

Iridium (III) complex-loaded liposomes as a drug delivery system for lung cancer through mitochondrial dysfunction

Cancheng Liao*
Danqiao Xu*
Xiaohong Liu
Yuqi Fang
Jun Yi
Xiaofang Li
Bohong Guo

Department of Pharmaceutics,
Guangdong Pharmaceutical University,
Guangzhou 510006, China

*These authors contributed equally
to this work

Background and aim: Iridium (Ir)-based complex is a potential antitumor ingredient, but its poor physicochemical properties such as hydrophobicity and low biocompatibility hamper further application. Liposome provides a potential delivery approach for improving the poor physicochemical property and reducing the side effects of antitumor drug. In this study, we aimed at incorporating Ir ($[\text{Ir}(\text{ppy})_2(\text{BTCP})]\text{PF}_6$) into liposomes to enhance the biocompatibility and sustained release of Ir for intravenous administration and to elucidate the mechanism in A549 cells.

Materials and methods: Ir-loaded PEGylated liposomes (Lipo-Ir) were formulated by thin-film dispersion and ultrasonic method. Morphology, size distribution, and zeta potential of Lipo-Ir were examined by transmission electron microscopy (TEM) and Zetasizer. The released profile and biocompatibility were investigated by dialysis method and hemolysis test, respectively. Additionally, the cytotoxic activity and mechanism of Lipo-Ir and Ir inducing apoptosis in A549 cells were evaluated.

Results: Lipo-Ir can keep sustained release, excellent biocompatibility, and physical stability. The average particle size, polydispersity index, zeta potential, encapsulation efficiency, and drug loading are 112.57 ± 1.15 nm, 0.19 ± 0.02 , -10.66 ± 0.61 mV, $94.71\% \pm 3.21\%$, and $4.71\% \pm 0.41\%$, respectively. 3-(4,5-dimethylthiazole)-2,5-diphenyltetraazolium bromide (MTT) assay show that Lipo-Ir and Ir display high cytotoxicity against selected cancer cells. Furthermore, the apoptotic features of morphology, depolarization of mitochondrial membrane potential, increase in the reactive oxygen species (ROS) levels, and disorder of Ca^{2+} homeostasis are observed after treating A549 cells with Ir and Lipo-Ir. Besides, Lipo-Ir can arrest the cell growth in G_0/G_1 phase.

Conclusion: The studies demonstrate that Lipo-Ir can trigger apoptosis in A549 cells via ROS-mediated mitochondrial dysfunctions, and the biocompatible and sustained Lipo-Ir will be a promising drug delivery system.

Keywords: iridium complex, liposome, apoptosis, reactive oxygen species, mitochondria

Introduction

Lung cancer occupies the leading cause of cancer incidence and mortality rates in the USA during the most recent 5 years.¹ At this point, most patients with lung cancer cannot accept curative surgery, and therefore, chemotherapy is still the major treatment method. Ever since the introduction of cisplatin into the field of oncology, the potential of metal-based anticancer agents had been fully realized and explored. However, cisplatin-based drug exhibited several severe side effects.^{2,3} Therefore, it is inevitable to explore new metal-based agents as a substitution of cisplatin-based drug. Iridium

Correspondence: Bohong Guo
Department of Pharmaceutics,
Guangdong Pharmaceutical University,
280 East Waihuan Road, Guangzhou
Higher Education Mega Center,
Guangzhou 510006, China
Email guobohong@gdpu.edu.cn

(Ir)-based complexes could be great alternatives attributed to their limited side effect, high antitumor activity, and rich photophysical properties.⁴⁻⁷ As a promising antitumor active pharmaceutical ingredient (API), Ir (III) complexes can evoke ROS overload, cause a decrease in the mitochondrial membrane potential (MMP), and eventually induce cancer cell apoptosis.⁸

The nonionic surfactants are used as formulation vehicles for many poor soluble anticancer agents such as paclitaxel and docetaxel, but severe hypersensitivity reactions may accompany with the administration. Numerous drawbacks of conventional drug delivery system such as burst release, low biocompatibility, and non-target specificity had emerged in the past.⁹⁻¹³ Irregular release may stimulate the fluctuation of drug plasma concentration and pose a potential risk to the patients. Insufficient biocompatibility impairs the physiological capacity of normal cells or tissue. To circumvent these deficiencies, liposomal technology has attracted a great interest in the nanomedicine field owing to the liposomal features of low toxicity, biodegradability, and sustained release.¹⁴ Liposome is a self-assembled lipid bilayer vesicle through the hydrophobic association of phospholipids. It exists in the shape of unilaminar or multilaminar vesicle that can encapsulate hydrophobic or hydrophilic molecules.¹⁵ In addition, liposome shows a “stealth” property when the surface was modified with polyethylene glycol (PEG) or PEG-derivative phospholipids,^{16,17} which prevents liposomes from binding most components in blood, especially opsonin. Therefore, the PEGylated liposome can increase stability, reduce the affinity of mononuclear phagocyte system, and extend its half-life.¹⁸ Due to the presence of a discontinuous endothelial lining in the tumor angiogenesis, PEGylated liposomes can extravert into the interstitial space of vasculature.¹⁹ Consequently, PEGylated liposomes can passively accumulate in tumor tissues.

Previous reports showed that Ir could induce autophagy and apoptosis of SGC-7901 cells, and exhibited good anti-neoplastic activity.²⁰ However, it was difficult to prepare pharmaceutical formulations for parenteral administration due to the poor physicochemical property of Ir complex. Hence, to ameliorate these shortcomings, we incorporated Ir into lipid bilayer to form an Ir-loaded PEGylated liposomes (Lipo-Ir) and then evaluated the sustained profile and biocompatibility of Ir and Lipo-Ir. Additionally, the anticancer activity of Lipo-Ir was performed against A549 cells. The cytotoxicity *in vitro* was examined by 3-(4,5-dimethylthiazole)-2,5-diphenyltetrazolium bromide (MTT) method, and anticancer activity was studied by apoptosis,

cellular uptake, intracellular localization, reactive oxygen species (ROS), MMP, intracellular Ca²⁺ measurement, and cell cycle arrest. Our findings offer promise for the drug delivery system of Lipo-Ir (Scheme 1).

Materials and methods

Materials

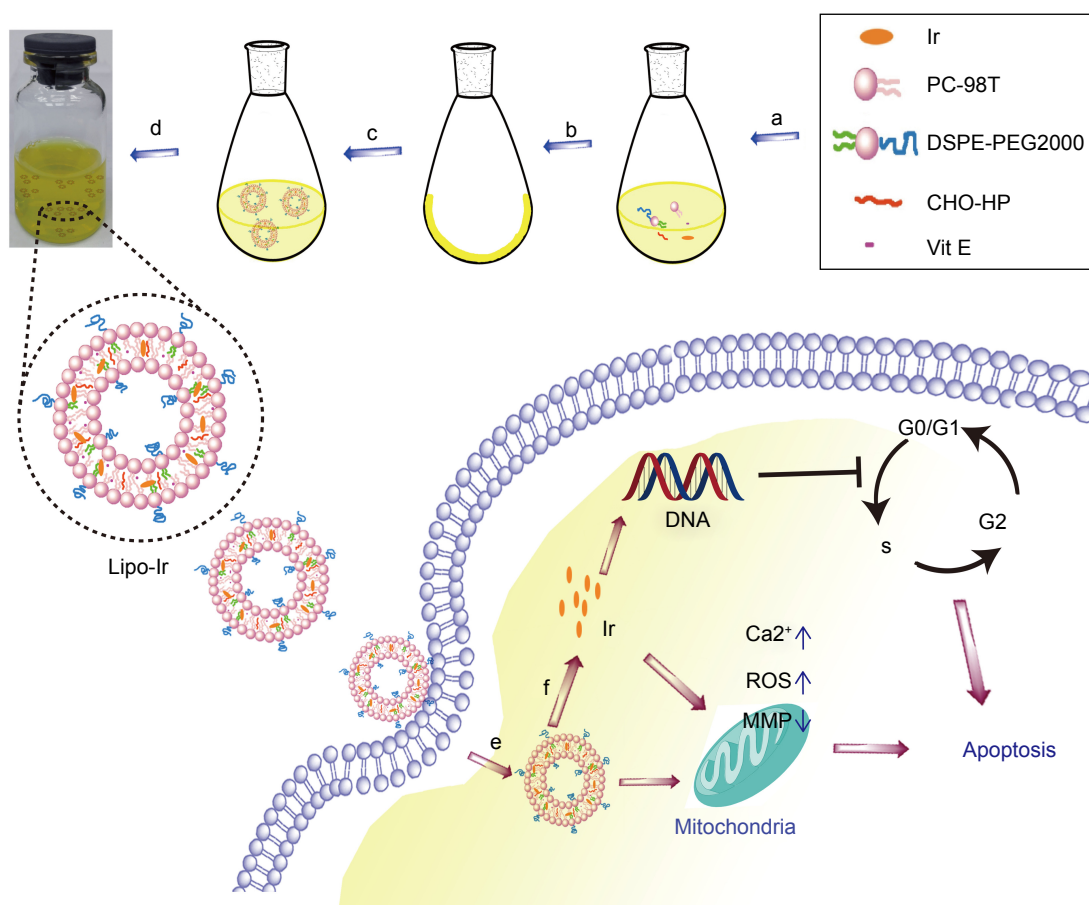
It was prepared according to the study by Zhang et al.²⁰ DSPE-MPEG2000, cholesterol (CHO-HP), and egg yolk lecithin (PC-98T) were purchased from Shanghai A.V.T. Pharmaceutical Ltd (Shanghai, China) (pharmaceutical injection grade, purity >98%). RPMI 1640 was obtained from Thermo Fisher Scientific (Waltham, MA, USA). A549 cells (human lung adenocarcinoma) were purchased from the American Type Culture Collection (ATCC) (Manassas, VA, USA). Fetal bovine serum (FBS) was obtained from Thermo Fisher Scientific (Waltham, MA, USA). All other chemicals and reagents were analytical or chromatographic grade.

Preparation of Lipo-Ir

Lipo-Ir was prepared using thin-film dispersion method as previously reported with minor modification.²¹ Briefly, PC-98T, CHO-HP, DSPE-MPEG2000, and vitamin E at a molar ratio of 79.7:15.6:3.98:0.7 were dissolved in a mixture of chloroform–alcohol (3:1, v/v). Then, Ir (Ir:PC-98T = 1:12.4, w/w) was added to the flask. To form the homogeneous thin film, organic solvent was removed with a rotary vacuum evaporator at 46°C and the residual solvent was totally removed under vacuum for 2 h at 45°C. Subsequently, the dried lipid film was hydrated with 5 mL phosphate-buffered saline (PBS; pH 7.4) by vortex shedding for 20 min at 45°C. To obtain a homogeneous size, the suspensions were sonicated in cell sonicator for 150 s at 300 W, and then filtered through 200 nm pore size polycarbonate membranes (EMD Millipore, Billerica, MA, USA). The final products were obtained by freeze-drying. The blank PEGylated liposomes (Blank-Lipo) were prepared using the same procedure without Ir.

Characterization of liposomes

The morphology of Lipo-Ir was characterized through a transmission electron microscopy (TEM) with negative staining by 3% phosphotungstic acid after the Lipo-Ir was diluted 10-fold. The particle size, polydispersity index (PDI), and zeta potential of the liposomes were analyzed using a Delsa Nano S Particle Analyzer (Beckman Coulter, Brea, CA, USA) at ambient temperature after diluting to appropriate concentration.



Scheme 1 Schematic design of Lipo-Ir: (a) mixture and dissolution of material; (b) evaporation of solvent under vacuum to form a lipid film; (c) hydration with PBS and self-assembly; (d) ultrasonic to reduce the diameter; (e) internalization; and (f) Ir release from Lipo-Ir to target mitochondria.

Abbreviations: Ir, iridium; Lipo-Ir, Ir-loaded PEGylated liposomes; PBS, phosphate-buffered saline; PEG, polyethylene glycol; ROS, reactive oxygen species; Vit, vitamin; MMP, mitochondrial membrane potential.

Encapsulation efficiency (EE) and drug loading (DL) of liposomes

The EE and DL of the liposomes were detected by high-velocity centrifugal method. The resulting liposomes were centrifuged at 35,000 rpm for 1 h at 4°C in a preparative ultracentrifuge. Then, the supernatant containing free Ir was measured by HPLC and the total content of Ir in liposomes suspension was determined after destroying liposomes with ethanol. The EE (%) and DL (%) of Lipo-Ir were calculated using the following equations:²²

$$EE (\%) = \frac{M_t - M_f}{M_t} \times 100 \quad (1)$$

$$DL (\%) = \frac{M_t - M_f}{M_t - M_f + M_p} \times 100 \quad (2)$$

where M_f is the analyzed weight of untrapped Ir in the outer aqueous phase, M_t is the total weight of Ir used in the

formulation, and M_p is the total weight of lipids added in the formulation.

Drug release from liposomes

In vitro release profile of Ir from Lipo-Ir suspension was performed using dialysis method. Briefly, Lipo-Ir formulation (300 µg Ir-equivalent) was sealed in cellulose dialysis bags (MWCO = 8–14 kDa) and immersed in 100 mL (pH 7.4) PBS containing 0.5% Tween 80 (w/v) to maintain sink condition. Afterward, the flask was kept on continuous stirring at 100 rpm using a magnetic stirrer at 37°C. At predetermined time, aliquot of dialysate (2 mL) was withdrawn and equivalent volume of fresh buffer was added. The amount of Ir in dialysate was quantified by HPLC, and the cumulative release was calculated. As a contrast, in vitro release of Ir (Ir dispersed in PBS containing 0.5% Tween 80 [w/v]) was implemented as mentioned earlier.

Physical stability of Lipo-Ir

The physical stability of Lipo-Ir was assessed by monitoring the particle size and EE of Lipo-Ir. Briefly, Lipo-Ir was stored

in refrigerator (4°C). After 0, 15, 30, and 60 days, Lipo-Ir was diluted appropriately and the particle size was analyzed by DelsaNano S Particle Analyzer. Moreover, the EE of Lipo-Ir was determined by using high velocity centrifugal method as above-mentioned process.

Hemolysis test

Hemolytic activity of Lipo-Ir was evaluated by measuring the hemolysis percentages of red blood cells (RBCs).²³ The venous blood was obtained from New Zealand rabbit. All procedures were approved by the GuangDong Pharmaceutical University Experimental Animal Ethics Committee and were performed in accordance with the NIH guidelines for the Care and Use of Laboratory Animals. The RBCs were harvested by centrifugation at 900 rpm for 5 min and washed several times with normal saline. Afterward, RBCs were resuspended in normal saline at a cell density of 2% (v/v). Equivalent volume of 2% RBC suspension was mixed with Lipo-Ir suspension to achieve a final Ir concentrations ranging from 18.75 to 93.75 µg/mL and incubated at 37°C for 2 h. In addition, RBCs were added to water and normal saline under the same condition as 100 and 0% hemolysis, respectively. Subsequently, the supernatants were collected by centrifugation at 900 rpm for 5 min. The absorption values of supernatants were measured by an UV-visible light spectrophotometer at 540 nm. For comparison, free Ir was formulated in 4.5% ethanol (v/v) and 12 mg/mL Tween 80 mixed saline solution. Then, the hemolytic activity of Ir was assessed as process mentioned earlier. The calculation formula of hemolysis percentages was as follows:

$$\text{Hemolysis (\%)} = \frac{A_{\text{sample}} - A_{0\%}}{A_{100\%} - A_{0\%}} \times 100 \quad (3)$$

where A_{sample} , $A_{0\%}$, and $A_{100\%}$ are the absorbance of samples, a solution of 0% hemolysis, and a solution of 100% hemolysis, respectively.

Cytotoxic activity evaluation in vitro

MTT assay was performed to evaluate the in vitro cytotoxic activity of Ir and Lipo-Ir in A549 cells. The cells were seeded in 96-well microassay culture plates (1×10^4 cells/well) and incubated at 37°C for overnight. The cells treated with Ir (0.47–15 µM; final DMSO was <0.5%), Lipo-Ir (0.47–15 µM Ir-equivalent), or Blank-Lipo (lipid concentration of 9.11–214.50 µg/mL) were allowed to incubate for 24 and 48 h and treated with RPMI 1640 medium as blank control. Upon completion of the incubation, the cells were

incubated in serum deprivation medium containing 0.5% MTT for 4 h. Subsequently, the medium was replaced with 100 µL of DMSO to dissolve the formazan. The absorbance was measured at 490 nm in a microplate spectrophotometer, and the experiments were repeated three times. For the viability of A549 cells, the following formula can be used:

$$\text{Viability of cells (\%)} = \frac{\text{Absorbance}_{\text{sample}}}{\text{Absorbance}_{\text{control}}} \times 100 \quad (4)$$

Cellular uptake

A549 cells were placed in 12-well plates at a seeding density of 1.5×10^5 cells/well and incubated overnight. Cells were then exposed to either free Ir or Lipo-Ir at a concentration of 8 µM for 0.5 or 2 h. After incubation, the cells were stained with Hoechst 33342 for 10 min and rinsed twice with cold PBS. The cells were imaged under the ImageXpress® High Content Screening System (IXM; Molecular Devices LLC, Sunnyvale, CA, USA) using 40× objectives with DAPI and FITC filters.²⁴

Intracellular localization

A549 cells were incubated in 12-well plates at a density of 1.5×10^5 cells/well. After 24 h, cells were incubated with free Ir (3 µM) and Lipo-Ir (3 µM Ir-equivalent) for 0.5, 2, or 12 h. Afterward, the cells were washed twice using cold PBS and stained with the MitoTracker® Deep Red FM (100 nM; Thermo Fisher Scientific, Waltham, MA, USA) for ~30 min and rinsed twice with cold PBS again. Fluorescence images of the cells were captured on IXM using 40× objectives with Texas Red and FITC filters.

Apoptosis morphological changes assay

The morphology of apoptosis was assessed using acridine orange (AO)/ethidium bromide (EB) and Hoechst 33342 staining methods. Briefly, following incubation of A549 cells in 12-well plates with free Ir or Lipo-Ir (3 µM Ir-equivalent) for 24 h, the medium was removed and the cells were incubated in FBS-free RPMI 1640 containing AO (50 µg/mL) and EB (50 µg/mL) for 10 min. After incubation, the cells were rinsed with cold PBS and imaged by IXM.

MMP ($\Delta\Psi_m$) assay

A549 cells were treated for 24 h with 3 µM of the Ir and Lip-Ir in 12-well plates and were then washed three times with cold PBS. The cells were incubated for 20 min with 1 µg/mL of 5,5',6,6'-tetrachloro-1,1',3,3'-tetraethylbenzimidazolcarbocyanine iodide (JC-1) in culture medium at 37°C. The cells

were rinsed with ice-cold PBS again and then were imaged by IXM. The ratio of red/green fluorescence intensity was analyzed by the MateXpress6 software.

ROS detection

A549 cells were seeded into 12-well plates at a density of 10×10^4 cells/well and incubated for 24 h. Then, A549 cells were exposed to free Ir (3 μM), Lipo-Ir (3 μM Ir-equivalent), or equal volume of PBS (negative control group) for 24 h. Afterward, the cells were stained with 10 μM 2',7'-dichlorodihydrofluorescein diacetate (DCFH-DA) in dark for 20 min. Subsequently, extracellular dye was discarded and cells were rinsed with cold PBS twice. Eventually, images were captured by IXM. The fluorescent intensity was analyzed by the MateXpress6 software.

Intracellular Ca^{2+} measurement

Intracellular Ca^{2+} (Ca_i^{2+}) concentration was monitored using Fluo-3 AM as Ca^{2+} indicator. A549 cells were treated with free Ir (3 μM) and Lipo-Ir (3 μM) for 24 h. After treatments, cells were loaded with Fluo-3 AM (3 μM) in dark for 30 min. After washing, the cells were imaged by IXM using 20 \times objectives with FITC filter and the fluorescent intensity was analyzed by the MateXpress6 software.

Cell cycle arrest by flow cytometry

A549 cells were dispensed into six-well plates at a density of 4×10^5 cells/well and incubated for 24 h. Cells were treated with Ir (3 and 5 μM) and Lipo-Ir (3 and 5 μM Ir) for 24 h, the cells were harvested by trypsinization, washed with PBS, and fixed with 70% ethanol at 4°C overnight. Then, the fixed cells were collected and resuspended in propidium iodide (PI) staining solution (20 $\mu\text{g}/\text{mL}$ PI, 200 $\mu\text{g}/\text{mL}$ RNase A, and 0.05% Triton X-100) for 30 min at 37°C in dark. Then, the cells were analyzed with a flow cytometer.

Statistical analysis

The data were evaluated using one-way analysis for statistical significance. The results were presented as mean \pm SD ($n=3$). Differences were considered to be statistically significant at $P < 0.05$.

Results and discussion

Preparation and characterization of liposomes

Liposomes were first proposed as carriers of biologically active substances in 1971,²⁵ and it could be used to increase the solubility and biocompatibility of drug and prolong the

drug duration in vivo, when targeted specifically. Consequently, we encapsulated Ir into liposomes for intravenous administration. Physicochemical properties of nanoparticles, in some way, determine their behavior in biological application and affect the safety, stability, and effectiveness of colloidal system.^{26,27} Hence, adequate characterization of liposomes is essential. Among the characteristics, surface charge and particle size are the two most commonly mentioned factors, which are associated with biological effects of nanoparticles including cellular uptake, toxicity, and dissolution.²⁶ Herein, the particle size, PDI, zeta potential (Figure S1C), EE (%), and DL (%) of Lipo-Ir were detected and are listed in Table S1. Additionally, we found that the Lipo-Ir was spherical or quasi-spherical particles (Figure S1B).

The average particle size of Lipo-Ir is 112.57 ± 1.15 nm, and the PDI value is 0.19 ± 0.02 , which indicate that Lipo-Ir has a comparatively homogeneous size (Figure S1A). The zeta potential, depending on the kind and composition proportion of lipids, was related with colloid physical stability, because the raise of zeta potential could resist the proximity of particles and promote the stability of dispersion.²⁸ Blank-Lipo and Lipo-Ir showed a negative charge with an average zeta potential up to -7.03 ± 0.12 and -10.66 ± 0.61 mV, respectively (Table S1). When the absolute value of zeta potential exceeded 30 mV, the liposomes were regarded as highly stable, whereas zeta potential in the range of 10–20 mV indicated that the liposomes were relatively stable.²⁹ PEGylation was known to facilitate the stability of nanoparticles with the low zeta potential.²⁶ Therefore, Lipo-Ir can also exhibit excellent stability in the condition of low zeta potential. In addition, the EE (%) and DL (%) of Lipo-Ir were 94.71 and 4.71%, respectively (Table S1). High EE elucidates that almost all of the Ir can be encapsulated into the liposomes.

Physical stability of liposomes

During storage, the unstable liposomes tend to aggregate or fuse and then cause size enlargement. Therefore, particle size is an important item to monitor the physical stability of liposomes. When liposomes agglutinate, the particle size of liposome will increase. Also, the decrease in EE will follow the instability of liposomes. As displayed in Table S2, Lipo-Ir possesses high stability in low temperature and no significant changes in particle size and EE are observed in 2 months, which reveals that Lipo-Ir can keep the high physical stability.

In vitro drug release

The release profile of Lipo-Ir and Ir was studied using the dialysis technique. Lipo-Ir (Figure S2A) displayed a slow

diffusion rate across the dialysis bag, and the release percentage of Lipo-Ir was only $0.80\pm 0.09\%$, $14.25\pm 3.09\%$, and $47.17\pm 1.90\%$ at 0.5, 24, and 96 h, respectively. Obviously, no burst release was observed during the first 30 min. However, the free Ir approximately released $12.11\pm 6.53\%$, $47.06\pm 5.02\%$, and $91.75\pm 4.51\%$ at 0.5, 24, and 96 h, respectively (Figure S2B). Considering the released result, the Lipo-Ir shows significantly sustained release compared with free Ir group. Ir slowly releases from Lipo-Ir, which may be the result of lipid bilayer-induced blockage. Liposomal technology can ameliorate the release profile and circumvent the side effect induced by the irregular drug release.

Hemolysis test

The first prerequisite for pharmaceuticals used for application in vivo is their adequate biocompatibility. Therefore, it is necessary to assess the biocompatibility of formulation for intravenous administration. In this study, we investigated whether or not the Lipo-Ir and Ir result in the rupture of RBCs by hemolysis assay. The hemolytic ratio caused by Ir is $>5\%$, which is identified as having a risk of hemolysis (Figure S3A).²³ However, Lipo-Ir does not show any hemolysis when the concentration of Ir reaches $93.75\ \mu\text{g/mL}$, which indicates that Lipo-Ir has a good hemocompatibility and is suitable for potential clinical applications (Figure S3B). The Lipo-Ir, as a drug delivery system, does show much less hemolytic activity than the free Ir complex, which is definitely an advantage of the liposome encapsulation approach.

Cytotoxic activity in vitro

MTT assay was performed to evaluate the biocompatibility of Blank-Lipo and the in vitro anticancer activity of Lipo-Ir and Ir. As depicted in Figure S4A, when the concentration of empty liposomes reached $214.50\ \mu\text{g/mL}$ (equivalent to Lipo-Ir containing $15\ \mu\text{M}$ Ir), significant cytotoxicity was not observed in A549 cells when incubated for 24 or 48 h (cell viability $>95\%$). The data suggest that the Lipo-Ir can be used for in vivo applications because of their good biocompatibility,³⁰ whereas the free Ir and Lipo-Ir show high cytotoxicity against A549 cells in a dose- and time-dependent manner. The half maximal inhibitory concentration (IC_{50}) of free Ir was 4.92 ± 0.22 and $3.59\pm 0.21\ \mu\text{M}$ at 24 and 48 h, respectively (Figure S4B and C and Table 1). Lipo-Ir also exhibited a strong cytotoxicity to A549 cells with the IC_{50} of 6.55 ± 0.32 and $3.70\pm 0.07\ \mu\text{M}$ at 24 and 48 h, respectively. The results suggest that Lipo-Ir can retain the antitumor activity of Ir. In addition, the phenomenon that the free Ir displays stronger cytotoxicity than Lipo-Ir during 48 h may be caused by sustained release of Lipo-Ir.

Table 1 IC_{50} values of Ir and Lipo-Ir formulation toward A549 cell

| Treatment group | IC_{50} (μM) at 24 h | IC_{50} (μM) at 48 h |
|-----------------|-------------------------------------|-------------------------------------|
| Free Ir | 4.92 ± 0.22 | 3.59 ± 0.21 |
| Lipo-Ir | $6.55\pm 0.32^*$ | 3.70 ± 0.07 |

Notes: Results are presented as the mean \pm SD of triplicates. $*P<0.05$ compared with free Ir.

Abbreviations: IC_{50} , half maximal inhibitory concentration; Ir, iridium; Lipo-Ir, Ir-loaded PEGylated liposomes; PEG, polyethylene glycol.

Apoptosis assay by AO/EB and Hoechst 33342 staining methods

To investigate the apoptotic effect induced by Ir and Lipo-Ir on A549 cells, the morphological changes in A549 cells were examined using Hoechst 33342 staining method and acridine orange/ethidium bromide (AO/EB) double staining technique. Compared to untreated cells, some typical apoptosis changes such as crenation, chromosome aggregation, apoptotic body, and fragmentation in chromatin morphology were observed in Ir and Lipo-Ir treatment groups (Figure 1A). In addition, AO/EB staining was used to characterize cell apoptosis induced by Ir and Lipo-Ir. As demonstrated in Figure 1B, living cells appeared as weak green fluorescing nuclei and no significant apoptosis was detected in the control group. After treating with Ir and Lipo-Ir, the apoptotic cells showed bright green fluorescing nuclei, chromatin condensation, and nuclear shrinkage. In addition, the necrotic cells appearing with red fluorescence were found. All these morphological changes indicate that Lipo-Ir can effectively induce similar apoptosis in A549 cells.

Cellular uptake

Cellular uptake was investigated using IXM under the microscope after treatment with $8\ \mu\text{M}$ of Ir and Lipo-Ir for 0.5 or 2 h. Hoechst 33342 was also used to stain the cellular nuclei. As shown in Figure 2, in Ir-treated group, green fluorescence points were detected in the cellular cytoplasm, whereas a slightly weaker signal was recorded in the Lipo-Ir treatment group. With increasing time, bright green fluorescent points are observed, which indicate the cellular uptake increases in a time-dependent manner. These findings suggest that free Ir can be rapidly taken into cytoplasm during 30 min, while the transport rate of Lipo-Ir into cells is slower than that of Ir. This may explain why the cytotoxicity induced by Ir is stronger than that induced by Lipo-Ir.

Assay of location and the changes of MMP

Mitochondria are potentially important therapeutic target.³¹ Lipophilic cations could be developed to target drugs to mitochondria in vivo.^{32,33} To further investigate the intracellular localization of free Ir and Lipo-Ir in the

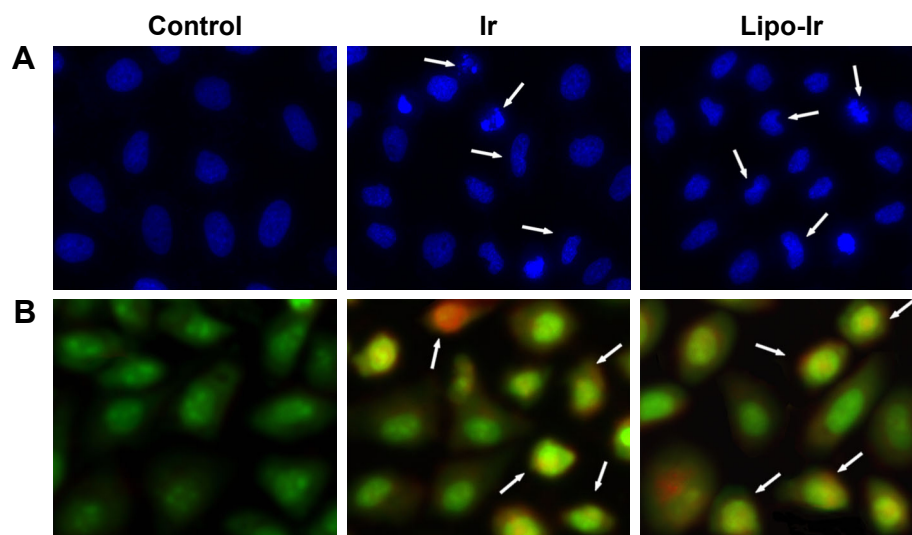


Figure 1 The morphology of apoptosis in A549 cells stained with Hoechst 33342 (A) and AO/EB (B) after treating with 3 μ M Ir and equivalent Lipo-Ir for 24 h. **Notes:** The photographs were imaged using 40 \times objectives with DAPI (blue) or FITC (green) and Texas Red (red) filters. Arrows show the apoptotic body, chromosome aggregation, or apoptotic cells.

Abbreviations: Ir, iridium; Lipo-Ir, Ir-loaded PEGylated liposomes; PEG, polyethylene glycol; AO/EB, acridine orange/ethidium bromide.

mitochondria, MitoTracker[®] Deep Red FM was used as red fluorescent probe. As shown in Figure 3, the mitochondria were stained red, and after treatment of the cells with Ir or Lipo-Ir for 30 min, 2 h, or 12 h, the Ir and Lipo-Ir emitted

green fluorescence. The merge of the red and the green fluorescence indicates that Ir and Lipo-Ir can enter into the mitochondria. The effect of Ir and Lipo-Ir on the changes of MMP ($\Delta\Psi_m$) was also investigated using JC-1 as fluorescent

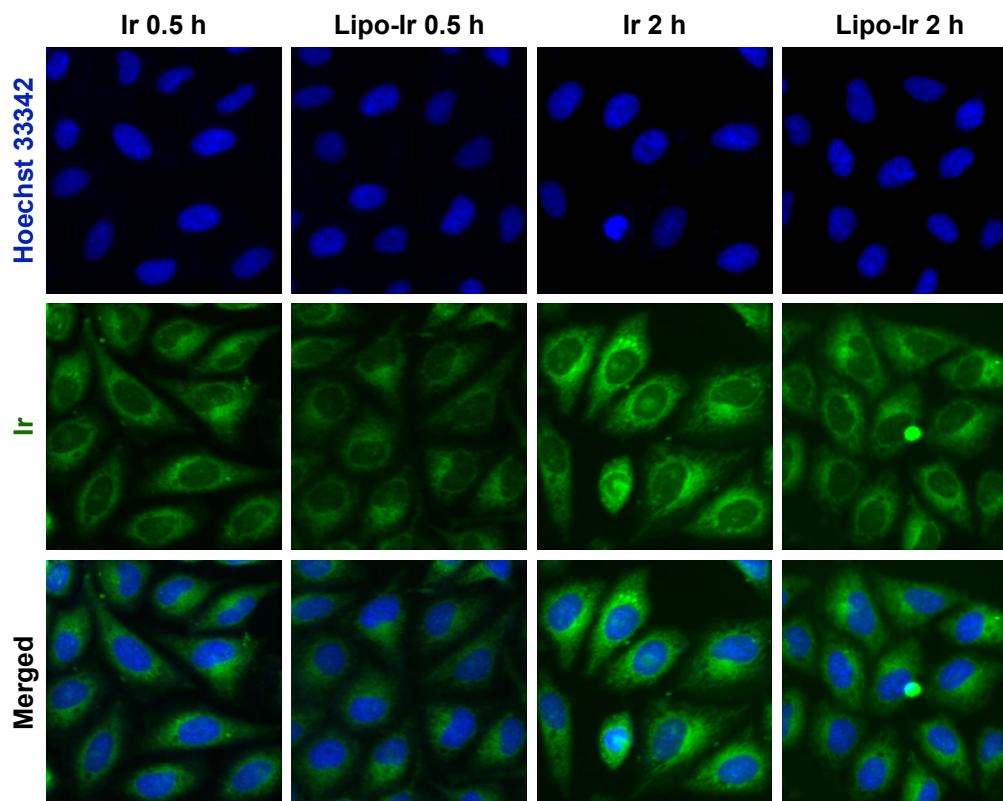


Figure 2 Cellular uptake of Ir and Lipo-Ir into A549 cells after treatment with 8 μ M Ir and equivalent Lipo-Ir (green) for 0.5 or 2 h.

Note: Hoechst 33342 (blue) was also used to identify the cellular nuclei.

Abbreviations: Ir, iridium; Lipo-Ir, Ir-loaded PEGylated liposomes; PEG, polyethylene glycol.

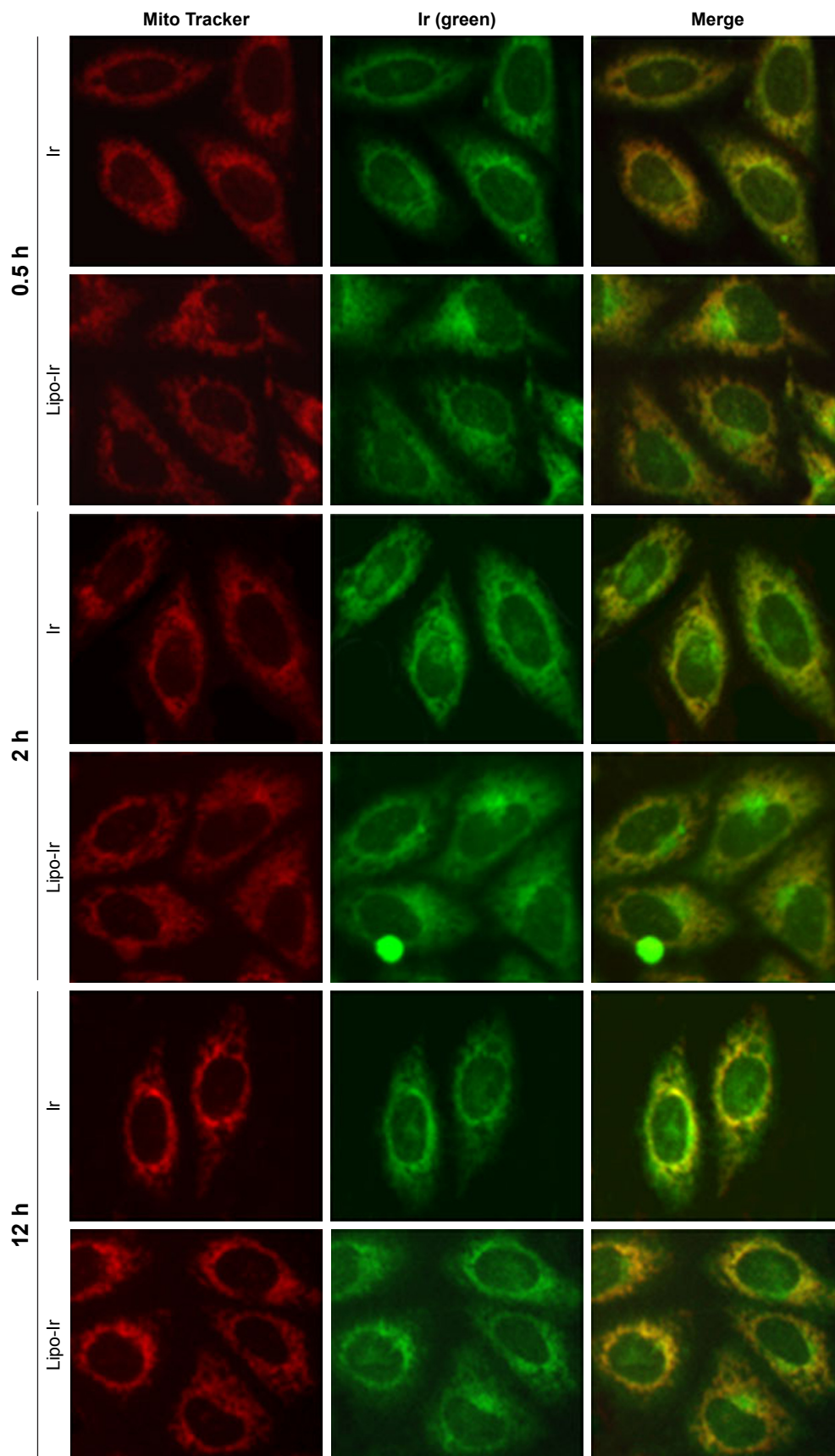


Figure 3 Assay of Ir and Lipo-Ir at the location of mitochondria.

Abbreviations: Ir, iridium; Lipo-Ir, Ir-loaded PEGylated liposomes; PEG, polyethylene glycol.

probe. At high MMP, JC-1 forms an aggregation and emits red fluorescence; at low MMP, JC-1, existing as a monomer, emits green fluorescence.³⁴ As shown in Figure 4A, in the control, JC-1 emits red fluorescence. After A549 cells were exposed to 3 μ M of Ir and Lipo-Ir or CCCP (positive control) for 24 h, JC-1 emits green fluorescence with little red fluorescence. The shift from red to green fluorescence shows that Ir and Lipo-Ir can result in dissipation of the MMP. To further compare the effect induced by Ir and Lipo-Ir on the changes in MMP, the ratio of red/green fluorescence was determined by the MateXpress6 software. As exhibited in Figure 4B, in the control, the ratio of red/green fluorescence was 1.72 ± 0.16 . After treating with Ir (3 μ M) and Lipo-Ir (3 μ M) for 24 h, the ratios of red/green fluorescence were 0.69 ± 0.06 and 1.08 ± 0.21 , respectively. The results demonstrate that Ir and Lipo-Ir can enter into the mitochondria and trigger collapse in the MMP.

ROS detection

Excess intracellular ROS is a potential element to destroy nucleic acid, lipid membranes, and organelles, which can activate apoptosis in cancer cells.³⁵ The intracellular ROS levels were assayed by using DCFH-DA as fluorescent

probe. It is well known that DCFH-DA can be converted into DCFH by intracellular esterase and DCFH can be oxidized by intracellular ROS to form a fluorescent DCF.³⁶ As shown in Figure 5A, in the control, weak green fluorescence was observed. After being treated with 3 μ M of Ir or Lipo-Ir for 24 h, a number of bright green fluorescence points were found. These findings suggest that Ir or Lipo-Ir enhances intracellular ROS levels. Additionally, the DCF fluorescent intensity was also determined by the MeteXpress6 software. As shown in Figure 5B, when A549 cells were treated with 3 μ M of Ir or Lipo-Ir for 24 h, the cellular fluorescence intensities of DCF increased ~ 2.79 and 2.27 times than that in the control, respectively. The result exhibits that the intracellular ROS levels are significantly elevated by Ir and Lipo-Ir.

Intracellular Ca²⁺ measurement

Cellular Ca²⁺ overload is recognized as a cause of cytotoxicity and often plays a prominent role in Ca²⁺-dependent effectors such as the process of necrotic, apoptotic, and autophagic cell death.^{37,38} To monitor the changes in intracellular calcium, Fluo-3 AM was used as fluorescent probe. As shown in Figure 6A, a significant increase in the fluorescent intensity of Fluo-3 in A549 cells was observed after A549 cells were

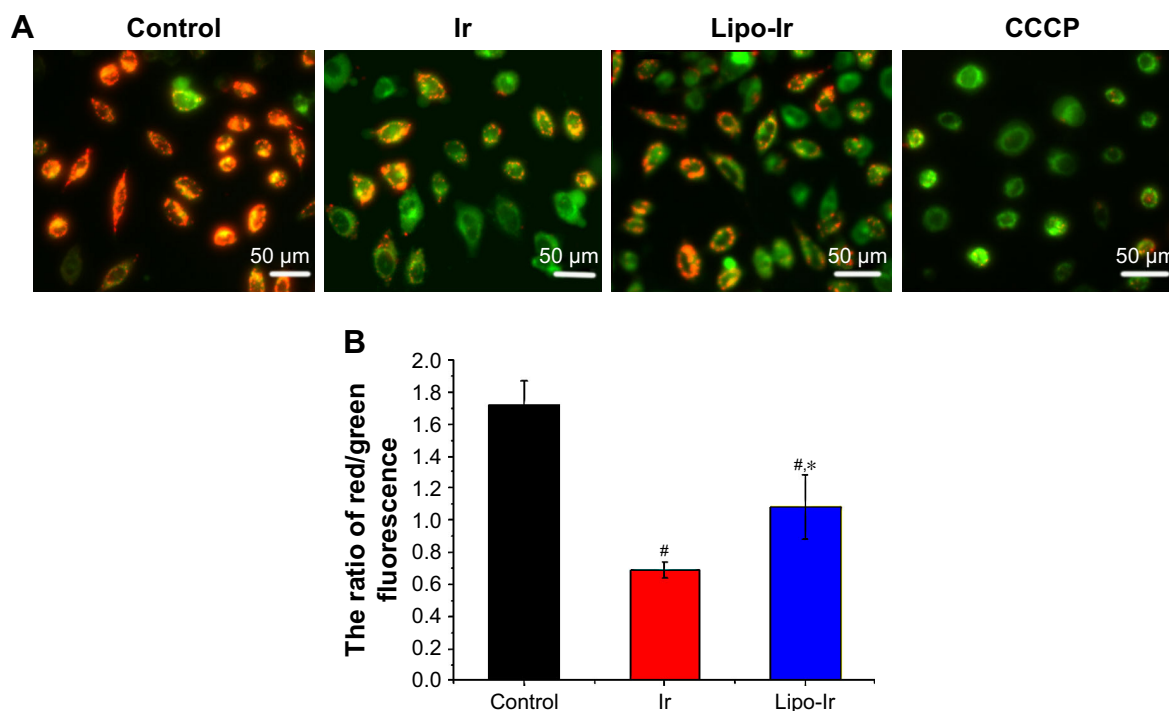


Figure 4 Assay of A549 cells mitochondrial membrane potential with JC-1 staining method.

Notes: (A) The depolarization of mitochondrial membrane potential was observed (the magnification for the figure is 200 \times) after the cells were exposed to Ir (3 μ M), equivalent Lipo-Ir for 24 h, or CCCP (as positive control). (B) Quantitative analysis of ratio of red/green fluorescent intensity. Results of the red and green fluorescence are overlapped and expressed as mean \pm SD of triplicates. The Lipo-Ir-treated group exhibits significant difference compared with the Ir (* $P < 0.05$). The significant difference is observed among the treatment group and the blank control group (** $P < 0.05$).

Abbreviations: Ir, iridium; Lipo-Ir, Ir-loaded PEGylated liposomes; JC-1, 5,5',6,6'-tetrachloro-1,1',3,3'-tetraethylbenzimidazolcarbocyanine iodide; PEG, polyethylene glycol.

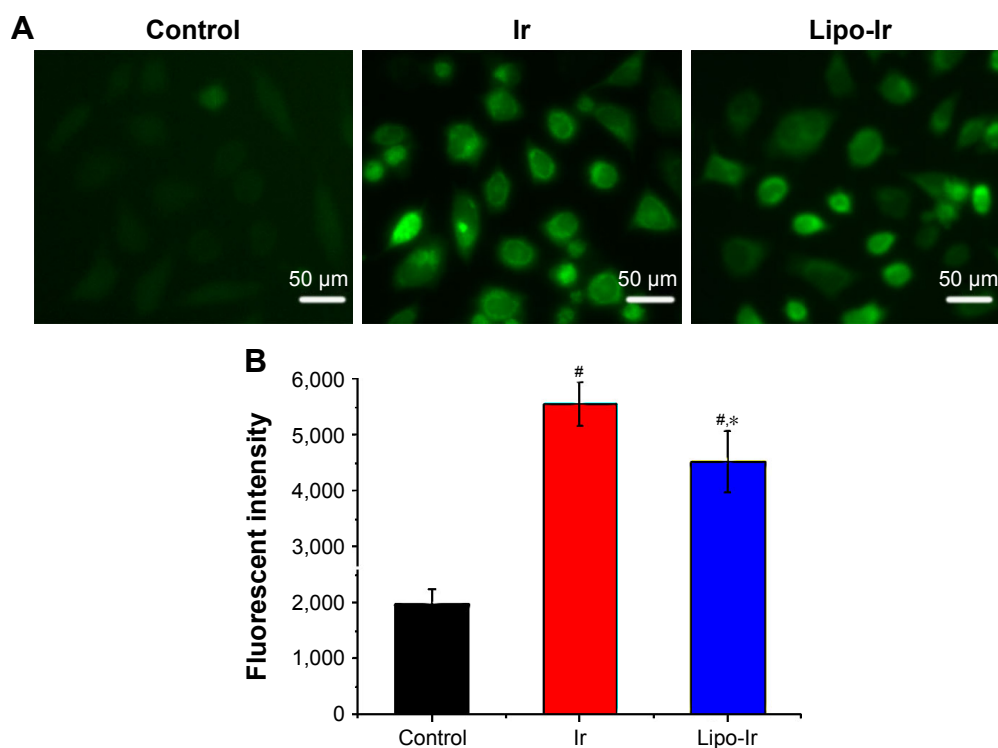


Figure 5 Analysis of the ROS level in A549 cells (n=3).

Notes: (A) ROS generation in the cells exposed to Ir (3 μM) and Lipo-Ir (μM Ir-equivalent) for 24 h; results are representative of 30 randomly captured images (the magnification for the figure is 200×). (B) Quantitative analysis of the DCF fluorescent intensity in A549 cells. Results are presented as mean ± SD. **P*<0.05 versus Ir; #*P*<0.05 versus the blank control.

Abbreviations: DCF, dichlorofluorescein; Ir, iridium; Lipo-Ir, Ir-loaded PEGylated liposomes; PEG, polyethylene glycol; ROS, reactive oxygen species.

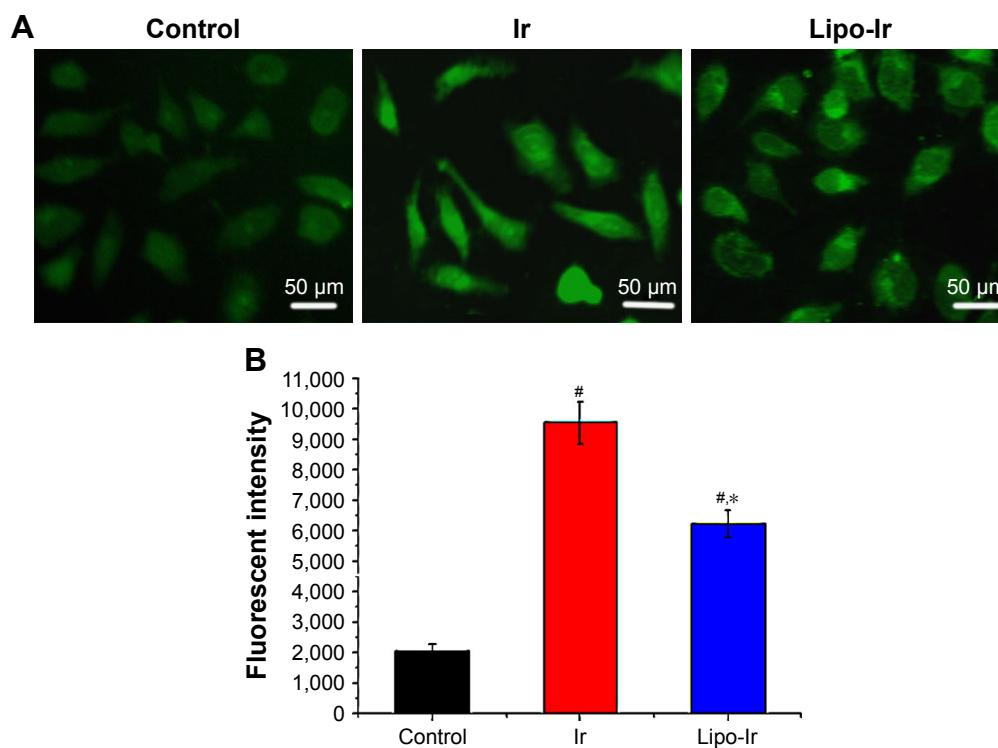


Figure 6 Determination of the levels of Ca²⁺ in A549 cells using Fluo-3 AM as fluorescent probe.

Notes: (A) The Ca²⁺ was monitored after being treated with 3 μM Ir and equivalent Lipo-Ir for 24 h. The magnification for the figure is 200×. (B) Quantitative results of the fluorescent intensity of Fluo-3. Results are displayed as mean ± SD (n=3). **P*<0.05 compared with Ir. #*P*<0.05 compared with the blank control.

Abbreviations: Ir, iridium; Lipo-Ir, Ir-loaded PEGylated liposomes; PEG, polyethylene glycol.

exposed to 3 μM Ir and equivalent Lipo-Ir for 24 h. The fluorescence intensity of Fluo-3 increased 4.5 times for Ir and 3.0 times for Lipo-Ir than that of control (Figure 6B). This result demonstrates that Ir and Lipo-Ir can enhance intracellular Ca^{2+} levels, which will lead to mitochondrial dysfunction and promote apoptosis.³⁹

Cell cycle arrest by flow cytometry

The apoptosis of tumor cells is associated with cell cycle perturbation.⁴⁰ To study the effects of Ir and Lipo-Ir on the blockage of cell cycle, the cell cycle arrest assay was performed by flow cytometry. As shown in Figure S5, in the control, the percentage at G₀/G₁ phase was 41.96. After the treatment of A549 cells with 3 μM of Ir or Lipo-Ir for 24 h, the percentage at G₀/G₁ phase was 50.72 and 49.51, respectively. An increase of 8.76% for Ir and 7.55% for Lipo-Ir was observed. In addition, an increase of 14.31% for Ir and 11.43% for Lipo-Ir was found after A549 cells were treated with 5 μM of Ir or Lipo-Ir for 24 h, which was accompanied by a reduction in the percentage of the cells at S phase. These data indicate that Ir and Lipo-Ir inhibit the cell growth at G₀/G₁ phase.

Conclusion

In the present work, we have successfully encapsulated Ir into PEGylated liposomes with high EE of 94.71%. The prepared Lipo-Ir has small size (112.57 \pm 1.15 nm) and spherical shape without any aggregation. Moreover, Lipo-Ir displays a good performance of physical stability, biocompatibility, and sustained effect. In the test, the hemolysis rate is <5% in the RBCs treated with 93.75 $\mu\text{g}/\text{mL}$ Lipo-Ir. However, when treated with Ir under the same concentration, it reaches up to 50%. Additionally, the accumulative release for 96 h in the Lipo-Ir treatment group and the Ir-treated group is 47.17% and 91.75%, respectively. The aforementioned results suggest that the Lipo-Ir is suitable for intravenous administration. Furthermore, Lipo-Ir can maintain the remarkable anticancer activity induced by the free Ir. In the assay of MMP, ROS, and intracellular Ca^{2+} , Lipo-Ir induces a 1.6-fold decrease in MMP, a 2.27-fold increase in the ROS levels, and a 3.0-fold increase in intracellular calcium compared with the blank control group, which further promotes cell apoptosis. Moreover, Lipo-Ir has the blockage efficacy in G₀/G₁ phase of cell cycle. In conclusion, Lipo-Ir induces apoptosis in A549 cells through the ROS-mediated mitochondrial dysfunction pathway and Lipo-Ir will be a promising approach for effective tumor therapy.

Acknowledgment

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Disclosure

The authors report no conflicts of interest in this work.

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Supplementary materials

Materials and methods

Materials

Tween-80 was obtained from Aladdin (Pharmaceutical grade; Shanghai, China). Acridine orange (AO), ethidium bromide (EB), propidium iodide (PI), RNase A, and vitamin E were obtained from Sigma-Aldrich Co. (St Louis, MO, USA). 3-(4,5-Dimethylthiazole)-2,5-diphenyltetrazolium bromide (MTT), 5,5',6,6'-tetrachloro-1,1',3,3'-tetraethylbenzimidazol carbocyanine iodide (JC-1), 2',7'-dichlorodihydrofluorescein diacetate (DCFH-DA), Fluo-3 AM, and Hoechst 33342 were purchased from Shanghai Beyotime Institute of Biotechnology (Shanghai, China). One percentage penicillin–streptomycin and MitoTracker[®] Deep Red FM were obtained from Thermo Fisher Scientific (Waltham, MA, USA). All other reagents were analytical or chromatographic grade.

RE-SZAA rotary vacuum evaporator (Shanghai YaRong Biochemical Instrument Factory, Shanghai, China), Scientz-IID

cell sonicator (Ningbo Scientz Biotechnology Co., Ltd., Ningbo, Zhejiang, China), Optima L-100XP Preparative ultracentrifuge (Beckman Coulter, Brea, CA, USA), Hitachi H-7650 transmission electron microscopy (TEM; Hitachi Ltd. Tokyo, Japan), ImageXpress[®] High Content Screening System (IXM; Molecular Devices LLC, Sunnyvale, CA, USA), FACS Calibur flow cytometer (Beckman Dickinson, Franklin Lakes, NJ, USA), and cell culture plates (Corning; Corning Incorporated, Corning, NY, USA) were used.

HPLC analysis

Iridium (Ir) was determined using a HPLC system (1200 LC; Agilent Technologies, Santa Clara, CA, USA). The samples were analyzed using a C₁₈ column (5 μm, 4.6×250 mm, Diamonsil). The mobile phase was acetonitrile and 0.02 M sodium acetate buffer containing 0.06 M NaClO₄ (final pH 4.65) (70:30, v/v). The flow rate, injection volume, and detection wavelength were set as 1.0 mL/min, 20 μL, and 260 nm, respectively.

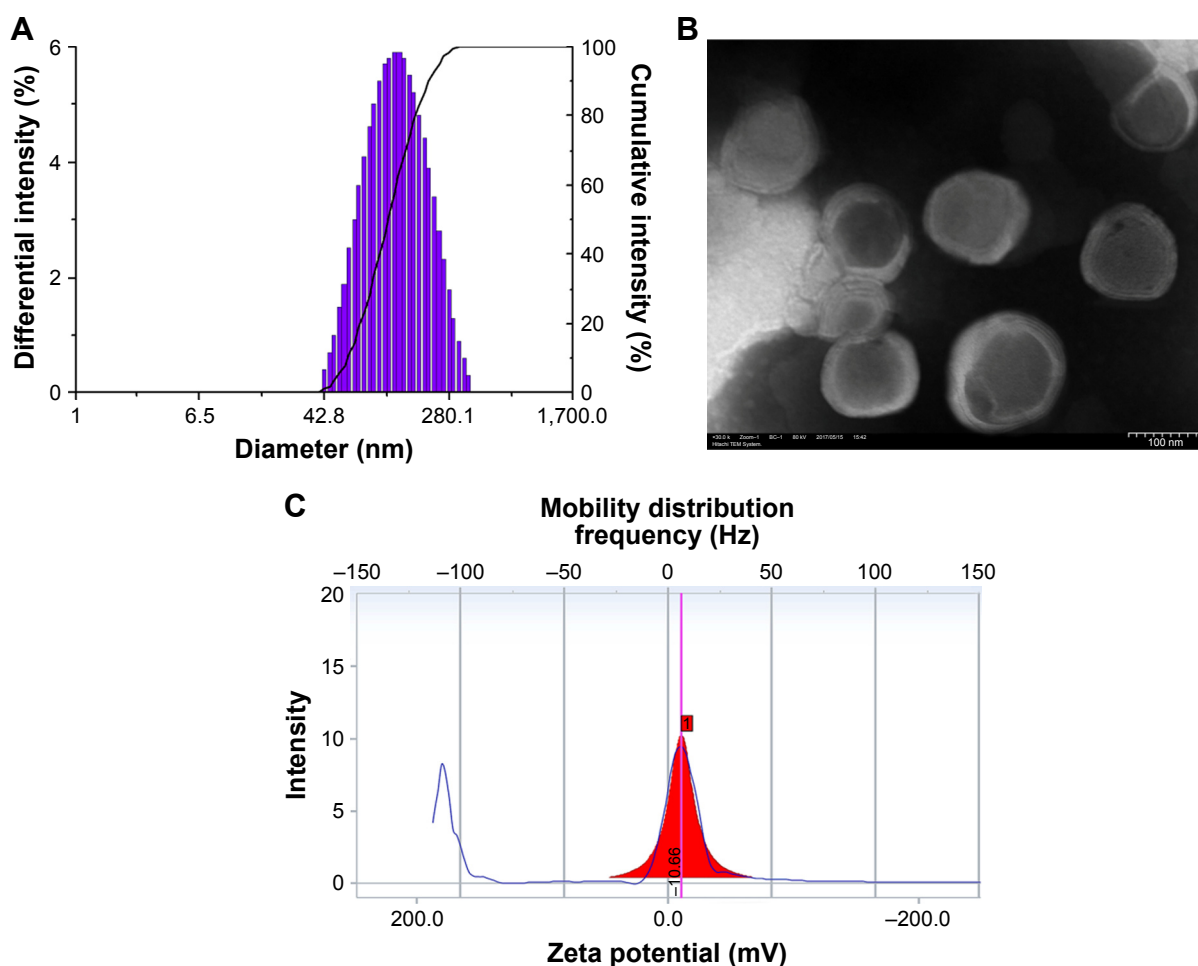


Figure S1 Characterization of Lipo-Ir.

Notes: (A) Size distribution, (B) TEM image, and (C) zeta potential.

Abbreviations: Ir, iridium; Lipo-Ir, Ir-loaded PEGylated liposomes; PEG, polyethylene glycol; TEM, transmission electron microscopy.

Table S1 Characterization parameters of liposomes (n=3)

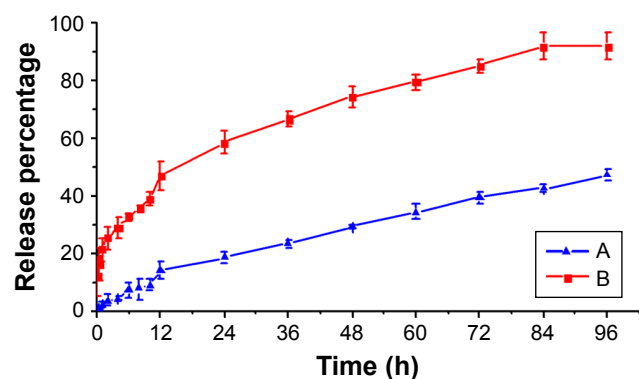
| Liposomes | Size (nm) | PDI | Zeta potential (mV) | EE (%) | DL (%) |
|------------|-------------|-----------|---------------------|------------|-----------|
| Blank-Lipo | 92.80±3.08 | 0.13±0.03 | -7.03±0.12 | - | - |
| Lipo-Ir | 116.57±1.15 | 0.19±0.02 | -10.66±0.61 | 94.71±3.21 | 4.71±0.41 |

Abbreviations: Blank-Lipo, blank PEGylated liposomes; DL, drug loading; EE, encapsulation efficiency; Ir, iridium; Lipo-Ir, Ir-loaded PEGylated liposomes; PDI, polydispersity index; PEG, polyethylene glycol.

Table S2 Physical stability of Lipo-Ir (n=3)

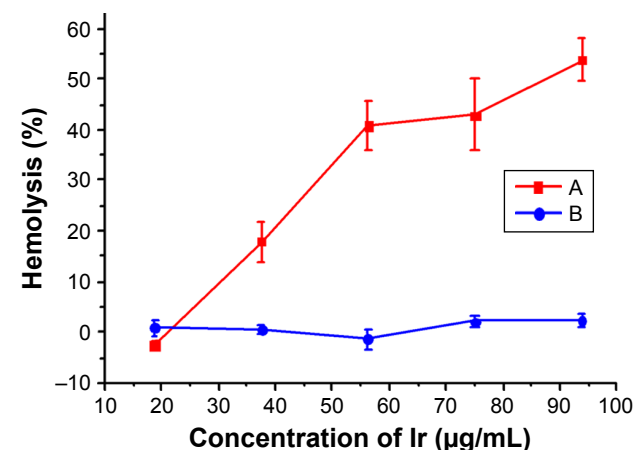
| Time (days) | Size (nm) | EE (%) |
|-------------|-------------|------------|
| 0 | 116.57±1.15 | 94.71±3.21 |
| 15 | 117.60±1.59 | 94.01±4.20 |
| 30 | 118.75±2.12 | 95.24±3.95 |
| 60 | 118.92±4.14 | 94.93±4.98 |

Abbreviations: EE, encapsulation efficiency; Ir, iridium; Lipo-Ir, Ir-loaded PEGylated liposomes; PEG, polyethylene glycol.

**Figure S2** In vitro release profiles of Ir from Lipo-Ir (A) and Ir (B).

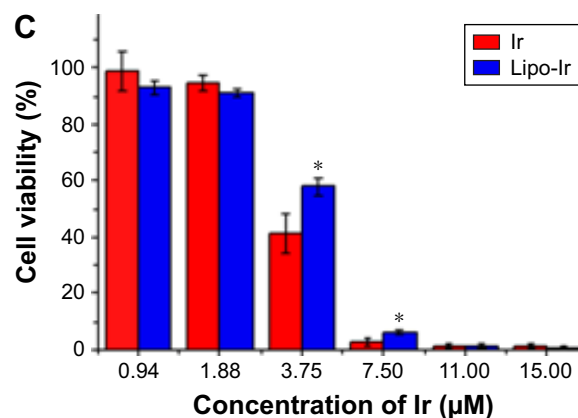
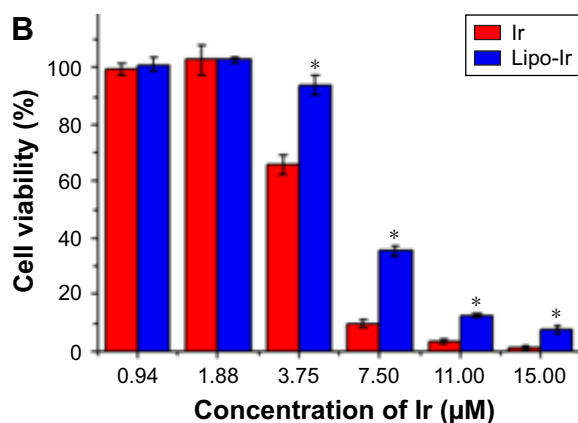
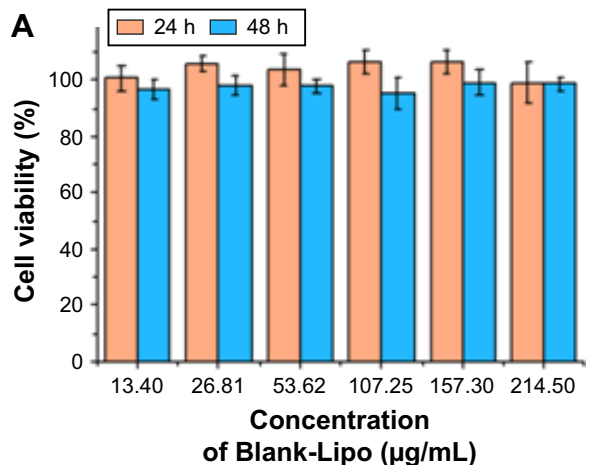
Note: Bars represent \pm SD (n=3).

Abbreviations: Ir, iridium; Lipo-Ir, Ir-loaded PEGylated liposomes; PEG, polyethylene glycol.

**Figure S3** Hemolysis percentages of Ir (A) and Lipo-Ir (B).

Note: Bars represent \pm SD (n=3).

Abbreviations: Ir, iridium; Lipo-Ir, Ir-loaded PEGylated liposomes; PEG, polyethylene glycol.

**Figure S4** Evaluation of cell viability (MTT).

Notes: (A) Viability of A549 cells incubated with various concentrations of Blank-Lipo for 24 and 48 h. Viability of A549 cells incubated with various concentrations of Ir or Lipo-Ir for 24 h (B) or 48 h (C). Results are presented as the mean \pm SD of triplicates. * P <0.05 compared with Ir.

Abbreviations: Blank-Lipo, blank PEGylated liposomes; Ir, iridium; Lipo-Ir, Ir-loaded PEGylated liposomes; MTT, 3-(4,5-dimethylthiazole)-2,5-diphenyltetrazolium bromide; PEG, polyethylene glycol.

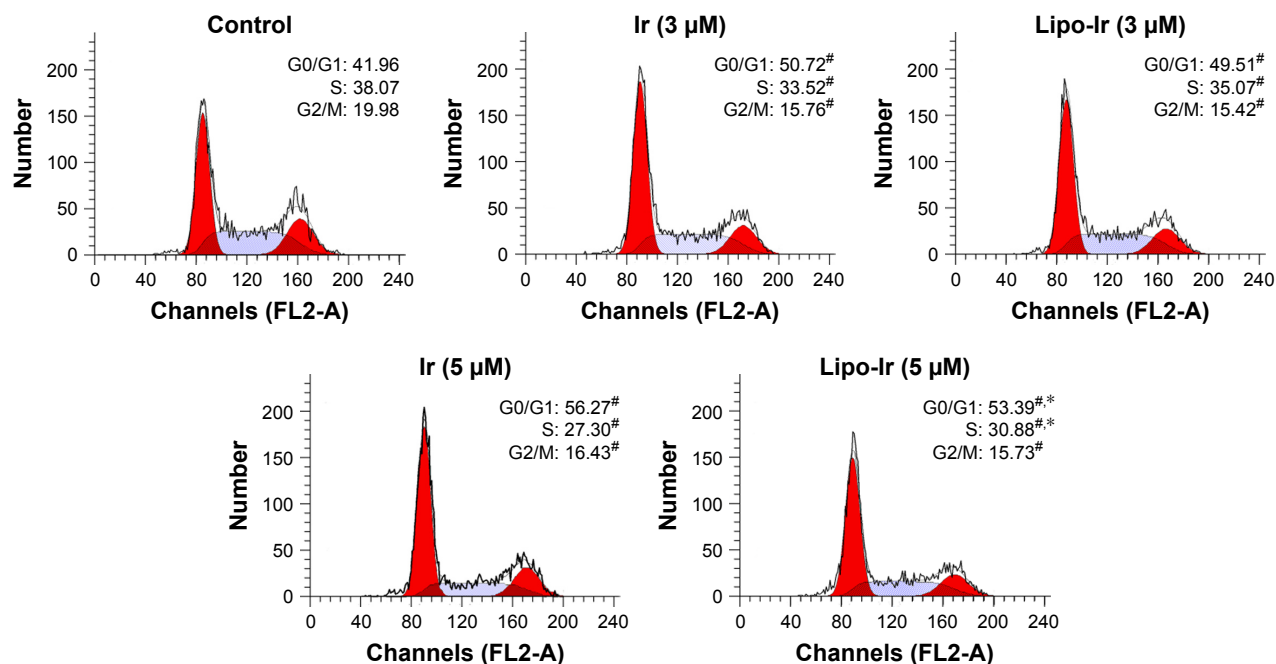


Figure S5 Cell cycle profiles in A549 cells were determined by flow cytometry after incubating with Ir (3 or 5 μM) and equivalent Lipo-Ir for 24 h.

Notes: * $P < 0.05$ compared with Ir (between same concentrations). [#] $P < 0.05$ compared with control.

Abbreviations: Ir, iridium; Lipo-Ir, Ir-loaded PEGylated liposomes; PEG, polyethylene glycol.

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