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Multiscale ATUM-FIB Microscopy Enables Targeted Ultrastructural Analysis at Isotropic Resolution



Georg Kislinger, Helmut Gnägi, Martin Kerschensteiner, Mikael Simons, Thomas Misgeld, Martina Schifferer

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martina.schifferer@dzne.de

HIGHLIGHTS

Fast nanometerresolution relocation and 3D imaging of preselected structures

Transparent tape-based multiscale light and volume electron microscopy

Heated ultramicrotomy at $2-10 \ \mu m$ with precured epoxy resin

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Multiscale ATUM-FIB Microscopy Enables Targeted Ultrastructural Analysis at Isotropic Resolution



Georg Kislinger,^{1,2,3} Helmut Gnägi,⁴ Martin Kerschensteiner,^{2,5,6} Mikael Simons,^{1,2,3} Thomas Misgeld,^{1,2,3} and Martina Schifferer^{1,2,7,*}

SUMMARY

Volume electron microscopy enables the ultrastructural analysis of biological tissue. Currently, the techniques involving ultramicrotomy (ATUM, ssTEM) allow large fields of view but afford only limited z-resolution, whereas ion beam-milling approaches (FIB-SEM) yield isotropic voxels but are restricted in volume size. Now we present a hybrid method, named ATUM-FIB, which combines the advantages of both approaches. ATUM-FIB is based on serial sectioning of tissue into "semithick" (2–10 μ m) sections collected onto tape. Serial light and electron microscopy allows the identification of regions of interest that are then directly accessible for targeted FIB-SEM. The set of semithick sections thus represents a tissue "library" which provides three-dimensional context information that can be probed "on demand" by local high-resolution analysis. We demonstrate the potential of this technique to reveal the ultrastructure of rare but pathologically important events by identifying microglia contact sites with amyloid plaques in a mouse model of familial Alzheimer's disease.

INTRODUCTION

Since the completion of the first connectomics dataset (White et al., 1986) volume electron microscopy (EM) techniques have been substantially refined and advanced. Although the interest in deciphering neuronal networks was the major driving force behind these technological developments, three-dimensional (3D) ultrastructural analysis has attracted considerable recent attention in a wide range of biological fields (Titze and Genoud, 2016). Applications range from classical cell biological questions to developmental biology, neuro- and cancer biology, botany, and microbiology (Karreman et al., 2014). Currently, 3D ultrastructure can be solved by destructive techniques including serial block-face electron microscopy (SB-SEM) (Mikula and Denk, 2015; Denk and Horstmann, 2004; Helmstaedter et al., 2013; Briggman et al., 2011) or focused ion beam-scanning electron microscopy (FIB-SEM) (Sonomura et al., 2013; Knott et al., 2008; Heymann et al., 2006). Although these methods benefit from high alignment accuracy, they lack the option of reacguisition and hierarchical imaging (Kornfeld and Denk, 2018). Alternatively, serial sectioning for transmission electron microscope camera array (TEMCA) (Lee et al., 2016; Bock et al., 2011; Zheng et al., 2018) or automated tape-collecting ultramicrotomy (ATUM) (Hayworth et al., 2014; Kasthuri et al., 2015; Mikula and Denk, 2015; Schalek et al., 2011; Tomassy et al., 2014; Hildebrand et al., 2017; Morgan et al., 2016; Terasaki et al., 2013) allow repetitive acquisition of regions of interest. However, as ultramicrotomy-based approaches are limited by their poor maximal z resolution of 30 nm, ion-milling techniques are required, if isotropic high-resolution voxels are needed. Still, the imaging volume in FIB-SEM is limited to a few tens of microns owing to the accumulation of milling artifacts caused by high-energy gallium ions (Xu et al., 2017). Despite recent advances in the application of alternative milling strategies (Kornfeld and Denk, 2018), targeted imaging is still required to restrict the acquisition volume. This is mainly achieved by correlated workflows involving targeted trimming guided by endogenous (Luckner et al., 2018) and artificial landmarks (Bishop et al., 2011; Karreman et al., 2014, 2016; Villani et al., 2019). X-ray micro computed tomography (microCT) (Villani et al., 2019; Karreman et al., 2014; Bushong et al., 2015; Sengle et al., 2012) has emerged as a tool for facilitated region of interest (ROI) relocation within the processed EM sample. This not only bridges multiple scales, from millimeter to micrometer dimensions, but also puts the site of interest into a broader morphological context (Maire and Withers, 2014). However, so far, microCT imaging options are not commonly accessible and the technique only provides a map for subsequent guided

¹German Center for Neurodegenerative Diseases (DZNE), Munich 81377, Germany

²Munich Cluster of Systems Neurology (SyNergy), Munich 81377, Germany

³Institute of Neuronal Cell Biology, Technical University Munich, Munich 80802, Germany

⁴Diatome SA, Helmstrasse 1, 2560 Nidau, Switzerland

⁵Institute of Clinical Neuroimmunology, University Hospital, Ludwig-Maximilians-University Munich, Planegg-Martinsried 82152, Germany

⁶Biomedical Center (BMC), Faculty of Medicine, Ludwig-Maximilians-University Munich, Planegg-Martinsried 82152, Germany

⁷Lead Contact

*Correspondence: martina.schifferer@dzne.de https://doi.org/10.1016/j.isci. 2020.101290

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Figure 1. Principle of ATUM-FIB as a Hybrid Volume EM Approach

Schematic of existing techniques for targeted volume SEM and comparison with the new ATUM-FIB approach (middle). Both ATUM and ATUM-FIB are microtomy-based, but ATUM-FIB generates semithick sections that can be selected by serial section light microscopy and SEM and subjected to further FIB-SEM investigation.

destructive sample preparation. An alternative prescreening of embedded tissue at a larger scale is implemented by rendering it accessible to light and electron microscopy (EM) modalities. Ultrathick sectioning at 10 to 20 μ m thickness by the hot knife method produces samples that are accessible to large-scale FIB-SEM (Hayworth et al., 2015; Luckner and Wanner, 2018) enabling seamless reconstruction of large tissue blocks. Although this method was designed for a complete reconstruction of big volumes, it would be desirable to reduce time and data load for biological questions that require targeted ultrastructural analysis.

Here, we developed a multiscale method for targeted FIB-SEM on semithick (2–10 µm) sections named ATUM-FIB. Our method combines the advantages of both ultramicrotomy-based and serial block face imaging approaches. This approach is based on the ultramicrotomy of partially cured (Droz et al., 1975) resinembedded samples facilitated by a custom-built diamond knife with temperature control. Serial thick sections are then collected onto carbon nanotube (CNT) tape (Kubota et al., 2018), compatible with both serial bright-field and scanning electron microscopy (SEM). While providing direct physical access to isotropic high-resolution imaging of multiple ROIs by FIB-SEM, this method simultaneously provides 3D tissue context information and allows archiving samples for future extended analysis.

RESULTS

Semithick Sections Provide Suitable Information Content for Sparse Ultramicrotomy-Guided Targeting

Here, we developed a method that allows the search for an ultrastructural feature within a volume and the subsequent acquisition of a defined isotropic volume by FIB-SEM (Figure 1). Our goal was to expose surfaces at defined distances by serial sectioning. Although traditional ultrathin sectioning combined with sparse imaging saves imaging time, it is not compatible with the investigation of isotropic volumes. As the information content for FIB-SEM increases with section thickness, we explored whether "semithick" sections ranging from 2 to 10 μ m would optimize ultramicrotomy time as well as screening efficiency (Figure 2A). Moreover, we aimed to apply water instead of an oil bath (as used in the ultrathick partitioning approach [Hayworth et al., 2015]) in order to avoid additional re-embedding and sectioning.

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Figure 2. Targeting Regions of Interest by Semithick Sectioning

(A) Cartoon of the information content of BSD surface imaging and the potential FIB-SEM analysis of sections of different thickness.

(B and C) (B) Transmitted light and (C) BSD images of semithin 0.5-µm and semithick 2-, 5-, and 10-µm sections of mouse brain tissue. cc, corpus callosum; ct, cortex; CA1, hippocampus CA1. Arrowheads indicate cracks, mainly in heavily stained tissue (corpus callosum). Scale bars 100 µm (top), 10 µm (bottom).

(D) Consecutive (upper, lower row) semithick (2, 5, 10 μ m) sections allow tracing cell bodies and blood vessels across sections. Somata and blood vessels that can be followed from one to the next section are colored blue; others are shown in orange. Black scale bar 10 μ m; white scale bars 2 (left), 5 (middle), and 10 μ m (right). See Figure S1 for similarity of opposing surfaces of consecutive sections.

Semithick sections (0.5–10 μ m) were generated using a diamond knife. Carbon nanotube (CNT) tape was chosen as a conductive and transparent section support for sequential light and electron microscopic assessment (Kubota et al., 2018). The tape strings with sections were placed onto a glass slide on a heating plate (60°C). A drop of water helped to adhere the strings flat on the glass slide and enable imaging with a slide scanner (Figure 2B). Transmitted light investigation was only possible for sections below 5 μ m thickness, as in thicker sections reduced transparency masked morphological details. The sections were transferred onto a silicon wafer, and the surface was scanned by backscattered detection SEM (BSD), which enables the exploration of the entire semithick section range (Figure 2C). We generated two consecutive sections with 2, 5, and 10 μ m thickness and looked at traceability of neuronal cell bodies and blood vessels. Although most of the structures could be recognized on the next 2- μ m-thick section, alignment between two sections was difficult at thicknesses above 5 μ m (Figure 2D). In summary, combined light microscopy and SEM with maximal FIB-SEM information content is optimal at 2 μ m thickness, whereas electron microscopy is possible at 2–5 μ m thickness depending on the needed alignment precision of the biological structure of interest.

Sequential Resin Curing and Heating Enables Semithick Sectioning and FIB Milling on the Same Sample

Diamond knives and resins have been successfully applied for ultrathin sectioning for decades. In order to routinely generate smooth surfaces by ultramicrotomy of serial sections with thickness of 2 µm or more, we speculated that the optimization of resin characteristics and ultramicrotomy parameters would be necessary. We therefore explored different contrasting methods and resins for semithick sectioning and subseguent SEM imaging. First, for contrasting, we settled on a standard rOTO (reduced osmium thiocarbohydrazide osmium) protocol without lead aspartate impregnation (Hua et al., 2015). Leaving out some heavy metal preembedding staining (e.g., in a rO protocol) would entail the need for post-contrasting strategies like the incubation in uranylacetate in ethanol at 60°C for 2–24 h (Locke and Krishnan, 1971). However, postcontrasting strategies carry the risk of uneven stain distribution within and between thick sections (Hayworth et al., 2015), so we avoided them (Table 1). Second, based on the rOTO stain, we optimized the resin choice as resin and contrasting requirements for thick sectioning and ion milling are conflicting: for semithick sectioning, softer resin and less heavy metal staining would be favored, whereas FIB-SEM requires hard resin and good contrasting to avoid charging artifacts. Various methacrylate (Norris et al., 2017) as well as epoxy resins including epon and durcupan (Hayworth et al., 2015) have been used for standard ultrathin serial sectioning. We investigated rOTO-processed mouse cortex samples embedded in different resins by semithick sectioning and subsequent backscattered detection SEM (Figure 3A). Regarding the sectioning characteristics, epon formulations as well as durcupan, which would be preferable for FIB-SEM (Xu et al., 2017), showed uneven surface topology at thicknesses above 1 µm (Figure 3A). Tissue embedded in epoxy resin LX112-embedded tissue could be sectioned up to 2-µm thickness without major surface defects (Figure 3A). LX112 resin (Ladd Research Industries) has been used for serial sectioning and is a replacement for Epon 812, which is not commercially available anymore (Ellis, 2014; Kizilyaprak et al., 2015). We reasoned that a two-step curing (Droz et al., 1975) would yield in resin characteristics that are optimal for both sectioning and FIB milling. Tissue embedded in LX112 was precured at 60°C for 10 and 48 h. Semithick sections of up to $10-\mu m$ thickness could be generated from the 10-h-cured blocks (Figure 3A). After shorter curing periods, resin blocks were too soft and sticky for sectioning (data not shown). Following ultramicrotomy, sections were post-cured for 2 days at 60°C ensuring the beam resistance required for both serial SEM and FIB-SEM imaging. Still, semithick sectioning proved difficult even in this softer pre-cured resin, therefore we explored a "hot knife" approach (Hayworth et al., 2015).

In order to facilitate semithick sectioning, we established a heated diamond knife (Figure 3B) approach. We drilled holes into the 35° and 45° knife boats to insert a temperature sensor (3 mm diameter) and a heater

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Reagent	Temperature	Microwave Protocol			Bench Protocol
		Time	Vacuum	Power (On-Off-On)	Time
0.1 M cacodylate buffer	23°C	3 × 10 min	off	250 W	3 × 10 min
2% osmium tetroxide, 2.5% potassium hexacyanoferrate in 0.1 M cacodylate buffer	23°C	6 × 1 min	on	300 W	2 h
	23°C	1h (shaker)	-	-	
0.1 M cacodylate buffer	23°C	2 × 10 min	off	250 W	2 × 10 min
Water	23°C	1 min	on	250 W	10 min
1% TCH	40°C	25 min	on	200 W	45 min
Water	23°C	3 × 10 min	on	-	3 × 10min
2% osmium tetroxide in water	23°C	6 × 1 min	on	300 W	2 h
	23°C	1h (shaker)	-	-	
Water	23°C	3 × 10 min	on	-	3 × 10min
1% uranylacetate in water	4°C	over night	-	-	over night
	50°C	2 h	-	-	2 h
Water	23°C	1 min	on	250 W	10 min
15, 30, 40, 50, 60, 70, 80, 90, 100, 100, 100% ethanol	23°C	1 min each	off	200 W	10 min each
25, 50, 75, 90% LX112	23°C	10 min	on	250 W	
100% LX112	23°C	10 min	on	250 W	over night
	23°C	over night	-	-	
100% LX112	23°C	10 min	on	250 W	3-6 h
	23°C	3-6 h	-	-	
Curing	60°C	10, 48 h			10, 48 h

Table 1. En bloc Embedding Protocol

(6 mm diameter). For further temperature stability of the sample itself, we installed infrared lights at both sides and adjusted the distance to the ultramicrotome sample arm to yield a sample temperature of 40°C (Figure 3B). At temperatures above 40°C, water evaporated onto the sample block, and consequently, the resin partially melted (data not shown). We compared sectioning of rOTO processed mouse cortex precured for 10 h in LX112 at 0.5- to 10- μ m thickness at room temperature, 30°C, and 40°C. Higher temperatures increased the smoothness of the section surface (Figure 3A). Surfaces in cortical areas with cell bodies and non-myelinated neurites were smooth, whereas myelinated axons and other heavily stained structures, e.g., the corpus callosum, showed some remaining cracks (Figures 2C and 3A). At higher temperatures, the water pumping system supplying the knife boat had to be adapted to increased flow rates to compensate increased evaporation. Therefore, a good compromise for serial sectioning were temperatures in the range of 35°C-40°C. Comparison of 35° ultra-with 45° ultra-knives did not show any major differences in semithick sectioning (data not shown), but higher long-term robustness is expected for the 45° knife (Matzelle et al., 2003). Consequently, a combination of two-step curing of LX112 and heated ultramicrotomy allows for semithick sectioning at 2–10 μ m.

Light and Electron Microscopy of Serial Semithick Sections Reveals Ultrastructural Details for Selection for FIB-SEM Imaging

For volume analysis of cortical mouse tissue, we collected serial semithick sections on CNT tape using a tape collector (ATUM system mounted on a PowerTome, RMC, Figure 4A). Sections were cut at a slow







в



Figure 3. Generation of Semithick Sections by Precuring and Elevated-Temperature Microtomy

(A) Comparison of resin performance for semithick sections of mouse cortex tissue. BSD images were acquired of 2 (top) and 5 μ m (bottom) semithick sections of epon and LX112 blocks cured for 48 or 10 h and sectioned at room temperature or at 40°C. Left to right: epon cured for 48 h, sectioned at 24°C; LX112 cured for 48 h, sectioned at 24°C; LX112 cured for 10 h, sectioned at 24°C; LX112 cured for 48 h, sectioned at 40°C. Scale bar, 5 µm. Arrowheads indicate major (filled) and minor (hollow) tissue cracks.

(B) Photographs of infrared lights installed at the sides of the microtome sample arm to warm the sample during semithick sectioning (left). The heated diamond knife is depicted with a lower heater and the upper sensor sticks and the temperature control (right). he, heating element; ir, infrared light; sa, sample arm; ta, tape; tac, tape collector; tec, temperature control; ts, temperature sensor.

See Figure S2 for details on the heated diamond knife construction.

speed (0.2-0.3 mm/s), both to limit compression of the sample and in order to keep the section on the heated water bath longer to smoothen. The tape speed was set to values above 0.3 mm/s within the cutting window to ensure efficient uptake of the section onto the tape. In order to maximize the number of sections per tape length and reduce inter-section gaps, the tape speed was reduced below 0.2 mm/s outside the cutting window. For test purposes, we cut 50 sections of mouse cortex tissue at 5 µm thickness. After sectioning and collection, the CNT tape was cut into 5-cm strips and reversibly adhered onto glass slides by application of a drop of water and incubation at 60° on a heating plate (Figure S3A). For 5-µm-thick sections, we acquired section overview images by transmitted light microscopy (Figure 4A). Samples were mounted onto carbon double adhesive tape attached to a silicon wafer as previously described (Kasthuri et al., 2015; Djannatian et al., 2019) and postcured (Figure S3B). BSD images were captured at 4 kV (Figure 4B). Serial section images were taken at 0.2 \times 0.2 \times 5 μ m and regions of interest at 0.01 \times 0.01 μ m. The beam dwell time was reduced to values below 2 μ s/pixel in order to avoid charging artifacts originating from increased sample thickness. Still, some charging at resin-rich regions like blood vessels or nuclei could not be prevented. Larger morphological features (such as cell bodies) were accessible by light microscopy, whereas SEM was needed to resolve objects













Figure 4. Serial Semithick Sectioning for Targeted FIB-SEM.

Serial 5- μm -thick sections of mouse cortex were collected on CNT tape.

(A) Overview of several consecutive sections on tape (left) and a single transmitted light micrograph (20x objective, right). Scale bars, 2 mm and 100 µm, respectively.

(B) Transmitted light (left) and BSD images (10 × 10 × 5,000 nm resolution) of a selected region on a single section shown in (A) and maximum projection of all 93 sections revealing the vasculature morphology (right). Scale bar, 20 µm.

(C) A random cortical FIB target site was chosen (blue box) (left). The selected region was prepared for FIB-SEM by carbon deposition and trench milling (right). Scale bars, 100 and 10 $\mu\text{m},$ respectively.

(D) Cross section after FIB-SEM preparation showing the section—CNT tape adhesion site and the surface covered by a carbon layer (top). Defects in the surface layer topology are highlighted (black arrowheads). After the FIB-SEM run an xy section was reconstructed (bottom) from 2000 SE images (resolution 5 \times 5 \times 5 nm³, bottom). Scale bar, 1 μ m. (E) 3D model of the FIB-SEM stack revealing myelinated axons (yellow), post synaptic densities (blue), and neuronal nuclei (gray). Scale bar, 2 µm.

(F) Schematic of the ATUM-FIB strategy: sequential resin (LX112) curing and heated ultramicrotomy are required for semithick sectioning. Serial sections are attached onto glass slides for light microscopy and remounted onto silicon wafers for serial SEM imaging and target selection. A section of interest is remounted, adhered onto a standard sample holder, and carbon-coated for FIB-SEM examination

See Figure S2 for photographs of the different processing steps.

in the range of large non-myelinated axons. Maximum projections revealed the tissue environment, such as vasculature patterns (Figure 4B).

Although FIB-SEM would be possible directly on the wafer, remounting onto FIB stubs is safer and gives much more freedom for the milling direction. It is possible to detach either the CNT tape directly by force or,





preferably, to cut out the carbon adhesive carrying tape and 5- μ m-thick section (Figure S3C). The latter option is preferred as it limits the risk of distorting the sections. The selected piece of section on tape(s) is then adhered onto a FIB-SEM stub by conducting carbon cement. A fine carbon layer was sputtered onto the sample providing surface accessibility for the electron beam while increasing conductivity. FIB-SEM was performed by milling an 8- μ m-deep trench (Figure 4C). We acquired a FIB-SEM stack of a 30 × 30 × 5 μ m cortical region data at 5 × 5 × 5 nm (Figure 4D). Ultrastructural features, such as post-synaptic densities and myelinated axons, were segmented and their three-dimensional orientation was depicted in a model (Figure 4E). Resin postcuring resulted in good milling characteristics without curtaining effects or other problems arising from samples embedded in soft epon. In summary, semithick sections can be imaged by light or electron microscopy to reveal (ultrastructural) details required for target site selection (Figure 4E). Selected regions on a particular section can then be subjected to targeted isotropic voxel acquisition by FIB-SEM.

Targeted FIB-SEM Enables Isotropic Ultrastructural Analysis of Amyloid Plaques in FAD

As a proof of concept, we combined serial semithick sectioning with targeted FIB-SEM to visualize microglia contacting dystrophic neurites in the cortex of a (familial) Alzheimer's disease (AD) mouse model. AD, the most common form of dementia in the elderly, causes gradual loss of memory, judgment, and the ability to function socially. It is characterized by the presence of extracellular plaques composed of amyloid- β (A β) peptides and intracellular tau aggregates (Kwak et al., 2020; Giacobini and Gold, 2013). The plaques are surrounded by microglia, phagocytic immune cells, which participate in the clearance of A β (Mattiace et al., 1990; Hemonnot et al., 2019). The ultrastructure of amyloid plaques has, so far, been studied by TEM (Gowrishankar et al., 2015; Terry et al., 1964) and also by correlated light microscopy and FIB-SEM (Blazquez-Llorca et al., 2017; El Hajj et al., 2019). Although the latter approach provides exact targeting of single events, ATUM-FIB allows unbiased sampling of cellular interactions around plaques. For ATUM-FIB, we collected 36 consecutive sections at 5 μ m thickness onto CNT tape. Three-dimensional reconstruction of the light and electron micrographs revealed the amyloid plaque distribution in the resulting 180- μ m-thick volume, as well as the vasculature pattern (Figures 5A and 5B).

We selected two consecutive sections containing a part of a plaque surrounded by a microglial cell for FIB-SEM examination (Figures 5A–5C). The ROI for the deposition of a protective carbon layer was relocated by overlaying the SEM image from the section series with a BSD image acquired at 8 kV. We imaged a 20 × $20 \times 5 \,\mu$ m volume at 5 × 5 × 5 nm resolution by FIB-SEM. In order to reveal the strength of isotropic imaging we aligned the FIB-SEM volume and reconstructed another xz plane image of the microglial cell. The original SEM surface image was comparable with this virtual section (Figure 5D). Notably, we were able to stitch cross-sectional images of the two consecutive sections investigated (Figure 5E) (Xu et al., 2017), enabling extended z-volume analysis beyond 5 μ m. Dystrophic neurites displayed ER structures at the contact sites opposing the microglial plasma membrane (Figure 5F). Although the target volume is resolved at high resolution and with isotropic voxels, light and electron microscopic images of the surrounding tissue provide a morphological context. Moreover, the non-destructive nature of serial sectioning on tape allows for reinspection of other ROIs at high resolution.

DISCUSSION

Here, we introduce ATUM-FIB as a straightforward approach to combine overview imaging of tissue sections with targeted high-resolution three-dimensional reconstruction of subvolumes. In summary, ATUM-FIB has the following advantages over previously developed 3D EM volume workflows (Figure 6): (1) The ATUM-based generation of semithick sections allows screening of larger tissue volumes for rare events or specific sites of interest based on either light microscopic or low-resolution SEM exploration of the semithin sections. Such sites can then be targeted by FIB-SEM with \sim 5 nm isotropic xyz-resolution. Thereby, the high-resolution volumes are put into a larger morphological context, similar to microCT investigations (Handschuh et al., 2013; Starborg et al., 2019), but with the advantage of providing direct access to target structures instead of coordinates. Moreover, this tissue context provides rich fiducial landmarks for correlated light/electron microscopy (Luckner et al., 2018). (2) In contrast to standard ultrathin ssTEM/SEM or ATUM techniques, our approach results in 100-fold fewer sections that need to be archived. This saves time, simplifies handling, and reduces cost. (3) Just as ATUM, ATUM-SEM is a non-destructive technique (except for the FIB-targeted areas) and thus preserves a library of semithick sections. These can be revisited to increase the number of detailed observations or explore new questions that emerge over time. The limitation in volume depth of ATUM-FIB due to the maximum thickness of semithick sections (\leq 5 μ m) compared with investigations of whole blocks can be overcome be analyzing the same region in







Figure 5. Targeted FIB-SEM on Selected Consecutive Sites of Semithick Sections in Familial Alzhiemer's Disease (FAD) Cortex Samples

(A) Schematic of ATUM-FIB on consecutive $5-\mu$ m-thick sections of mouse FAD cortex samples. Microglia (blue) contacts to plaques (orange) are targeted.

(B) Transmitted light image of one section (20x objective, left) and average projection SEM of 18 sections (middle) revealing plaques (arrowheads). The 3D model (right) was segmented from a set of 36 serial transmitted light images. Blood vessels (gray), plaques (yellow), and the target plaque (orange) are highlighted. Scale bar 100 µm.

(C–E) Schematics showing the imaging planes (gray) in the respective subfigures. (C) Three consecutive 5- μ m-semithick sections of the FAD cortex sample on CNT tape. The microglial cell (blue), dystrophic neurites (orange), and amyloid core (yellow) are highlighted. The white box indicates the magnified image in (D). Scale bar, 5 μ m. (D) Magnified surface image of the microglia to plaque contact site of section 1 (left). This region was targeted for FIB-SEM at 5 × 5 × 5 nm resolution. Reconstructions of two deeper levels within the semithick sections are shown (middle, right). Scale bar, 1 μ m. (E) Stitched cross sections of corresponding areas in consecutive semithick sections 1 and 2 after FIB-SEM. Scale bar, 500 nm. (F) Region of interest of the selected section 1 of a FIB-SEM run. The 3D model shows the ER network (yellow) opposing the microglial plasma membrane (blue). Lysosomal structures are shown in light gray and mitochondria in dark gray (top). Scale bar, 500 nm. Representative SEM image revealing ER structures (black arrowheads) at sites of contact between microglia and dystrophic neurites (bottom). Scale bar, 200 nm.

consecutive semithick sections. Stitching of regions across serial sections has been successfully applied before for ultrathick partitioning (Hayworth et al., 2015) as well as for (S)TEM tomography (Aoyama et al., 2008; He and He, 2014; Baumeister et al., 1999) and has been shown to result in minimal loss of







Figure 6. Comparison of Volume SEM Techniques for Targeting Rare Events

Structures of interest like cell-cell interactions (microglia, magenta, dystrophic neurite, ocher) can be visualized by volume EM techniques. Current approaches for targeted imaging involve ATUM and FIB-SEM. ATUM-FIB combines the advantages of both approaches. High-precision targeting based on ultrastructural features is enabled, whereas increased section thickness reduces screening time and complexity compared with ATUM. Targeted FIB-SEM targeting is usually based on microCT data with limited xy resolution combined with trimming (arrows). A 500 µm z depth would be covered by 100 semithick sections (at 5 µm thickness, ATUM-FIB) instead of 10,000 ultrathin sections (at 50 nm thickness, ATUM). Comparable with FIB-SEM, ATUM-FIB allows for acquisition of the region of interest (black box) at isotropic voxels.

information (Hayworth et al., 2015) (Figure S1). (4) The information in surface scans that are 2–5 μ m apart are similar enough to be matched and aligned without the need for FIB-SEM information of the surrounding tissue section. Moreover, there is no need to section into oil instead of standard water baths compared with the ultrathick sectioning approach (Hayworth et al., 2015), which circumvents the need for re-embedding. (5) With the adaptation of standard diamond knives, our method can be applied in any EM laboratory with established FIB-SEM and ATUM workflows without the need of further equipment. This includes the standard rOTO staining method employed, which circumvents the need to establish novel *en bloc* contrasting protocols.

Plaques in AD and their complex cellular environment provide a good proof of concept of these advantages of ATUM-FIB: As Alzheimer plaques are sized roughly 10–100 μ m diameter, these structures can be identified by light microscopy. The microglia-to-plaque contact sites can only be identified by serial SEM with a resolution of less than 10–100 nm. This would not be possible using microCT with a resolution limited to 500 nm at best. On top, with ATUM-FIB the identified regions of interest can be directly subjected to high-resolution FIB-SEM imaging, whereas microCT investigation requires targeted trimming. FIB-SEM on two consecutive semithick sections furthermore shows that not only several regions of interested can be analyzed but also information on semithick section images can be stitched.

As the implementation of ATUM-FIB is comparably simple and imaging modalities and section thickness can be flexibly adapted to scientific questions and biological tissues of interest, we envisage a broad range of applications. The information content of subsequent isotropic FIB-SEM investigations is especially suited for the analysis of organellar ultrastructure and cell-cell contacts in defined physiological or pathological circumstances, which are currently commonly screened on serial ultrathin sections. The fact that ATUM-FIB preserves the tissue library and provides histology-like context makes the method especially attractive in settings, where rare and precious samples are being archived for long-term reinvestigations. This includes material from complex treatment studies or correlated *in vivo* imaging/EM investigations (Karreman et al., 2014) in animals. Moreover, multi-scale investigations of human samples, e.g., brain biopsies, require cross-referencing with standard histopathology and will be increasingly needed to validate ultrastructural findings, e.g., from animal models of disease (Lewis et al., 2019; Jonkman et al., 2019; Shahmoradian et al., 2019).

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Limitations of the Study

Similar to other serial sectioning techniques, ATUM-FIB has to be fine-tuned for the specific sample of interest, e.g., regarding block geometries (Baena et al., 2019). As standard volume EM embedding protocols differ, we recommend optimizing different contrasting and embedding conditions for each sample type. Adaptation of heavy metal load, resin composition, and curing time might be needed to achieve sections in the "semithickness" range. Transition regions from high to low contrast within a section like gray and white matter areas are especially prone to cause fractures. The approach presented here has been developed to target concrete structures but, in contrast to ultrathick partitioning (Xu et al., 2017; Hayworth et al., 2015), has not been optimized for a minimal loss of material between sections required for dense reconstruction and large-scale (connectomics) projects.

Resource Availability

Lead Contact

Further information and requests for resources and reagents should be directed to and will be fulfilled by the Lead Contact, Martina Schifferer (martina.schifferer@dzne.de).

Materials Availability

This study did not generate new unique reagents.

Data and Code Availability

The datasets supporting the current study have not been deposited in a public repository but are available from the corresponding author on request.

METHODS

All methods can be found in the accompanying Transparent Methods supplemental file.

SUPPLEMENTAL INFORMATION

Supplemental Information can be found online at https://doi.org/10.1016/j.isci.2020.101290.

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AUTHOR CONTRIBUTIONS

Conceptualization, M. Schifferer and T.M.; Methodology, M. Schifferer, H.G., and G.K.; Investigation, G.K. and M. Schifferer; Resources H.G.; Visualization, G.K. and M. Schifferer; Supervision, Funding Acquisition, and Writing – Review & Editing, M.K., T.M., and M. Simons; Writing – Original Draft and Project Administration, M. Schifferer.

DECLARATION OF INTERESTS

The authors declare no competing interest.

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Supplemental Information

Multiscale ATUM-FIB Microscopy Enables

Targeted Ultrastructural Analysis

at Isotropic Resolution

Georg Kislinger, Helmut Gnägi, Martin Kerschensteiner, Mikael Simons, Thomas Misgeld, and Martina Schifferer



Figure S1. Consecutive semithick section tissue loss. Related to Figure 2. Middle panel shows schematics of opposing section surfaces revealing one section top face (light grey) and the bottom side of the consecutive one (dark grey). The remaining cross section thickness is shown in yellow. Top and bottom panels show matching BSD images of consecutive 2, 5 and 10 μ m sections. The first row shows the bottom of one section and the lower row shows the opposing surface of the following section. The latter were turned upside down and deposited on CNT tape. Folds (arrowhead) could not be prevented in this turning procedure of thinner sections (< 5 μ m). Scale bar 2 μ m.



Figure S2. Design details of the heated knife. Related to Figure 3. Construction scheme (A) and photo (B) of the knife tub including the 3 and 6 mm drillings for the sensor and heater elements, respectively. Photographs of the front (C) and side (E) views of the knife boat including upper sensor and lower heater elements (D).





Figure S3. Experimental workflow for section mounting. Related to Figure 3. (A-C) Photos of the mounting steps are shown. (A) For slide scanner imaging a drop of water is placed on the glass slide (left). After the water spreads below the strip of CNT tape with the semithick sections (right), the glass slide is heated on a hot plate (at 60°C) for a few minutes. (B) After light microscopy, the CNT tape strip can be easily removed from the glass slide using a forceps (left). A strip of carbon adhesive tape is placed on a 4 inch silicon wafer and the CNT tape strip attached onto the tape (right). When sections are covered by a piece of plastic, a roller can be used to flatten the tape. (C) Narrow stripes of carbon adhesive tape can be attached between wafer and CNT tape for better grounding (left). Using a scalpel, the section of interest including CNT and carbon adhesive tape is excised from the wafer (left). Carbon adhesive is added on a FIB stub fixed in a stub holder (second) and the piece of section adhered onto it (third). Silver paint is distributed around the tape for better grounding (fourth) and a layer of carbon sputtered on over the surface (right).

Transparent Methods

Animals

For this study we worked with fixed brain tissue of wildtype mice (18 months) and a model expressing five familial AD gene mutations (5xFAD₃₁; 2 months) (Oakley et al., 2006). Mice were group-housed under pathogen-free conditions and bred in the animal housing facility of the Center of Stroke and Dementia Research. All experiments were carried out in compliance with the National Guidelines for Animal Protection, Germany, with the approval of the regional Animal care committee of the Government of Upper Bavaria, and were overseen by a veterinarian.

Sample preparation

Mice were perfused with fixative containing 2.5% glutaraldehyde (Science Services), 2% PFA (Science Services) and 2 mM CaCl₂ in 0.1 M sodium cacodylate buffer (Science Services). Brains were dissected and transferred into fixative for incubation at 4°C for two additional days. Tissue sections of maximal 1 mm thickness comprising cortex and corpus callosum regions were prepared.

Fixed samples were stained en bloc by a varied rOTO protocol (Tapia et al., 2012, Hua et al., 2015) without lead aspartate. Both, microwave-based (BioWave Pro, Pelco) and bench protocols were successfully applied as detailed in Table 1. We applied a sequence of reduced 2% osmium tetroxide in 0.1 M cacodylate buffer pH 7.4 followed by 2.5% potassium hexacyanoferrate in the same buffer. After washes the tissue was incubated in 1% agueous thiocarbohydrazide (TCH) and subsequently in 2% agueous osmium tetroxide. After overnight incubation in 1% uranylacetate at 4°C and 2h in 50°C, samples were dehydrated and infiltrated at least 2h at different resin in acetone concentrations (25, 50, 75, 90%) and overnight and for another 4h in 100% of the respective resin. Durcupan (Science Services) resin was prepared by mixing 11.4 g of component A (epoxy resin), 10.0 g of component B (964 hardener), 0.1 mL of component D (dibutyl phthalate) and component C (964 accelerator). For standard epon (Serva) 21.4 g glycidether 100 with 14.4 g dodecenylsuccinic anhydride (DDSA) and 11.3 g nadic methyl anhydride (NMA) were combined for 10 min and 0.84 mL 2,4,6 tris(dimethylaminomethyl)phenol (DMP-30) were added while stirring for another 20 min. LX112 resin (Ladd Research Industries) (Ellis, 2014) was prepared by mixing 4.5 g of mix A (mixture of 5 g of LX112 and 6,45 g of nonenyl succinic anhydride), 10.5 g

of mix B (mixture of 5 g of LX112 and 4.35 g of NMA) and 0.6 ml of DMP-30 (all components from Ladd Research Industries). Resins were cured at 60 °C for 10 or 48 h. Curing times below 10 h did not result in properly hardened blocks.

Automated tape-collecting ultramicrotomy (ATUM)

Epon blocks were roughly trimmed with EM TRIM2 (Leica) and subsequently, a rectangular tissue block (~ $2 \times 1.5 \times 0.2$ -0.4 µm) was exposed using the trimtool 45 diamond knife (Diatome). Thick sections were initially generated using a histo jumbo knife (45°, 6 mm, Diatome) in a RMC ultramicrotome (Powertome). The 35° and 45° ultra knife boats for the custom-made heated knives were provided by Diatome. Two holes (3 and 6 mm diameter, respectively) were milled into the base part of the knife boat to fit a temperature sensor (cable probe 3 x 30 mm, Sensorshop24) and a heater (Hotend Heater Catridge CNC for 3D printer, 24V, 40W; Ebay). We used a digital on/off temperature regulator (for PT100, Sensorhop24). Standard infrared lights (230 V, 150 W, Conrad Electronics) were installed at both sides of the microtome. Temperature was controlled by standard probe (VWR) and infrared thermometers (Conrad Electronics) to values within the range of 35-45 °C.

Single sections were fished from the water bath by ~0.3 x 0.8 mm carbon nanotube tape (CNT) tape (Science Services) pieces using inverse forceps. For serial sectioning the RMC tape collector was adapted to the knife by bypassing the tension lever and guiding the CNT tape behind the knife directly to the collector nose. Sectioning speed was set to 0.2-0.3 mm/sec with increased tape speed within (0.4 mm/sec) and reduced tape speed outside (0.1 mm/sec) the cutting window. This assured efficient uptake and minimization of empty intersection space on the tape. Slow speed was required both for limiting compression, as well as for keeping the sections longer in the heated water bath to smoothen. If needed, sections were guided onto the tape collector using fine brushes.

Slide scanner serial light microscopy

For light microscopic investigation, CNT tape strips with single sections or 5 cm strips with serial sections were positioned on a glass slide. For better adherence, a few drops of water were placed between tape and glass and the slide put onto a heating plate at 60 °C (see Figure S3A). Good adherence was important for tape flattening as a prerequisite of the slide scanner autofocusing function. Serial transmitted light

microscopy was performed on a slide scanner (Pannoramic MIDI II 2.0.5, 3D Histech). We selected sections by thresholding and imaged using the autofocusing and the extended focus level functions (9 focus levels, focus step size $0.2 \ \mu m \ x \ 5$) using the 20x objectives. By choosing the extended focus option, the software selects the sharpest image from each focus level for each image field, and combines them into one single image. The autofocus was restricted and the range set by testing it for several sections on different slide locations. Jpeg files were generated from the original data using the Pannoramic software CaseViewer2.2 (3D Histech).

Serial scanning electron microscopy

Sections on glass slides were postcured for 30-48 h at 60 °C. CNT strips with tissue sections were detached and assembled onto carbon tape (Science Services), mounted onto a 4-inch silicon wafer (Siegert Wafer) and grounded with adhesive carbon tape (see Figure S3B). Serial section images were acquired on a Crossbeam Gemini 340 SEM (Zeiss) in backscatter mode at 4 keV (high gain) at 7-8 mm WD and 30 or 60 μ m aperture. In ATLAS5 Array Tomography (Fibics, Ottawa, Canada) a wafer overview map at 1000-3000 nm/pixel was generated. On this basis, sections were mapped and imaged at medium (60 x 60 – 100 x 100 nm) resolution. Regions of interest from these section sets were acquired at 10x10 nm/pixel (2 μ s dwell time, line average 2). Image series were aligned in TrakEM2 using a combination of automated and manual steps, registered and analysed in Fiji (Schindelin et al., 2012).

Focused Ion Beam Scanning Electron Microscopy (FIB-SEM)

Selected thick sections on CNT tape were cut from the silicon wafer including the adhesive carbon tape underneath using a scalpel (see Figure S3C). Theses samples were mounted with conductive carbon cement (LEIT-C, Plano) and conductive silver colloid (Plano) onto standard aluminum specimen mount (Science Services). A thin layer of carbon was sputtered onto the sections (carbon cord, Science Services; sputter coater Q150T ES, Quorum). Milling and imaging were performed on a Crossbeam Gemini 340 FIB-SEM operating under SmartSEM (Zeiss) and Atlas-3D (Fibics Incorporated). Ion beam currents of 50 pA - 15 nA were used. The milling rate was set to 5 nm slices. SEM images were recorded with an aperture of 60 μ m in the high current mode at 2 kV of the InlenseDuo detector with the BSE grid set to 300-500 V and the SE detector. Voxel sizes of 5 x 5 x 5 nm were chosen. Images series of

1000-2000 consecutive sections were recorded. In ATLAS, the milling current and depth were adjusted to match with exposure time of the SEM (line average 2, dwell time 3 μ s). Automatic correction of focus (auto tune) and astigmatism (auto stig) was applied every 30 minutes. FIB-SEM image stacks were aligned and analyzed in Fiji (Schindelin et al., 2012). VAST (Berger et al., 2018) was used for segmentation and Blender for rendering of the 3D models (Community, 2017).

Key Resource Table

REAGENT or	SOURCE	IDENTIFIER			
RESOURCE					
Chemicals and Materials					
Cable sensor	SensorShop24	Cat# 003-KS-PT100-2L-1.0-			
		330-W			
Carbon adhesive	Science Services	Cat# P77819-25			
tape					
Controller for PT100	SensorShop24	Cat# TR-PT100-A-24V			
Diamond knife 35°,	Diatome	Cat# DU3530; DU4530,			
45°, 3 mm					
Epon (Glycid ether	Serva	Cat# 21045.02, 29452.05,			
100, MNA, DDSA,		20755.02, 36975.01,			
DMP-30)					
Glutaraldehyde	Science Services	Cat# E16216			
Heating cartridge,	Ebay	N/A			
24V, 40W					
Leit-C	Plano	Cat# G3300			
Leitsilber, Acheson	Plano	Cat# G3692			
1415					
LX112 Embedding	LADD Research Laboratories	Cat# 21210			
Kit					
Osmium tetroxide	Science Services	Cat# E19130			
Paraformaldehyde	Science Services	Cat# E15713			

Potassium	Sigma	Cat# 455989				
hexacyanoferrate(II)						
trihydrate						
Silicon wafer, 4", 1-	MicroChemicals	Cat#				
side polished, p-type		WSM40525200P1334SNN1				
(Boron), 1-0 Ohm						
cm						
Sodium cocodulato	Science Services	Cat# E12300				
tribydrato		Cal# L12500				
liniyulate						
Specimen mount	Science Services	Cat# 7536-30				
Thiocarbohydrazido	Sigma-Aldrich	Cat# 222220				
Thiocarbonyurazide	Sigma-Alunch	Gal# 223220				
Uranyl acetate	Science Services	Cat# E22400-05G				
Experimental Models: Organisms/Strains						
wt mice	The Jackson Laboratory	C57BL/6J				
5xFAD ₃₁	MMRRC	Stock# 34840-JAX / 5XFAD				
(five human familial						
AD gene mutations)						
mice						
Software and Algorithms						
ImageJ 2.0.0	NIH	https://imagej.nih.gov/ij/;				
		RRID:SCR_003070				
VAST	Harvard	https://software.rc.fas.harvar				
		d.edu/lichtman/vast/				
Blender	The Blender Foundation	https://www.blender.org/				
SmartSEM	Carl Zeiss Microscopy GmbH	N/A				
ATLAS 5, Array	Fibics Incorporated, Canada	N/A				
Tomography, 3D						

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