Check for updates

OPEN ACCESS

EDITED BY Xiaomin Niu, Shanghai Jiao Tong University, China

REVIEWED BY

Song Xu, Tianjin Medical University General Hospital, China Qiang Yan, Taiyuan University of Technology, China

*CORRESPONDENCE Xue-ning Yang yangxuening@gdph.org.cn Yi-long Wu syylwu@live.cn

[†]These authors have contributed equally to this work

SPECIALTY SECTION This article was submitted to Thoracic Oncology, a section of the journal Frontiers in Oncology

RECEIVED 25 July 2022 ACCEPTED 20 September 2022 PUBLISHED 12 October 2022

CITATION

Liao R-q, Li A-w, Yan H-h, Lin J-t, Liu S-y, Wang J-w, Fang J-s, Liu H-b, Hou Y-h, Song C, Yang H-f, Li B, Jiang B-y, Dong S, Nie Q, Zhong W-z, Wu Y-l and Yang X-n (2022) Deep learning-based growth prediction for sub-solid pulmonary nodules on CT images. *Front. Oncol.* 12:1002953. doi: 10.3389/fonc.2022.1002953

COPYRIGHT

© 2022 Liao, Li, Yan, Lin, Liu, Wang, Fang, Liu, Hou, Song, Yang, Li, Jiang, Dong, Nie, Zhong, Wu and Yang. This is an open-access article distributed under the terms of the Creative Commons Attribution License (CC BY). The use. distribution or reproduction in other forums is permitted, provided the original author(s) and the copyright owner(s) are credited and that the original publication in this journal is cited, in accordance with accepted academic practice. No use, distribution or reproduction is permitted which does not comply with these terms.

Deep learning-based growth prediction for sub-solid pulmonary nodules on CT images

Ri-qiang Liao^{1†}, An-wei Li^{2†}, Hong-hong Yan^{1†}, Jun-tao Lin¹, Si-yang Liu¹, Jing-wen Wang², Jian-sheng Fang², Hong-bo Liu², Yong-he Hou³, Chao Song³, Hui-fang Yang³, Bin Li⁴, Ben-yuan Jiang¹, Song Dong¹, Qiang Nie¹, Wen-zhao Zhong¹, Yi-long Wu^{1*} and Xue-ning Yang^{1*}

¹Guangdong Lung Cancer Institute, Guangdong Provincial People's Hospital, Guangdong Academy of Medical Sciences, Guangzhou, China, ²Guangzhou Shiyuan Electronics Co., Ltd, Guangzhou, China, ³Yibicom Health Management Center, CVTE, Guangzhou, China, ⁴Automation Science and Engineering, South China University of Technology, Guangzhou, China

Background: Estimating the growth of pulmonary sub-solid nodules (SSNs) is crucial to the successful management of them during follow-up periods. The purpose of this study is to (1) investigate the measurement sensitivity of diameter, volume, and mass of SSNs for identifying growth and (2) seek to establish a deep learning-based model to predict the growth of SSNs.

Methods: A total of 2,523 patients underwent at least 2-year examination records retrospectively collected with sub-solid nodules. A total of 2,358 patients with 3,120 SSNs from the NLST dataset were randomly divided into training and validation sets. Patients from the Yibicom Health Management Center and Guangdong Provincial People's Hospital were collected as an external test set (165 patients with 213 SSN). Trained models based on LUNA16 and Lndb19 datasets were employed to automatically obtain the diameter, volume, and mass of SSNs. Then, the increase rate in measurements between cancer and non-cancer groups was studied to evaluate the most appropriate way to identify growth-associated lung cancer. Further, according to the selected measurement, all SSNs were classified into two groups: growth and non-growth. Based on the data, the deep learning-based model (SiamModel) and radiomics model were developed and verified.

Results: The double time of diameter, volume, and mass were 711 vs. 963 days (P = 0.20), 552 vs. 621 days (P = 0.04) and 488 vs. 623 days (P < 0.001) in the cancer and non-cancer groups, respectively. Our proposed SiamModel performed better than the radiomics model in both the NLST validation set and external test set, with an AUC of 0.858 (95% CI 0.786–0.921) and 0.760

(95% CI 0.646–0.857) in the validation set and 0.862 (95% CI 0.789–0.927) and 0.681 (95% CI 0.506–0.841) in the external test set, respectively. Furthermore, our SiamModel could use the data from first-time CT to predict the growth of SSNs, with an AUC of 0.855 (95% CI 0.793–0.908) in the NLST validation set and 0.821 (95% CI 0.725–0.904) in the external test set.

Conclusion: Mass increase rate can reflect more sensitively the growth of SSNs associated with lung cancer than diameter and volume increase rates. A deep learning-based model has a great potential to predict the growth of SSNs.

KEYWORDS

sub solid pulmonary nodules, growth, mass, deep learning, radiomics

Introduction

Lung cancer is the leading cause of cancer death, with an estimated 1.8 million deaths (18.0%) worldwide in 2020 (1). However, low-dose computed tomography (LDCT) is an effective screening tool for reducing lung cancer mortality in high-risk individuals (2). With the popularization of the LDCT for lung cancer screening, the detection rate for pulmonary nodules, particularly sub-solid nodules (SSNs), has been significantly improved (3).

SSNs, which include both ground-glass (GGNs) and part-solid (PSNs) nodules, have a higher likelihood of malignancy than solid nodules regardless of size (4). Although SSNs have a good prognosis when treated early, they are at serious risk of overdiagnosis and overtreatment (5). Further, predicting the growth of SSNs is crucial to the successful management of SSNs during follow-up periods. Compared with diameter and volume, an increase in mass is an early indicator of growth. However, manual measurement of tumor quality requires many human resources and is difficult to carry out in routine clinical practice (6). Artificial intelligence (AI) has provided great improvements in cancer imaging (7). For example, many studies have used radiomics and deep learning to progress their fields (8–12). However, in the field of SSNs, little progress has been made with the use of AI or other automatic methods.

Therefore, the aim of this study is to investigate the most sensitive measurement of diameter, volume, and mass, using automatic methods, for identifying the growth of SSNs, and further, to establish a deep learning-based model to predict the growth of SSNs based on consecutive computed tomography (CT) scans to provide evidence for follow-up and treatment plans.

Materials and methods

Study protocol

We retrospectively analyzed sub-solid nodule cases from the National Lunch Screening Trial (NLST) (2) from August 2002 to December 2009, Yibicom Health Management Center from August 2017 to January 2022, and Guangdong Provincial People's Hospital from July 2011 to September 2021. The inclusion criteria for Yibicom Health Management Center and Guangdong Provincial People's Hospital were as follows: (a) $30 \le aged \le 80$ years old; (b) underwent at least 2year examination records with thin-section (2.5 mm) CT images; (c) at least one sub-solid nodule; and (d) the diameter 5 and 30 mm of the sub-solid nodule on initial CT images. The exclusion criteria were as follows: (a) only received one CT examination; (b) follow-up time was less than 2 years from the first CT examination; and (c) combined with other malignant tumors with history of less than 5 years, except for lung cancer. If the patient had multiple sub-solid nodules, the largest of the two nodules meeting the above conditions was selected for the study.

In total, 2,358 patients with 3,120 SSNs from the NLST dataset were enrolled and were randomly divided into the training set (1,894 patients with 2,493 SSNs) and validation set (464 patients with 627 SSNs), according to the ratio of 8:2 (Figure 1). In addition, 165 patients with 213 SSNs from Yibicom Health Management Center and Guangdong Provincial People's Hospital were collected as an external test set (Figure 2).

CT examinations

Axial images from 7,177 LDCT/CT examinations (6,812 CT examinations of 2,358 patients from NLST, 365 CT examinations of 165 patients from our two hospitals) were included in this study and were reconstructed by standard or lung kernel. If there were more than three available CT examinations, the latest three exams were enrolled. In total, 9,411 sub-solid nodule volumes from the axial images were extracted to assess the growth (Figures 1, 2).

Image analysis

In order to analyze the changes in diameter, volume, and mass of SSNs over consecutive years, we followed the method in Fang et al., to pair the same nodules between different CT scans (13). Our data organization approach aimed to ascertain the diameter, volume, and mass change of SSNs in consecutive CT scans (Figure 3). A semiautomatic pipeline was developed to process the consecutive CT scans. First, we detected and identified the SSNs on original CT scans. We then performed 3D image registration for the second (T_t) and third (T_{t+1}) CT scans in terms of the first scan (T_{t-1}) and paired 3D volumes of interest (VOIs) containing SSNs to match the same sub-solid nodule at different time points. Next, we employed a segmenter to automatically crop out the lesion of nodules in VOIs to calculate their diameter, volume, and mass. After automatically annotating, we performed a manual review to acquire reliable labels.

Specifically, two popular CT datasets, Lung Nodule Analysis (LUNA)16 (14) and Lung Nodule Database (LNDb) (15), were used to train our models (detector and segmenter), in which the detector for VOI identification was a 3D variant of CenterNet (16) and the segmenter for lesion segmentation was a multi-scale 3D UNet (17). The results of the detector on LUNA16 were FROC = 0.966, recall = 0.978, and precision = 0.654. The segmenter has a dice of 0.838 on LUNA16.

Growth measurement

There were three measurements for evaluating the growth of nodule, after semiautomatic acquisition of the nodule mask (1): the diameter, which was the longest side of the smallest circumscribed rectangle on the maximal surface of the nodule mask; (2) the volume (V in mm³), which was computed by multiplying the voxel number and the volume of a single voxel; and (3) the mass, which was computed as follows: $M = V \times (A + 1,000)/1,000$ (18), where A is the average CT attenuation value (HU) and V is the volume of the nodule.

The SSNs from NLST were divided into cancer group and non-cancer group according to follow-up confirmation results. For each SSN, we calculated the increase rates of the diameter, volume, and mass during follow-up, respectively,





then compared the three relative rates between the cancer group and non-cancer group to evaluate the most appropriate way for identifying the growth.

Growth prediction model

According to the selected measurement, all SSNs were classified into two groups: growth group and non-growth group. The deep learning-based model and radiomics model were developed using the training set and were verified in the validation and test sets, respectively.

The radiomics model was the logistic regression model based on radiomics features, which was extracted from the shape and appearance of SSN in 3D VOIs and selected by the Least Absolute Shrinkage and Selection Operator (LASSO) (19). In total, 1,218 features were extracted and 60 features were selected for modeling the logistic regression model.

Following selection (13), the deep learning-based model was identified (called SiamModel, Figure 4), where FGt, FLt, and FLt-1 represent global feature embedding of Tt VOI, local feature embedding of Tt VOI, and local feature embedding of Tt-1 VOI, respectively. A learnable embedding FL_{t-1} was provided if T_{t-1} VOI was unavailable, which occurred when there were only two CT scans. For a given subject, the 3D VOI pairs $(T_{t-1} \text{ and } T_t)$ taken from CT scans at sequential time points were fed into the Siamese encoder for extracting feature embedding. After fusing the features using the spatial-temporal mixer (STM) module (13), the fully connected layer was used to predict the growth probability. It was worth mentioning that the global information of VOIs was changeless on T_{t-1} and T_t. Hence, we only learned global feature embedding from Tt without Tt-1. However, the local information of the same nodule in T_{t-1} and T_t was different and highly discriminative for growth prediction. Therefore, we learned local feature embeddings from both T_{t-1} and T_t to capture the evolving local information.



FIGURE 3

The pipeline of organizing the dataset, including CT scan registration, ROI pairing, and class annotation. The letters d, v, and m denote the diameter, volume, and mass of lung nodules, respectively.



To efficiently leverage changing information of SSNs in both non-growth and growth groups, we took the weighted smooth-L1 loss instead of cross-entropy loss to train our model, as follows:

$$L = \alpha \times SmoothL_1(p, y) \times I_{\geq} + SmoothL_1(p, y)$$
$$\times (1 - I_{\geq})$$
(1)

In this model, p and y are the model output and ground truth of the relative growth rate, respectively. The indicator function $Iy \ge r = 1$ if $y \ge r$, and 0 otherwise, and r was set to 0.1. α is the imbalance coefficient and was set to 1.0, 2.0, 3.0, 4.0, and 5.0 for our experiments, where we found that 3.0 was the best value.

The model was trained from scratch for 100 epochs with the AdamW optimizer (20), with a weight decay of 0.05 and a momentum of 0.9. The batch size was set as 16, and learning rate from 10e-6 to $lr\timesBatchsize/64$ in the first five epochs, where lr = 5e-4, and then scheduled by the cosine annealing strategy (20).

Statistical analysis

Python 3.6.8 software with scipy.stats (1.8) and sklearn.metrics (1.0) packages was employed for data processing and statistical analysis. The reported statistical significance levels were all two-sided, and P< 0.05 was considered statistically significant.

Continuous variables were expressed as means \pm standard deviations and compared with t-tests. Categorical variables were expressed by frequency and compared using the χ^2 test. The discriminatory ability of these growth prediction models was

evaluated with receiver operating characteristic (ROC) curves. Then, the non-parametric bootstrap was used to estimate the variability around each of the performance measures.

Results

Growth-to-variability ratio

In total, 3,120 SSNs from 2,358 patients in the NLST dataset, including 2,983 (96%) GGNs and 137 (4%) part-solid nodules (PSNs), were selected for the study. Most patients with a total of 2,695 SSNs received at least three CT scans. To evaluate the best way for identifying the sub-solid nodule growth, we divided those SSNs from NLST into the cancer group (403 SSNs) and non-cancer group (2,717 SSNs) according to follow-up confirmation results. The increase rate and doubling time (21) of diameter, volume, and mass were calculated respectively (Table 1). The P-values of the measurements (without diameter double time) compared between cancer and noncancer groups were less than 0.05. In addition, mass had the smallest P-value, indicating that the difference in mass was more pronounced for cancer and non-cancer groups. In addition, mass had the shortest double time in the cancer group, which means mass has a better sensitivity for growth.

The mean time between the first and last CT examinations of the selected SSNs was 739 days (range, 521–1,274 days). During this period, the diameter, volume, and mass of the SSNs in the cancer group increased with a mean of 14%, 90%, and 121%, respectively, while in the non-cancer group the mean increased at 4%, 26%, and 19%, respectively. For distinguishing growth in the cancer and non-cancer groups, the increase rate in mass was

Ca	Cancer	1	Non-cancer	P	-value
	187		2508		-
0.07	0.07 ± 0.23		0.01 ± 0.16		0.002
711 (11 (638, 894)		793 (716, 899)		0.2
0.49	0.49 ± 2.05		0.06 ± 0.66		0.005
552 (52 (344, 725)		621 (458, 801)		0.04
0.74	0.74 ± 3.39		0.08 ± 0.83		0.009
488 (88 (321, 630)		623 (463, 799)		< 0.001
0.07 711 (0.49 552 (0.74 488 (0.07 ± 0.23 11 (638, 894) 0.49 ± 2.05 52 (344, 725) 0.74 ± 3.39 88 (321, 630)		$\begin{array}{l} 0.01 \pm 0.16 \\ \\ 793 \ (716, 899) \\ 0.06 \pm 0.66 \\ \\ 621 \ (458, 801) \\ 0.08 \pm 0.83 \\ \\ 623 \ (463, 799) \end{array}$		0. 0. 0. <0

TABLE 1 Different rates of change (between the latest two consecutive examine) in the NLST dataset.

Double time* (Q1, Q3): selected within [1, 1,000] for statistics. Number**: SSNs with consecutive Tt-1, Tt, and Tt+1.

more significant than those in volume and diameter (Figure 5). When the mass increased at greater than 25%, the SSNs showed a significant growth trend and were more likely to deteriorate into lung cancer.

Growth and non-growth subsolid nodule characteristics

According to the above analysis, the growth of SSNs was defined as an increase in mass at 25% within 1 year. There were 2,493 SSNs (174 growth, 2,319 non-growth), 627 SSNs (38 growth, 589 non-growth), and 213 SSNs (9 growth, 204 non-growth) in the training, validation, and external test sets, respectively (Table 2). In the training and validation sets from NLST, there were significant differences in average CT value (P< 0.01) and diameter (P< 0.001) between the growth and non-growth groups. However, in the external test set, only diameter

(P = 0.04) was significantly different between the growth and non-growth groups.

Model performance comparison

The deep learning-based and radiomics models were developed using the training set and were verified in the validation and test sets. The AUC of SiamModel was 0.858 (95% CI 0.786–0.921) in the validation set and 0.862 (95% CI 0.789–0.927) in the external test set (Table 3). The comparable results between the validation and external test sets showed that SiamModel had good generalization ability.

Compared with STM (13), our SiamModel obtained better performance with the AUC of 0.858 (95% CI 0.786–0.921) vs. 0.823 (95% CI 0.731–0.898) in the validation set and 0.862 (95% CI 0.789–0.927) vs. 0.806 (95% CI 0.693–0.902) in the external test set, which indicated the superiority of our proposed weighted smooth-l1 loss for SSN growth prediction.



Dataset	Characteristics	Growth (Q_1, Q_3)	Non-growth (Q_1, Q_3)	T/χ^2 value	P value
	Number	174	2319	-	_
	Age (years)	63 (59, 67)	62 (58, 66)	1.48	0.14
	Gender (male/female)	102/72	1312/1007	0.2	0.66
NLST train set	Average CT value (HU)	-598.4 (-692.1, 538.7)	-640.6 (-703.3, -589.7)	4.1	< 0.001
	Diameter (mm)	9.6 (5, 12.2)	5.6 (4, 6)	8.1	< 0.001
	Texture (GGNs/PSNs)	142/32	2247/72	90.82	0
	Number	38	589	-	_
	Age (years)	65 (61, 69)	62 (58, 66)	3.6	< 0.001
	Gender (male/female)	19/19	363/226	1.57	0.21
NLST Val Set	Average CT value (HU)	-564.2 (-679.8, -454.1)	-630.1 (-684.3, -581.1)	2.72	<0.01
	Diameter (mm)	12.9 (5.8, 20.5)	5.6 (4.0, 6.4)	6.03	< 0.001
	Texture (GGNs/PSNs)	19/19	363/226	31.6	0
	Number	9	204	-	_
	Age (years)	58 (47, 67)	53 (46, 61)	0.83	0.43
	Gender (male/female)	4/5	84/120	0.02	0.88
External test set	Average CT value (HU)	-553.2 (-700.1, -460.9)	-657.5 (-723.2, 600.9)	1.51	0.17
	Diameter(mm)	9.6 (7.1, 12)	6.2 (4, 7.1)	2.47	0.04
	Texture (GGNs/PSNs)	8/1	202/2	1.16	0.28

TABLE 2 The characteristics of patients and sub-solid nodules and the results of univariate analysis on training, validation, and external test sets.

Assuming all T_{t-1} scans were unavailable in datasets (using only T_t VOI as input), the performance of SiamModel and radiomics model was compared as shown in Table 3 and Figure 6. In the NLST validation set, the AUC values of SiamModel and radiomics model were 0.855 (95% CI 0.793– 0.908) and 0.760 (95% CI 0.646–0.857), respectively, and 0.821 (95% CI 0.725–0.904) and 0.681 (95% CI 0.506–0.841) in the external test set. Therefore, our SiamModel performed better than the radiomics model in both the NLST validation set and external test set (Figure 6).

Comparing one using only T_t VOI as input, we saw that our SiamModel with two VOIs $(T_{t-1} \mbox{ and } T_t)$ as input could perform slightly better, with an AUC of 0.858 vs. 0.855 in the NLST validation set and 0.862 vs. 0.821 in the external test set.

Examples of model prediction

Figure 7 provides examples predicted by our SiamModel in the external test set.

The probability of growth was calculated as shown in Eq. 2, where p and th are the model output and threshold selected for sensitivity and specificity as shown in Table 3, respectively, and τ is the sharpening coefficient, set as 0.1 to map p to 0-1:

$$prob = \frac{e(p-th)/\tau}{1+e(p-th)/\tau}$$
(2)

The predicted result with prob ≥ 0.5 indicated the growth, which required more attention from doctors and relatively intensive follow-up.

Data set	Method	AUC (95% CI)	Sensitivity (95% CI)	Specificity (95% CI)	PPV (95% CI)	NPV (95% CI)
NLST val	SiamModel	0.858	0.632	0.921	0.341	0.975
	(our)	(0.786-0.921)	(0.485-0.786)	(0.898-0.942)	(0.239-0.456)	(0.961-0.987)
	SiamModel	0.855	0.843	0.651	0.136	0.985
	(once, our)	(0.793-0.908)	(0.724-0.952)	(0.613-0.692)	(0.094-0.184)	(0.973-0.995)
	STM[13]	0.823	0.764	0.738	0.157	0.98
		(0.731-0.898)	(0.622-0.897)	(0.702-0.774)	(0.109-0.217)	(0.965-0.991)
	Radiomics (once)	0.76	0.763	0.465	0.085	0.968
		(0.646-0.857)	(0.615-0.889)	(0.424-0.506)	(0.059-0.114)	(0.947-0.986)
External test	SiamModel	0.862	0.893	0.749	0.134	0.994
	(our)	(0.789-0.927)	(0.625-1.000)	(0.685-0.807)	(0.056-0.230)	(0.980-1.000)
	SiamModel	0.821	0.889	0.669	0.106	0.993
	(once, our)	(0.725-0.904)	(0.625-1.000)	(0.608-0.731)	(0.040-0.179)	(0.977-1.000)
	STM[13]	0.806	0.895	0.574	0.083	0.992
		(0.693-0.902)	(0.636-1.000)	(0.507-0.664)	(0.034-0.141)	(0.972-1.000)
	Radiomics (once)	0.681	0.663	0.528	0.059	0.972
		(0.506-0.841)	(0.333-1.000)	(0.461-0.599)	(0.019-0.107)	(0.939-1.000)

TABLE 3 Performance of different models using only one CT scan in the validation and external test sets.

Discussion

Our study first compared the effectiveness of diameter, volume, and mass for assessing SSN growth based on the big data from NLST and found that mass had a better sensitivity to assess SSN growth. Then, we developed the deep learning-based model (SiamModel) to predict the mass growth of SSNs and achieved good performance in both the validation set (AUC = 0.858) and the external test set (AUC = 0.862).

For pulmonary nodules discovered in screening or incidentally, the first task was to assess risk of malignancy. There are several models (22–24) which combined clinical and radiographic factors to estimate the malignancy probability and achieve fair performance (25). For those indeterminate nodules, follow-up would be recommended (26). The growth pattern of lung nodules (18, 27) would increase the accuracy rate to diagnose malignant nodules and reduce the false positives, although some benign nodules would grow (28).

In addition, there are several methods to measure nodule growth, such as diameter, volume, and mass. Nodule growth or the solid component in part-solid nodule growth is defined as an increase in diameter of more than 1.5 mm in Lung-Reporting and Data Systems (RADS) (27) and in the National Comprehensive Cancer Network (NCCN) algorithm (NCCN 2022 screening). While 2 mm was chosen as the threshold for defining growth in both overall nodule size and the solid component of a part-solid nodule in the Fleischner Society (24), I-ELCAP requires different sizes of growth according to



FIGURE 6

Receiver operating characteristic (ROC) curves on NLST validation set (left) and external test set (right). SiamModel (once) and radiomics (once) are only using Tt VOI as input.



initial diameter of nodules (I-ELCAP protocol. Available at https://www.ielcap.org/protocols Accessed June 14,2022). Because the investigator of NELSON thought volume measurements are more accurate than size by means of semiautomatic software calculation, growth was defined as a change in volume of at least 25% growth of pulmonary nodules (29, 30) and volume measurement was also recommended in the British Thoracic Society pulmonary nodule management guidelines (22). Additionally, the volume doubling time (VDT) of SSN would be longer, and VDT may not be sensitive to different indolent lung cancers from benign nodules. Our study also showed a mean of VDT cancer growth and non-cancer growth (552 vs. 621 days, P = 0.04) and was close to the NLST databases.

Furthermore, Hoop et al. (6) compared measurements of diameter, volume, and mass in 52 pulmonary GGNs and found that mass is the best method for identifying malignant GGNs and detection of growth of GGNs. Our study also found that mass growth was the most sensitive method to identify the growth of SSNs, since the growth of mass might reflect the volume, density, or solid component growth. Compared with Hoop et al.'s study (6), we investigated growth rate in SSNs from NLST and validated the data in a larger number of patients. Moreover, we used an automatic machine learning method to measure volume and mass, which would reduce the consumption of time and labor.

Initial size (31), CT attenuation (3), and history of lung cancer (30) were associated with GGN growth according to the first-time CT results and clinical factors. For those pulmonary nodules which require follow-up, previous studies focus on classifying and few rely on prediction factors for the GGO

growth. Radiomics and deep learning techniques have been investigated to detect, segment, and classify in the field of pulmonary nodule management (7, 32) in the past 10 years. Radiomics could extract the high quantitative image features from medical imaging (32, 33) and build high-performance models with limited datasets. Several studies (34) have demonstrated that radiomic signatures can differentiate malignant and benign nodules with a sensitivity ranging from 76.2 to 92.9% and a specificity ranging from 72.7 to 96.1%. The combined radiographic factor or supervised machine learning with the radiomics model could achieve better performance (34, 35). In the traditional radiomics methods to classify pulmonary nodules (11), large amounts of labor are required for manual tumor segmentation and feature extraction. Deep learning algorithms could detect and segment pulmonary nodules automatically and build predictive models. Ardila et al. (8) developed a predictive model of the risk of lung cancer by the 3D deep learning method and achieved algorithms that were comparable to, or could even outperform, radiologists with or without prior CT imaging. A Lung Cancer Prediction Convolutional Neural Network model (36) was also found to outperform the Brock model to predict risk of lung cancer. A deep machine learning algorithm developed by Huang et al. (21) was compared with Lung-RADS and volume doubling time to inform lung cancer incidence with 1, 2, and 3 years. As for growth of pulmonary nodules, Tao et al. (18) first manually segmented 313 lung nodules in 246 patients in their hospital then developed a convolutional neural network (CNN) to model the imagery change in the nodules from the baseline CT image to the follow-up CT image and achieved an AUC of 0.857 for solid nodules and 0.843 for GGNs in differentiating growth and nongrowth nodules. Compared with Tao et al. (18), we first trained the detection and segmentation models on LUNA16 and LNDb datasets and then used them to identify and segment SSNs automatically which was easily reproducible. As for the growth of SSNs, we developed a deep learning-based model, called SiamModel. In the independent external test set, our SiamModel could predict the growth of SSNs with good performance (AUC = 0.862) and showed a significant improvement, compared with the radiomics model.

This study has the following limitations: (a) the growth and non-growth SSNs were extremely imbalanced in our external test set, so a validation bias might exist; and (b) the training set only contained low-dose CT scans, but the external set enrolled both normal CT and low-dose CT scans, therefore, it is still necessary to expand the training and test sets with more normal CT scans in further study; and (c) we defined an increase of at least 25% in mass as the growth of SSNs without an exact derivation which should be tested in further clinical practice.

Mass increase rate can reflect the growth of SSNs associated with lung cancer more sensitively than diameter and volume increase rates. Further, we established a deep learning-based model (called SiamModel) that could better predict the growth of SSNs on the base of mass, compared with the radiomics model.

Data availability statement

The original contributions presented in the study are included in the article/supplementary material. Further inquiries can be directed to the corresponding authors.

Ethics statement

This study was reviewed and approved by Guangdong Provincial People's Hospital (KY-Z-2022-125-01). Written informed consent for participation was not required for this study in accordance with the national legislation and the institutional requirements.

References

1. Sung H, Ferlay J, Siegel RL, Laversanne M, Soerjomataram I, Jemal A, et al. Global cancer statistics 2020: Globocan estimates of incidence and mortality worldwide for 36 cancers in 185 countries. *CA Cancer J Clin* (2021) 71:209–49. doi: 10.3322/caac.21660

2. Aberle DR, Adams AM, Berg CD, Black WC, Clapp JD, Fagerstrom RM, et al. Reduced lung-cancer mortality with low-dose computed tomographic screening. *N Engl J Med* (2011) 365:395–409. doi: 10.1056/NEJMoa1102873

3. Gao C, Li J, Wu L, Kong D, Xu M, Zhou C. The natural growth of subsolid nodules predicted by quantitative initial ct features: A systematic review. *Front Oncol* (2020) 10:318. doi: 10.3389/fonc.2020.00318

Author contributions

XY contributed to conception and design of the study. RL wrote the first draft of the manuscript and analyze data. AL organized the database. HHY performed the statistical analysis. JL, SL, BJ, SD, QN, WZ contributed to collect clinical data. BL, YW, JF, HL, YH, CS, HFY contributed to analyze data. YW supervised the study. All authors contributed to manuscript revision, read, and approved the submitted version.

Funding

This work was supported by the research fund from Guangzhou Municipal Science and Technology Bureau (grant no. 202201011664 to XY).

Conflict of interest

XY, YW, RL, HHY, JL, SL, BJ, SD, QN, WZ are employed by Guangdong Provincial People's Hospital. BL is employed by South China University of Technology. Authors AL, JW, JF and HL are employed by Guangzhou Shiyuan Electronics Co., Ltd.

The remaining authors declare that the research was conducted in the absence of any commercial or financial relationships that could be construed as a potential conflict of interest.

Publisher's note

All claims expressed in this article are solely those of the authors and do not necessarily represent those of their affiliated organizations, or those of the publisher, the editors and the reviewers. Any product that may be evaluated in this article, or claim that may be made by its manufacturer, is not guaranteed or endorsed by the publisher.

4. Singh R, Kalra MK, Homayounieh F, Nitiwarangkul C, McDermott S, Little BP, et al. Artificial intelligence-based vessel suppression for detection of sub-solid nodules in lung cancer screening computed tomography. *Quant Imaging Med Surg* (2021) 11:1134–43. doi: 10.21037/qims-20-630

 Sun Q, Huang Y, Wang J, Zhao S, Zhang L, Tang W, et al. Applying CT texture analysis to determine the prognostic value of subsolid nodules detected during low-dose CT screening. *Clin Radiol* (2019) 74:59–66. doi: 10.1016/j.crad.2018.07.103

6. de Hoop B, Gietema H, van de Vorst S, Murphy K, van Klaveren RJ, Prokop M. Pulmonary ground-glass nodules: increase in mass as an early indicator of growth. *Radiology* (2010) 255:199–206. doi: 10.1148/radiol.09090571

7. Bi WL, Hosny A, Schabath MB, Giger ML, Birkbak NJ, Mehrtash A, et al. Artificial intelligence in cancer imaging: Clinical challenges and applications. *CA Cancer J Clin* (2019) 69:127–57. doi: 10.3322/caac.21552

8. Ardila D, Kiraly AP, Bharadwaj S, Choi B, Reicher JJ, Peng L, et al. Endto-end lung cancer screening with three-dimensional deep learning on lowdose chest computed tomography. *Nat Med* (2019) 25:954–61. doi: 10.1038/ s41591-019-0447-x

9. Ather S, Kadir T, Gleeson F. Artificial intelligence and radiomics in pulmonary nodule management: current status and future applications. *Clin Radiol* (2020) 75:13–9. doi: 10.1016/j.crad.2019.04.017

10. Li R, Xiao C, Huang Y, Hassan H, Huang B. Deep learning applications in computed tomography images for pulmonary nodule detection and diagnosis: A review. *Diagno (Basel)* (2022) 12(2):298. doi: 10.3390/diagnostics12020298

11. Fahmy D, Kandil H, Khelifi A, Yaghi M, Ghazal M, Sharafeldeen A, et al. How ai can help in the diagnostic dilemma of pulmonary nodules. *Cancers (Basel)* (2022) 14(7):1840. doi: 10.3390/cancers14071840

12. Murchison JT, Ritchie G, Senyszak D, Nijwening JH, van Veenendaal G, Wakkie J, et al. Validation of a deep learning computer aided system for CT based lung nodule detection, classification, and growth rate estimation in a routine clinical population. *PloS One* (2022) 17:e0266799. doi: 10.1371/journal.pone.0266799

13. Fang J, Wang J, Li A, Yan Y, Hou Y, Song C, et al. Siamese Encoder- based spatial-temporal mixer for growth trend prediction of lung nodules on ct scans. *arXiv* (2022) 2206:03049. doi: 10.1007/978-3-031-16431-6_46

14. Setio AAA, Traverso A, de Bel T, Berens MSN, Bogaard CVD, Cerello P, et al. Validation, comparison, and combination of algorithms for automatic detection of pulmonary nodules in computed tomography images: The LUNA16 challenge. *Med Image Anal* (2017) 42:1–13. doi: 10.1016/j.media.2017.06.015

15. Pedrosa J, Aresta G, Ferreira C, Rodrigues M, Leit⁻ao P, Carvalho AS, et al LNDb: A lung nodule database on computed tomography. *arXiv* (2019). doi: 10.48550/arXiv.1911.08434

16. Zhou X, Wang D, Kr"ahenbu"hl P. Objects as points. arXiv (2019) 1904:07850. doi: 10.48550/arXiv.1904.07850

17. Kushnure DT, Talbar SN. MS-UNet: A multi-scale UNet with feature recalibration approach for automatic liver and tumor segmentation in CT images. *Comput Med Imaging Graph* (2021) 89:101885. doi: 10.1016/j.compmedimag.2021.101885

18. Tao G, Zhu L, Chen Q, Yin L, Li Y, Yang J, et al. Prediction of future imagery of lung nodule as growth modeling with follow-up computed tomography scans using deep learning: a retrospective cohort study. *Transl Lung Cancer Res* (2022) 11:250–62. doi: 10.21037/tlcr-22-59

19. Tibshirani R. Regression shrinkage and selection via the lasso. J R Stat Soc: Ser B (Methodological) (1996) 58:267–88. doi: 10.1111/j.2517-6161.1996.tb02080.x

20. Loshchilov I, Hutter F. Stochastic gradient descent with warm restarts. *Proceedings 5th Int Conf Learn Represent* (2016). 1–16. Available at: https://arxiv.org/abs/1608.03983v1

21. Huang P, Lin CT, Li Y, Tammemagi MC, Brock MV, Atkar-Khattra S, et al. Prediction of lung cancer risk at follow-up screening with low-dose CT: a training and validation study of a deep learning method. *Lancet Digit Health* (2019) 1:e353– e62. doi: 10.1016/S2589-7500(19)30159-1 22. Baldwin DR, Callister ME. The British thoracic society guidelines on the investigation and management of pulmonary nodules. *Thorax* (2015) 70:794–8. doi: 10.1136/thoraxjnl-2015-207221

23. Gould MK, Ananth L, Barnett PG. A clinical model to estimate the pretest probability of lung cancer in patients with solitary pulmonary nodules. *Chest* (2007) 131:383–8. doi: 10.1378/chest.06-1261

24. Bankier AA, MacMahon H, Goo JM, Rubin GD, Schaefer-Prokop CM, Naidich DP. Recommendations for measuring pulmonary nodules at ct: A statement from the fleischner society. *Radiology* (2017) 285:584–600. doi: 10.1148/radiol.2017162894

25. Zhang K, Wei Z, Nie Y, Shen H, Wang X, Wang J, et al. Comprehensive analysis of clinical logistic and machine learning-based models for the evaluation of pulmonary nodules. *JTO Clin Res Rep* (2022) 3:100299. doi: 10.1016/j.jtocrr.2022.100299

26. Wood DE, Kazerooni EA, Aberle D, Berman A, Brown LM, Eapen GA, et al. NCCN guidelines[®] insights: Lung cancer screening, version 1.2022 (2022). Available at: https://jnccn.org/view/journals/jnccn/20/7/article-p754.xml.

27. Pinsky PF, Gierada DS, Black W, Munden R, Nath H, Aberle D, et al. Performance of lung-rads in the national lung screening trial: A retrospective assessment. *Ann Intern Med* (2015) 162:485–91. doi: 10.7326/M14-2086

28. Zhang R, Tian P, Qiu Z, Liang Y, Li W. The growth feature and its diagnostic value for benign and malignant pulmonary nodules met in routine clinical practice. *J Thorac Dis* (2020) 12:2019–30. doi: 10.21037/jtd-19-3591

29. van Klaveren RJ, Oudkerk M, Prokop M, Scholten ET, Nackaerts K, Vernhout R, et al. Management of lung nodules detected by volume CT scanning. *N Engl J Med* (2009) 361:2221–9. doi: 10.1056/NEJMoa0906085

30. de Koning HJ, van der Aalst CM, de Jong PA, Scholten ET, Nackaerts K, Heuvelmans MA, et al. Reduced lung-cancer mortality with volume ct screening in a randomized trial. *N Engl J Med* (2020) 382:503–13. doi: 10.1056/NEJMoa1911793

31. Hiramatsu M, Inagaki T, Inagaki T, Matsui Y, Satoh Y, Okumura S, et al. Pulmonary ground-glass opacity (GGO) lesions-large size and a history of lung cancer are risk factors for growth. *J Thorac Oncol* (2008) 3:1245–50. doi: 10.1097/ JTO.0b013e318189f526

32. Lambin P, Leijenaar RTH, Deist TM, Peerlings J, de Jong EEC, van Timmeren J, et al. Radiomics: the bridge between medical imaging and personalized medicine. *Nat Rev Clin Oncol* (2017) 14:749–62. doi: 10.1038/ nrclinonc.2017.141

33. Lambin P, Rios-Velazquez E, Leijenaar R, Carvalho S, van Stiphout RG, Granton P, et al. Radiomics: extracting more information from medical images using advanced feature analysis. *Eur J Cancer* (2012) 48:441–6. doi: 10.1016/j.ejca.2011.11.036

34. Wu YJ, Wu FZ, Yang SC, Tang EK, Liang CH. Radiomics in early lung cancer diagnosis: From diagnosis to clinical decision support and education. *Diagno (Basel)* (2022) 12(5):1064. doi: 10.3390/diagnostics12051064

35. Tan M, Ma W, Sun Y, Gao P, Huang X, Lu J, et al. Prediction of the growth rate of early-stage lung adenocarcinoma by radiomics. *Front Oncol* (2021) 11:658138. doi: 10.3389/fonc.2021.658138

36. Massion PP, Antic S, Ather S, Arteta C, Brabec J, Chen H, et al. Assessing the accuracy of a deep learning method to risk stratify indeterminate pulmonary nodules. *Am J Respir Crit Care Med* (2020) 202:241–9. doi: 10.1164/rccm.201903-0505OC