



ORIGINAL ARTICLE

# Efficiency of calcium phosphate composite nanoparticles in targeting Ehrlich carcinoma cells transplanted in mice



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## ABSTRACT

The present study aimed to investigate the mode of action of nano-CaPs *in vivo* as a therapy for solid tumor in mice. To achieve this goal, Ehrlich Ascites Carcinoma (EAC) was transplanted into 85 Swiss male albino mice. After nine days, the mice were divided into 9 groups. Groups 1 and 2 were allocated as the EAC control. Groups 3 and 4 were injected once intratumorally (IT) by nano-calcium phosphate (nano-CaP). Groups 5 and 6 received once intraperitoneal injection (IP) of nano-CaP. Groups 7, 8, and 9 received nano-CaP (IP) weekly. Blood samples and thigh skeletal muscle were collected after three weeks from groups 1, 3, 5, and 7 and after four weeks from groups 2, 4, 6, and 8. On the other hand, group 9 received nano-CaP (IP) for four weeks and lasted for three months to follow up the recurrence of tumor and to ensure the safety of muscle by histopathological analysis. Tumor growth was monitored twice a week throughout the experiment. DNA fragmentation of tumor cells was evaluated. In thigh tissue, norepinephrine, dopamine, serotonin (5HT), and gamma-aminobutyric acid (GABA) were measured. In serum, 8-Hydroxy-deoxyguanosine (8-OHDG), adenosine triphosphate (ATP), and vascular endothelial growth factor (VEGF) were analyzed. Histopathological and biochemical results showed a significant therapeutic effect of nano-CaP on implanted solid tumor and this effect

**Abbreviations:** EAC, Ehrlich Ascites Carcinoma; Nano-CaP, nano calcium phosphate; GABA, gamma aminobutyric acid; 5HT, serotonin; 8-OHDG, 8-hydroxy-deoxyguanosine; ATP, adenosine triphosphate; IP, intraperitoneal; IT, intratumoral; FAK, focal adhesion kinase; DNA, deoxyribonucleic acid; MAPK, mitogen-activated protein kinase; XRD, X-ray diffraction; FTIR, Fourier transform infrared; SEM, scanning electron microscopy; TEM, transmission electron microscope; RIR, reference intensity ratio; VEGFR2, vascular endothelial growth factor receptor 2.

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was more pronounced in the animals treated IP for four weeks. This improvement was evident from the repair of fragmented DNA, the significant decrease of caspase-3, 8-OHDG, myosin, and VEGF, and the significant increase of neurotransmitters (NA, DA, 5HT, and GABA). Additionally, histopathological examination showed complete recovery of cancer cells in the thigh muscle after three months.

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## Introduction

Cancer nanotechnology provides a unique approach and comprehensive technology against cancer through early diagnosis, prediction, prevention, and personalized therapy and medicine [1]. Nanoparticles provide opportunities for designing and tuning properties that are not possible with other types of therapeutic drugs due to its ability to interact with cells and tissues at a molecular level which provides them with a distinct advantage over other polymeric or macromolecular substances [2]. As with any cancer therapy, the key issue is to achieve the desired concentration of therapeutic agent in tumor sites, thereby destroying cancerous cells while minimizing damage to normal cells [3]. Frequent challenges encountered by current cancer therapies include nonspecific systemic distribution of antitumor agents, inadequate drug concentrations reaching the tumor site, intolerable cytotoxicity, limited ability to monitor therapeutic responses, and development of multiple drug resistance [4]. In addition to the complex physiological and biochemical factors tumoral processes involve, and numerous observations concluded that tumor cells, as biological entities, interact with their surrounding cells, lymphatic circulation, blood circulation and nervous system [5]. Thus, the use of biocompatible materials of biological origin is paramount for biomedical applications in supports, casings, or implants needed to integrate within the human body to minimize immune responses. Among them, calcium phosphate particles had a suppressive effect on the proliferation of tumor cells. Since it was almost impossible to excise malignant tumor

completely due to their capability of rapid proliferation, local invasion and distance migration, the influence of the nanoparticles of calcium phosphate with different morphology, size, and ions substitution on tumor cells, especially highly malignant ones, was significant in clinic [6]. The granular morphologies of the CaP nanoparticles (i.e., isotropic structure) are also likely to affect their biological effects [7]. So, these particles inhibit the proliferation of tumor cells and do not cause the threat for health.

Based on the effects of administration route, particle size and properties on biodistribution, a variety of nanoparticulate designs have been proposed for cancer therapy and diagnosis. Targeting of tumor tissues occurs through the extravasation of nanoparticles post-injection into the systemic blood circulation. The biodistribution of these particles is dependent on the characteristics of blood capillaries in the organs and tissues as well as the administration site, particle size and surface properties [8]. Even in intratumoral (i.t.) administration, understanding the mechanism of the extravasation is critical to retain the particles at the injection sites. In addition to such macro biodistribution of particles, their diffusion in the tissues, association to cells, internalization into the cells and intracellular distribution are important issues in cancer therapy and diagnosis [9]. Moreover, recent study has investigated the potential of calcium phosphate nanoparticles for transcutaneous vaccine delivery [10] and can be used also as multifunctional tools for near-infrared fluorescence (NIRF) optical imaging and Photodynamic therapy (PDT) [11]. The current study aimed to investigate the ability of nano-calcium

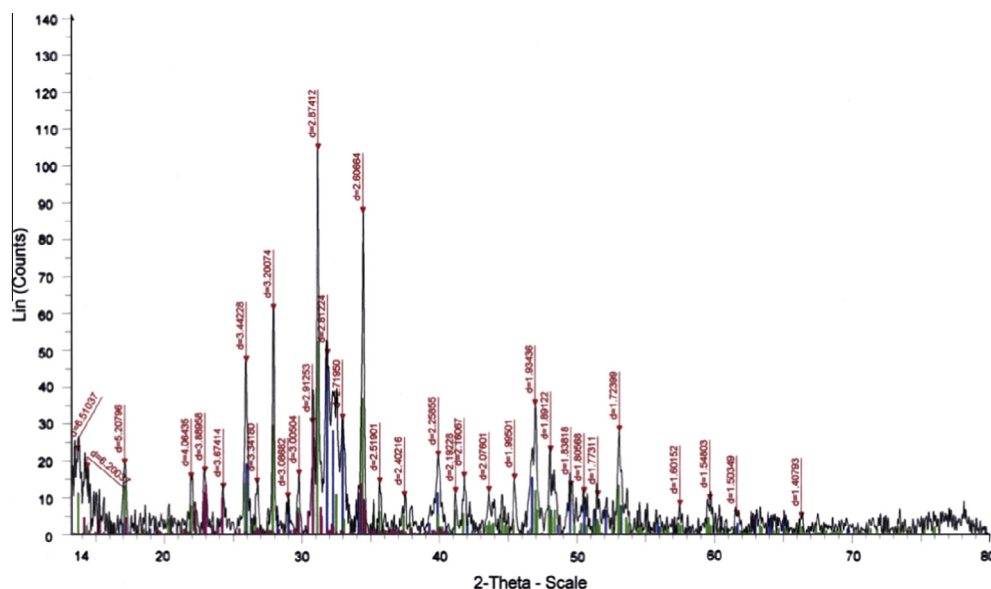
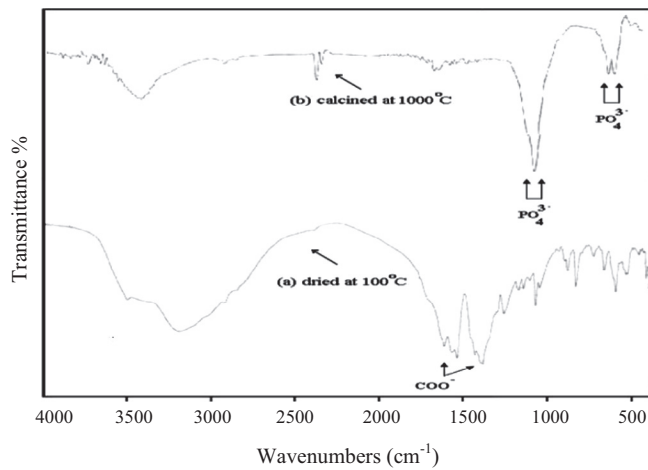


Fig. 1 XRD patterns of the sample prepared calcined at 1000 °C.



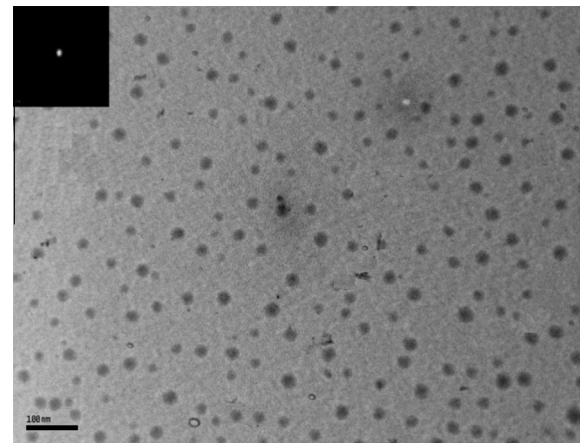
**Fig. 2** IR spectra of the sample prepared (a) dried at 100 °C and (b) calcined at 1000 °C.

phosphate particles to eliminate the implanted solid tumor in the thigh in addition to overcome the associated symptoms from affected skeletal muscle.

### Material and methods

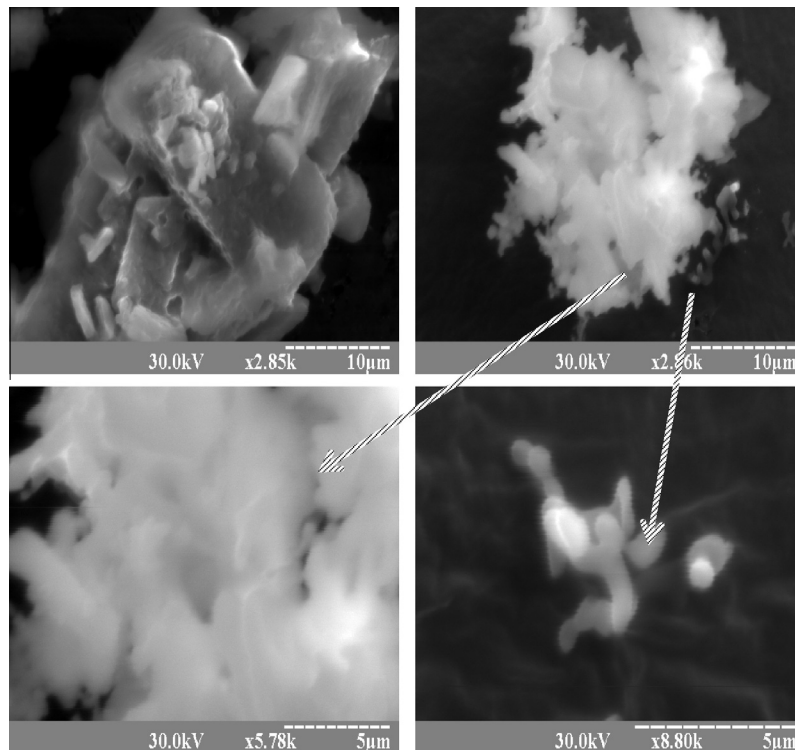
#### Particles preparation and characterization

A polymeric solution was prepared by dissolving 0.5 g of chitosan in 200 mL of 2% acetic acid while stirring for 24 h in 1-L flat round-bottomed flask. After complete dissolution of

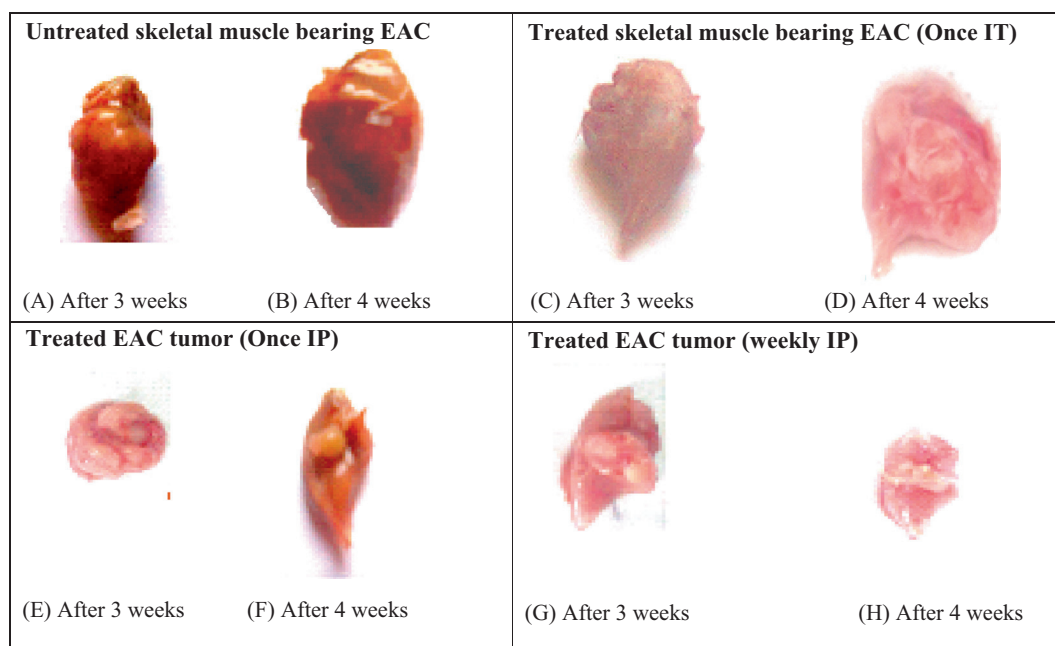


**Fig. 4** TEM micrograph analysis of synthesized materials with its diffraction pattern.

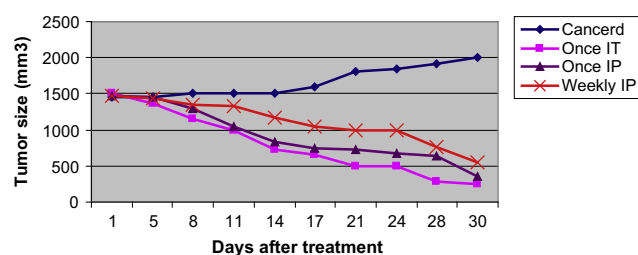
chitosan, a dissolved soluble calcium salt was added to polymeric media with stirring and heating until complete dissolution. Finally diammonium hydrogen orthophosphate was added to the mixture with natural Ca/P molar ratio while stirring and heating at 80 °C and completed to 500 mL with deionized water [12]. The final solution was filtrated and dried at 100 °C for 24 h then calcined at 1000 °C. The formed powder was characterized using The X-ray Diffraction (XRD), Fourier transform infrared (FTIR), Scanning electron microscopy (SEM), and Transmission electron microscope (TEM), which proved the synthesis of composite in nano range as shown in results.



**Fig. 3** SEM of calcined sample prepared at 1000 °C.



**Fig. 5a** Morphological features of EAC tumor in different groups.



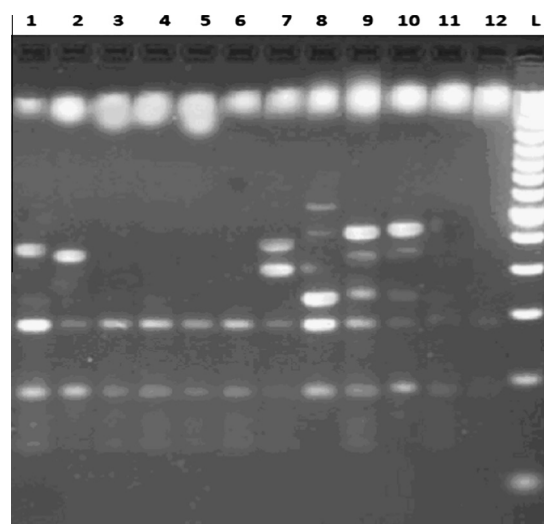
**Fig. 5b** EAC tumor size in different groups.

### Animals

85 Male Swiss albino mice weighing 20–22 g were used in the present study. They were acclimatized to the laboratory conditions prior to the study for seven days. The animals were kept at  $25 \pm 2$  °C and a relative humidity of 40–45% with alternative day and night cycles of 12 h each. They were fed with pelleted rat chow and water *ad libitum*. Anesthetic procedures and handling with animals were approved by and complied with the ethical guidelines of Medical Ethical Committee of the National Research Centre in Egypt (Approval number: 14077).

### Tumor transplantation

Ehrlich Ascites Carcinoma (EAC) cells were chosen due to its high hematogenous metastatic propensity and reproducible biological behavior. EAC cells were collected by sterile disposable syringe from donor mice (Swiss albino) of 18–20 g body weight and suspended in sterile isotonic saline. The viability of the cells was 99% as judged by trypan blue exclusion assay. To assess a solid mass of Ehrlich tumor, a fixed number of viable cells 0.2 mL EAC cells containing  $2 \times 10^6$  cells/mouse



**Fig. 6** DNA fragmentation of implanted tumor. Lanes (1 & 2): Once IT after 3 and 4 weeks respectively. Lanes (3 & 4): once IP nano-CaP after 3 weeks. Lanes (5 and 6): once IP nano-CaP after 4 weeks and (7 and 8) weekly IP nano-CaP after 3 weeks. Lanes 9 and 10 weekly IP nano-CaP after 4 weeks and 11 and 12 represent EAC without treatment.

were inoculated intraperitoneally into the femoral region of recipient male mouse [13] and left for 7–10 days to allow tumor to grow as big as its diameter achieved 0.7–1.2 cm.

### Treatment schedule

The animals were divided into nine groups: each equal 10 except group 9 comprises 5 animals. All groups received EAC cells ( $2 \times 10^6$  cells/mouse IP) and this day was considered

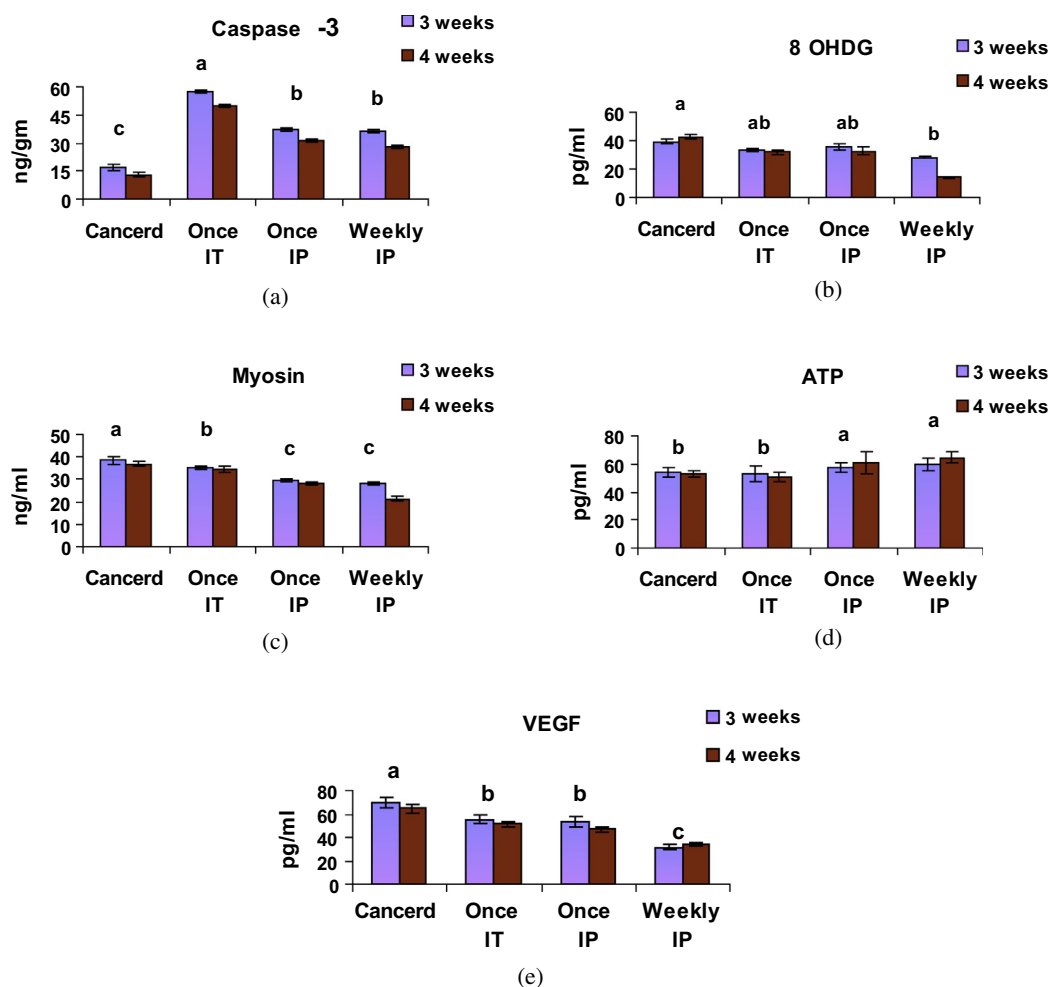


Fig. 7 (a) Serum caspase-3, b) OHDG, c) myosin, d) ATP, and e) VEGF levels in different groups.

as day zero. Groups 1 and 2 served as EAC control. Nine days after EAC transplantation, groups 3 and 4 were injected once intratumorally (IT) by nano-CaP (200 mg/kg body weight); groups 5 and 6 received nano-CaP once intraperitoneally (IP) and groups 7 and 8 received nano-CaP weekly (IP). Concerning the group 9, two animals were injected once and three animals were injected weekly for four weeks. The nano-CaP was thermally heated at  $<1000^{\circ}\text{C}$ . The SEM analysis had shown fused grains with average size 70 nm. The ground fused grains were dispersed in sterile water before administration.

#### Tumor size

Tumor growth was monitored twice a week throughout the experimental work. The tumor growth was measured regularly using Vernier calipers and represented in terms of tumor size. The tumor size was estimated using the following formula: Tumor size ( $\text{mm}^3$ ) =  $4\pi(A/2)^2(B/2)$ , where  $A$  is the minor tumor axis;  $B$  is the major tumor axis, and  $\pi$  equals to 3.14 [14]. The mean tumor size with the corresponding standard error was calculated in each experimental group.

#### Sample preparation

Blood samples and thigh skeletal muscle were collected after three weeks from groups 1, 3, 5, and 7 and after four weeks from groups 2, 4, 6, and 8. In case of group 9, the tissues were collected after 3 months to follow up the recurrence of tumor and to ensure the safety of muscle. Immediately Ehrlich tumor bearing thigh was excised and rinsed with saline. Small portion was placed in 10% phosphate-buffered formalin for histopathological examination. The rest was homogenized in 0.25 M ice-cold isotonic sucrose for DNA fragmentation and biochemical analyses.

#### DNA fragmentation

Qualitative analysis of DNA fragmentation was measured by agarose gel electrophoresis. Tumor cells were extracted from the animals and kept on ice during and after homogenization. Tissue samples were homogenized in chilled homogenization buffer (Ultra Turrax IKA T25-Germany) (pH 7.5), containing 75 mM NaCl and 24 mM Na<sub>2</sub>EDTA to obtain a 10% tissue solution, and then measured [15].

**Biochemical analysis**

Serum 8-hydroxy-deoxyguanosine (8-OHDG), myosin, and adenosine triphosphate (ATP) were assayed based on a solid phase enzyme linked immunosorbent assay (ELISA) (Life Sciences Advanced Technologies, Saint Petersburg FL 33710). Also, serum vascular endothelial growth factor (VEGF) (Boster Biological Technology LTD, Malden, MA, USA) and ELISA were determined according to the method of Ferrara [16]. Noradrenaline (NA) was measured using appropriate [<sup>125</sup>I] radioimmunoassay kit (IBL, Hamburg, Germany) while dopamine (DA), serotonin, and gamma-aminobutyric acid (GABA) were estimated in the skeletal muscle [17].

*Histopathological examination*

Necropsy samples were collected from the skeletal muscle of mice thigh of different groups and fixed in 10% formol saline. Samples were washed with water and then serial dilutions of alcohols were used for dehydration. Specimens were cleared in xylene and embedded in paraffin at 56 °C in hot air oven. Paraffin bees wax tissue blocks were prepared for sectioning at 4 μm by sledge microtome. The obtained tissue sections were collected on glass slides, deparaffinized, stained by hematoxylin and eosin, and then examined through the electric light microscope [18].

*Quantification of the percentage of tumor necrosis*

Stained samples were subjected to reading and determination of necrosis areas, through the tumor mass using Auto CAD software (Free version for testing). After being scanned, the images were analyzed in AutoCAD software and areas of necrosis bounded by the electronic cursor were calculated in mm.

The following formula was used to calculate the percentage of necrosis:

$$\% \text{ necrosis area} = (\text{necrosis area} / \text{total tumoral mass area}) \times 100$$

*Statistical analysis*

The data were statistically analyzed according to Steel and Torrie [19] using SPSS computer Program (v.17). The results were presented as mean ± SE. The differences between mean values were determined by two way analysis of variance (ANOVA) test, followed by Waller–Duncan k-ratio [20]. All statements of significance were based on probability of  $P \leq 0.05$ . Statistical significance of the relationships between variables was calculated by correlation analysis.

**Results**

*Material characterizations*

The X-ray Diffraction (XRD) analysis of the powder calcined at 1000 °C, identified the presence of different structures of calcium phosphate or tricalcium diphosphate Ca<sub>3</sub>(PO<sub>4</sub>)<sub>2</sub> (these amounts were calculated using reference-intensity-ratio (RIR) method in XRD instrument semi-quantitatively) (Fig. 1) as the main characteristic bands of calcium phosphate

**Table 1** The levels of serum caspase-3, 8OHDG, myosin, ATP and VEGF in cancer control and experimental groups.

Parameters	Cancer		Once IT		Once IP		Weekly IP		F1	F2
	Time after treatment		Time after treatment		Time after treatment		Time after treatment			
	3 W	4 W	3 W	4 W	3 W	4 W	3 W	4 W		
Caspase-3 ng/g	16.84 <sup>b</sup> ± 1.49	13.0 <sup>b</sup> ± 0.73	57.34 <sup>a</sup> ± 0.84	50.11 <sup>a</sup> ± 2.46	37.34 <sup>a</sup> ± 1.59	31.30 <sup>a</sup> ± 0.56	36.70 <sup>a</sup> ± 1.68	28.11 <sup>a</sup> ± 0.69	58.05 <sup>*</sup>	0.18 <sup>†</sup>
8 OHDG Pg/mL	39.30 <sup>a</sup> ± 1.83	42.70 <sup>a</sup> ± 1.67	33.50 <sup>ab</sup> ± 1.27	31.98 <sup>ab</sup> ± 1.49	35.60 <sup>ab</sup> ± 1.74	32.50 <sup>ab</sup> ± 2.81	28.10 <sup>b</sup> ± 0.81	14.0 <sup>b</sup> ± 0.66	8.78 <sup>*</sup>	1.84 <sup>†</sup>
Myosin ng/mL	38.55 <sup>a</sup> ± 1.77	36.92 <sup>a</sup> ± 1.35	35.32 <sup>b</sup> ± 0.83	34.50 <sup>b</sup> ± 1.15	29.31 <sup>c</sup> ± 0.69	28.40 <sup>c</sup> ± 0.72	28.11 <sup>c</sup> ± 0.83	21.46 <sup>c</sup> ± 1.32	33.2 <sup>*</sup>	9.28 <sup>*</sup>
ATP Pg/mL	54.10 <sup>b</sup> ± 3.08	52.90 <sup>b</sup> ± 2.41	52.80 <sup>b</sup> ± 5.26	50.8 <sup>b</sup> ± 3.28	57.62 <sup>a</sup> ± 3.02	60.91 <sup>a</sup> ± 7.48	60.11 <sup>a</sup> ± 4.48	64.60 <sup>a</sup> ± 3.68	10.29 <sup>*</sup>	0.587 <sup>†</sup>
VEGF Pg/mL	69.90 <sup>a</sup> ± 4.49	64.78 <sup>a</sup> ± 3.84	55.42 <sup>b</sup> ± 3.21	51.20 <sup>b</sup> ± 2.59	53.81 <sup>b</sup> ± 4.65	46.70 <sup>b</sup> ± 2.69	31.73 <sup>c</sup> ± 1.88	34.11 <sup>c</sup> ± 0.98	9.38 <sup>*</sup>	0.89 <sup>†</sup>

The different letters are statistically significant ( $P < 0.05$ ). F1: different treatments (transplantation of solid tumor in mice and treatment with nano-CaP); F2: Time after treatment (weeks (W)).  
<sup>\*</sup> ( $P < 0.05$ ).  
<sup>†</sup> ( $P > 0.05$ ).

at  $d = 2.87, 2.60,$  and  $3.20 \text{ \AA}$ . While the Infrared analysis showed that the characteristic bands of  $\text{PO}_4^{3-}$  due to calcium phosphate structure ( $\text{Ca}_3(\text{PO}_4)_2$ ) appeared clearly after calcinations (Fig. 2), the morphological analysis of the powder calcined at  $1000 \text{ }^\circ\text{C}$  showed fused grains with crystal growth to form large crystals of a tubular shape and size from  $0.5$  to  $10 \text{ }\mu\text{m}$ . The large magnification clarified the molten grains of average grain size  $500 \text{ nm}$  (Fig. 3). Fig. 4 shows the TEM micrograph analysis of the synthesized calcium phosphates composite in nano range.

The EAC tumor of untreated mice grew faster than any other groups. The tumor not only rapidly shrunk in groups 5, 6, 7, and 8, but also they became nearly flat within 4 weeks post-treatment. Furthermore, in group 1 (untreated), central necrotic area was noted in the tumor that was enlarged till the 4th week (Figs. 5a and 5b).

#### DNA fragmentation of implanted tumor

DNA derived from animals bearing EAC, expressed distinct ladder pattern of DNA fragments (L) reaching less than  $200 \text{ bp}$ ; a characteristic for apoptosis (lanes 1–10). The fragmentation pattern of nano-CaP treated cells was evident with various degrees depending on the way of injection and time. The DNA of untreated mice (EAC mice) was found to be intact as shown in lanes 11 and 12 (Fig. 6).

#### Biochemical findings

Fig. 7a–d represents the effect of CaP nanoparticles on some biochemical analysis in serum of different groups. Caspase-3 activity showed significant increase in all treated groups especially in mice groups injected intratumorally compared to untreated mice (Fig. 7a). A significant decrease in 8-OHdG, myosin, ATP, and VEGF levels was observed in experimental animals treated with nano-CaP compared to untreated animals (Fig. 7b–e). Additionally, the level of 8-OHDG was decreased

after four weeks in mice injected weekly with nano-CaP (Table 1).

Statistical analysis showed significant increase in neurotransmitter levels (NA, DA, serotonin, and GABA) in skeletal muscle of nano-CaP treated groups compared to untreated group. The effect was more pronounced after four weeks in mice either injected only one time (once) or injected once a week as shown in Fig. 8a–d and Table 2.

#### Histopathological findings

Histopathological examination of the skeletal muscle under light microscope showed compact and aggregation of tumor cells within the muscular tissues in all wide implanted area. Ehrlich carcinoma showed groups of large, round, and polygonal cells, with pleomorphic shapes. The nuclei appeared hyperchromic and binucleated Fig. 9a–d.

According to histopathological results, treatment with nano-CaP diminished the majority of histopathological changes in the portal area after 3 weeks. Treatment of male mice bearing solid tumor by single dose of nano-CaP showed the presence of necrosis in 20% of implanted cancer cells after three weeks (Fig. 9e and f) and reached to 40% after four weeks (Fig. 9g and h).

Severe destruction and necrosis of tumor cells were recorded in solid tumor bearing mice treated weekly with nano-CaP. Necrosis was observed in 75% of the implanted cancer cells after three weeks (Fig. 9i) reaching to 80% after four weeks (Fig. 9j).

According to the histopathological results, necrosis was observed in 80% of the implanted cancer cells in mice bearing solid tumor and injected once intratumorally by nano-CaP after three weeks (Fig. 9k) and four weeks (Fig. 9l).

With respect to group 9, histopathological examination showed few inflammatory cells infiltration in focal manner at the muscle bundles (Fig. 9m), while the periphery zone showed focal inflammatory cells infiltration, red blood cells,

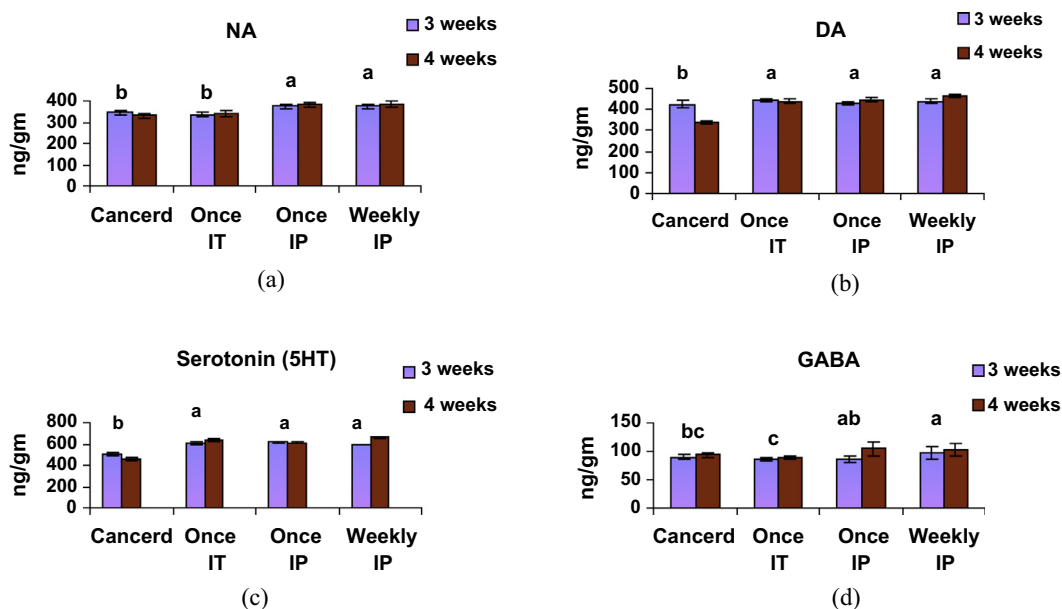


Fig. 8 (a) Tissue NA, b) DA, c) serotonin, and d) GABA levels in different groups.

**Table 2** The levels of neurotransmitters (NA, DA, 5HT and GABA) in cancer control and experimental groups.

Parameters	Groups												
	Cancer			Once IT			Once IP			Weekly IP			
	Time after treatment			Time after treatment			Time after treatment			Time after treatment			
	3 W	4 W	4 W	3 W	3 W	4 W	3 W	3 W	4 W	3 W	3 W	4 W	
NA ng/g	344.80 <sup>b</sup> ± 10.83	331.28 <sup>b</sup> ± 12.67	343.54 <sup>b</sup> ± 15.49	335.00 <sup>b</sup> ± 11.27	376.40a ± 9.74	381.50a ± 12.81	375.40a ± 10.81	382.90a ± 13.66	382.90a ± 13.66	375.40a ± 10.81	382.90a ± 13.66	11.56 <sup>*</sup>	0.027 <sup>†</sup>
DA ng/g	425.80 <sup>b</sup> ± 15.77	338.90 <sup>b</sup> ± 7.35	438.71a ± 10.15	443.50a ± 8.83	430.90a ± 7.69	445.30a ± 11.72	438.20a ± 9.83	464.9a ± 5.32	464.9a ± 5.32	438.20a ± 9.83	464.9a ± 5.32	7.00 <sup>*</sup>	0.42 <sup>†</sup>
5HT ng/g	503.25 <sup>b</sup> ± 9.08	458.00 <sup>b</sup> ± 11.41	634.10a ± 11.28	606.30a ± 15.26	615.50a ± 13.02	613.00a ± 7.38	593.50a ± 6.34	662.24a ± 8.68	662.24a ± 8.68	593.50a ± 6.34	662.24a ± 8.68	4.192 <sup>*</sup>	0.127 <sup>†</sup>
GABA ng/g	90.12 <sup>bc</sup> ± 4.19	93.40 <sup>bc</sup> ± 3.81	89.30 <sup>c</sup> ± 2.59	85.90 <sup>c</sup> ± 3.29	86.11a <sup>b</sup> ± 5.65	105.10a <sup>b</sup> ± 12.67	98.30a ± 10.88	102.60a ± 12.18	102.60a ± 12.18	98.30a ± 10.88	102.60a ± 12.18	7.27 <sup>*</sup>	14.57 <sup>*</sup>

The different letters are statistically significant ( $P < 0.05$ ). F1: different treatments (transplantation of solid tumor in mice and treatment with nano-CaP); F2: Time after treatment (weeks (W)).

\* ( $P < 0.05$ ).

† ( $P > 0.05$ ).

and edema in mice injected weekly (Fig. 9n and o). A nano-CaP injected once in solid tumor bearing mice achieved complete recovery of cancer cells, as edema was only detected between the muscle bundles as shown in (Fig. 9p).

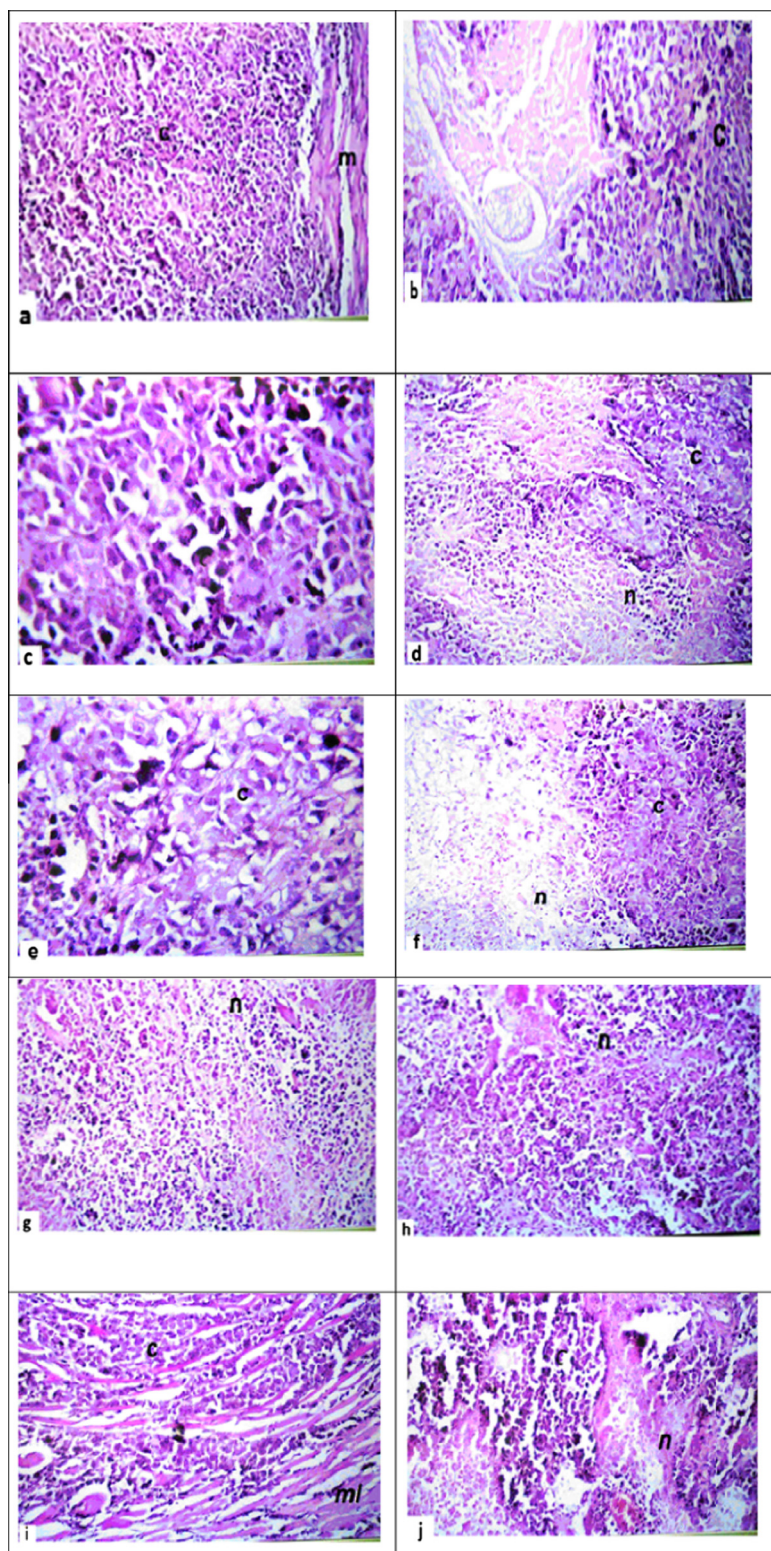
## Discussion

Ehrlich carcinoma, an undifferentiated carcinoma, is originally hyperdiploid, has high transplantable capability, no-regression, rapid proliferation, short life span, 100% malignancy and does not have tumor-specific transplantation antigen. It resembles human tumors, which are the most sensitive to chemotherapy. Following implantation of Ehrlich tumor cells, morphological and metabolic changes occur such as structural deterioration, decreased number of mitochondria, decreased DNA and RNA synthesis, loss of intracellular purine and pyrimidine nucleotides, nucleosides and bases and a decline of ATP concentration and turnover [14]. Nuclear morphology changes characteristic of apoptosis appear within the cell together with a distinctive biochemical event the endonuclease-mediated cleavage of nuclear DNA.

In the present study, nano-CaP inhibited the growth of tumor cells and induced morphological changes typical of apoptosis. The incidence of DNA fragmentation and increased level of caspase-3 of tumor cells confirmed such morphological findings. Treatment with nano-CaP induced ladder-like DNA fragmentation in tumor cells, which is a characteristic of DNA damage. Increased levels of DNA damage could cause the synthesis of a variety of incorrect proteins and therefore impaired cellular function [21]. Most anticancer drugs either natural or synthetic have been known to cause DNA damage or suppress its replication, not necessarily killing the cells directly but inducing apoptosis. During apoptosis, a specific nuclease (caspase-activated Dnase or CAD) cuts the genomic DNA between nucleosomes and generates apoptotic chromatin condensation and DNA fragments [21]. Among them, caspase-3 is a frequently activated death protease, catalyzing the specific cleavage of many key cellular proteins. Thus, caspase-3 is essential for certain processes associated with the dismantling of the cell and the formation of apoptotic bodies, but it may also function before or at the stage when commitment to loss of cell viability is made.

Skeletal muscle is the tissue with the largest mass in the body, and consists of post-mitotic cells, which are more prone to accumulate oxidative damage [22]. Thus, it is highly plausible that the muscle damage associated with muscle soreness causes oxidative damage by enhancement of free radical generation. The cytotoxic effects of free radicals include the oxidative damage of cellular DNA [23]. The inhibition of 8-OHdG level in serum of tumor bearing mice after nano-CaP treatment is strongly referable to the efficiency of material in scalable cancer cells and maintaining the integrity of DNA in the body cells. Adduct of 8-OHdG indicated oxidative DNA damage because this lesion is a frequently found adduct in mutated oncogenes and tumor suppressor genes [24]. Several tumor-derived vasoactive compounds have been pointed out to drive this increase in vascular permeability (VEGF) [25]. The thrust of nano-CaP regimen was to decrease VEGF level which is thought to be the single most important angiogenic cytokine in cancer and its secretion by tumor cells is responsible for initiation and maintenance of the ascites pattern of tumor growth [26]. It is well known that solid tumor growth requires the





**Fig. 9** (a–d) Skeletal muscle of mice bearing EAC, showed compact and aggregation of the tumor tissue cells spread within the muscular tissues. (e–h) Skeletal muscle of mice bearing EAC treated by single dose of nano-CaP after three weeks, showed the presence of necrosis in 20% of implanted cancer cells. (i) Skeletal muscle of solid tumor bearing mice treated weekly with nano-CaP after three weeks. (j) Skeletal muscle solid tumor bearing mice treated weekly with nano-CaP after four weeks. (k) Skeletal muscle of mice bearing solid tumor and injected once intratumorally by nano-CaP after three weeks. (l) Skeletal muscle of mice bearing EAC and injected once intratumorally by nano-CaP after four weeks. (m–o) Skeletal muscle of solid tumor bearing mice to follow-up of the treatment of nano-CaP after three months on cancer cells invasion in thigh skeletal muscle, and p-once injection of nano-CaP in solid tumor bearing mice achieved complete recovery of cancer cells after three months.

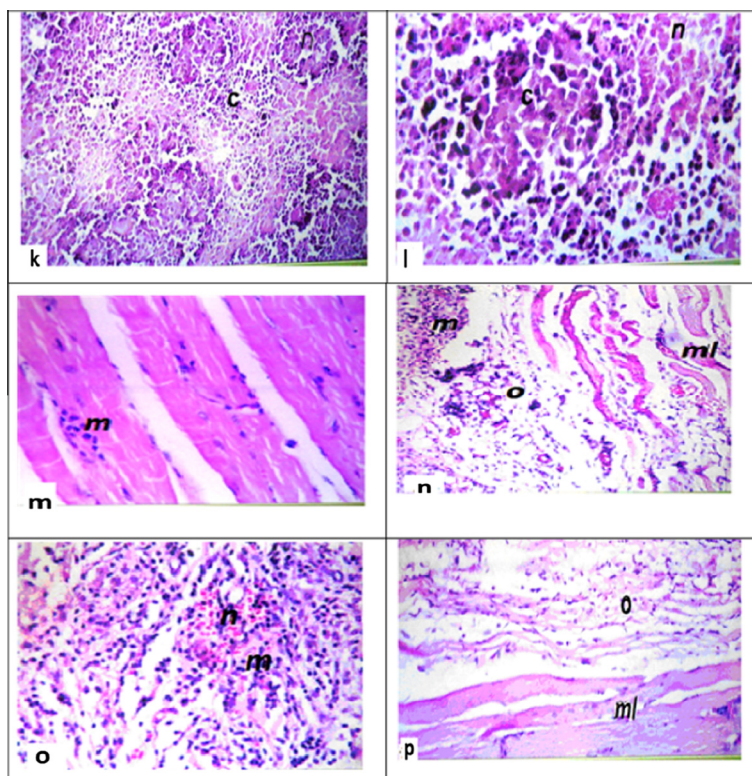


Fig 9. (continued)

generation of new blood vessels from an established vascular network. The newly formed vascular network provides necessary nutrients and oxygen to meet the increased metabolic demand of the growing tumor and increase the probability of tumor dissemination via the vascular system [27]. Interestingly, tumor tissues lack a lymphatic system for eliminating lipophilic and polymeric materials from them; therefore, once the particles penetrate the tumor tissues, they cannot be eliminated easily. Thus, tumors exhibit enhanced penetration and retention effect for 50- to 100-nm particles [28]. Long-circulating nanoparticles with the appropriate particle size have more frequent opportunities to encounter 'leaky tumor capillaries' and extravasate into the tumor tissue [29]. On the other hand, accompanying between levels of myosin with ATP in tumor bearing mice is consistent with biological rationality. Since, myosin is released into the circulation following muscle injury and acts as an ATPase. It can hydrolyze ATP to generate the force for the contraction of muscle cells and movement along actin filaments necessary to drive a wide variety of cellular functions [30].

The most important rendering of nano-CaP therapy observed in the present study was improvement of neurotransmitters content in thigh muscle because novel neurological aspects of tumors were more elucidated and many evidences have further shown that tumors growth process is also related to the nervous system. More important, numerous neurotransmitters influence tumor vascularization and cell migration [31]; in addition, they may also suppress the immune response in cancer [32]. These influences are increased by the ability of the cancer cells to secrete neurogenic factors [33], which influences neurons development. Numerous papers have pointed a correlation between the GABA and tumor cells migration,

indicating a local antitumor effect of GABA [34]. Another neurotransmitter, which is the dopamine, plays an important role within the neuro-tumoral interactions and has effects on both cancer growth and anticancer drugs. It blocks VEGF-induced angiogenesis of endothelial progenitors in the bone marrow and contributes in the growth diminution of cancers. In this aspect, further evidence provided by [35,36] that DA can inhibit the functions of adult endothelial cells by suppressing phosphorylation of vascular endothelial growth factor receptor 2 (VEGFR2), focal adhesion kinase (FAK), and mitogen-activated protein kinase (MAPK) and by acting through its D2 receptors, can inhibit the mobilization of BM-derived endothelial progenitor cells (EPCs). Joseph et al. [37] reported that GABA can inhibit colon cancer migration associated with the norepinephrine-induced pathway [38]. On the other hand, Alves et al. [39] reported a decrease in hypothalamic noradrenaline (NA) levels and increase in NA turnover in Ehrlich tumor-bearing mice.

The performance of CaP nano-particles validated the general view of the literature because the development of multifunctional nanoparticles might eventually render nanoparticles able to target and kill cancer cells simultaneously providing low side effects [40]. Targeting tumor tissues occurs through the extravasations of nanoparticles post-injection into the systemic blood circulation. The biodistribution of these particles is dependent on the characteristics of blood capillaries in the organs and tissues as well as the administration site, particle size and particle surface properties. Even in intratumoral (IT) administration, understanding the mechanism of the extravasations is critical to retain the particles at the injection sites. In addition to such macro bio-distribution of particles, their diffusion in the tissues, association to cells,

internalization into the cells and intracellular distribution are important issues in cancer therapy and diagnosis [41].

Owing to general histopathological observations agreed to potency of nano-CaP in DNA fragmentation of tumor cells included a great percentage of necrotic tumor cells increase with time. Interestingly, the extension of pathological examination to three months reflects the irreversible mode of nano-CaP therapy. The specimen of skeletal muscle appeared devoid of any tumor cells but contained only few inflammatory cells and edema.

## Conclusions

The newly-formed nano-calcium phosphates particle had shown good biocompatibility and low cytotoxicity to normal cells when injected intraperitoneally. It has potent therapeutic effect on implanted solid tumor within four weeks and achieved complete recovery of EAC after three months. This study provides a comprehensive insight into the mode of action of the usage of nanoparticle of CaP *in vivo* as a therapy of solid tumor.

## Conflict of interests

*The authors have declared no conflict of interest.*

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