveliers, V., Lahoutte, T., Muyldermans, S., and Devoogdt, N. (2014) Site-specific labeling of cysteine-tagged camelid single-domain antibody-fragments for use in molecular imaging. *Bioconjugate Chem.* 25 (5), 979–88.

(20) Witte, M. D., Cragnolini, J. J., Dougan, S. K., Yoder, N. C., Popp, M. W., and Ploegh, H. L. (2012) Preparation of unnatural N-to-N and C-to-C protein fusions. *Proc. Natl. Acad. Sci. U. S. A.* 109 (30), 11993–8.

(21) Rahbarizadeh, F., Ahmadvand, D., and Sharifzadeh, Z. (2011) Nanobody; an old concept and new vehicle for immunotargeting. *Immunol. Invest.* 40 (3), 299–338.

(22) Debets, M. F., van Berkel, S. S., Schoffelen, S., Rutjes, F. P., van Hest, J. C., and van Delft, F. L. (2010) Aza-dibenzocyclooctynes for fast and efficient enzyme PEGylation via copper-free (3 + 2) cycloaddition. *Chem. Commun. (Cambridge, U. K.)* 46 (1), 97–9.

(23) Chen, I., Dorr, B. M., and Liu, D. R. (2011) A general strategy for the evolution of bond-forming enzymes using yeast display. *Proc. Natl. Acad. Sci. U. S. A.* 108 (28), 11399–404.

(24) Roodink, I., Raats, J., van der Zwaag, B., Verrijp, K., Kusters, B., van Bokhoven, H., Linkels, M., de Waal, R. M., and Leenders, W. P. (2005) Plexin D1 expression is induced on tumor vasculature and tumor cells: a novel target for diagnosis and therapy? *Cancer Res.* 65 (18), 8317–23.

(25) Parthasarathy, R., Subramanian, S., and Boder, E. T. (2007) Sortase A as a novel molecular "stapler" for sequence-specific protein conjugation. *Bioconjugate Chem.* 18 (2), 469–76.

(26) Baeuerle, P. A., and Reinhardt, C. (2009) Bispecific T-cell engaging antibodies for cancer therapy. *Cancer Res.* 69 (12), 4941–4.

(27) Kontermann, R. E., and Brinkmann, U. (2015) Bispecific antibodies. *Drug Discovery Today* 20 (7), 838–47.

(28) Els Conrath, K., Lauwereys, M., Wyns, L., and Muyldermans, S. (2001) Camel single-domain antibodies as modular building units in bispecific and bivalent antibody constructs. *J. Biol. Chem.* 276 (10), 7346–50.

(29) Veronese, F. M., and Mero, A. (2008) The impact of PEGylation on biological therapies. *BioDrugs* 22 (5), 315–29.

(30) Rashidian, M., Wang, L., Edens, J. G., Jacobsen, J. T., Hossain, I., Wang, Q., Victora, G. D., Vasdev, N., Ploegh, H., and Liang, S. H. (2016) Enzyme-Mediated Modification of Single-Domain Antibodies for Imaging Modalities with Different Characteristics. *Angew. Chem., Int. Ed.* 55 (2), 528–33.

(31) Hofman, J. W., Carstens, M. G., van Zeeland, F., Helwig, C., Flesch, F. M., Hennink, W. E., and van Nostrum, C. F. (2008) Photocytotoxicity of mTHPC (temoporfin) loaded polymeric micelles mediated by lipase catalyzed degradation. *Pharm. Res.* 25 (9), 2065–73.

(32) Navis, A. C., van Lith, S. A., van Duijnhoven, S. M., de Pooter, M., Yetkin-Arik, B., Wesseling, P., Hendriks, W. J., Venselaar, H., Timmer, M., van Cleef, P., et al. (2015) Identification of a novel MET mutation in high-grade glioma resulting in an auto-active intracellular protein. *Acta Neuropathol.* 130 (1), 131–44.

(33) Roovers, R. C., Vosjan, M. J., Laeremans, T., el Khoulati, R., de Bruin, R. C., Ferguson, K. M., Verkleij, A. J., van Dongen, G. A., and van Bergen en Henegouwen, P. M. (2011) A biparatopic anti-EGFR nanobody efficiently inhibits solid tumour growth. *Int. J. Cancer* 129 (8), 2013–24.

(34) Claes, A., Schuuring, J., Boots-Sprenger, S., Hendriks-Cornelissen, S., Dekkers, M., van der Kogel, A. J., Leenders, W. P., Wesseling, P., and Jeuken, J. W. (2008) Phenotypic and genotypic characterization of orthotopic human glioma models and its relevance for the study of antiglioma therapy. *Brain Pathol.* 18 (3), 423–33.