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In vitro histological investigation of interactions between rat decellularized large intestine scaffold and human adipose derived mesenchymal stem cells

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Article Info	Abstract
Article history:	The aim of this study was to investigate the interactions between rat intestine
	decellularized scaffold and human adipose derived mesenchymal stem cells. Rat large intestine
Received: 21 April 2014	was dissected in fragments and decellularized by physicochemical methods. The scaffolds were
Accepted: 10 May 2015	loaded by human adipose derived mesenchymal stem cells expressing green fluorescent
Available online: 15 September 2015	protein. Microscopic sections were prepared from the scaffolds after two weeks of culture with
-	stem cells and studied by histological methods. The interactions of scaffolds with MSCs were
Key words:	also studied by electron microscopy. Histological and electron microscopy studies revealed
·	human mesenchymal stem cell adhesion, migration, division and maintenance during the 14
Extracellular matrix	days of culture <i>in vitro</i> . According to the results, scaffolds prepared from rat intestine matrix
Large Intestine	could be a suitable scaffold for studying in vitro cell behaviors such as division, migration and
Mesenchymal stem cells	attachment. These various behaviors of cultured cells might be due to inductive effects of the
Rat	extracellular matrix derived scaffold. However, more investigations are required to discover the
Scaffold	exact effects of this scaffold and its interactions with mesenchymal stem cells.
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مطالعه برون زیستی رویدادهای هیستولوژیکی برهم کنش بین داربست سلول زدایی شده روده بزرگ رت و سلول های بنیادی مزانشیمی مشتق از بافت چربی انسان

چکیدہ

هدف از این مطالعه بررسی بر هم کنش های بین داربست سلول زدایی شده روده بزرگ رت با سلول های بنیادی مزانشیمی مشتق از بافت چربی انسانی می باشد. روده بزرگ رت جداسازی و با استفاده از روش های فیزیکی وشیمیایی سلول زدایی گردید. سپس سلولهای بنیادی مزانشیمی مشتق از چربی انسانی بر روی داربست ها انتقال یافت. از داربستهای تهیه شده پس از گذشت دو هفته از کشت، مقاطع میکروسکوپی تهیه و مطالعه برهم کنش داربست و سلول های بنیادی مزانشیمی مشتق از چربی انسانی بر روی داربست ها انتقال یافت. از داربستهای تهیه شده پس از گذشت دو هفته از میکروسکوپ الکترونی در هفته دوم کشت، چسبندگی، مهاجرت، تقسیم و بقاء سلول های بنیادی مزانشیمی انسانی را نشان داد. طبق نتایج، ماتریکس مشتق از روده بزرگ رت می تواند داربست مناسی و میکروسکوپ الکترونی در هفته دوم کشت، چسبندگی، مهاجرت، تقسیم و بقاء سلول های بنیادی مزانشیمی انسانی را نشان داد. طبق نتایج، ماتریکس مشتق از روده بزرگ رت می تواند داربست مناسی و میکروسکوپ الکترونی در هفته دوم کشت، چسبندگی، مهاجرت، تقسیم و بقاء سلول های بنیادی مزانشیمی انسان داد. طبق نتایج، ماتریکس مشتق از روده بزرگ رت می تواند داربست مناسی و جهت بررسی رفتارهای سلولی از قبیل تقسیم، مهاجرت و چسندگی سلولی باشد. انواع رفتارهای سلولی مشاهده شده احتمالاً به دلیل اثرات القایی داربست مشتق از ماتریکس خارج سلولی می باشد. البته آزمایش های بیشتری جهت شناسایی این گونه اثرات القایی داربست های می می و به هم کنش آنها با سلول های بنیادی مزانشیمی همی ا

واژه های کلیدی: داربست، رت، روده بزرگ، سلول های بنیادی مزانشیمی، ماتریکس خارج سلولی

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Introduction

Cells are able to interact with their surrounding extracellular matrix (ECM), which regulates the cellular behaviors by affecting on morphology, survival, proliferation, migration and differentiation of the cells. The scaffold acts as a template for cell organization and tissue development in tissue engineering process. Biologic scaffolds prepared from ECM of decellularized mammalian tissues have been shown to facilitate constructive remodeling in injured tissues.^{1,2} Decellularization is an important process to prepare an ECM derived scaffold. Many methods including physical, chemical and enzymatic protocols have been developed to reach the goal of decellularization.² A wide range of decellularized tissues, which retain both structure and molecules of the ECM have been studied for tissue engineering and regenerative medicine applications.³⁻⁸ The ECM is a molecular complex composed of molecules like collagen, elastin, glycoproteins, proteoglycans, glycosaminoglycans and proteins like growth factors, cytokines, enzymes and their inhibitors and plays role in various processes like cell adhesion, growth, migration and differentiation.9-12

We have focused on using human adipose derived mesenchymal stem cells (AD-MSCs) because they are an attractive and readily available source of adult stem cells, which due to ease of harvest, abundance and their immunomodulating properties are popular for use in many stem cell applications. They have been widely studied as an autologous mesenchymal cell source to produce chondrocytes, osteoblasts, and fibroblasts.¹²⁻¹⁶ This study was aimed to develop a decellularized rat large intestine scaffold using a combination of physical and chemical methods and then investigate the inductive effects of this scaffold on seeded AD-MSCs.

Materials and Methods

Decellularization process. In this experimental research, adult male Wistar rats (n = 4) weighting 250 -300 g were used. Animal experiments were performed according to the Iranian Council for the Use and Care of Animals Guidelines and were approved by the Animal Research Ethical Committee of Ferdowsi University of Mashhad, Mashhad, Iran. After removing the large intestine from male Wistar rats, it was washed with normal saline, and dissected in cylindrical shapes with 7 mm height. Intestine pieces were washed with sterile phosphatebuffered saline (PBS), immersed in liquid nitrogen (– 196 °C) for 2 min and thawed in distilled water and then PBS at room temperature for 5 min. The freeze/thaw process, which leads to cell lysis, was repeated five times. In the chemical phase of decellularization, specimens were treated with 1% (*w*/*v*) sodium dodecyl sulfate (SDS) solution (Merck, Darmstadt, Germany) for 24 hr at 37 °C.

Then, in order to reduce residual SDS from the scaffolds and to sterilize them, two washing steps were performed. Hence, specimens were washed first with 70% ethanol to remove residual SDS from tissues and a second wash with PBS was performed for 60 min at room temperature to complete the decellularization process.¹⁷

Cell seeding and culture method. The scaffolds were cultivated with the AD-MSCs expressing green fluorescent protein (GFP).¹⁸ In this regard, after sterilization, decellularized scaffolds were transferred to 12-well plates and seeded with 100 μ L aliquots containing 5 × 10⁵ cells and incubated at 37 °C with 5% CO₂ in air for 1 hr to allow cell attachment. In the final step, seeded scaffolds were immersed in 2 mL Dulbecco's modified Eagle's medium (Gibco, Paisley, Scotland) supplemented with 15% fetal bovine serum (Gibco) and 100 μ L penicillin/streptomycin (Biosera, Sussex, UK), which was changed every two day. Unseeded scaffolds were used as controls, and all samples were subjected to histological staining and scanning electron microscopy on day 14 after cell seeding.

Histological studies. All samples were fixed in 4% paraformaldehyde solution and dehydrated through a graded series of ethanol, embedded in paraffin, cross-sectioned at a thickness of 5 μ m with a microtome (Leits, Vienna, Austria), deparaffinized by xylene, rehydrated, and stained appropriately. To determine construct cellularity, hematoxylin and eosin (H & E) staining was used. To detect the labeled AD-MSCs, the sections were deparaffinized and observed by a fluorescent microscope.

Scanning electron microscopy (SEM). Scanning electron micrographs were taken to examine the surface topology of prepared scaffolds. In order to prepare samples for electron microscopy, specimens were fixed with 2.5% gluteraldehyde for 24 hr at room temperature and then washed with PBS for three times. Then, they were dehydrated in an ethanol-graded series (20%, 50%, 70%, 90%, 100%). Subsequently, the samples were examined under a scanning electron microscope (Leo VP 1450; Carl-Zeiss, Oberkochen, Germany) after coating with gold.

Transmission electron microscopy (TEM). For TEM evaluation, specimens were fixed with gluteraldehyde and 1% osmium tetroxide and dehydrated with incremental concentrations of ethanol. Specimens were placed in propylene oxide for 30 min, and finally placed in pure resin for 30 min (Araldite 502 resin kit; TAAB, Aldermaston, UK). The specimens were segmented into a thickness of 80 nm with ultra-microtome (LKB, Bromma, Sweden). These sections were studied and photographed with a TEM (Leo 910; Carl-Zeiss, Oberkochen, Germany).

Results

Acombination of physical and chemical decellularization methods was used in this research. Snap freeze-thaw using liquid nitrogen as a physical method and 24 hr treatment with 1% SDS as chemical method, resulted in elimination of cells while preserving intestine structure. AD-MSCs were seeded on the scaffolds for up to two weeks. On day 14, AD-MSCs were spread on scaffold surface and migration took place inside the matrix. The morphology and attachment of seeded cells on the scaffold are illustrated in Figure 1. The AD-MSCs were able to form epithelium-like structures at two weeks after culture. Penetration and survival of GFP labeled AD-MSCs were detected, two weeks after culture (Fig. 2). The SEM micrographs revealed preservation of collagen and elastin fibers in decellularized scaffolds (Fig. 3). The SEM micrographs of seeded scaffolds also demonstrated the adherence and attachment of AD-MSCs to scaffolds two weeks after culture (Fig. 4). The TEM micrographs revealed cells and also cell division after initial seeding (Fig. 5).



Fig. 1. Transverse sections prepared from large intestine scaffold. **A** and **B**) after culture with AD-MSCs (arrows); **C**) control scaffold (H & E, A and C 40×; B 400×). AD-MSCs were spread on scaffold surface and migration took place inside the matrix. The morphology and attachment of seeded cells on the scaffold are illustrated.



Fig. 2. Transverse sections prepared from large intestine scaffold. GFP labeled AD-MSCs (arrows) are attached on the surface of the scaffold (200×).



Fig. 3. SEM images of the decellularized large intestine tissue. SEM of scaffold demonstrated the collagen fibers (arrows) in decellularized scaffold.



Fig. 4. A, B) SEM images of the decellularized large intestine scaffold after two weeks of culture with AD-MSCs. Cell attachments are obvious on the surface of the scaffold (arrows).

forces and the mechanical stiffness, or elasticity of the ECM can have major influence on cell behaviors such as migration, apoptosis, and proliferation.²⁵⁻²⁷

Beckstead et al. compared esophageal epithelial cell interactions with Allo-Derm, the decellularized skin product, and degradable polyesters, and demonstrated that esophageal epithelial cell adhesion and proliferation were supported by both natural and synthetic scaffolds, however, the natural scaffold showed superior morphology compared to the synthetic scaffold.²⁸ Rodrigues et al. showed that fibroblast seeding onto acellular dermal matrix for 14 days can allow good conditions for cell adhesion and spreading on the matrix, whereas, migration inside the matrix was limited.²⁹ In the present study, although cells adhered and spread on decellularized intestine scaffold surface, the low number of cells inside the matrix, suggested that during the culture interval cells were unable to alter the dense organization of the collagen bundles, which acted as a physical barrier. The SEM and TEM images proved successful adhesion and proliferation of cells on the scaffold at 14 days after culture and indicated the microstructure of decellularized scaffolds with a suitable interconnected structure which facilitated cell adhesion and the transportation of nutrients and waste during cell culture. Findings of the present study showed that cell division was detectable in penetrated AD-MSCs in to the scaffold after two weeks of culture. These various behaviors of cultured cells might be due to inductive effects of the large intestine ECM derived scaffold. Several studies have been performed to demonstrate the inductive effects of different ECM scaffolds on behaviors of seeded cells. For instance, Lindberg and Badylak demonstrated the ability of small intestinal submucosa ECM to support epidermal cell and fibroblast attachment, migration, proliferation and differentiation with deposition of basement membrane components.²⁶ Ozeki et al. seeded esophageal epithelial cells inside decellularized esophagus and demonstrated the potential of the ECM derived scaffold to induce the polarity, proliferation and differentiation of seeded cells.³⁰ In agreement with these studies, the results of the present study demonstrated retaining of main ECM components such as collagen and elastin after decellularization, and also showed migration and proliferation of cultured AD-MSCs. It could be concluded that decellularized scaffold utilized in this study may have induced the adhesion, migration and proliferation of cultured AD-MSCs. More experiments to detect the differentiation of penetrated cells into the scaffold are required to improve our knowledge about cell - matrix interactions.

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Fig. 5. TEM image of the decellularized large intestine scaffold after two weeks of culture with AD-MSCs. **A, B)** AD-MSCs are obvious in the scaffold. Cell division is indicated by arrow.

Discussion

The aim of this study was to investigate the interactions between rat decellularized intestine scaffold with human AD-MSCs. Tissue engineering systems are being used as model systems to study cellular behaviors. It is essential to understand the mechanisms involved in interaction of cells with their ECM. The cells of each tissue are able to interact with their surrounding (i.e. ECM), which regulates the cell behaviors by affecting on morphology, survival, proliferation, migration and differentiation of the cells. Several researches have focused on interactions between various cell types and a wide range of synthetic or natural scaffolds to find pieces of the puzzle in tissue engineering. Several studies have been performed to demonstrate the inductive effects of different ECM scaffolds on behaviors of seeded cells. The chemical composition and physical properties of natural ECM have been shown to prominently influence cell morphology, motility, and migration. Cell-ECM interactions are accompanied by cytoskeletal action, matrix remodeling and contraction, which modulate cell fate.¹⁹⁻²⁴ Furthermore, the relationship between contractile forces, resulting in tensile stresses in the cytoskeleton

B Fig. 5. TEM image of the decellularized large intestine scaffold



References

- 1. Daley WP, Peters SB, Larsen M. Extracellular matrix dynamics in development and regenerative medicine. J Cell Sci 2008; 121: 255-264.
- Wolf MT, Daly KA, Reing JE, et al. Biologic scaffold composed of skeletal muscle extracellular matrix. J Biomaterials 2012; 33: 2916-2925.
- 3. Crapo PM, Gilbert TW, Badylak SF. An overview of tissue and whole organ decellularization processes. J Biomaterials 2011; 32: 3233-3243.
- 4. Lehr EJ, Rayat GR, Chiu B, et al. Decellularization reduces immunogenicity of sheep pulmonary artery vascular patches. J Thorac Cardiovasc Surg 2010; 141: 1056-1062.
- 5. Guo SZ, Ren XJ, Wu B, et al. Preparation of the acellular scaffold of the spinal cord and the study of biocompatibility. J Spinal Cord 2010; 48: 576-581.
- 6. Baiguera S, Jungebluth P, Burns A, et al. Tissue engineered human tracheas for *in vivo* implantation. J Biomaterials 2010; 31: 8931-8938.
- Yang B, Zhang Y, Zhou L, et al. Development of a porcine bladder acellular matrix with well-preserved extracellular bioactive factors for tissue engineering. J Tissue Eng Part C Methods 2010; 16: 1201-1211.
- 8. Tan JY, Chua CK, Leong KF, et al. Esophageal tissue engineering: An in-depth review on scaffold design. J Biotechnol Bioeng 2012; 109: 1-15.
- 9. Hou N,Cui P,Luo J, et al. Tissue-engineered larynx using perfusion-decellularized technique and mesenchymal stem cells in a rabbit model. J Acta Oto-Laryngol 2011; 131: 645-652.
- 10. Badylak SF, Freytes DO, Gilbert TW. Extracellular matrix as a biological scaffold material: Structure and function. J Acta Biomater 2009; 5: 1-13.
- 11. Pariente JL, Kim BS, Atala A. *In vitro* biocompatibility evaluation of naturally derived and synthetic biomaterials using normal human bladder smooth muscle cells. J Urol 2002; 167:1867.
- 12. Lee M, Chang PC, Dunn JC. Evaluation of small intestinal submucosa as scaffolds for intestinal tissue engineering. J Surg Res 2008; 147:168.
- 13. Zuk PA, Zhu M, Mizuno H, et al. Multilineage cells from human adipose tissue: Implications for cell-based therapies. J Tissue Eng 2001; 7: 211-226.
- 14. Chen Q, Yang Z, Sun S, et al. Adipose-derived stem cells modified genetically *in vivo* promote reconstruction of bone defects. J Cytotherapy 2010; 12: 831-840.
- 15. Kajiyama H, Hamazaki TS, Tokuhara M, et al. Pdx1transfected adipose tissue-derived stem cells differentiate into insulin-producing cells *in vivo* and reduce hyperglycemia in diabetic mice. Int J Dev Biol 2010; 54: 699-705.
- 16. Li K, Han Q, Yan X, et al. Not a process of simple vicariousness, the differentiation of human adipose-

derived mesenchymal stem cells to renal tubular epithelial cells plays an important role in acute kidney injury repairing. J Stem Cells Dev 2010; 19: 1267-1275.

- 17. Abousleiman RI, Reyes Y, Fetridge P, et al. The human umbilical vein: A novel scaffold for musculo-skeletal soft tissue regeneration. JArtif Organs 2008; 32: 735-741.
- 18. Mashadrizeh HA, Bahrami AR, Moghaddam MM, et al. Human adipose-derived mesenchymal stem cells can survive and integrate into the adult rat eye following xenotransplantation. Xenotransplantation 2013; 20: 165-176.
- 19. Ketchedjian A, Jones AL, Krueger P, et al. Recellularization of decellularized allograft scaffolds in ovine great vessel reconstructions. J Ann Thorac Surg 2005; 79: 888-896.
- 20. Leong MF, Rasheed MZ, Lim TC, et al. *In vitro* cell infiltration and *in vivo* cell infiltration and vascularization in a fibrous, highly porous poly (DL-lactide) scaffold fabricated by cryogenic electrospinning technique. J Biomed Mater Res 2009; 91: 231-240.
- 21. Ma R, Li M, Luo J, et al. Structural integrity, ECM components and immunogenicity of decellularized laryngeal scaffold with preserved cartilage. J Biomaterials 2013; 34: 1790-1798.
- 22. Hung SH, Su CH, Lee FP, et al. Larynx decellularization: Combining freeze-drying and sonication as an effective method. J Voice 2013; 27: 289-294.
- 23. Kanungo BP, Gibson LJ. Density-property relationships in collagen-glycosaminoglycan scaffolds. J Acta Biomater 2010; 6: 344-353.
- 24. Hadjipanayi E, Mudera V, Brown RA. Close dependence of fibroblast proliferation on collagen scaffold matrix stiffness. J Tissue Eng Regen Med 2009; 3: 77-84.
- 25. Guilak F, Cohen DM, Estes BT, et al. Control of stem cell fate by physical interactions with the extracellular matrix. J Cell Stem Cell 2009; 5: 17-26.
- 26. Lindberg K, Badylak SF. Porcine small intestinal submucosa: A bioscaffold supporting *invitro* primary human epidermal cell differentiation and synthesis of basement membrane proteins. J Burns 2001; 27: 254-266.
- 27. Zhang Y, Lin HK, Frimberger D, et al. Growth of bone marrow stromal cells on small intestinal submucosa: an alternative cell source for tissue engineered bladder. Br J Urol Int 2005; 96: 1120-1125.
- 28. Becksteada BL, Pana S, Bhranyb AD, et al. Esophageal epithelial cell interaction with synthetic and natural scaffolds for tissue engineering. J Biomaterials 2005; 26: 6217-6228.
- 29. Rodrigues AZ, Oliveira PT, Novaes AB, et al. Evaluation of *in vitro* human gingival fibroblast seeding on acellular dermal matrix. Braz Dent J 2010; 21: 179-185.
- Ozeki M, Narita Y, Kagami H, et al. Evaluation of decellularized esophagus as a scaffold for cultured esophageal epithelial cells. J Biomed Mater Res A 2006; 79: 771-778.