REVIEW ARTICLE



The Influence of Growth and Maturation on Stretch-Shortening Cycle Function in Youth

John M. Radnor¹ · Jon L. Oliver^{1,2} · Charlie M. Waugh⁶ · Gregory D. Myer^{3,4,5} · Isabel S. Moore¹ · Rhodri S. Lloyd^{1,2,7}

Published online: 12 September 2017 © The Author(s) 2017. This article is an open access publication

Abstract Hopping, skipping, jumping and sprinting are common tasks in both active play and competitive sports. These movements utilise the stretch-shortening cycle (SSC), which is considered a naturally occurring muscle action for most forms of human locomotion. This muscle action results in more efficient movements and helps optimise relative force generated per motor unit recruited. Innate SSC development throughout childhood and adolescence enables children to increase power (jump higher and sprint faster) as they mature. Despite these improvements in physical performance, the underpinning mechanisms of SSC development during maturational years remain unclear. To the best of our knowledge, a comprehensive review of the potential structural and neuromuscular adaptations that underpin the SSC muscle action does not exist in the literature. Considering the importance of

John M. Radnor jradnor@cardiffmet.ac.uk

- ¹ Youth Physical Development Centre, School of Sport, Cardiff Metropolitan University, Cyncoed Campus, Cyncoed Road, Cardiff CF23 6XD, UK
- ² Sport Performance Research Institute New Zealand, AUT University, Auckland, New Zealand
- ³ Division of Sports Medicine, Cincinnati Children's Hospital Medical Center, Cincinnati, OH, USA
- ⁴ Department of Pediatrics and Orthopaedic Surgery, College of Medicine, University of Cincinnati, Cincinnati, OH, USA
- ⁵ The Micheli Centre for Sports Injury Prevention, Boston, MA, USA
- ⁶ Department of Physical Therapy, University of British Columbia, Vancouver, BC, Canada
- ⁷ Centre for Sport Science and Human Performance, Waikato Institute of Technology, Waikato, New Zealand

the SSC in human movement, it is imperative to understand how neural and structural adaptations throughout growth and maturation can influence this key muscle action. By understanding the factors that underpin functional SSC development, practitioners and clinicians will possess a better understanding of normal development processes, which will help differentiate between training-induced adaptations and those changes that occur naturally due to growth and maturation. Therefore, the focus of this article is to identify the potential underpinning mechanisms that drive development of SSC muscle action and to examine how SSC function is influenced by growth and maturation.

Key Points

Stretch-shortening cycle (SSC) performance increases with age in various forms of hopping, jumping, and sprinting tasks.

Research suggests that changes in the neuromuscular system during growth and maturation include increases in muscle size, pennation angle, fascicle length, tendon stiffness, motor unit recruitment and preactivation.

Combined, these adaptations may result in an improved SSC function due to increased elastic energy reutilisation, increased neural potentiation and an enhanced stretch-reflex contribution, predominantly due to an increase in force producing capabilities and a reduced electro-mechanical delay.

Operational Definitions

- *Childhood* represents the developmental period of life from the end of infancy to the beginning of adolescence. The term children refers to girls and boys (generally up to the age of 11 and 13 years, respectively) who have not developed secondary sex characteristics.
- The term *adolescence* refers to a period of life between childhood and adulthood. Although adolescence is a more difficult period to define in terms of chronological age due to differential maturation rates [1], girls 12–18 years and boys 14–18 years are generally considered adolescents.
- The terms *youth* and *young athletes* represent global terms which include both children and adolescents.
- *Growth* refers to quantifiable changes in body composition, either the size of the body as a whole or the size of specific regions of the body [2].
- *Maturation* refers to qualitative system changes, both structural and functional, in the body's progress toward adulthood, such as the change of cartilage to bone in the skeleton, appearance of pubic hair or menstruation [1, 2]. The timing and tempo of maturation varies greatly between individuals during growth. Timing refers to when specific maturational events occur and tempo refers to the rate at which maturation progresses. All tissues, organs and systems of the body mature with growth, but they do so at different times and rates [1]. Within the current article, maturation is referring to biological maturation unless specifically stated.
- *Natural development* represents the increase in physical ability (strength, power, speed, etc.) that is apparent in children as they experience growth and maturation, independent of any specific physical training.
- Adaptation, in the context of this article, refers to changes in structure or neuromuscular properties.
- *Peak height velocity* is a somatic biological maturity indicator and reflects the maximum acceleration of growth during adolescence, providing a universal landmark to reflect the occurrence of other body dimension velocities within and between individuals [3].

1 Introduction

Active play constitutes a large part of physical activity for children [4], with various forms of hopping, skipping and jumping tasks being performed frequently during the early years. Additionally, sprinting, jumping and throwing are key components of athletic motor skill competencies that are important for success in most sports [5]. These movements utilise the stretch-shortening cycle (SSC), which is characterised by an eccentric 'stretching' action prior to a subsequent concentric 'shortening' action [6]. The prior eccentric stretching (e.g. pre-load of the muscle) has been shown to enhance the performance of the final concentric phase in comparison to an isolated concentric action [7, 8]. For example, jump height improves 18-30% in adults when utilising a preceding countermovement [9, 10]. These values may be lower in a younger population, however, as pre-stretch only increased jump height in children by approximately 1-5% [11]. The SSC has been categorised into fast and slow actions based on a ground contact thresholds [12]; ground contact times shorter than 250 ms were classified as fast SSC activities, whereas slow SSC actions have ground contact times in excess of 250 ms. It has been suggested that slow SSC actions may enable greater force production because of increased contraction time and working range [7, 13], whereas fast SSC actions promote greater movement speed via elastic energy usage, stretch reflex contributions and a greater level of neural excitation from the preceding stretch [7, 13–17].

SSC performance increases non-linearly with age in various forms of hopping and jumping tasks [1, 18, 19], and the underlying mechanisms of such neuromuscular developments associated with maturation remain unclear. SSC performance is governed by effective neuromuscular function, requiring an efficient interaction between both neural and muscular systems [6, 8] and the structure of the musculo-tendon unit (MTU) [20, 21]. Figure 1 presents a visual representation of the primary neuromuscular and structural qualities that are likely to influence the natural development of SSC function. Specifically, age-related developments in the neural system that could influence SSC function include greater preactivation [22, 23], increased stretch reflex magnitude [24] and musculotendinous stiffness [25], and reduced co-contraction ratios [26]. A number of musculo-tendinous adaptations also occur throughout childhood and adolescence, including increases in muscle thickness, cross-sectional area (CSA) and fascicle length, and changes in fascicle pennation angle (Table 1) [27–29]. Furthermore, adaptations to the tendinous structures occur, including increases in tendon CSA, length and stiffness [28, 30-34]. This review explains how the qualities highlighted in Fig. 1 develop throughout maturation, and the manner in which development influences SSC function in children and adolescents.

2 Structural Adaptations

2.1 Fibre Type Composition

Differences in fibre type composition between children and adults has been proposed as one of the reasons that children produce less force than adults [35]. Research surrounding the



Fig. 1 Visual representation of the primary mechanisms underpinning growth- and maturity-related changes in stretch-shortening cycle function. *CSA* cross-sectional area, *EMD* electromagnetic delay, *MU* motor-

unit, *RFD* rate of force development, *SSC* stretch-shortening cycle, *RER* rate of EMG rise

effects of age on fibre type composition is scarce, and researchers have suggested ethical constraints as the main reason behind this [36]. From the available research into fibre type composition between adults and children, there is no clear consensus as to whether these differences exist. Children aged 3-21 months have been shown to have a lower percentage of type IIb fibres in comparison to adults (6.2 \pm 1.1%) [mean \pm standard deviation (SD)] vs. 20.5 \pm 1.6%), and a higher proportion of type IIa and type I fibres. Furthermore, a previous study has reported that the proportion of type I fibres decreases from approximately 65% at age 5 years to 50% at age 20 years [36]. Longitudinal data have demonstrated that gender differences in fibre type composition may also become apparent as adolescents transition towards adulthood. Research has shown that type I fibre percentage tended to increase in women (51 \pm 9% to 55 \pm 12%) and decrease significantly in the men (55 \pm 12% to 48 \pm 13%) between the ages of 16 and 27 years. On the other hand, there has been support for similar fibre type composition between children and adults [37].

While the available data are conflicting, the majority of research suggests that there may be child–adult differences in fibre type composition. Considering the fact that type I fibres produce less force and have a slower shortening velocity than type II fibres [38], throughout maturation the

potential higher proportion of type II muscle fibres may result in an improved ability to rapidly produce force, resulting in greater benefit from the SSC.

2.2 Muscle Size

During growth, large increases in muscle size are seen in a number of lower limb muscles [27, 28, 39]. Adults demonstrate greater muscle thickness than children [33, 39] and older adolescents exhibit greater muscle thickness relative to their younger peers [28, 32]. A recent review reported that the contribution of hyperplasia to changes in human muscle CSA is assumed to be small [40], and therefore the developmental increases in muscle size could mainly be attributed to increases in fibre hypertrophy. Considering that the muscle's anatomical CSA (ACSA) is a major predictor of maximum strength and power in both adults and children [41, 42], increases in muscle size are a major factor contributing to the improved capacity to produce force as children experience biological maturation, resulting in greater performance outcomes (e.g. jump heights) during SSC activities.

Maximal muscle force is lower in children than in adults [30, 43, 44], but when normalised to body mass or muscle size, child–adult and sex-related differences in relative force production are inconclusive. There is evidence

Adaptation with maturation?	Influence on kinetic variables	Likely influence on stretch-shortening cycle function	Supporting evidence
Fibre type composition	Force production	Increased force production	[33–36]
	Shortening velocity	Increased RFD	
Increased muscle size	Force production	Increased impulse	[5, 25, 26, 37, 39, 40, 56, 59, 60]
		Increased RFD	
		Increased cross bridges	
		Increased EE storage	
Increased pennation angle	L-T and F-V relationship	Increased force production	[27, 52, 55, 60, 64, 65, 70, 73–78]
	Gearing	Increased RFD	
		Increased EE reutilisation	
		Increased stiffness	
Increased fascicle length	Shortening velocity	Increased RFD	[25, 26, 32, 37, 60, 65, 68, 70, 72]
		Increased EE reutilisation	
		Increased stiffness	
Increased tendon size	Rate of force production	Increased tendon stiffness	[25, 26, 28, 29, 31, 84]
		Increased RFD	
Increased tendon stiffness	Rate of force production	Increased RFD	[17, 23, 26, 28, 29, 32, 92, 94, 99–101]
		Decreased EMD	
		Increased stretch reflex	
MU recruitment	Force production	Increased RFD	[33, 42, 103–107]
		Increased contraction speed	
Co-contraction	Force production	Increased EE reutilisation	[4, 17, 23, 42, 108, 109, 111]
		Increased stretch reflex	
		Increased neural potentiation	
Preactivation	Rate of force production	Reduced EMD	[20, 21, 114, 115]
		Increased RFD	
Reflex control	Force production	Increased force production	[20–23, 60, 72, 114]
		Increased RFD	
		Increased stiffness	
RER	Rate of force production	Increased RFD	[33, 41, 94, 107, 118]

Table 1 Influence of structural and neural adaptations throughout biological maturation on stretch-shortening cycle function

EE elastic energy, *EMD* electromagnetic delay, *F-V* force–velocity, *L-T* length–tension, *MU* motor-unit, *RER* rate of EMG rise, *RFD* rate of force development

indicating that adults have a greater muscle force when normalised to body mass [25, 43, 45] and ACSA [25, 43, 44]; however, the majority of muscles studied have been pennate in nature [27, 32, 34, 46–56], and ACSA does not account for the entire contractile mass in a pennate muscle. Conversely, physiological CSA (PCSA) includes all sarcomeres in parallel and theoretically represents the sum of the CSAs of all the muscle fibres within the muscle [57]. PCSA can be calculated as the ratio between muscle volume and optimum fascicle length [27]. When normalising force to PCSA, boys were found to have a 21% higher force per unit area of muscle than men, also known as muscle-specific tension [56]. However, a number of methodological assumptions and omissions were made during the research process, including the assumption that the voluntary activation of the muscle was 100% in both groups, which have since been addressed in a follow-up study that identified no difference in muscle-specific tension between children and adults [39]. This finding indicates that increased muscle strength during growth could be less associated with muscle quality, although this is the only study to report such findings, and thus knowledge of child–adult differences in muscle-specific tension is still lacking.

As muscle size increases during growth and biological maturation [27, 28, 39], higher force output may be achievable during both the concentric and eccentric phases of the SSC. While this is yet to be researched, in isolated

concentric and eccentric muscle actions, muscle size has been correlated with both quadriceps and hamstring concentric strength and hamstring eccentric strength [58]. The benefit of increased concentric strength during SSC actions include greater impulse, defined as the product of force and the period of time in which the force is expressed [59] and rate of force development (RFD), and therefore a superior performance during sprinting and jumping tasks [60, 61]. However, the benefits of increased eccentric strength are less clear. During a SSC action, the force produced is heavily dependent on the conditions involved in the eccentric phase [62]. Enhanced force generation during the eccentric phase may result in a greater number of active actin-myosin cross bridges, thus increasing the potential for contractile potentiation during the stretch [62]. Additionally, as muscles increase in size during growth, the higher forces during the eccentric phase may result in an increased potential for storage of elastic energy [8]. More force produced during the eccentric phase may result in the muscle resisting stretch, causing a greater tendinous lengthening [8, 62], and resulting in a more efficient elastic energy storage and reutilisation due to the shorter amortisation periods [63]. The influence of muscle size on the eccentric and concentric phases of the SSC has not been quantified and still needs further research before we can understand how muscle size may influence the underpinning mechanisms of SSC actions. Voluntary strength increases by a larger extent than anthropometric measures in pre-pubertal children [44], indicating that muscle strength depends not only on the muscle mass but also on the extent to which it is activated. This suggests that there are additional structural and neuromuscular qualities that develop throughout biological maturation that drive increased force production as children transition to adults.

2.3 Muscle Architecture

Different muscles have distinct functions about each articulation, with each muscle group being of a specific design for their optimised performance [64]. The architectural arrangement of fibres within the muscle is important because it has implications for muscle function [65], particularly the fascicle's force-length and force-velocity characteristics [66, 67]. There is substantial variability in measurements between distal, central and proximal aspects of a muscle that reflect the heterogeneity of pennate muscles, making direct comparisons between specific muscle groups difficult [27]. Whilst increases in muscle CSA directly correlate with force output increases during growth, changes in the specific architecture of the muscle may play a large role in strength gains as children transition towards adulthood. Despite these conceptions, there is a surprising dearth of evidence that has specifically investigated alterations in muscle architecture as a result of growth and development.

2.3.1 Fascicle Length

Fascicle length likely impacts muscle function by influencing the shortening velocity of a muscle. Longer fascicles result in an improved ability to produce force at higher velocities and over larger length ranges [68]. While there is limited research in human subjects, the relationship between fascicle length and shortening velocity has been investigated in animal models. Analysis of the feline semitendinosus demonstrated that the longer fascicles exhibited by the distal head resulted in a significantly faster shortening velocity than the proximal head [69]. In human subjects, trained sprinters have longer muscle fascicles than endurance runners [70], which highlight the importance of fascicle length for shortening velocity and explosive force production.

Fascicle length of the lower limb muscles are usually longer in men and women in comparison to boys and girls, respectively [27, 28, 34, 39]. Furthermore, 15-year-old adolescents have significantly longer muscle fascicles than children, but do not differ from adults [28]. This may imply that fascicle length reaches adult levels by the approximate age of 15 years; however, more research is needed before any substantial claims are made about the growth rates of tendon structures throughout adolescence. As longer fascicles allow for greater absolute maximum shortening velocities, these findings help explain significantly slower contraction velocities in boys compared with men [71]. Interestingly, involuntary muscle action responses, measured via supramaximal electrical stimulations, do not appear to change throughout maturation [72], which suggests that increases in fascicle length during this period would allow for the production of higher forces at similar contraction speeds, likely a result of more in-series contractile elements working simultaneously [68]. Nevertheless, longer fascicles should have a positive influence on the RFD. Gastrocnemius fascicle length was found to be a positive predictor of RFD during a countermovement jump in adults [73] and may highlight the potential for improved SSC function throughout childhood and adolescence, should greater fascicle lengths increase their ability to develop force rapidly. Moreover, the ability to develop force rapidly may ultimately enhance SSC performance by reducing ground contact times, leading to an improved mechanical efficiency by the reutilisation of elastic energy [63]. Additionally, shorter contact times could influence the impact neural potentiation has on the subsequent concentric action, as longer transition times between the eccentric and concentric contraction causes a decay in the magnitude of potentiation [74]. Increased RFD may also reduce yielding upon ground contact, enabling a greater overall system stiffness, which has established links with SSC-related jumping and sprinting performance [75].

2.3.2 Pennation Angle

Alterations in pennation angle throughout biological maturation appear to be muscle and site specific. The pennation angle of the knee extensor muscles seems to remain consistent from childhood through to adulthood [27, 28], whereas the pennation angle of the gastrocnemius medialis has been reported to increase from birth before becoming stable following the adolescent growth spurt [29, 76, 77], which might suggest that relative muscle growth to bone growth underlies differences in pennation adaptions in given limb segments. An increase in pennation angle throughout maturation might be expected to improve the force-generating capabilities of a muscle [57], and therefore improve the function of the SSC. For a given muscle volume, a larger pennation angle will increase the PCSA [78], which would result in a greater number of contractile elements attaching to the aponeurosis or tendon for a greater force transfer [79].

Fascicle pennation not only influences strength by enabling a greater PCSA, but it is functionally important as an increase in pennation (in conjunction with muscle thickening) during a contraction means that fascicles do not need to shorten as much overall, permitting slower fascicle velocities in relation to whole muscle or MTU velocities in a process known as *gearing* [67]. By enabling the muscle to (a) operate on a more optimal region of its force-velocity curve and (b) work at a favourable region of its forcelength curve over a longer period, this maximises the force that the muscle can develop, without impacting on the capacity for rapid movement production [80]. Intuitively, a greater resting pennation would result in a higher gearing ratio, facilitating the muscle to take advantage of the forcevelocity relationship during the SSC action. This would allow an individual to produce either more force at the same velocities, or greater velocities at similar forces.

Finally, a larger pennation angle may result in a greater passive resistance and therefore increased stiffness during SSC activities [73, 81]. Subjects with highly pennate muscles have greater early RFD during drop jumps, attributed to having an enhanced ability to cope with eccentric loads [54]. It has been hypothesized that because of the indirect line of pull of pennate muscles, a highly pennate muscle will have an increased ability to resist external forces [73], as the direct tendon force acting on the muscle are dissipated along the aponeurosis. An increased stiffness upon landing could lead to shorter ground contact times and therefore a better reutilisation of elastic energy [63]. Consequently, increases in pennation angle throughout maturation results in superior SSC performance through greater *gearing* and more force due to exploitation of both the force–velocity and length–tension relationships, in addition to the greater number of muscle fibres inserting to the aponeurosis [68], resulting in greater force being transferred to the skeleton. Additionally, a greater ability to cope with the high eccentric loads during SSC activities may result in greater RFD in these specific muscle actions [54].

2.4 Tendon

Tendons are interposed between muscles and bones to form an MTU that transmits muscular forces directly to the bone, creating movement or stability around a joint. Tendons are predominantly composed of collagen fibrils which are arranged in a number of hierarchical structures [82] and oriented with the line of force transmission [83]. With the progression in technology, researchers have a better understanding of the three-dimensional fibriller structure of the tendon, which also includes horizontally and transversely oriented collagen fibrils forming spirals and plaits [84]. This complex biological structure and the fact that tendons are fibroelastic in nature, permits tendons to withstand heavy forces whilst maintaining its structural integrity, allowing the transfer of force between the muscle and bone to occur with minimal dispersion of energy [85]. The tendon plays a key role in SSC function, and the action of the MTU as a whole will differ from what happens to the muscle fascicles and tendon individually, influencing both force output and economy [86].

2.4.1 Tendon Dimensional and Material Properties

Tendon development throughout childhood and adolescence involves both dimensional and material adaptations [28, 30, 31, 33]. The specific dimensions of the tendon has a large influence on its function. For example, long, thin tendons are more compliant [87] and can be described as force amplifiers, which take advantage of the tendon's ability to store and reuse elastic energy (the amount of energy stored is directly proportional to its extension). In contrast, short, thick tendons are stiffer [87] and are more effective at transferring muscular forces to bone due to their resistance to being stretched, hence their association with greater RFD and reduced electro-mechanical delay (EMD; the delay between muscle activation and the onset of force production [97]). Based on Hookean law, thicker tendons (greater CSA) are associated with higher stiffness as more spring-like material is arranged in parallel, whereas longer tendons are associated with lower stiffness as more spring-like tissue is arranged in series [88].

Therefore, the specific dimensions of the tendon could either result in a more economical SSC action (due to reutilisation of the elastic energy and the muscle having to perform less work), or increase speed of movement due to a faster transference of force from the working muscle to the bone.

Patella tendon length is significantly shorter in elementary school boys (~ 11 years) than in junior school boys (~ 14 years) and adult males, whilst patellar tendon CSA increased in size across all age groups [33], indicating a difference in the temporal growth of the tendon dimensions. However, both the length and CSA of the Achilles tendon were similar between the 14-year-olds and adults, and significantly greater than 11-year-olds, suggesting that these variables may become stable in boys around 14 years of age [32]. A dimensional bias underpinning the age-related increases in Achilles tendon stiffness between prepubertal children and adults evidences this reported effect [30]. Specifically, both tendon length and CSA were shown to increase by \sim 53 and \sim 93%, respectively, between 5- to 7-year-old children and adults, suggesting that the greater increase in CSA as opposed to tendon length would result in an increase in tendon stiffness [30]. Based on these data, tendon hypertrophy is likely a major adaptation influencing tendon stiffness and possible consequence of chronic loading through increased body mass and force production with age.

The internal properties of the tendon also play a role in stiffness properties. Young's modulus is a dimensionless measure of a material's stiffness and provides an indication of the underlying microstructure. It has been shown to increase with age [27, 28, 30, 33] and these internal adaptations play a role in the increased tendon stiffness reported throughout maturation. Increases in Young's modulus are due to increases in collagen fibril diameter and density [89], alongside greater intra-fibrillar cross-linking [90], that are driven by the increases in tendon loading throughout maturation.

2.4.2 Tendon Stiffness

A tendon's stiffness describes its resistance to elongation when a muscular force is applied. Stiffness of the patellar and Achilles tendon, and vastus lateralis aponeurosis have been shown to be stiffer in adults than in children [28, 30, 31, 34]. Furthermore, the stiffness of both the patellar and Achilles tendons appear to increase throughout childhood and into adolescence, with lower stiffness values reported in ~10-year-old children than in ~13-year-old children and adults [32, 33]. By age 15 years, the mechanical properties of the knee extensor tendon is similar to adults [28], suggesting that tendon stiffness may reach adult values following the approximate age of peak height velocity (PHV). PHV is a somatic biological maturity indicator, and reflects the maximum acceleration of growth during adolescence, providing a universal landmark to reflect the occurrence of other body dimension velocities within and between individuals [3]. These findings also suggest that differences in SSC ability between adolescent and adult populations may not be a result of tendon stiffness differences. Considering that the tendon is the optimal storage site for elastic energy, the key factor in the overall stiffness of the MTU is that the contractile element is required to be stiffer than the tendon to utilise its elastic storage potential. If this is not the case, the muscle could yield under load instead of the tendon, resulting in a sub-optimal muscle mechanics to produce force. Therefore, it could be postulated that adolescents do not have the ability to create this optimal muscle stiffness through the correct muscle activation strategies or motor unit recruitment [35].

Increases in body and muscle mass with growth and development result in an increased loading of the tendons [1]. Combined, body mass and force production has been shown to account for up to 78% of tendon stiffness variation in children and adults [30], demonstrating that ageincreases in tendon stiffness are related likely attributable to increased tendon loading from weightbearing tasks and increased plantar-flexor force production capabilities. This additional tendon loading with increases in body mass and force-producing capabilities as children mature likely acts as a stimulus for adaptation, resulting in changes to both tendon dimensions and material properties, which determine stiffness. Therefore, the observed increases in tendon stiffness during childhood and adolescence would appear to be mediated by growth- and maturity-related alterations of the material properties of the MTU [30, 31].

Gender differences in tendon stiffness have revealed inconclusive results. Recent research has demonstrated that males have a greater level of stiffness than females in both the patellar [91, 92] and Achilles tendon [93]. Previous research has suggested that gender differences may partly be due to differences in tendon dimensions [91]. Prior to adjusting for dimensions, tendon stiffness has been shown to be 115% greater in males than in females [91], whereas after adjusting for tendon size and CSA (Young's modulus), the difference between males and females decreased to 53% [91]. There is, however, evidence to suggest that there are no differences in tendon stiffness between boys and girls, and women and men [31]; these authors suggested that the contrast in findings may be due to methodological differences when quantifying tendon stiffness. Interestingly, while no differences were identified in absolute tendon stiffness between adult males and females [31], the mechanisms underpinning tendon stiffness

increases between childhood and adulthood may differ between sexes [31]. In males, increased stiffness appears to be modulated by the material properties of the tendon (i.e. Young's modulus, a dimensionless measure of a materials stiffness), as the relative increase in tendon length and CSA have been shown to be approximately equal [31]. This would result in these two dimensions negating one another, demonstrating that the alterations to tendon dimensions would not affect stiffness. However, in adult females, tendon CSA increased by a greater amount than tendon length [31], suggesting that natural adaptation in tendon stiffness in females is due to both tendon hypertrophic responses and increases in Young's modulus. These potential sex differences in the mechanisms of tendon development have not been reported in other studies, but provide an interesting rationale to explore the interacting effects of sex and maturation on mechanical properties of the tendon. Before making conclusive statements about gender differences in tendon stiffness, further research is needed in this area.

Tendon stiffness may affect functional movement by enhancing efficient transfer of force to the skeleton [94] influencing the RFD, an important determinant of force production characteristics [95]. A number of studies have reported that children have a reduced RFD relative to adults [43, 71, 72], which may partly be explained by the lower stiffness of the tendinous structures [96]. Additionally, EMD has been shown to influence the rapid generation of muscular force [98–100]. Children exhibit a longer EMD than adults [43, 71, 72] and EMD decreases as a child's neuromuscular system matures [96]. Moreover, tendon stiffness is negatively correlated with EMD in children [96] and could help explain improvements in rapid force production ability as children age; certainly, such enhancements should improve SSC function with maturation. In contrast, in adults, a more compliant tendon has been shown to have a greater ability to store and reutilise elastic energy under the same loading conditions [101–103]. Throughout maturation, while tendon stiffness increases, tendon strain (a tendon's displacement with respect to its resting length) does not change between childhood and adulthood [30, 33], and the increase in stiffness with maturation is likely due to the ability of the tendon to withstand greater force production, rather than reducing the displacement of the tendon [30, 33]. Conceptually, reutilisation of elastic energy and tendon stiffness may develop independently of each other; however, this has not been established, and further research is needed to examine changes in tendon properties and their influence on elastic energy reutilisation during maturation. Additionally, a stiffer MTU has been shown to elicit a greater stretch reflex in children [25], which would lead to shorter

breaking phases and reduced contact times as well as greater electromyographic (EMG) activity [23].

3 Neuromuscular Adaptations as a Result of Growth and Maturation

While the mechanical properties of the muscle and tendon will have a significant role in the regulation of the SSC, it is the interaction of the muscular and neural system that governs SSC performance [6, 8]. Similar to alterations in MTU structure, neural adaptations throughout childhood and adolescence will have a significant impact on the ability to regulate the SSC [22]. For example, a reduced RFD in children is partly caused by a greater agonist–antagonist co-contraction [25, 44], reduced ability to recruit high-threshold type II motor units [43, 71, 104] and lower muscle activation rates [43, 44], highlighting the importance of the neuromuscular system for explosive force production during SSC [35].

3.1 Motor Unit Recruitment

The disparity in strength between children and adults, even when normalized to body size, has been attributed to children's inability to activate their muscles to the same extent as adults [35]. In fact, children recruit a smaller percentage of their total motor-unit pool than adults during voluntary contractions [44, 105]. Using twitch interpolation techniques during maximal voluntary efforts to gauge the percentage of activated muscle, lower motor-unit activation was found in boys than in men (78 vs. 95%) during knee extension exercise [106]. Furthermore, motor-unit activation deficits seem to decrease with age [44, 107]. Considering that high threshold type II motor units have a larger twitch force, faster contraction speeds and rapid conduction velocities [108], researchers have hypothesised that it is a specific inability to recruit or utilise these motor units that limit a child's force production capabilities [104]. Recently, it has been reported that boys have a higher EMG threshold, suggesting a delayed and lesser utilisation of type II motor units in progressive exercise compared with men [109]. Considering the difference between a child's and adult's ability to recruit high threshold motor units, it is postulated that children become more adept at recruiting high-threshold motor units as their central nervous system matures, which will lead to improvements in their ability to produce rapid force during SSC activities.

3.2 Co-Contraction

Co-contraction is the simultaneous contraction of agonist and antagonist muscles around a joint [26] and provides joint stability. Children demonstrate greater co-contraction than adults [25, 44], which decreases with age [110]. Surface EMG analysis of the tibialis anterior and triceps surae musculature during quick-release movements at different levels of sub-maximal contractions revealed that cocontraction of the tibialis anterior was greater in younger participants [25]. Co-contraction can help provide joint stability, but greater antagonistic co-contraction will also increase the agonistic muscle energy cost of exercise [111] and reduce net force output [1]. Aberrant co-contraction neural factors likely result in less efficient movement and proprioception. When the magnitude or velocity of muscular contraction during SSC activities exposes the MTU to excessive tensile forces or rapid changes in length, the Golgi tendon organs increase afferent activity, thereby inhibiting the motor neurons innervating the agonist muscle and facilitating the antagonist motor units [112], reducing the overall efficiency of the SSC action by increasing ground contact times and reducing force output. A greater density and size of Golgi tendon organs is noted in children than in adults [113], but these undergo a process of desensitisation during maturation. Therefore, the process of reduced co-contraction throughout maturation will decrease agonist inhibition, resulting in a more efficient SSC action, as net force around each force would be higher. Reduced co-contraction may enable an increased pre-stretch of the muscle during the eccentric phase of the SSC [113], which would have positive effects on elastic energy reutilisation, stretch reflex response and neural potentiation [7].

3.3 Preactivation

Preactivation is used to describe levels of muscle activity prior to an impact or landing [114]. This neuromuscular strategy has predominantly been measured during bilateral hopping tasks and has been defined as the muscle activation in the 50–100 ms prior to ground contact [115]. When performing two-legged hopping at a slow frequency, boys and men display similar muscle activation strategies; however, children display significantly lower preactivation at faster frequencies [116]. Similar results were reported during a 20 cm drop jump task, with children displaying significantly less preactivation than adults [23]. This reduced ability to utilise feed-forward mechanisms results in children producing longer ground contact times during hopping [116], which results in sub-optimal SSC function. Research shows that these neural mechanisms adapt with age, demonstrated by the fact that 15-year-old children produce significantly greater levels of pre-activity than 9 and 12 year olds during maximal hopping [22]. This trend could be stimulated by the greater drop heights and landing velocities that are evident in older children during hopping tasks. Due to the association between increased preactivation and increased muscle stiffness [117], the reduced feed-forward activity in younger children reflects a protective mechanism, aiming to prevent excessive rapid overload of the MTU upon ground contact. During maturation, SSC performance may improve as children transition from a reactive regulation of movement to a more preactive control of movement, reflected by an increased reliance on preactivation prior to ground contact [22].

A greater muscle activation prior to ground contact may reduce EMD, as force can be immediately generated upon ground contact. However, the relationships between preactivation, EMD and the subsequent RFD during dynamic activity have yet to be established and further research is required to identify how muscle activation strategies could influence rapid force production in children. In addition, greater background muscle activity and short latency reflexes would dictate increased muscle activity during the eccentric phase of SSC, which will augment the interaction effects of the contractile and elastic elements and the storage and utilisation of elastic energy by reducing fascicle stretch and promoting length change in the tendinous structures.

3.4 Reflex Control

The mean EMG from 30 to 60 ms, 60 to 90 ms and 90 to 120 ms after landing or impact is used to represent short-, medium- and long-latency stretch reflex components, respectively [114]. The short-latency reflex reflects the spinal involuntary command to activate the muscle during the 30-60 ms time phase of ground contact [115], whilst the medium- and long-latency reflex allows for supraspinal input [114]. Stretch reflex activity has been shown to improve with age in pre-pubertal boys and girls [24]. However, the researchers used protocols that involved isolated joint actions and an artificial stimulus to invoke the twitch response, which fails to elicit sufficient tension modifications to activate Golgi tendon organs and bypasses muscle spindle activation [116]. When using a SSC task to quantify the stretch reflex, researchers have found that the reflex amplitude is reduced in children compared with adults during a drop jump task [23]. Additionally, children have a greater reliance on longer-latency stretch reflexes during repeated hopping-in-place [22, 116]; however, as they transition through to adolescence, they appear to become more adept at regulating lower-limb stiffness through a greater utilisation of short-latency stretch reflexes [22]. Improved spindle sensitivity, maturation of the sensorimotor pathways, and increased stiffness within the MTU have been suggested as potential explanatory mechanisms [24]. A larger stretch reflex would result in greater EMG activity, allowing greater force to be produced in SSC actions. Furthermore, considering that MTU stiffness is regulated by the amplitude and timing of the stretch reflex, a greater reliance on the short-latency stretch reflex, evident as a child matures, would allow greater stiffness upon landing, positively influencing the SSC [75]. Increased stiffness upon landing will lead to shorter ground contact times and therefore a better reutilisation of elastic energy [63]. Additionally, a stiffer MTU may elicit a greater stretch reflex in children [25], resulting in shorter breaking phases and reduced contact times.

3.5 Rate of EMG Rise

The rate that EMG increases with contraction, represented by the initial slope of the rectified EMG curve, usually calculated over the first 30 ms of muscle activation, characterises the initial rate of muscle activation [118]. Research has demonstrated that the rate of muscle activation determines the subsequent RFD [119]. Children display significantly lower rates of EMG increase than adults [43, 96], which has been related to reduced RFD [96], suggesting that the lower rates of muscle activation negatively influences their ability to produce force rapidly. This may be due to differential motor-unit recruitment or differential rate coding of the higher-threshold type II motor units [35, 109]. Depolarising potentials are greater in amplitude for larger motor units [120]; thus, individuals who are able to recruit high-threshold motor units earlier should display a steeper rate of EMG increase, which should correspond to a heightened RFD. Theoretically, improvements in children's ability to recruit higherthreshold motor units with maturation should translate to an escalation in the rate of EMG increase, resulting in an improved ability to produce force rapidly during the SSC.

4 Trainability of Stretch-Shortening Cycle Function

A growing number of studies have examined the effects of training on SSC ability in youth, typically using a range of jump protocols to quantify indirect measures of SSC function [121]. A number of studies have demonstrated positive effects of plyometric training [122–132], traditional strength training [133–137], and combined plyometric and strength training [138, 139] on jump performance in both children and adolescents. Furthermore, recent meta-analytical data have demonstrated that various forms of resistance training can improve measures of SSC function in youth [140, 141]. From these data, plyometric training has been proven to elicit a larger overall effect on vertical jump height than interventions consisting solely of resistance training, or a combination of

strength training and plyometric/speed training [141]. Research shows that the effectiveness of certain training interventions to enhance jumping performance in boys is influenced by maturation [142]. There is evidence to suggest that pre-PHV boys benefit more from plyometric training, while boys who are post-PHV respond more favourably to a combined training intervention, inclusive of both plyometric and traditional strength training exercise [142]. These maturity-dependent responses may be indicative of 'synergistic adaptation', which refers to the symbiotic relationship between specific adaptations of an imposed training demand and concomitant growth and maturity-related adaptations [142].

There is a significant lack of research exploring the training-induced improvements in SSC function in youth. However, research has determined the positive effect plyometric training has on motor unit recruitment, contraction velocity, excitability of soleus muscle short latency stretch reflexes and muscle activation strategies in adults [143–146]. In an adult population, research has demonstrated that an 8-week plyometric training programme results in significant increases in peak force and maximal contraction velocity in type I, type IIa and type IIb/IIx muscle fibres [146]. Similarly, a 4-week plyometric training programme was sufficient to elicit a positive training effect on the excitability of the soleus short-latency stretch reflex [145]. Plyometric training has also produced significant improvements in adductor muscle activation during the preparatory phase (150 ms prior to ground contact) during drop jump performance [144]. These studies highlight the potential effects that plyometrics have on mechanistic adaptation to muscle activation strategies in adults; however, whether the same adaptation can hold true for children and adolescents remains unclear. It may be possible to infer that the improvements in SSC function from plyometric training in children and adolescents is due to increased motor unit activation, contraction velocity, preactivation and a greater reliance on the short-latency stretch reflex, resulting in a more feed-forward SSC function.

Traditional strength training may also result in greater motor-unit activation [147, 148], resulting in positive effects on SSC function; however, this form of training is commonly linked with structural and architectural changes to the MTU. While there is a scarcity of research investigating the effects of training on muscle architecture in children and adolescents, many studies have found that resistance training alters aspects of muscle architecture in adults, specifically causing increases in muscle fascicle length [149–154], pennation angle [79, 150, 155, 156] and PCSA [79, 151]. However, it is unclear whether training will have the same effects on children and adolescents, and more research is required to understand the training-induced adaptations.

Recently, the effects of traditional strength training on the mechanical properties of the Achilles tendon have been shown to increase in stiffness following 10 weeks of twiceweekly resistance training in previously untrained pre-pubertal children [157]. This increase in tendon stiffness seems to occur due to changes to the internal properties of the tendon, as no changes to tendon CSA were found [157]. This suggests that a higher loading intensity or a greater duration of training may be required to elicit significant tendon hypertrophy. While this increase in tendon stiffness also resulted in a decreased EMD, changes to the rate of EMG rise and RFD did not occur, indicating that the magnitude of improvement in tendon stiffness ($\sim 29\%$), was not sufficient enough to alter these qualities [157]. Potentially, longer or more intensive training periods may yield more favourable results with respect to RFD adaptations resulting directly from greater increases in tendon stiffness.

5 Conclusions

As children transition towards adulthood they demonstrate natural improvements in their ability to perform hopping and jumping tasks. Children display increases in muscle volume, fascicle length and fascicle pennation in many muscles as they mature. Additionally, tendon dimensions and mechanical properties develop with age-related body mass and force production increases, influencing its stiffness. At younger ages, the natural regulation of movement is more reactive in nature, transitioning to a more preactive control of movement as children improve their neuromuscular capacity as they age. Additionally, agonist-antagonist co-contraction may reduce as children age, stemming from a desensitisation of the Golgi tendon organs, resulting in a greater net force output. Increases in tendon stiffness, motor-unit recruitment and preactivation, and reduced cocontraction should impart a positive effect on force production characteristics and SSC function. With age and maturation, adaptations to the MTU and neuromuscular system enhance the rapid force-producing potential and result in better utilisation of the underpinning mechanisms of the SSC, resulting in an improved SSC function. Through training, SSC function seems to improve in children; however, the specific mechanisms that underpin these improvements are unclear, and further research is required to better understand the structural and neural adaptations that occur through training that lead to improved SSC function. Longitudinal studies, where key indicators of growth (size attained, rate of growth) and maturation (sexual, skeletal, age at PHV) are measured alongside SSC actions, are needed to provide more evidence into the natural development of the SSC throughout childhood and into adolescence.

Compliance with Ethical Standards

Funding No sources of funding were used to assist in the preparation of this article. Gregory Myer would like to acknowledge funding support from National Institutes of Health Grants.

Conflict of interest John Radnor, Jon Oliver, Isabel Moore, Charlie Waugh and Rhodri Lloyd declare that they have no conflicts of interest relevant to the content of this review. Gregory Myer would like to declare that he receives book royalties on topics related to the manuscript.

Open Access This article is distributed under the terms of the Creative Commons Attribution 4.0 International License (http://creativecommons.org/licenses/by/4.0/), which permits unrestricted use, distribution, and reproduction in any medium, provided you give appropriate credit to the original author(s) and the source, provide a link to the Creative Commons license, and indicate if changes were made.

References

- Malina RM, Bouchard C, Bar-Or O. Growth, maturation and physical activity. 2nd ed. Champaign: Human Kinetics; 2004.
- Beunen G, Malina RM. Growth and biologic maturation: relevance to athletic performance. In: Bar-Or O, Hebestreit H, editors. The child and adolescent athlete. Oxford: Blackwell Publishing; 2005. p. 3–17.
- Mirwald RL, Baxter-Jones AD, Bailey DA, Beunen GP. An assessment of maturity from anthropometric measurements. Med Sci Sports Exerc. 2002;34:689–94.
- Payne S, Townsend N, Foster C. The physical activity profile of active children in England. Int J Behav Nutr Phys Act. 2013;10:136.
- Lloyd RS, Oliver JL, Faigenbaum AD, Howard R, De Ste Croix MBA, Williams CA, et al. Long-term athletic development, part 2: barriers to success and potential solutions. J Strength Cond Res. 2015;29:1451–64.
- Nicol C, Avela J, Komi P. The stretch-shortening cycle: a model to study naturally occurring neuromuscular fatigue. Sports Med. 2006;36:977–99.
- 7. Flanagan EP, Comyns TM. The use of contact time and the reactive strength index to optimize fast stretch-shortening cycle training. Strength Cond J. 2008;30:32–8.
- Komi PVP. Stretch-shortening cycle: a powerful model to study normal and fatigued muscle. J Biomech. 2000;33:1197–206.
- Bosco C, Viitasalo J, Komi P, Luthanen P. Combined effect of elastic energy and myoelectrical potentiation during stretchshortening cycle exercise. Acta Physiol Scand. 1982;114:557–65.
- Bosco C, Montanari G, Tarakka I, Latteri F, Cozzi M, Iachelli G, et al. The effect of pre-stretch on mechanical efficiency of human skeletal muscle. Acta Physiol Scand. 1987;131:323–9.
- Lloyd RS, Oliver JL, Hughes MG, Williams CA. Reliability and validity of field-based measures of leg stiffness and reactive strength index in youths. J Sports Sci. 2009;27:1565–73.
- Schmidtbleicher D. Training for power events. In: Komi PV, editor. Strength and power in sport. Encyclopaedia of sports medicine, vol. 3. Oxford: Blackwell; 1992. p. 169–79.

- Turner AN, Jeffreys I. The stretch-shortening cycle: proposed mechanisms and methods for enhancement. Strength Cond J. 2010;32:87–99.
- Walshe AD, Wilson GJ, Ettema GJ. Stretch-shorten cycle compared with isometric preload: contributions to enhanced muscular performance. J Appl Physiol. 1998;84(1):97–106.
- Van Schenau GJI, Bobbert MF, De Haan A. Mechanics and energetics of the stretch-shortening cycle: a stimulating discussion. J Appl Biomech. 1997;13:484–96.
- Komi PV, Bosco C. Utilization of stored elastic energy in leg extensor muscles by men and women. Med Sci Sport. 1978;10:261–5.
- Komi PV, Gollhofer A. Stretch reflexes can have an important role in force enhancement during SSC exercise. J Appl Biomech. 1997;33:1197–206.
- Laffaye G, Choukou M, Benguigui N, Padulo J. Age- and gender-related development of stretch shortening cycle during a sub-maximal hopping task. Biol Sport. 2016;33:29–35.
- Lloyd R, Oliver J, Hughes M, Williams C. The influence of chronological age on periods of accelerated adaptation of stretch-shortening cycle performance in pre and postpubescent boys. J Strength Cond Res. 2011;25:1889–97.
- Lichtwark GA, Wilson AM. Optimal muscle fascicle length and tendon stiffness for maximising gastrocnemius efficiency during human walking and running. J Theor Biol. 2008;252:662–73.
- Lichtwark G, Wilson A. Is Achilles tendon compliance optimised for maximum muscle efficiency during locomotion? J Biomech. 2007;40:1768–75.
- Lloyd RS, Oliver JL, Hughes MG, Williams CA. Age-related differences in the neural regulation of stretch-shortening cycle activities in male youths during maximal and sub-maximal hopping. J Electromyogr Kinesiol. 2012;22:37–43.
- Lazaridis S, Bassa E, Patikas D, Giakas G, Gollhofer A, Kotzamanidis C. Neuromuscular differences between prepubescents boys and adult men during drop jump. Eur J Appl Physiol. 2010;110:67–74.
- Grosset J-F, Mora I, Lambertz D, Pérot C. Changes in stretch reflexes and muscle stiffness with age in prepubescent children. J Appl Physiol. 2007;102:2352–60.
- Lambertz D, Mora I, Grosset J-F, Perot C. Evaluation of musculotendinous stiffness in prepubertal children and adults, taking into account muscle activity. J Appl Physiol. 2003;95:64–72.
- Croce R, Russell P, Swartz E, Decoster L. Knee muscular response strategies differ by developmental level but not gender during jump landing. Electromyogr Clin Neurophysiol. 2004;44:339–48.
- O'Brien TD, Reeves ND, Baltzopoulos V, Jones DA, Maganaris CN. Muscle-tendon structure and dimensions in adults and children. J Anat. 2010;216:631–42.
- Kubo K, Kanehisa H, Kawakami Y, Fukanaga T. Growth changes in the elastic properties of human tendon structures. Int J Sports Med. 2001;22:138–43.
- 29. Binzoni T, Bianchi S, Hanquinet S, Kaelin A, Sayegh Y, Dumont M, et al. Human gastrocnemius medialis pennation angle as a function of age: from newborn to the elderly. J Physiol Anthr Appl Hum Sci. 2001;20:293–8.
- Waugh CM, Blazevich A, Fath F, Korff T. Age-related changes in mechanical properties of the Achilles tendon. J Anat. 2012;220:144–55.
- O'Brien TD, Reeves ND, Baltzopoulos V, Jones DA, Maganaris CN. Mechanical properties of the patellar tendon in adults and children. J Biomech. 2010;43:1190–5.
- Kubo K, Teshima T, Hirose N, Tsunoda N. A cross-sectional study of the plantar flexor muscle and tendon during growth. Int J Sports Med. 2014;35:828–34.

- 33. Kubo K, Teshima T, Hirose N, Tsunoda N. Growth changes in morphological and mechanical properties of human patellar tendon in vivo. J Appl Biomech. 2014;30:415–22.
- Kubo K, Teshima T, Ikebukuro T, Hirose N, Tsunoda N. Tendon properties and muscle architecture for knee extensors and plantar flexors in boys and men. Clin Biomech. 2014;29:506–11.
- Dotan R, Mitchell C, Cohen R, Klentrou P, Gabriel D, Bareket F. Child-adult differences in muscle activation—a review. Clin Neurophysiol. 2012;123:106–16.
- 36. Lexell J, Sjöström M, Nordlund A, Taylor C. Growth and development of human muscle: a quantitative morphological study of whole vastus lateralis from childhood to adult age. Muscle Nerve. 1992;15:404–9.
- Bell RD, MacDougall JD, Billeter R, Howald H. Muscle fiber types and morphometric analysis of skeletal muscle in six-yearold children. Med Sci Sport Exerc. 1980;12:28–31.
- Bottinelli R, Canepari M, Pellegrino MA, Reggiani C. Forcevelocity properties of human skeletal muscle fibres: myosin heavy chain isoform and temperature dependence. J Physiol. 1996;495:573–86.
- O'Brien TD, Reeves ND, Baltzopoulos V, Jones DA, Maganaris CN. In vivo measurements of muscle specific tension in adults and children. Exp Physiol. 2010;95:202–10.
- Folland JP, Williams AG. The adaptations to strength training: morphological and neurological contributions to increased strength. Sports Med. 2007;37(2):145–68.
- 41. Jones EJ, Bishop PA, Woods AK, Green JM. Cross-sectional area and muscular strength: a brief review. Sports Med. 2008;38:987–94.
- 42. Tonson A, Ratel S, Le Fur Y, Cozzone P, Bendahan D. Effect of maturation on the relationship between muscle size and force production. Med Sci Sports Exerc. 2008;40:918–25.
- 43. Falk B, Usselman C, Dotan R, Brunton L, Klentrou P, Shaw J, et al. Child-adult differences in muscle strength and activation pattern during isometric elbow flexion and extension. Appl Physiol Nutr Metab. 2009;34:609–15.
- 44. Grosset JF, Mora I, Lambertz D, Pérot C. Voluntary activation of the triceps surae in prepubertal children. J Electromyogr Kinesiol. 2008;18:455–65.
- 45. De Ste Croix MBA, Armstrong N, Welsman JR. Concentric isokinetic leg strength in pre-teen, teenage and adult males and females. Biol Sport. 1999;16:75–86.
- 46. O'Brien TD, Reeves ND, Baltzopoulos V, Jones DA, Maganaris CN. Strong relationships exist between muscle volume, joint power and whole-body external mechanical power in adults and children. Exp Physiol. 2009;94:731–8.
- 47. Kubo K, Ikebukuro T, Yata H. Time course of changes in muscle and tendon properties during strength training and detraining. J Strength Cond Res. 2010;24(2):322–31.
- Kubo K, Ikebukuro T, Yata H, Tsunoda N, Kanehisa H. Effects of training on muscle and tendon in knee extensors and plantar flexors in vivo. J Appl Biomech. 2010;26:316–23.
- 49. Kubo K, Kanehisa H, Azuma K, Ishizu M, Kuno S-Y, Okada M, et al. Muscle architectural characteristics in women aged 20-79 years. Med Sci Sports Exerc. 2003;35:39–44.
- Blazevich A, Gill N, Zhou S. Intra and intermuscular variation in human quadriceps femoris architecture assessed in vivo. J Anat. 2006;209:289–310.
- 51. Blazevich AJ, Gill ND, Bronks R, Newton RU. Trainingspecific muscle architecture adaptation after 5-wk training in athletes. Med Sci Sports Exerc. 2003;35:2013–22.
- 52. Secomb J, Lundgren L, Farley O, Tran T, Nimphius S, Sheppard J. Relationships between lower-body muscle structure and lower-body strength, power, and muscle-tendon complex stiffness. J Strength Cond Res. 2015;29:2221–8.

- 53. Secomb JL, Farley ORL, Lundgren L, Tran TT, King A, Sheppard JM, et al. Associations between the performance of scoring manoeuvres and lower-body strength and power in elite surfers. Int J Sports Sci Coach. 2015;10:911–8.
- 54. Earp JE, Kraemer WJ, Cormie P, Volek JS, Maresh CM, Joseph M, et al. Influence of muscle-tendon unit structure on rate of force development during the squat, countermovement, and drop jumps. J Strength Cond Res. 2011;25:340–7.
- Nimphius S, McGuigan MR, Newton RU. Changes in muscle architecture and performance during a competitive season in female softball players. J Strength Cond Res. 2012;26:2655–66.
- Morse CI, Tolfrey K, Thom JM, Vassilopoulos V, Maganaris CN, Narici MV. Gastrocnemius muscle specific force in boys and men. J Appl Physiol. 2008;104:469–74.
- Lieber RL, Fridén J. Functional and clinical significance of skeletal muscle architecture. Muscle Nerve. 2000;23:1647–66.
- Evangelidis PE, Massey GJ, Pain MTG, Folland JP. Strength and size relationships of the quadriceps and hamstrings with special reference to reciprocal muscle balance. Eur J Appl Physiol. 2016;116:593–600.
- Suchomel TJ, Nimphius S, Stone MH. The importance of muscular strength in athletic performance. Sports Med. 2016;46:1419–49.
- Tillin NA, Pain MTG, Folland J. Explosive force production during isometric squats correlates with athletic performance in rugby union players. J Sports Sci. 2013;31:66–76.
- McLellan CP, Lovell DI, Gass GC. The role of rate of force development on vertical jump performance. J Strength Cond Res. 2011;25:379–85.
- 62. Cormie P, McGuigan MR, Newton RU. Changes in the eccentric phase contribute to improved stretch-shorten cycle performance after training. Med Sci Sports Exerc. 2010;42:1731–44.
- Henchoz Y, Malatesta D, Gremion G, Belli A. Effects of the transition time between muscle-tendon stretch and shortening on mechanical efficiency. Eur J Appl Physiol. 2006;96:665–71.
- Lieber RL, Ward SR. Skeletal muscle design to meet functional demands. Philos Trans R Soc B. 2011;366:1466–76.
- Blazevich AJ, Sharp NCC. Understanding muscle architectural adaptation: macro- and micro-level research. Cells Tissues Organs. 2005;181:1–10.
- Azizi E, Brainerd EL, Roberts TJ. Variable gearing in pennate muscles. Proc Natl Acad Sci USA. 2008;105:1745–50.
- Wakeling JM, Blake OM, Wong I, Rana M, Lee SSM. Movement mechanics as a determinate of muscle structure, recruitment and coordination. Philos Trans R Soc Lond B Biol Sci. 2011;366:1554–64.
- Blazevich AJ. Effects of physical training and detraining, immobilisation, growth and aging on human fascicle geometry. Sports Med. 2006;36:1003–17.
- 69. Bodine SC, Roy RR, Meadows DA, Zernicke RF, Sacks RD, Fournier M, et al. Architectural, histochemical, and contractile characteristics of a unique biarticular muscle: the cat semitendinosus. J Neurophysiol. 1982;48:192–201.
- Abe T, Kumagai K, Brechue WF. Fascicle length of leg muscles is greater in sprinters than distance runners. Med Sci Sport Exerc. 2000;32:1125–9.
- Asai H, Aoki J. Force development of dynamic and static contractions in children and adults. Int J Sports Med. 1996;17:170–4.
- Grosset JF, Mora I, Lambertz D, Perot C. Age-related changes in twitch properties of plantar flexor muscles in prepubertal children. Pediatr Res. 2005;58:966–70.
- Earp JE, Kraemer WJ, Newton RU, Comstock BA, Fragala MS, Dunn-Lewis C, et al. Lower-body muscle structure and its role in jump performance during squat, countermovement, and depth drop jumps. J Strength Cond Res. 2010;24:722–9.

- Wilson GJ, Wood GA, Elliott BC. Optimal stiffness of series elastic component in a stretch-shorten cycle activity. J Appl Physiol. 1991;70:825–33.
- Mcmahon JJ, Comfort P, Cscs D, Pearson S. Lower limb stiffness: effect on performance and training considerations. Strength Cond J. 2012;34:94–101.
- Kannas T, Kellis E. Medial gastrocnemius architectural properties during isometric contractions in boys and men. Pediatr Exerc Sci. 2010;22:152–64.
- Kurihara T, Kanehisa H, Abe T. Gastrocnemius muscle architecture and external tendon length in young boys [poster]. J Biomech. 2007;40:S690.
- Fukunaga T, Miyatani M, Tachi M, Kouzaki M, Kawakami Y, Kanehisa H. Muscle volume is a major determinant of joint torque in humans. Acta Physiol Scand. 2001;172:249–55.
- Kawakami Y, Abe T, Kuno SY, Fukunaga T. Training-induced changes in muscle architecture and specific tension. Eur J Appl Physiol Occup Physiol. 1995;72:37–43.
- Askew GN, Marsh RL. Optimal shortening velocity (V/V_{max}) of skeletal muscle during cyclical contractions: length-force effects and velocity-dependent activation and deactivation. J Exp Biol. 1998;201:1527–40.
- Secomb JL, Nimphius S, Farley ORL, Lundgren LE, Tran TT, Sheppard JM. Relationships between lower-body muscle structure and lower-body strength, explosiveness and eccentric leg stiffness in adolescent athletes. J Sports Sci Med. 2015;14:691–7.
- Kastelic J, Galeski A, Baer E. The multicomposite structure of tendon. Connect Res. 1978;6:11–23.
- Kannus P. Structure of the tendon connective tissue. Scand J Med Sci Sport. 2000;10:312–20.
- Jozsa L, Kannus P, Balint J, Reffy A. Three-dimensional infrastructure of human tendons. Cells Tissues Organs. 1991;142:306–12.
- Shadwick RE. Elastic energy storage in tendons: mechanical differences related to function and age. J Appl Physiol. 1990;68:1033–40.
- Ishikawa M, Komi PV. Muscle fascicle and tendon behavior during human locomotion revisited. Exerc Sport Sci Rev. 2008;36:193–9.
- Van Soest A, Huijing P, Solomonow M. The effect of tendon on muscle force in dynamic isometric contractions a simulation study. J Biomech. 1995;28:801–7.
- Proske U, Morgan D. Tendon stiffness: methods of measurement and significance for the control of movement. A review. J Biomech. 1987;20:75–82.
- Bailey AAJ, Paul RGRG, Knott L. Mechanisms of maturation and ageing of collagen. Mech Ageing Dev. 1998;106:1–56.
- 90. Parry D, Barnes G, Craig A. A comparison of the size distribution of collagen fibrils in connective tissues as a function of age and a possible relation between fibril size distribution and mechanical properties. Proc R Soc B Biol Sci. 1978;203:305–21.
- Onambele G, Burgess K, Pearson S. Gender-specific in vivo measurement of the structural and mechanical properties of the human patellar tendon. J Orthop Res. 2007;25:1635–42.
- Hicks KM, Onambele-Pearson GL, Winwood K, Morse CI. Gender differences in fascicular lengthening during eccentric contractions: the role of the patella tendon stiffness. Acta Physiol. 2013;209:235–44.
- Kubo K, Kanehisa H, Fukunaga T. Gender differences in the viscoelastic properties of tendon structures. Eur J Appl Physiol. 2003;88:520–6.
- 94. Wilson A, Lichtwark G. The anatomical arrangement of muscle and tendon enhances limb versatility and locomotor performance. Philos Trans R Soc Lond B Biol Sci. 2011;366:1540–53.

- 95. Bojsen-Møller J, Magnusson SP, Rasmussen LR, Kjaer M, Aagaard P. Muscle performance during maximal isometric and dynamic contractions is influenced by the stiffness of the tendinous structures. J Appl Physiol. 2005;99:986–94.
- Waugh CM, Korff T, Fath F, Blazevich AJ. Rapid force production in children and adults: mechanical and neural contributions. Med Sci Sports Exerc. 2013;45:762–71.
- Norman R, Komi P. Electromechanical delay in skeletal muscle under normal movement conditions. Acta Physiol Scand. 1979;106:241–8.
- Blazevich A, Horne S, Cannavan D, Coleman D, Aagaard P. Effect of contraction mode of slow-speed resistance training on the maximum rate of force development in the human quadriceps. Muscle Nerve. 2008;38:1133–46.
- Pijnappels M, Bobbert MF, Van Dieën JH. How early reactions in the support limb contribute to balance recovery after tripping. J Biomech. 2005;38:627–34.
- Grosset J-FF, Piscione J, Lambertz D, Pérot C. Paired changes in electromechanical delay and musculo-tendinous stiffness after endurance or plyometric training. Eur J Appl Physiol. 2009;105:131–9.
- 101. Kubo K, Morimoto M, Komuro T, Tsunoda N, Kanehisa H, Fukunaga T. Influences of tendon stiffness, joint stiffness, and electromyographic activity on jump performances using single joint. Eur J Appl Physiol. 2007;99:235–43.
- 102. Kubo K, Kawakami Y, Fukunaga T. Influence of elastic properties of tendon structures on jump performance in humans. J Appl Physiol. 1999;87:2090–6.
- 103. Kubo K, Kanehisa H, Fukunaga T. Effects of viscoelastic properties of tendon structures on stretch-shortening cycle exercise in vivo. J Sports Sci. 2005;23:851–60.
- 104. Halin R, Germain P, Bercier S, Kapitaniak B, Buttelli O. Neuromuscular response of young boys versus men during sustained maximal contraction. Med Sci Sports Exerc. 2003;35:1042–8.
- 105. Stackhouse S, Binder-Macleod S, Lee S. Voluntary muscle activation, contractile properties, and fatigability in children with and without cerebral palsy. Muscle Nerve. 2005;31:594–601.
- 106. Blimkie CJ. Age- and sex-associated variation in strength during childhood: anthropometric, morphologic, neurologic, biomechanical, endocrinologic, genetic, and physical activity correlates. In: Gisolfi CV, Lamb D, editors. Perspectives in exercise science and sports medicine. Vol. 2: Youth, exercise and sports. Indianapolis: Benchmark Press; 1989. p. 99–163.
- 107. Belanger AY, McComas AJ. Contractile properties of human skeletal muscle in childhood and adolescence. Eur J Appl Physiol. 1989;58:563–7.
- Sale D. Influence of exercise and training on motor unit activation. Exerc Sport Sci Rev. 1987;15:95–151.
- 109. Pitt B, Dotan R, Millar J, Long D, Tokuno C, O'Brien TD, et al. The electromyographic threshold in boys and men. Eur J Appl Physiol. 2015;115:1273–81.
- Frost G, Dowling J, Dyson K, Bar-Or O. Cocontraction in three age groups of children during treadmill locomotion. J Electromyogr Kinesiol. 1997;7:179–86.
- 111. Frost G, Bar-Or O, Dowling J, Dyson K. Explaining differences in the metabolic cost and efficiency of treadmill locomotion in children. J Sports Sci. 2002;20:451–61.
- 112. Brooks GA, Fahey TD, White TP, Baldwin KM. Exercise physiology: human bioenergetics and its applications. Mountain View: Mayfield Publishing; 2000.
- 113. Ovalle W. The human muscle-tendon junction. A morphological study during normal growth and maturity. Anat Embryol (Berl). 1987;176:281–94.
- 114. Hobara H, Kimura K, Omuro K, Gomi K, Muraoka T, Iso S, et al. Determinants of difference in leg stiffness between

🖄 Springer

endurance- and power-trained athletes. J Biomech. 2008;41:506–14.

- 115. Hobara H, Kanosue K, Suzuki S. Changes in muscle activity with increase in leg stiffness during hopping. Neurosci Lett. 2007;418:55–9.
- Oliver JL, Smith PM. Neural control of leg stiffness during hopping in boys and men. J Electromyogr Kinesiol. 2010;20:973–9.
- 117. Horita T, Komi PV, Nicol C, Kyröläinen H. Interaction between pre-landing activities and stiffness regulation of the knee joint musculoskeletal system in the drop jump: implications to performance. Eur J Appl Physiol. 2002;88:76–84.
- 118. Aagaard P, Simonsen EB, Andersen JL, Magnusson P, Dyhre-Poulsen P, Anderson J, et al. Increased rate of force development and neural drive of human skeletal muscle following resistance training. J Appl Physiol. 2002;93:1318–26.
- Corcos DM, Gottlieb GL, Agarwal GC. Organizing principles for single-joint movements. A speed-sensitive strategy. J Neurophysiol. 1989;62:358–68.
- Milner-Brown H, Stein R. The relation between the surface electromyogram and muscular force. J Physiol. 1975;246:549–69.
- 121. Lloyd R, Oliver J, Hughes M, Williams C. Specificity of test selection for the appropriate assessment of different measures of stretch-shortening cycle function in children. J Sports Med Phys Fit. 2011;51(4):595–602.
- 122. Lloyd RS, Oliver JL, Hughes MG, Williams CA. The effects of 4-weeks of plyometric training on reactive strength index and leg stiffness in male youths. J Strength Cond Res. 2012;26:2812–9.
- 123. Meylan C, Malatesta D. Effects of in-season plyometric training within soccer practice on explosive actions of young players. J Strength Cond Res. 2009;23:2605–13.
- Kotzamanidis C. Effect of plyometric training on running performance and vertical jumping in prepubertal boys. J Strength Cond Res. 2006;20:441–5.
- 125. King JA, Cipriani DJ. Comparing preseason frontal and sagittal plane plyometric programs on vertical jump height in highschool basketball players. J Strength Cond Res. 2010;24:2109–14.
- 126. Matavulj D, Kukolj M, Ugarkovic D, Tihanyi J, Jaric S. Effects of plyometric training on jumping performance in junior basketball players. J Sports Med Phys Fit. 2001;41:159–64.
- 127. Thomas K, French D, Hayes PR. The effect of two plyometric training techniques on muscular power and agility in youth soccer players. J Strength Cond Res. 2009;23:332–5.
- 128. Faigenbaum AD, McFarland JE. Effects of a short-term plyometric and resistance training program on fitness performance in boys age 12 to 15 years. J Sports Sci Med. 2007;6:519–25.
- 129. Zribi A, Zouch M, Chaari H, Bouajina E, Ben Nasr H, Zaouali M, et al. Short-term lower-body plyometric training improves whole-body BMC, bone metabolic markers, and physical fitness in early pubertal male basketball players. Pediatr Exerc Sci. 2014;26:22–32.
- 130. Ramírez-Campillo R, Burgos C, Henriquez-Olguin C, Andrade D, Martínez C, Alvarez C, et al. Effect of unilateral, bilateral, and combined plyometric training on explosive and endurance performance of young soccer players. J Strength Cond Res. 2015;29:1317–28.
- 131. Ramirez-Campillo R, Meylan C, Àlvarez C, Henriquez-Olguibn C, Martinez C, Cañas-Jamett R, et al. Effects of in-season lowvolume high-intensity plyometric training on explosive actions and endurance of young soccer players. J Strength Cond Res. 2014;28:1335–42.
- 132. Ramirez-Campillo R, Meylan C, Àlvarez C, Henriquez-Olguibn C, Martinez C, Andrade DC, et al. The effects off interday rest

on adaptation to 6 weeks of plyometric training in young soccer players. J Strength Cond Res. 2015;29:972–9.

- 133. Chelly MS, Fathloun M, Cherif N. Effects of a back squat training program on leg power, jump, and sprint performances in junior soccer players. J Strength Cond Res. 2009;23:2241–9.
- 134. Coutts AJ, Murphy AJ, Dascombe BJ. Effect of direct supervision of a strength coach on measures of muscular strength and power in young rugby league players. J Strength Cond Res. 2004;18:316–23.
- Christou M, Smilios I, Sotiropoulos K, Volaklis K, Pilianidis T, Tokmakidis SP. Effects of resistance training on the physical capacities of adolescent soccer players. J Strength Cond Res. 2006;20:783–91.
- 136. Gorostiaga EM, Izquierdo M, Ruesta M, Iribarren J, González-Badillo JJ, Ibáñez J. Strength training effects on physical performance and serum hormones in young soccer players. Eur J Appl Physiol. 2004;91:698–707.
- 137. Gorostiaga EM, Izquierdo M, Iturralde P, Ruesta M, Ibáñez J. Effects of heavy resistance training on maximal and explosive force production, endurance and serum hormones in adolescent handball players. Eur J Appl Physiol Occup Physiol. 1999;80:485–93.
- 138. Wong P, Chamari K, Wisløff U. Effects of 12-week on-field combined strength and power training on physical performance among U-14 young soccer players. J Strength Cond Res. 2010;24:644–52.
- 139. Maio Alves JMV, Rebelo AN, Abrantes C, Sampaio J. Shortterm effects of complex and contrast training in soccer players' vertical jump, sprint, and agility abilities. J Strength Cond Res. 2010;24:936–41.
- 140. Behringer M, Vom Heede A, Matthews M, Mester J. Effects of strength training on motor performance skills in children and adolescents: a meta-analysis. Pediatr Exerc Sci. 2011;23:186–206.
- 141. Harries SK, Lubans DR, Callister R. Resistance training to improve power and sports performance in adolescent athletes: a systematic review and meta-analysis. J Sci Med Sport. 2012;15:532–40.
- 142. Lloyd RS, Radnor JM, De Ste Croix MBA, Cronin JB, Oliver JL. Changes in sprint and jump performance after traditional, plyometric, and combined resistance training in male youth preand post-peak height velocity. J Strength Cond Res. 2016;30:1239–47.
- 143. Markovic G, Mikulic P. Neuro-musculoskeletal and performance adaptations to lower-extremity plyometric training. Sports Med. 2010;40:859–95.
- 144. Chimera NJ, Swanik KA, Buz Swanik C, Straub SJ. Effects of plyometric training on muscle-activation strategies and performance in female athletes. J Athl Train. 2004;39:24–31.

- 145. Voigt M, Chelli F, Frigo C. Changes in the excitability of soleus muscle short latency stretch reflexes during human hopping after 4 weeks of hopping training. Eur J Appl Physiol Occup Physiol. 1998;78:522–32.
- 146. Malisoux L, Francaux M, Nielens H, Theisen D. Stretch-shortening cycle exercises: an effective training paradigm to enhance power output of human single muscle fibers. J Appl Physiol. 2006;100:771–9.
- 147. Aagaard P, Simonsen E, Andersen J, Magnusson S, Halkjaer-Kristensen J, Dyhre-Poulsen P. Neural inhibition during maximal eccentric and concentric quadriceps contraction: effects of resistance training. J Appl Physiol. 2000;89:2249–57.
- Duchateau J, Semmler JG, Enoka RM. Training adaptations in the behavior of human motor units. J Appl Physiol. 2006;101:1766–75.
- 149. Potier TG, Alexander CM, Seynnes OR. Effects of eccentric strength training on biceps femoris muscle architecture and knee joint range of movement. Eur J Appl Physiol. 2009;105:939–44.
- 150. Seynnes OR, de Boer M, Narici MV. Early skeletal muscle hypertrophy and architectural changes in response to high-intensity resistance training. J Appl Physiol. 2013;102:368–73.
- Blazevich AJ, Cannavan D, Coleman DR, Horne S. Influence of concentric and eccentric resistance training on architectural adaptation in human quadriceps muscles. J Appl Physiol. 2007;103:1565–75.
- 152. Alegre LM, Jiménez F, Gonzalo-Orden JM, Martín-Acero R, Aguado X. Effects of dynamic resistance training on fascicle length and isometric strength. J Sports Sci. 2006;24:501–8.
- 153. Reeves ND, Maganaris CN, Longo S, Narici MV. Differential adaptations to eccentric versus conventional resistance training in older humans. Exp Physiol. 2009;94:825–33.
- 154. Baroni BM, Geremia JM, Rodrigues R, De Azevedo Franke R, Karamanidis K, Vaz MA. Muscle architecture adaptations to knee extensor eccentric training: rectus femoris vs. vastus lateralis. Muscle Nerve. 2013;48:498–506.
- 155. Aagaard P, Andersen JL, Dyhre-Poulsen P, Leffers AM, Wagner A, Magnusson SP, et al. A mechanism for increased contractile strength of human pennate muscle in response to strength training: changes in muscle architecture. J Physiol. 2001;534:613–23.
- 156. Guilhem G, Cornu C, Guével A. Muscle architecture and EMG activity changes during isotonic and isokinetic eccentric exercises. Eur J Appl Physiol. 2011;111:2723–33.
- 157. Waugh CM, Korff T, Fath F, Blazevich A. Effects of resistance training on tendon mechanical properties and rapid force production in prepubertal children. J Appl Physiol. 2014;117:257–66.