

RESEARCH

Open Access

Tibialis Anterior muscle coherence during controlled voluntary activation in patients with spinal cord injury: diagnostic potential for muscle strength, gait and spasticity

Elisabeth Bravo-Esteban^{1,2}, Julian Taylor¹, Manuel Aleixandre², Cristina Simon-Martínez¹, Diego Torricelli², José L Pons² and Julio Gómez-Soriano^{1,3*}

Abstract

Background: Coherence estimation has been used as an indirect measure of voluntary neurocontrol of residual motor activity following spinal cord injury (SCI). Here intramuscular Tibialis Anterior (TA) coherence estimation was performed within specific frequency bands for the 10-60 Hz bandwidth during controlled ankle dorsiflexion in subjects with incomplete SCI with and without spasticity.

Methods: In the first cohort study 15 non-injured and 14 motor incomplete SCI subjects were recruited to evaluate TA coherence during controlled movement. Specifically 15-30 Hz EMG was recorded during dorsiflexion with: i) isometric activation at 50, 75 and 100% of maximal voluntary torque (MVT), ii) isokinetic activation at 60 and 120°/s and iii) isotonic dorsiflexion at 50% MVT. Following identification of the motor tasks necessary for measurement of optimal TA coherence a second cohort was analyzed within the 10-16 Hz, 15-30 Hz, 24-40 Hz and 40-60 Hz bandwidths from 22 incomplete SCI subjects, with and without spasticity.

Results: Intramuscular 40-60 Hz, but not 15-30 Hz TA, coherence calculated in SCI subjects during isometric activation at 100% of MVT was lower than the control group. In contrast only isometric activation at 100% of MVT 15-30 Hz TA coherence was higher in subjects with less severe SCI (AIS D vs. AIS C), and correlated functionally with dorsiflexion MVT. Higher TA coherence was observed for the SCI group during 120°/s isokinetic movement. In addition 15-30 Hz TA coherence calculated during isometric activation at 100% MVT or 120°/s isokinetic movement correlated moderately with walking function and time from SCI, respectively. Spasticity symptoms correlated negatively with coherence during isometric activation at 100% of MVT in all tested frequency bands, except for 15-30 Hz. Specifically, 10-16 Hz coherence correlated inversely with passive resistive torque to ankle dorsiflexion, while clinical measures of muscle hypertonia and spasm severity correlated inversely with 40-60 Hz.

Conclusion: Analysis of intramuscular 15-30 Hz TA coherence during isometric activation at 100% of MVT is related to muscle strength and gait function following incomplete SCI. In contrast several spasticity symptoms correlated negatively with 10-16 Hz and 40-60 Hz TA coherence during isometric activation at 100% MVT. Validation of the diagnostic potential of TA coherence estimation as a reliable and comprehensive measure of muscle strength, gait and spasticity should facilitate SCI neurorehabilitation.

Keywords: Electromyography, Intramuscular coherence, Spasticity, Isometric activation, WISCI II, AIS, Isokinetic activation, Residual voluntary motor function recovery, Neuroplasticity, Neurorehabilitation

* Correspondence: julio.soriano@uclm.es

¹Sensorimotor Function Group, Hospital Nacional de Paraplégicos, Toledo, Spain

³Nursing and Physiotherapy School, Castilla La Mancha University, Toledo, Spain

Full list of author information is available at the end of the article

Introduction

Spinal cord injury (SCI) has a devastating impact on sensorimotor function, often leading to reduced quality of life, presenting a serious socioeconomic problem for national healthcare systems [1]. Although spinal damage is incomplete in approximately half of all SCI cases [2], only limited recovery of residual voluntary motor function is observed during the subacute phase of neurorehabilitation [3]. Indeed neurophysiological studies demonstrate only limited spontaneous recovery of voluntary motor function after incomplete SCI diagnosed with the American Spinal Injury Association Impairment Scale (AIS) [4]. Approximately 15-40% of individuals diagnosed with AIS B convert to AIS C, compared to 40% of subjects with AIS B SCI which convert to AIS D, and between 60-80% of AIS C which convert to AIS D [3]. Limited functional recovery could be mediated via several neuromotor control systems including automatic spinal motor control and descending corticospinal or extrapyramidal tract activity [5,6]. Furthermore the development of specific motor disorder symptoms associated with the spasticity syndrome [7,8] may further limit the recovery of voluntary motor strength, gait and activities of daily living [6-10]. As such the development of an objective and comprehensive measure of residual motor function recorded during subacute SCI neurorehabilitation which in turn reflects recovery or deterioration of descending or spinal neuromotor control mechanisms would help facilitate clinical diagnosis and improve treatment strategies. Ideally the neurophysiological measure should be clinically relevant, reflecting recovery of voluntary muscle strength and residual gait function during rehabilitation, while highlighting the development of debilitating central effects of problematic spasticity symptoms.

Electromyographic (EMG) muscle coherence estimation is a mathematical index that calculates the degree of synchronization of two independent EMG signal sources calculated in the frequency domain [11], and which can be obtained either within the same muscle (intramuscular coherence) [12,13], or between muscles [13-15]. Clinical studies have observed that measurement of synchronous motoneurone discharge (coherence) as an indirect measure of voluntary common drive is best recorded during isometric muscle contraction, and is significantly decreased following SCI [16]. Interestingly Hansen et al. [14] postulated that central common drive responsible for motor unit synchronization during walking may also be similar to that measured during tonic voluntary contraction. This analysis technique can also be applied to upper and lower limbs in subjects with central nervous system disorders, such as SCI or stroke, where the evidence also demonstrates reduced or absent motor unit synchrony during movement [16-18]. More recently the potential for muscle coherence analysis to demonstrate damage to voluntary motor control

mechanisms and clinical function such as gait has been demonstrated in subjects with SCI [12,13].

Surprisingly no systematic studies are available that demonstrate the optimal testing conditions required to analyze motor unit synchronization during controlled movement, at moderate to strong muscle contractions or at slow and fast speeds, in subjects with residual voluntary muscle strength and gait function after incomplete SCI. Several physiological studies justify the application of muscle coherence estimation as an indirect measure of voluntary motor drive with respect to specific motor tasks. A relationship between the force of isometric contraction [16] and corticospinal activation has been alluded to in man [19], based partly on the observation of reduced intracortical inhibition [20] which in turn can be modulated by muscle strength training [21]. With respect to the velocity of movement, a study in subjects with SCI also alludes to a relationship between gait velocity and corticospinal tract activity which was calculated as intramuscular 10-20 Hz TA coherence activity, although the relationship between these measures were related to their common correlation with foot drop [13].

Spinal cord injury invariably leads to different degrees of corticospinal tract injury [3]. Given that EMG coherence activity is related to corticospinal tract function [11,13] this technique has been used in several research studies to indirectly address the state of descending motor control mechanisms. As an example, Hansen [22] observed an alteration in muscle coherence related to walking dysfunction. Several clinical neurophysiological studies have also proposed that muscle coherence activity calculated within specific frequency bands reflects activity of different neuronal systems, where high frequency activity (15-30, 24-40 Hz) [23] may reflect descending neuromotor control [15], compared to low frequency coherence (1-12 Hz) which may be associated with spinal activity [24-26]. Importantly for the diagnosis of SCI, coherence activity within the 15-30 Hz range has been estimated as a standard indirect measure of pyramidal tract integrity [27-29].

Measurement of residual voluntary activity within the Tibialis Anterior (TA) muscle may represent an interesting diagnostic marker of function after SCI, particularly as this muscle receives strong innervation from the corticospinal system [30]. Indeed ankle dorsiflexion has been used to indirectly measure central adaptive neuroplasticity of the corticospinal tract during rehabilitation [31,32], while the detection of TA coactivation during plantarflexion can also detect the development of maladaptive mechanisms after incomplete SCI, such as specific symptoms of spasticity [6]. Although spasticity has been reported in up to 78% of chronic SCI individuals [10,33-35] it is not clear whether the presence of symptoms such as muscle hypertonia or spasms directly

affect the central neuronal drive that mediates the limited recovery of residual motor function [6,36]. Therefore analysis of intramuscular TA coherence could represent a comprehensive measure of functional change after SCI during subacute rehabilitation.

Systematic evaluation of the optimal movement testing conditions for muscle coherence analysis and the intramuscular TA frequency band best related to residual voluntary muscle strength and gait function should provide important orientative data to guide the diagnostic potential of monitoring motor unit synchronization as a comprehensive diagnostic tool for clinical motor function after incomplete SCI.

Methods

The study was divided into two trials. The objective of the first trial was to identify the optimal specific kinematic condition to measure differences in motor unit synchronization between healthy non-injured subjects and individuals with incomplete SCI (Table 1). Therefore standard intramuscular TA coherence estimation within the 15-30 Hz band [27-29] during different types of controlled dorsiflexion movement was performed. Once the optimal movement tasks were identified a second trial was performed on a larger cohort of patients (Table 2) with an additional emphasis on analyzing TA coherence within different frequency ranges within the total 10-60 Hz bandwidth. The selection of these frequency bands was based on the standard 15-30 Hz frequency band [27-29] and studies that have implicated a physiological significance to low frequency [24-26] and high

frequency coherence [37]. In addition, the second trial investigated the impact of specific spasticity symptoms on TA coherence calculated during the optimal controlled test movement protocols.

Subjects

The study was performed following approval by the Local Toledo Hospital Clinical Ethical Committee (number of approval 152, 2012). All recruited subjects signed a consent form and gave their permission for data publication. Healthy non-injured subjects (n=15) and individuals with incomplete motor SCI (n=14) with a TA and Triceps Surae muscle score ≥ 2 [38], were recruited in the first trial (SCI cohort I). In the second trial (cohort II) 22 subjects were recruited with the same inclusion criteria. Patients were diagnosed with spasticity if they presented a modified Ashworth score [39] >1 and/or Penn score [40] ≥ 1 . The exclusion criteria included diagnosis of musculoskeletal or peripheral nervous system disorders.

Controlled movement tasks

Analysis of TA coherence was carried out during controlled movement with the subjects comfortably seated in a dynamometer (KinCom, Chattanooga Group Inc.). The trunk and pelvis of the tested leg were supported using straps. The hip, knee and the ankle joints were flexed at 90°. In SCI subjects the criteria included muscle activity calculated from the global muscle score TA muscle score greater than 2. Consequently the leg was capable of generating moderate contraction levels to perform the controlled movement protocols which also avoided methodological problems associated with coherence analysis with non-rectified signals [41]. For the non-injured control subjects the TA of the right leg was recorded for coherence estimation. The EMG activity was recorded using double differential surface electrodes, at a preamplifier gain of 10 V/V and open bandwidth (Delsys Inc. Signal Conditioning Electrodes 3.1), placed in two specific locations on the TA muscle belly, and separated by a minimum of 10 cm to avoid electrical cross-talk [12,14,42]. In the first trial 15 healthy subjects and 14 individuals with SCI (cohort I) performed three different types of controlled TA muscle movement tasks: i) two isometric activations maintained for 5 s, at 50%, 75% and 100% of the maximal voluntary torque (MVT) level, recorded with the dynamometer; ii) five cycles of isotonic activation with a range of motion from 30° plantarflexion to 0° dorsiflexion, with the required active force set to 50% of MVT; iii) ten cycles of isokinetic activation at 60°/s and 120°/s, from 30° plantarflexion to 0° dorsiflexion. All the controlled movement tasks, with the exception of the 100% MVT isometric activation, were randomized. The comprehensive movement testing

Table 1 Individual SCI characteristics for Cohort I

	Age (Years)	Gender	Etiology	Level	Time (Weeks)	MT	DMVT (Nm)
1	25	M	T	C4	22	4+	105
2	64	M	T	C4	480	4	112
3	27	M	T	C5	4	4	82
4	43	F	T	C6	40	4	70
5	59	F	NT	T3	28	3	73
6	45	F	NT	T7	20	4	110
7	21	M	NT	T7	14	4	103
8	22	M	T	T7	14	4	55
9	44	M	T	L1	36	3	115
10	41	M	T	C6	16	5	150
11	31	M	NT	C6	4	3	208
12	30	M	T	C6	12	4+	179
13	26	M	T	D7	6	4	84
14	30	M	T	D12	6	3	65

M: male; F: female; T: traumatic; NT: non-traumatic; Level: neurological level of injury; Time: time from injury (weeks); MT: Tibialis Anterior muscle testing score; DMVT: dorsiflexion maximal voluntary torque (Nm).

Table 2 Individual SCI characteristics for Cohort II

	Gender	Age (Years)	Asia	Level	Etiology	Ashw	Penn	Time (Weeks)
1	F	40	C	C4	NT	0	0	10
2	M	55	C	C5	NT	0	0	10
3	F	68	C	T8	NT	0	0	20
4	F	70	C	T10	NT	0	0	10
5	F	64	C	T12	NT	0	0	22
6	M	36	D	C3	NT	1	0	8
7	M	40	D	T11	T	0	0	18
8	M	57	C	C4	T	3	1	24
9	M	62	C	C5	T	7	2	48
10	M	26	C	C5	T	3	1	20
11	M	57	C	T6	T	9	3	20
12	M	22	C	T7	T	1	1	24
13	M	54	C	T7	T	3	1	28
14	F	68	C	T8	NT	1	2	12
15	M	70	C	T11	T	5	1	24
16	M	37	D	C2	T	6	1	18
17	M	62	D	C4	T	2	1	40
18	M	25	D	C4	T	2	1	48
19	M	48	D	C4	NT	2	1	8
20	M	36	D	C5	T	4	3	4
21	M	63	D	C5	T	4	2	16
22	M	45	D	C7	T	2	1	8

M: male; F: female; T: traumatic; NT: non-traumatic; Level: neurological level of injury; ASHW: total modified Ashworth score calculated for the knee and ankle joints during flexion and extension movement; Penn: Penn spasm scale; Time: time from injury (weeks).

conditions precluded the analysis of long EMG segments (see below).

In the second trial 22 SCI subjects (15 of whom presented spasticity) performed two types of controlled TA activation i) two isometric activation at 100% of MVT maintenance for 5 s and ii) ten cycles of isokinetic movement at 60°/s and 120°/s, from 30° plantarflexion to 0° dorsiflexion. In addition several clinical tests were applied in the second trial including i) gait function measured with the WISCI II [43], ii) the modified Ashworth scale to measure muscle hypertonia in the knee and ankle joint during flexion-extension movement, iii) spasm frequency quantified with the Penn scale and iv) severity of evoked spasms measured with the spinal cord assessment tool for spastic reflexes scale (SCATS) [44]. Passive resistive torque to ankle dorsiflexion was also tested in the second cohort at slow (30°/s) and fast (120°/s) movements in order to evaluate both the viscoelastic and reflexive components respectively of muscle hypertonia [45]. Passive torque measures were obtained with the subject seated in the dynamometer, with the hip joint flexed at 90° and the knee joint at 10°, and obtained

from ten ankle joint mobilizations from 30° plantarflexion to 0° dorsiflexion at 30°/s and 120°/s. EMG data was collected from 21/22 subjects during isometric activation at 100% of MVT, with data not recorded from 1/15 of the 15 spastic subjects. Correlation between intramuscular TA coherence during isometric activation at 100% of MVT and spasticity measures was performed for the 14 patients with hypertonia or spasm activity [6,10].

Data analysis and statistical evaluation

Coherence is a measure of how closely the two EMG signals are related by a linear transformation [46]. Coherence is estimated between 0–1, where a value of 1 indicates that the two signals are highly correlated, while a value of 0 means that both signals are independent. Electromyographic signals were recorded with a 10 KHz sampling frequency (MicroPlus 1401, Cambridge Electronic Design) and were subsequently down sampled to 2 KHz using a low pass filter of 700 Hz to avoid aliasing (Matlab 7.11). Muscle coherence activity was calculated with the Signal Processing Toolbox of Matlab 7.11 by estimating the power spectral densities with Welch's method [47]. Due to the methodological requirements of measuring intramuscular TA coherence during several controlled movement tasks in subjects with SCI, the criteria of recording EMG signals of at least 3.5 seconds was observed for all subjects and movement tasks. The signal was divided into 8 data segments with 50% overlapping segments performed with a Hamming window [48]. To obtain the coherence in each frequency band (10–16, 15–30, 24–40, and 40–60 Hz), all the coherences points within each specific band from each subject were averaged to obtain the grand average coherence for the specific frequency band.

There is some controversy regarding the requirement of rectifying EMG signal activity for coherence analysis with studies for [49–51] and against this process [52,53]. Indeed rectification of EMG activity amplifies the power spectrum of lower frequencies [49,54] and more clearly provides information regarding neuronal firing timings to assess the general activity envelope [53]. However rectification of EMG activity for coherence analysis has been demonstrated to be necessary at low muscle contraction levels [41]. This suggests coherence estimation of the moderate to strong muscle activity levels recorded in this study may not be affected by collection of non-rectified EMG signals and may not present problems in identifying common inputs to motoneurons in general [41]. Nevertheless rectification is preferable to reject other artefacts during coherence analysis [55].

The velocity dependence of intramuscular TA coherence was calculated by calculating the ratio of its value during isokinetic TA muscle movement at 120°/s and at 60°/s. Statistical analysis was performed with a commercial

software package (SigmaStat version 3.1, Systat software, Inc, USA). Due to the non normal distribution of the data, non-parametric tests were adopted. The Kruskal Wallis test was used to compare different controlled muscle activation protocols within the first SCI cohort. The Mann-Whitney test was used to compare intramuscular TA coherence between the healthy non-injured group with both SCI cohorts (Median and 25th-75th Percentiles) and to analyze differences between SCI subjects with and without spasticity in the second cohort. The Spearman correlation test was used to identify the relationship between TA coherence with MVT, gait function and spasticity measures. Statistical significance was defined as $p \leq 0.05$, with trends described at $p \leq 0.07$.

Results

Clinical characteristics of subjects

Fifteen healthy subjects (8 male) with a median age of 26.6 years (23.2-28.3, 25th percentile-75th percentile range) and 14 subjects with SCI (11 male) with a median age of 30.5 (26.4-44.3) years (SCI cohort I, Table 1), were recruited for the study of intramuscular TA coherence during different controlled muscle activation protocols. A difference in age was found between the healthy subjects and the individuals with SCI in cohort I, ($p = 0.032$) but no differences in gender were found. In the second larger SCI cohort an additional 22 subjects with SCI (17 male) with a median age of 54.5 (37.0-63.0) were enrolled for the more specific analysis of the relationship between frequency-specific TA coherence estimation and residual voluntary muscle strength, gait and spasticity (Table 2). This patient group were older than SCI subjects from cohort I ($p = 0.018$) and also showed significant differences with respect to the non-injured group ($p = 0.001$). Fifteen of the subjects in the second cohort were diagnosed with spasticity. Importantly no significant difference between the SCI clinical characteristics were identified between cohorts I and II for gender, time from injury or maximal dorsiflexion torque (Tables 1 and 2).

15-30 Hz TA coherence activity during controlled movement in subjects with or without SCI

Analysis of the complete coherence spectra for 10-60 Hz recorded during maximal isometric activation in subjects with SCI and non-injured control subjects (Figure 1A) suggested that activity within the 15-30 and 40-60 Hz bands was higher for the non-injured subjects compared to the SCI individuals, and minor differences within the 10-16 Hz band suggesting greater activity in subjects with SCI. Intramuscular TA muscle coherence calculated within the 15-30 Hz frequency band and compared between non-injured healthy subjects and individuals with SCI (cohort I, Table 1) revealed no significant differences during isotonic or isometric dorsiflexion at 50%, 75% or

100% of the MVT (Figure 1B). However 15-30 Hz TA coherence activity calculated during isometric activation at 100% of MVT in the first SCI cohort correlated positively with MVT during dorsiflexion ($\rho = 0.56$, $p = 0.01$, Figure 1C), although this correlation was not present in the non-injured healthy group ($\rho = 0.32$, $p = 0.23$). The level of 15-30 Hz TA coherence activity calculated during isokinetic contraction at 60°/s showed no differences between non-injured and SCI group. Nevertheless TA coherence activity during isokinetic activation at 120°/s revealed higher values during fast muscle activation in the SCI cohort I group (0.20, 0.13-0.38) when compared to the non-injured group (0.06, 0.04-0.11, $p = <0.001$; Figure 1B). Calculation of the ratio of TA coherence for isokinetic activation at 120/60°/s revealed higher values for the 15-30 Hz band for the first SCI cohort I (2.1, 0.6-3.9) when compared to the non-injured healthy group (0.58, 0.35-1.00, $p = 0.029$). No relationship was identified between the velocity-dependent 15-30 Hz TA coherence ratio and dorsiflexion MVT in the first SCI cohort (Figure 1D). Following identification of differences of intramuscular TA coherence activity during isometric activation at 100% of MVT and at faster isokinetic movement, an analysis of the physiological significance of each of the selected coherence frequency bands was sought with the optimal kinetic tasks in the second cohort.

Although no differences were identified for the 10-16 Hz (Figure 2A) or 15-30 Hz TA coherence bands (Figure 2B) between healthy and SCI groups during isometric activation at 100% of MVT in the second SCI cohort, calculation of the 40-60 Hz band revealed a lower level of activity in SCI subjects (0.11, 0.08-0.16) compared to the non-injured group (0.17, 0.11-0.19; $p = 0.05$, Figure 2C). The velocity-dependence of TA coherence activity in subjects with SCI was corroborated in the second cohort for most of the frequency bands between 10-60 Hz (Figure 2A-C). In the 15-30 Hz bandwidth, the difference for intramuscular TA coherence compared to the non-injured group during isokinetic activation at 120°/s from the first cohort were replicated in the second cohort with SCI subjects (0.14, 0.07-0.28) when compared to healthy subjects (0.065, 0.04-0.11; $p = 0.01$, Figure 2B) and for differences between the 120°/s/60°/s ratio calculation in the SCI group (1.5, 0.8-2.02) compared to the non-injured group (0.59, 0.37-1.87; $p = 0.04$). Moreover the 10-16 Hz activity revealed higher TA coherence during isokinetic activation at 120°/s (Figure 2A) in SCI subjects (0.16, 0.09-0.35) with respect to non-injured subjects (0.08, 0.03-0.16; $p = 0.05$). Higher 40-60 Hz TA coherence was also identified in SCI subjects during isokinetic activation at 120°/s (0.16, 0.08-0.26, Figure 2C) and with the 120/60°/s ratio (1.64, 0.92-2.5) compared to the non-injured subjects (0.08, 0.03-0.16; $p = 0.05$ and 0.8, 0.31-1.8; $p = 0.06$ respectively).

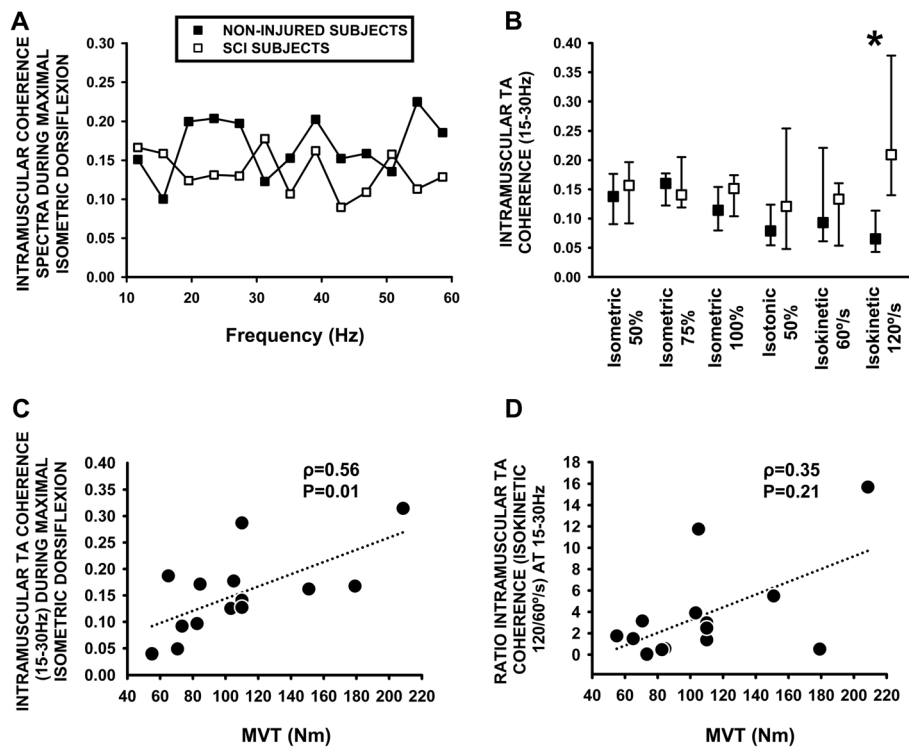


Figure 1 Intramuscular TA coherence in the SCI group and in the non-injured group. **A:** Intramuscular TA coherence spectra (10-60 Hz) calculated during maximal isometric dorsiflexion in the SCI group (white symbols) and in the non-injured group (black symbols). **B:** Analysis of 15-30 Hz intramuscular TA coherence from healthy subjects and individuals with SCI during isometric, isotonic and isokinetic muscle activation. *: $p \leq 0.05$. **C:** Correlation between intramuscular TA coherence calculated during isometric activation at 100% of MVT with maximal voluntary dorsiflexion torque. **D:** Correlation between velocity-dependent intramuscular TA coherence during 120/60°/s isokinetic activation with maximal voluntary dorsiflexion torque.

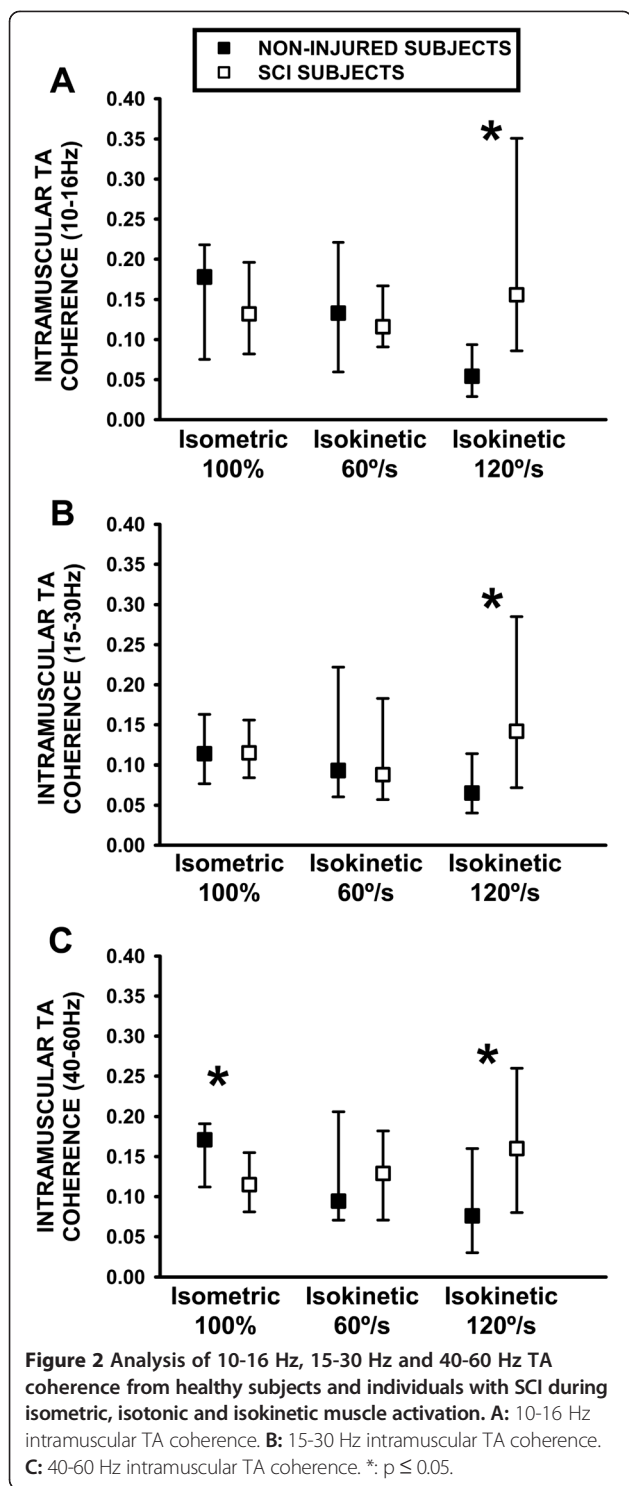
TA muscle coherence, muscle strength and gait function after spinal cord injury

The functional relationship between TA coherence calculated during isometric or isokinetic activation was investigated by assessing muscle strength and gait function in the second larger SCI cohort, with a special emphasis on analysis of the frequency specific bandwidths ($n = 22$, Table 2). As such the positive association observed between TA coherence during isometric activation at 100% of MVT and dorsiflexion MVT was corroborated for both the 15–30 Hz (replicating results from the first SCI cohort) and 24-40 Hz frequency bands (Table 3). Moreover 15-30 Hz TA coherence estimated during isometric activation at 100% of MVT correlated with the grade of residual gait function in subjects with SCI ($\rho = 0.41$, $p = 0.05$), with a trend present for coherence activity within the 24-40 Hz bandwidth (Table 3). TA muscle coherence calculated as the 120/60°/s ratio failed to correlate with residual MVT or gait function in the second cohort (data not shown).

TA muscle coherence, time of evolution and severity of incomplete SCI

Intramuscular 15-30 Hz TA coherence calculated either during maximal isometric or isokinetic activation in

subjects with SCI recruited from the second cohort (Table 2) also revealed differences in individuals diagnosed according to AIS severity and time from injury. In subjects diagnosed as AIS D, higher 15–30 Hz TA coherence was estimated during isometric activation at 100% of MVT (0.17, 0.12-0.20) when compared to individuals diagnosed with a SCI grade of AIS C (0.13, 0.06-0.13; $p = 0.019$, Figure 3B). Furthermore 15-30 Hz TA coherence activity estimated during 120°/s isokinetic activation was higher in subjects with AIS D (0.27, 0.15-0.40) compared to AIS C (0.08, 0.04-0.15, $p = 0.015$) (Figure 3B) and also for the 10-16 Hz frequency band (AIS D, 0.33, 0.04-0.20 compared to AIS C 0.12, 0.17-0.44; $p = 0.035$ Figure 3A). This was also the case when the ratio of 15-30 Hz TA coherence was calculated during isokinetic activation for the 120/60°/s ratio; AIS D (1.9, 1.7-3.4) and AIS C (1.00, 0.6-1.4, $p = 0.019$). No differences were found for the other movement tasks or specific coherence frequency bands. Finally a positive correlation was determined between the TA coherence calculated as the 120/60°/s ratio within the 24-40 Hz frequency band and the time from SCI, significantly for the first cohort ($\rho = 0.54$, $p = 0.05$) and as a trend for the second SCI cohort ($\rho = 0.50$, $p = 0.07$).



TA coherence and specific spasticity symptoms after spinal cord injury

Analysis of the impact of spasticity on intramuscular TA coherence was performed in 14 subjects with SCI in the second cohort compared to seven subjects without SCI spasticity (Table 4 and Figure 4A and 4B). In general no

Table 3 Correlation between isometric activation at 100% of MVT intramuscular TA coherence with residual muscle strength and gait function in subjects with SCI in Cohort II

Frequency ranges (Hz)	MVT (Nm)	WISCI II (21 points)
10-16 Hz	0.07 $p = 0.74$	0.26 $p = 0.24$
15-30 Hz	0.50 $p = 0.01$	0.41 $p = 0.05$
24-40 Hz	0.41 $p = 0.05$	<i>0.40</i> $p = 0.06$
40-60 Hz	0.01 $p = 0.95$	0.36 $p = 0.10$

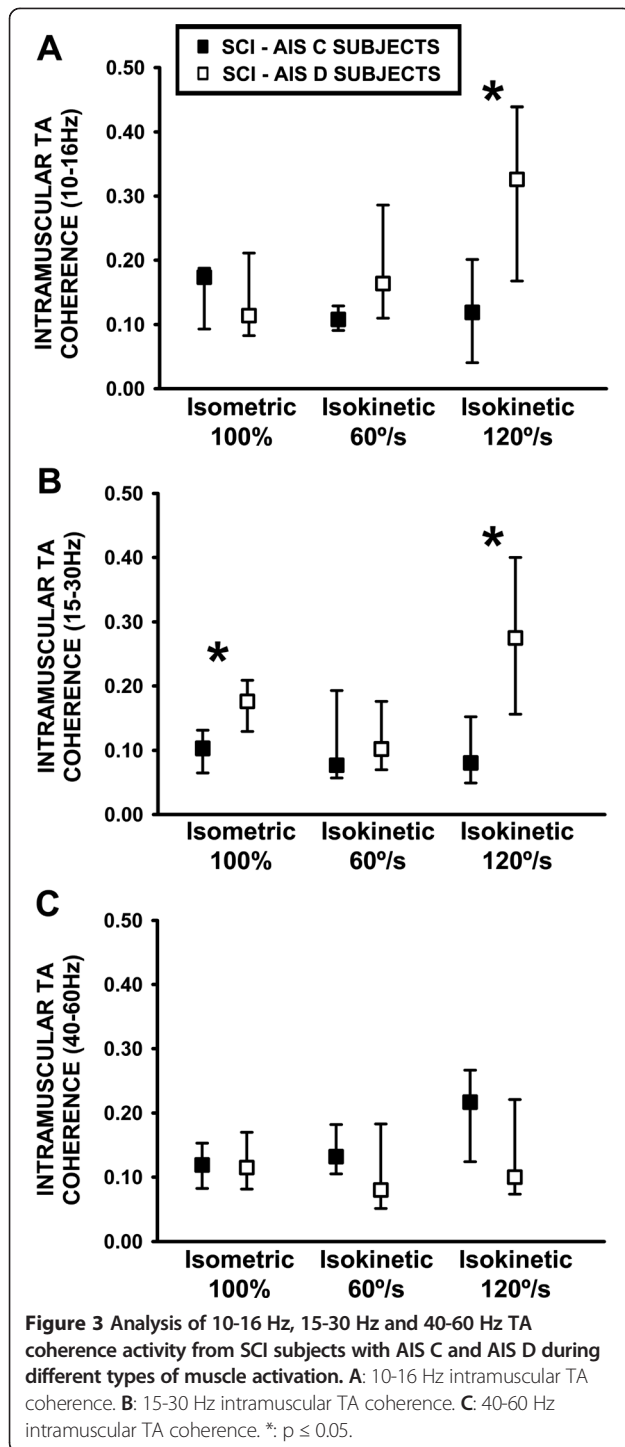
MVT (Nm): maximal voluntary torque; TA: Tibialis Anterior. $n = 21$. $p \leq 0.05$ in bold and $p \leq 0.06$ in italics.

differences were identified for TA coherence observed during isometric activation at 100% of MVT for subjects diagnosed without or with spasticity within the 10–16 Hz, 15–30 Hz, 24–40 Hz or 40–60 Hz bands (Figure 3A) even though a non-significant higher level of coherence activity was identified within the lower frequency band in the SCI spasticity group. TA coherence calculated as the ratio of 120/60°/s isokinetic activation was higher in the group with SCI spasticity (2.18, 1.03-2.89, $p = 0.05$) compared to individuals without spasticity (0.90, 0.64-1.47, Figure 4B).

Correlation analysis of the relationship between TA coherence activity estimated during isometric activation at 100% of MVT with specific symptoms of SCI spasticity generally revealed a negative effect of muscle hyper-tonia, passive resistive torque, and involuntary muscle contractions within different bandwidths (Table 4). Specifically, passive resistive torque to ankle dorsiflexion in subjects with spasticity measured at 30°/s ($\rho = -0.58$, $p = 0.04$) or 120°/s ($\rho = -0.59$, $p = 0.03$) revealed a negative correlation with 10-16 Hz TA coherence. In contrast, the modified Ashworth scores correlated negatively with TA coherence within the higher 24-60 Hz TA frequency band (Table 4). The severity of evoked spasms measured with the SCATS also highlighted a negative relationship for high frequency 40-60 Hz TA coherence ($\rho = -0.56$, $p = 0.05$) and an inverse correlation trend was also present for the Penn score but only within the 15-30 Hz bandwidth. In contrast, a positive correlation was identified between the degree of clonus activity and TA coherence estimated during isometric activation at 100% of MVT within the low frequency 10–16 Hz bandwidth.

Discussion

This is the first study that has systematically analyzed intramuscular TA coherence from subjects with incomplete SCI during different movement tasks and within specific frequency bands between 10-60 Hz. Comprehensive analysis highlighted the functional and clinical relationship between specific TA muscle coherence activity with residual voluntary dorsiflexion strength, clinical characteristics of SCI including the severity and time from injury, and the negative impact of different spasticity signs. Estimation of standard



15–30 Hz TA coherence during maximal isometric contraction or fast (120°/s) isokinetic movement was related to several functional and clinical parameters in subjects with SCI, while a novel change in 40–60 Hz coherence was identified specifically in subjects with clinical measures of SCI spasticity. The identification of the optimal task and frequency bands required to support the physiological and

functional significance of TA coherence activity should facilitate the diagnosis of motor recovery mediated by central motor control mechanisms, in addition to detecting early signs of adaptive and maladaptive neuroplasticity during subacute neurorehabilitation after incomplete SCI.

TA coherence estimation: Relationship with strength and velocity of voluntary muscle contraction after SCI

Several clinical studies have demonstrated that 15-30 Hz muscle coherence reflect neural activation of muscle function via cortical activation of synchronous motor units in antagonist muscles [28,56]. Indeed both intramuscular and intermuscular coherence is often regarded as an indirect measure of corticospinal activity [56-58]. In this study isometric activation at 100% of MVT was identified as the best controlled movement task to demonstrate higher 15-30 Hz TA motor unit synchronisation in subjects clinically graded with less severe SCI, but not when compared to the non-injured group (c.f. 40-60 Hz activity). Muscle coherence estimation has previously been estimated in the lower limb of healthy subjects, especially during tasks that involve co-contraction of lower limb muscles at the same joint, such as with balance [17], a motor task mediated by a subpopulation of the total corticospinal system [6]. In other studies isometric contraction has demonstrated changes in motor unit synchronisation following SCI or motoneuron disease [15,27,29].

In the present study several consistent correlations indicated that 15-30 Hz TA coherence calculated during isometric activation at 100% of MVT correlated significantly with muscle strength following SCI. The reduction or absence of lower limb muscle coherence with an associated loss of lower limb muscle strength following damage to the corticospinal pathway has been identified at these frequencies [11,22,25,26]. Furthermore recovery of corticospinal tract function in subjects with incomplete SCI during intensive locomotor training has been measured directly neurophysiologically in parallel with an increase in TA motor unit synchronisation [15], suggesting that estimations of muscle coherence may approximate descending motor control function.

Systematic analysis of TA coherence in this study also revealed consistently higher values for all the frequency bands when calculated during fast isokinetic dorsiflexion in subjects with SCI, compared to healthy subjects. However when TA motor unit synchronisation was compared within subjects with different grades of SCI, higher velocity-dependent coherence activity was observed in subjects with a more incomplete SCI, but only within the 10-16 Hz and 15-30 Hz bandwidths. In this regard, recovery of cortical motor evoked potential amplitude during subacute SCI correlated only with maximal movement velocity of dorsiflexion rather than maximal

Table 4 Correlational analysis between intramuscular TA coherence calculated during isometric activation at 100% of MVT with spasticity measures in subjects with SCI in Cohort II

Frequency ranges	Ashw	PRT 30°/s	PRT 120°/s	Penn	SCATS	Clonus
10-16 Hz	0.22 <i>p</i> = 0.45	-0.58 p = 0.04	-0.59 p = 0.03	0.03 <i>p</i> = 0.90	-0.05 <i>p</i> = 0.80	0.58 p = 0.04
15-30 Hz	-0.30 <i>p</i> = 0.09	-0.41 <i>p</i> = 0.17	-0.39 <i>p</i> = 0.19	-0.53 <i>p</i> = 0.06	-0.18 <i>p</i> = 0.54	0.25 <i>p</i> = 0.41
24-40 Hz	-0.58 p = 0.02	-0.15 <i>p</i> = 0.61	-0.17 <i>p</i> = 0.57	-0.18 <i>p</i> = 0.55	-0.33 <i>p</i> = 0.27	-0.41 <i>p</i> = 0.16
40-60 Hz	-0.60 p = 0.02	-0.26 <i>p</i> = 0.38	-0.23 <i>p</i> = 0.45	0.16 <i>p</i> = 0.60	-0.56 p = 0.05	-0.04 <i>p</i> = 0.88

MVT (Nm): maximal voluntary torque. Ashw: Ashworth scale during knee flexion. PRT: passive resistive torque to dorsiflexion. SCATS: total flexor and extensor spasm. n = 21. *p* ≤ 0.05 in bold and *p* ≤ 0.06 in italics.

isometric muscle strength in general [31,32]. Indeed hyperexcitability of the corticospinal system demonstrated during task dependent movement conditions may reflect cortical compensation for the functional deficit produced following SCI [59] leading to higher coherence activity in subjects with mild AIS scores.

This study also supports the relatively new identification of the physiological relevance of 40-60 Hz EMG coherence activity [37]. Lower 40-60 Hz TA coherence activity observed in subjects with SCI during isometric activation at 100% of MVT in the second cohort was clear, but no functional correlation was identified with this high frequency TA coherence activity and muscle strength, gait or SCI severity. Coherence activity within the 40-60 Hz band has been associated with non-pyramidal tract neuronal activity possibly related to residual activity within either reticulospinal and/or propriospinal tracts following SCI [37] or following motor neurone disease [27]. Both these studies suggest that measurement of high-frequency activity may lead to important physiological information regarding mechanisms of functional recovery unrelated to corticospinal neuroplasticity after SCI [27,37].

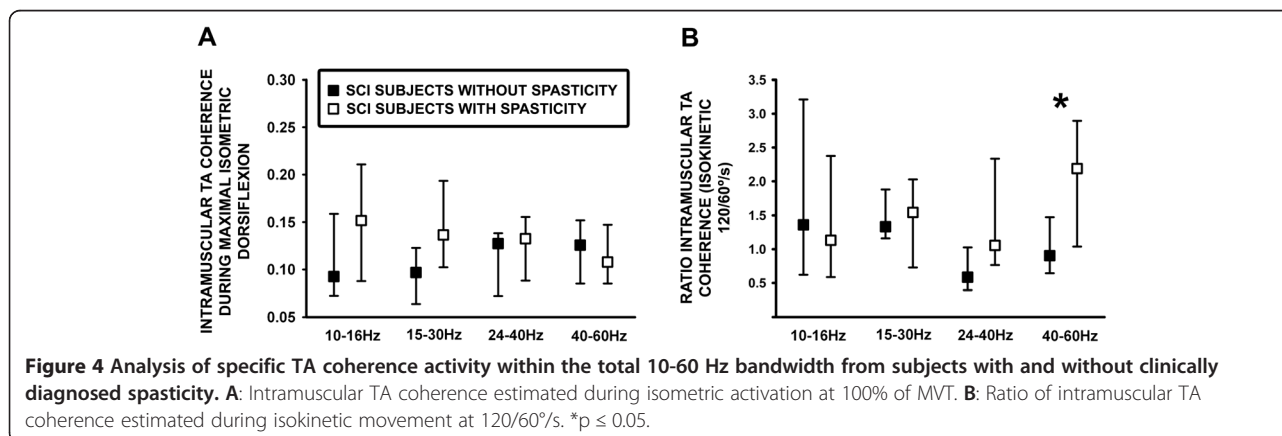
TA coherence estimation as an approximation of residual clinical motor function after SCI

Residual voluntary motor function after SCI is initially diagnosed with the AIS scale, which characterises AIS C from AIS D with the presence of useful motor activity but without normal strength or gait [4]. Furthermore both SCI grades are associated with a different degree of motor recovery throughout the course of subacute SCI [3], which is usually corroborated with neurophysiological testing of corticospinal motor evoked potentials [60]. The results from our study also suggest that the estimation of 15-30 Hz TA coherence during isometric contraction may be useful as an approximation of corticospinal function and SCI grade based on higher motor unit synchronization in subjects diagnosed as AIS D compared to AIS C. This observation is supported by the correlation between motor evoked potentials amplitude, motor recovery and muscle coherence activity stimulated in subjects with SCI identified during rehabilitation [15].

Subjects diagnosed within the AIS D classification group demonstrate different degrees of gait function, which is usually assessed by qualitative clinical tests in the rehabilitation setting [43,61]. It is of interest to note therefore that calculation of 15-30 Hz TA coherence activity estimated during isometric movement also correlates with the grade of gait function (WISCI II). Other studies have also shown the clinical utility of measurement of motor unit synchronization, corticospinal tract integrity and gait function after SCI [13,15], particularly as TA coherence activity within this frequency band is strongly reduced or absent after SCI [22].

TA coherence estimation and SCI spasticity

The pathophysiology of spasticity following SCI is complex and most probably involves parallel changes in pyramidal, extrapyramidal and spinal motor control mechanisms [62-64], some of which are better evaluated during residual voluntary motor activity function [6]. Many symptoms of motor dysfunction have been



associated with subjects with spasticity, including muscle hypertonia, spinal hyperreflexia, coactivation, spasms and clonus [6,8,63]. Although no difference was observed for TA coherence activity in subjects with or without spasticity during isometric dorsiflexion, correlational analysis revealed inverse relationships between motor unit synchronisation and several symptoms of spasticity within the low (10-16 Hz) and high (40-60 Hz) frequency bands. Specifically passive resistive torque in subjects with hypertonia inversely correlated with 10-16 Hz TA coherence activity, in contrast to the modified Ashworth or SCATS scores which negatively correlated with high frequency (40-60 Hz) motor unit synchronisation. Interestingly another study also associated low-frequency coherence activity with neuronal activity within spinal pathways [25,26], which would explain the relationship between TA coherence within this bandwidth and the tonic stretch reflex activity. Of passing interest here also is that clonus activity [65] measured in patients with spasticity was associated positively with 10-16 Hz TA coherence activity supporting the hypothesis that clonus and passive tonic stretch reflex activity measured in subjects with spasticity are predominantly mediated via different spinal mechanisms [66]

In contrast the association between high frequency 40-60 Hz TA coherence activity and the clinical measures of spasticity (modified Ashworth scale and SCATS) most probably reflects central neuronal activity unrelated to the 15-30 Hz activity that approximates pyramidal activity (see above). Indeed evidence suggests that lower limb hypertonia, as assessed with the modified Ashworth scale, may also be mediated by hyperexcitability of extrapyramidal neuronal mechanisms organized at the brainstem level [67].

TA coherence activity as an approximation of adaptive and maladaptive neuroplasticity after SCI

The presence of both muscle hypertonia and evoked spasm activity in subjects with lower 40-60 Hz coherence following SCI also suggests that non-pyramidal adaptive mechanisms could mediate residual motor recovery, which would be masked by the development of spasticity in our cohort. Closer neurophysiological analysis of the activity within these pathways after SCI should be made to provide more detailed evidence regarding both maladaptive neuroplasticity related to spasticity [68] and adaptive neuroplasticity related to recovery of residual motor function [69,70].

It is interesting to observe the correlation between the time from SCI with 15-30 Hz and 24-40 Hz TA motor unit synchronisation estimated during fast isokinetic movement which suggests that a closer examination of velocity-dependent dorsiflexor muscle coherence activity would provide prognostic information regarding the potential for residual motor function recovery. Indeed

coherence activity calculated within these mid-range frequency bands during maximal isometric contraction also correlate with gait function after SCI in our study. Whether recovery of gait function depends on the development of velocity-dependent activity of residual pyramidal and extrapyramidal motor control systems after incomplete SCI will need to be addressed with more sophisticated neurophysiological techniques.

Clinical application and limitations of intramuscular TA coherence estimation

Measurement of TA motor unit synchronisation as an approximation for descending motor control activity in subjects with incomplete SCI within the neurorehabilitation setting is an obvious clinical goal. In addition the possibility that TA coherence activity could reflect residual motor control recovery with training or deterioration following the development of spasticity needs to be addressed in a closely controlled subacute longitudinal study of SCI. Further studies should more closely analyse the functional significance of a more detailed coherence spectra in the future with longer EMG signals which will lead to a more precise identification of the frequency bands. In addition analysis of EMG coherence in those subjects with SCI with low levels of muscle contraction should be preprocessed using rectification [41].

Conclusion

Intramuscular TA coherence estimation calculated between 15-30 Hz or 40-60 Hz during isometric activation at 100% of MVT or during fast 120°/s isokinetic activation may provide important diagnostic information regarding the state of voluntary motor control mechanisms following incomplete SCI. In patients without spasticity these coherence bands may reflect recovery of residual motor control. In contrast the clinical diagnosis of muscle hypertonia and evoked involuntary muscle spasms negatively affect 40-60 Hz TA coherence estimation. Systematic analysis of TA motor unit synchronization during specific motor tasks within specific bandwidths provides a basis for the development of a quantitative diagnostic method that approximate adaptive and maladaptive lower limb residual motor control mechanisms and neuroplasticity during subacute SCI. Further studies in a larger cohort of subjects with incomplete SCI, using longer rectified EMG signals will be required to test this hypothesis, including corroborative data obtained from neurophysiological and functional longitudinal studies.

Abbreviations

EMG: Electromyographic activity; SCI: Spinal cord injury; TA: Tibialis anterior; AIS: American spinal injury association impairment scale; MVT: Maximal voluntary torque; SCATS: Spinal cord assessment tool for spastic reflexes scale; MUAP: Motor unit action potential.

Competing interests

The authors declare that they have no competing interests.

Authors' contributions

EBE participated in collecting the subject data, conducting data and statistical analysis, and helped to draft the manuscript. MA developed the software required to analyse EMG activity and muscle coherence analyses. CS helped collect the subject data and to draft the manuscript. DT and JLP helped to draft the manuscript and supervise the research. JT and JG-S conceived the study, interpreted the data, drafted the manuscript and critically revised it. All authors read and approved the final manuscript.

Acknowledgements

This project was funded by the Spanish Ministry of Science and Innovation CONSOLIDER-INGENIO HYPER (Hybrid NeuroProsthetic and NeuroRobotic Devices for Functional Compensation and Rehabilitation of Motor Disorders, CSD2009-00067) project. Also financed by the Fundación Mutual Madrileña (2010), Fiscam (PI2010/030) and Pfizer (LIRA to JST).

Author details

¹Sensorimotor Function Group, Hospital Nacional de Paraplégicos, Toledo, Spain. ²Spanish National Research Council (CSIC), Madrid, Spain. ³Nursing and Physiotherapy School, Castilla La Mancha University, Toledo, Spain.

Received: 15 February 2013 Accepted: 12 February 2014

Published: 4 March 2014

References

- Pershous KJ, Barker RN, Kendall MB, Buettner PG, Kuipers P, Schuurs SB, Amstutz DL: **Investigating changes in quality of life and function along the lifespan for people with spinal cord injury.** *Arch Phys Med Rehabil* 2012, **93**:413–419.
- Devivo MJ: **Epidemiology of traumatic spinal cord injury: trends and future implications.** *Spinal Cord* 2012, **50**:365–372.
- Fawcett JW, Curt A, Steeves JD, Coleman WP, Tuszynski MH, Lammertse D, Bartlett PF, Blight AR, Dietz V, Ditunno J, Dobkin BH, Havton LA, Ellaway PH, Fehlings MG, Privat A, Grossman R, Guest JD, Kleitman N, Nakamura M, Gairia M, Short D: **Guidelines for the conduct of clinical trials for spinal cord injury as developed by the ICCP panel: spontaneous recovery after spinal cord injury and statistical power needed for therapeutic clinical trials.** *Spinal Cord* 2007, **45**:190–205.
- Maynard FM, Bracken MB, Creasey G, Ditunno JF Jr, Donovan WH, Ducker TB, Garber SL, Marino RJ, Stover SL, Tator CH, Waters RL, Wilberger JE, Young W: **International Standards for Neurological and Functional Classification of Spinal Cord Injury.** American Spinal Injury Association. *Spinal Cord* 1997, **35**:266–274.
- McKay WB: **Neurophysiological characterization of the 'new anatomy' and motor control that results from neurological injury or disease.** *Clin Neurol Neurosurg* 2012, **114**:447–454.
- Gomez-Soriano J, Castellote JM, Perez-Rizo E, Esclarin A, Taylor JS: **Voluntary ankle flexor activity and adaptive coactivation gain is decreased by spasticity during subacute spinal cord injury.** *Exp Neurol* 2010, **224**:507–516.
- BurrIDGE JH, Wood DE, Hermens HJ, Voerman GE, Johnson GR, van Wijck F, Platz T, Gregoric M, Hitchcock R, Pandyan AD: **Theoretical and methodological considerations in the measurement of spasticity.** *Disabil Rehabil* 2005, **27**:69–80.
- Gomez-Soriano J, Cano-de-la-Cuerda R, Munoz-Hellin E, Ortiz-Gutierrez R, Taylor JS: **Evaluation and quantification of spasticity: a review of the clinical, biomechanical and neurophysiological methods.** *Rev Neurol* 2012, **55**:217–226.
- Little JW, Micklesen P, Umlauf R, Britell C: **Lower extremity manifestations of spasticity in chronic spinal cord injury.** *Am J Phys Med Rehabil* 1989, **68**:32–36.
- Bravo-Esteban E, Taylor J, Abián-Vicén J, Albu S, Simón-Martínez C, Torricelli D, Gómez-Soriano JI, et al: **Impact of specific symptoms of spasticity on voluntary lower limb muscle function, gait and daily activities during subacute and chronic spinal cord injury.** *J NeuroRehabilitation* 2013. In press.
- Farmer SF, Bremner FD, Halliday DM, Rosenberg JR, Stephens JA: **The frequency content of common synaptic inputs to motoneurons studied during voluntary isometric contraction in man.** *J Physiol* 1993, **470**:127–155.
- Halliday DM, Conway BA, Christensen LO, Hansen NL, Petersen NP, Nielsen JB: **Functional coupling of motor units is modulated during walking in human subjects.** *J Neurophysiol* 2003, **89**:960–968.
- Barthelemy D, Willerslev-Olsen M, Lundell H, Conway BA, Knudsen H, Biering-Sorensen F, Nielsen JB: **Impaired transmission in the corticospinal tract and gait disability in spinal cord injured persons.** *J Neurophysiol* 2010, **104**:1167–1176.
- Hansen NL, Hansen S, Christensen LO, Petersen NT, Nielsen JB: **Synchronization of lower limb motor unit activity during walking in human subjects.** *J Neurophysiol* 2001, **86**:1266–1276.
- Norton JA, Gorassini MA: **Changes in cortically related intermuscular coherence accompanying improvements in locomotor skills in incomplete spinal cord injury.** *J Neurophysiol* 2006, **95**:2580–2589.
- Smith HC, Davey NJ, Savic G, Maskill DW, Ellaway PH, Frankel HL: **Motor unit discharge characteristics during voluntary contraction in patients with incomplete spinal cord injury.** *Exp Physiol* 1999, **84**:1151–1160.
- Gibbs J, Harrison LM, Stephens JA: **Organization of inputs to motoneurone pools in man.** *J Physiol* 1995, **485**(1):245–256.
- Kakuda N, Nagaoka M, Wessberg J: **Common modulation of motor unit pairs during slow wrist movement in man.** *J Physiol* 1999, **520**(3):929–940.
- Cros D, Soto O, Chiappa KH: **Transcranial magnetic stimulation during voluntary action: directional facilitation of outputs and relationships to force generation.** *Brain Res* 2007, **1185**:103–116.
- Zoghi M, Nordstrom MA: **Progressive suppression of intracortical inhibition during graded isometric contraction of a hand muscle is not influenced by hand preference.** *Exp Brain Res* 2007, **177**(2):266–274.
- Weier AT, Pearce AJ, Kidgell DJ: **Strength training reduces intracortical inhibition.** *Acta Physiol (Oxf)* 2012, **206**(2):109–119.
- Hansen NL, Conway BA, Halliday DM, Hansen S, Pyndt HS, Biering-Sorensen F, Nielsen JB: **Reduction of common synaptic drive to ankle dorsiflexor motoneurons during walking in patients with spinal cord lesion.** *J Neurophysiol* 2005, **94**:934–942.
- Kilner JM, Baker SN, Salenius S, Jousmäki V, Hari R, Lemon RN: **Task-dependent modulation of 15–30 Hz coherence between rectified EMGs from human hand and forearm muscles.** *J Physiol* 1999, **516**(2):559–570.
- Farmer SF, Gibbs J, Halliday DM, Harrison LM, James LM, Mayston MJ, Stephens JA: **Changes in EMG coherence between long and short thumb abductor muscles during human development.** *J Physiol* 2007, **579**:389–402.
- Norton JA, Wood DE, Marsden JF, Day BL: **Spinally generated electromyographic oscillations and spasms in a low-thoracic complete paraplegic.** *Mov Disord* 2003, **18**:101–106.
- Norton JA, Wood DE, Day BL: **Is the spinal cord the generator of 16-Hz orthostatic tremor?** *Neurology* 2004, **62**:632–634.
- Fisher KM, Zaaimi B, Williams TL, Baker SN, Baker MR: **Beta-band intermuscular coherence: a novel biomarker of upper motor neuron dysfunction in motor neuron disease.** *Brain* 2012, **135**:2849–2864.
- Jackson A, Spinks RL, Freeman TC, Wolpert DM, Lemon RN: **Rhythm generation in monkey motor cortex explored using pyramidal tract stimulation.** *J Physiol* 2002, **541**:685–699.
- Baker MR, Baker SN: **The effect of diazepam on motor cortical oscillations and corticomuscular coherence studied in man.** *J Physiol* 2003, **546**:931–942.
- Brouwer B, Ashby P: **Corticospinal projections to lower limb motoneurons in man.** *Exp Brain Res* 1992, **89**:649–654.
- Wirth B, Van Hedel HJ, Curt A: **Changes in corticospinal function and ankle motor control during recovery from incomplete spinal cord injury.** *J Neurotrauma* 2008, **25**:467–478.
- Wirth B, van Hedel HJ, Curt A: **Ankle paresis in incomplete spinal cord injury: relation to corticospinal conductivity and ambulatory capacity.** *J Clin Neurophysiol* 2008, **25**:210–217.
- Maynard FM, Karunas RS, Waring WP 3rd: **Epidemiology of spasticity following traumatic spinal cord injury.** *Arch Phys Med Rehabil* 1990, **71**:566–569.
- Skold C, Levi R, Seiger A: **Spasticity after traumatic spinal cord injury: nature, severity, and location.** *Arch Phys Med Rehabil* 1999, **80**:1548–1557.
- Sköld C: **Spasticity in spinal cord injury: self- and clinically rated intrinsic fluctuations and intervention-induced changes.** *Arch Phys Med Rehabil* 2000, **81**:144–149.
- Curt A, Schwab ME, Dietz V: **Providing the clinical basis for new interventional therapies: refined diagnosis and assessment of recovery after spinal cord injury.** *Spinal Cord* 2004, **42**:1–6.

37. Nishimura Y, Morichika Y, Isa T: **A subcortical oscillatory network contributes to recovery of hand dexterity after spinal cord injury.** *Brain* 2009, **132**(3):709–721.
38. Seddon HWJ: **Medical Research Council: Aids to the exam of the peripheral nervous system.** In *in Memorandum 45*. London: Her Majesty's Stationery Office; 1976.
39. Bohannon RW, Smith MB: **Interrater reliability of a modified Ashworth scale of muscle spasticity.** *Phys Ther* 1987, **67**:206–207.
40. Penn RD, Savoy SM, Corcos D, Latash M, Gottlieb G, Parke B, Kroin JS: **Intrathecal baclofen for severe spinal spasticity.** *N Engl J Med* 1989, **320**:1517–1521.
41. Farina D, Negro F, Jiang N: **Identification of common synaptic inputs to motor neurons from the rectified electromyogram.** *J Physiol* 2013, **591**(10):2403–2418.
42. Halliday DM, Rosenberg JR, Amjad AM, Breeze P, Conway BA, Farmer SF: **A framework for the analysis of mixed time series/point process data—theory and application to the study of physiological tremor, single motor unit discharges and electromyograms.** *Prog Biophys Mol Biol* 1995, **64**:237–278.
43. Ditunno JF Jr, Ditunno PL, Graziani V, Scivoletto G, Bernardi M, Castellano V, Marchetti M, Barbeau H, Frankel HL, D'Andrea Greve JM, Ko HY, Marshall R, Nance P: **Walking index for spinal cord injury (WISCI): an international multicenter validity and reliability study.** *Spinal Cord* 2000, **38**:234–243.
44. Benz EN, Hornby TG, Bode RK, Scheidt RA, Schmit BD: **A physiologically based clinical measure for spastic reflexes in spinal cord injury.** *Arch Phys Med Rehabil* 2005, **86**:52–59.
45. Rabita G, Dupont L, Thevenon A, Lenseil-Corbeil G, Perot C, Vanvelcenaher J: **Quantitative assessment of the velocity-dependent increase in resistance to passive stretch in spastic plantarflexors.** *Clin Biomech (Bristol, Avon)* 2005, **20**:745–753.
46. Gardner WA: **A unifying view of coherence in signal processing.** *Signal Process* 1992, **29**:113–140.
47. Welch P: **The use of fast Fourier transform for the estimation of power spectra: a method based on time averaging over short, modified periodograms.** *Audio and Electroacoustics, IEEE Transactions* 1967, **15**:70–73.
48. Harris FJ: **On the use of windows for harmonic analysis with the discrete Fourier transform.** *Proceedings of the IEEE* 1978, **66**:51–83.
49. Farina D, Merletti R, Enoka RM: **The extraction of neural strategies from the surface EMG.** *J Appl Physiol* 2004, **96**:1486–1495.
50. Neto OP, Christou EA: **Identification of oscillatory input to the muscle rectification of the EMG signal impairs the identification of oscillatory input to the muscle.** *J Neurophysiol* 2010, **103**:1093–1103.
51. McClelland VM, Cvetkovic Z, Mills KR: **Rectification of the EMG is an unnecessary and inappropriate step in the calculation of Corticomuscular coherence.** *J Neurosci Methods* 2012, **205**:190–201.
52. Yao B, Salenius S, Yue GH, Brown RW, Liu JZ: **Effects of surface EMG rectification on power and coherence analyses: an EEG and MEG study.** *J Neurosci Methods* 2007, **159**:215–223.
53. Myers LJ, Lowery M, O'Malley M, Vaughan CL, Heneghan C, St Clair Gibson A, Harley YX, Sreenivasan R: **Rectification and non-linear pre-processing of EMG signals for cortico-muscular analysis.** *J Neurosci Methods* 2003, **124**:157–165.
54. Stegeman DF, van de Ven WJ, van Elswijk GA, Oostenveld R, Kleine BU: **The alpha-motoneuron pool as transmitter of rhythmicities in cortical motor drive.** *Clin Neurophysiol* 2010, **121**:1633–1642.
55. Boonstra TW, Breakspear M: **Neural mechanisms of intermuscular coherence: implications for the rectification of surface electromyography.** *J Neurophysiol* 2012, **107**(3):796–807.
56. Kilner JM, Baker SN, Salenius S, Hari R, Lemon RN: **Human cortical muscle coherence is directly related to specific motor parameters.** *J Neurosci* 2000, **20**:8838–8845.
57. Conway BA, Halliday DM, Farmer SF, Shahani U, Maas P, Weir AI, Rosenberg JR: **Synchronization between motor cortex and spinal motoneuronal pool during the performance of a maintained motor task in man.** *J Physiol* 1995, **489**(Pt 3):917–924.
58. Halliday DM, Conway BA, Farmer SF, Rosenberg JR: **Using electroencephalography to study functional coupling between cortical activity and electromyograms during voluntary contractions in humans.** *Neurosci Lett* 1998, **241**:5–8.
59. Lundell H, Christensen MS, Barthélemy D, Willerslev-Olsen M, Biering-Sørensen F, Nielsen JB: **Cerebral activation is correlated to regional atrophy of the spinal cord and functional motor disability in spinal cord injured individuals.** *Neuroimage* 2011, **54**(2):1254–1261.
60. Curt A, Keck ME, Dietz V: **Functional outcome following spinal cord injury: significance of motor-evoked potentials and ASIA scores.** *Arch Phys Med Rehabil* 1998, **79**:81–86.
61. van Hedel HJ, Dietz V, Curt A: **Assessment of walking speed and distance in subjects with an incomplete spinal cord injury.** *Neurorehabil Neural Repair* 2007, **21**:295–301.
62. Nielsen JB, Crone C, Hultborn H: **The spinal pathophysiology of spasticity—from a basic science point of view.** *Acta Physiol (Oxf)* 2007, **189**:171–180.
63. Biering-Sørensen F, Nielsen JB, Klinge K: **Spasticity-assessment: a review.** *Spinal Cord* 2006, **44**:708–722.
64. Adams MM, Hicks AL: **Spasticity after spinal cord injury.** *Spinal Cord* 2005, **43**:577–586.
65. Wallace DM, Ross BH, Thomas CK: **Characteristics of lower extremity clonus after human cervical spinal cord injury.** *J Neurotrauma* 2012, **29**:915–924.
66. Boyraz I, Oktay F, Celik C, Akyuz M, Uysal H: **Effect of cold application and tizanidine on clonus: clinical and electrophysiological assessment.** *J Spinal Cord Med* 2009, **32**:132–139.
67. Kumru H, Stetkarova I, Schindler C, Vidal J, Kofler M: **Neurophysiological evidence for muscle tone reduction by intrathecal baclofen at the brainstem level.** *Clin Neurophysiol* 2011, **122**:1229–1237.
68. Kumru H, Vidal J, Kofler M, Benito J, Garcia A, Valls-SolAC J: **Exaggerated auditory startle responses in patients with spinal cord injury.** *J Neurol* 2008, **255**:703–709.
69. Avila-Martin G, Galan-Arriero I, Gómez-Soriano J, Taylor J: **Treatment of rat spinal cord injury with the neurotrophic factor albumin-oleic acid: translational application for paralysis, spasticity and pain.** *PLoS One* 2011, **6**:e26107.
70. Courtine G, Gerasimenko Y, van den Brand R, Yew A, Musienko P, Zhong H, Song B, Ao Y, Ichiyama RM, Lavrov I, Roy RR, Sofroniew MV, Edgerton VR: **Transformation of nonfunctional spinal circuits into functional states after the loss of brain input.** *Nat Neurosci* 2009, **12**:1333–1342.

doi:10.1186/1743-0003-11-23

Cite this article as: Bravo-Esteban et al.: Tibialis Anterior muscle coherence during controlled voluntary activation in patients with spinal cord injury: diagnostic potential for muscle strength, gait and spasticity. *Journal of NeuroEngineering and Rehabilitation* 2014 **11**:23.

Submit your next manuscript to BioMed Central and take full advantage of:

- Convenient online submission
- Thorough peer review
- No space constraints or color figure charges
- Immediate publication on acceptance
- Inclusion in PubMed, CAS, Scopus and Google Scholar
- Research which is freely available for redistribution

Submit your manuscript at
www.biomedcentral.com/submit

