



Establishing predictive models for malignant and inflammatory pulmonary nodules using clinical data and CT imaging features

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Background: The detection of pulmonary nodules has become increasingly common; however, accurate qualitative diagnosis remains a clinical challenge. This study sought to distinguish between malignant and inflammatory solid lung nodules using clinical data and computed tomography (CT) imaging features.

Methods: A total of 948 patients with pulmonary nodules who underwent surgery or percutaneous biopsy from four centers were included in the study. The patients were divided into the following four groups based on nodule diameter: Group 1: nodules ≤ 10 mm; Group 2: nodules >10 and ≤ 20 mm; Group 3: nodules >20 and ≤ 30 mm; and Group 4: all nodules. The independent risk factors were identified and merged by univariate and multivariate analyses in the four groups to establish four models. The overall performance of the four models was evaluated using the area under the curve (AUC) of the receiver operating characteristic curve. Differences between Models 1–3 and Model 4 were compared using the DeLong test.

Results: Of the nodules, 638 were classified as malignant and 310 as inflammatory. The patients with malignant and inflammatory nodules had median ages of 64.3 ± 9.8 and 56.0 ± 11.9 years, respectively ($P < 0.001$). To build the four models, 17 features were identified, of which 2 were clinical features and 15 were imaging features. Notably, the frequency of lobulation, age, multiple lesions, and satellite lesions was relatively high in the four models. The AUC, accuracy, sensitivity, and specificity of Models 1–4 were 0.861 (0.803–0.921), 73.5%, 81.0%, and 78.9%; 0.902 (0.873–0.931), 82.8%, 74.7%, and 88.0%; 0.943 (0.914–0.972), 90.5%, 87.3%, and 89.7%; and 0.921 (0.903–0.940), 84.7%, 83.1%, and 86.8%; respectively. However, there were no statistically significant differences between Models 1–3 and Model 4.

Conclusions: Our novel subgrouping models were able to effectively distinguish between inflammatory and malignant lung nodules using a reduced feature set. Our models could facilitate the accurate diagnosis of patients with potentially malignant lesions.

Keywords: Computed tomography image (CT image); prediction model; malignant; inflammatory pulmonary nodules

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Introduction

With the rise in global health awareness and the widespread adoption of early lung cancer screening, the detection of pulmonary nodules has become increasingly common (1-4). Lung cancer is the leading cause of cancer-related death worldwide (4) and is the most common cancer in China (5). In 2022, new cases of lung cancer accounted for 22.0% of all malignant tumors, and 28.5% of deaths were attributed to malignant tumors (5). Thus, the accurate qualitative diagnosis of pulmonary nodules is an important clinical issue that needs to be addressed (6,7). However, the pathological basis of pulmonary nodules is notably intricate and diverse (8), which adds to the diagnostic challenge they pose. Solid pulmonary nodules, in particular, have heightened diagnostic complexities compared to other nodule types (9). Timely detection, precise diagnosis, and prompt intervention are paramount in improving patient prognosis and the survival rate (10).

Computed tomography (CT) has emerged as the cornerstone imaging modality for lung nodule diagnosis (6,11-14) and plays an indispensable role in the assessment of lung nodules. Despite the use of established guidelines based on CT examinations, such as Fleischner's Guidelines and the American College of Chest Physicians Guidelines, existing models for predicting the benign and malignant nature of pulmonary nodules still lack optimal accuracy (15), potentially leading to delayed diagnosis and unnecessary invasive procedures (16).

Artificial intelligence (AI) has demonstrated promise in augmenting the interpretation of lung nodule malignancy. However, due to various limitations, such as those related to the development of universal AI algorithms, current AI models cannot be fully integrated into clinical practice, and their widespread clinical application is difficult (17). Standardized big data study on the application of AI for the adjunctive diagnosis of pulmonary nodules remain relatively scarce (11). Further, the accuracy of these models has yet to surpass that of manual interpretation (18-20). However, traditional logistic regression models can provide higher values for clinical use, this is because traditional logistic regression models are both interpretable and operable.

Guidelines issued by professional societies provide

clinicians and institutions with a framework for nodule management while allowing flexibility for individual patient decision making (12). Notably, the overwhelming majority (at least 95%) of pulmonary nodules identified are benign and commonly comprise granulomas or intrapulmonary lymph nodes (11). Research has established a positive correlation between nodule size on CT images and the likelihood of malignancy, such that nodule size serves as a primary determinant of nodule classification (21,22). Consequently, there is a pressing need to enhance the ability of physicians to differentiate between benign granulomas and malignant nodules, particularly in solid nodules.

The primary objective of this study was to establish a methodology that assists clinical diagnosticians to predict the malignancy of solid nodules through the use of clinical imaging models. Specifically, we conducted comprehensive quantitative and qualitative analyses of nodule characteristics based on clinical imaging parameters. Our analyses involved stratifying nodules by size and establishing a simple and convenient clinical imaging model. We present this article in accordance with the TRIPOD reporting checklist (available at <https://qims.amegroups.com/article/view/10.21037/qims-24-2338/rc>).

Methods

Study population

This multicenter retrospective study was conducted in accordance with the Declaration of Helsinki (as revised in 2013), and was approved by the respective Ethics Committees of Tongde Hospital of Zhejiang Province (No. 2022-029-JY), Anqing Municipal Hospital (No. 83230471), Taizhou Municipal Hospital (No. LWYJ2023059), and Shaoxing People's Hospital (No. 2019-K-Y-257-01). The requirement of individual informed consent for this retrospective analysis was waived. The study focused on incidentally detected lung nodules identified through CT scan imaging between 2014 and 2023. The dataset comprised the data of 5,201 patients who underwent surgical resection or percutaneous biopsy with confirmed pathologic results. The above-mentioned healthcare facilities maintain electronic health records and have

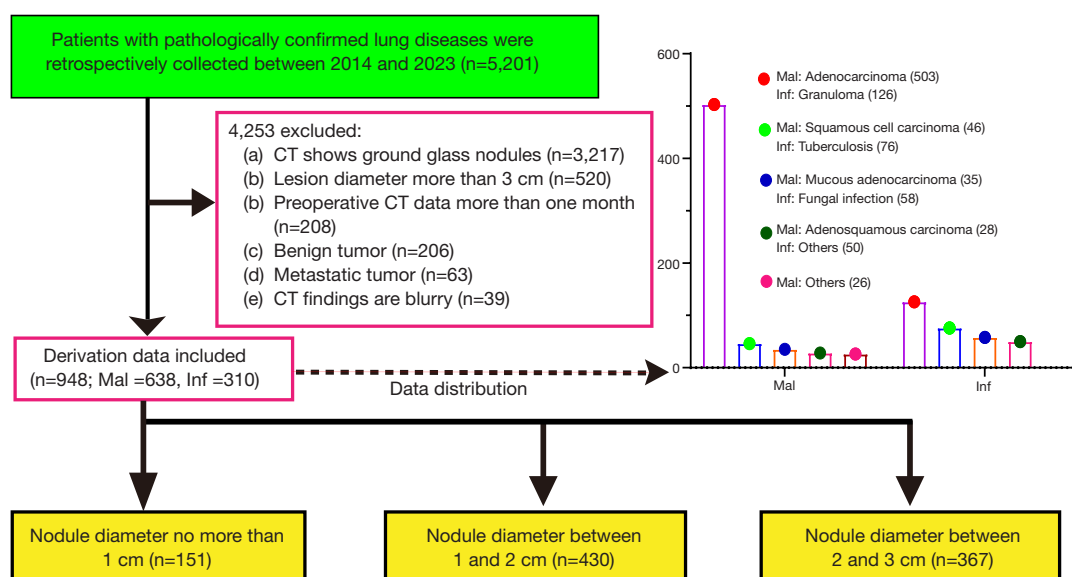


Figure 1 Flow chart showing selection of case samples. In total, 948 patients were selected according to the inclusion criteria. They were divided into the following four groups according to the CT nodule size: Group 1: nodules ≤ 10 mm; Group 2: nodules >10 and ≤ 20 mm; Group 3: nodules >20 and ≤ 30 mm; and Group 4: all nodules. CT, computed tomography; Inf, inflammatory; Mal, malignant.

standardized variable definitions for demographics, smoking history, surgical history, and tumor indicators. Patients were excluded from the study if they met any of the following exclusion criteria: (I) had ground-glass nodules on CT scans; (II) had a lesion diameter >3 cm; (III) had preoperative CT time interval more than one month; (IV) had benign tumors; (V) had metastatic tumors; and/or (VI) had blurry CT findings (Figure 1).

CT image acquisition

The chest CT scans were conducted using nine CT scanners (SOMATOM Definition Flash, FORCE CT, Sensation16, Definition AS 40, Siemens Medical, Forchheim, Germany; Revolution, Optima 680, LightSpeed VCT XT, GE Medical, Waukesha, WI, USA; Brilliant CT 64, Philips Medical, Best, Netherlands; and the Aquilion one tsx-301c CT, Canon Medical, Otawara, Japan). All patients were placed in the supine position with their arms raised and instructed to hold their breath at the end of a deep inhalation during scanning. The scanning area covered the area from the thoracic inlet to the level of the adrenal glands. The scanning parameters were set as follows: tube voltage: 120 kV; automatic tube current modulation technology; collimation: 0.6 mm or 0.625 mm (adjustable);

field of view (FOV) range: 360 mm \times 360 mm to 400 mm \times 400 mm; matrix: 512 \times 512 (fixed); and helical scanning speed: 0.6–0.8 seconds per rotation.

Images analysis

Two radiologists, who had 18 and 15 years of diagnostic radiography experience, respectively, and who were blinded to the patients' clinical information, independently analyzed the imaging features of the lung nodules. The radiologists performed the imaging analysis and evaluation on the CT characteristics of the nodules. When the evaluation results were consistent, they were directly accepted. In cases of disagreement, a third senior radiologist evaluated the results. All features were processed using the z-score normalization method to ensure the comparability of the quantitative and qualitative data. Intraclass correlation coefficients (ICCs) and the kappa test were separately used to evaluate the stability and homogenization of the imaging continuous and categorical feature extraction. After the observer analyses, a total of 15 imaging features with ICCs >0.75 (continuous variables) and kappa values >0.80 (categorized variables) were used in the subsequent modeling. All the CT images were displayed at standard lung [window width: 1,200–1,500 Hounsfield unit (HU),

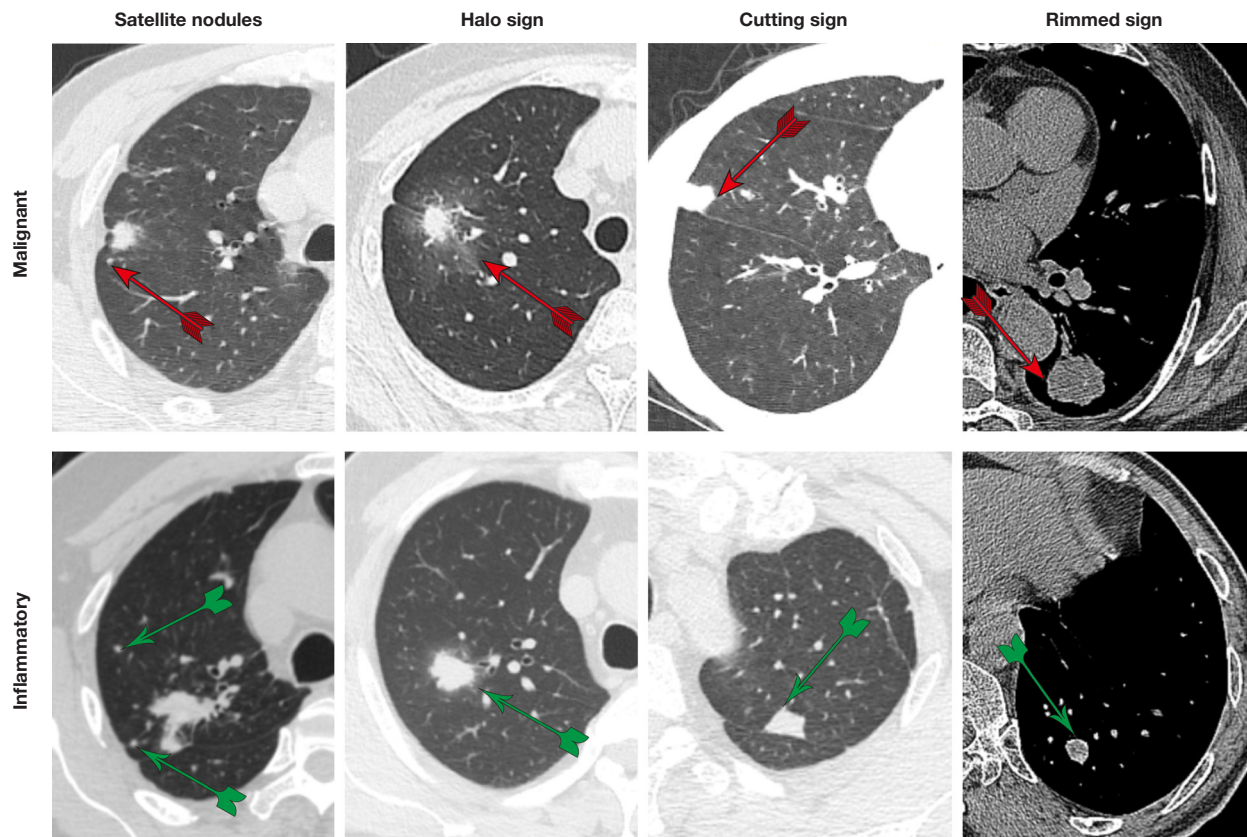


Figure 2 Four groups of imaging manifestations of inflammatory granuloma nodules and lung adenocarcinomas. The four groups of imaging manifestations are shown by red arrows in the malignant nodules and green arrows in the inflammatory nodules. “Satellite nodules” were defined as small solid nodules that are found surrounding a larger nodule. The “halo sign” appears on lung window settings as ground-glass opacity surrounding a pulmonary nodule or mass. The “cutting sign” indicates that the edge of the lesion is straight, resembling a knife cut, and has a diameter of >5 mm. The “rimmed sign” is defined as the ratio more than 3 or difference more than 100 HU of the mean CT value of the edge compared to the interior of a lung nodule. CT, computed tomography; HU, Hounsfield unit.

window level: -600 to -400 HU] and mediastinal (window width: 400 HU, window level: 40 HU) window settings.

The following characteristics were assessed: (I) the long diameter and short diameter (SD) of the nodules; (II) the intrapulmonary conditions, including emphysema/bullae, heterogeneous ventilation or perfusion, bronchiectasis or interstitial lung disease, and multiple lung comorbidity (MLC); (III) nodule signs and surroundings, such as location, lobulation, spiculation, airspace, air bronchogram, pleural tag, calcification, pleural effusion, the rimmed sign, satellite nodules, the halo sign, the cutting sign, mixed signs, and multiple lesions; and (IV) the quantitative CT characteristics of nodules, such as the maximum, minimum, mean, and standard deviation of the CT values. The “rimmed sign” was defined as the ratio of more than 3 or the difference of more than 100 HU of the mean CT value

of the edge compared to the interior of a lung nodule. “Multiple lesions” were defined as the presence of several nodules within the lungs, of which the largest nodule was selected for analysis. “Satellite nodules” were described as the small solid nodules that are found surrounding a larger nodule (11). The “Halo sign” was defined as ground-glass opacity surrounding a pulmonary nodule or mass on lung window settings (Figure 2). The “cutting sign” was defined as a straight lesion edge resembling a knife cut with a diameter of >5 mm (Figure 2).

Descriptive statistics and statistical analysis

The patients were allocated to the following four groups based on nodule size: Group 1: nodules ≤ 10 mm; Group 2: nodules >10 and ≤ 20 mm; Group 3: nodules >20 and

≤ 30 mm; and Group 4: all nodules. The patient and nodule characteristics are presented as the frequency and percentage for the categorical variables and the mean \pm standard deviation or median for the continuous variables. The independent sample *t*-test was used for the continuous variables conforming to a normal distribution, otherwise, the Mann-Whitney *U* test was used. For the qualitative variables, Pearson's χ^2 test, Spearman's χ^2 test, and Fisher's exact test were employed. Prediction models were obtained through binary logistic regression for the four groups of patients. Receiver operating characteristic (ROC) curves were used to evaluate the two-category capability of the prediction models, and the area under the curve (AUC) was used to assess the classification performance of the models. The statistical significance of the improvement in the AUC was calculated using Delong's test. A *P* value <0.05 was considered statistically significant.

Results

A total of 948 patients (536 males) presenting with malignant and inflammatory solid pulmonary nodules were enrolled in the study. The mean age of the patients with malignant nodules was 64.3 ± 9.8 years, and that of the patients with inflammatory nodules was 56.0 ± 11.9 years. After applying the inclusion and exclusion criteria, 4,253 patients were excluded from the analysis as illustrated in the flow chart presented in *Figure 1*. The remaining 948 patients were categorized into the following two groups: malignant ($n=638$) and inflammatory ($n=310$). The malignant nodules were further categorized as follows: adenocarcinoma ($n=503$), squamous cell carcinoma ($n=46$), mucous adenocarcinoma ($n=35$), adenosquamous carcinoma ($n=28$), and other types of malignant nodules ($n=26$). The inflammatory nodules included granuloma ($n=126$), tuberculosis ($n=76$), fungal infection ($n=58$), and other types of inflammatory nodules ($n=50$).

Demographic characteristics of patients with malignant and inflammatory lung nodules

The demographic characteristics of the patients included in the study are detailed in *Table 1*. A statistically significant difference was observed in the age distribution between the patients with malignant and inflammatory lung nodules. Specifically, in Group 1, the mean age of the patients with malignant nodules was significantly higher than that of those with inflammatory nodules (malignant:

62.0 ± 8.8 years, inflammatory: 55.9 ± 11.1 years) ($P < 0.001$). Similar significant differences in age were also noted in Group 2 (malignant: 64.2 ± 10.1 years, inflammatory: 55.5 ± 12.3 years) and Group 4 (malignant: 64.3 ± 9.8 years, inflammatory: 56.0 ± 11.9 years).

CT qualitative features of patients with malignant and inflammatory lung nodules

The analysis of the qualitative CT features revealed notable differences between the malignant and inflammatory lung nodules across various groups. Notably, lobulation was significantly more pronounced in the malignant nodules than the inflammatory nodules in all groups ($P < 0.001$). In Group 2, the inflammatory nodules were found to be more prevalent in the right lower lobe ($P < 0.05$). Additionally, calcification was more commonly observed in the inflammatory nodules in Groups 2 and 4 ($P < 0.001$). Satellite lesions were also more frequently observed in the inflammatory nodules than the malignant nodules in Groups 2, 3, and 4 ($P < 0.001$). The presence of the halo sign and cutting sign was more common in the inflammatory nodules in Groups 3 and 4 ($P < 0.05$). Conversely, mixed signs were less prevalent in the malignant nodules in Groups 2 and 4 ($P < 0.001$). However, no statistically significant differences were observed in the remaining quantitative CT characteristics between the malignant and inflammatory lung nodules (*Table 2*).

CT quantitative features of patients with malignant and inflammatory lung nodules

Significant differences were observed in the quantitative CT features of the patients with malignant and inflammatory lung nodules, particularly in Groups 2 and 4. In these groups, the inflammatory nodules had shorter SDs than the malignant nodules ($P < 0.001$). Further, in Group 3, the minimum CT value of the inflammatory nodules was measured at -101.3 HU with a standard deviation of ± 104.6 HU, while that of the malignant nodules was -65.6 HU with a standard deviation of ± 76.9 HU, and this difference was statistically significant ($P < 0.001$) (*Table 3*).

Feature selection and model construction

To construct each model, different independent risk factors were screened from 29 features using binary logistic regression. Ultimately, four models were constructed,

Table 1 Demographic characteristics of patients with malignant and inflammatory lung nodules

Variable	Group 1				Group 2				Group 3				Group 4			
	Mal (n=42)	Inf (n=109)	P value		Mal (n=297)	Inf (n=133)	P value		Mal (n=299)	Inf (n=68)	P value		Mal (n=638)	Inf (n=310)	P value	
Gender			0.231				0.024	0.136			0.473				0.101	
Male	28 (66.7)	61 (56.0)			155 (52.2)	85 (63.9)			166 (55.5)	41 (60.3)			349 (54.7)	187 (60.3)		
Female	14 (33.3)	48 (44.0)			142 (47.8)	48 (36.1)			133 (44.5)	27 (39.7)			289 (45.3)	123 (39.7)		
Age (years)	62.0±8.8	55.9±11.1	0.001	0.004	64.2±10.1	55.5±12.3	<0.001	<0.001	64.8±9.6	57.0±12.6	<0.001	0.246	64.3±9.8	56.0±11.9	<0.001	<0.001
Smoke			0.308				0.298				0.285				0.135	
Never	32 (76.2)	94 (86.2)			237 (79.8)	106 (79.7)			230 (76.9)	58 (85.3)			499 (78.2)	258 (83.2)		
Current	7 (16.7)	9 (8.3)			39 (13.1)	22 (16.5)			46 (15.4)	7 (10.3)			92 (14.4)	38 (12.3)		
Former	3 (7.1)	6 (5.5)			21 (7.1)	5 (3.8)			23 (7.7)	3 (4.4)			47 (7.4)	14 (4.5)		
Surgical history			<0.001	0.003			0.639				0.814				0.349	
No	29 (69.0)	103 (94.5)			270 (90.9)	119 (89.5)			271 (90.6)	61 (89.7)			570 (89.3)	283 (91.3)		
Yes	13 (31.0)	6 (5.5)			27 (9.1)	14 (10.5)			28 (9.4)	7 (10.3)			68 (10.7)	27 (8.7)		
Tumor indicator			0.048	0.272			0.075				0.024	0.397			<0.001	0.678
Normal	28 (66.7)	89 (81.7)			215 (72.4)	107 (80.5)			195 (65.2)	54 (79.4)			438 (68.7)	250 (80.6)		
Abnormal	14 (33.3)	20 (18.3)			82 (27.6)	26 (19.5)			104 (34.8)	14 (20.6)			200 (31.3)	60 (19.4)		

Data are presented as mean ± standard deviation, and the statistical values are the independent sample *t*-test results or *n* (%) for the qualitative variables, and the statistical values are the Pearson's χ^2 test, Spearman's χ^2 test and Fisher's exact test results. Group 1: nodules ≤10 mm; Group 2: nodules >10 and ≤20 mm; Group 3: nodules >20 and ≤30 mm; and Group 4: all nodules. Mal, malignant; Inf, inflammatory.

Table 2 CT qualitative features of patients with malignant and inflammatory lung nodules

Variable	Group 1				Group 2				Group 3				Group 4			
	Mal (n=42)	Inf (n=109)	P value		Mal (n=297)	Inf (n=133)	P value		Mal (n=299)	Inf (n=68)	P value		Mal (n=638)	Inf (n=310)	P value	
			Single	Multiple			Single	Multiple			Single	Multiple			Single	Multiple
Emphysema/bullae	9 (21.4)	16 (14.7)	0.317		77 (25.9)	23 (17.3)	0.050		84 (28.1)	4 (5.9)	<0.001	0.004	170 (26.6)	43 (13.9)	<0.001	0.242
HVP	5 (11.9)	19 (17.4)	0.405		43 (14.5)	15 (11.3)	0.369		40 (13.4)	9 (13.2)	0.975		88 (13.8)	43 (13.9)	0.974	
Bronchiectasis or ILD	3 (7.1)	0	0.005	0.999	11 (3.7)	4 (3.0)	0.937		20 (6.7)	2 (2.9)	0.372		34 (5.3)	6 (1.9)	0.015	0.596
Multiple lung comorbidity	1 (2.4)	2 (1.8)	0.830		15 (5.1)	6 (4.5)	0.810		19 (6.4)	0	0.067		35 (5.5)	8 (2.6)	0.044	0.028
Location			0.869				0.014	0.034			0.056				0.076	
Right upper lobe	16 (38.1)	32 (29.4)			75 (25.3)	39 (29.3)			78 (26.1)	18 (26.5)			169 (26.5)	89 (28.7)		
Right middle lobe	5 (11.9)	17 (15.6)			23 (7.7)	3 (2.3)			23 (7.7)	9 (13.2)			51 (8.0)	29 (9.4)		
Right lower lobe	7 (16.7)	18 (16.5)			58 (19.5)	41 (30.8)			65 (21.7)	9 (13.2)			130 (20.4)	68 (21.9)		
Left upper lobe	6 (14.3)	17 (15.6)			80 (26.9)	26 (19.5)			83 (27.8)	13 (19.1)			169 (26.5)	56 (18.1)		
Left lower lobe	8 (19.0)	25 (22.9)			61 (20.5)	24 (18.0)			50 (16.7)	19 (27.9)			119 (18.7)	68 (21.9)		
Lobulation	19 (45.2)	11 (10.1)	<0.001	<0.001	233 (78.5)	48 (36.1)	<0.001	<0.001	259 (86.6)	37 (54.4)	<0.001	<0.001	511 (80.1)	96 (31.0)	<0.001	<0.001
Spiculation	12 (28.6)	22 (20.2)	0.269		124 (41.8)	22 (16.5)	<0.001	0.361	208 (69.6)	28 (41.2)	<0.001	0.048	397 (62.2)	106 (34.2)	<0.001	0.340
Airspace	6 (14.3)	5 (4.6)	0.088		50 (16.8)	12 (9.0)	0.033	0.172	61 (20.4)	7 (10.3)	0.053		117 (18.3)	24 (7.7)	<0.001	0.021
Air bronchogram	4 (9.5)	3 (2.8)	0.180		51 (17.2)	15 (11.3)	0.117		65 (21.7)	20 (29.4)	0.176		120 (18.8)	38 (12.3)	0.011	0.197
Pleural tag	22 (52.4)	68 (62.4)	0.262		228 (76.8)	106 (79.7)	0.500		271 (90.6)	60 (88.2)	0.548		521 (81.7)	234 (75.5)	0.027	0.292
Calcification	1 (2.4)	10 (9.2)	0.276		6 (2.0)	16 (12.0)	<0.001	<0.001	15 (5.0)	8 (11.8)	0.073		22 (3.4)	34 (11.0)	<0.001	<0.001
Pleural effusion	1 (2.4)	0	0.108		3 (1.0)	0	0.135		9 (3.0)	0	0.310		13 (2.0)	0	0.026	0.998
Rimmed sign	15 (35.7)	18 (16.5)	0.011	0.140	97 (32.7)	31 (23.3)	0.050		68 (22.7)	14 (20.6)	0.700		180 (28.2)	63 (20.3)	0.009	0.020
Satellite nodules	0	5 (4.6)	0.366		4 (1.3)	27 (20.3)	<0.001	<0.001	5 (1.7)	26 (38.2)	<0.001	<0.001	9 (1.4)	58 (18.7)	<0.001	<0.001
Halo sign	1 (2.4)	9 (8.3)	0.349		0	9 (6.8)	<0.001	0.998	4 (1.3)	10 (14.7)	<0.001	<0.001	5 (0.8)	28 (9.0)	<0.001	<0.001
Cutting sign	0	3 (2.8)	0.279		3 (1.0)	3 (2.3)	0.567		1 (0.3)	3 (4.4)	0.013	0.018	4 (0.6)	9 (2.9)	0.011	0.028
Mixed signs	0	3 (2.8)	0.279		1 (0.3)	14 (10.5)	<0.001	0.009	2 (0.7)	11 (16.2)	<0.001	0.619	3 (0.5)	28 (9.0)	<0.001	<0.001
Multiple lesions	0	16 (14.7)	0.020	0.998	7 (2.4)	28 (21.1)	<0.001	<0.001	3 (1.0)	19 (27.9)	<0.001	<0.001	10 (1.6)	63 (20.3)	<0.001	<0.001

Data are presented as the number of lesions. Data in parentheses are the percentage. Group 1: nodules ≤10 mm; Group 2: nodules >10 and ≤20 mm; Group 3: nodules >20 and ≤30 mm; and Group 4: all nodules. CT, computed tomography; Mal, malignant; Inf, inflammatory; HVP, heterogeneous ventilation or perfusion; ILD, interstitial lung disease.

Table 3 CT quantitative features of patients with malignant and inflammatory lung nodules

Variable	Group 1				Group 2				Group 3				Group 4			
	Mal (n=42)		Inf (n=109)		Mal (n=297)		Inf (n=133)		Mal (n=299)		Inf (n=68)		Mal (n=638)		Inf (n=310)	
	Mean	SD	Mean	SD	Mean	SD	Mean	SD	Mean	SD	Mean	SD	Mean	SD	Mean	SD
LD (mm)	8.8±1.5	7.7±1.7	<0.001	0.807	15.8±2.9	14.9±2.9	0.002	0.098	25.3±2.9	25.0±2.7	0.439	0.439	19.8±6.1	14.6±6.8	<0.001	0.604
SD (mm)	7.2±1.8	6.1±1.8	0.001	0.087	12.5±3.0	11.2±2.8	<0.001	<0.001	19.4±3.6	18.6±4.5	0.114	0.114	15.4±5.2	11.1±5.5	<0.001	<0.001
CT _{max} value (HU)	219.2±93.0	167.8±99.6	0.004	0.118	195.0±86.1	167.0±84.9	0.002	0.202	181.0±87.0	190.8±98.2	0.412	0.412	190.0±87.5	172.5±94.5	0.006	0.175
CT _{min} value (HU)	-9.8±89.8	-19.0±72.0	0.513		-61.0±82.6	-48.0±66.7	0.111		-65.6±76.9	-101.3±104.6	0.009	<0.001	-59.8±81.5	-49.5±83.6	0.071	
CT _{mean} value (HU)	94.3±64.9	71.5±47.3	0.042	0.904	64.6±44.9	57.4±39.5	0.110		55.2±31.0	45.6±24.2	0.006	0.673	62.1±41.8	59.8±40.9	0.408	
CT _{sd} value (HU)	69.0±34.5	61.5±39.8	0.289		67.6±34.3	58.5±34.0	0.011	0.885	58.5±33.5	67.9±40.8	0.079		63.4±34.2	61.6±37.7	0.466	

Data are presented as mean ± standard deviation, and the statistical values are the independent sample t-test results. Group 1: nodules ≤10 mm; Group 2: nodules >10 and ≤20 mm; Group 3: nodules >20 and ≤30 mm; and Group 4: all nodules. CT, computed tomography; CT_{max}, CT density maximum; CT_{min}, CT density minimum; CT_{mean}, CT density mean; CT_{sd}, CT density standard deviation; inf, inflammatory; LD, long diameter; mal, malignant; SD, short diameter.

comprising variations of two clinical features (age and surgical history) and 15 imaging features (lobulation, multiple lesions, satellite lesions, the halo sign, calcification, mixed signs, the cutting sign, airspace, the rimmed sign, MLC, SD, location, spiculation, minimum CT value, and the standard deviations of the CT values), all of which had AUC values >0.86.

Models 1–4 were based on Groups 1–4. Model 1 incorporated only three features, including two clinical features (age and surgical history) and one imaging feature (lobulation). Model 2, which was used to detect malignant nodules in lung nodules measuring 1–2 cm, included 8 features (lobulation, age, multiple lesions, satellite lesions, calcification, mixed signs, SD, and location), and had an AUC value of 0.902 [95% confidence interval (CI): 0.873–0.931], a sensitivity of 0.747, a specificity of 0.880, and an accuracy of 0.828. Model 3, which was used to detect malignant nodules measuring 2–3 cm, included 8 features (lobulation, multiple lesions, satellite lesions, the halo sign, the cutting sign, airspace, spiculation, and the minimum CT value), and had an AUC value of 0.943 (95% CI: 0.914–0.972), a sensitivity of 0.873, a specificity of 0.897, and an accuracy of 0.905. Model 4, which was used to predict malignancy, included one clinical feature (age) and 11 imaging features (lobulation, multiple lesions, satellite lesions, the halo sign, calcification, mixed signs, the cutting sign, airspace, the rimmed sign, MLC, and the standard deviations of the CT values), and had an AUC of 0.921 (95% CI: 0.903–0.940), a sensitivity of 0.831, a specificity of 0.868, and an accuracy of 0.847 (Table 4 and Figure 3). A confusion matrix was used to show the diagnostic efficiency of the different models, and the accuracy, sensitivity, specificity, positive predictive value, and negative predictive value of the models were calculated (Figure 4). The weight ratio of each feature in predicting inflammatory and malignant nodules in the models was calculated (Figure 4). Notably, the model features of lobulation, age, multiple lesions, and satellite lesions had greater weighting in the models (Figure 5).

Discussion

This study found that all four models had high efficacy in differentiating between inflammatory and malignant lung nodules (all models had AUC values >0.86). Specifically, Model 3, which included eight features for differentiation and which assigned greater weight to the four features of lobulation, age, the presence of multiple lesions,

Table 4 Comparison of diagnostic efficacy between the three-layered models and Model 4

Model type	AUC (95% CI)	Standard error	Accuracy (%)	Sensitivity (%)	Specificity (%)	Z value	P value
Model 1	0.861 (0.803–0.921)	0.030	73.5	81.0	78.9	−1.916	0.055
Model 2	0.902 (0.873–0.931)	0.015	82.8	74.7	88.0	−1.086	0.277
Model 3	0.943 (0.914–0.972)	0.015	90.5	87.3	89.7	1.258	0.209
Model 4	0.921 (0.903–0.940)	0.009	84.7	83.1	86.8	NA	NA

Model 1: two clinical features (age and surgical history) and one imaging feature (lobulation). Model 2: 8 features (lobulation, age, multiple lesions, satellite lesions, calcification, mixed signs, short diameter, and location); Model 3: 8 features (lobulation, multiple lesions, satellite lesions, the halo sign, the cutting sign, airspace, spiculation, and the minimum CT value); Model 4: one clinical feature (age) and 11 imaging features (lobulation, multiple lesions, satellite lesions, the halo sign, calcification, mixed signs, the cutting sign, airspace, the rimmed sign, MLC, and the standard deviations of the CT values). AUC, area under the curve; CI, confidence interval; CT, computed tomography; MLC, multiple lung comorbidity; NA, not applicable.

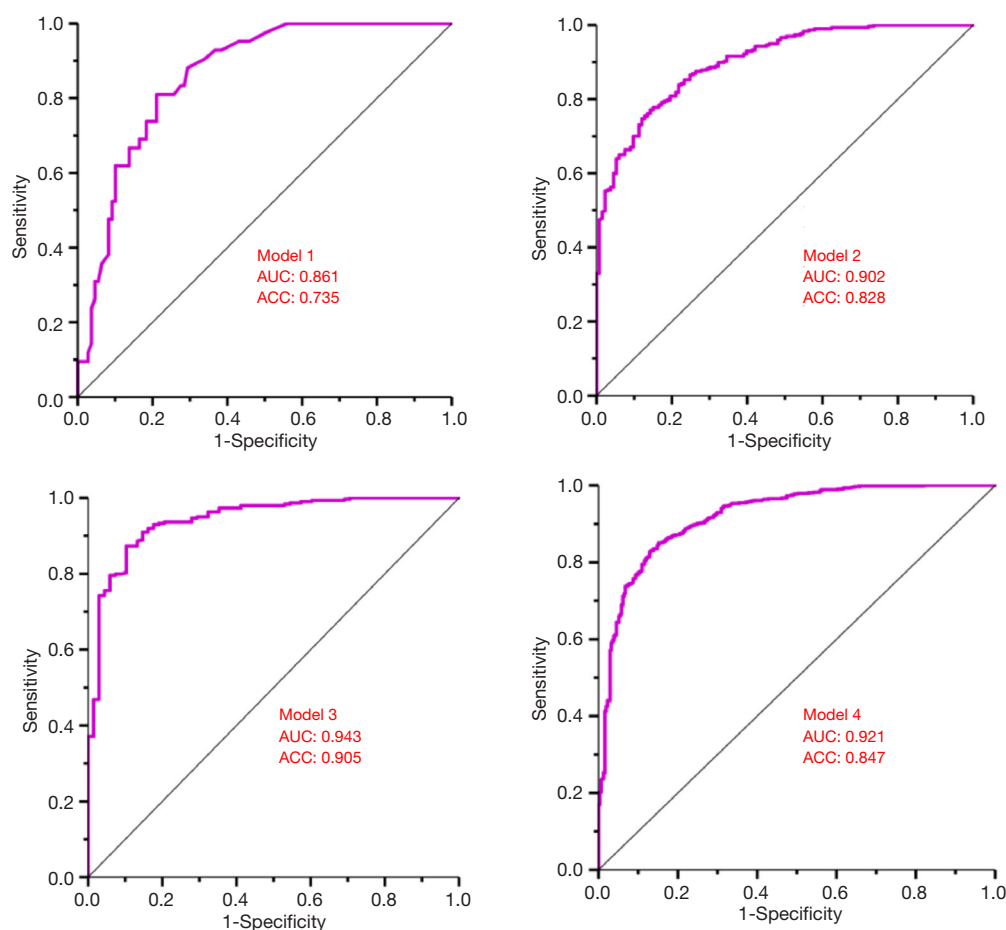


Figure 3 Receiver operating characteristic curves of Models 1, 2, 3, and 4. Model 1: two clinical features (age and surgical history) and one imaging feature (lobulation). Model 2: 8 features (lobulation, age, multiple lesions, satellite lesions, calcification, mixed signs, short diameter, and location); Model 3: 8 features (lobulation, multiple lesions, satellite lesions, the halo sign, the cutting sign, airspace, spiculation, and the minimum CT value); Model 4: one clinical feature (age) and 11 imaging features (lobulation, multiple lesions, satellite lesions, the halo sign, calcification, mixed signs, the cutting sign, airspace, the rimmed sign, MLC, and the standard deviations of the CT values). ACC, accuracy; AUC, area under the curve; CT, computed tomography; MLC, multiple lung comorbidity.

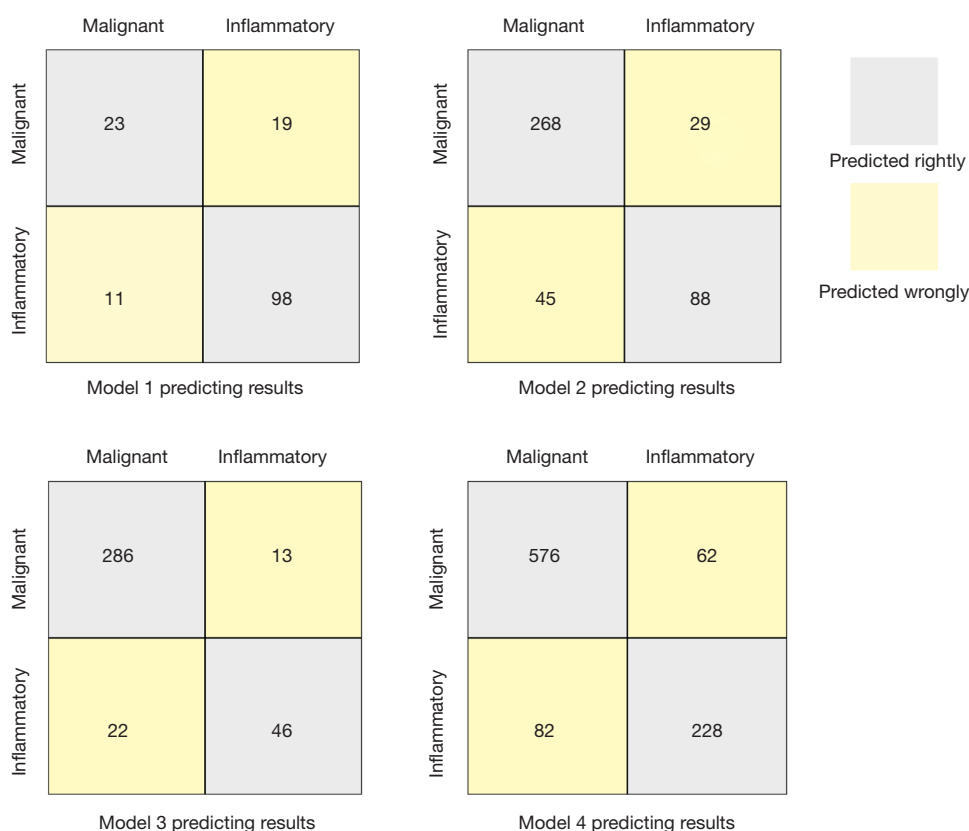


Figure 4 Confusion matrix results for Models 1, 2, 3, and 4. Model 1: two clinical features (age and surgical history) and one imaging feature (lobulation). Model 2: 8 features (lobulation, age, multiple lesions, satellite lesions, calcification, mixed signs, short diameter, and location); Model 3: 8 features (lobulation, multiple lesions, satellite lesions, the halo sign, the cutting sign, airspace, spiculation, and the minimum CT value); Model 4: one clinical feature (age) and 11 imaging features (lobulation, multiple lesions, satellite lesions, the halo sign, calcification, mixed signs, the cutting sign, airspace, the rimmed sign, MLC, and the standard deviations of the CT values). CT, computed tomography; MLC, multiple lung comorbidity.

and the presence of satellite lesions, exhibited superior discriminative ability, particularly in nodules ranging from 2 to 3 cm. This model enables rapid and efficient differential diagnosis using fewer imaging features, thereby enhancing diagnostic efficiency. Thus, in this study, we established a novel clinical imaging model characterized by simplicity and clarity that can provide diagnosticians with a reliable basis for diagnosis.

We identified 17 features for the differential diagnosis of lung nodules. These features align with the factors such as age, spiculation, and calcification reported in previous studies by Yi *et al.*, Wu *et al.* and Tan *et al.* (9,23,24). Further, we found no correlation between smoking status, gender, and age in the diagnosis of inflammatory and malignant lung nodules (25). Smoking history was not included as a characteristic in our models due to the low

percentage of squamous carcinomas in the patient cohort (46/638) and the weaker association between smoking history and adenocarcinomas and other malignant tumors relative to squamous carcinomas. Using features such as spiculation and airspace, our models were able to effectively differentiate between solid lung adenocarcinomas and tuberculous granulomatous nodules. Additionally, consistent with previous findings (24), we found that satellite nodules were a characteristic manifestation of inflammatory granulomas. Moreover, our study reaffirmed the importance of nodule size and nodule growth rate as crucial predictors of malignancy (6). Smaller diameters are more effective at distinguishing between inflammatory and malignant nodules, diameter of pulmonary nodule might be caused by differing growth patterns.

Model 1 only included three features (age, surgical

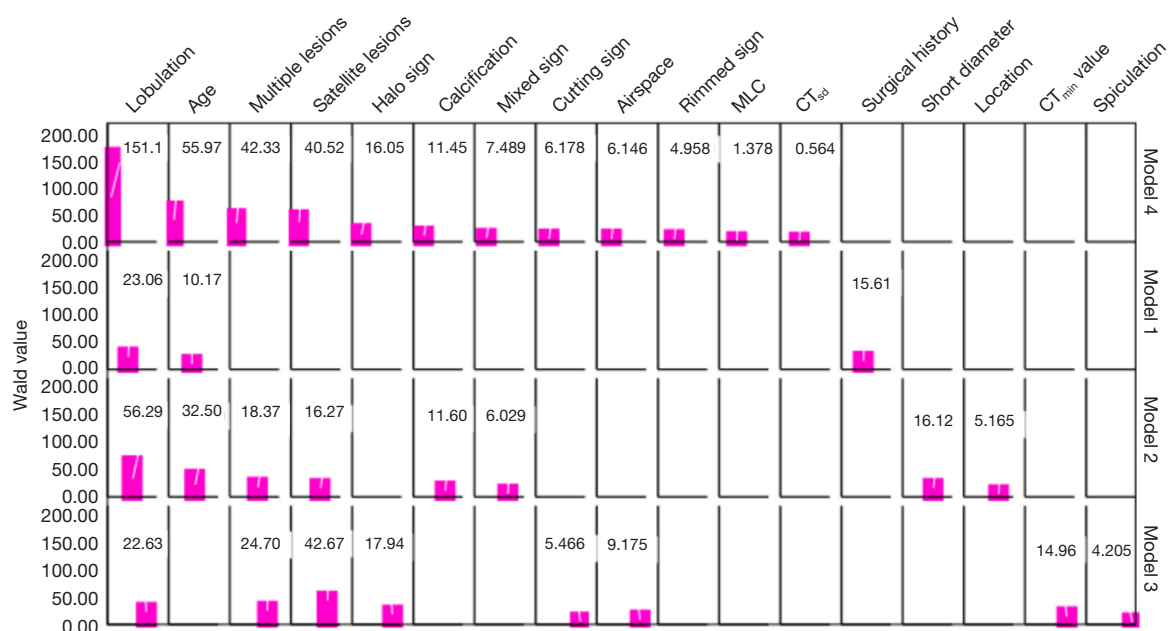


Figure 5 The weight table of the selected features for different model constructions. Model 1: two clinical features (age and surgical history) and one imaging feature (lobulation). Model 2: 8 features (lobulation, age, multiple lesions, satellite lesions, calcification, mixed signs, short diameter, and location); Model 3: 8 features (lobulation, multiple lesions, satellite lesions, the halo sign, the cutting sign, airspace, spiculation, and the minimum CT value); Model 4: one clinical feature (age) and 11 imaging features (lobulation, multiple lesions, satellite lesions, the halo sign, calcification, mixed signs, the cutting sign, airspace, the rimmed sign, MLC, and the standard deviations of the CT values). CT, computed tomography; MLC, multiple lung comorbidity; CT_{min} , CT density minimum; CT_{sd} , CT density standard deviation.

history, and lobulation). For nodules <1 cm, lobulation served as the primary identifier between inflammatory and malignant nodules, which is consistent with Chen *et al.*'s findings for patients with solitary sub-centimeter solid nodules (26). As lesions decrease in size, distinguishing between two lesions becomes more challenging due to limited information availability. We found that lobulation and satellite lesions served as common differentiation in Models 2 and 3. In nodules of 1–2 cm, malignant nodules progress faster than inflammatory nodules, resulting in more pronounced lobulation signs and an increased occurrence of satellite lesions in inflammatory nodules. These two imaging features had significant value in differentiating between malignant and inflammatory nodules. Model 4, which included 12 features, was developed to predict malignant nodules in lung nodules measuring <3 cm, and had an AUC value of 0.921. Despite its broader diagnostic scope, Model 4 did not outperform the other models. Lobulation was consistently effective across all models in discriminating between inflammatory and malignant nodules. Unlike inflammatory nodules, malignant nodules grow unevenly

in all directions. All models showed strong performance, achieving AUC values >0.86. Model 3 had the highest AUC value. Model 4 was able to effectively identify progression between the inflammatory and malignant nodules; however, the simplicity of the other models facilitated the rapid identification of inflammatory and malignant lung nodules, enabling the accurate diagnosis of patients with potential malignant lesions.

The Mayo Clinic Model (MCM) holds considerable significance in clinical settings for assessing the lung cancer risk associated with pulmonary nodules. In one training set, the AUC of the Mayo model was 0.8328 (27). The MCM enjoys widespread international recognition and is extensively cited in the literature. Gould *et al.* established a clinical model of 375 confirmed solid pulmonary nodules, which had good accuracy and an AUC of the ROC curve of 0.79 (95% CI: 0.74 to 0.84) (28). We constructed Model 4 to predict malignant nodules, and it had an AUC of 0.921, and thus surpassed the performance of the aforementioned models. By incorporating additional valuable imaging features, we enhanced the accuracy of nodule

characterization. Our models could provide clinicians and radiologists with essential imaging evidence that could aid in diagnostic decision-making.

AI is advancing rapidly, especially in the realm of lung nodule detection. However, extensive external validation is necessary to ensure models can accurately distinguish between benign and malignant nodules (29). Many AI systems are not yet available commercially for clinical use (2); thus, diagnosticians remain pivotal in nodule characterization. Some studies have indicated that validated risk calculator scores (ranging from 0.70 to 0.80) are effective at identifying malignant lung nodules (30–32). In our study, the AUC of all models exceeded 0.86, demonstrating strong model performance. Our models exhibited superior discriminatory power in this regard.

Our study had a number of advantages. First, all the patients included in the study underwent either surgical resection or percutaneous biopsy and had a clear pathological diagnosis. Second, we developed four new models using patients from multiple centers, an approach rarely employed in other similar studies. Third, data grouping modeling meets the needs of precision medical and could better guide clinical diagnosis and differentiation. Our models could reduce the misdiagnosis of malignant nodules, as relevant clinical and imaging data are easily available. We presented the risk coefficients of the independent risk factors in different models in the form of scale plots (*Figure 4*). The main limitations of this study include insufficient data and a lack of a proper external validation cohort. Despite the standardization of features, our images were obtained from different hospitals using different equipment; therefore, there are still certain differences in the qualitative and quantitative CT features. These limitations indicate areas for future research. In this study, nodule size was classified and modeled; in a subsequent study, nodule growth will be analyzed. We also intend to employ CT imaging deep-learning technology to determine the nature of pulmonary nodules. By effectively combining these aspects, we aim to conduct valuable research into the qualitative diagnosis of lung nodules.

Conclusions

The lung nodule grouping models based on clinical data and chest CT features were better able to directly determine whether the solid pulmonary nodules were inflammatory or malignant. Such grouping models could enable convenient and rapid diagnosis. In the future, we intend to explore the

whole process related to the scientific management of lung nodules to achieve individualized precision medicine for lung nodules.

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None.

Footnote

Reporting Checklist: The authors have completed the TRIPOD reporting checklist. Available at <https://qims.amegroups.com/article/view/10.21037/qims-24-2338/rc>

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Conflicts of Interest: All authors have completed the ICMJE uniform disclosure form (available at <https://qims.amegroups.com/article/view/10.21037/qims-24-2338/coif>). The authors have no conflicts of interest to declare.

Ethical Statement: The authors are accountable for all aspects of the work in ensuring that questions related to the accuracy or integrity of any part of the work are appropriately investigated and resolved. This retrospective study was conducted in accordance with the Declaration of Helsinki (as revised in 2013) and was approved by the respective Ethics Committees of Tongde Hospital of Zhejiang Province (No. 2022-029-JY), Anqing Municipal Hospital (No. 83230471), Taizhou Municipal Hospital (No. LWYJ2023059), and Shaoxing People's Hospital (No. 2019-K-Y-257-01). The requirement of individual informed consent for this retrospective analysis was waived.

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