



## Do Muscle Changes Contribute to the Neurological Disorder in Spastic Paresis?

Maud Pradines<sup>1,2\*</sup>, Mouna Ghédira<sup>1,2</sup>, Blaise Bignami<sup>2</sup>, Jordan Vielotte<sup>2</sup>, Nicolas Bayle<sup>1,2</sup>, Christina Marciniak<sup>3,4</sup>, David Burke<sup>5</sup>, Emilie Hutin<sup>1,2</sup> and Jean-Michel Gracies<sup>1,2</sup>

<sup>1</sup> UR 7377 BIOTN, Laboratoire Analyse et Restauration du Mouvement, Université Paris Est Créteil (UPEC), Créteil, France, <sup>2</sup> AP-HP, Service de Rééducation Neurolocomotrice, Unité de Neurorééducation, Hôpitaux Universitaires Henri Mondor, Créteil, France, <sup>3</sup> Department of Physical Medicine and Rehabilitation, Northwestern University and the Shirley Ryan AbilityLab, Chicago, IL, United States, <sup>4</sup> Department of Neurology, Northwestern University and the Shirley Ryan AbilityLab, Chicago, IL, United States, <sup>5</sup> Department of Neurology, Royal Prince Alfred Hospital and the University of Sydney, Sydney, NSW, Australia

#### **OPEN ACCESS**

#### Edited by:

Andreas R. Luft, University of Zurich, Switzerland

#### Reviewed by:

Carlo Trompetto, University of Genoa, Italy Francesco Negro, University of Brescia, Italy Raymond Lotilla Rosales, University of Santo Tomas, Philippines

> \*Correspondence: Maud Pradines maud.pradines@u-pec.fr

#### Specialty section:

This article was submitted to Stroke, a section of the journal Frontiers in Neurology

Received: 17 November 2021 Accepted: 01 February 2022 Published: 14 March 2022

#### Citation:

Pradines M, Ghédira M, Bignami B, Vielotte J, Bayle N, Marciniak C, Burke D, Hutin E and Gracies J-M (2022) Do Muscle Changes Contribute to the Neurological Disorder in Spastic Paresis? Front. Neurol. 13:817229. doi: 10.3389/fneur.2022.817229 **Background:** At the onset of stroke-induced hemiparesis, muscle tissue is normal and motoneurones are not overactive. Muscle contracture and motoneuronal overactivity then develop. Motor command impairments are classically attributed to the neurological lesion, but the role played by muscle changes has not been investigated.

**Methods:** Interaction between muscle and command disorders was explored using quantified clinical methodology—the Five Step Assessment. Six key muscles of each of the lower and upper limbs in adults with chronic poststroke hemiparesis were examined by a single investigator, measuring the angle of arrest with slow muscle stretch (X<sub>V1</sub>) and the maximal active range of motion against the resistance of the tested muscle (X<sub>A</sub>). The coefficient of shortening  $C_{SH} = (X_N-X_{V1})/X_N$  (X<sub>N</sub>, normally expected amplitude) and of weakness  $C_W = (X_{V1}-X_A)/X_{V1}$ ) were calculated to estimate the muscle and command disorders, respectively. Composite  $C_{SH}$  (CC<sub>SH</sub>) and  $C_W$  (CC<sub>W</sub>) were then derived for each limb by averaging the six corresponding coefficients. For the shortened muscles of each limb (mean  $C_{SH} > 0.10$ ), linear regressions explored the relationships between coefficients of shortening and weakness below and above their median coefficient of shortening.

**Results:** A total of 80 persons with chronic hemiparesis with complete lower limb assessments [27 women, mean age 47 (SD 17), time since lesion 8.8 (7.2) years], and 32 with upper limb assessments [18 women, age 32 (15), time since lesion 6.4 (9.3) years] were identified. The composite coefficient of shortening was greater in the lower than in the upper limb ( $0.12 \pm 0.04$  vs.  $0.08 \pm 0.04$ ; p = 0.0002, while the composite coefficient of weakness was greater in the upper limb ( $0.28 \pm 0.12$  vs.  $0.15 \pm 0.06$ , lower limb; p < 0.0001). In the lower limb shortened muscles, the coefficient of weakness correlated with the composite coefficient of shortening above the 0.15 median C<sub>SH</sub> (R = 0.43, p = 0.004) but not below (R = 0.14, p = 0.40).

**Conclusion:** In chronic hemiparesis, muscle shortening affects the lower limb particularly, and, beyond a threshold of severity, may alter descending commands. The latter might occur through chronically increased intramuscular tension, and thereby increased muscle afferent firing and activity-dependent synaptic sensitization at the spinal level.

Keywords: spastic myopathy, spastic cocontraction, chronic hemiparesis, synaptic sensitization, clinical extensibility, muscle disorder, stretch-sensitive paresis, quantified assessment

#### INTRODUCTION

In spastic paresis, muscle changes coexist with neurologic abnormalities (1, 2) and the two have been suggested to potentiate each other (3-5). Disruption of the motor command causes immediate paresis, i.e., reduced voluntary motor unit recruitment, which, in the context of muscle hypo-mobilization, triggers a cascade of pathological changes affecting muscle tissue extensibility and motor neuronal excitability (4, 5).

In the acute stages, the common occurrence of hypomobilization of several paretic muscles in a shortened position (6) represents an assault on muscle tissue, causing acute transformation in molecular genetics and gene transcription (4, 5, 7–9). Within days, muscle mass is reduced and muscle extensibility decreases, in parallel with sarcomere loss (10–12); in addition, collagen tissue is modified and deposits around muscle fibers with fascial thickening (13–16). These muscle changes can be demonstrated through biomechanical and clinical measurements; they gradually worsen if hypo-mobilization is not addressed (16–21).

In the subacute stages of spastic paresis, additional plastic neural mechanisms come into play, whereby stretch-sensitive (spastic) muscle overactivity causes a third mechanism to contribute to the motor impairment, along with the agonist paresis and the muscle disorder (4, 5, 21–23). Antagonist muscle overactivity predominates in some muscles, producing agonistantagonist imbalance around joints (5, 24, 25). Among the various types of muscle overactivity in spastic paresis, spastic cocontraction has been defined as a misdirection of the supraspinal drive that abnormally recruits antagonist motor units during agonist command, independent of any phasic stretch (5, 26, 27). This form of overactivity directly impedes and may sometimes reverse the desired voluntary movement (26). Stretch receptor recruitment in the overactive muscle aggravates this antagonistic co-contraction, hence the term spastic co-contraction (26-28). Finally, for the agonist muscles responsible for the movement, the responsiveness of agonist motor neurons to descending command may be negatively impacted by the stretch imposed on the antagonist, producing a *stretch-sensitive paresis* (4, 28, 29).

Decreased extensibility of the antagonist muscle in hemiparesis can be estimated clinically as reduced passive range of motion when attempting maximal slow and strong passive movement against the resistance of the tested muscle group. Here, we question whether decreased muscle extensibility might play a role in the later plastic neural events described above (spastic co-contraction and stretch-sensitive agonist paresis). The second question is whether motor function seems compromised more by the muscle disorder or the abnormal descending command. A better understanding of the respective contributions of muscle and neural disorders to functional impairment in chronic hemiparesis might then indicate where interventions should be mostly directed for individual patients. To answer these questions, we conducted a retrospective investigation of two coefficients of impairment designed as normalized, clinical estimates of the muscle and the neural components of spastic paresis. The overarching hypothesis tested here was that, beyond a threshold of muscle shortening in chronic hemiparesis, the transmission of active command to an agonist may depend, at least in part, on the severity of collagenous modifications of the antagonist, i.e., on the degree of antagonist hypo-extensibility.

## METHODS

#### **Study Design**

This study was conducted in compliance with the Declaration of Helsinki (2008), Good Clinical Practice guidelines, and local regulatory requirements for the Henri Mondor University Hospital, Créteil, France. We retrospectively reviewed the charts of subjects with chronic hemiparesis that had been consecutively evaluated using at least steps 1, 2, and 4 of the Five *Step Assessment* (an expansion of the Tardieu scale, see below) (30) in the lower and/or the upper limb, by a single clinician (JMG) between January 2014 and December 2019 (**Figure 1**).

## **Inclusion and Exclusion Criteria**

All the patient charts were included in this study if they fulfilled the following criteria: (i) adults (age  $\geq$  18 years) with chronic hemiparesis due to a single stroke that occurred > 1 year before the assessment (**Figure 1**); (ii) assessment using at least Steps 1, 2, and 4 of the Five Step Assessment in soleus (SO), gastrocnemius (GN), gluteus maximus (GM), hamstrings (HS), vastus (VA) and rectus femoris (RF) for the lower limb, or shoulder extensors (SE), subscapularis (SS), pronator quadratus (PQ), elbow flexors (EF), wrist flexors (WF) and finger flexors (FF) for the upper limb, performed between January 2014 and December 2019 (iii) ability for independent ambulation (Functional Ambulation Classification score of 5–6) (31); (iv) absence of botulinum toxin injection in the evaluated muscles in the 3 months before the assessment; and (v) clinically stable condition. Exclusion criteria were: (i) recurrent strokes or other neurological or



orthopedic disorders affecting the evaluated muscles; (ii) severe cognitive impairment (Mini-Mental Status test score < 23 or major receptive aphasia) interfering with the ability to assess the patient; (iii) treatment with antispasticity medications that could produce synaptic depression, whether oral or intrathecal (baclofen, benzodiazepines, etc) (32, 33). In each patient chart, the first visit chronologically that met these criteria was selected for analysis.

#### **Description of the Five Step Assessment**

For each subject, the same clinician used the Five Step Assessment for the six muscles defined above in the lower limb and/or the upper limb (30). The patient was always seated for the upper limb assessments and supine for the lower limb assessments (apart from locomotion).

Step 1 of the Five Step Assessment evaluates active function. For the lower limb, this involved measurement of ambulation speed in meters/second (m/s) over 10 m (AT10) performed barefoot at maximal speed with the assessment starting and ending in a seated position (19, 30, 34). For the upper limb, the active function was measured using the Modified Frenchay Scale (MFS), and consisted of videotaping ten activities of daily living (4 uni-manual activities using the paretic hand and 6 bimanual activities, in which the paretic hand assists the other hand) and rating each of them on a ten-point visual analog scale based on video review (19, 35). In that visual analog scale, zero means no movement, 10 is the perfect achievement of the task, and 5 is a task barely accomplished (36). The 10 scores were averaged to derive the MFS score for each patient. Individual task rating on the MFS has excellent intra- and inter-reliability and the MFS has been validated against a subjective scale of perceived function (Disability Assessment Scale, DAS) as well as the Fugl-Meyer score, a classic measurement of motor impairment (19, 36–38).

Step 2 of the Five Step Assessment is the measurement of the *passive range of motion* of the tested muscle, referred to as the  $X_{V1}$  angle of the Tardieu scale (19, 30, 39), using zero as the theoretical angle of minimal stretch for each muscle (19, 30, 39). Stretch was applied slowly and strongly, up to the point where further passive stretch was not possible or would cause pain or would jeopardize joint integrity (30, 39). The stretch was performed as slowly as possible to avoid triggering a phasic stretch reflex and as strong as possible to overcome most of the spastic dystonia (30, 40).  $X_{V1}$  angle measurements were made visually, as the reliability of these angle measurements has been shown to be similar between visual or goniometric evaluations (41), except at the knee where a goniometer was used.  $X_{V1}$ 

measurements have shown good to excellent intra- and interrater reliability in paretic adults (41–44); this measure provides information primarily about the extensibility of *muscle* tissue (45). From the X<sub>V1</sub> measure, the coefficient of shortening C<sub>SH</sub> was derived for each muscle (19), based on the formula  $C_{SH} = (X_N-X_{V1})/X_N$  where X<sub>N</sub> is the normally expected passive joint amplitude for each tested muscle (46). The normally expected passive amplitude X<sub>N</sub> is also defined using zero as the theoretical angle of minimal stretch for each muscle (as in the Tardieu Scale). In this study, the normal reference X<sub>N</sub> was considered to be 120° for the SO, 115° for GN, 150° for GM, 270° for HS (180° knee extension + 90° hip flexion), 150° for VA muscles, 240° for RF (150° knee flexion + 90° hip extension), 180° for the SE, SS, EF and WF, PQ, and 270° for FF (46, 47).

Step 4 of the Five Step Assessment is the measurement of the maximal active range of motion XA, against the resistance of the evaluated antagonist muscle (30). The patient was asked to accomplish one movement of maximal amplitude against the resistance of the tested antagonist; here a goniometer was used to measure the angle (Figure 2). The maximal range of active movement represents the balance between the forces generated by agonist activation and those related to the passive and active resistances generated by the tested antagonist muscle group. From the X<sub>A</sub> measure, the coefficient of weakness C<sub>W</sub> was derived for each tested muscle, using the formula  $C_W$  =  $(X_{V1}-X_A)/X_{V1}$  (19). The coefficient of weakness estimates the impairment of active command against the resistance of the tested antagonist, its maximal passive extensibility being taken into account (19). The intra- and inter-rater reliabilities of XA and of the coefficient of weakness have been established (44).

#### **Data Treatment**

Over the period from January 2014 to December 2019, data for each (upper/lower) limb of each subject from the first visit that met the inclusion criteria were systematically collected. For each lower and upper limb muscle, we normalized its  $X_{V1}$  value to a theoretically expected value of  $180^{\circ}$ , using the formula  $X_{V1normalized} = X_{V1} \times 180/X_N$ . From here on, the symbol  $X_{V1}$  represents these normalized  $X_{V1}$  values. This normalization allowed a Composite  $X_{V1}$  to be derived, by averaging the normalized  $X_{V1}$  values for the six key muscle groups of each limb:

Composite 
$$X_{V1-LL} = (X_{V1SO} + X_{V1GN} + X_{V1GM} + X_{V1HS} + X_{V1VA} + X_{V1RF})/6;$$
  
Composite  $X_{V1-UL} = (X_{V1SE} + X_{V1SS} + X_{V1EF} + X_{V1PQ} + X_{V1WF} + X_{V1FF})/6.$ 

Composite  $X_A$  for each limb was calculated using the same process (48). We then calculated a *composite coefficient of shortening* as (180-Composite  $X_{V1}$ )/180 and a *composite coefficient of weakness* as (Composite  $X_{V1}$ -Composite  $X_A$ )/Composite  $X_{V1}$ .

Finally, for the shortened muscle groups defined as those with a mean  $C_{SH} > 0.10$ , two subgroups were considered: those below and those above their median coefficient of shortening.

#### Statistical Analysis

Descriptive statistics were used for the parameters  $X_{V1}$  and  $X_A$  for each muscle, Composite  $X_{V1}$ , Composite  $X_A$ , coefficient of shortening and coefficient of weakness per muscle, composite, ambulation speed, and Modified Frenchay Score. *t*-tests for paired data were used to compare the coefficients of shortening between individual muscles. Univariate logistic regression analyses then explored correlations between the Composite  $X_{V1}$  and the Composite  $X_A$  (raw data) and between the coefficient of shortening and the coefficient of weakness (normalized data) for each individual muscle group, for the mean of the six muscles of each limb (composite scores) and for the most shortened muscle groups only ( $C_{SH} > 0.10$ ). In those muscles, correlations between the coefficient of shortening and the coefficient of weakness were explored in the total sample and in the two subgroups below or above the median coefficient of shortening.

Secondarily, univariable regression analyses explored, for each muscle group of the upper and lower limb and





for the composite scores, the respective impacts of the coefficient of shortening and of the coefficient of weakness on motor function (Modified Frenchay score or maximal ambulation speed). If both the coefficient of shortening and the coefficient of weakness were predictive of motor function on univariable analyses, bivariable regression analysis was used, for each individual muscle and for the composite score. Lastly, for each limb, if the coefficients of shortening of several muscle groups were predictive of motor function in univariable analyses, multivariable regression explored which of these muscles remained important determinants of motor function once the regression coefficients were adjusted for the effects of the other predictors. Statistical significance was set at 0.01. All analyses were conducted with SPSS (18.0) software.

## RESULTS

#### **Subject Characteristics**

Of 110 consecutive patients with adult-onset chronic hemiparesis in whom the lower limb was evaluated during the study period, 80 patients met the criteria for inclusion (aged 51  $\pm$  16 years; 26 women, 54 men; 42 injured on the left hemisphere, 58 right hemisphere; 66 with ischemic stroke, time since lesion, 9  $\pm$ 8 years; Figure 1). For the upper limb group, 46 consecutive patients with adult-onset chronic spastic paresis were evaluated during the study period and 32 patients met the inclusion criteria (aged  $39 \pm 15$  years; 18 women, 14 men; 19 injured on the left hemisphere, 13 on the right; 22 with ischemic stroke, time since lesion,  $6 \pm 9$  years). In 15 of these 32 patients, investigations were performed on both the upper limb and the lower limb. At the selected visit, the Modified Frenchay score was 5.47  $\pm$  1.09 for the upper limb cohort (normal function = 10), and the maximal ambulation speed barefoot was 0.88  $\pm$  0.39 m/s for the lower limb cohort (normal around 1.7 m/s) (34).

# Muscle Shortening and Motor Command Disorder

Overall, the coefficient of shortening (C<sub>SH</sub>) was greater in the lower limb than in the upper limb [0.12, CI 95 (0.11–0.13) vs. 0.08 (0.07–0.09), upper limb; p = 0.0002, *t*-test; see **Figure 3A**, **Table 1**]. Conversely, the coefficient of weakness (C<sub>W</sub>) was greater in the upper than in the lower limb [0.28 (0.24–0.32) vs. 0.15 (0.14–0.16) lower limb; p < 0.0001, *t*-test]. These relationships were similar in the 15 patients in whom there was documentation for both the upper and lower limbs [C<sub>SH</sub> lower limb 0.11 (0.085; 0.133) vs. upper limb 0.08 (0.055; 0.097); p = 0.03 t-test; C<sub>W</sub> upper limb 0.35 (0.277; 0.423) vs. lower limb 0.16 (0.125; 0.195); p = 0.0015; not illustrated].

The individual coefficients of shortening, and of weakness, for the six muscles in each limb are displayed in **Figures 3B,C**, respectively. In the lower limb, over the six evaluated muscles, GN exhibited the greatest shortening:  $C_{SH-GN} = 0.17$  (0.16; 0.18). Then SO:  $C_{SH-SO} = 0.15$  (0.14; 0.16), GM  $C_{SH-GM} = 0.14$ 



**FIGURE 3** | Degree of muscle shortening and of motor command impairment in chronic hemiparesis. (A) Coefficients of impairment of the Composite score of the upper and lower limbs. (B) Coefficient of Shortening of each of the investigated muscles. (C) Coefficient of Weakness of each of the investigated muscles. SE, shoulder extensor; SS, subscapularis; EF, elbow flexors; PQ, pronatus quadratus; WF, wrist flexors; FF, finger flexors; SO, soleus; GN, gastrocnemius; GM, gluteus maximus; HS, hamstrings; VA, vastus; RF, rectus femoris. \*\*p < 0.01; \*\*\*p < 0.001.

Α.	Clinical	parameters
----	----------	------------

Lower limb	Soleus	Gastroc	Glut Max	Hamst	Vastus	Rect Fem	Comp score
X <sub>V1</sub>	$102 \pm 6$	95 ± 4	129 ± 12	253 ± 13	$137 \pm 7$	208 ± 16	$154 \pm 7$
X <sub>A</sub>	$91 \pm 9$	$76\pm13$	$116 \pm 16$	$222 \pm 23$	$112 \pm 16$	$176 \pm 25$	$132\pm13$
C <sub>SH</sub>	$0.15\pm0.05$	$0.17\pm0.04$	$0.14\pm0.08$	$0.06\pm0.05$	$0.09\pm0.05$	$0.13\pm0.07$	$0.12\pm0.04$
Cw	$0.10\pm0.07$	$0.21 \pm 0.12$	$0.10\pm0.07$	$0.12\pm0.08$	$0.18\pm0.11$	$0.15\pm0.09$	$0.15\pm0.06$
Ambul speed	$0.88\pm0.39$						
Upper limb	Sh Ext	Subscap	Elbow flex	Pron quad	Wrist flex	Finger flex	Comp score
X <sub>V1</sub>	150 ± 22	$152 \pm 23$	177 ± 4	177 ± 16	$175 \pm 6$	264 ± 13	$183 \pm 15$
X <sub>A</sub>	$116\pm33$	$111 \pm 37$	$165 \pm 13$	$128 \pm 44$	$138 \pm 21$	$121 \pm 63$	$130\pm11$
C <sub>SH</sub>	$0.16\pm0.12$	$0.15\pm0.13$	$0.01 \pm 0.02$	$0.04\pm0.08$	$0.03\pm0.03$	$0.12\pm0.04$	$0.08\pm0.04$
Cw	$0.23\pm0.18$	$0.29\pm0.17$	$0.07\pm0.06$	$0.28\pm0.23$	$0.21 \pm 0.11$	$0.54\pm0.25$	$0.28\pm0.12$
MFS	$5.5 \pm 1.1$						

#### B. Differences between coefficients of shortening of individual muscles

			Upper Lin	ıb				Lower Limb								
	C <sub>SH-SE</sub>	C <sub>SH-SS</sub>	C <sub>SH-EF</sub>	C <sub>SH-QP</sub>	C <sub>SH-WF</sub>	C <sub>SH-FF</sub>		C <sub>SH-SOL</sub>	C <sub>SH-GAS</sub>	C <sub>SH-GM</sub>	C <sub>SH-HS</sub>	C <sub>SH-VA</sub>	C <sub>SH-RF</sub>			
$C_{\text{SH}-\text{SE}}$							$C_{\text{SH}-\text{SOL}}$									
C <sub>SH-SS</sub>	0.55						$C_{\text{SH}-\text{GAS}}$	3E-06								
$C_{\text{SH}-\text{EF}}$	8E-08	2E-06					$C_{\text{SH}-\text{GM}}$	0.011	3E-04							
$C_{\text{SH}-\text{QP}}$	2E-06	4E-06	0.053				$C_{\text{SH}-\text{HS}}$	3E-15	6E-26	1E-10						
$C_{\text{SH}-\text{WF}}$	9E-08	2E-06	0.03	0.31			$C_{\text{SH}-\text{VA}}$	2E-11	2E-19	2E-06	0.013					
$C_{\text{SH}-\text{FF}}$	0.11	0.17	2E-15	3E-06	4E-11		$C_{\text{SH}-\text{RF}}$	0.22	2E-03	6E-01	9E-07	2E-04				

X<sub>V1</sub>, Maximal passive range of motion against the resistance of the investigated muscle; X<sub>A</sub>, active range of motion against the resistance of the investigated muscle; C<sub>SH</sub>, coefficient of shortening; C<sub>W</sub>, coefficient of weakness; MFS, Modified Frenchay Scale; Ambul Speed, ambulation speed over 10 meters (AT10) at maximal speed, barefoot.

B. Comparison of muscle shortening (C\_{SH}) between individual muscles within each limb.

SE, shoulder extensor; SS, subscapularis; EF, elbow flexors; PQ, pronatus quadratus; WF, wrist flexors; FF, finger flexors; SO, soleus; GN, gastrocnemius; GM, gluteus maximus; HS, hamstrings; VA, vastus muscles; RF, rectus femoris.

(0.06; 0.22) and RF  $C_{SH-RF} = 0.13$  (0.06; 0.20) were shortened to about the same extent (**Table 1B**; **Figure 3B**). In the upper limb, the three most shortened muscles were SE:  $C_{SH-SE} = 0.16$  (0.12; 0.20), SS:  $C_{SH-SS} = 0.15$  (0.10; 0.18), and FF:  $C_{SH-FF} = 0.10$  (0.06; 0.14) (**Table 1B**; **Figure 3B**). GN:  $C_{W-GN} = 0.21$  (0.18; 0.24) and FF:  $C_{W-FF} = 0.54$  (0.45; 0.63), were exhibiting the highest coefficient of weakness at the lower and upper limb, respectively (**Figure 3C**).

#### Relation Between Coefficients of Shortening and Coefficients of Weakness

In terms of raw values in the upper and lower limbs, the maximal active range of motion against the resistance of the examined muscle (Composite  $X_A$ ) correlated with the angle of arrest with slow muscle stretch (Composite  $X_{V1}$ ), the correlation being strong in the lower limb (upper limb, R = 0.43, p = 0.017; lower limb R = 0.73, p < 0.0001; univariable analysis; see **Figure 4**). After normalizing and taking the mean coefficients across the six muscles, the composite coefficient of weakness still correlated with the composite coefficient of shortening for the lower limb (R = 0.36, p = 0.0009). Evaluation of each muscle group individually found this dependency in the GN only (R = 0.36, p < 0.0001),

with trends in the GM (R = 0.22, p = 0.045) and HS (R = 0.21, p = 0.052). In the upper limb, however, the composite coefficient of weakness did not correlate with the composite coefficient of shortening (R = 0.19, p = 0.30). A trend for this correlation was found only in SS, when examined by individual muscles (R = 0.48, p = 0.016).

Univariable analysis for the most shortened muscles of the lower limb taken together (**Figures 5A–C**) (i.e., those muscles with  $C_{SH} > 0.10$ , which was the case for SO (**Figures 5D–F**) GN, GM, and RF), showed that  $C_{SH}$  correlated with the coefficient of weakness for patients with values above the median (**Figure 5B**), but not for patients with coefficients of shortening below the median (**Figure 5C**). This was also true for the SO (**Figures 5E,F**) and GN (not shown), taken individually.

## Relationships of the Coefficients of Shortening and Weakness With Motor Function

In univariable analyses for the lower limb, each of the composite coefficients of shortening (strongly) and of weakness predicted motor function (R = -0.62, p <



0.0001; R = -0.48, p < 0.0001, respectively, **Table 2A**). When exploring the impact of the extensibility loss in each of the six lower limb muscles taken individually, ambulation speed depended on the coefficient of shortening primarily (**Table 2A**). In the upper limb, the Modified Frenchay score depended on coefficients of weakness only (**Figure 6B**, **Table 2A**).

In the bivariable analysis for the lower limb, the composite coefficient of shortening and the composite coefficient of weakness remained both predictors of maximal ambulation speed once the regression coefficients were adjusted for the effect of the other predictor, although the coefficient of shortening remained a stronger predictor (composite coefficient of shortening  $\beta = -0.51$ , p < 0.0001; coefficient of weakness  $\beta = -0.29$ ; p = 0.003; **Figure 6A**, **Table 2B**). In multivariable analysis, none of the six evaluated lower limb muscles remained a sole predictor of maximal ambulation speed once the regression coefficients were adjusted for the effects of the other muscles.

#### DISCUSSION

The present findings suggest that, in chronic hemiparesis, abnormal muscle properties reach greater severity and contribute more to disability in the lower limb than in the upper limb, while in contrast, the upper limb is affected more by the severity of the impairment of the descending command. In the more shortened lower limb muscles (SO, GN, RF, and GM), the coefficient of weakness correlated with the coefficient of muscle shortening above the median coefficient of shortening only. In the upper limb, a trend for such correlation was present for SS only, one of the most shortened upper limb muscles. In chronic spastic paresis, a tipping point may exist where, past a certain threshold of severity, muscle shortening starts worsening the disordered descending command.

## Value of a Clinical Methodology Such as the Five Step Assessment to Draw Inferences Into Actual Muscle Shortening and Actual Impairment of the Descending Command

The Five Step Assessment represents a clinical attempt to distinguish between the muscle disorder and the neurological disorder of spastic paresis, using specific coefficients of impairment (19, 30). However, there is a "double nature" in coefficients of shortening and of weakness, both combining muscular and neural components, that should be discussed.

As for passive X<sub>V1</sub> measurements (passive range of motion against the tested muscle), when stretching a muscle slowly in a patient at rest, one faces the classic impossibility to safely distinguish between residual spastic dystonia (a neural component of stiffness) and true, passive muscle hypoextensibility (muscular component) at the end of the passive range (40). Yet, it is commonly accepted by the clinical community that the limitations encountered during maximal passive movements are, for the most part, linked to muscle shortening rather than to residual dystonia. Indeed, except possibly for very large muscles (GM), it is likely that the hand of the examiner typically manages to overcome most of the muscle activation due to residual dystonia. On the other hand, the examiner's hand is bound to fail to overcome all of the passive resistance, as that resistance to passive movement is known to increase exponentially with the amount of stretch in a resting muscle; therefore, passive resisting force is bound to become greater than the maximal force developed by the examiner (49, 50). Thus, while the respective contributions of passive and active resistance at the end of the available range are difficult to clinically quantify, passive phenomena constitute the primary source of range limitation, as demonstrated through X<sub>V1</sub> measurements after lidocaine blocks that still remain far from the expected physiological values  $(X_N)$  (51).

Reciprocally, active  $X_A$  measurements also partially depend on the passive resistance that the agonist has to overcome along the way. Yet, the agonist muscle is rarely able to achieve the amplitude reached by the hand of the examiner, therefore  $X_A$  is almost invariably lower than  $X_{V1}$ , and frequently far





lower (52). This means that the agonist recruitment-induced torque cannot make the limb segment reach the maximal passive range that would be allowed by the antagonist, so that  $X_A$  often finds itself far below "exponential" levels of passive antagonist resistance. Therefore, it is likely—even though difficult to clinically demonstrate, except by the marked increase in active range motion observed after lidocaine blocks (51)—that once arrived at that "submaximal"  $X_A$  level, the agonist recruitment is mostly limited by active antagonist co-contractions more than by passive antagonist hypo-extensibility.

Overall, once it is accepted that  $C_{SH}$  and  $C_W$  represent substantially passive vs. active phenomena through these  $X_{V1}$ and  $X_A$  clinical estimates, why would the relationship between them vary depending on  $X_{V1}$  or on the limb (upper vs. lower) from which one selects muscles? In other words, if both  $X_{V1}$  (maximal passive movements) and  $X_A$  (maximal active movements) manoeuvers were to be hindered in constant proportions by passive and active components, the correlation between the coefficients of shortening and the coefficients of weakness would be constant, whichever the values of  $X_{V1}$ . The fact that the correlation emerges only beyond a certain threshold value of  $X_{V1}$  is a strong suggestion—if not a demonstration—that muscle shortening itself is associated with further deterioration of the quality of the descending command (e.g., by causing increased co-contraction).

## Causal Relationship or "Casual" Association Between Muscle Shortening and Weakness of Motor Command

Although the correlations do not prove causality by themselves, the respective time courses between the muscle disorder and motoneuronal overactivity, the strength of the correlations above a certain threshold and physiological plausibility suggest a causal relationship, as developed below. Interestingly, it has already been demonstrated that ameliorating the changes in the properties of muscle and soft tissue that constitute the "spastic myopathy" (19) is accompanied by gains in function in the lower limb (53).

## Chronology: The Muscle Disorder Precedes Motoneuronal Overactivity

A substantial body of biological and histological evidence from animal models with limb immobilization demonstrates very early qualitative and quantitative changes in muscle protein synthesis, measured within hours of immobilization, long before any detectable muscle overactivity (7, 8, 11). This chronology has been confirmed in patients with severe hemiparesis from biomechanical measurements, where the onset of passive tissue stiffness of WF was detected long before true neural reflexive stiffness (21). TABLE 2 | Respective contribution of the muscular and the neurological disorders to functional impairments.

Lower limb	Pred Fact	Soleus		Gastroc		Glut Max		Hamst		Vastus		Rect Fem		Comp score	
		r	р	r	р	r	р	r	р	r	р	r	р	r	p
Max ambul Speed	C <sub>SH</sub>	-0.33	0.004	-0.39	<0.001	-0.50	<0.001	-0.58	<0.001	-0.51	<0.001	-0.45	<0.001	-0.62	<0.001
	C <sub>W</sub>	-0.37	< 0.001	-0.48	< 0.001	-0.31	0.006	-0.30	0.008	-0.41	< 0.001	-0.16	0.17	-0.48	< 0.001
Upper Limb	Pred Fact	Sh Ext		Subscap		Elbow Flex		Pron Quad		I: Wrist Fex		I: Finger Fex		Comp score	
		r	р	r	p	r	p	r	р	r	p	r	p	r	p
MFS (Frenchay)	C <sub>SH</sub>	-0.32	0.08	-0.31	0.12	0.30	0.10	-0.11	0.54	0.01	0.95	0.18	0.26	-0.22	0.21
	C <sub>W</sub>	-0.48	0.008	-0.27	0.20	-0.37	0.04	-0.48	0.006	-0.53	0.002	-0.69	< 0.001	-0.43	0.013

#### A. Univariable analyses: for C<sub>SH</sub> and C<sub>W</sub>, respectively

B. Bivariable analyses: impact of  $C_{SH}$  and  $C_W$  (taken together) on motor function when for a given muscle, each of the two coefficients ( $C_{SH}$  and  $C_W$ ) was individually correlated to motor function

Lower limb	Pred Fact	So	Soleus		Gastroc		Glut Max		Hamst		Vastus		ect Fem	Comp score	
		β	р	β	р	β	р	β	р	β	р	β	р	β	р
Max ambul Speed	C <sub>SH</sub>	-0.33	0.002	-0.22	0.045	-0.45	<0.001	-0.54	<0.001	-0.49	<0.001	-	_	-0.51	<0.001
	C <sub>W</sub>	-0.37	<0.001	-0.39	<0.00	-0.20	0.047	-0.19	0.049	-0.38	< 0.001	-	_	-0.29	0.003
Upper Limb	Pred Fact	Sh Ext		Subscap		Elbow Flex		Pron Quad		I: Wrist Fex		I: Finger Fex		Comp score	
		β	p	β	р	β	p	β	p	β	р	β	p	β	р
	C <sub>SH</sub>	-0.34	0.03	_	_	_	-	_	-	_	_	-	-	-	-
	Cw	-0.46	0.008	-	-	-	-	-	-	-	-	-	-	-	-

C<sub>SH</sub>, coefficient of shortening; C<sub>W</sub>, coefficient of weakness; MFS, Modified Frenchay Scale; Max Ambul Speed, ambulation speed over 10 meters (AT10) at maximal speed, barefoot.

#### Physiological Plausibility: Can Muscle Shortening Aggravate the Abnormal Motor Command?

In models of muscle immobilization in a shortened position in *healthy* animals, muscle spindle firing pathologically increases as shortening of the muscle develops (54-56). These findings were not evident from human microneurography data in spastic paresis, but those studies had insufficient numbers to reach such conclusions (57) or recorded from muscles that were not immobilized in a shortened position [elbow and wrist extensors in Wilson et al. (58) and ankle dorsiflexors in Macefield et al. (59)]. More recently, neuromusculoskeletal models in individuals with chronic stroke-induced hemiparesis suggest that absolute muscle fiber length plays a significant role in the spastic reflex response to imposed movements (60-63). Accordingly, stretch reflex hypersensitivity may be occurring partly through muscle length and extensibility changes, as the pulling force is transmitted more readily to spindles through stiffer hyperelastic structures (4, 5, 54, 56, 64).

A greater muscle afferent input could lead to activitydependent synaptic plasticity at the spinal level. In chronic hemiparesis, a permanent increase in muscle afferent feedback from the shortened muscle (54, 56) could lead to chronic synaptic sensitization at homonymous  $\alpha$ -motoneurons (64–66), decreasing the firing thresholds of these target  $\alpha$ -motoneurons. For the antagonist motoneuron pool, a reciprocal situation may occur where activity-dependent synaptic plasticity (66) could sensitize inhibitory synapses in the reciprocal inhibitory pathway, and this would in turn result in increased inhibition of that antagonist motor neuron (and thereby stretch-sensitive paresis). For both the agonist and antagonist motoneuron pools, such facilitatory, respiratory inhibitory, influence from peripheral afferents, might be unleashed by the potentially decreased presynaptic inhibition linked to disengaging supraspinal control after central lesions (67–70). Interestingly, it has been found in animals that remobilization through step-training may restore reciprocal presynaptic inhibition (71).

## Threshold of Effect: Level of Severity Beyond Which Muscle Shortening Might Worsen the Abnormal Motor Command

A relationship between the clinical estimates of shortening and of weakness was observed in the more shortened lower limb muscles, beyond the median value of the composite coefficients of shortening only. The same relationship was not found below the median value of the composite coefficients of shortening in the lower limb or in the upper limb, except for a trend noted for the SS muscle. The low level of muscle shortening (8%) in the upper limb may have been insufficient to create significant muscle afferent firing and synaptic sensitization at the spinal level. On the other hand, the mean shortening found in the lower limb (12%) may be sufficient to reveal this relationship with the clinical tools used here. When looking at individual examples, several muscles fit with this hypothesis: the EF and the WF were characterized by only 2 and 4% of extensibility loss, respectively, and we did not observe any dependence of the neural command on their shortening. In contrast, the extensibility loss was 15% in SS and data did suggest this relationship for this muscle.

## Impact of Passive Mechanical Properties on Active Function

This study confirmed that, in each of the six investigated muscles of the lower limb, the loss of muscle extensibility and impairment of the motor command both affect motor function in spastic paresis. Considering the composite scores of the lower limb, muscle shortening correlated with ambulation speed more strongly than did the estimated neural command component, with a steeper slope, explaining 26% of the variance of walking speed. Furthermore, individual correlations between each of the six coefficients of muscle shortening in the lower limb and motor function in multivariable analysis indicate the need to consider *all* of these six antagonist muscles to swing phase for assessment, and potentially for treatment. None of the lower limb antagonists alone predicted lower limb function once the regression coefficients were adjusted for the effects of the other predictors.

This strong dependence of motor function on mechanical impairment in the lower limb corroborates previous results. For example, passive resistance of the plantar flexors significantly affects active dorsiflexion amplitude during the swing phase in subjects with hemiparesis (1, 72). Similarly, in adults with cerebral palsy muscle shortening starts in early life, is more severe than in acquired paresis and correlates with walking speed, stair ascent, and descent speeds (73–76). In the upper limb, even though the composite coefficient of shortening did not correlate with motor function in this study, ultrasound measured average fascicle length in EF correlated with impairment level in the upper limb of stroke subjects in recent reports (77, 78).

#### The Predominance of Muscle Shortening in the Lower Limb and of Primary Motor Command Impairment in the Upper Limb

Muscle shortening was 50% more severe in the lower than in the upper limb. In contrast, the composite coefficient of weakness in the upper limb was almost double that in the lower limb.

The overall mild coefficients of shortening found in the upper limb muscle groups confirm previous results obtained in large international studies also using the Five Step Assessment (46, 52, 79). In the lower limb, GN had the highest coefficient of shortening in this study, similar to values found in previous large studies (80, 81). Such findings reflect the dramatic changes in muscle structure known from previous biomechanical investigations in the hemiparetic lower limb, including reduced pennation angle, shorter fascicle length, decreased passive dorsiflexion, and increased ankle stiffness (82–87).

Greater impairment of the motor command occurred in the upper limb even though there was less muscle shortening.



This may indicate that muscle shortening may be only one determinant of the disorder of descending command, obvious other factors being the location and size of the lesion, and the amount of limb disuse since the lesion. Specifically, there is likely to be more severe disuse of the paretic upper limb (also called "functional motor amnesia" or "learned non-use") (88–90), than of the lower limb. Walking represents a critical daily activity necessarily involving both legs while the use of one upper limb might be partly offset when the other functions normally.

#### **Clinical Implications**

The understanding of the role of the muscle disorder on the neural command and on motor function should encourage therapists to consider the muscle disorder as a nosologic entity in hemiparesis and to implement meaningful therapeutic interventions specifically on this target (21, 91). Descriptive results found in this study will help to direct these interventions, addressing particularly the plantar flexors, GM and RF in the lower limb, and the shoulder muscles and FF in the upper limb. Besides the central nervous system, skeletal muscle is another

plastic tissue with response to changes in stimulation and in the environment (18, 91–93). Spastic myopathy should be treated with an appropriate physical treatment, using techniques such as prolonged daily self-stretch postures at high load (53), active stretching (94), short wave and ultrasound therapies (95), as it is known that botulinum toxin injections alone will not allow any long-term meaningful muscle lengthening (52, 96, 97). To minimize muscle damage from the acute stages, vibrations (98), stretching postures through positioning (99, 100) and specific splinting (101), or Leucine and vitamin D (102, 103) might also be helpful.

#### **Study Limitations**

As considered above in the first section of this discussion, the main limitation of this study lies in the clinical nature of its methodology, which comes short of physiologically assessing "true" descending command and "true" passive muscle extensibility. In addition, the weight of the limb segment to lift up against gravity could have impacted the measure of  $X_A$  particularly against the resistance of three of the investigated muscles (SE, GM, and HS). In addition, brain imaging and the role of lesion locations were not analyzed in this study. Lesion locations may have factored into the observed discrepancy between upper and lower limb features. Also, patients were supposed to be affected by purely singular strokes, but some of them, through a long post-stroke state, might have acquired additional subclinical strokes.

*In conclusion*, increased attention should be directed toward abnormal muscle properties in chronic hemiparesis, particularly in the lower limb in which muscle shortening is severe and harmful to ambulation. Beyond a threshold of severity, the

#### REFERENCES

- Dietz V, Quintern J, Berger W. Electrophysiological studies of gait in spasticity and rigidity. Evidence that altered mechanical properties of muscle contribute to hypertonia. *Brain.* (1981) 104:431–49. doi: 10.1093/brain/104.3.431
- Dietz V, Sinkjaer T. Spastic movement disorder: impaired reflex function and altered muscle mechanics. *Lancet Neurol.* (2007) 6:725–33. doi: 10.1016/S1474-4422(07)70193-X
- O'Dwyer NJ, Ada L, Neilson PD. Spasticity and muscle contracture following stroke. *Brain.* (1996) 119:1737–49. doi: 10.1093/brain/119.5.1737
- Gracies JM. Pathophysiology of spastic paresis. Part I. Paresis and soft tissue contracture. *Muscle Nerve*. (2005) 31:535–51. doi: 10.1002/mus.20284
- Gracies JM. Pathophysiology of spastic paresis. Part II. The emergence of muscle overactivity. *Muscle Nerve*. (2005) 31:552– 71. doi: 10.1002/mus.20285
- Norvang OP, Hokstad A, Taraldsen K, Tan X, Lydersen S, Indredavik B, et al. Time spent lying, sitting, and upright during hospitalization after stroke: a prospective observation study. *BMC Neurol.* (2018) 18:138. doi: 10.1186/s12883-018-1134-0
- Urso ML, Scrimgeour AG, Chen YW, Thompson PD, Clarkson PM. Analysis of human skeletal muscle after 48 h immobilization reveals alterations in mRNA and protein for extracellular matrix components. *J Appl Physiol.* (2006) 101:1136–48. doi: 10.1152/japplphysiol.00180.2006
- Kelleher AR, Gordon BS, Kimball SR, Jefferson LS. Changes in REDD1, REDD2, and atrogene mRNA expression are prevented in skeletal muscle fixed in a stretched position during hindlimb immobilization. *Physiol Rep.* (2014) 2:e00246. doi: 10.1002/phy2.246

passive biomechanical and structural abnormalities of the most affected muscles may make a significant contribution to the neural command disorder and to functional disability.

## DATA AVAILABILITY STATEMENT

The original contributions presented in the study are included in the article/supplementary material, further inquiries can be directed to the corresponding author/s.

## **ETHICS STATEMENT**

Ethical review and approval was not required for the study on human participants in accordance with the local legislation and institutional requirements. Written informed consent for participation was not required for this study in accordance with the national legislation and the institutional requirements. Written informed consent was obtained from the individual(s) for the publication of any potentially identifiable images or data included in this article.

## **AUTHOR CONTRIBUTIONS**

J-MG and MP were involved in the conception and design of the study, in the acquisition and analysis of data, and the draft of the manuscript and figures. CM, DB, JV, BB, NB, EH, and MG participated in the analysis of data, the draft of the manuscript, and checked the final draft of the manuscript. All authors read and approved the final manuscript.

- 9. Abadi A, Glover EI, Isfort RJ, Raha S, Safdar A, Yasuda N, et al. Limb immobilization induces a coordinate down-regulation of mitochondrial and other metabolic pathways in men and women. *PLoS ONE.* (2009) 4:e6518. doi: 10.1371/journal.pone.0006518
- Dirks ML, Wall BT, Nilwik R, Weerts DH, Verdijk LB, van Loon LJ. Skeletal muscle disuse atrophy is not attenuated by dietary protein supplementation in healthy older men. J Nutr. (2014) 144:1196–203. doi: 10.3945/jn.114.194217
- McLachlan EM, Chua M. Rapid adjustment of sarcomere length in tenotomized muscles depends on an intact innervation. *Neurosci Lett.* (1983) 35:127–33. doi: 10.1016/0304-3940(83)90539-6
- Tabary JC, Tabary C, Tardieu C, Tardieu G, Goldspink G. Physiological and structural changes in the cat's soleus muscle due to immobilization at different lengths by plaster casts. J Physiol. (1972) 224:231–44. doi: 10.1113/jphysiol.1972.sp009891
- de Bruin M, Smeulders MJ, Kreulen M, Huijing PA, Jaspers RT. Intramuscular connective tissue differences in spastic and control muscle: a mechanical and histological study. *PLoS ONE*. (2014) 9:e101038. doi: 10.1371/journal.pone.0101038
- 14. Honda Y, Sakamoto J, Nakano J, Kataoka H, Sasabe R, Goto K, et al. Upregulation of interleukin-1β/transforming growth factor-β1 and hypoxia relate to molecular mechanisms underlying immobilization-induced muscle contracture. *Muscle Nerve.* (2015) 52:419–27. doi: 10.1002/mus. 24558
- Honda Y, Tanaka M, Tanaka N, Sasabe R, Goto K, Kataoka H, et al. Relationship between extensibility and collagen expression in immobilized rat skeletal muscle. *Muscle Nerve.* (2018) 57:672–8. doi: 10.1002/mus. 26011

- Jalal N, Gracies JM, Zidi M. Mechanical and microstructural changes of skeletal muscle following immobilization and/or stroke. *Biomech Model Mechanobiol.* (2020) 19:61–80. doi: 10.1007/s10237-019-01196-4
- McLachlan EM. Rapid atrophy of mouse soleus muscles after tenotomy depends on an intact innervation. *Neurosci Lett.* (1981) 25:269-74. doi: 10.1016/0304-3940(81)90403-1
- Kelleher AR, Pereira SL, Jefferson LS, Kimball SR. REDD2 expression in rat skeletal muscle correlates with nutrient-induced activation of mTORC1: responses to aging, immobilization, and remobilization. *Am J Physiol Endocrinol Metab.* (2015) 308:E122–9. doi: 10.1152/ajpendo.00341.2014
- Gracies JM. Coefficients of impairment in deforming spastic paresis. Ann Phys Rehabil Med. (2015) 58:173–8. doi: 10.1016/j.rehab.2015.04.004
- Diong J, Harvey LA, Kwah LK, Clarke JL, Bilston LE, Gandevia SC, et al. Gastrocnemius muscle contracture after spinal cord injury: a longitudinal study. *Am J Phys Med Rehabil.* (2013) 92:565–74. doi: 10.1097/PHM.0b013e318274605a
- De Gooijer-van de Groep KL, de Groot JH, van der Krogt H, de Vlugt E, Arendzen JH, Meskers CGM. Early shortening of wrist flexor muscles coincides with poor recovery after stroke. *Neurorehabil Neural Repair.* (2018) 32:645–54. doi: 10.1177/1545968318779731
- Ibrahim IK, Berger W, Trippel M, Dietz V. Stretch-induced electromyographic activity and torque in spastic elbow muscles. Differential modulation of reflex activity in passive and active motor tasks. *Brain.* (1993) 116 (Pt 4):971. doi: 10.1093/brain/116.4.971
- Dietz V, Sinkjaer T. Spasticity. Handb Clin Neurol. (2012) 109:197– 211. doi: 10.1016/B978-0-444-52137-8.00012-7
- 24. Denny-Brown D. *The Cerebral Control of Movement*. Liverpool: Liverpool University Press (1966).
- Tardieu C, Tardieu G, Colbeau-Justin P, Huet de la Tour E, Lespargot A. Trophic muscle regulation in children with congenital cerebral lesions. J Neurol Sci. (1979) 42:357–64. doi: 10.1016/0022-510X(79)90169-2
- Gracies JM, Wilson L, Gandevia SC, Burke D. Stretched position of spastic muscles aggravates their co-contraction in hemiplegic patients. *Ann Neurol.* (1997) 42:438–9.
- Vinti M, Couillandre A, Hausselle J, Bayle N, Primerano A, Merlo A, et al. Influence of effort intensity and gastrocnemius stretch on co-contraction and torque production in the healthy and paretic ankle. *Clin Neurophysiol.* (2013) 124:528–35. doi: 10.1016/j.clinph.2012.08.010
- Vinti M, Bayle N, Hutin E, Burke D, Gracies JM. Stretch-sensitive paresis and effort perception in hemiparesis. J Neural Transm. (2015) 122:1089– 97. doi: 10.1007/s00702-015-1379-3
- Vinti M, Bayle N, Merlo A, Authier G, Pesenti S, Jouve JL, et al. Muscle shortening and spastic cocontraction in gastrocnemius medialis and peroneus longus in very young hemiparetic children. *Biomed Res Int.* (2018) 2018:2328601. doi: 10.1155/2018/2328601
- Gracies JM, Bayle N, Vinti M, Alkandari S, Vu P, Loche CM, et al. Five-step clinical assessment in spastic paresis. *Eur J Phys Rehab Med.* (2010) 46:411– 21.
- Holden MK, Gill KM, Magliozzi MR, Nathan J, Piehl-Baker L. Clinical gait assessment in the neurologically impaired. Reliability and meaningfulness. *Phys Ther.* (1984) 64:35–40. doi: 10.1093/ptj/64.1.35
- Jones TA, Schallert T. Subcortical deterioration after cortical damage: effects of diazepam and relation to recovery of function. *Behav Brain Res.* (1992) 51:1–13. doi: 10.1016/S0166-4328(05)80306-7
- Bütefisch CM, Davis BC, Wise SP, Sawaki L, Kopylev L, Classen J, et al. Mechanisms of use-dependent plasticity in the human motor cortex. *Proc Natl Acad Sci USA*. (2000) 97:3661–5. doi: 10.1073/pnas.97.7.3661
- Hutin E, Ghédira M, Loche CM, Mardale V, Hennegrave C, Gracies JM, Bayle N. Intra- and inter-rater reliability of the 10-meter ambulation test in hemiparesis is better barefoot at maximal speed. *Top Stroke Rehabil.* (2018) 17:1–6. doi: 10.1080/10749357.2018.1460932
- Gracies JM, Hefter H, Simpson D, Moore P. Botulinum toxin in spasticity. In: Moore P, Naumann M, editors. *Handbook of Botulinum Toxin*. New York, Blackwell Science (2002). p. 221–74.
- Baude M, Mardale V, Loche CM, Hutin E, Gracies JM, Bayle N. Intraand inter-rater reliability of the modified frenchay scale to measure active upper limb function in hemiparetic patients. *Ann Phys Rehabil Med.* (2016) 59S:e59–60. doi: 10.1016/j.rehab.2016.07.138

- Gracies JM, Yablon S, Raghavan P, Barbano R, Brashear A, Simpson D. Relationship between active function and tone in a placebo-controlled study of botulinum neurotoxin vs tizanidine in upper limb spasticity. *Arch Phys Med Rehabil.* (2009) 90:e5–6. doi: 10.1016/j.apmr.2009. 08.013
- Pila O, Duret C, Gracies JM, Francisco GE, Bayle N, Hutin É. Evolution of upper limb kinematics four years after subacute robotassisted rehabilitation in stroke patients. *Int J Neurosci.* (2018) 25:1– 10. doi: 10.1080/00207454.2018.1461626
- Gracies JM, Marosszeky JE, Renton R, Sandanam J, Gandevia SC, Burke D. Short-term effects of dynamic lycra splints on upper limb in hemiplegic patients. *Arch Phys Med Rehabil.* (2000) 81:1547–55. doi: 10.1053/apmr.2000.16346
- Lorentzen J, Pradines M, Gracies JM, Nielsen JB. On denny-brown's 'spastic dystonia' - what is it and what causes it? *Clin Neurophysiol.* (2018) 129:89– 94. doi: 10.1016/j.clinph.2017.10.023
- Gracies JM, Burke K, Clegg NJ, Browne R, Rushing C, Fehlings D, et al. Reliability of the Tardieu scale for assessing spasticity in children with cerebral palsy. *Arch Phys Med Rehabil.* (2010) 91:421– 8. doi: 10.1016/j.apmr.2009.11.017
- Patrick E, Ada L. The Tardieu scale differentiates contracture from spasticity whereas the Ashworth scale is confounded by it. *Clin Rehabil.* (2006) 20:173– 82. doi: 10.1191/0269215506cr9220a
- Ben-Shabat E, Palit M, Fini NA, Brooks CT, Winter A, Holland AE. Intra- and interrater reliability of the modified Tardieu scale for the assessment of lower limb spasticity in adults with neurologic injuries. *Arch Phys Med Rehabil.* (2013) 94:2494–501. doi: 10.1016/j.apmr.2013.06.026
- 44. Baude M, Loche CM, Gault-Colas C, Pradines M, Gracies JM. Intra- and inter-raters reliabilities of a stepped clinical assessment of chronic spastic paresis in adults. *Ann Phys Rehab Med.* (2015) 58:e4–5. doi: 10.1016/j.rehab.2015.07.016
- 45. Trudel G, Laneuville O, Coletta E, Goudreau L, Uhthoff HK. Quantitative and temporal differential recovery of articular and muscular limitations of knee joint contractures; results in a rat model. *J Appl Physiol.* (2014) 117:730–7. doi: 10.1152/japplphysiol.00409.2014
- 46. Kapandji AI, editor. Anatomie Fonctionnelle: Tome 2-Membre Inférieur. Paris: Maloine (2009).
- Vielotte J, Bignami B, James-Belin E, Colas C, Gracies JM. Degree of muscle shortening in chronic hemiparesis in patients not treated with guided self-rehabilitation contracts (GSC). *Ann Phys Rehab Med.* (2015) 58:e5. doi: 10.1016/j.rehab.2015.07.018
- Bayle N, Maisonobe P, Raymond R, Balcaitiene J, Gracies JM. Composite active range of motion (CX<sub>A</sub>) and relationship with active function in upper and lower limb spastic paresis. *Clin Rehabil.* (2020) 34:803– 11. doi: 10.1177/0269215520911970
- Singer BJ, Dunne JW, Singer KP, Allison GT. Velocity dependent passive plantarflexor resistive torque in patients with acquired brain injury. *Clin Biomech*. (2003) 18:157–65. doi: 10.1016/S0268-0033(02)00173-0
- Tardieu C, Colbeau-Justin P, Bret MD, Lespargot A, Huet de la Tour E, Tardieu G. An apparatus and a method for measuring the relationship of triceps surae torques to tibio-tarsal angles in man. *Eur J Appl Physiol Occup Physiol.* (1976) 35:11–20. doi: 10.1007/BF00444653
- Winston P, Mills PB, Reebye R, Vincent D. Cryoneurotomy as a percutaneous mini-invasive therapy for the treatment of the spastic limb: case presentation, review of the literature, and proposed approach for use. *Arch Rehabil Res Clin Transl.* (2019) 1:100030. doi: 10.1016/j.arrct.2019.100030
- Gracies JM, O'Dell M, Vecchio M, Hedera P, Kocer S, Rudzinska-Bar M, et al. Effects of repeated abobotulinumtoxinA injections in upper limb spasticity. *Muscle Nerve.* (2018) 57:245–54. doi: 10.1002/ mus.25721
- Pradines M, Ghedira M, Portero R, Masson I, Marciniak C, Hicklin D, et al. Ultrasound structural changes in triceps Surae after a 1year daily self-stretch program: a prospective randomized controlled trial in chronic hemiparesis. *Neurorehabil Neural Repair.* (2019) 33:245– 59. doi: 10.1177/1545968319829455
- Gioux M, Petit J. Effects of immobilising cat peroneus longus muscle on the activity of its own spindles. J Appl Physiol. (1993) 75:2629– 35. doi: 10.1152/jappl.1993.75.6.2629

- Giroux-Metges MA, Pennec JP, Petit J, Morel J, Talarmin H, Droguet M, et al. Effects of immobilizing a single muscle on the morphology and the activation of its muscle fibers. *Exp Neurol.* (2005) 194:495– 505. doi: 10.1016/j.expneurol.2005.03.008
- Rosant C, Nagel MD, Pérot C. Adaptation of rat soleus muscle spindles after 21 days of hindlimb unloading. *Exp Neurol.* (2006) 200:191– 9. doi: 10.1016/j.expneurol.2006.02.003
- Hagbarth KE, Wallin GB, L Löfstedt L. Muscle spindle responses to stretch in normal and spastic subjects. Scand J Rehabil Med. (1973) 5:156-9.
- Wilson LR, Gandevia SC, Inglis JT, Gracies J, Burke D. Muscle spindle activity in the affected upper limb after a unilateral stroke. *Brain.* (1999) 122:2079-88. doi: 10.1093/brain/122.11.2079
- Macefield VG. Discharge rates and discharge variability of muscle spindle afferents in human chronic spinal cord injury. *Clin Neurophysiol.* (2013) 124:114–9. doi: 10.1016/j.clinph.2012.05.015
- Wang R, Herman P, Ekeberg Ö, Gäverth J, Fagergren A, Forssberg H. Neural and non-neural related properties in the spastic wrist flexors: an optimization study. *Med Eng Phys.* (2017) 47:198–209. doi: 10.1016/j.medengphy.2017.06.023
- Kamper DG, Harvey RL, Suresh S, Rymer WZ. Relative contributions of neural mechanisms versus muscle mechanics in promoting finger extension deficits following stroke. *Muscle Nerve.* (2003) 28:309–18. doi: 10.1002/mus.10443
- Mirbagheri MM, Alibiglou L, Thajchayapong M, Rymer WZ. Muscle and reflex changes with varying joint angle in hemiparetic stroke. J Neuroeng Rehabil. (2008) 5:6. doi: 10.1186/1743-0003-5-6
- De Vlugt E, de Groot JH, Wisman WH, Meskers CG. Clonus is explained from increased reflex gain and enlarged tissue viscoelasticity. J Biomech. (2012) 45:148–55. doi: 10.1016/j.jbiomech.2011.09.023
- Maier A, Eldred E, Edgerton VR. The effects on spindles of muscle atrophy and hypertrophy. *Exp Neurol.* (1972) 37:100– 23. doi: 10.1016/0014-4886(72)90229-4
- Klein M, Kandel ER. Presynaptic modulation of voltage-dependent Ca2+ current: mechanism for behavioral sensitization in *Aplysia californica. Proc Natl Acad Sci USA.* (1978) 75:3512–6. doi: 10.1073/pnas.75.7.3512
- Antonov I, Antonova I, Kandel ER, Hawkins RD. The contribution of activity-dependent synaptic plasticity to classical conditioning in Aplysia. J Neurosci. (2001) 21:6413–22. doi: 10.1523/JNEUROSCI.21-16-06413.2001
- 67. Delwaide PJ. Etude Experimentale de L'hyperreflexie Tendineuse en Clinique Neurologique. Bruxelles: Editions Arscia (1971).
- Delwaide PJ. Human monosynaptic reflexes and presynaptic inhibition. In: Desmedt JE, editor. New Developments in Electromyography and Clinical Neurophysiology, Vol 3. Basel: Karger (1973). p. 508–22. doi: 10.1159/000394164
- Koelman JH, Bour LJ, Hilgevoord AA, van Bruggen GJ, Ongerboer de Visser BW. Soleus H-reflex tests and clinical signs of the upper motor neuron syndrome. J Neurol Neurosurg Psychiatry. (1993) 56:776– 81. doi: 10.1136/jnnp.56.7.776
- Faist M, Mazevet D, Dietz V, Pierrot-Deseilligny E. A quantitative assessment of presynaptic inhibition of Ia afferents in spastics. Differences in hemiplegics and paraplegics. *Brain.* (1994) 117:1449–55. doi: 10.1093/brain/117. 6.1449
- Caron G, Bilchak JN, Côté MP. Direct evidence for decreased presynaptic inhibition evoked by PBSt group I muscle afferents after chronic SCI and recovery with step-training in rats. J Physiol. (2020) 598:4621– 42. doi: 10.1113/JP280070
- Santos MJ, Liu H, Liu W. Unloading reactions in functional ankle instability. *Gait Posture.* (2008) 27:589–94. doi: 10.1016/j.gaitpost. 2007.08.001
- Willerslev-Olsen M, Choe Lund M, Lorentzen J, Barber L, Kofoed-Hansen M, Nielsen JB. Impaired muscle growth precedes development of increased stiffness of the triceps surae musculotendinous unit in children with cerebral palsy. *Dev Med Child Neurol.* (2018) 60:672–9. doi: 10.1111/ dmcn.13729
- 74. Van Reeth C, Bayle N, Pauwels C, Gracies JM. Passive mechanical obstacles vs impairment of neurological command in infant vs adult-acquired spastic paresis. *Ann Phys Rehab Med.* (2014) 57:e45. doi: 10.1016/j.rehab.2014.03.161

- Crosbie J, Alhusaini AA, Dean CM, Shepherd RB. Plantarflexor muscle and spatiotemporal gait characteristics of children with hemiplegic cerebral palsy: an observational study. *Dev Neurorehabil.* (2012) 15:114– 8. doi: 10.3109/17518423.2011.643927
- Geertsen SS, Kirk H, Lorentzen J, Jorsal M, Johansson CB, Nielsen JB. Impaired gait function in adults with cerebral palsy is associated with reduced rapid force generation and increased passive stiffness. *Clin Neurophysiol.* (2015) 126:2320–9. doi: 10.1016/j.clinph.2015.02.005
- Nelson CM, Murray WM, Dewald JPA. Motor impairmentrelated alterations in biceps and *Triceps brachii* fascicle lengths in chronic hemiparetic stroke. *Neurorehabil Neural Repair*. (2018) 32:799–809. doi: 10.1177/1545968318792618
- Thielman G, Yourey L. Ultrasound imaging of upper extremity spastic muscle post-stroke and the correlation with function: a pilot study. *NeuroRehabilitation*. (2019) 45:213–20. doi: 10.3233/NRE-192742
- 79. Gracies JM, Esquenazi A, Brashear A, Banach M, Kocer S, Jech R, et al. Efficacy and safety of abobotulinumtoxinA for hemiparesis after stroke or traumatic brain injury in adult patients with upper limb spasticity: a randomised controlled trial. *Lancet Neurol.* (2015) 14:992–1001. doi: 10.1016/S1474-4422(15)00216-1
- Gracies JM, Esquenazi A, Brashear A, Banach M, Kocer S, Jech R, et al. Efficacy and safety of abobotulinumtoxinA in spastic lower limb: Randomized trial and extension. *Neurology.* (2017) 89:2245– 53. doi: 10.1212/WNL.000000000004687
- Ghédira M, Pradines M, Mardale V, Gracies JM, Bayle N, Hutin E. Quantified clinical measures linked to ambulation speed in hemiparesis. *Top Stroke Rehabil.* (2021) 6:1–12. doi: 10.1080/10749357.2021.1943799
- Harlaar J, Becher JG, Snijders CJ, Lankhorst GJ. Passive stiffness characteristics of ankle plantar flexors in hemiplegia. *Clin Biomech.* (2000) 15:261–70. doi: 10.1016/S0268-0033(99)00069-8
- Svantesson U, Takahashi H, Carlsson U, Danielsson A, Sunnerhagen KS. Muscle and tendon stiffness in patients with upper motor neuron lesion following a stroke. *Eur J Appl Physiol.* (2000) 82:275–9. doi: 10.1007/s004210000216
- Gao F, Zhang LQ. Altered contractile properties of the gastrocnemius muscle poststroke. J Appl Physiol. (2008) 105:1802– 8. doi: 10.1152/japplphysiol.90930.2008
- Gao F, Grant TH, Roth EJ, Zhang LQ. Changes in passive mechanical properties of the gastrocnemius muscle at the muscle fascicle and joint levels in stroke survivors. *Arch Phys Med Rehabil.* (2009) 90:819– 26. doi: 10.1016/j.apmr.2008.11.004
- Diong JH, Herbert RD, Harvey LA, Kwah LK, Clarke JL, Hoang PD, et al. Passive mechanical properties of gastrocnemius muscles of people with ankle contracture after stroke. *Arch Phys Med Rehabil.* (2012) 93:1185– 90. doi: 10.1016/j.apmr.2012.02.009
- Zhao H, Ren Y, Roth EJ, Harvey RL, Zhang LQ. Concurrent deficits of soleus and gastrocnemius muscle fascicles and *Achilles tendon* post stroke. J Appl Physiol. (2015) 118:863–71. doi: 10.1152/japplphysiol.00226.2014
- Meige H. Les amnésies motrices fonctionnelles et le traitement des hémiplégiques. *Rev Neurol.* (1905) 13:183–4.
- Taub E, Miller NE, Novack TA, Cook EW, Fleming WC, Nepomuceno CS, et al. Technique to improve chronic motor deficit after stroke. *Arch Phys Med Rehabil.* (1993) 74:347–54.
- André JM, Didier JP, Paysant J. "Functional motor amnesia" in stroke 1904 and "learned non-use phenomenon" 1966. J Rehabil Med. (2004) 36:138– 40. doi: 10.1080/16501970410026107
- Azzollini V, Dalise S, Chisari C. How does stroke affect skeletal muscle? State of the art and rehabilitation perspective narrative review. *Front Neurol.* (2021) 12:797559. doi: 10.3389/fneur.2021.797559
- McComas AJ. Human neuromuscular adaptations that accompany changes in activity. *Med Sci Sports Exerc.* (1994) 26:1498– 509. doi: 10.1249/00005768-199412000-00014
- Williams PE, Goldspink G. Connective tissue changes in immobilised muscle. J Anat. (1984) 138:343–50.
- 94. Ghasemi E, Khademi-Kalantari K, Khalkhali-Zavieh M, Rezasoltani A, Ghasemi M, Akbarzadeh Baghban A, et al. The effect of functional stretching exercises on neural and mechanical properties of the spastic medial gastrocnemius muscle in patients with chronic stroke:

a randomized controlled trial. *J Stroke Cerebrovasc Dis.* (2018) 27:1733–42. doi: 10.1016/j.jstrokecerebrovasdis.2018.01.024

- Rantanen J, Thorsson O, Wollmer P, Hurme T, Kalimo H. Effects of therapeutic ultrasound on the regeneration of skeletal myofibers after experimental muscle injury. *Am J Sports Med.* (1999) 27:54– 9. doi: 10.1177/03635465990270011701
- 96. Gordon MF, Brashear A, Elovic E, Kassicieh D, Marciniak C, Liu J, et al. Repeated dosing of botulinum toxin type A for upper limb spasticity following stroke. *Neurology*. (2004) 63:1971–3. doi: 10.1212/01.WNL.0000144349.95487.91
- 97. Elovic EP, Brashear A, Kaelin D, Liu J, Millis SR, Barron R, et al. Repeated treatments with botulinum toxin type a produce sustained decreases in the limitations associated with focal upper-limb post-stroke spasticity for caregivers and patients. *Arch Phys Med Rehabil.* (2008) 89:799– 806. doi: 10.1016/j.apmr.2008.01.007
- Guang H, Ji L, Shi Y. Focal vibration stretches muscle fibers by producing muscle waves. *IEEE Trans Neural Syst Rehabil Eng.* (2018) 26:839– 46. doi: 10.1109/TNSRE.2018.2816953
- 99. Ada L, Goddard E, McCully J, Stavrinos T, Bampton J. Thirty minutes of positioning reduces the development of shoulder external rotation contracture after stroke: a randomized controlled trial. *Arch Phys Med Rehabil.* (2005) 86:230–4. doi: 10.1016/j.apmr.2004. 02.031
- 100. de Jong LD, Dijkstra PU, Gerritsen J, Geurts AC, Postema K. Combined arm stretch positioning and neuromuscular electrical stimulation during rehabilitation does not improve range of motion, shoulder pain or function in patients after stroke: a randomised trial. *J Physiother.* (2013) 59:245– 54. doi: 10.1016/S1836-9553(13)70201-7
- Salazar AP, Pinto C, Ruschel Mossi JV, Figueiro B, Lukrafka JL, Pagnussat AS. Effectiveness of static stretching positioning on post-stroke upper-limb

spasticity and mobility: systematic review with meta-analysis. Ann Phys Rehabil Med. (2019) 62:274–82. doi: 10.1016/j.rehab.2018.11.004

- 102. Yoshimura Y, Bise T, Shimazu S, Tanoue M, Tomioka Y, Araki M, et al. Effects of a leucine-enriched amino acid supplement on muscle mass, muscle strength, and physical function in post-stroke patients with sarcopenia: a randomized controlled trial. *Nutrition*. (2019) 58:28. doi: 10.1016/j.nut.2018.05.028
- Zielińska-Nowak E, Cichon N, Saluk-Bijak J, Bijak M, Miller E. Nutritional supplements and neuroprotective diets and their potential clinical significance in post-stroke rehabilitation. *Nutrients*. (2021) 13:2704. doi: 10.3390/nu13082704

**Conflict of Interest:** The authors declare that the research was conducted in the absence of any commercial or financial relationships that could be construed as a potential conflict of interest.

**Publisher's Note:** All claims expressed in this article are solely those of the authors and do not necessarily represent those of their affiliated organizations, or those of the publisher, the editors and the reviewers. Any product that may be evaluated in this article, or claim that may be made by its manufacturer, is not guaranteed or endorsed by the publisher.

Copyright © 2022 Pradines, Ghédira, Bignami, Vielotte, Bayle, Marciniak, Burke, Hutin and Gracies. This is an open-access article distributed under the terms of the Creative Commons Attribution License (CC BY). The use, distribution or reproduction in other forums is permitted, provided the original author(s) and the copyright owner(s) are credited and that the original publication in this journal is cited, in accordance with accepted academic practice. No use, distribution or reproduction is permitted which does not comply with these terms.