

# Semiquantitative assessment of osteoblastic, osteolytic, and mixed lytic-sclerotic bone lesions on fluorodeoxyglucose positron emission tomography/computed tomography and bone scintigraphy

## ABSTRACT

Bone scintigraphy is widely used to detect bone metastases, particularly osteoblastic ones, and F-18 fluorodeoxyglucose (FDG) positron emission tomography (PET) scan is useful in detecting lytic bone metastases. In routine studies, images are assessed visually. In this retrospective study, we aimed to assess the osteoblastic, osteolytic, and mixed lytic-sclerotic bone lesions semiquantitatively by measuring maximum standardized uptake value ( $SUV_{max}$ ) on FDG PET/computed tomography (CT), maximum lesion to normal bone count ratio ( $ROI_{max}$ ) on bone scintigraphy, and Hounsfield unit (HU) on CT. Bone scintigraphy and FDG PET/CT images of 33 patients with various solid tumors were evaluated. Osteoblastic, osteolytic, and mixed lesions were identified on CT and  $SUV_{max}$ ,  $ROI_{max}$ , and HU values of these lesions were measured. Statistical analysis was performed to determine if there is a difference in  $SUV_{max}$ ,  $ROI_{max}$ , and HU values of osteoblastic, osteolytic, and mixed lesions and any correlation between these values. Patients had various solid tumors, mainly lung, breast, and prostate cancers. There were 145 bone lesions (22.8% osteoblastic, 53.1% osteolytic, and 24.1% mixed) on CT. Osteoblastic lesions had a significantly higher value of CT HU as compared to osteolytic and mixed lesions ( $P < 0.01$ ). There was no significant difference in mean  $ROI_{max}$  and mean  $SUV_{max}$  values of osteolytic and osteoblastic bone lesions. There was no correlation between  $SUV_{max}$  and  $ROI_{max}$ ,  $SUV_{max}$  and HU, and  $ROI_{max}$  and HU values in osteolytic, osteoblastic, and mixed lesions ( $P > 0.05$ ). Not finding a significant difference in  $SUV_{max}$  and  $ROI_{max}$  values of osteoblastic, osteolytic, and mixed lesions and also lack of correlation between  $SUV_{max}$ ,  $ROI_{max}$ , and HU values could be due to treatment status of the bone lesions, size of the lesion, nonmetastatic lesions, erroneous measurement of  $SUV_{max}$  and  $ROI_{max}$ , or varying metabolism in bone metastases originating from various malignancies.

**Keywords:** Bone scintigraphy, fluorodeoxyglucose positron emission tomography/computed tomography, osteoblastic, osteolytic, semiquantitative

## INTRODUCTION

Bone is one of the most common sites for metastatic spread of tumors. Tumors most commonly metastasizing to bone are prostate, breast, kidney, lung, and thyroid. In children, common causes of skeletal metastases include neuroblastoma, Ewing sarcoma, and osteosarcoma. In men, carcinoma of the prostate accounts for 60% of bone metastases, while in women, breast cancer accounts for 70% of such metastases. Metastases typically involve the axial skeleton, which is the region rich in red bone marrow. Bone metastases could be purely osteoblastic, mixed osteoblastic/osteolytic, or

osteolytic. Prostate cancer metastases are purely osteoblastic, whereas metastases of thyroid and kidney carcinomas are

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**How to cite this article:** Gurkan G, Sarikaya I, Sarikaya A. Semiquantitative assessment of osteoblastic, osteolytic, and mixed lytic-sclerotic bone lesions on fluorodeoxyglucose positron emission tomography/computed tomography and bone scintigraphy. World J Nucl Med 2019;18:132-6.

Access this article online	
<b>Website:</b> www.wjnm.org	<b>Quick Response Code</b> 
<b>DOI:</b> 10.4103/wjnm.WJNM_31_18	

purely lytic. Mixed osteolytic/osteoblastic lesions occur in carcinomas of the breast, lung, cervix, ovary, and testis.

Bone metastasis can be identified only when the distortion of the compact bone structure in the direct X-ray and computed tomography (CT) reach a certain level. Bone scintigraphy is the easiest and cheapest way to scan the whole body with a higher sensitivity than the specificity.<sup>[1-6]</sup> Whole body bone scan allows scanning the whole skeletal system. Single photon emission CT (SPECT), particularly SPECT/CT, further increases the sensitivity and specificity of bone scintigraphy for the detection of bone metastases. F-18 fluorodeoxyglucose (FDG) positron emission tomography/CT (PET/CT) imaging is commonly used in oncology for staging of the tumors as well as detecting recurrences and assessing response to treatments. While bone scintigraphy assesses the osteoblastic activity of bone metastases, FDG PET scan evaluates the glucose metabolism/glycolysis of the lesions. Bone scintigraphy has higher sensitivity in detecting osteoblastic bone metastases than osteolytic ones.<sup>[7,8]</sup> In detecting osteolytic bone metastases, FDG PET/CT has been reported to be superior to bone scintigraphy.<sup>[3,4,7]</sup> Metastatic bone lesions can be detected in early stage on magnetic resonance imaging (MRI) with the signal changes in the bone marrow which is hypointense in suppressed T1 images and hyperintense in T2 images. Diffusion-weighted whole-body MRI was found to be equivalent to bone scintigraphy and FDG PET/CT in assessing bone metastases in non-small cell lung cancer.<sup>[9]</sup> There are various studies comparing FDG PET/CT with bone scintigraphy visually for the detection of bone metastases.<sup>[7,10-17]</sup> However, to the best of our knowledge, there is no study determining and comparing semiquantitative values of bone lesions on bone scintigraphy and FDG PET in patients with malignancies.

In this study, we aimed to determine semiquantitative measurement values of osteolytic, osteoblastic, and mixed-type bone lesions on bone scintigraphy and FDG PET/CT images in patients with solid organ malignancies.

## MATERIALS AND METHODS

Bone scintigraphy and F-18 FDG PET/CT images of patients with various solid tumors were selected for further analysis. This retrospective study was approved by the Ethics Committee of Trakya University Faculty of Medicine.

For bone scintigraphy, the patients were injected 20–25 mCi (740–925 MBq) technetium-99 m methylene diphosphonate, and images were obtained 2–4 h after the injection. Images included anterior and posterior whole body (10–15 cm/min

scan speed), and SPECT (64 images for 20–40 s each), and spot (500–1000 kct) images of the area of interest. Images were obtained at dual-head gamma camera (Siemens E. CAM, Erlangen, Germany and Philips BrightView, Milpitas, CA, USA) using low-energy high-resolution collimator with 120 keV energy settings and 20% window. 1024 × 512 matrix was used for whole body images and 64 × 64 matrix for SPECT. Images were evaluated visually and semiquantitatively. For semiquantitative analysis, a region of interest (ROI) was drawn over the bone lesion and normal bone to obtain maximum lesion to normal bone count ratio (ROI<sub>max</sub>). JETStream Workspace version 3.0 was used for this semiquantitative analysis.

For FDG PET/CT study, the patients fasted 6 h before imaging. Blood glucose level was checked before FDG injection. The patients were given oral contrast 1 h before the study. FDG was injected when the blood glucose level was <150 mg/dl. PET/CT images were obtained at GE discovery 8 PET/CT camera (GE Medical Systems, Waukesha, USA) 60 min following intravenous injection of 296–555 MBq (8–15 mCi) F-18 FDG. Before PET image acquisition, a low-dose CT was obtained for attenuation correction and anatomic localization purposes. PET acquisition was 3 min/bed from top of the head to mid thighs. PET images were corrected for attenuation on the basis of the CT data and reconstructed using a standard iterative algorithm and reformatted into transaxial, coronal, and sagittal views. Maximum intensity projection images were also generated. Both attenuation corrected and non-corrected PET images as well as PET/CT fusion images were visually evaluated. Low-dose CT images were also assessed by a radiologist to determine osteoblastic, osteolytic, and mixed lesions which are consistent or suspicious for bone metastases. For semiquantitative analysis, maximum standardized uptake value (SUV<sub>max</sub>), and Hounsfield unit (HU) values were measured from the lesions.

Number Cruncher Statistical System 2007 and PASS 2008 Statistical Software (Utah, USA) program were used for statistical analysis. Mann–Whitney U, Spearman's correlation coefficient, Pearson's Chi-squared, and Kruskal–Wallis tests were used.

## RESULTS

A total of 33 patients were included in this study. Fifteen patients were female and 18 were male with an age range of 37–79 years (mean 60.09 ± 8.77). Patients had various solid tumors including lung cancer (42.4%), breast cancer (30.4%), prostate cancer (6.1%), and other (endometrial cancer, pancreatic cancer, malignant melanoma, parathyroid tumor,

renal cell carcinoma, soft-tissue sarcoma, and oral cavity tumor). There were 145 bone lesions (22.8% osteoblastic, 53.1% osteolytic, and 24.1% mixed osteoblastic-osteolytic metastases) on CT. Distribution of bone metastases included pelvis (24.1%), lower thoracic spine (17.9%), lumbar spine (16.6%), ribs and sternum (10.3%), lower limbs (9.7%), upper thoracic spine (7.6%), upper limbs (4.8%), and other regions (9%).

Mean  $SUV_{max}$  of osteolytic bone lesions ( $7.73 \pm 4.35$ ) was higher than mean  $SUV_{max}$  of osteoblastic ( $6.84 \pm 3.03$ ) and mixed ( $6.88 \pm 3.10$ ) lesions, but it was not statistically significant (0.876) [Tables 1 and 2].

Mean  $ROI_{max}$  of osteoblastic bone lesions ( $6.42 \pm 4.22$ ) was higher than mean  $ROI_{max}$  of osteolytic lesions ( $5.33 \pm 3.60$ ), but it was not statistically significant (0.077) [Tables 1 and 2]. Mean  $ROI_{max}$  of mixed metastases was  $6.32 \pm 4.03$ .

Mean HU  $SUV_{max}$  of osteoblastic bone lesions ( $344.09 \pm 140.62$ ) was higher than mean HU of osteolytic ( $233.39 \pm 125.29$ ) and mixed ( $254.86 \pm 105.69$ ) lesions and it was statistically significant ( $P < 0.01$ ) [Tables 1 and 2].

In osteoblastic metastases, there was no correlation between  $SUV_{max}$  and  $ROI_{max}$ ,  $SUV_{max}$  and HU, and  $ROI_{max}$  and HU values [Table 3].

In osteolytic metastases, there was no correlation between  $SUV_{max}$  and  $ROI_{max}$ ,  $SUV_{max}$  and HU, and  $ROI_{max}$  and HU values [Table 3].

In mixed metastases, there was no correlation between  $SUV_{max}$  and  $ROI_{max}$ ,  $SUV_{max}$  and HU, and  $ROI_{max}$  and HU values [Table 3].

## DISCUSSION

Bone scintigraphy and FDG PET/CT imaging play an important role in the management of patients with malignancies. Bone scintigraphy images, whole body, spot, or SPECT, are usually assessed visually. Several studies have been published on

semiquantitative analysis of bone scintigraphy. Erdi *et al.* developed a semiautomated image segmentation program to determine the total fraction of skeletal involvement with bone metastases.<sup>[18]</sup> Bone scan lesion area, bone scan lesion intensity, and bone scan lesion count were calculated from identified lesions to determine response to treatment.<sup>[19]</sup> Regional activity concentration of the injected tracer was measured on SPECT images.<sup>[20]</sup> In our study, we obtained maximum uptake ratio of bone lesion to normal bone to determine the degree of osteoblastic activity of the bone lesions.

$SUV_{max}$  is a commonly used parameter on FDG PET/CT studies to assess the metabolic activity of the lesions which can help to differentiate benign from malignant lesion and determine the aggressiveness of the tumor. In a study by Cook *et al.*, 81% of lytic bone metastases showed increased FDG uptake; however, only 40% of sclerotic bone lesions were detected on FDG PET.<sup>[21]</sup> Abe *et al.* found that FDG PET was superior to bone scintigraphy in detecting osteolytic metastases, while bone scintigraphy was superior to FDG PET in detecting osteoblastic lesions.<sup>[12]</sup> In a study by Hur *et al.*,  $SUV_{max}$  was significantly higher in osteolytic metastasis than in osteoblastic lesions.<sup>[16]</sup> Cook *et al.* found that the FDG uptake of osteoblastic metastases (mean  $SUV_{max}$ : 0.95) was significantly lower than the FDG uptake of osteolytic metastases (mean  $SUV_{max}$ : 6.77).<sup>[21]</sup>

As opposed to literature, in our study, we did not find a significant difference in mean  $SUV_{max}$  and  $ROI_{max}$  values of osteoblastic, osteolytic, and mixed lesions and there was also no correlation between the  $SUV_{max}$ ,  $ROI_{max}$ , and HU values. Various factors may alter the mean  $SUV_{max}$  and  $ROI_{max}$  values. In our cases, some of the lesions seen on CT could be active metastatic disease and some inactive. For example, some of the sclerotic lesions on CT could be active osteoblastic metastases and some could be treated old lesions. Increased uptake on bone scan in a sclerotic lesion could be due to flare phenomenon in a treated osteoblastic, osteolytic, or mixed metastases.<sup>[22]</sup> Lack of increased activity on bone scan in a sclerotic lesion may be due to treated very old osteoblastic

**Table 1: Kruskal-Wallis test comparing mean maximum standardized uptake value, region of interest, and hounsfield unit values in osteoblastic, osteolytic and mixed lesions**

	Metastaz tipi			P
	Osteoblastic Mean ± SD (median)	Osteolytic Mean ± SD (median)	Mixed Mean ± SD (median)	
PET $SUV_{max}$	6.84 ± 3.03 (6)	7.73 ± 4.35 (6.3)	6.88 ± 3.10 (5.9)	0.876
Bone $ROI_{max}$	6.42 ± 4.22 (5.2)	5.33 ± 3.60 (4.2)	6.32 ± 4.03 (5.1)	0.077
CT HU	344.09 ± 140.62 (347)	233.39 ± 125.29 (203)	254.86 ± 105.69 (222)	0.001**

\*\* : Significant,  $P < 0.01$ ; HU: Hounsfield unit;  $SUV_{max}$ : Maximum standardized uptake value; PET: Positron emission tomography; CT: Computed tomography;  $ROI_{max}$ : Maximum region of interest; SD: Standard deviation

**Table 2: Post hoc Mann-Whitney U-test results**

	Osteoblastic/ osteolytic (P)	Osteoblastic/ mixed (P)	Osteolytic/ mixed (P)
PET SUV <sub>max</sub>	0.737	0.893	0.638
Bone ROI <sub>max</sub>	0.098	0.995	0.053
CT HU	0.001**	0.003**	0.155

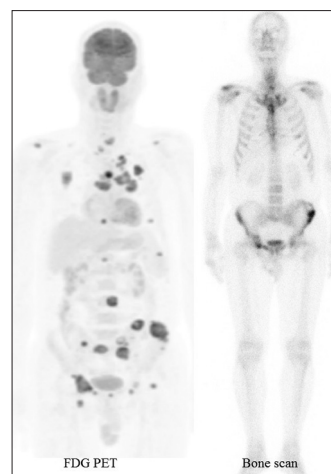
\*\* : Significant,  $P < 0.01$ ; HU: Hounsfield unit; SUV<sub>max</sub>: Maximum standardized uptake value; PET: Positron emission tomography; CT: Computed tomography; ROI<sub>max</sub>: Maximum region of interest

**Table 3: Spearman's rho correlation analysis results in between Maximum standardized uptake value, Maximum region of interest, and hounsfield unit values**

	PET SUV <sub>max</sub> / bone ROI <sub>max</sub>	PET SUV <sub>max</sub> / CT HU	BoneROI <sub>max</sub> / CT HU
Osteoblastic			
<i>r</i>	0.107	0.064	0.075
<i>P</i>	0.552	0.723	0.679
Osteolytic			
<i>r</i>	-0.194	0.159	-0.216
<i>P</i>	0.091	0.167	0.060
Mixed			
<i>r</i>	-0.160	-0.180	0.086
<i>P</i>	0.359	0.301	0.623

HU: Hounsfield unit; SUV<sub>max</sub>: Maximum standardized uptake value; PET: Positron emission tomography; CT: Computed tomography; ROI<sub>max</sub>: Maximum region of interest

metastasis. Sclerotic changes on CT in a treated bone metastasis may last longer than osteoblastic activity on bone scan. Increased uptake on bone scan due to flare is usually not seen on follow-up bone scan at 6 mos.<sup>[23]</sup> Flare phenomenon in bone metastases has also been reported with FDG PET/CT study.<sup>[24]</sup> Development of fracture in a lytic lesion may cause increased uptake on bone scan. Some sclerotic, lytic, or mixed lesions on CT may not be metastatic and could be due to various benign pathologies such as cyst or hemangioma. Measurement of SUV<sub>max</sub> is also affected by various factors such as blood glucose level at the time of injection, duration of the uptake period, body weight, and body composition. SUV<sub>max</sub> may be overestimated in sclerotic lesions due to over attenuation correction by CT, and it may be underestimated in osteolytic lesions due to under attenuation correction by CT. In small lesions, partial volume averaging may cause erroneous results for bone scintigraphy and FDG PET scan. For example, uptake of a small osteolytic lesion on bone scintigraphy may be overestimated and uptake of a small osteoblastic lesion may be underestimated. ROI<sub>max</sub> value of bone lesion is affected by underlying normal bone uptake on planar imaging. SPECT or SPECT/CT may provide more accurate ROI<sub>max</sub> values. Lytic lesions, particularly large ones, are not always seen cold on bone scan as seen in Figure 1 which can further increase mean value of the ROI<sub>max</sub>. Our study consisted of various malignancies. Metabolic behavior of the osteoblastic and osteolytic bone lesions may vary in malignancies.



**Figure 1: Fluorodeoxyglucose positron emission tomography/computed tomography maximum intensity projection image and bone scan in a patient with non-small cell lung cancer. Fluorodeoxyglucose positron emission tomography demonstrates multiple bone and lymph node metastases in addition to primary tumor in the left lung. Bone scan demonstrates metastasis in the left iliac bone and right acetabulum and superior pubic ramus. Computed tomography, not shown here, demonstrated multiple osteolytic bone metastases. Note that bone scan shows cold and hot pattern in the left iliac lytic lesion. There is also mildly increased uptake in right distal clavicle, sternum, and few left anterior ribs**

## CONCLUSION

We did not find a significant difference in SUV<sub>max</sub> and ROI<sub>max</sub> values of osteoblastic, osteolytic, and mixed lesions and also lack of correlation between SUV<sub>max</sub>, ROI<sub>max</sub>, and HU values which could be due to various technical or patient-related causes or varying metabolism of bone metastases from various malignancies. A study with a larger number of patients who had untreated and proven bone metastases and also using SPECT instead planar bone imaging can be valuable to assess the metabolic and osteoblastic activities of bone metastases.

## Financial support and sponsorship

Nil.

## Conflicts of interest

There are no conflicts of interest.

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