

Synergistic combination therapy of lung cancer using paclitaxel- and triptolide-co-loaded lipid-polymer hybrid nanoparticles

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Purpose: Non-small cell lung cancer (NSCLC) accounts for the majority of lung cancer. Lipid-polymer hybrid nanoparticles (LPNs) combine the advantages of both polymeric nanoparticles and liposomes into a single delivery platform. In this study, we engineered LPNs as the co-delivery system of paclitaxel (PTX) and triptolide (TL) to achieve synergistic therapeutic effect and reduced drug resistance.

Materials and methods: In this study, PTX- and TL-co-loaded LPNs (P/T-LPNs) were fabricated by nanoprecipitation method using lipid and polymeric materials. The P/T-LPNs combination effects on human lung cancer cells were studied. Therapeutic potentials of P/T-LPNs were further determined using lung cancer cells-bearing mice model.

Results: The average particle sizes of LPNs were around 160 nm, with narrow size distribution below 0.2. The zeta potential value of LPNs was about -30 mV. The encapsulating efficiency (EE) of PTX and TL loaded in LPNs was over 85%. The cytotoxicity of dual drug loaded LPNs was higher than single drug loaded LPNs. The combination therapy showed synergistic when PTX:TL weight ratio was 5:3, indicating the synergy effects of the LPNs. In vivo tumor growth curve of the experimental group was more gentle opposed to the control group, and tumor volumes of P/T-LPNs and control group were 392 and 1,737 mm³, respectively. The inhibition rate on day 20 was 77.4% in the P/T-LPNs group, which is higher than the free drugs solution.

Conclusion: The in vivo and in vitro results proved the synergetic effect of the two drugs co-loaded in LPNs on the lung cancer xenografts, with the least systemic toxic side effect.

Keywords: non-small cell lung cancer, multidrug resistance, combination therapy, paclitaxel, triptolide

Introduction

Lung cancer is the most common cancer worldwide and nearly 23% of the total cancer-related deaths are caused by lung cancer globally.¹ Non-small cell lung cancer (NSCLC) accounts for the majority (more than 80%) of lung cancer. Current therapeutic strategies for NSCLC are generally dependent on their stages at the time of diagnosis. However, in 85% of patients, NSCLC is diagnosed in their advanced stages and surgery is not suitable for them.² Therefore, the most preferred therapy prevalent clinically is chemotherapy.³ Currently, the third-generation chemotherapy agents such as paclitaxel (PTX) in combination with a platinum compound is the recommended first-line treatment for advanced NSCLC.^{4,5} However, systemic toxicity of PTX or platinum and drug resistance have led to a high rate of mortality in NSCLC.⁶ As such, it is urgent to design novel treatment approaches for NSCLC.

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Nanotechnology-based drug delivery system (DDS) potentially represents such a disruptive technology for improving therapeutic efficacy and reducing systemic toxicity by enhancing the pharmacokinetics parameters such as large volume distribution and tumor deposition of the payloads through enhanced permeability and retention (EPR) effect.⁷⁻⁹ Among various kinds of nanoparticles, lipid-polymer hybrid nanoparticles (LPNs) combine the advantages of both polymeric nanoparticles and liposomes into a single delivery platform.¹⁰⁻¹² Specifically, based on the LPNs' dual-component structure, it provides an ideal platform for combinatorial drug delivery, whereby different drugs can be loaded to either the polymer core or the lipid shell, on account of the desired release kinetics and therapeutic roles.¹⁰ In this study, we engineered LPNs as the co-delivery system of PTX and triptolide (TL) to achieve synergistic therapeutic effect and reduced drug resistance.

TL, an active compound isolated from the Chinese herb *Tripterygium wilfordii*, possesses a broad-spectrum therapeutic effect including anti-inflammatory, immunosuppressive, and antitumor activities.^{13,14} TL has also been shown to induce cell apoptosis and inhibit cell proliferation of various cancer cells including pancreatic, gastric, NSCLC, etc.¹⁵⁻¹⁸ Its cytotoxic effect against NSCLC has been demonstrated in vitro and in vivo via the inhibition of nuclear factor (NF)- κ B; upregulation of p-p38, p-ERK, p-GSK-3 β , Bax, and cleaved caspases-3 and -9; and downregulation of p-JNK, p-Akt, and Bcl-2.¹⁹ Moreover, TL exerts its anti-multidrug resistance (MDR) role on A549/Taxol cell lines by inhibiting the NF- κ B signaling pathway and selective modulation of mitogen-activated protein kinase signaling.^{20,21} However, TL has a poor solubility in water (0.017 mg/mL).²² Significant and rapid fluctuations of TL in plasma by oral administration (T_{max} from 10.0 to 19.5 minutes; $t_{1/2}$ from 16.8 to 50.6 minutes) likely contribute to its toxicity, which is characterized by injury to hepatic, renal, digestive, reproductive, and hematological systems.²³ Therefore, it is necessary to design LPNs for prolonging drug release and improving its safety.

In this study, PTX- and TL-co-loaded LPNs (P/T-LPNs) were fabricated by nanoprecipitation method using lipid and polymeric materials (Figure 1). The P/T-LPNs combination effects on human lung cancer cells were investigated.²⁴ The therapeutic potentials of P/T-LPNs were further determined using lung cancer cells-bearing mice model. Single drug loaded LPNs and free drugs combination were applied for contrast. As expected, such a co-delivery system would combine the desirable properties of LPNs and the synergistic effect of PTX and TL and thus provide a fascinating opportunity to treat lung cancer.

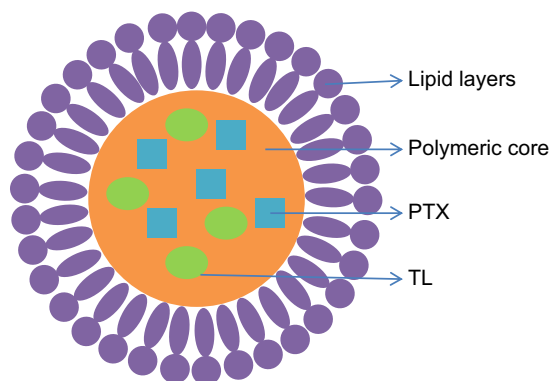


Figure 1 Schematic diagram PTX- and TL-co-loaded LPNs (P/T-LPNs).
Abbreviations: LPN, lipid-polymer hybrid nanoparticle; P/T-LPN, PTX- and TL-co-loaded LPN; PTX, paclitaxel; TL, triptolide.

Materials and methods

Chemicals and reagents

TL (isolated from *T. wilfordii*, $\geq 98\%$ HPLC, solid) and PTX (semisynthetic drug isolated from *Taxus* sp., $\geq 97\%$) were purchased from Sigma-Aldrich (Shanghai, China). Poly(lactic-co-glycolic acid) (PLGA; 75/25; molecular weight, 23–37 kDa) was obtained from Dalian Meilun Biotechnology Co., Ltd. (Dalian, China). 1,2-Distearoyl-sn-glycero-3-phosphoethanolamine-*N*-[methoxy(polyethylene glycol)-₅₀₀₀] (DSPE-mPEG₅₀₀₀) and 1,2-distearoyl-sn-glycero-3-phosphoethanolamine-*N*-[(polyethylene glycol)-₅₀₀₀]-fluorescein isothiocyanate (DSPE-PEG₅₀₀₀-FITC) were provided by Xi'an ruixi Biological Technology Co., Ltd. (Xi'an, China). Injectable soybean lecithin (ISL) was provided by Shanghai A.V.T. Pharmaceutical Co., Ltd (Shanghai, China). DMEM, Roswell Park Memorial Institute medium (RPMI-1640), FBS, penicillin/streptomycin, and MTT were purchased from Thermo Fisher Scientific, Waltham, MA, USA. All other chemicals and reagents used were of analytical or HPLC grade.

Cells and culture

A549 human lung adenocarcinoma cells (A549 cells) were obtained from American Type Culture Collections (Manassas, VA, USA). A549/PTX (PTX resistant) cells were purchased from Shanghai MEIXUAN Biological Science and Technology Co, Ltd. (Shanghai, China). A549 cells were cultured in DMEM, and A549/PTX cells were cultured in RPMI-1640 and supplemented with 10% FBS and penicillin (100 U/mL)/streptomycin (100 U/mL) at 37°C in a humidified atmosphere with 5% CO₂.²⁵

Animals and xenografts

Balb/c-nude mice (8–10 weeks old, 20–25 g weight) were purchased from Laboratory Animal Center of Shaanxi

Province (Xi'an, China) and maintained in plastic cages in an specific pathogen free-grade animal room with access to food and water ad libitum. A549/PTX cells (10^7) suspended in 0.9% saline (200 μ L) were subcutaneously injected into the right flank of mice to produce the lung tumor xenografts. All animal experiments were complied with the guideline: National Institutes of Health Guide for the Care and Use of Laboratory Animals (NIH Publications No 8023). All the procedures were ethically and scientifically approved by the Institutional Animal Care and Treatment Committee of Tumor Hospital of Shaanxi Province (No 20180119-01, 2018-01-19).

Preparation of P/T-LPNs

P/T-LPNs were prepared by nanoprecipitation method.²⁶ DSPE-mPEG5000 (100 mg) and ISL (100 mg) were dispersed in distilled water (aqueous phase). PTX (50 mg), TL (30 mg), and PLGA (200 mg) were dissolved in acetone (oil phase). Oil phase is added dropwise into the aqueous phase stirred at 400 rpm at room temperature for 8 hours until complete evaporation of acetone. The mixture was centrifuged to remove the unloaded PTX and/or TL at a speed of 3,000 rpm for 10 minutes and then filtered through a syringe filter (pore size, 0.45 μ M). PTX-loaded LPNs (P-LPNs) were produced using the same method by dissolving PTX (100 mg) and PLGA (200 mg) in acetone to produce the oil phase. TL-loaded LPNs (T-LPNs) were produced using the same method by dissolving TL (60 mg) and PLGA (200 mg) in acetone to produce the oil phase. Blank LPNs were produced using the same method by dissolving PLGA (200 mg) in acetone to produce the oil phase. FITC-loaded LPNs were prepared using the same method, replacing DSPE-mPEG₅₀₀₀ with DSPE-PEG₅₀₀₀-FITC.

PTX solution (P solution) was prepared by dissolving 10 mg PTX in 10 mL solvent 1 (acetone:ethanol = 3:2, v:v). TL solution (T solution) was prepared by dissolving 6 mg TL in 10 mL solvent 1. PTX and TL mixed solution (P/T solution) was prepared by dissolving 5 mg PTX and 3 mg TL in 10 mL solvent 1.

Particle size and zeta potential

Particle sizes, polydispersity indexes, and zeta potentials of LPNs were determined 1 hour after preparation by placing the LPNs in a cuvette.²⁷ A ZETA SIZER3000 laser particle size analyzer and dynamic light scattering software were used to detect their average diameter and surface potential. The tests were conducted in triplicate, and the average data were calculated.

Drug-loading (DL) content and encapsulating efficiency (EE)

DL content and EE of PTX in the LPNs was determined by UV/Vis method.²⁸ PTX was also isolated from the carriers by centrifugation at 15,000 rpm at 4°C for 30 minutes, the supernatants were collected, and the concentration of PTX was measured by UV/Vis spectrophotometer at 233 nm. The content of TL in the nanoparticles was determined by HPLC using a reversed-phase column (C18; 250 mm \times 4.6 mm, 5 μ m).²⁹ The gradient mobile phase consisted of a mixture of methanol and water, and the flow rate was 1.0 mL/min. The column effluent was detected at 218 nm, and the column temperature was 30°C. DL and EE were calculated according to the following equations:

$$\text{DL (\%)} = \frac{\text{The weight of drug incorporated in the LPNs}}{\text{The weight of the LPNs}} \times 100;$$

$$\text{EE (\%)} = \frac{\text{The weight of drug incorporated in the LPNs}}{\text{The weight of the initial feeding drug}} \times 100.$$

Storage stability

LPNs dispersions were stored at 4°C, and the stability of LPNs was evaluated by measuring average vesicle size and EE during 3 months.³⁰ Results are recorded at 0, 10, 20, 30, 60, and 90 days.

In vitro release behavior

In vitro release behavior of PTX and TL from LPNs was explored by placing 1 mL of LPNs in dialysis bags (molecular weight cutoff, 3.5 kDa).³¹ The dialysis bags were incubated in 30 mL phosphate buffer (pH, 7.4) containing Tween 80 (0.5%, w/w) at 37°C under gentle shaking (100 rpm). At different time intervals, incubation medium (2 mL) was taken out and replaced by the same volume of fresh pre-heated medium at specific time points. The release medium was vortexed and analyzed by the same method explained in the section "Drug-loading (DL) content and encapsulating efficiency (EE)". The tests were conducted in triplicate, and the average data were calculated.

Cellular uptake

A549 and A549/PTX cells were seeded in glass bottom dishes at a density of 2×10^5 cells per dish.³² After 24 hours of incubation, cells were treated with a concentration of 20 μ g/mL LPNs. The cells were washed three times with cold PBS after 2 hours of incubation at 37°C. The fluorescence intensity was measured at an excitation wavelength of 488 nm using an

inversion fluorescence microscope (OLYMPUS Corporation, Tokyo, Japan), and the picture was captured. At the indicated time points, the cells were washed with PBS, harvested, and dispersed in 0.5 mL of PBS solution for flow cytometric measurements using a FACSCalibur flow cytometer (BD Biosciences, San Jose, CA, USA).³³

Cytotoxicity assay and synergistic effects

A549 and A549/PTX cells were cultured in 96-well plate (5×10^3 cells per well) for 24 hours.³⁴ Then, the cells were incubated with fresh culture medium containing free drugs or drugs loaded LPNs for 48 hours. The medium was replaced with the fresh medium to recapitulate the effects of the process. MTT solution (20 μ L, 5 mg/mL) was then added into each well, and the cells were incubated for another 4 hours. Next, the culture medium was discarded, and 200 μ L DMSO was added into the well. Finally, the absorbance of liquid in each well was measured at 490 nm by using a Microplate Reader (Bio-Rad Laboratories Inc., Hercules, CA, USA). Cell viability was calculated according to the following equation: (Absorbance of cells treated with samples/Absorbance of cells treated with fresh medium) \times 100%. The mean drug concentration required for 50% growth inhibition (IC_{50}) was calculated.

To study the synergistic effect of the combination treatment of the formulation, Combination Index (CI) analysis was undertaken.³⁵ The results of cytotoxicity were evaluated via the CI. The CI of a combination of drugs less than 1 indicates the synergistic effect, CI equal to 1 means additive effect, and CI greater than 1 means an antagonistic effect. To evaluate the CI value, both individual drugs and drug combinations treatment in a range of concentrations were performed on the cell lines as described above. Combination index when 50% growth inhibition (CI_{50}) was considered. Briefly, for each level of Fa (the fraction of affected cells), the CI values of PTX and TL combinations were calculated by the following equation³⁶: $CI_{50} = (D)_A / (D_{50})_A + (D)_B / (D_{50})_B$. In this equation, $(D)_A$ and $(D)_B$ represent the IC_{50} value of PTX and TL alone,

respectively. $(D_{50})_A$ and $(D_{50})_B$ represent the concentration of PTX and TL in the combination system at the IC_{50} value. The CI_{50} values curves were drawn according to Fa. Fa values between 0.2 and 0.8 are considered validate.

In vivo antitumor efficacy

The lung tumor xenografts were randomly assigned to eight groups (n = 10 each): 0.9% saline control, P solution (10 mg/kg), T solution (6 mg/kg), P/T solution (5 mg/kg of PTX and 3 mg/kg of TL), blank LPNs, P-LPNs (10 mg/kg), T-LPNs (6 mg/kg), and P/T-LPNs (5 mg/kg of PTX and 3 mg/kg of TL) were administered intravenously every other day for 18 days.³⁷ Mice were sacrificed by cervical dislocation on day 20, and the tumor tissues were collected for further analysis. During the treatment, tumor size (length and width) was measured using calipers every 4 days. Tumor volumes (V) were calculated by the formula $V = a \times b^2 / 2$, where a is the longest axis, and b is the perpendicular shorter tumor axis. The tumor volume inhibition rate (TIR) on day 20 was calculated according to the following equation: $TIR (\%) = [1 - (V_{Day 1 treatment} - V_{Day 20 treatment}) / (V_{Day 1 control} - V_{Day 20 control})] \times 100$, where $V_{Day 1 treatment}$ and $V_{Day 20 treatment}$ are the tumor volumes of the treatment groups at day 1 and day 20 and $V_{Day 1 control}$ and $V_{Day 20 control}$ are the tumor volumes of the control group at day 1 and day 20. Body weights of mice were measured for the evaluation of systematic toxicity.

Statistical analysis

Quantitative data were expressed as mean \pm SD. Statistical analysis was performed using an unpaired *t*-test. *P*-value less than 0.05 was considered statistically significant.

Results

Characterization of P/T-LPNs

The average particle sizes of LPNs were around 160 nm, with narrow size distribution with polydispersity index values below 0.2 (Table 1). The zeta potential value of LPNs was

Table 1 Characterization of LPNs (mean \pm SD, n = 3)

LPNs	Blank LPNs	P-LPNs	T-LPNs	P/T-LPNs
Particle size (nm)	156.7 \pm 5.1	159.8 \pm 5.6	158.3 \pm 5.5	160.1 \pm 5.9
Polydispersity index	0.16 \pm 0.02	0.15 \pm 0.03	0.14 \pm 0.02	0.17 \pm 0.03
Zeta potential (mV)	-31.2 \pm 4.2	-30.9 \pm 4.6	-29.8 \pm 4.9	-30.4 \pm 4.4
EE of PTX (%)	N/A	90.3 \pm 3.6	N/A	88.7 \pm 4.1
EE of TL (%)	N/A	N/A	86.2 \pm 4.5	85.4 \pm 4.8
DL content of PTX (%)	N/A	10.4 \pm 1.2	N/A	11.1 \pm 1.5
DL content of TL (%)	N/A	N/A	6.5 \pm 0.8	6.2 \pm 0.9

Abbreviations: DL, drug loading; EE, encapsulating efficiency; LPN, lipid-polymer hybrid nanoparticles; P-LPN, PTX-loaded LPN; P/T-LPN, PTX- and TL-co-loaded LPN; PTX, paclitaxel; TL, triptolide; T-LPN, TL-loaded LPN.

about -30 mV. The EE of PTX and TL loaded in LPNs was over 85%. The DL of PTX and TL loaded in LPNs were approximately 10% and 6%, respectively. During the period of 90 days, LPNs showed no significant changes of average vesicle size and EE (Figure 2).

In vitro release behavior

As shown in Figure 3, approximately 90% of drugs was slowly released from LPNs in a sustained behavior within 48 hours, with no burst effect. Drugs solutions showed faster release within 2 hours. Dual drugs coloaded LPNs did not exhibit differences during the release compared with single drug loaded LPNs.

Cellular uptake

To determine the intracellular accumulation of LPNs to assess the efficacy of the formulations, qualitative and quantitative

studies of cellular uptake were performed. In the qualitative study, both A549 and A549/PTX cells with LPNs exhibited obvious fluorescence at 2 hours after treatments (Figure 4A). The quantitative study of cellular uptake was further performed to confirm the percentage of cells that have been entered by LPNs (Figure 4B).

Cytotoxicity assay and synergistic effects

The blank LPNs exhibited no significant cytotoxicity on A549 (Figure 5A) and A549/PTX cells (Figure 5B) and when its concentration ranged from 0.5 to 10 mg/mL. Drugs loaded LPNs exhibited marked cytotoxicity on cells in a dose-dependent manner and showed higher cytotoxicity compared with their free drugs counterparts ($P < 0.05$). The cytotoxicity of dual drugs loaded LPNs was higher than single drug loaded LPNs ($P < 0.05$). Table 2 showed the effects of LPNs on A549/PTX cells: combination therapy showed

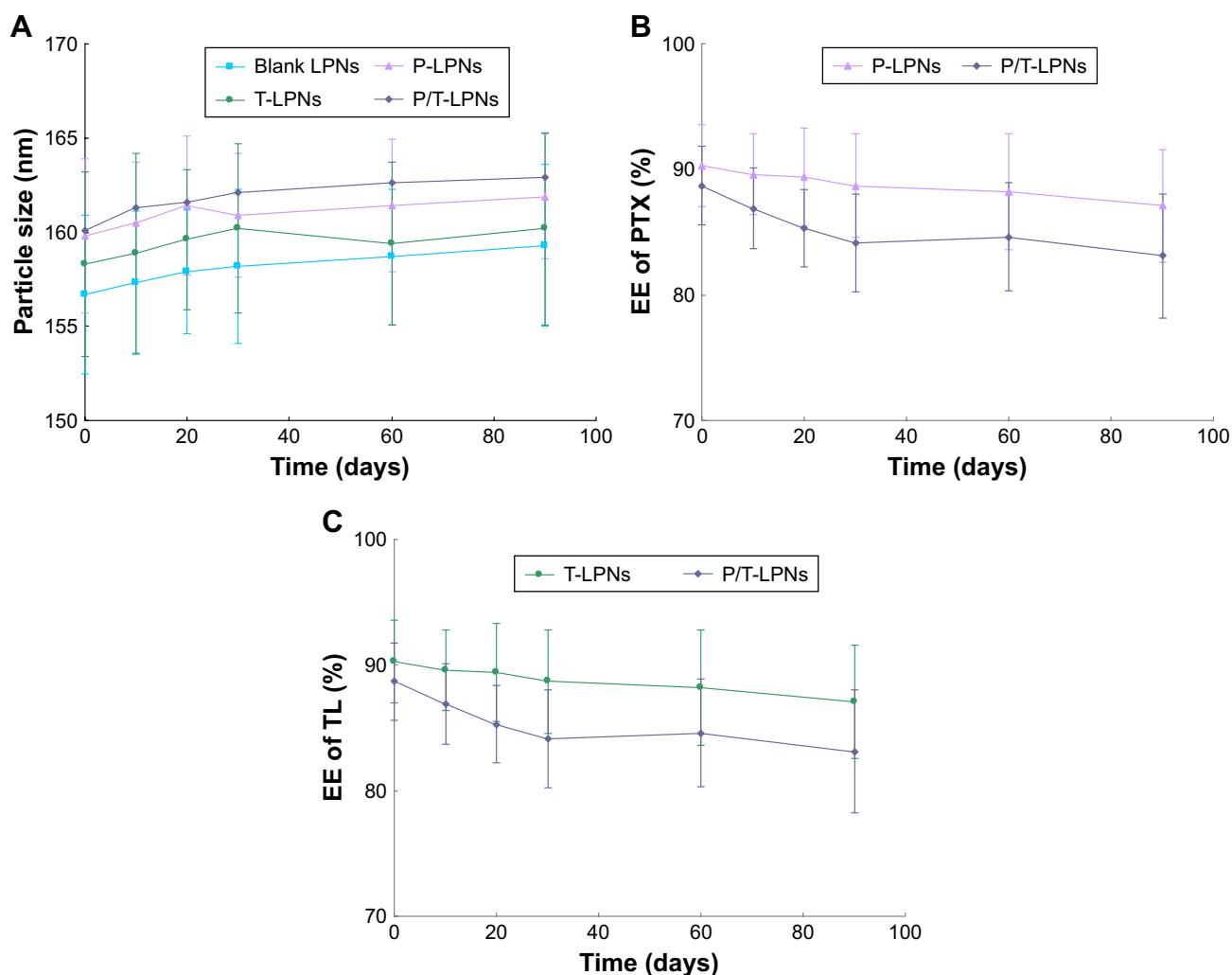


Figure 2 Storage stability of LPNs dispersions evaluated by measuring of average vesicle size (A) and EE of PTX (B) and TL (C). LPNs showed no significant changes of average vesicle size and EE during 3 months.

Abbreviations: EE, encapsulating efficiency; LPN, lipid-polymer hybrid nanoparticle; P-LPN, PTX-loaded LPN; P/T-LPN, PTX- and TL-coloaded LPN; PTX, paclitaxel; TL, triptolide; T-LPN, TL-loaded LPN.

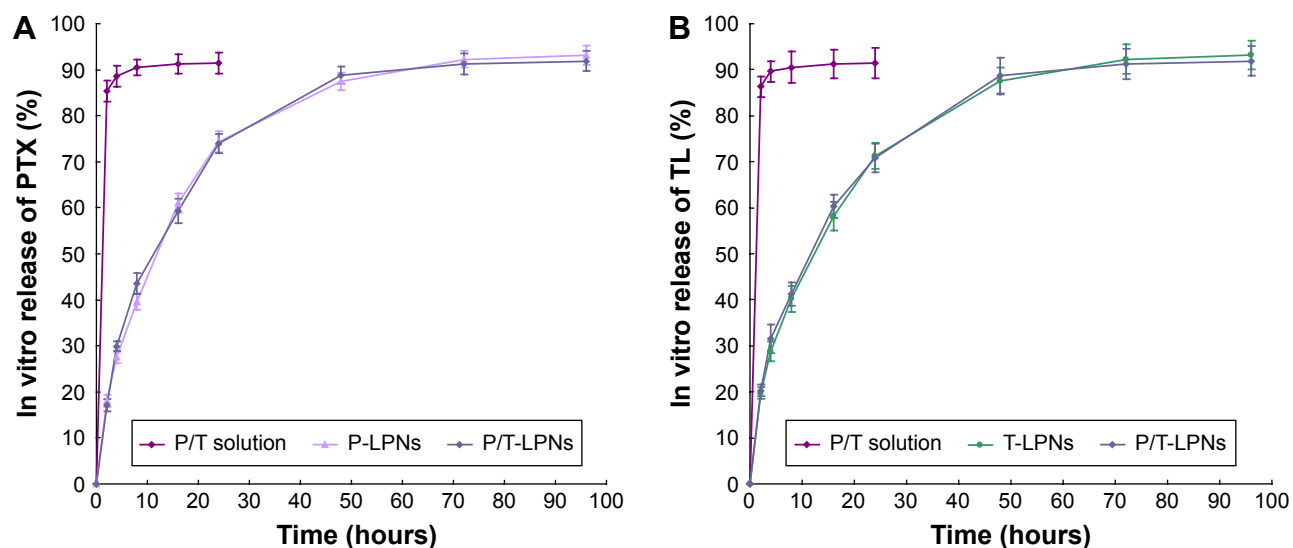


Figure 3 In vitro PTX (A) and TL (B) release behavior of drugs loaded LPNs and drugs solutions. Approximately 90% of drugs was slowly released from LPNs in a sustained behavior within 48 hours, with no burst effect.

Abbreviations: LPN, lipid-polymer hybrid nanoparticle; P-LPN, PTX-loaded LPN; P/T-LPN, PTX- and TL-co-loaded LPN; PTX, paclitaxel; TL, triptolide; T-LPN, TL-loaded LPN.

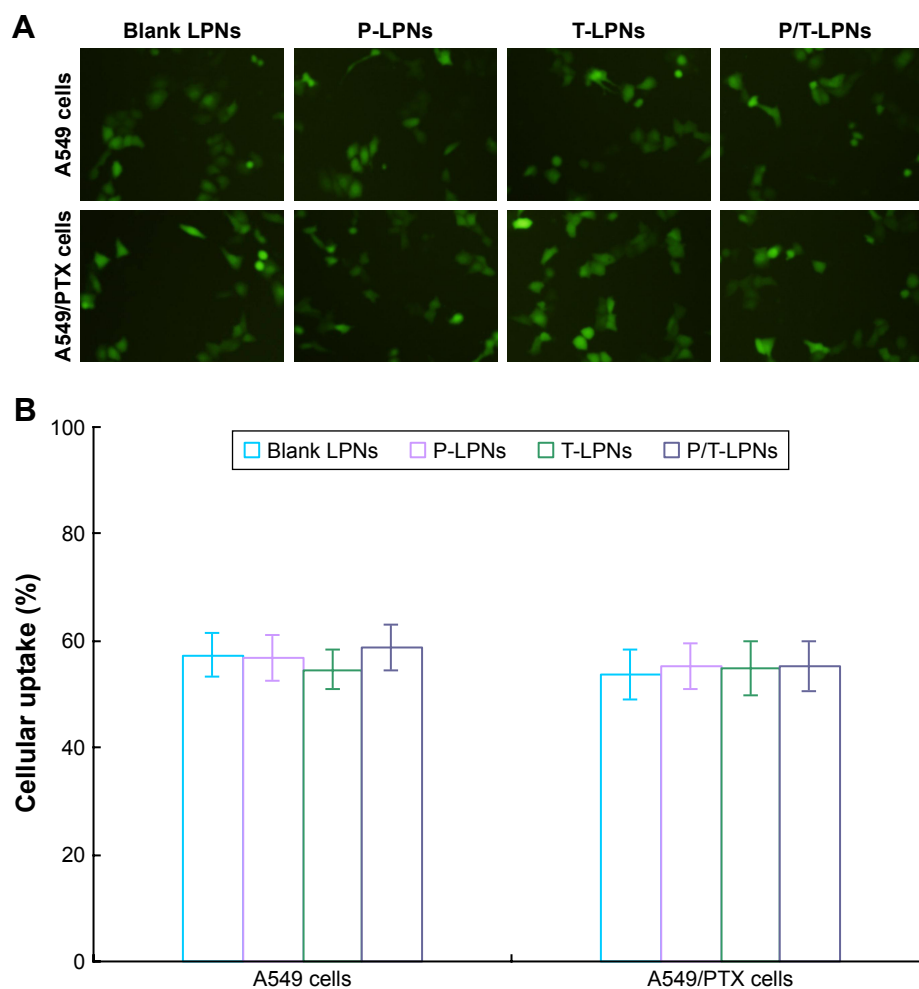


Figure 4 Qualitative (A) and quantitative (B) studies of cellular uptake of LPNs. Both A549 and A549/PTX cells exhibited high cellular uptake by LPNs.

Abbreviations: LPN, lipid-polymer hybrid nanoparticle; P-LPN, PTX-loaded LPN; P/T-LPN, PTX- and TL-co-loaded LPN; PTX, paclitaxel; T-LPN, TL-loaded LPN.

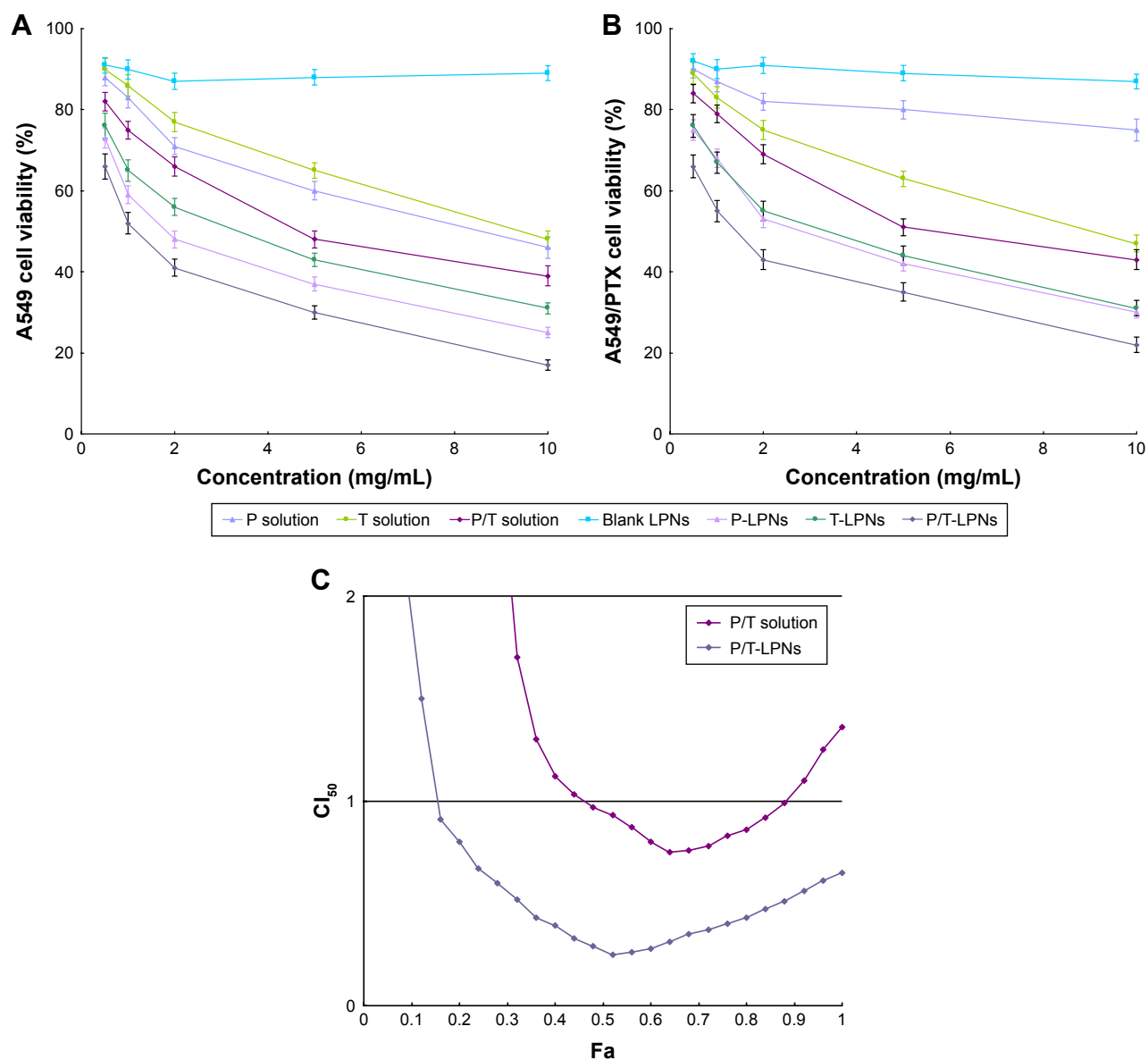


Figure 5 Cytotoxicity assay of drugs loaded LPNs and drugs solutions on A549 (A) and A549/PTX cells (B). Synergistic effects evaluated by Fa determination on A549 cells (C).

Abbreviations: LPN, lipid-polymer hybrid nanoparticle; P-LPN, PTX-loaded LPN; P/T-LPN, PTX- and TL-co-loaded LPN; PTX, paclitaxel; T-LPN, TL-loaded LPN.

Table 2 CI_{50} values of P/T-LPNs on A549/PTX cells with different PTX:TL ratios

LPNs	PTX:TL (w:w)	IC_{50} of PTX (mg/mL)	IC_{50} of TL (mg/mL)	CI_{50}
P-LPNs	N/A	2.56	N/A	N/A
T-LPNs	N/A	N/A	3.39	N/A
P/T-LPNs	5:1	2.49	0.51	1.12
P/T-LPNs	5:2	2.37	0.95	1.21
P/T-LPNs	2:1	2.21	1.10	1.19
P/T-LPNs	5:3	1.49	0.89	0.84
P/T-LPNs	5:4	1.68	1.34	1.05
P/T-LPNs	1:1	1.87	1.87	1.28

Abbreviations: CI_{50} , combination index when 50% growth inhibition; IC_{50} , 50% growth inhibition; LPN, lipid-polymer hybrid nanoparticle; P-LPN, PTX-loaded LPN; P/T-LPN, PTX- and TL-co-loaded LPN; PTX, paclitaxel; TL, triptolide; T-LPN, TL-loaded LPN.

synergistic when PTX:TL weight ratio was 5:3 ($CI_{50} = 0.84$), suggesting the best drugs ratios in the LPNs. This ratio was used for the in vivo antitumor study. For Fa determination on A549 cells, P/T-LPNs displayed an overall CI_{50} value < 1 when Fa value was between 0.2 and 0.8 (Figure 5C), indicating the synergy effects of the LPNs. Table 3 summarized the IC_{50} values evaluated on A549 and A549/PTX cells. IC_{50} of PTX on A549/PTX cells was significantly higher than A549 cells, showing the drug resistance in A549/PTX cells.

In vivo antitumor efficacy

In vivo tumor growth inhibition curve of the experimental group was more gentle compared to that of the control group.

Table 3 IC₅₀ values of free drugs or drugs loaded LPNs on A549 and A549/PTX cells

Samples	A549 cells		A549/PTX cells	
	IC ₅₀ of PTX (mg/mL)	IC ₅₀ of TL (mg/mL)	IC ₅₀ of PTX (mg/mL)	IC ₅₀ of TL (mg/mL)
P solution	8.62	N/A	106.9	N/A
T solution	N/A	9.13	N/A	9.21
P/T solution	4.87	2.92	8.64	5.18
P-LPNs	1.92	N/A	2.56	N/A
T-LPNs	N/A	3.58	N/A	3.39
P/T-LPNs	1.27	0.76	1.49	0.89

Abbreviations: IC₅₀, 50% growth inhibition; LPN, lipid-polymer hybrid nanoparticle; P-LPN, PTX-loaded LPN; P/T-LPN, PTX- and TL-co-loaded LPN; PTX, paclitaxel; TL, triptolide; T-LPN, TL-loaded LPN.

After 20 days, tumor volume of the P/T-LPNs group was significantly smaller than the P-LPNs and T-LPNs groups ($P < 0.05$; Figure 6A). The drugs loaded LPNs exhibited smaller tumor size than the free drugs loaded counterparts (Figure 6B). The inhibition rate on day 20 was 77.4% in the P/T-LPNs group, 53.9% in the P-LPNs group, 49.3% in the T-LPNs group, and 41.1% in the P/T solution group (Figure 6C). There were no significant differences in the body

weight of mice treated with drugs loaded LPNs groups, but reduction of weights were found in the drugs solution and control groups (Figure 6D).

Discussion

Nanoparticles are known to exploit the EPR effect for targeting the tumors, thereby increasing tumor drug concentrations while minimizing systemic toxicity.³⁸ Many recent studies have highlighted the significance of nanoparticle sizes, which would greatly affect the fate of nanoparticle in vivo: less than 200 nm showed longer blood circulation time, greater stability, lower cytotoxicity, and favorable uptake by the EPR effect.^{39,40} Moreover, the EE of PTX and TL for all kinds of LPNs were over 80%, indicating the good loading ability of the LPNs.

Storage stability evaluation of the nanoparticles was essential to confirm that the structural properties were preserved over storage time, since disruption of nanocarriers in the DDSs could affect their therapeutic potential.⁴¹ For all kinds of LPNs, the particle sizes remained almost constant for 90 days. The EE of two drugs loaded in LPNs also remained

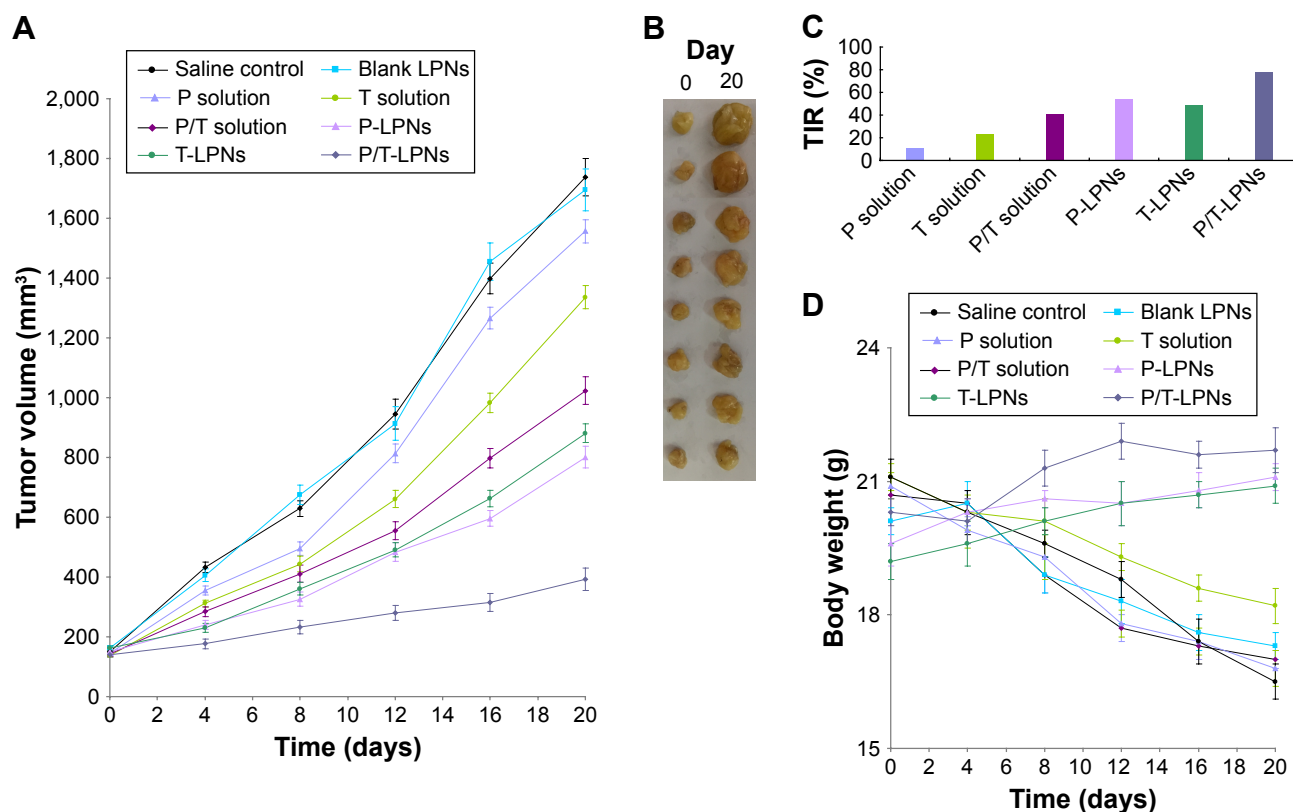


Figure 6 In vivo tumor growth inhibition curve of the experimental group (A), tumor images (B), tumor inhibition rate (C), and body weight of mice (D).

Abbreviations: LPN, lipid-polymer hybrid nanoparticle; P-LPN, paclitaxel-loaded LPN; P/T-LPN, paclitaxel- and TL-co-loaded LPN; TIR, tumor volume inhibition rate; T-LPN, TL-loaded LPN.

stable at all the time points tested in the research, indicating that the LPNs were stable and will not disassemble or aggregate within 3 months. In this study, DSPE-mPEG10000, DSPE-mPEG5000, DSPE-mPEG2000, and DSPE-mPEG550 were tried, and only DSPE-mPEG5000 could form nanoparticles with uniform particle sizes and polydispersity index. We also tried soybean lecithin, egg lecithin, and cholesterol in the oil phase; some precipitated immediately after preparation or storage stability would not last for a week. Only ISL gain good stability. So, DSPE-mPEG₅₀₀₀ and ISL were chosen for making the LPNs.

In vitro drug release of the drug loaded nanoparticles may be controlled by the erosion, corrosion, and diffusion process.⁴² Drug depot effects could be obtained by the carriers, which could lead to the sustained release of hydrophobic drugs. More sustained-release behavior of drugs from LPNs was found in the in vitro drug release study. As the drugs are restrained within the LPNs, the cytotoxicity of drugs may be lowered until the LPNs entered the tumor cells. Once within the cells, the PTX and TL can be released from the LPNs and induce their toxic impacts.⁴³ These results indicate that the lipid layer at the interface of the PLGA core and the PEG shell acts as a molecular fence that helps to retain the drugs inside the LPNs, thus let the drugs release slowly from the nanoparticles.

Effective cytotoxicity of nanoparticle-based therapies usually demands a high level of accumulation within the cancer cells.⁴⁴ Cellular uptake of LPNs into the cells was examined to distinguish the uptake efficiency. The results of qualitative and quantitative studies of cellular uptake indicate that the functionalization of LPNs encapsulation played a key role in the uptake of drugs in lung cancer cells in vitro. High internalization of the drugs loaded nanoparticles into the cells could directly account for the anticancer efficacy, which leads to more efficacy of cell growth inhibition, induction of apoptosis, and cell cycle arrest in cancer cells.

The prepared blank LPNs nanoparticles showed no cytotoxicity on A549/PTX cells in vitro and in vivo in nude mice, demonstrating that LPNs were safe as DDS as many studies reported.⁴⁵ Drugs were released in a controlled manner from the LPNs, but higher cell toxicity was observed in MTT assay than the drugs solutions. The use of multiple drugs in combination has possible favorable outcomes, such as synergism, additive, and antagonism. Evaluation of drug–drug interaction plays an important role in all areas of medicine and particularly in cancer chemotherapy where combination therapy is commonly used.⁴⁶ To determine

the possible effect of the drug combination, mathematical model-based method has been introduced. LPNs combining the mechanical advantages of biodegradable polymers and liposomes are core-shell nanoparticles structures comprising polymer cores and lipid shells.⁴⁷ Also, dual drugs coloaded LPNs has better ability and showed obvious synergism effect than the single drug loaded systems. The novel carrier might have the enhanced ability to adhere to the cell membrane due to the similar nature of the lipids and the cell membrane. Table 3 showed the cytotoxicity data that could demonstrate the extent of drug resistance in A549/PTX cells. CI analyses are the most popular methods for evaluating drug interactions in combination cancer chemotherapy.³⁶ In this research, CI₅₀ was determined to validate the synergistic effect and suitable PTX to TL ratio to be loaded in the LPNs. P/T-LPNs displayed an overall CI₅₀ value <1 when Fa value was between 0.2 and 0.8, showing the synergy effects of the LPNs. TL has been shown to induce cell apoptosis and inhibit cell proliferation of various cancer cells including NSCLC. TL may exert its anti-MDR role on A549/PTX cells by inhibiting the NF-κB signaling pathway and selective modulation of mitogen-activated protein kinase signaling.

To evaluate the effect of P/T-LPNs on lung cancer-bearing mouse xenografts, tumor volume was measured and plotted. With regard to the inhibition of tumor growth, the P/T-LPNs exhibited the strongest inhibitory effect. These results demonstrated that P/T-LPNs system was the most effective treatment in reducing the tumor volume. No noticeable loss of body weight of mice was considered as an indicator of safety.⁴⁸ The in vivo antitumor results were in line with the in vitro results and proved the synergetic effect of the two drugs coloaded in LPNs in the lung cancer xenografts, with the least systemic toxic side effect.

Conclusion

The cytotoxicity of dual drugs loaded LPNs was higher than single drug loaded LPNs. Combination therapy showed synergy effects of the LPNs. In vivo tumor growth inhibition curve of the experimental group was more gentle compared to that of the control group. The drugs loaded LPNs exhibited smaller tumor size than the free drugs loaded counterparts. The in vivo and in vitro results proved the synergetic effect of the two drugs coloaded in LPNs in the lung cancer xenografts, with the least systemic toxic side effect.

Disclosure

The authors report no conflicts of interest in this work.

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