

# A Continuous and Noninvasive Method to Estimate $P_{aO_2}/F_{iO_2}$ Ratio

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**OBJECTIVES:** To validate a method for continuously estimating the  $P_{aO_2}/F_{iO_2}$  (PF) ratio in all critically ill pediatric patients using only standard continuous data monitoring.

**DESIGN:** Retrospective study on a high temporal resolution database.

**SETTING:** PICU in Montreal, QC, Canada.

**PATIENTS/SUBJECTS:** We included any patients admitted from May 2015 to May 2023 who had an arterial blood gas (ABG) with concurrent continuous pulsed oximetry saturation ( $SpO_2$ ) values. We used our previously validated mathematical model to determine the magnitude of hypoxemia by computing the estimated  $eP_{aO_2}/F_{iO_2}$  (ePF) ratio and comparing it to the  $SpO_2/F_{iO_2}$  (SF), using PF ratio as the reference standard.

**INTERVENTIONS:** None.

**MEASUREMENTS AND MAIN RESULTS:** We analyzed a total of 20,828 ABGs. When  $SpO_2$  was below or equal to 97%, the ePF ratio showed a significantly better hypoxemia classification (none, light/moderate, or severe) than the SF ratio (0.80 vs. 0.72;  $p < 0.001$ ), a lower fixed bias (16.26 vs. -35.24;  $p < 0.001$ ), a lower mean absolute error (37.92 vs. 63.93;  $p < 0.001$ ) and a lower proportional bias (slope of 1.01 vs. 0.81;  $p < 0.001$ ). ePF ratio has also a better limits of agreement difference from Bland-Altman plot (248.10 vs. 292.45;  $p < 0.001$ ) and coefficient of determination (0.68 vs. 0.59;  $p < 0.001$ ). When  $SpO_2$  was above 97%, the ePF ratio had better classification with Kappa (0.53 vs. 0.43;  $p < 0.001$ ) and lower fixed bias (-0.63 vs. 65.68;  $p < 0.001$ ).

**CONCLUSIONS:** The PF ratio based on ePF allows for a continuous estimation of hypoxemia severity with a better performance than the SF ratio.

**KEYWORDS:** automatic data processing; clinical decision support systems; critical care; hypoxemia

Acute hypoxemic respiratory failure accounts for more than half of the PICU admissions and has high morbidity and mortality (1). Clinicians often fail to preemptively identify hypoxemia, particularly in the setting of acute respiratory distress syndrome (ARDS), with recognition rates ranging from 50% for mild to 80% for severe hypoxemia (2). Although  $P_{aO_2}$  is considered the reference, the Pediatric Acute Respiratory Distress Syndrome Incidence and Epidemiology study revealed that only 44% of patients underwent an arterial blood gas (ABG) analysis at the time of pediatric ARDS (pARDS) diagnosis (3). ABGs are invasive and only allow for occasional assessments. This precludes its use for continuous evaluation, early detection of hypoxemia and the development of precise detection models.

Continuous pulsed oximetry saturation ( $SpO_2$ ) is commonly monitored in PICUs using pulse oximeters, but the asymptotic relationship amid  $P_{aO_2}$  and  $SpO_2$  is limiting its use to estimate the  $P_{aO_2}$ , especially when the saturation is

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## KEY POINTS

**Question:** Can our previously validated mathematical equation, which compute an estimated  $\text{PaO}_2$  using only readily available continuous data in the PICU, be used to monitor an estimated  $\text{PaO}_2/\text{FiO}_2$  (PF) ratio?

**Findings:** When continuous pulsed oximetry saturation ( $\text{SpO}_2$ ) was below or equal to 97%, the estimated  $\text{ePaO}_2/\text{FiO}_2$  ratio showed a significantly better hypoxemia classification (Kappa) than the  $\text{SpO}_2/\text{FiO}_2$  ratio, a lower fixed bias, a lower mean absolute error, and a lower proportional bias.

**Meanings:** Our equation can be used to continuously estimate PF ratio, monitor patient hypoxemia level, aid in the early diagnosis of pediatric acute respiratory distress syndrome and be integrated into clinical decision systems.

high (> 97%) (4, 5). The 2023 Pediatric Acute Lung Injury Consensus Conference (PALICC) states that the  $\text{SpO}_2/\text{FiO}_2$  (SF) ratio cannot be used to precisely monitor hypoxemia when  $\text{SpO}_2$  is above 97%, which is the case for the majority of PICU patients (6, 7). Our team previously developed and validated a mathematical model using only noninvasive data readily available ( $\text{SpO}_2$  pulse rate, and electrical heart rate) to estimate the  $\text{PaO}_2$  in real-time and the oxygenation index ( $\text{OI} = [100 \text{ FiO}_2 \times \text{mean airway pressure}]/\text{PaO}_2$ ) (8). We aim to validate this method to continuously determine the magnitude of hypoxemia by computing the estimated  $\text{PaO}_2/\text{FiO}_2$  (ePF) ratio and measuring its accuracy, precision, and bias in comparison to the SF ratio, using the  $\text{PaO}_2/\text{FiO}_2$  (PF) ratio as the reference.

## MATERIALS AND METHODS

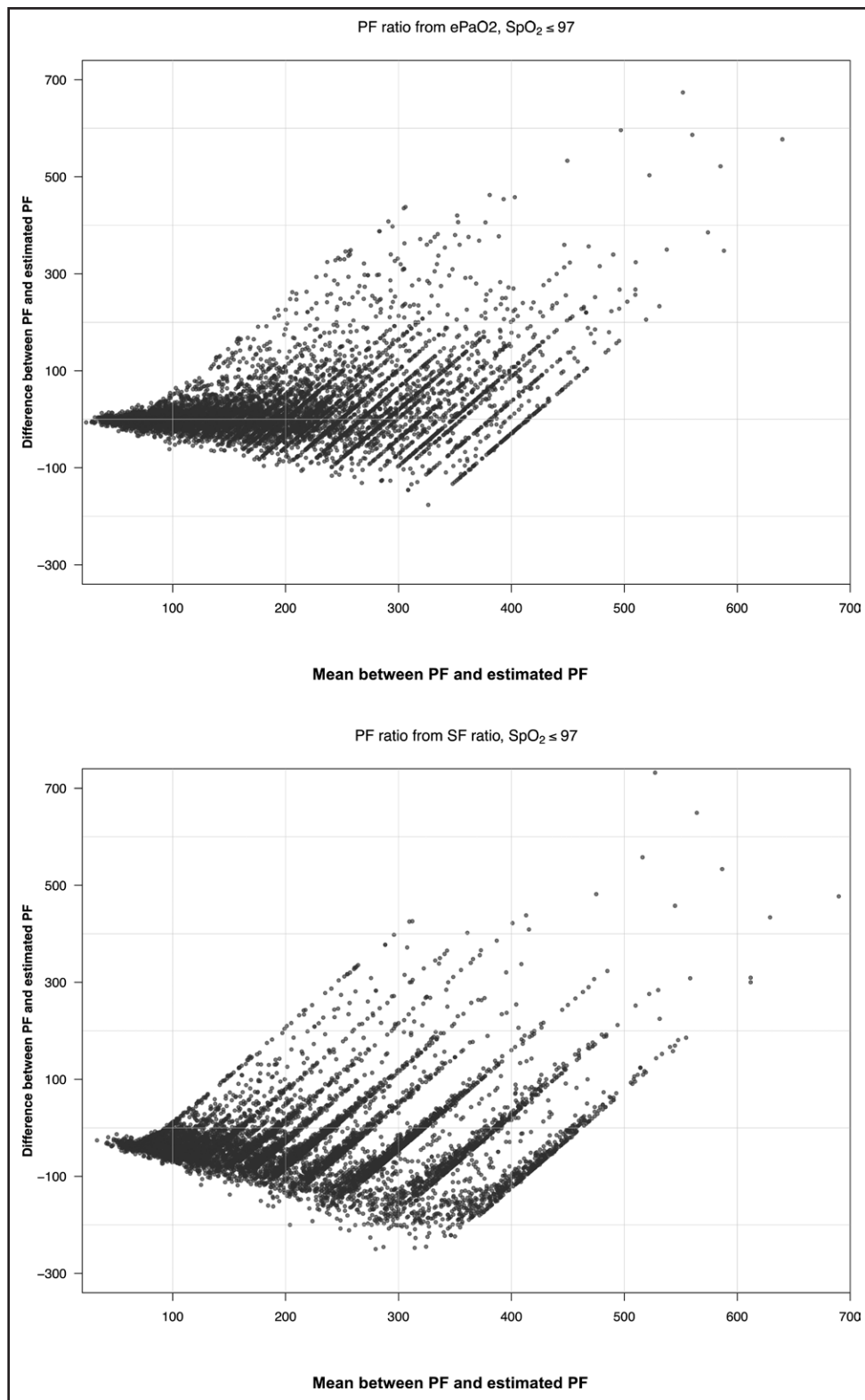
The initial equation was developed on the Boston Children's Hospital (Boston, MA) data and validated on a separate external cohort (Sainte-Justine Hospital [SJH], Montreal, QC, Canada) from 2017 to 2020. In this project, we used an updated version of SJH's database with new data and included any patient admitted in the PICU who had an ABG with coexisting continuous  $\text{SpO}_2$  values from May 2015 to May 2023, including patients with cyanotic cardiopathies. ABG

with missing  $\text{PaO}_2$  values or patients with missing  $\text{SpO}_2$  values in the minute before the gas were excluded. This study was approved by SJH institutional review board and waived the need for informed consent (Name of project: "Empirical determination of lung recruitment potential using the continuous oxygenation index in mechanically ventilated patients in pediatric intensive care," Number of project: 2024-4984, Approval date: June 10, 2023). Procedures were followed in accordance with the ethical standards of the responsible committee on human experimentation and with the Helsinki Declaration of 1975.

Data were retrieved from the hospital's secure server at a 5-second rate from custom-built software. ABGs were tested using Radiometer ABL90 FLEX (Radiometer Medical ApS, Copenhagen, Denmark) and  $\text{SpO}_2$  was assessed using Masimo (Masimo, Irvine, CA) probes (RD SET Neo and RD SET Inf). Location of the probe on the patient was not available in the dataset. Data were archived and managed on a secured local PostgreSQL 12.15 server (The PostgreSQL Global Development Group, Sweden, Germany) and was analyzed with R 4.3.1 (R Core Team, Vienna, Austria). In accordance with our previously validated method, we excluded  $\text{SpO}_2$  values associated with a pulse oximeter rate differing by 3% or more from the electrical heart rate, as this discrepancy was linked to higher bias (8). We opted for the mean function for data aggregation and a 1-minute time window preceding the ABG, as these methods had demonstrated optimal  $\text{SpO}_2$  aggregation in our prior study (8).

Categorical data were described as count and percentage, and continuous data as median and interquartile range (IQR). CIs and *p* values were calculated using 10,000 boot-strap repetitions. We used the type 3 intraclass correlation coefficient (ICC) and the Cohen Kappa as global metrics for agreement for the categorical variable of hypoxemia severity. The accuracy was estimated with the mean of the differences (fixed bias) and precision was estimated with the mean absolute error (MAE), the limits of agreements on the Bland-Altman plot and the slope on the regression model plot. Using PALICC 2023 thresholds, hypoxemia severity using PF ratio was defined as: no hypoxemia (PF > 300), mild-moderate (PF 100–300), and severe (PF < 100). When using SF ratio, no hypoxemia (SF > 250), mild-moderate (SF 150–250), and severe (SF < 150) (6). We completed subgroup analyses with  $\text{SpO}_2$  values equal to or below 97% and above 97%.





**Figure 1.** Bland-Altman plots comparing two methods estimating the  $P_{aO_2}/F_{iO_2}$  (PF) ratio. The first part is the continuous pulsed oximetry saturation ( $SpO_2$ )/ $F_{iO_2}$  (SF) ratio converted to PF using original published equations and the second is using the estimated  $P_{aO_2}$  ( $eP_{aO_2}$ ). A perfect model would have a cluster of data point on the x-axis line showing no difference with the reference.

(88–97%) (6, 9). This mathematical model could be used to develop a clinical tool to continuously monitor hypoxemia in pediatric patients on noninvasive ventilation and help identify patients at risk for respiratory deterioration. Clinical decision support systems using  $SpO_2$  should automatically filter out values when a difference between electronic heart rate and oximeter heart rate is more than 3% to account for artifacts and patient’s movements.

For  $SpO_2$  above 97%, our mathematical model showed a significantly better hypoxemia severity classification compared with the SF ratio and a lower fixed bias. Despite this improvement, absolute result is still low indicating that caution is needed when the  $SpO_2$  exceeds 97%. For the MAE, ICC and coefficient of determination both methods obtained comparable results.

Our study has strengths. We present a model that can continuously estimate a PF ratio using only noninvasive data that will allow early hypoxemia detection. We included a large number of ABGs from a wide variety of patients’ ages, suggesting a good applicability for all patients in the PICU. On the Bland-Altman plot, we can observe that our model seems to be even more accurate for severe hypoxemia, as the cluster of data points are near the axis for PF ratio of less than 100. Further studies

using adult data need to be done to validate this mathematical model in this population.

The retrospective nature of the study is our principal limitation, limiting our ability to validate the arterial labeling on the ABGs and the location of the probe. This is mitigated by the fact that our database is used by caregivers and that we filtered the data to exclude erroneous measurements. Acquisition of an ABG is a clinical decision mostly based on clinical severity and induces a selection bias. No data were available on skin pigmentation. Since it can influence  $\text{SpO}_2$  accuracy for individuals with darker skin tones, ePF assessment can also be biased in this population (10). More studies in pediatric population are needed. Our model needs validation specifically on a pARDS cohort as this model was tested on a nonspecific PICU population, which may not fully capture the nuances of pARDS cases.

## CONCLUSIONS

In this single-center retrospective study including more than 20,000 ABGs paired with continuous monitoring data, we validated a mathematical model to automatically estimate the PF ratio using only noninvasive data. These results are important for future real time decision support systems.

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