

Since January 2020 Elsevier has created a COVID-19 resource centre with free information in English and Mandarin on the novel coronavirus COVID-19. The COVID-19 resource centre is hosted on Elsevier Connect, the company's public news and information website.

Elsevier hereby grants permission to make all its COVID-19-related research that is available on the COVID-19 resource centre - including this research content - immediately available in PubMed Central and other publicly funded repositories, such as the WHO COVID database with rights for unrestricted research re-use and analyses in any form or by any means with acknowledgement of the original source. These permissions are granted for free by Elsevier for as long as the COVID-19 resource centre remains active. Contents lists available at ScienceDirect

Talanta

journal homepage: www.elsevier.com/locate/talanta

Review Current methods and prospects of coronavirus detection

Jiaqi Bu, Zhiwei Deng, Hui Liu, Jiacheng Li, De Wang, Yanjing Yang^{*}, Shian Zhong^{**}

College of Chemistry and Chemical Engineering, Central South University, Changsha, 410083, PR China

ARTICLE INFO

Keywords: Coronavirus SARS-COV-2 Detection SM-MIT

ABSTRACT

SARS-COV-2 is a novel coronavirus discovered in Wuhan in December 30, 2019, and is a family of SARS-COV (severe acute respiratory syndrome coronavirus), that is, coronavirus family. After infection with SARS-COV-2, patients often experience fever, cough, gas prostration, dyspnea and other symptoms, which can lead to severe acute respiratory syndrome (SARS), kidney failure and even death. The SARS-COV-2 virus is particularly infectious and has led to a global infection crisis, with an explosion in the number of infections. Therefore, rapid and accurate detection of the virus plays a vital role. At present, many detection methods are limited in their wide application due to their defects such as high preparation cost, poor stability and complex operation process. Moreover, some methods need to be operated by professional medical staff, which can easily lead to infection. In order to overcome these problems, a Surface molecular imprinting technology (SM-MIT) is proposed for the first time to detect SARS-COV-2 virus. For this SM-MIT method, this review provides detailed detection principles and steps. In addition, this method not only has the advantages of low cost, high stability and good specificity, but also can detect whether it is infected at designated points. Therefore, we think SM-MIT may have great potential in the detection of SARS-COV-2 virus.

1. Introduction

In December 2019, patients with pneumonia of unknown cause appeared in some medical institutions in Wuhan, Hubei Province, China [1-3]. Wuhan continued to carry out surveillance of influenza and related diseases, and 27 cases of viral pneumonia were found, all diagnosed as viral pneumonia/pulmonary infection. Until January 2020, the World Health Organization officially named it 2019-nCOV [4-6]. Subsequently, the International Committee on Virus Taxonomy announced on its official website that the novel Coronavirus had the English name "SARS-COV-2" [7,8]. To date (October 26, 2020), there have been 35, 347,404 confirmed human cases of SARS-COV-2 worldwide, including 1039,406 deaths (https://www.who.int/home) [9]. The symptoms of SARS-COV-2 virus infection are as follows: Asymptomatic period, the virus was detected only in respiratory tract, but no obvious symptoms. Mild patients are also in the incubation period, patients may have symptoms similar to cold, including fever, cough, fear of cold, physical discomfort and so on. Severe patients, patients will soon develop pneumonia, and appear rapid breathing, respiratory failure, multiple organ damage and so on [10-13].

SARS-COV-2 virus belongs to beta-COV lineage B, which is a group of

enveloped single stranded RNA viruses. It is characterized by prominent stick like protrusions on the surface of the virus and abnormally large RNA genome. SARS-COV-2 genome encodes four major structural proteins: spike (s) protein, Nucleocapsid (n) protein, membrane (m) protein and envelope (E) protein, which are essential components of virus particles [14,15]. The onset time of SARS-COV-2 patients was different, which was related to the severity and incubation period of infection. The incubation period of general patients is 1-14 days. For patients with mild infection, it may take 1-2 weeks to develop the disease, and for patients with severe infection, the related clinical symptoms may appear in 2-3 days. But after epidemiological investigation, the patients were infected in 3-7 days [16]. In addition, the SARS-COV-2 virus has demonstrated the possibility of human to human transmission [17] and has found that it can be transmitted through airborne droplets and close contact with patients [18-20]. Like all coronaviruses, SARS-COV-2 uses S-glycoprotein to promote its entry into host cells. The protein has two functional domains: one is S1 receptor binding domain (RBD), the other is S2 domain which mediates the fusion of virus and host cell membrane. SARS-COV-2 protein first binds to ACE2 receptor on host cells through S1 receptor binding domain. Then, S1 domain was detached from the surface of the virus, and S2 domain was fused to the host cell membrane.

https://doi.org/10.1016/j.talanta.2020.121977

Received 7 October 2020; Received in revised form 29 November 2020; Accepted 3 December 2020 Available online 31 December 2020 0039-9140/© 2020 Elsevier B.V. All rights reserved.





^{*} Corresponding author. ** Corresponding author.

E-mail addresses: yangyanjing@csu.edu.cn (Y. Yang), zhongshian@aliyun.com (S. Zhong).

Table 1

CT characterization of various viral infections.

| Virus | symptom | CT features | Reference |
|-------------------------------|------------------------------|---|-----------|
| Influenza A (H1N1) virus | Severe headache, fever | Ground-glass opacity and consolidation | [36] |
| SARS-COV-2 virus | Fever, cough, fatigue | Double lung multiple ground glass images and infiltrating shadows | [37] |
| Avian Influenza H7N9 virus | Fever, cough, sputum | Ground-glass opacity and consolidation | [38] |
| Cytomegalovirus | Fever, cough, dyspnea | Ground glass attenuation, bronchial consolidation and thickening | [39] |
| MERS CoV virus | Fever, cough, dyspnea | Ground glass attenuation, bronchial consolidation and thickening | [40] |

This process requires activation of S protein, which is achieved by cleavage of furin and TMPRSS2 at two sites (S1/S2 and S2 '). Furin cleavage at S1/S2 site can lead to conformational changes of virus S protein, thus exposing RBD or S2 domains. The researchers believe that the TMPRSS2 cleavage of SARS-COV-2 protein can promote the fusion of virus capsid and host cells, thus allowing the virus to enter [21-23]. Due to the rapid growth of the number of people infected with SARS-COV-2 virus, the pressure of detecting SARS-COV-2 is very great [24-26]. Many people die at home because they can't get timely detection. With the development of the epidemic, the global economy will fall into a serious recession. According to the International Monetary Fund, the global economic recession in 2020 will be more severe than the global financial crisis in 2008. Deutsche Bank, on the other hand, said GDP in the US and Europe could fall by 15.0-30.0% in the second quarter of 2020. At present, the epidemic has led to the sudden stagnation of economic activities in most countries, resulting in the contraction of the global supply chain. Therefore, controlling the epidemic has become the responsibility of people all over the world. The first step in controlling the disease is testing for SARS-COV-2. However, a simple, efficient and short-time detection method has become an important task [27–29]. At present, there are many methods to detect SARS-COV-2. For example: Computed tomography scan, Haematological detection, Polymer chain reaction, Loop mediated isothermal amplification, SHERLOCK technology, Microarray-based methods, Enzyme-linked immunosorbent assay, Electrochemical method and Immunoassay technology, etc. [30-32]. These methods have their own advantages and disadvantages. In this review, a Surface molecular imprinting technology (SM-MIT) for the detection of SARS-COV-2 virus was proposed for the first time, and its steps and mechanism were mentioned in this paper.

2. Detection method

2.1. Simple detection

The simplest way to detect SARS-COV-2 infection is to observe the physiological characteristics. Fever, dry cough and fatigue were the main manifestations [33,34]. A few patients were accompanied by nasal congestion, runny nose, sore throat, myalgia and diarrhea. Severe patients had dyspnea and hypoxemia. Severe cases can rapidly progress to acute respiratory distress syndrome, septic shock, metabolic acidosis, coagulation dysfunction and multiple organ failure [35]. However, these symptoms may also be caused by other viruses or causes, so the accuracy of this method is very poor, which is only suitable for the preliminary work of screening a large number of patients.

2.2. Computed tomography scan (CT-scan)

CT-scan has the characteristics of fast scanning time and clear image, which can be used for the examination of various diseases (See Table 1).

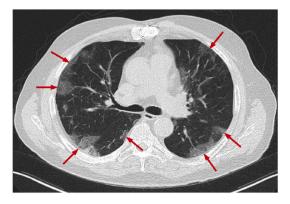


Fig. 1. CT-scan of novel coronavirus pneumonia patients.

Table 2

| Serological manifestations of | of various vir | al infections. |
|-------------------------------|----------------|----------------|
|-------------------------------|----------------|----------------|

| Virus | Serological features | Reference |
|------------------------|---|-----------|
| Hepatitis B virus | The mean platelet volume, red blood cell distribution width and the ratio of platelet to lymphocyte are increased, while the ratio of lymphocyte to monocyte is decreased. | [50] |
| SARS-CoV-2 virus | A large number of lymphocytes, CD4 ⁺ T cells and CD8 ⁺ T cells are lost, on the contrary, inflammatory cytokines and D-dimers are increased. | [2,35] |
| Schmallenberg virus | The mid-size white blood cell (mid) and red blood cell count (RBC) are decreased, while the average red blood cell hemoglobin is increased. | [51] |
| Hepatitis E virus | Transaminase and serum bilirubin concentration are significantly increased. | [52] |
| Ebola virus | Haematological abnormalities were common, including raised haematocrit thrombocytopenia, and granulocytosis. | [53] |
| Papillomaviruses | The CD8 + T cells of natural killer cells, IFN- γ and IL-17 are increased, on the contrary, the ratio of $\gamma\delta$ + T cells and CD4+/CD8+ is decreased. | [54] |

CT-scan can be used to detect suspected and confirmed patients with SARS-COV-2 [41-43]. The CT-scan manifestations of novel coronavirus pneumonia showed multiple small patches and interstitial changes at the early stage. The lung was obviously exuded, and gradually developed into double lung multiple ground glass images and infiltrating shadows (see Fig. 1). Severe cases of pulmonary consolidation and pleural effusion were found [44,45]. CT-can cannot completely determine the presence of a novel Coronavirus, as the CT-scan can only determine the clarity of the chest and lungs, and may also be caused by another virus [46]. It can be seen from Table 1 that the representation phenomena of CT-scan diagram are very similar. Ground glass opacity (GGO) usually refers to the high-density area found in the lung parenchyma during fluoroscopy, which is often manifested as a mass or nodule on chest X-ray or CT. However, GGO and consolidation can appear after infection of various viruses. Therefore, this method is only suitable for the preliminary brush selection in the early stage, and other methods need to be combined to determine whether they are infected.

2.3. Haematological detection

Haematological testing has been applied to various virus screening [47–49] (See Table 2). According to the literature, when the absolute lymphocyte count was less than 0.8×10^9 /L or the CD⁴⁺ and CD⁸⁺ T cell count significantly decreased, it suggested that the patient might be infected with SARS-COV-2 virus [35]. In addition, the levels of muscle enzymes, liver enzymes, troponin, myoglobin, erythrocyte sedimentation rate (ESR) and C-reactive protein (CRP) were increased in some patients. In severe cases, the lymphocyte count in the blood decreases

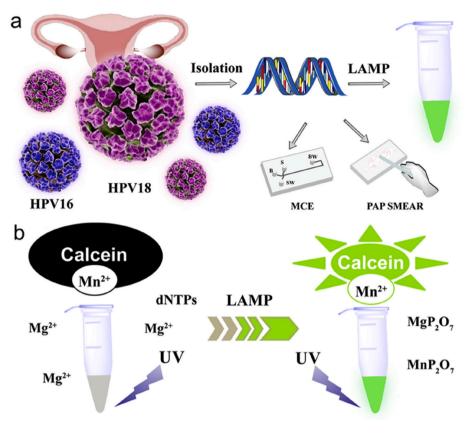


Fig. 2. Working principle of loop-mediated isothermal amplification detection.

gradually. In contrast, inflammatory cytokines and D-dimers were elevated [2]. SARS-COV-2 infection may be considered if prothrombin time is prolonged or aspartate transaminase, creatine kinase, creatinine and lactate dehydrogenase are increased [55,56]. According to reports in the literature, IL1 β , IFN- γ , IP10 and MCP1 are expressed at higher levels in SARS-COV-2 patients. In addition, granulocyte colony stimulating factor (GCSF), IP10, MCP1A, MIP1A and TNF- α are more highly expressed in critically ill patients [57]. The changes of these expression factor also can be triggered by various infectious or non-infectious diseases [58]. Therefore, haematological detection is a good method for virus detection. Then, it can be seen from Table 2 that different viruses will have similar changes in blood factors. For example, the number of lymphocytes and inflammatory cytokines increased, CD4 + T cells decreased. Therefore, haematological detection methods need to be further optimized.

2.4. Polymerase chain reaction (PCR) methods

PCR is an enzyme method with high sensitivity and strong sequence specificity [59–64]. At present, it has become a detection technology of SARS-COV-2 virus [65,66]. However, this method is time-consuming and expensive, so it has great limitations in clinical application.

Real time reverse transcription polymerase chain reaction (RT-PCR), as a specific and simple quantitative detection method [67,68], has been widely used in the detection of various viruses [69–72]. For example, Nunes et al. used RT-qPCR to detect four Brazilian Amazon hantaviruses with a detection limit of 0.9 copies/ μ L. The specificity and sensitivity of RT qPCR were 100% and 97.63%, respectively [73]. Zhang et al. developed a real-time RT-PCR method to detect the Seneca Valley virus with a detection limit of 7.0 copies/ μ L. The specificity and sensitivity of RT-qPCR were 98.08% and 100.0%, respectively [74]. In addition, RT-PCR method has been used by many researchers to test SARS-COV-2 virus and has been widely used in clinical trials [75–77]. For example, Li

et al. developed a novel qRT-PCR method to detect SARS-COV-2 virus with a detection limit of 365.0 copies/mL. The specificity and sensitivity of RT-qPCR were 100.00% and 97.62%, respectively [78]. Wang et al. detected SARS-COV-2 virus by combining serological total antibody and RT-PCR. The detection limit of RT-PCR was 2.0 copies/µL, and the sensitivity and specificity were 98.6% and 98.7% respectively [79]. Corman et al. developed a novel real-time RT-PCR method to detect SARS-COV-2 virus with 95% specificity and 100% sensitivity. In addition, the limit of detection for E gene and RdRp gene was 3.9 and 3.6 copy RNA per reaction, respectively [80]. At present, all kinds of optimized RT-PCR detection methods are the mainstream of SARS-COV-2 virus detection, which lays a solid foundation for the detection of infection or not. If the virus material is insufficient or the operation is wrong, the RT-PCR test may be false negative. Therefore, the method has strict requirements on material quantity and operation [81]. As a result, this method increases the risk of health care workers contacting suspected infected persons. In addition, when RT-PCR method is used, the temperature setting range of the thermal cycling device of the detection equipment is 50–95 °C, so the temperature requirement is very high. These shortcomings limit its clinical application to a certain extent [60].

2.5. Loop-mediated isothermal amplification (LAMP) methods

LAMP is a novel and efficient isothermal nucleic acid (DNAs and RNAs) amplification method [82–85], showing high sensitivity and specificity [86–88]. LAMP analysis method is often used in clinical detection of coronavirus [89,90]. As shown in Fig. 2, Fan et al. used LAMP method to detect high-risk HPV16 and HPV18 viruses, and the mechanism was as follows: As shown in Fig. 2a, the DNA of the virus was obtained by centrifugation. Then, THE HPV16 and HPV18 viruses were detected by LAMP and PCR-MCE (Polymerase Chain reaction-microchip electrophoresis system), and the accuracy was higher than that of conventional cytology. They were both used for visual detection of HPV16

and HPV18 by Papanicolaou (PAP) staining. As can be seen from Fig. 2b, the virus DNA was obtained by centrifugation. Calcein then acts as a fluorescent indicator and is premixed with manganese ions in the lamp reaction mixture and then irradiated with 365.0 nm ultraviolet light. The binding of manganese ions and pyrophosphate ions results in the release of calcein. Free calcein combines with magnesium ions, resulting in the reaction system turning light yellow and emitting green fluorescence under 365.0 nm UV radiation. These are to determine the presence of HPV in the samples [91]. In addition, Guenther et al. used LAMP method to detect feline Coronavirus virus with a detection limit of 5.0 copies/ μ L. The specificity and sensitivity of LAMP were 97.3% and 58.8%, respectively [92]. Thai et al. used LAMP method to detect severe acute respiratory syndrome coronavirus with a detection limit of 0.01 copies/mL. The specificity and sensitivity of LAMP were 87.0% and 100.0%, respectively [93]. Pyrc et al. developed a LAMP detection method for human coronavirus nl63 with a detection limit of 1.0 copies/ μ L. The specificity and sensitivity of LAMP were 100.0% and 100.0%, respectively [94]. Kitagawa et al. developed a LAMP method to detect SARS-COV-2 virus with a detection limit of 1.0×10^1 copies/µL. The specificity and sensitivity of LAMP were 97.6% and 100.0%, respectively [95]. Herein, a number of LAMP-based coronavirus detection methods have been developed and applied in clinical diagnosis.

Reverse transcription loop mediated isothermal amplification (RT-LAMP) is a new method for detecting miRNA. This method has the advantages of low background noise, fast, simple and reliable. We believe LAMP is a promising method for virus detection [96]. According to the literature reports, many researchers use lamp method to detect SARS-COV-2 virus [97,98]. For example, Dao et al. used RT-LAMP method to detect SARS-COV-2 virus with a detection limit of 100.0 copies/µL. The specificity and sensitivity of RT-LAMP were 99.7% and 97.5%, respectively [99]. Klein et al. used RT-LAMP method to detect SARS-COV-2 virus with a detection limit of 10.0 copies/reaction. The specificity and sensitivity of RT-LAMP were 100.0% and 100.0%, respectively [100]. Yan et al. used RT-LAMP method to detect SARS-COV-2 virus with 100% specificity and 100% sensitivity. The lower limit of detection was less than 2×10^1 RNA copies/reaction [101]. Ben-Assa et al. used RT-LAMP method to detect SARS-COV-2 virus with a detection limit of 12.0 copies/reaction. The specificity and sensitivity of RT-LAMP were 100.0% and 100%, respectively [102]. Zhu et al. devised a multiplex reverse transcription loop-mediated isothermal amplification (mRT-LAMP) method to detect SARS-COV-2 virus with a detection limit of 12.0 copies/reaction. The specificity and sensitivity of mRT-LAMP were 100.0% and 100.0%, respectively [103]. Current RT-LAMP detection methods are used by WHO and nursing sites around the world to detect SARS-COV-2 virus, and a large number of optimized RT-LAMP methods have been proposed and even combined with other methods. However, this method also requires a high temperature (52-94 °C) and all virus isolation procedures and RNA extraction are performed in a biosafety level III facility. Therefore, the high cost, complex operation, high detection environment and high equipment requirements of this method limit the clinical application of this method, which requires further optimization [86].

2.6. SHERLOCK technique

SHERLOCK technique is a detection method which combines isothermal amplification with CRISPR-mediated detection [104–107], and the technology reduces reliance on equipment. At present, this method is often used for virus detection [108–110]. Moreover, the SHERLOCK technique can be used to detect SARS-COV-2 virus and has clinical applications [111]. For example, Joung et al. used SHERLOCK technique to detect SARS-COV-2 virus with a detection limit of 100.0 copies/reaction. The specificity and sensitivity of SHERLOCK technique were 100.0% and 100.0%, respectively [112]. Broughton et al. used CRISPR-based lateral flow assay to detect SARS-COV-2 virus with 95.0% positive predictive agreement and 100.0% negative predictive

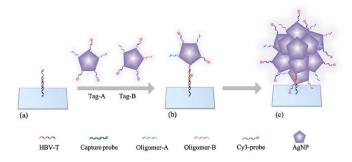


Fig. 3. Working principle of Enzyme-free fluorescence microarray detection.

agreement. The detection limit of each reaction was 1.0 copy per μ l reaction [113]. Ail et al. used CRISPR-based method to detect SARS-COV-2 virus with a detection limit of 10.0 copies/reaction. The specificity and sensitivity of SHERLOCK technique were 100.0% and 100.0%, respectively [114]. This detection method not only has good sensitivity and specificity, but also does not require complex instruments. However, this method requires DNA extraction and amplification, and the operation of the instrument is complex, and patients cannot self-detect, which increases the risk of contact and infection of medical staff [107].

2.7. Microarray-based methods

Microarray is a rapid, high-throughput detection method [115–117], which can reverse transcription of viral RNA and produce a specific probe labeled cDNA. The cDNA was then loaded into each well and hybridized with solid-phase oligonucleotides on the Microarray, which is then washed to remove the free DNAs. Finally, viral RNA is detected by a detection-specific probe, and Microarray has been widely used in the detection of virus [118-122]. As shown in Fig. 3, Jin et al. used Enzyme-free fluorescence microarray to detect hepatitis B virus DNA, and the mechanism was as follows: Fig. 3 shows the formation mechanism of AgNP aggregates for target detection on DNA microarrays. Two kinds of nucleic acid-modified AgNP probes, Tag-A and Tag-B were obtained separately by the attachments of recognition probes (Cy3-probe) and hybrid probes (Oligomer-A and Oligomer-B) to AgNPs through Ag-S bonds [123]. In addition, Lung et al. used Multiplex RT-PCR and Automated Microarray for Detection of rinderpest virus (RPV) with good specificity and sensitivity. The limit of detection of the microarray assay was as low as 1.0 TCID₅₀/ml for RPV [124]. Guo et al. used 6 a single nucleotide polymorphism DNA microarray method to detect SARS virus with 100% accuracy, and this method has able to detect 24 SNPs and determine the type of a given strain [125]. De Souza Luna et al. used nonfluorescent low-density microarray method to detect severe acute respiratory syndrome virus with a detection limit of 100.0 copies/reaction. The specificity and sensitivity of nonfluorescent low-density microarray were 100.0% and 100.0%, respectively [126]. Hardick et al. used a spotted array Mobile Analysis Platform (MAP) method to detect respiratory syncytial virus with a detection limit of 30.0 copies/reaction. The specificity and sensitivity of MAP were 100.0% and 100.0%, respectively [127]. In addition, we think this method may be of great significance for the rapid detection of SARS-COV-2. However, this method also requires DNA extraction and amplification, and the operation of the instrument is more complex, and this method not only operates at high temperature, but also takes a long time. These reasons will limit its future clinical application [118].

2.8. Enzyme linked immunosorbent assay (ELISA) method

At present, ELISA is usually used to detect viruses in clinical practice [128–132]. ELISA is an analytical method based on the specific binding between antigen and antibody [133–136]. For example, Li et al. used a

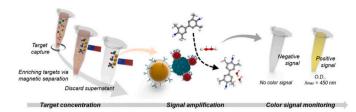


Fig. 4. Working principle of ELISA colorimetric detection.

sandwich ELISA method to detect Chinese sacbrood virus (CSBV) with a detection limit of 3.675×10^4 copies/µL. The method is specific to CSBV and has no cross reactivity with other bee viruses [137]. Tan et al. used an indirect ELISA based on glycoprotein B gene method to detect Feline herpesvirus type 1 virus. The indirect ELISA, characterized by high sensitivity showed no cross-reaction with two types of feline virus, had detection limit at 1:2000 dilution [138]. Li et al. used IDVET ELISA method to detect Akabane virus with a detection limit of 1:64 dilution. The specificity and sensitivity of IDVET ELISA were 82.31% and 93.46%, respectively [139]. Wang et al. used GP5 Protein-based ELISA method to detect Porcine reproductive and respiratory syndrome virus with a detection limit of 1:800 dilution. The specificity and sensitivity of GP5 Protein-based ELISA were 100.0% and 80.39%, respectively [140]. Qi et al. used an antigen-capture enzyme-linked immunosorbent assay (AC-ELISA) to detect equine arteritis virus with a detection limit of 36.0 PFU/mL. The specificity and sensitivity of AC-ELISA were 100.0% and 100.0%, respectively [141]. In, addition, specific antibodies (such as angiotensin-converting enzyme 2, ACE2) were immobilized and then bound to the spinous glycoprotein (S protein, viral surface spinous protein) on the surface of SARS-COV-2 to form a solid phase complex. Then the complex was combined with the enzyme labeled antibody. After adding the substrate of enzyme reaction, the substrate was catalyzed into colored products. The color reaction is analyzed according to the depth of color reaction [142]. As shown in Fig. 4, Oh et al. used Magnetic Nanozyme-Linked Immunosorbent Assay to detect Influenza A Virus, and the mechanism was as follows: Firstly, the nucleic acid was enriched by magnetic separation. Then, MagNB-Abs, which is a specific combination of magnetic nanoparticles (MagNB) and Influenza A virus antibody (Abs), acts as capture probe to recognize target viral nucleic acid through specific antigen antibody interaction. The AuNZs, which is represent the enzyme like activity of gold nanoenzyme, acts as signal amplifier to form sandwich structure with magnbs complex. After the immune response, the sandwich like structures were collected by magnetic force. AuNZs on sandwich like immune complexes act as catalysts to promote the oxidation of TMB by H_2O_2 , thus producing colorimetric signals. Meanwhile, the absence of virus cannot assemble the immunocomplex, leading to the lack of oxidation reaction of TMB for colorimetric signaling. The concentration of influenza virus directly related to the color change of TMB can be detected by the catalytic activity of AuNZs with H_2O_2 as electron acceptor [143]. The method is accurate and effective, but it has some defects such as high cost of antibody preparation, poor stability and complex operation process, which limits its wide application [144,145];

2.9. electrochemical method

In recent years, electrochemical biosensor has become a reliable analytical equipment [146–148], which can detect various viruses that threaten human health [149-151]. Electrochemical biosensor is a kind of equipment which has both electrochemical sensing and biosensor [152,153]. It can convert biochemical information, and has the advantages of simple instrument, high sensitivity, high cost-effectiveness and miniaturization [154]. The working principle of electrochemical biosensor is the enzyme catalyzed reaction between biomolecules and target analytes, which generates electrons and affects the electrical properties of the solution [155]. In addition, electrochemical biosensors have different kinds of sensors due to different biological elements [156, 157]. In recent years, electrochemical biosensors have achieved great success in the field of pathogen detection due to its unique performance. For example, it can be seen from Fig. 5 that various viruses (Influenza, Zika, HIV, HEP-B, COVID-19) can be detected by electrochemical biosensor. The method monitors the activity of living cells or enzymes by measuring interactions between analytes and biological receptors with electrochemical biosensors. The strength of each virus's electrochemical signal is different, so that the presence of such a virus can be accurately detected [146]. In addition, Zhou et al. used a novel Electrochemiluminescence Immunosensor (P-RGO@Au@Ru-SiO2) to detect HIV-1 p24 Antigen with a detection limit of 1.0×10^{-9} mg/mL. The specificity and sensitivity of Electrochemiluminescence Immunosensor were 100.0% and 100.0%, respectively [158]. Kor et al. used an electrochemical sensor, which is based on electropolymerized molecularly imprinted polymer, to detect furosemide with good specificity and sensitivity. The detection limit of electrochemical sensor was 7.0×10^{-8} mol/L [159]. Heo et al. developed a new electrochemical method to

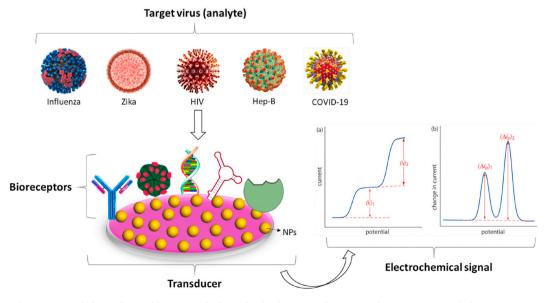


Fig. 5. Potential electrochemical biosensor platforms for the detection of various pathogenic viruses including COVID-19.

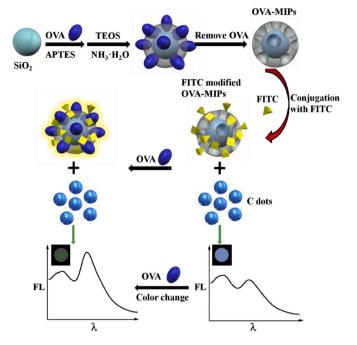


Fig. 6. Construction of molecularly imprinted double fluorescence emission system.

detect hepatitis B virus (HBV) with good specificity and sensitivity. The detection limit of electrochemical method was 0.14 ng/mL [160]. Layqah et al. used an electrochemical immunosensor to detect MERS-CoV and HCoV virus with good specificity and sensitivity. The detection limits for HCoV and MERS-CoV were as low as 0.4 pg/ml and 1.0 pg/ml, respectively [161]. To sum up, we believe that the electrochemical method will be applied to the detection of new coronavirus in the near future. However, they also face many challenges. For example, high cost, limited equipment and complex operation limit its clinical application [153].

2.10. Immunoassay technology

Immunoassay is a technology which combines specific reaction of antigen and antibody [162–164]. At present, many researchers use this technology to detect new coronavirus [165–168]. For example, Mairesse et al. used Chemiluminescence immunoassay technology to detect SARS-CoV-2 IgM antibodies. Using optimized cut-off, the specificity and sensitivity for IgM was 94.7% and 81.6%, respectively. The detection limit is 2.81 AU/mL for IgM [169]. Kohmer et al. used automated immunoassays technology to detect SARS-CoV-2 IgG antibodies with 100.0% specificity and 77.8% sensitivity [170]. Liu et al. used Chemiluminescence Microparticle Immunoassay to detect SARS-CoV-2 IgM and Ab antibodies. The specificity of IgM and Ab detection were 99.3% and 98.9%, respectively. The sensitivity of IgM and Ab detection were 72.3% and 90.8%, respectively [171]. Montesinos et al. used chemiluminescent immunoassays to detect SARS-CoV-2 IgM and IgG antibodies. The specificity of IgM and IgG detection were 58.7% and 53.2%, respectively. The sensitivity of IgM and IgG detection were 100.0% and 100.0%, respectively. The detection limit is 1.0 AU/mL for IgM and IgG [172]. To sum up, Immunoassay technology is a particularly good method for the detection of specificity and sensitivity, and has been widely used for the detection of various viruses. However, the cost of this method is too high, the operation is complex and time-consuming, which limits its clinical application [165].

2.11. New method

As mentioned above, the existing detection methods still have room for further improvement in the aspects of detection cost, detection time, convenience, and susceptibility of detection personnel [173]. Therefore, how to design a low cost, convenient, rapid, specific and sensitive SARS-COV-2 detection method is one of the important issues that need to be solved urgently at present. Surface molecular imprinting technology (SM-MIT) can be applied to the identification of biological macromolecules (such as proteins and nucleic acids), viruses and cells [174-181]. SM-MIT is a technique for synthesizing polymer networks around template molecules to obtain rich polymer materials that can be used to identify specific target molecules. This technique has good physical and chemical stability, simple preparation method, low cost, and high selectivity in recognition and recombination. Due to these excellent properties, SM-MIT has been widely used in protein specific recognition [182,183]. For example, the basic principle is that the virus specific protein is used as a template. A surface imprinting material was synthesized by using silica gel particles [184], organic polymer microspheres [185] or chitosan [186] as inert carriers, and amino and carboxyl groups as binding sites [187–189]. Then, the template protein was removed to obtain a surface imprinting material with specific and selective recognition of viral protein. For example, as can be seen from Fig. 6, Wang et al. synthesized silica core-shell surface molecularly imprinted microspheres (MIPs) using ovalbumin (OVA) as template, and used fluorescein isothiocyanate (FITC) modified microspheres as fluorescence enhancement signal, and then prepared a ratio nano sensor for the fluorescence determination of ovalbumin (OVA) by mixing blue carbon quantum dots (C dots). The sensor can be observed by naked eyes, and the fluorescence color changes from blue to dark olive green and finally to green. In addition, the detection limit is as low as 15.4 nm [190]. Klangprapan et al. used a quartz crystal microbalance molecularly imprinted polymer material to detect classical swine fever virus with good specificity and sensitivity, and the detection limit was 1.7 µg/mL [191]. Yang et al. prepared a fluorescent molecularly imprinted sensor material based on a metal-organic framework for identifying Japanese encephalitis virus (JEV). It is found through experiments that it has high selectivity and high sensitivity, and its maximum detection limit is 13.0 pmol/L [192]. Luo et al. prepared a magnetic molecularly imprinted polymer resonance light scattering sensor material to identify Japanese encephalitis virus. It is found through experiments that it has high selectivity and high sensitivity, and its maximum detection limit is 1.3 pM [193]. For example, as can be seen from Fig. 7, Zhang et al.

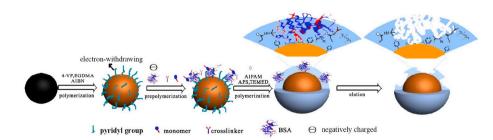


Fig. 7. Schematic diagram of protein separation by core-shell molecularly imprinted polymer microspheres.

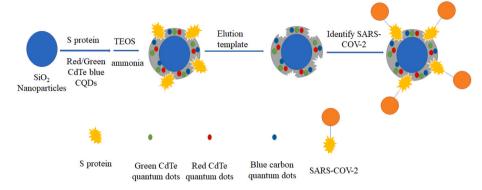


Fig. 8. Synthesis of S-protein molecularly imprinted microspheres with core-shell trichromatic fluorescence SARS-COV-2.

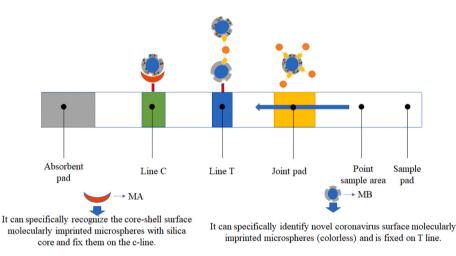
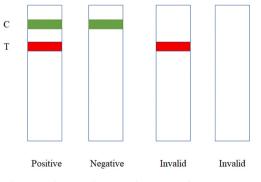


Fig. 9. Construction of three-color fluorescence-like immunotype test paper. (For interpretation of the references to color in this figure legend, the reader is referred to the Web version of this article.)

prepared a core-shell protein surface molecularly imprinted microsphere material (MIMPs), the preparation of MIMPS consists of three steps. Firstly, magnetic beads were prepared by improved solvothermal reaction. Then, 4-Vinyl pyridine (4-VP) was polymerized on the surface of the magnetic beads. Finally, the polymer membrane complementary to the template was obtained. N-isopropylacrylamide (NIPAM) monomer is added as a temperature sensitive component, which allows expansion and contraction with the change of temperature, thus realizing the recognition and release of bowene serum albumin (BSA). Pyridine group is hydrophilic, which is conducive to the dispersion of carrier microspheres in water. In addition, recognition of pyridine group at the bottom of the cavity and recognition of polymer chain are conducive to the interaction between BSA and electrostatic and hydrogen bonds, which is suitable for the selective adsorption of BSA.



After the removal of the template protein, a surface molecularly imprinted material was obtained to specifically recognize BSA [194]. To sum up, we think SM-MIT technology provides an important reference value for the research on how to target and recognize the spike glycoprotein (s protein) on the surface of SARS-COV-2. Fluorescence emission detection technology provides a visual and effective way to detect infection. The concentration of the detected substance can be reflected by the fluorescence intensity of the fluorescent emission group, which can be easily captured by the naked eye. In recent years, a series of detection technologies based on single fluorescence emission and double fluorescence emission systems have been developed for the detection of proteins, small molecules and ions [195-197]. In addition, the single fluorescence emission system can identify very few kinds of colors, and the degree of visualization is low [198]. However, the dual fluorescence emission system can not only self-tuning, but also expand the range of color change [199,200]. Therefore, silica core-shell surface molecularly imprinted microspheres [201] embedded with red, green and blue fluorescent quantum dots can be constructed by sol-gel polymerization. Then, the response of the ratio of red, green and blue quantum dots to spike glycoprotein (S-protein) on the surface of SARS-COV-2 was studied (as shown in Fig. 8). With the increase of the concentration of S-protein on the surface of SARS-COV-2, the color change effect of fluorescence color from green, yellow, orange, red, purple to blue can be observed. The surface molecularly imprinted microspheres were mixed with fluorescent quantum dots, and then grafted onto the surface of appropriate chromatographic test paper by grafting, so as to construct the SARS-COV-2 type immune test paper with visualization, specific and selective detection and convenient operation (as shown in Fig. 9). The

Fig. 10. Schematic diagram of test paper determination.

Table 3

| Method | Pros and cons | Reference |
|-----------------|---|-----------|
| Simple | A simple method can be used to determine whether a virus is infected by some symptoms of the body, but the accuracy of this method is poor, and it can | [34] |
| CT-scan | only be used for pre-screening in special period. CT-scan can determine whether a certain organ is infected with virus to some extent, but there are many kinds of viruses that can infect an organ. Therefore, it needs to combine with other methods to determine. This method is suitable for the | [45] |
| Haematological | examination of respiratory tract infection. Haematological detection has been used in the screening of various viruses, and the change of blood components can be used to determine whether some viruses are infected. However, the detection time of this method is too long, and its blood components may change the same after different virus infection. Therefore, this method | [2,54] |
| PCR | also needs further optimization. PCR is a highly sensitive and sequence specific enzyme method. This method is widely used in virus detection and has been widely accepted by researchers. However, the process is time- consuming and requires a variety of biochemical reagents, laboratory level instruments and trained | [63] |
| LAMP | professionals. LAMP is an efficient isothermal nucleic acid (DNAs and RNAs) amplification method with high sensitivity and specificity, and is widely used in the detection of coronavirus. However, this method also needs high temperature, so it has certain risk. Not only that, all virus isolation procedures and RNA extraction are carried out in a tertiary biosafety facility. Therefore, the cost of this method is high, the operation is complex, and the equipment requirements are high. | [86] |
| SHERLOCK | SHERLOCK technology is very simple, convenient and low-cost to detect viruses. It can detect gene expression and interaction in human or animal genomes one by one or even in batches, so as to clarify the function and regulatory network of genes. However, this method is easy to miss the target and is relatively difficult to transfect. It has the preference of base recognition, which limits the application scope of gene editing, and leads to different editing efficiency of different gene sites. | [107] |
| Microarray | Microarray-based method is to detect DNA hybridization signal to realize rapid, parallel and efficient detection or medical diagnosis of biological samples. This method can achieve high- throughput and parallel detection of microorganisms. All the results can be obtained in one experiment, and the operation is simple and fast. But this method requires a large amount of viral nucleic acid. In addition, there are many kinds of this method, so it is difficult to establish a unified quality standard, which limits its clinical application. | [116] |
| ELISA | At present, ELISA is commonly used in clinical detection of viruses, which is based on the specific binding of antigen and antibody. The procedure of this method is simple, because there is no need to use the second antibody, it can avoid the interaction reaction, high sensitivity and high specificity, and the antigen does not need to be purified in advance, so it can be applied to relatively impure samples, and the data reproducibility is very high. However, this method is not repeatable and easy to be interfered by autoantibodies and heterophilic antibodies. In addition, the first antibody in the test must be labeled with enzyme, but not every antibody is suitable for labeling, and the cost is relatively high. | [130] |
| Electrochemical | At present, electrochemical biosensors are often used to detect various viruses. It has the advantages | [147] |

Table 3 (continued)

| Method | Pros and cons | Reference |
|-------------|---|-----------|
| Immunoassay | of simple instrument, high sensitivity and low cost. However, this method has poor selectivity, small temperature range and short instrument life. Therefore, this method needs further optimization. Immunoassay is a method based on the specific binding of antigen and antibody. This method has the advantages of high specificity, simple and rapid operation, relatively few influencing factors, easy control, good repeatability and easy standardization. However, the results of this method have great influence on the source and affinity of the antibody used, and the sensitivity is | [167] |
| SM-MIT | relatively low. Therefore, this method needs further optimization. SM-MIT is a technology of synthesizing polymer networks around template molecules to obtain rich polymer materials, which can be used to identify specific target molecules. The technology has good physical and chemical stability, simple preparation method, low cost and high selectivity for recognition and recombination. Moreover, the surface molecularly imprinted materials can be reused. Because of these excellent properties, SM- MIT has been widely used in protein specific recognition. | [187] |

core-shell surface molecularly imprinted microspheres with silica core could specifically recognize the S-protein of SARS-COV-2 virus and form a complex with SARS-COV-2 virus after the detection sample was added to the sample area. Then the complex moves forward under the traction of the chromatographic test paper. When it moves to the position of T line, the complex can be captured by MB, and the color of T line can be determined according to the concentration of the tested substance. Some parts of the surface molecularly imprinted microspheres that are not bound to SARS-COV-2 cannot be captured by MB. Continue to move forward with the chromatography test paper. When it moves to the C line position, the surface molecularly imprinted microspheres will be captured by the MA and trapped on the C line. At this time, the C line shows green, indicating that there is no virus infection. The determination of the test results is shown in Fig. 10. If color rendering occurs on both Lines T and C, the result is positive; if only line C produces color rendering but line T does not, the result is negative; if no color rendering occurs on Line C, the test result is invalid and should be tested again. Therefore, this method can effectively shorten the detection time, reduce the cost and reduce the risk of infection of the detection personnel, and the operation is particularly simple (suspected patients can test by themselves). Therefore, early screening and early detection of SARS-COV-2 pneumonia patients can be carried out. It is believed that SM-MIT will become the focus of attention of all researchers and has great potential for application in the detection of SARS-COV-2 virus.

3. Summary and prospect

As SARS-COV-2 virus swept the world, a large number of people were infected and even died. Moreover, with the development of the epidemic, the global economy will fall into a serious recession. Some countries even disintegrated because of the epidemic. The epidemic has seriously affected the normal survival of people all over the world. The first step in controlling the epidemic is to screen suspected patients. At present, the detection methods of SARS-COV-2 virus are changing with each passing day. For the published methods, this paper not only analyzes their advantages and disadvantages (see Table 3), but also discusses their clinical performance (see Table 4). It is found from Tables 3 and 4 that the detection time of Surface molecular imprinting technology (SM-MIT) method is short, the detection limit is low and the accuracy is high. To sum up, this review is the first time to propose SM-MIT for the detection of SARS-COV-2 virus, and the steps and mechanisms of

Table 4

Different detection methods detect different viruses.

| Method | Virus species | Accuracy (%) | Detection limit | Detection time | Reference |
|-----------------|-----------------------------------|--------------|------------------------------|----------------|-----------|
| Simple | / | / | / | / | [33] |
| CT-scan | / | / | / | / | [41] |
| Haematological | / | / | / | / | [47] |
| PCR | SARS-CoV-2 | 100.0 | 5.0 copies/reaction | 70.0 min | [69] |
| | Brazilian Amazon hantaviruses | 97.6 | 0.9 copies∕µL | 92.0 min | [73] |
| LAMP | Zika virus | 100.0 | 20.0 copies/reaction | 60.0 min | [90] |
| | Feline Coronavirus virus | 100.0 | 5.0 copies/μL | 77.0 min | [92] |
| SHERLOCK | SARS-CoV-2 | 100.0 | 100.0 copies/reaction | 70.0 min | [112] |
| | SARS-CoV-2 | 100.0 | 10.0 copies/µL | 45.0 min | [113] |
| Microarray | Severe acute respiratory syndrome | 100.0 | 100.0 copies/reaction | 45.0 min | [126] |
| | Respiratory syncytial virus | 100.0 | 30.0 copies/reaction | 110.0 min | [127] |
| ELISA | Chinese sacbrood virus | 100.0 | 3.67×10^4 copies/µL | 70.0 min | [137] |
| | Equine arteritis virus | 100.0 | 36.0 PFU/mL | 60.0 min | [141] |
| Electrochemical | Chikungunya virus | 100.0 | 8.0 ng/mL | 90.0 min | [149] |
| | Hepatitis B virus | 100.0 | 0.14 ng/mL | 120.0 min | [152] |
| Immunoassay | SARS-COV-2 | 100.0 | 20.0 copies/µL | 48.0 min | [90] |
| | SARS-COV-2 | 88.6 | 20.0 copies/µL | 15.0 min | [162] |
| SM-MIT | Swine fever virus | 100.0 | 1.7 μg/mL | 10.0 min | [191] |
| | Japanese encephalitis virus | 100.0 | 13.0 pmol/L | 20.0 min | [192] |

this method are described in detail. We believe that the SM-MIT method will become a hot spot for many researchers and has great potential in the detection of SARS-COV-2 virus.

Declaration of competing interest

The authors declare that there are no conflicts of interest.

Acknowledgments

This study was funded by the National Natural Science Foundation of China (Grant No.21576295), the Hunan Provincial Natural Science Foundation of China (2019JJ50759), and the Fundamental Research Funds for the Central Universities of Central South University (2017zzts175 and 2018zzts371).

References

- [1] J.Y. Li, Z. You, Q. Wang, Z.J. Zhou, Y. Qiu, R. Luo, X.Y. Ge, The epidemic of 2019novel-coronavirus (2019-nCoV) pneumonia and insights for emerging infectious diseases in the future, Microb. Infect. 22 (2020) 80–85, https://doi.org/10.1016/ j.micinf.2020.02.002.
- [2] S.T. Kang, W.Y. Peng, Y.H. Zhu, S.Y. Lu, M. Zhou, W. Lin, W.F. Wu, S. Huang, L. P. Jiang, X. Luo, M.C. Deng, Recent progress in understanding 2019 novel coronavirus (SARS-CoV-2) associated with human respiratory disease: detection, mechanisms and treatment, Int. J. Antimicrob. Agents 55 (2020) 105950, https://doi.org/10.1016/j.ijantimicag.2020.105950.
- [3] H. Harapan, N. Itoh, A. Yufika, W. Winardi, S. Keam, H. Te, D. Megawati, Z. Hayati, A.L. Wagner, M. Mudatsir, Coronavirus disease 2019 (COVID-19): a literature review, J. Infect. Public. Heal. 13 (2020) 667–673, https://doi.org/ 10.1016/j.jiph.2020.03.019.
- [4] X. Peng, X. Xu, Y.Q. Li, L. Cheng, X.D. Zhou, B. Ren, Transmission routes of 2019nCoV and controls in dental practice, Int. J. Oral Sci. 12 (2020) 9, https://doi. org/10.1038/s41368-020-0075-9.
- H.Z. Lu, Drug treatment options for the 2019-new coronavirus (2019-nCoV), Biosci Trends 14 (2020) 69–71, https://doi.org/10.5582/bst.2020.01020.
- [6] W.G. Carlos, C.S.D. Cruz, B. Cao, S. Pasnick, S. Jamil, Novel wuhan (2019-nCoV) coronavirus, Am. J. Respir. Crit. Care Med. 201 (2020), https://doi.org/10.1164/ rccm.2014P7.
- [7] A.E. Gorbalenya, S.C. Baker, R.S. Baric, R.J. De Groot, C. Drosten, A.A. Gulyaeva, B.L. Haagmans, C. Lauber, A.M. Leontovich, B.W. Neuman, D. Penzar, S. Perlman, L.L. M Poon, D.V. Samborskiy, I.A. Sidorov, I. Sola, J. Ziebuhr, The species Severe acute respiratory syndrome-related coronavirus: classifying 2019-nCoV and naming it SARS-CoV-2, Nat. Microbiol. 5 (2020) 536–544, https://doi.org/ 10.1038/s41564-020-0695-z.
- [8] T. Lupia, S. Scabini, S.M. Pinna, G.D. Perri, F.G. De Rosa, S. Corcione, 2019 novel coronavirus (2019-nCoV) outbreak: a new challenge, J. Glob. Antimicrob. Re. 21 (2020) 22–27, https://doi.org/10.1016/j.jgar.2020.02.021.
- [9] World Health Organization, WHO Coronavirus Disease (COVID-19) Dashboard, 2020. Accessed, https://covid19.who.int/. (Accessed 26 October 2020).
- [10] L.W. Fu, B.Y. Wang, T.W. Yuan, X.T. Chen, Y.L. Ao, T. Fitzpatrick, P.Y. Li, Y. G. Zhou, Y.F. Lin, Q.B. Duan, G.F. Luo, S. Fan, Y. Lu, A.P. Feng, Y.W. Zhan, B. W. Liang, W.P. Cai, L. Zhang, X.J. Du, L.H. Li, Y.L. Shu, H.C. Zou, Clinical

characteristics of coronavirus disease 2019 (COVID-19) in China: a systematic review and meta-analysis, J. Infect. 80 (2020) 656–665, https://doi.org/ 10.1016/j.jinf.2020.03.041.

- [11] D.W. Wang, B. Hu, F.F. Zhu, X. Liu, J. Zhang, B.B. Wang, H. Xiang, Z.S. Cheng, Y. Xiong, Y. Zhao, Y.R. Li, X.H. Wang, Z.Y. Peng, Clinical characteristics of 138 hospitalized patients with 2019 novel coronavirus-infected pneumonia in wuhan, China, JAMA, J. Am. Med. Assoc. 323 (2020) 1061–1069, https://doi.org/ 10.1001/jama.2020.1585.
- [12] J.J. Zhang, X. Dong, Y.Y. Cao, Y.D. Yuan, Y.B. Yang, Y.Q. Yan, C.A. Akdis, Y. D. Gao, Clinical characteristics of 140 patients infected with SARS-CoV-2 in Wuhan, China, Allergy 75 (2020) 1730–1741, https://doi.org/10.1111/all.14238.
- [13] B.E. Young, S.W.X. Ong, S. Kalimuddin, J.G. Low, S.Y. Tan, J. Loh, O.T. Ng, K. Marimuthu, L.W. Ang, T.M. Mak, S.K. Lau, D.E. Anderson, K.S. Chan, T.Y. Tan, T.Y. Ng, L. Cui, Z. Said, L. Kurupatham, M.I.C. Chen, M. Chan, S. Vasoo, L. F. Wang, B.H. Tan, R.T.P. Lin, V.J.M. Lee, Y.S. Leo, D.C. Lye, Novel coronavirus outbreak research team, epidemiologic features and clinical course of patients infected with SARS-CoV-2 in Singapore, J. Am. Med. Assoc. 323 (2019) 1488–1494, https://doi.org/10.1001/jama.2020.3204.
- [14] Y. Yan, L. Chang, L.N. Wang, Laboratory testing of SARS-CoV, MERS-CoV, and SARS-CoV-2 (2019-nCoV): current status, challenges, and countermeasures, Rev. Med. Virol. 30 (2020), e2106, https://doi.org/10.1002/rmv.2106.
- [15] D. Bestle, M.R. Heindl, H. Limburg, T. Van Lam van, O. Pilgram, H. Moulton, D. A. Stein, K. Hardes, M. Eickmann, O. Dolnik, C. Rohde, H.D. Klenk, W. Garten, T. Steinmetzer, E. Böttcher-Friebertshäuser, TMPRSS2 and furin are both essential for proteolytic activation of SARS-CoV-2 in human airway cells, Life. Sci. Alliance 23 (2020), e202000786, https://doi.org/10.26508/lsa.202000786.
- [16] J. Riou, C.L. Althaus, Pattern of early human-to-human transmission of Wuhan 2019 novel coronavirus (2019-nCoV), December 2019 to January 2020, Euro Surveill. 25 (2020) 2000058, https://doi.org/10.2807/1560-7917. ES.2020.25.4.2000058.
- [17] Y. Yin, R.G. Wunderink, MERS, SARS and other coronaviruses as causes of pneumonia, Respirology 23 (2018) 130–137, https://doi.org/10.1111/ resp.13196.
- [18] Y. Feng, T. Marchal, T. Sperry, H. Yi, Influence of wind and relative humidity on the social distancing effectiveness to prevent COVID-19 airborne transmission: a numerical study, J. Aerosol Sci. 147 (2020) 105585, https://doi.org/10.1016/j. jaerosci.2020.105585.
- [19] Y.X. Chen, X. Tong, J. Wang, W.J. Huang, S.X. Yin, R. Huang, H.L. Yang, Y. Chen, A.J. Huang, Y. Liu, Y. Chen, L. Yuan, X.M. Yan, H. Shen, C. Wu, High SARS-CoV-2 antibody prevalence among healthcare workers exposed to COVID-19 patients, J. Infect. 81 (2020) 420–426, https://doi.org/10.1016/j.jinf.2020.05.067.
- [20] S. Romano-Bertrand, L.S. Aho Glele, B. Grandbastien, D. Lepelletier, French Society for Hospital Hygiene, Preventing SARS-CoV-2 transmission in rehabilitation pools and therapeutic water environments, J. Hosp. Infect. 105 (2020) 625–627, https://doi.org/10.1016/j.jhin.2020.06.003.
- [21] X.H. Zhang, Y. Zhang, W.Z. Qiao, J. Zhang, Z.G. Qi, Baricitinib, a drug with potential effect to prevent SARS-COV-2 from entering target cells and control cytokine storm induced by COVID-19, Int. Immunopharm. 86 (2020) 106749, https://doi.org/10.1016/j.intimp.2020.106749.
- [22] M. Bosso, T.A. Thanaraj, M. Abu-Farha, M. Alanbaei, J. Abubaker, F. Al-Mulla, The two faces of ACE2: the role of ACE2 receptor and its polymorphisms in hypertension and COVID-19. Molecular therapy, Mol. Ther-Meth. Clin. D. 18 (2020) 321–327, https://doi.org/10.1016/j.omtm.2020.06.017.
- [23] N.S. Sharif-Askari, F.S. Sharif-Askari, M. Alabed, M.H. Temsah, S.A. Heialy, Q. Hamid, R. Halwani, Airways expression of SARS-CoV-2 receptor, ACE2, and TMPRSS2 is lower in children than adults and increases with smoking and COPD, Mol. Ther. Methods. Cli. Dev. 18 (2020) 1–6, https://doi.org/10.1016/j. omtm.2020.05.013.

- [24] R. Liu, H. Han, F. Liu, Z.H. Lv, K.L. Wu, Y.L. Liu, Y. Feng, C.L. Zhu, Positive rate of RT-PCR detection of SARS-CoV-2 infection in 4880 cases from one hospital in Wuhan, China, from Jan to Feb 2020, Clin. Chim. Acta 505 (2020) 172–175, https://doi.org/10.1016/j.cca.2020.03.009.
- [25] B. Vásárhelyi, K. Kristóf, E. Ostorházi, D. Szabó, Z. Prohászka, B. Merkely, The diagnostic value of rapid anti IgM and IgG detecting tests in the identification of patients with SARS CoV-2 virus infection, Orv. Hetil. 161 (2020) 807–812, https://doi.org/10.1556/650.2020.31859.
- [26] A.K. Nalla, A.M. Casto, M.W. Huang, G.A. Perchetti, R. Sampoleo, L. Shrestha, Y. L. Wei, H.Y. Zhu, K.R. Jerome, A.L. Greninger, Comparative performance of SARS-CoV-2 detection assays using seven different primer-probe sets and one assay kit, J. Clin. Microbiol. 58 (2020) e00557, https://doi.org/10.1128/ JCM.00557-20.
- [27] J. Liu, A.M. Babka, B.J. Kearney, S.R. Radoshitzky, J.H. Kuhn, X.K. Zeng, Molecular detection of SARS-CoV-2 in formalin-fixed, paraffin-embedded specimens, JCI. Insight. 5 (2020), e139042, https://doi.org/10.1172/jci. insight.139042.
- [28] A.K. Nalla, A.M. Casto, M.L.W. Huang, G.A. Perchetti, R. Sampoleo, L. Shrestha, Y.L. Wei, H.Y. Zhu, K.R. Jerome, A.L. Greninger, Comparative performance of SARS-CoV-2 detection assays using seven different primer-probe sets and one assay kit, J. Clin. Microbiol. 58 (2020) e00557, https://doi.org/10.1128/ JCM.00557-20.
- [29] F. Qiu, H.J. Wang, Z.K. Zhang, L.B. Cao, C.L. Wang, J.B. Wu, Q.F. Du, Laboratory testing techniques for SARS-CoV-2, J. South. Med. Univ. 40 (2020) 164–167, https://doi.org/10.12122/j.issn.1673-4254.2020.02.04.
- [30] R.A. Perera, C.K. Mok, O.T. Tsang, H.B. Lv, R.L. Ko, N.C. Wu, M. Yuan, W. S. Leung, J.M. Chan, T.S. Chik, C.Y. Choi, K. Leung, K.H. Chan, K.C. Chan, K.C. Li, J.T. Wu, I.A. Wilson, A.S. Monto, L.L. Poon, M. Peiris, Serological assays for severe acute respiratory syndrome coronavirus 2 (SARS-CoV-2), March 2020, Euro Surveili. 25 (2020) 2000421, https://doi.org/10.2807/1560-7917. ES.2020.25.16.2000421.
- [31] A.J. Gorzalski, H. Tian, C. Laverdure, S. Morzunov, S.C. Verma, S. VanHooser, M. W. Pandori, High-Throughput Transcription-mediated amplification on the Hologic Panther is a highly sensitive method of detection for SARS-CoV-2, J. Clin. Virol. 129 (2020) 1386–6532, https://doi.org/10.1016/j.jcv.2020.104501.
- [32] W.H. Kong, Y. Li, M.W. Peng, D.G. Kong, X.B. Yang, L.Y. Wang, M.Q. Liu, SARS-CoV-2 detection in patients with influenza-like illness, Nat. Microbiol. 5 (2020) 675–678, https://doi.org/10.1038/s41564-020-0713-1.
- [33] W.R.B. Md, A.H. Md, M.P.C. Ba, M.A.L.A. Ba, S.K.S.M. MSCE, Universal testing for SARS-CoV-2 in two philadelphia hospitals: carrier prevalence and symptom development over two weeks, Am. J. Obstet. Gyn. MFM. (2020), https://doi.org/ 10.1016/j.ajogmf.2020.100226.
- [34] F. Pérez-García, R. Pérez-Tanoira, J. Romanyk, T. Arroyo, P. Gómez-Herruz, J. Cuadros-González, Alltest rapid lateral flow immunoassays is reliable in diagnosing SARS-CoV-2 infection from 14 days after symptom onset: a prospective single-center study, J. Clin. Virol. 129 (2020) 104473, https://doi. org/10.1016/j.jcv.2020.104473.
- [35] Y.H. Jin, L. Cai, Z.S. Cheng, H. Cheng, T. Deng, Y.P. Fan, C. Fang, D. Huang, L. Q. Huang, Q. Huang, Y. Han, B. Hu, F. Hu, B.H. Li, Y.R. Li, K. Liang, L.K. Lin, L. S. Luo, J. Ma, L.L. Ma, Z.Y. Peng, Y.B. Pan, Z.Y. Pan, X.Q. Ren, H.M. Sun, Y. Wang, Y.Y. Wang, H. Weng, C.J. Wei, D.F. Wu, J. Xia, Y. Xiong, H.B. Xu, X.M. Yao, Y. F. Yuan, T.S. Ye, X.C. Zhang, Y.W. Zhang, Y.G. Zhang, H.M. Zhang, Y. Zhao, M. J. Zhao, H. Zi, X.T. Zeng, Y.Y. Wang, X.H. Wang, For the zhongnan hospital of wuhan university novel coronavirus management and research team, evidence-based medicine chapter of China international exchange and promotive association for medical and health care (CPAM), A rapid advice guideline for the diagnosis and treatment of 2019 novel coronavirus (2019-nCoV) infected pneumonia (standard version), Mil. Med. Res. 7 (2020) 4, https://doi.org/10.1186/s40779-020-0233-6.
- [36] P. Li, D.J. Su, J.F. Zhang, X.D. Xia, H. Sui, D.H. Zhao, Pneumonia in novel swineorigin influenza A (H1N1) virus infection: high-resolution CT findings, Eur. J. Radiol. 80 (2011) e146–e152, https://doi.org/10.1016/j.ejrad.2010.05.029.
- [37] G. Turcato, L. Panebianco, A. Zaboli, C. Scheurer, D. Ausserhofer, A. Wieser, N. Pfeifer, Correlation between arterial blood gas and CT volumetry in patients with SARS-CoV-2 in the emergency department, Int. J. Infect. Dis. 97 (2020) 233–235, https://doi.org/10.1016/j.ijid.2020.06.033.
- [38] H.J. Ma, Z.J. Zhu, Y. Lin, Y.Y. Shen, W. Hu, W.B. Zheng, G.R. Liu, H.J. Li, D. J. Mikulis, R.H. Wu, Radiological findings of chest in patients with H7N9 avian influenza from a hospital, Radiology. Infect. Dis. 2 (2015) 177–182, https://doi.org/10.1016/j.jrid.2015.11.010.
- [39] P. Hulo, Y. Touchefeu, E. Cauchin, I. Archambeaud, N. Chapelle, C. Bossard, J. Bennouna, Acute ulceronecrotic gastritis with cytomegalovirus reactivation: uncommon toxicity of immune checkpoint inhibitors in microsatellite instabilityhigh metastatic colorectal cancer, Clin. Colorectal Canc. (2020), https://doi.org/ 10.1016/j.clcc.2020.04.006.
- [40] Middle East respiratory syndrome (MERS) coronavirus, in: R.B.M. DO, F.A.C.P. M. MPH, C.T. FAA (Eds.), Dis. Mon. (2020), https://doi.org/10.1016/j. disamonth.2020.101053.
- [41] M. Chung, A. Bernheim, X.Y. Mei, N. Zhang, M.Q. Huang, X.J. Zeng, J.F. Cui, W. J. Xu, Y. Yang, Z.A. Fayad, A. Jacobi, K.W. Li, S.L. Li, H. Shan, CT imaging features of 2019 novel coronavirus (2019-nCoV), Radiology 295 (2020) 202–207, https://doi.org/10.1148/radiol.2020200230.
- [42] L.B. Deng, A. Khan, W. Zhou, Y. Dai, M. Eftekhar, R.Z. Chen, G.X. Cheng, Followup study of clinical and chest CT scans in confirmed COVID-19 patients, Radiol. Infect. Dis. (2020), https://doi.org/10.1016/j.jrid.2020.07.002.

- [43] K. Pautrat, N. Chergui, SARS-CoV-2 infection may result in appendicular syndrome: chest CT scan before appendectomy, J. Vis. Surg. 157 (2020) S63–S64, https://doi.org/10.1016/j.jviscsurg.2020.04.007.
- [44] N. Zhu, D.Y. Zhang, W.L. Wang, X.W. Li, B. Yang, J.D. Song, X. Zhao, B.Y. Huang, W.F. Shi, R.J. Lu, P.H. Niu, F.X. Zhan, X.J. Ma, D.Y. Wang, W.B. Xu, G.Z. Wu, G. F. Gao, W.J. Tan, China novel coronavirus investigating and research team, A novel coronavirus from patients with pneumonia in China, 2019, N. Engl. J. Med. 382 (2020) 727–733, https://doi.org/10.1056/NEJMoa2001017.
- [45] Y.X. Liu, Y. Yang, C. Zhang, F.M. Huang, F.X. Wang, J. Yuan, Z.Q. Wang, J.X. Li, J.M. Li, C. Feng, Z. Zhang, L.F. Wang, L. Peng, L. Chen, Y.H. Qin, D.D. Zhao, S. G. Tan, L. Yin, J. Xu, C.Z. Zhou, C.Y. Jiang, L. Liu, Clinical and biochemical indexes from 2019-nCoV infected patients linked to viral loads and lung injury, Sci. China Life Sci. 63 (2020) 364–374, https://doi.org/10.1007/s11427-020-1643-8.
- [46] A. El-Badrawy, A. Zeidan, M.A. Ebrahim, 64 multidetector CT findings of influenza A (H1N1) virus in patients with hematologic malignancies, Acta Radiol. 53 (2012) 662–667, https://doi.org/10.1258/ar.2012.120038.
- [47] J.H. Ko, M.A. Müller, H. Seok, G.E. Park, J.Y. Lee, S.Y. Cho, Y.E. Ha, J.Y. Baek, S. H. Kim, J.M. Kang, Y.J. Kim, I.K.J. Jo, C.R. Chung, M.J. Hahn, C. Drosten, C. I. Kang, D.R. Chung, J.H. Song, E.S. Kang, K.R. Peck, Serologic responses of 42 MERS-coronavirus-infected patients according to the disease severity, Diagn. Microbiol. Infect. Dis. 89 (2017) 106–111, https://doi.org/10.1016/j. diagmicrobio.2017.07.006.
- [48] A.L. Marca, M. Capuzzo, T. Paglia, L. Roli, T. Trenti, S.M. Nelson, Testing for SARS-CoV-2 (COVID-19): a systematic review and clinical guide to molecular and serological in-vitro diagnostic assays, Reprod. Biomed. Online 41 (2020) 483–499, https://doi.org/10.1016/j.rbmo.2020.06.001.
- [49] T. Nicol, C. Lefeuvre, O. Serri, A. Pivert, F. Joubaud, V. Dubée, A. Kouatchet, A. Ducancelle, F. Lunel-Fabiani, H.L. Guillou-Guillemette, Assessment of SARS-CoV-2 serological tests for the diagnosis of COVID-19 through the evaluation of three immunoassays: two automated immunoassay (Euroimmun and Abbott) and one rapid lateral flow immunoassay (NG Biotech), J. Clin. Virol. 129 (2020) 104511, https://doi.org/10.1016/j.jcv.2020.104511.
- [50] W.L. Mao, J.P. Wu, Haematologic indices in hepatitis B virus-related liver disease, Clin. Chim. Acta 500 (2020) 135–142, https://doi.org/10.1016/j. cca 2019.10.007.
- [51] J. Kęsik-Maliszewska, M. Pomorska-Mól, Á.B. Collins, J. Rola, M. Larska, Potential use of hematological and acute phase protein parameters in the diagnosis of acute Schmallenberg virus infection in experimentally infected calves, Comp. Immunol. Microb. 64 (2019) 146–152, https://doi.org/10.1016/j. cimid.2019.03.008.
- [52] S. Tavitian, J.M. Péron, A. Huynh, J.M. Mansuy, L. Ysebaert, F. Huguet, J. P. Vinel, M. Attal, J. Izopet, C. Récher, Hepatitis E virus excretion can be prolonged in patients with hematological malignancies, J. Clin. Virol. 49 (2010) 141–144, https://doi.org/10.1016/j.jcv.2010.06.016.
 [53] L. Hunt, A. Gupta-Wright, V. Simms, F. Tamba, V. Knott, K. Tamba,
- [53] L. Hunt, A. Gupta-Wright, V. Simms, F. Tamba, V. Knott, K. Tamba, S. Heisenberg-Mansaray, E. Tamba, A. Sheriff, S. Conteh, T. Smith, S. Tobin, T. Brooks, C. Houlihan, R. Cummings, T. Fletcher, Clinical presentation, biochemical, and haematological parameters and their association with outcome in patients with Ebola virus disease: an observational cohort study, Lancet Infect. Dis. 15 (2015) 1292–1299, https://doi.org/10.1016/S1473-3099(15)00144-9.
- [54] P.B. Bassi, F.F. Araujo, G.C. Garcia, M.F. Costa e Silva, E.R. Bittar, C.M. Bertonha, O.A. Martins-Filho, M.S.S. Araujo, J.F. Bittar, Haematological and immunophenotypic evaluation of peripheral blood cells of cattle naturally infected with bovine papillomavirus, Vet. J. 224 (2019) 112–115, https://doi. org/10.1016/j.tvjl.2018.12.004.
- [55] Y. Bai, L.S. Yao, T. Wei, F. Tian, D.Y. Jin, L.J. Chen, M.Y. Wang, Presumed asymptomatic carrier transmission of COVID-19, JAMA, J. Am. Med. Assoc. 323 (2020) 1406–1407, https://doi.org/10.1001/jama.2020.2565.
 [56] J.F.W. Chan, S.F. Yuan, K.H. Kok, K.K.-W. To, H. Chu, J. Yang, F.F. Xing, J.L. Liu,
- [56] J.F.W. Chan, S.F. Yuan, K.H. Kok, K.K.-W. To, H. Chu, J. Yang, F.F. Xing, J.L. Liu, C.C.-Y. Yip, R.W.S. Poon, H.-W. Tsoi, S.K.-F. Lo, K.-H. Chan, V.K.-M. Poon, W.-M. Chan, J.D. Ip, J.P. Cai, V.C.C. Cheng, H.L. Chen, C.K.M. Hui, K.Y. Yuen, A familial cluster of pneumonia associated with the 2019 novel coronavirus indicating person-toperson transmission: a study of a family cluster, Lancet 395 (2020) 514–523, https://doi.org/10.1016/S0140-6736(20)30154-9.
- [57] C.L. Huang, Y.M. Wang, X.W. Li, L.L. Ren, J.P. Zhao, Y. Hu, L. Zhang, G.H. Fan, J. Y. Xu, X.Y. Gu, Z.S. Cheng, T. Yu, J.A. Xia, Y. Wei, W.J. Wu, X.L. Xie, W. Yin, H. Li, M. Liu, Y. Xiao, H. Gao, L. Guo, J.G. Xie, G.F. Wang, R.M. Jiang, Z.C. Gao, Q. Jin, J.W. Wang, B. Cao, Clinical features of patients infected with 2019 novel coronavirus in Wuhan, China, Lancet 395 (2020) 497–506, https://doi.org/10.1016/S0140-6736(20)30183-5.
- [58] Y.N. Gu, A.C.Y. Hsu, Z.Q. Pang, H. Pan, X. Zuo, G.Q. Wang, J.T. Zheng, F. Wang, Role of the innate cytokine storm induced by the influenza A virus, Viral Immunol. 32 (2019) 244–251, https://doi.org/10.1089/vim.2019.0032.
- [59] H.J. Kim, Validation of the sensitivities of one-step and two-step reversetranscription PCR methods for detection of viral hemorrhagic septicemia virus (VHSV) IVa isolates from cultured olive flounder in Korea, Aquaculture 448 (2015) 359–364, https://doi.org/10.1016/j.aquaculture.2015.06.034.
- [60] R. Narushima, T.S.T. Takahashi, Development of a real-time reversetranscription-PCR method for detection of RD114 virus in canine vaccines, Biologicals 39 (2011) 89–93, https://doi.org/10.1016/j.biologicals.2011.01.004.
- [61] K. Matsuda, A. Yamaguchi, C. Taira, A. Sueki, H. Koeda, F. Takagi, M. Sugano, T. Honda, A novel high-speed droplet-polymerase chain reaction can detect human influenza virus in less than 30min, Clin. Chim. Acta 413 (2012) 1742–1745, https://doi.org/10.1016/j.cca.2012.06.026.

- [62] L.P. Yan, S. Peng, P.X. Yan, J.W. Zhou, Q.Y. Teng, G.X. Li, X.S. Li, Z.J. Li, Comparison of real-time reverse transcription loop-mediated isothermal amplification and real-time reverse transcription polymerase chain reaction for duck Tembusu virus, J. Virol Methods 182 (2012) 50–55, https://doi.org/ 10.1016/j.jviromet.2012.03.007.
- [63] L. Hyndman, S. Vilcek, J. Conner, P.F. Nettleton, A novel nested reverse transcription PCR detects bovine viral diarrhoea virus in fluids from aborted bovine fetuses, J. Virol Methods 71 (1998) 69–76, https://doi.org/10.1016/ S0166-0934(97)00206-1.
- [64] C. Guittré, I. Baginski, G.L. Gall, M. Prave, C. Trépo, L. Cova, Detection of rabbit haemorrhagic disease virus isolates and sequence comparison of the N-terminus of the capsid protein gene by the polymerase chain reaction, Res. Vet. Sci. 58 (1995) 128–132, https://doi.org/10.1016/0034-5288(95)90065-9.
- [65] M.Z. Shen, Y. Zhou, J.W. Ye, A.A.A. AL-maskri, Y. Kang, S. Zeng, S. Cai, Recent advances and perspectives of nucleic acid detection for coronavirus, J. Pharm. Anal. 10 (2020) 97–101, https://doi.org/10.1016/j.jpha.2020.02.010.
- [66] J.E. Corral, S.A. Hoogenboom, P.T. Kröner, M.I. Vazquez-Roque, M.F. Picco, F. A. Farraye, M.B. Wallace, COVID-19 polymerase chain reaction testing before endoscopy: an economic analysis, Gastrointest. Endosc. 92 (2020) 524–534, https://doi.org/10.1016/j.gie.2020.04.049.
- [67] M.R. Green, J. Sambrook, Quantification of RNA by real-time reverse transcription-polymerase chain reaction (RT-PCR), Cold Spring Harb. Protoc. (2018), https://doi.org/10.1101/pdb.prot095042.
- [68] L.L. Liu, X.M. Qi, B.J. Zou, Q.X. Song, G.H. Zhou, Quantitative detection of gene methylated level of stool samples based on invader assay coupled with real-time polymerase chain reaction and its application in non-invasive screening of colorectal cancer, Chinese, J. Anal. Chem. 46 (2018) 1552–1559, https://doi.org/ 10.1016/S1872-2040(18)61117-X.
- [69] S. Petrillo, G. Carrà, P. Bottino, E. Zanotto, M.C. De Santis, J.P. Margaria, A. Giorgio, G. Mandili, M. Martini, R. Cavallo, D. Barberio, F. Altruda, A novel multiplex qRT-PCR assay to detect SARS-CoV-2 infection: high sensitivity and increased testing capacity, Microorganisms 17 (2020) 1064, https://doi.org/ 10.3390/microorganisms8071064.
- [70] S.P. Yip, S.S.T. To, P.H.M. Leung, T.S. Cheung, P.K.C. Cheng, W.W.L. Lim, Use of dual TaqMan probes to increase the sensitivity of 1-step quantitative reverse transcription-PCR: application to the detection of SARS coronavirus, Clin. Chem. 51 (2005) 1885–1888, https://doi.org/10.1373/clinchem.2005.054106.
- [71] Y.J. Sohn, J.H. Choi, Y.Y. Choi, Y.J. Choe, K. Kim, Y.K. Kim, B. Ahn, S.H. Song, M. S. Han, J.Y. Park, J.K. Lee, E.H. Choi, Effectiveness of trivalent inactivated influenza vaccines in children during 2017-2018 season in Korea: comparison of test-negative analysis by rapid and RT-PCR influenza tests, Int. J. Infect. Dis. 99 (2020) 199–203, https://doi.org/10.1016/j.ijid.2020.07.032.
- [72] I. Sakamaki, Y. Morinaga, H. Tani, Y. Takegoshi, Y. Fukui, H. Kawasuji, A. Ueno, Y. Miyajima, M. Wakasugi, T. Kawagishi, H. Kuwano, T. Hatano, T. Shibuya, H. Okudera, Y. Yamamoto, Monitoring of viral load by RT-PCR caused decision making to continue ECMO therapy for a patient with COVID-19, J. Infect. Chemother. 26 (2020) 1324–1327, https://doi.org/10.1016/j.jiac.2020.08.014.
- [73] B.T.D. Nunes, M.H.R. De Mendonça, D.D. Simith, A.F. Moraes, C.C. Cardoso, I.T. E. Prazeres, A.A. De Aquino, A.D.M. Santos, A.L.N. Queiroz, D.S.G. Rodrigues, Development of RT-qPCR and semi-nested RT-PCR assays for molecular diagnosis of hantavirus pulmonary syndrome, PLoS Neglected Trop. Dis. 13 (2019), e0007884, https://doi.org/10.1371/journal.pntd.0007884.
- [74] J.Q. Zhang, C. Nfon, C.F. Tsai, C.H. Lee, L. Fredericks, Q. Chen, A. Sinha, S. Bade, K. Harmon, P. Piñeyro, P. Gauger, Y.L. Tsai, H.T.T. Wang, P.Y.A. Lee, Development and evaluation of a real-time RT-PCR and a field-deployable RT-insulated isothermal PCR for the detection of Seneca Valley virus, BMC Vet. Res. 15 (2019) 168, https://doi.org/10.1186/s12917-019-1927-4.
- [75] F. Mei, M. Bonifazi, S. Menzo, A.D.M. Berardino, M. Sediari, L. Paolini, A. Re, F. Gonnelli, M. Grilli, G.S. Vennarucci, M.A. Latini, L. Zuccatosta, S. Gasparini, First detection of SARS-CoV-2 by real-time reverse transcriptase-polymerase chain reaction assay in pleural fluid, Chest (2020), https://doi.org/10.1016/j. chest.2020.05.583.
- [76] J. Lu, J.J. Peng, Q.L. Xiong, Z. Liu, H.F. Lin, X.H. Tan, M. Kang, R.Y. Yuan, L. L. Zeng, P.P. Zhou, C.M. Liang, L.N. Yi, L. Du Plessis, T. Song, W.J. Ma, J.F. Sun, O.G. Pybus, C.W. Ke, Clinical, immunological and virological characterization of COVID-19 patients that test re-positive for SARS-CoV-2 by RT-PCR, EBioMedicine 59 (2020) 102960, https://doi.org/10.1016/j.ebiom.2020.102960.
- [77] S. Assaad, V. Avrillon, M.L. Fournier, B. Mastroianni, B. Russias, A. Swalduz, P. Cassier, L. Eberst, M.P. Steineur, M. Kazes, M. Perol, A.S. Michallet, P. Rey, A. S. Erena-Penet, A. Morel, M. Brahmi, A. Dufresne, O. Tredan, G. Chvetzoff, J. Fayette, C.D.L. Fouchardiere, I. Ray-Coquard, T. Bachelot, P. Saintigny, M. Tabutin, A. Dupré, E. Nicolas-Virelizier, A. Belhabri, P.E. Roux, C. Fuhrmann, F. Pilleul, A. Basle, A. Bouhamama, C. Galvez, A.L. Herr, J. Gautier, S. Chabaud, P. Zrounba, D. Perol, J.Y. Blay, High mortality rate in cancer patients with symptoms of COVID-19 with or without detectable SARS-COV-2 on RT-PCR, Eur. J. Canc. 135 (2020) 251–259, https://doi.org/10.1016/j.ejca.2020.05.028.
- [78] Y.C. Li, J. Li, Y. Zhang, L.Z. Dai, L. Li, J. Liu, S. Zhang, X.Y. Wu, Y. Hu, C.F. Qin, T. Jiang, X.P. Kang, Development of an automatic integrated gene detection system for novel severe acute respiratory syndrome-related coronavirus (SARSCoV2), Emerg. Microb. Infect. 9 (2020) 1489–1496, https://doi.org/ 10.1080/22221751.2020.1782774.
- [79] P. Wang, Combination of serological total antibody and RT-PCR test for detection of SARS-COV-2 infections, J. Virol Methods 283 (2020) 113919, https://doi.org/ 10.1016/j.jviromet.2020.113919.
- [80] V.M. Corman, O. Landt, M. Kaiser, R. Molenkamp, A. Meijer, D.K. Chu, T. Bleicker, S. Brünink, J. Schneider, M.L. Schmidt, D.G. Mulders, B.L. Haagmans,

B. Van Der Veer, S. Van Den Brink, L. Wijsman, G. Goderski, J.L. Romette, J. Ellis, M. Zambon, M. Peiris, H. Goossens, C. Reusken, M.P. Koopmans, C. Drosten, Detection of 2019 novel coronavirus (2019-nCoV) by real-time RT-PCR, Euro Surveill. 25 (2020) 2000045, https://doi.org/10.2807/1560-7917. FS.2020.25.3.2000045.

- [81] X.Z. Xie, Z. Zhong, W. Zhao, C. Zheng, F. Wang, J. Liu, Chest CT for typical coronavirus disease 2019 (COVID-19) pneumonia: relationship to negative RT-PCR testing, Radiology 296 (2020) E41–E45, https://doi.org/10.1148/ radiol.2020200343.
- [82] K. Shirato, S.H. Semba, S.A. El-Kafrawy, A.M. Hassan, A.M. Tolah, I. Takayama, T. Kageyama, T. Notomi, W. Kamitani, S. Matsuyama, E.I. Azhar, Development of fluorescent reverse transcription loop-mediated isothermal amplification (RT-LAMP) using quenching probes for the detection of the Middle East respiratory syndrome coronavirus, J. Virol Methods 258 (2018) 41–48, https://doi.org/ 10.1016/j.jviromet.2018.05.006.
- [83] X.R. Lv, L. Wang, J.F. Zhang, H.Y. Zeng, X. Chen, L. Shi, H.L. Cui, X.X. He, L. C. Zhao, Rapid and sensitive detection of VBNC Escherichia coli O157: H7 in beef by PMAxx and real-time LAMP, Food Contr. 115 (2020) 107292, https://doi.org/10.1016/j.foodcont.2020.107292.
- [84] J. Kashir, A. Yaqinuddin, Loop mediated isothermal amplification (LAMP) assays as a rapid diagnostic for COVID-19, Med. Hypotheses 141 (2020), https://doi. org/10.1016/j.mehy.2020.109786.
- [85] H. Wang, F. Cong, F.W. Zeng, Y.X. Lian, X.G. Liu, M.L. Luo, P.J. Guo, J.Y. Ma, Development of a real time reverse transcription loop-mediated isothermal amplification method (RT-LAMP) for detection of a novel swine acute diarrhea syndrome coronavirus (SADS-CoV), J. Virol Methods 260 (2018) 45–48, https:// doi.org/10.1016/j.jviromet.2018.06.010.
- [86] L. Shi, X.W. Yu, W. Yao, B.L. Yu, L.K. He, Y. Gao, Y.X. Zhang, G.B. Tian, J.H. Ping, X.R. Wang, Development of a reverse-transcription loop-mediated isothermal amplification assay to detect avian influenza viruses in clinical specimens, J. Integr. Agr. 18 (2019) 1428–1435, https://doi.org/10.1016/S2095-3119(19) 62700-0.
- [87] P.F.N. Estrela, G.D.M. Mendes, K.G.D. Oliveira, A.M. Bailão, C.M.D.A. Soares, N. A. Assunção, G.R.M. Duarte, Ten-minute direct detection of Zika virus in serum samples by RT-LAMP, J. Virol Methods 271 (2019) 113675, https://doi.org/ 10.1016/j.jviromet.2019.113675.
- [88] D.W. Lai, Y.L. Zhang, Q.X. Huang, G.H. Yin, K.K. Pennerman, Z.X. Liu, A.P. Guo, Reverse transcription loop-mediated isothermal amplification to rapidly detect Rice ragged stunt virus, Saudi J. Biol. Sci. 25 (2018) 1577–1584, https://doi.org/ 10.1016/j.sjbs.2016.02.024.
- [89] D. Hu, L.N. Hao, J.H. Zhang, P.P. Yao, Q. Zhang, H. Lv, X.F. Gong, X.Z. Pan, M. Cao, J. Zhu, Y. Zhang, Y.J. Feng, C.J. Wang, Development of reverse transcription loop-mediated isothermal amplification assays to detect Hantaan virus and Seoul virus, J. Virol Methods 221 (2015) 68–73, https://doi.org/ 10.1016/j.jviromet.2015.04.017.
- [90] T.X. Ji, Z.W. Liu, G.Q. Wang, X.G. Guo, S. Akbar khan, C.C. Lai, H.Y. Chen, S. W. Huang, S.M. Xia, B. Chen, H.Y. Jia, Y.C. Chen, Q. Zhou, Detection of COVID-19: a review of the current literature and future perspectives, Biosens. Bioelectron. 15 (2020) 112455, https://doi.org/10.1016/j.bios.2020.112455.
- [91] Z.X. Fan, X. Feng, W.F. Zhang, N. Li, X.J. Zhang, J.M. Lin, Visual detection of high-risk HPV16 and HPV18 based on loop-mediated isothermal amplification, Talanta 217 (2020) 121015, https://doi.org/10.1016/j.talanta.2020.121015.
- [92] S. Guenther, S. Felten, G. Wess, K. Hartmann, K. Weber, Detection of feline Coronavirus in effusions of cats with and without feline infectious peritonitis using loop-mediated isothermal amplification, J. Virol Methods 256 (2018) 32–36, https://doi.org/10.1016/j.jviromet.2018.03.003.
 [93] H.T.C. Thai, M.Q. Le, C.D. Vuong, M. Parida, H. Minekawa, T. Notomi, F. Hasebe,
- [93] H.T.C. Thai, M.Q. Le, C.D. Vuong, M. Parida, H. Minekawa, T. Notomi, F. Hasebe, K. Morita, Development and evaluation of a novel loop-mediated isothermal amplification method for rapid detection of severe acute respiratory syndrome coronavirus, J. Clin. Microbiol. 42 (2004) 1956–1961, https://doi.org/10.1128/ JCM.42.5.1956-1961.2004.
- [94] K. Pyrc, A. Milewska, J. Potempa, Development of loop-mediated isothermal amplification assay for detection of human coronavirus-NL63, J. Virol Methods 175 (2011) 133–136, https://doi.org/10.1016/j.jviromet.2011.04.024.
- [95] Y. Kitagawa, Y. Orihara, R. Kawamura, K. Imai, J. Sakai, N. Tarumoto, M. Matsuoka, S. Takeuchi, S. Maesaki, T. Maeda, Evaluation of rapid diagnosis of novel coronavirus disease (COVID-19) using loop-mediated isothermal amplification, J. Clin. Virol. 129 (2020) 104446, https://doi.org/10.1016/j. jcv.2020.104446.
- [96] A.A.A. Al-Maskri, J.W. Ye, J. Talap, H.H. Hu, L.L. Sun, L.S. Yu, S. Cai, S. Zeng, Reverse transcription-based loop-mediated isothermal amplification strategy for real-time miRNA detection with phosphorothioated probes, Anal. Chim. Acta 1126 (2020) 1–6, https://doi.org/10.1016/j.aca.2020.06.007.
- [97] G.S. Park, K. Ku, S.H. Baek, S.J. Kim, S.I. Kim, B.T. Kim, J.S. Maeng, Development of reverse transcription loop-mediated isothermal amplification assays targeting severe acute respiratory syndrome coronavirus 2 (SARS-CoV-2), J. Mol. Diagn. 22 (2020) 729–735, https://doi.org/10.1016/j.jmoldx.2020.03.006.
- [98] C. Yan, J. Cui, L. Huang, B. Du, L. Chen, G. Xue, S. Li, W. Zhang, L. Zhao, Y. Sun, H. Yao, N. Li, H. Zhao, Y. Feng, S. Liu, Q. Zhang, D. Liu, J. Yuan, Rapid and visual detection of 2019 novel coronavirus (SARS-CoV-2) by a reverse transcription loop-mediated isothermal amplification assay, Clin. Microbiol. Infect. 26 (2020) 773–779, https://doi.org/10.1016/j.cmi.2020.04.001.
- [99] V.L.D. Thi, K. Herbst, K. Boerner, M. Meurer, L.P.M. Kremer, D. Kirrmaier, A. Freistaedter, D. Papagiannidis, C. Galmozzi, M.L. Stanifer, A colorimetric RT-LAMP assay and LAMP-sequencing for detecting SARS-CoV-2 RNA in clinical

samples, Sci. Transl. Med. 12 (2020), eabc7075, https://doi.org/10.1126/

- scitranslmed.abc7075.
 S. Klein, T.G. Müller, D. Khalid, V. Sonntag-Buck, A.M. Heuser, B. Glass, M. Meurer, I. Morales, A. Schillak, A. Freistaedter, I. Ambiel, S.L. Winter, L. Zimmermann, T. Naumoska, F. Bubeck, D. Kirrmaier, S. Ullrich, I.B. Miranda, S. Anders, D. Grimm, P. Schnitzler, M. Knop, H.G. Krausslich, V.L. Dao Thi, K. Borner, P. Chlanda, SARS-CoV-2 RNA extraction using magnetic beads for rapid large-scale testing by RT-qPCR and RT-LAMP, Viruses 12 (2020) 8, https:// doi.org/10.3390/v12080863.
- [101] C. Yan, J. Cui, L. Huang, B. Du, L. Chen, G. Xue, S. Li, W. Zhang, L. Zhao, Y. Sun, H. Yao, N. Li, H. Zhao, Y. Feng, S. Liu, Q. Zhang, D. Liu, J. Yuan, Rapid and visual detection of 2019 novel coronavirus (SARS-CoV-2) by a reverse transcription loop-mediated isothermal amplification assay, Clin. Microbiol. Infect. 26 (2020) 773–779, https://doi.org/10.1016/j.cmi.2020.04.001.
- [102] N. Ben-Assa, R. Naddaf, T. Gefen, T. Capucha, H. Haijo, N. Mandelbaum, L. Elbaum, P. Rogov, D.A. King, S. Kaplan, A. Rotem, M. Chowers, M. Szwarcwort-Cohen, M. Paul, N. Geva-Zatorsky, Direct on-the-spot detection of SARS-CoV-2 in patients, Exp. Biol. Med. 245 (2020) 1187–1193, https://doi.org/10.1177/ 1535370220941819.
- [103] X. Zhu, X.X. Wang, L.M. Han, T. Chen, L.C. Wang, H. Li, S. Li, L. He, X.Y. Fu, S. J. Chen, M. Xing, H. Chen, Y. Wang, Multiplex reverse transcription loop-mediated isothermal amplification combined with nanoparticle-based lateral flow biosensor for the diagnosis of COVID-19, Biosens, Bioelectron 166 (2020) 112437, https://doi.org/10.1016/j.bios.2020.112437.
- [104] M.J. Kellner, J.G. Koob, J.S. Gootenberg, O.O. Abudayyeh, F. Zhang, SHERLOCK: nucleic acid detection with CRISPR nucleases, Nat. Protoc. 14 (2019) 2986–3012, https://doi.org/10.1038/s41596-019-0210-2.
- [105] J. Joung, A. Ladha, M. Saito, M. Segel, R. Bruneau, M.L.W. Huang, N.G. Kim, X. Yu, J. Li, B.D. Walker, A.L. Greninger, K.R. Jerome, J.S. Gootenberg, O. O. Abudayyeh, F. Zhang, Point-of-care testing for COVID-19 using SHERLOCK diagnostics, MdeRxiv (2020), https://doi.org/10.1101/2020.05.04.20091231.
- [106] H. Khan, A. Khan, Y.F. Liu, S. Wang, S. Bibi, H.P. Xu, Y. Liu, S. Durrani, L. Jin, N. Y. He, T. Xiong, CRISPR-Cas13a mediated nanosystem for attomolar detection of canine parvovirus type 2, Chinese, Chem. Lett. 30 (2019) 2201–2204, https://doi.org/10.1016/j.cclet.2019.10.032.
- [107] T. Chaijarasphong, T. Thammachai, O. Itsathitphaisarn, K. Sritunyalucksana, R. Suebsing, Potential application of CRISPR-Cas12a fluorescence assay coupled with rapid nucleic acid amplification for detection of white spot syndrome virus in shrimp, Aquaculture 512 (2019) 734340, https://doi.org/10.1016/j. aquaculture.2019.734340.
- [108] X.J. Wang, M.T. Zhong, Y. Liu, P.X. Ma, L. Dang, Q.Z. Meng, W.W. Wan, X.D. Ma, J. Liu, G. Yang, Z.F. Yang, X.X. Huang, M. Liu, Rapid and sensitive detection of COVID-19 using CRISPR/Cas12a-based detection with naked eye readout, CRISPR/Cas12a-NER, Sci. Bull. 65 (2020) 1436–1439, https://doi.org/10.1016/j. scib.2020.04.041.
- [109] B. Koo, D.E. Kim, J. Kweon, C.E. Jin, S.H. Kim, Y. Kim, Y. Shin, CRISPR/dCas9mediated biosensor for detection of tick-borne diseases, Sensor. Actuator. B Chem. 273 (2018) 316–321. https://doi.org/10.1016/j.spb.2018.06.069.
- Chem. 273 (2018) 316–321, https://doi.org/10.1016/j.snb.2018.06.069.
 [110] O. Mukama, T. Yuan, Z.X. He, Z.Y. Li, J.D.D. Habimana, M. Hussain, W. Li, Z.J. Yi, Q.X. Liang, L.W. Zeng, A high fidelity CRISPR/Cas12a based lateral flow biosensor for the detection of HPV16 and HPV18, Sensor. Actuator. B Chem. 316 (2020) 128119, https://doi.org/10.1016/j.snb.2020.128119.
- [111] Z. Huang, D. Tian, Y. Liu, Z. Lin, C.J. Lyon, W.H. Lai, D. Fusco, A. Drouin, X. M. Yin, T. Hu, B. Ning, Ultra-sensitive and high-throughput CRISPR-p owered COVID-19 diagnosis, Biosens, Bioelectron 164 (2020) 112316, https://doi.org/10.1016/j.bios.2020.112316.
- [112] J. Joung, A. Ladha, M. Saito, M. Segel, R. Bruneau, M.L.W. Huang, N.G. Kim, X. Yu, J. Li, B.D. Walker, A.L. Greninger, K.R. Jerome, J.S. Gootenberg, O. O. Abudayyeh, F. Zhang, Point-of-care testing for COVID-19 using SHERLOCK diagnostics, MedRxiv (2020), https://doi.org/10.1101/2020.05.04.20091231.
- [113] J.P. Broughton, X.D. Deng, G.X. Yu, C.L. Fasching, V. Servellita, J. Singh, X. Miao, J.A. Streithorst, A. Granados, A. Sotomayor-Gonzalez, K. Zorn, A. Gopez, E. Hsu, W. Gu, S. Miller, C.Y. Pan, H. Guevara, D.A. Wadford, J.S. Chen, C.Y. Chiu, CRISPR-Cas12-based detection of SARS-CoV-2, Nat. Biotechnol. 38 (2020) 870, https://doi.org/10.1038/s41587-020-0513-4.
- [114] Z. Ali, R. Aman, A. Mahas, G.S. Rao, M. Tehseen, T. Marsic, R. Salunke, A. K. Subudhi, S.M. Hala, S.M. Hamdan, A. Pain, F.S. Alofi, A. Alsomali, A. M. Hashem, A. Khogeer, N.A.M. Almontashiri, M. Abedalthagafi, N. Hassan, M. M. Mahfouz, iSCAN: an RT-LAMP-coupled CRISPR-Cas12 module for rapid, sensitive detection of SARS-CoV-2, Virus Res. 288 (2020) 198129, https://doi.org/10.1016/j.virusres.2020.198129.
- [115] X.Q. Tian, D.F. Sun, Y.J. Zhang, J.Y. Fang, Microarray-based methods to identify DNA methylation in cancer, Hereditas 30 (2008) 295–303, https://doi.org/ 10.3724/sp.j.1005.2008.00295.
- [116] Y. Song, F.N. Dou, Z. Zhou, N.M. Yang, J. Zhong, J. Pan, Q.Q. Liu, J.Z. Zhang, S. Q. Wang, Microarray-based detection and clinical evaluation for Helicobacter pylori resistance to clarithromycin or levofloxacin and the genotype of CYP2C19 in 1083 patients, BioMed Res. Int. 2018 (2018) 2684836, https://doi.org/10.1155/2018/2684836.
- [117] C. Schnee, K. Sachse, DNA microarray-based detection of multiple pathogens: mycoplasma spp. and Chlamydia spp, Methods, Mol. Biol. 1247 (2015) 193–208, https://doi.org/10.1007/978-1-4939-2004-4_15.
- [118] E.A. Engel, P.F. Escobar, L.A. Rojas, P.A. Rivera, N. Fiore, P.D.T. Valenzuela, A diagnostic oligonucleotide microarray for simultaneous detection of grapevine viruses, J. Virol Methods 163 (2010) 445–451, https://doi.org/10.1016/j. jviromet.2009.11.009.

- [119] I.C.S. Ferreira, A.P. Alegretti, F.D. Paris, R.M. Paiva, V.C.B.G. Chakr, Comparison of a direct immunofluorescence assay (Oxoid IMAGEN®) and a multiplex RT-PCR DNA microarray assay (CLART® PneumoVir) for the detection of respiratory viruses in hospitalized children, J. Virol Methods 284 (2020) 113930, https://doi. org/10.1016/j.jviromet.2020.113930.
- [120] M. Nicolaisen, An oligonucleotide-based microarray for detection of plant RNA viruses, J. Virol Methods 173 (2011) 137–143, https://doi.org/10.1016/j. jviromet.2011.01.022.
- [121] X.Q. Wang, E. Dang, J.Z. Gao, S. Guo, Z. Li, Development of a gold nanoparticlebased oligonucleotide microarray for simultaneous detection of seven swine viruses, J. Virol Methods 91 (2013) 9–15, https://doi.org/10.1016/j. jviromet.2013.03.023.
- [122] X.H. Li, X. Qi, L. Miao, Y. Wang, F.Z. Liu, H.W. Gu, S.W. Lu, Y.H. Yang, F.Y. Liu, Detection and subtyping of influenza A virus based on a short oligonucleotide microarray, Diagn. Microbiol. Infect. Dis. 65 (2009) 261–270, https://doi.org/ 10.1016/j.diagmicrobio.2009.07.016.
- [123] F.R. Jin, H. Li, D.K. Xu, Enzyme-free fluorescence microarray for determination of hepatitis B virus DNA based on silver nanoparticle aggregates-assisted signal amplification, Anal. Chim. Acta 1077 (2019) 297–304, https://doi.org/10.1016/ j.aca.2019.05.066.
- [124] O. Lung, T. Furukawa-Stoffer, K. Burton Hughes, J. Pasick, D.P. King, D. Hodko, Multiplex RT-PCR and automated microarray for detection of eight bovine viruses, Transbound. Emerg. Dis. 64 (2017) 1929–1934, https://doi.org/ 10.1111/tbed.12591.
- [125] X. Guo, P. Geng, Q. Wang, B.Y. Cao, B. Liu, Development of a single nucleotide polymorphism DNA microarray for the detection and genotyping of the SARS coronavirus, J. Microbiol. Biotechnol. 24 (2014) 1445–1454, https://doi.org/ 10.4014/jmb.1404.04024.
- [126] L.K. De Souza Luna, V. Heiser, N. Regamey, M. Panning, J.F. Drexler, S. Mulangu, L. Poon, S. Baumgarte, B.J. Haijema, L. Kaiser, C. Drosten, Generic detection of coronaviruses and differentiation at the prototype strain level by reverse transcription-PCR and nonfluorescent low-density microarray, J. Clin. Microbiol. 45 (2007) 1049–1052, https://doi.org/10.1128/JCM.02426-06.
- [127] J. Hardick, D. Metzgar, L. Risen, C. Myers, M. Balansay, T. Malcom, R. Rothman, C. Gaydos, Initial performance evaluation of a spotted array Mobile Analysis Platform (MAP) for the detection of influenza A/B, RSV, and MERS coronavirus, Diagn. Microbiol. Infect. Dis. 91 (2018) 245–247, https://doi.org/10.1016/j. diagmicrobio.2018.02.011.
- [128] W.Y. Tsai, K. Driesse, J.J. Tsai, S.C. Hsieh, R. Sznajder Granat, O. Jenkins, G. J. Chang, W.K. Wang, Enzyme-linked immunosorbent assays using virus-like particles containing mutations of conserved residues on envelope protein can distinguish three flavivirus infections, Emerg. Microb. Infect. 9 (2020) 1722–1732, https://doi.org/10.1080/22221751.2020.1797540.
- [129] G. Elia, G. Fiermonte, A. Pratelli, V. Martella, M. Camero, F. Cirone, C. Buonavoglia, Recombinant M protein-based ELISA test for detection of antibodies to canine coronavirus, J. Virol Methods 109 (2003) 139–142, https:// doi.org/10.1016/S0166-0934(03)00064-8.
- [130] P.Y. Lim, M.J. Cardosa, Development of a sandwich ELISA to detect virus-likeparticles in enterovirus A71 vaccines, J. Virol Methods 270 (2019) 113–119, https://doi.org/10.1016/j.jviromet.2019.05.005.
- [131] H. Dhanze, M.S. Kumar, V. Singh, M. Gupta, K.N. Bhilegaonkar, A. Kumar, B. P. Mishra, R.K. Singh, Detection of recent infection of Japanese encephalitis virus in swine population using IgM ELISA: a suitable sentinel to predict infection in humans, J. Immunol. Methods (2020) 112848, https://doi.org/10.1016/j. jim.2020.112848.
- [132] S. Zhou, S.Y. Zhang, M.S. Wang, A.C. Cheng, D.K. Zhu, S. Chen, M.F. Liu, X. X. Zhao, R.Y. Jia, Q. Yang, Y. Wu, S.Q. Zhang, Y.Y. Liu, Y.L. Yu, L. Zhang, X. Y. Chen, Development and evaluation of an indirect ELISA based on recombinant nonstructural protein 3A to detect antibodies to duck hepatitis A virus type 1, J. Virol Methods 268 (2019) 56–61, https://doi.org/10.1016/j. jviromet.2019.03.012.
- [133] M.L. Edwards, J.I. Cooper, Plant virus detection using a new form of indirect ELISA, J. Virol Methods 11 (1985) 309–319, https://doi.org/10.1016/0166-0934 (85)90024-2.
- [134] K. Chand, S.K. Biswas, M.A. Ramakrishnan, A multi-species indirect ELISA for detection group-specific antibodies against VP7 protein of bluetongue virus, Small Rumin. Res. 180 (2019) 6–8, https://doi.org/10.1016/j. smallrumres.2019.09.019.
- [135] P.V. Hornbeck, Enzyme-linked immunosorbent assays, Curr. Protoc. Im. 110 (2015) 2, https://doi.org/10.1002/0471142735.im0201s110.
- [136] U. Kavita, Y.S. Dai, L. Salvador, W. Miller, L.P. Adam, P.C. Levesque, Y.J. Zhang, Q.C. Ji, R.C. Pillutla, Development of a chemiluminescent ELISA method for the detection of total anti-adeno associated virus serotype 9 (AAV9) antibodies, Hum. Gene Ther. Methods 29 (2018) 237–250, https://doi.org/10.1089/ hgtb.2018.131.
- [137] M. Li, L. Sun, Y.Y. Ma, D.L. Fei, M.X. Ma, Development of a sandwich ELISA for the detection of Chinese sacbrood virus infection, Arch. Virol. 165 (2020) 1551–1556, https://doi.org/10.1007/s00705-020-04634-2.
- [138] Y. Tan, G. Dong, J. Niu, Y. Guo, S. Yi, M. Sun, K. Wang, G. Hu, Development of an indirect ELISA based on glycoprotein B gene for detecting of Feline herpesvirus type 1, Pol. J. Vet. Sci. 22 (2019) 631–633, https://doi.org/10.24425/ pivs.2019.129971.
- [139] X.L. Li, H.L. Jing, X.F. Liu, Q. Wang, S.Y. Qiu, D.D. Liu, S.Q. Wu, X.M. Lin, Comparative evaluation of two commercial ELISA kits for detection of antibodies against Akabane virus in cattle serum, BMC Vet. Res. 15 (2019) 408, https://doi. org/10.1186/s12917-019-2156-6.

- [140] Y. Wang, J. Guo, S. Qiao, Q. Li, J. Yang, Q. Jin, G. Zhang, GP5 protein-based ELISA for the detection of PRRSV antibodies, Pol. J. Vet. Sci. 19 (2016) 495–501, https://doi.org/10.1515/pjvs-2016-0062.
- [141] T. Qi, Y. Hu, Z. Hu, S.H. Zhao, A. Cullinane, P. Lyons, S. Gildea, X.J. Wang, Development of an antigen-capture ELISA for the quantitation of equine arteritis virus in culture supernatant, Arch. Virol. 163 (2018) 1469–1478, https://doi.org/ 10.1007/s00705-018-3746-5.
- [142] S.A. Walper, G.L. Aragonés, K.E. Sapsford, C.W. Brown III., C.E. Rowland, J. C. Breger, I.L. Medintz, Detecting biothreat agents: from current diagnostics to developing sensor technologies, ACS Sens. 3 (2018) 1894–2024, https://doi.org/ 10.1021/acssensors.8b00420.
- [143] S. Oh, J. Kim, V.T. Tran, D.K. Lee, S.R. Ahmed, J.C. Hong, J. Lee, E.Y. Park, J. Lee, Magnetic nanozyme-linked immunosorbent assay for ultrasensitive influenza a virus detection, ACS Appl. Mater. Interfaces 10 (2018) 12534–12543, https://doi. org/10.1021/acsami.8b02735.
- [144] S. Boonkaew, S. Chaiyo, S. Jampasa, S. Rengpipat, W. Siangproh, O. Chailapakul, An origami paper-based electrochemical immunoassay for the C-reactive protein using a screen-printed carbon electrode modified with graphene and gold nanoparticles, Microchimi. Acta. 186 (2019) 153, https://doi.org/10.1007/ s00604-019-3245-8.
- [145] M. Gast, H. Sobek, B. Mizaikoff, Advances in imprinting strategies for selective virus recognition a review, Trac. Trends Anal. Chem. 114 (2019) 218–232, https://doi.org/10.1016/j.trac.2019.03.010.
- [146] M.Z.H. Khan, M.R. Hasan, S.I. Hossain, M.S. Ahommed, M. Daizya, Ultrasensitive detection of pathogenic viruses with electrochemical biosensor: state of the art, Biosens. Bioelectron. 166 (2020) 112431, https://doi.org/10.1016/j. bios.2020.112431.
- [147] A.D. Chowdhury, K. Takemura, T.C. Li, T. Suzuki, E.Y. Park, Electrical pulseinduced electrochemical biosensor for hepatitis E virus detection, Nat. Commun. 10 (2019) 3737, https://doi.org/10.1038/s41467-019-11644-5.
- [148] H. Ilkhani, S. Farhad, A novel electrochemical DNA biosensor for Ebola virus detection, Anal. Biochem. 557 (2018) 151–155, https://doi.org/10.1016/j. ab.2018.06.010.
- [149] A. George, M.S. Amrutha, P. Srivastava, V.V.R. Sai, S. Sunil, R. Srinivasan, Labelfree detection of chikungunya non-structural protein 3 using electrochemical impedance spectroscopy, J. Electrochem. Soc. 166 (2019) B1356–B1363, https:// doi.org/10.1149/2.1081914jes.
- [150] M. Manzano, S. Viezzi, S. Mazerat, R.S. Marks, J. Vidic, Rapid and label-free electrochemical DNA biosensor for detecting hepatitis A virus, Biosens. Bioelectron. 100 (2018) 89–95, https://doi.org/10.1016/j.bios.2017.08.043.
- [151] H.Y. Que, D.C. Zhang, B. Guo, T. Wang, H.P. Wu, D.B. Han, Y.R. Yan, Label-free and ultrasensitive electrochemical biosensor for the detection of EBV-related DNA based on AgDNCs@DNA/AgNCs nanocomposites and lambda exonucleaseassisted target recycling, Biosens. Bioelectron. 143 (2019) 111610, https://doi. org/10.1016/j.bios.2019.111610.
- [152] N.S. Heo, S. Zheng, M. Yang, S.J. Lee, S.Y. Lee, H.J. Kim, J.Y. Park, C.S. Lee, T. J. Park, Label-free electrochemical diagnosis of viral antigens with genetically engineered fusion protein, Sensors 12 (2012) 10097–10108, https://doi.org/ 10.3390/s120810097.
- [153] J.Y. Huang, J. Meng, S.H. Chen, S.Y. Zhang, T. Liu, C. Li, F. Wang, A soft metal-polyphenol capsule-based ultrasensitive immunoassay for electrochemical detection of Epstein-Barr (EB) virus infection, Biosens. Bioelectron. 164 (2020) 112310, https://doi.org/10.1016/j.bios.2020.112310.
 [154] M. Silvestrini, L. Fruk, L.M. Moretto, P. Ugo, Detection of DNA hybridization by
- [154] M. Silvestrini, L. Fruk, L.M. Moretto, P. Ugo, Detection of DNA hybridization by methylene blue electrochemistry at activated nanoelectrode ensembles, J. Nanosci. Nanotechnol. 15 (2015) 3437–3442, https://doi.org/10.1166/ jnn.2015.10214.
- [155] T.L. Kamikawa, M.G. Mikolajczyk, M. Kennedy, P. Zhang, W. Wang, D.E. Scott, E. C. Alocilja, Nanoparticle-based biosensor for the detection of emerging pandemic influenza strains, Biosens. Bioelectron. 26 (2010) 1346–1352, https://doi.org/10.1016/j.bios.2010.07.047.
- [156] L. Krejcova, D. Huska, D. Hynek, P. Kopel, V. Adam, J. Hubalek, L. Trnkova, R. Kizek, Using of paramagnetic microparticles and quantum dots for isolation and electrochemical detection of influenza viruses' specific nucleic acids, Int. J. Electrochem. Sc. 8 (2013) 689–702, https://doi.org/10.1109/ WCICA.2006.1712399.
- [157] Y.T. Liu, J. Deng, X.L. Xiao, L. Ding, Y.L. Yuan, H. Li, X.T. Li, X.N. Yan, L.L. Wang, Electrochemical sensor based on a poly (para-aminobenzoic acid) film modified glassy carbon electrode for the determination of melamine in milk, Electrochem. Acta. 56 (2011) 4595-4602, https://doi.org/10.1016/j.electacta.2011.02.088.
 [158] L.M. Zhou, J.S. Huang, B. Yu, Y. Liu, T.Y. You, A novel electrochemiluminescence
- [158] L.M. Zhou, J.S. Huang, B. Yu, Y. Liu, T.Y. You, A novel electrochemiluminescence immunosensor for the analysis of HIV-1 p24 antigen based on P-RGO@Au@Ru-SiO₂ composite, ACS Appl. Mater. Interfaces 7 (2015) 24438–24445, https://doi. org/10.1021/acsami.5b08154.
- [159] K. Kor, K. Zarei, Development and characterization of an electrochemical sensor for furosemide detection based on electropolymerized molecularly imprinted polymer, Talanta 146 (2016) 181–187, https://doi.org/10.1016/j. talanta.2015.08.042.
- [160] N.S. Heo, S. Zheng, M.H. Yang, S.J. Lee, S.Y. Lee, H.J. Kim, J.Y. Park, C.S. Lee, T. J. Park, Label-free electrochemical diagnosis of viral antigens with genetically engineered fusion protein, Sensors 12 (2012) 10097–10108, https://doi.org/ 10.3390/s120810097.
- [161] L.A. Layqah, S. Eissa, An electrochemical immunosensor for the corona virus associated with the Middle East respiratory syndrome using an array of gold nanoparticle-modified carbon electrodes, Mikrochim. Acta 186 (2019) 224, https://doi.org/10.1007/s00604-019-3345-5.

- [162] Z.T. Li, Y.X. Yi, X.M. Luo, N.A. Xiong, Y. Liu, S.Q. Li, R.L. Sun, Y.Q. Wang, B. C. Hu, W. Chen, Y.C. Zhang, J. Wang, B.F. Huang, Y. Lin, J.S. Yang, W.S. Cai, X. F. Wang, J. Cheng, Z.Q. Chen, K.J. Sun, W.M. Pan, Z.F. Zhan, L.Y. Chen, F. Ye, Development and clinical application of a rapid IgM-IgG combined antibody test for SARS-CoV-2 infection diagnosis 92 (2020) 1518–1524, https://doi.org/10.1002/jmv.25727.
- [163] Z.T. Li, Y.X. Yi, X.M. Luo, N. Xiong, Y. Liu, S.Q. Li, R.L. Sun, Y.Q. Wang, B.C. Hu, W. Chen, Y.C. Zhang, J. Wang, B.F. Huang, Y. Lin, J.S. Yang, W.S. Cai, X.F. Wang, J. Cheng, Z.Q. Chen, K.J. Sun, W.M. Pan, Z.F. Zhan, L.Y. Chen, F. Ye, Development and clinical application of A rapid IgM-IgG combined antibody test for SARS-CoV-2 infection diagnosis, J. Med. Virol. 92 (2020) 1518–1524, https:// doi.org/10.1002/jmv.25727.
- [164] J.H. Bong, H.R. Kim, J.W. Yoo, M.J. Kang, M.G. Shin, J.S. Lee, W.B. Shim, S. D. Lee, J.C. Pyun, One-step immunoassay without washing steps for influenza A virus detection using ISFET, Biosens. Bioelectron. 165 (2020) 112341, https://doi.org/10.1016/j.bios.2020.112341.
- [165] T.A. Freitas, C.A. Proença, T.A. Baldo, E.M. Materón, A. Wong, R.F. Magnani, R. C. Faria, Ultrasensitive immunoassay for detection of Citrus tristeza virus in citrus sample using disposable microfluidic electrochemical device, Talanta 205 (2019) 120110, https://doi.org/10.1016/j.talanta.2019.07.005.
- [166] R. Selvarajan, P.S. Kanichelvam, V. Balasubramanian, S.S. Subramanian, A rapid and sensitive lateral flow immunoassay (LFIA) test for the on-site detection of banana bract mosaic virus in banana plants, J. Virol Methods 284 (2020) 113929, https://doi.org/10.1016/j.jviromet.2020.113929.
- [167] K. Nishiyama, Y. Takeda, M. Maeki, A. Ishida, H. Tani, K. Shigemura, A. Hibara, Y. Yonezawa, K. Imai, H. Ogawa, M. Tokeshi, Rapid detection of anti-H5 avian influenza virus antibody by fluorescence polarization immunoassay using a portable fluorescence polarization analyzer, Sensor. Actuator. B Chem. 316 (2020) 128160, https://doi.org/10.1016/j.snb.2020.128160.
- [168] M. Xiao, K.X. Xie, X.H. Dong, L. Wang, C.H. Huang, F. Xu, W. Xiao, M.L. Jin, B. Y. Huang, Y. Tang, Ultrasensitive detection of avian influenza A (H7N9) virus using surface-enhanced Raman scattering-based lateral flow immunoassay strips, Anal. Chim. Acta 1053 (2019) 139–147, https://doi.org/10.1016/j. aca.2018.11.056.
- [169] A. Mairesse, J. Favresse, C. Eucher, M. Elsen, M. Tré-Hardy, C. Haventith, D. Gruson, J. Dogné, J. Douxfils, P. Göbbels, High clinical performance and quantitative assessment of antibody kinetics using a dual recognition assay for the detection of SARS-CoV-2 IgM and IgG antibodies, Clin. Biochem. (2020), https:// doi.org/10.1016/j.clinbiochem.2020.08.009.
- [170] N. Kohmer, S. Westhaus, C. Rühl, S. Ciesek, H.F. Rabenau, Brief clinical evaluation of six high-throughput SARS-CoV-2 IgG antibody assays, J. Clin. Virol. 129 (2020) 104480, https://doi.org/10.1016/j.jcv.2020.104480.
- [171] W.B. Liu, G.M. Kou, Y.Y. Dong, Y.Q. Zheng, Y.J. Ding, W.X. Ni, W.L. Wu, S. Tang, Z. Xiong, Y. Zhang, L. Liu, S.G. Zheng, Clinical application of chemiluminescence Microparticle immunoassay for SARS-CoV-2 infection diagnosis, J. Clin. Virol. 130 (2020) 104576, https://doi.org/10.1016/j.jcv.2020.104576.
- [172] I. Montesinos, D. Gruson, B. Kabamba, H. Dahma, S.V. Den Wijngaert, S. Reza, V. Carbone, O. Vandenberg, B. Gulbis, F. Wolff, H. Rodriguez-Villalobos, Evaluation of two automated and three rapid lateral flow immunoassays for the detection of anti-SARS-CoV-2 antibodies, J. Clin. Virol. 128 (2020) 104413, https://doi.org/10.1016/j.jcv.2020.104413.
- [173] J. Qi, B.W. Li, N. Zhou, X.Y. Wang, D.M. Deng, L.Q. Luo, L.X. Chen, The strategy of antibody-free biomarker analysis by in-situ synthesized molecularly imprinted polymers on movable valve paper-based device, Biosens. Bioelectron. 142 (2019) 111533, https://doi.org/10.1016/j.bios.2019.111533.
- [174] B. Yang, H. Gong, C.Y. Chen, X.M. Chen, C.Q. Cai, A virus resonance light scattering sensor based on mussel-inspired molecularly imprinted polymers for high sensitive and high selective detection of Hepatitis A Virus, Biosens. Bioelectron. 87 (2017) 679–685, https://doi.org/10.1016/j.bios.2016.08.087.
- [175] J. Mandli, A. Attar, M.M. Ennaji, A. Amine, Indirect competitive electrochemical immunosensor for hepatitis A virus antigen detection, Electroanal. Chem. 799 (2017) 213–221, https://doi.org/10.1016/j.jelechem.2017.05.047.
- (2017) 213–221, https://doi.org/10.1016/j.jelechem.2017.05.047.
 [176] Y. Liu, T. Shen, L. Hu, H. Gong, C.Y. Chen, X.M. Chen, C.Q. Cai, Development of a thermosensitive molecularly imprinted polymer resonance light scattering sensor for rapid and highly selective detection of hepatitis A virus in vitro, Sensor. Actuator. B Chem. 253 (2017) 1188–1193, https://doi.org/10.1016/j. snb.2017.07.166.
- [177] Y. Ma, X.L. Shen, Q. Zeng, H.S. Wang, L.S. Wang, A multi-walled carbon nanotubes based molecularly imprinted polymers electrochemical sensor for the sensitive determination of HIV-p24, Talanta 164 (2007) 121–127, https://doi. org/10.1016/j.talanta.2016.11.043.
- [178] L.D. Bolisay, J.N. Culver, P. Kofinas, Molecularly imprinted polymers for tobacco mosaic virus recognition, Biomaterials 27 (2006) 4165–4168, https://doi.org/ 10.1016/j.biomaterials.2006.03.018.
- [179] Y.J. Yu, Q. Zhang, J. Buscaglia, C.C. Chang, Y. Liu, Z.H. Yang, Y.C. Guo, Y. T. Wang, K. Levon, M. Rafailovich, Quantitative real-time detection of carcinoembryonic antigen (CEA) from pancreatic cyst fluid using 3-D surface molecular imprinting, Analyst 141 (2016) 4424–4431, https://doi.org/10.1039/ c6an00375c.
- [180] Y.J. Yu, Q. Zhang, C.C. Chang, Y. Liu, Z.H. Yang, Y.C. Guo, Y.T. Wang, D. K. Galanakis, K. Levon, M. Rafailovich, Design of a molecular imprinting biosensor with multi-scale roughness for detection across a broad spectrum of biomolecules, Analyst 141 (2016) 5607–5617, https://doi.org/10.1039/ c6an01157h.
- [181] V. Ricotta, Y.J. Yu, N. Clayton, Y.C. Chuang, Y.T. Wang, S. Mueller, K. Levon, M. Simon, M. Rafailovich, A chip-based potentiometric sensor for a Zika virus

J. Bu et al.

diagnostic using 3D surface molecular imprinting, Analyst 144 (2019) 4266–4280, https://doi.org/10.1039/c9an00580c.

- [182] A. Jahanban-Esfahlan, L. Roufegarinejad, R. Jahanban-Esfahlan, M. Tabibiazar, R. Amarowicz, Latest developments in the detection and separation of bovine serum albumin using molecularly imprinted polymers, Talanta 207 (2020) 120317, https://doi.org/10.1016/j.talanta.2019.120317.
- [183] J.X. Guo, Y.Z. Wang, Y.J. Liu, C.J. Zhang, Y.G. Zhou, Magnetic-graphene based molecularly imprinted polymer nanocomposite for the recognition of bovine hemoglobin, Talanta 144 (2015) 411–419, https://doi.org/10.1016/j. talanta.2015.06.057.
- [184] P.Y. He, H.J. Zhu, Y. Ma, N. Liu, X.H. Niu, M.B. Wei, J.M. Pan, Rational design and fabrication of surface molecularly imprinted polymers based on multiboronic acid sites for selective capture glycoproteins, Chem. Eng. J. 367 (2019) 55–63, https://doi.org/10.1016/j.cej.2019.02.140.
- [185] H.Q. Guo, Y. Liu, W.T. Ma, L.S. Yan, K.X. Li, S. Lin, Surface molecular imprinting on carbon microspheres for fastand selective adsorption of perfluorooctane sulfonate, J. Hazard Mater. 348 (2018) 29–38, https://doi.org/10.1016/j. jhazmat.2018.01.018.
- [186] D. Rahangdale, A. Kumar, Chitosan as a substrate for simultaneous surface imprinting of salicylic acid and cadmium, Carbohydr. Polym. 202 (2018) 334–344, https://doi.org/10.1016/j.carbpol.2018.08.129.
- [187] Y.H. Sun, Y.Q. Li, J.F. Xu, L. Huang, T.Y. Qiu, S.A. Zhong, Interconnectivity of macroporous molecularly imprinted polymers fabricated by hydroxyapatitestabilized Pickering high internal phase emulsions-hydrogels for the selective recognition of protein, Colloids Surf. B Biointerfaces 155 (2017) 142–149, https://doi.org/10.1016/j.colsurfb.2017.04.009.
- [188] Y.H. Sun, S.A. Zhong, Nanoscale trifunctional bovine hemoglobin for fabricating molecularly imprinted polydopamine via Pickering emulsions-hydrogels polymerization, Colloids Surf. B Biointerfaces 159 (2017) 131–138, https://doi. org/10.1016/j.colsurfb.2017.07.069.
- [189] Y.H. Sun, S.A. Zhong, Molecularly imprinted polymers fabricated via Pickering emulsions stabilized solely by food-grade casein colloidal nanoparticles for selective protein recognition, Anal. Bioanal. Chem. 410 (2018) 3133–3143, https://doi.org/10.1007/s00216-018-1006-x.
- [190] X.Y. Wang, S.M. Yu, J.R. Wang, J.L. Yu, M. Arabi, L.W. Fu, B.W. Li, J.H. Li, L. X. Chen, Fluorescent nanosensor designing via hybrid of carbon dots and postimprinted polymers for the detection of ovalbumin, Talanta 211 (2020) 120727, https://doi.org/10.1016/j.talanta.2020.120727.
- [191] S. Klangprapan, B. Choke-Arpornchai, P.A. Lieberzeit, K. Choowongkomon, Sensing the classical swine fever virus with molecularly imprinted polymer on

quartz crystal microbalance, Heliyon 6 (2020), e04137, https://doi.org/10.1016/j.heliyon.2020.e04137.

- [192] J.Y. Yang, W.B. Feng, K.S. Liang, C.Y. Chen, C.Q. Cai, A novel fluorescence molecularly imprinted sensor for Japanese encephalitis virus detection based on metal organic frameworks and passivation-enhanced selectivity, Talanta 212 (2020) 120744, https://doi.org/10.1016/j.talanta.2020.120744.
- [193] L.H. Luo, J.Y. Yang, K.S. Liang, C.Y. Chen, X.M. Chen, C.Q. Cai, Fast and sensitive detection of Japanese encephalitis virus based on a magnetic molecular imprinted polymer-resonance light scattering sensor, Talanta 202 (2019) 21–26, https:// doi.org/10.1016/j.talanta.2019.04.064.
- [194] X.N. Zhang, H. Liu, J. Kang, X.H. Zhu, W. Peng, H. Zhou, S.A. Zhong, Y. Wang, The synthesis of temperature-sensitive molecularly imprinted film on support beads and its application for bovine serum albumin separation, Colloids Surf., A 504 (2016) 367–375, https://doi.org/10.1016/j.colsurfa.2016.05.102.
- [195] H.Z. Lu, C.W. Yu, Y. Zhang, S.F. Xu, Efficient core shell structured dual response ratiometric fluorescence probe for determination of H₂O₂ and glucose via etching of silver nanoprisms, Anal. Chim. Acta 1048 (2019) 178–185, https://doi.org/ 10.1016/j.aca.2018.10.025.
- [196] H.Z. Lu, S.F. Xu, J.Q. Liu, One pot generation of blue and red carbon dots in one binary solvent system for dual channel detection of Cr³⁺ and Pb²⁺ Based on Ion Imprinted Fluorescence Polymers, ACS Sens. 4 (2019) 1917–1924, https://doi. org/10.1021/acssensors.9b00886.
- [197] Z.N. Wei, H.Q. Li, S.B. Liu, W. Wang, H.L. Chen, L.H. Xiao, C.L. Ren, X.G. Chen, Carbon dots as fluorescent/colorimetric probes for real-time detection of hypochlorite and ascorbic acid in cells and body fluid, Anal. Chem. 91 (2019) 15477–15483, https://doi.org/10.1021/acs.analchem.9b03272.
- [198] C.L. Jiang, B.H. Liu, M.Y. Han, Z.P. Zhang, Fluorescent nanomaterials for colormultiplexing test papers toward qualitative/quantitative assays, Small. Methods. 2 (2018) 1700379, https://doi.org/10.1002/smtd.201700379.
- [199] Y.Q. Cai, J.H. You, Z.Y. You, F. Dong, S.H. Du, L.Y. Zhang, Profuse colorevolution-based fluorescent test paper sensor for rapid and visual monitoring of endogenous Cu²⁺ in human urine, Biosens. Bioelectron. 99 (2018) 332–337, https://doi.org/10.1016/j.bios.2017.07.072.
- [200] Q. Yang, J.H. Li, X.Y. Wang, H. Xiong, L.X. Chen, Ternary emission of a blue-, green-, and red-based molecular imprinting fluorescence sensor for the multiplexed and visual detection of bovine hemoglobin, Anal. Chem. 91 (2019) 6561–6568, https://doi.org/10.1021/acs.analchem.9b00082.
- [201] L.H. Luo, F. Zhang, C.Y. Chen, C.Q. Cai, Visual simultaneous detection of hepatitis A and B viruses based on a multifunctional molecularly imprinted fluorescence sensor, Anal. Chem. 91 (2019) 15748–15756, https://doi.org/10.1021/acs. analchem.9b04001.