

Irinotecan and 5-fluorouracil-co-loaded, hyaluronic acid-modified layer-by-layer nanoparticles for targeted gastric carcinoma therapy

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Abstract: For targeted gastric carcinoma therapy, hyaluronic acid (HA)-modified layer-by-layer nanoparticles (NPs) are applied for improving anticancer treatment efficacy and reducing toxicity and side effects. The aim of this study was to develop HA-modified NPs for the co-loading of irinotecan (IRN) and 5-fluorouracil (5-FU). A novel polymer–chitosan (CH)–HA hybrid formulation (HA–CH–IRN/5-FU NPs) consisting of poly(D,L-lactide-*co*-glycolide) (PLGA) and IRN as the core, CH and 5-FU as a shell on the core and HA as the outmost layer was prepared. Its morphology, average size, zeta potential and drug encapsulation ability were evaluated. Human gastric carcinoma cells (MGC803 cells) and cancer-bearing mice were used for the testing of in vitro cytotoxicity and in vivo antitumor efficiency of NPs. HA–CH–IRN/5-FU NPs displayed enhanced antitumor activity in vitro and in vivo than non-modified NPs, single drug-loaded NPs and drugs solutions. The results demonstrate that HA–CH–IRN/5-FU NPs can achieve impressive antitumor activity and the novel targeted drug delivery system offers a promising strategy for the treatment of gastric cancer.

Keywords: gastric carcinoma, irinotecan, 5-fluorouracil, hyaluronic acid, layer-by-layer nanoparticles

Introduction

Gastric cancer (GC) is the fourth most common cancer worldwide and the third leading cause of global cancer mortality, with an estimated 951,600 new cases and 723,100 deaths in 2012.^{1,2} Depending on GC classification and stage, clinical therapeutic regimens include surgery, systemic therapy, radiation therapy and multimodality treatments.^{3–5} However, GC is often diagnosed at an advanced stage, at which surgical techniques are not suitable for these patients. It has been demonstrated that chemotherapy can provide both palliation and improved survival in patients with advanced and metastatic GC.⁶

Older agents such as fluoropyrimidines, platinum compounds and, recently, taxanes and irinotecan (IRN) have shown the most activity as a single active ingredient and in combination regimens in patients with advanced GC.^{7–10} Combination chemotherapy regimens have been widely applied in clinics and bring superior time-to-treatment failure (TTF), progression-free survival (PFS) and overall survival (OS) than single ones.^{11,12} These first-line combination regimens contain cisplatin and fluorouracil (CF); epirubicin, cisplatin and fluorouracil (ECF); epirubicin, oxaliplatin and capecitabine (ECX); fluorouracil, leucovorin and irinotecan (FOLFIRI), etc. The results of a randomized Phase III study comparing FOLFIRI to ECX in patients with advanced

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gastric or esophagogastric junction (EGJ) adenocarcinoma showed longer TTF and better toleration with FOLFIRI than with ECX.¹² To optimize both or multi-drugs' synergistic therapeutic efficacies and reduce side effects, recent efforts have been devoted to developing novel combination nanomedicines. Therefore, we designed multifunctional nanoparticles (NPs) to co-deliver the hydrophilic drug (5-fluorouracil [5-FU]) and the hydrophobic drug (IRN) for gastric carcinoma therapy.

Layer-by-layer (LBL) assembly is a versatile technique to develop multilayer films by the electrostatic attraction of oppositely charged polyelectrolytes.^{13–15} LBL techniques possess the ability to incorporate various agents with different physicochemical properties.^{16,17} In addition, LBL-based NPs could be engineered as the active targeting drug delivery system by the layering materials, which are targeting moieties.^{18,19} Moreover, the assembled polymer layers could carry a large amount of agents and control the release of them, thus having long blood circulation time.¹³

The main purpose of this study was to specifically target and kill GC cells through co-delivery of 5-FU and IRN. As a result, we designed a novel polymer–chitosan (CH)–hyaluronic acid (HA) hybrid formulation (HA–CH–IRN/5-FU NPs) consisting of poly(D,L-lactide-*co*-glycolide) (PLGA) and IRN as the core, CH and 5-FU as a shell on the core and HA as the outmost layer to target GC cells. CH, the natural linear polysaccharide, is a biocompatible, biodegradable and mucoadhesive cationic polymer that exhibits increased and rapid uptake by cancer cells.²⁰ Recently, CH NPs have been exploited extensively in the effective delivery of anticancer agents to the tumor area.^{21,22} HA is a nontoxic, biocompatible, biodegradable and negative polymer that could actively target the variant CD44 receptor commonly overexpressed on various cancers, including breast cancer and GC.^{23,24} HA-decorated NPs have been developed for CD44-targeted GC therapy.^{25–27} Results showed that HA-coated NPs can be effectively used as a targeted antitumor drug delivery system to enhance therapeutic effects and overcome multi-drug resistance. In order to evaluate HA–CH–IRN/5-FU NPs, we further investigated the physical–chemical and biological characteristics, especially the *in vitro* and *in vivo* antitumor efficacy.

Materials and methods

Materials

PLGA (50:50, molecular weight 5,000–15,000) was purchased from the Jinan Daigang Biomaterial Co., Ltd. (Jinan, China). HA (molecular weight 66–90 kDa) was obtained

from Shandong Freda Biochem Co., Ltd. (Jinan, China). CH (degree of deacetylation: 80%; molecular weight 400 kDa), 5-FU, IRN, Pluronic F-68 and 3-(4,5-dimethyl-2-thiazolyl)-2,5-diphenyl-2H-tetrazolium bromide (MTT) were purchased from Sigma-Aldrich Co. (St Louis, MO, USA). Roswell Park Memorial Institute-1640 (RPMI-1640) and fetal bovine serum (FBS) were purchased from Thermo Fisher Scientific (Waltham, MA, USA). All chemicals and reagents used were of analytical grade or better.

Cells and culture

Human gastric carcinoma cells (MGC803 cells) were purchased from American Type Culture Collection (Manassas, VA, USA) and were grown in an RPMI-1640 medium containing 10% FBS and 1% antibiotic antimycotic at 37°C and a humidified 5% CO₂ atmosphere.

Animals and guidelines

Balb/c nude mice (8 weeks old, 20 g weight) were purchased from Shanghai Slack Laboratory Animal Co., Ltd. (Shanghai, China) and housed in ventilated cages at a temperature of 20°C±2°C and a relative humidity of 60%±5%. All animal experiments comply with the National Institutes of Health Guide for the care and use of laboratory animals (NIH Publication No 8023, revised 1978), and the animal experiments was approved by the medical ethics committee of Shandong University (No 100120160189).

Preparation of IRN-loaded PLGA NPs

IRN-loaded PLGA NPs (IRN NPs) was prepared by solvent displacement technique.²⁸ Briefly, IRN (20 mg) and PLGA (100 mg) were dissolved in acetone (5 mL) to get the organic phase. In all, 1% F68 (w/v) was dissolved in Milli-Q water (50 mL) to obtain the aqueous solution. The organic phase was added drop by drop into the aqueous solution (50 mL) and stirred by a laboratory magnetic stirrer (400 rpm at room temperature) for 8 h to completely evaporate the organic solvent. The obtained NP suspensions were collected by centrifugation at 10,000 rpm for 15 min, resuspended in Milli-Q water, washed three times and filtered through a 0.45 µm membrane. The obtained NPs were stored at 2°C–8°C.

Preparation of 5-FU-loaded CH NPs

5-FU-loaded CH NPs (5-FU NPs) were prepared by the self-assembly technique.²⁹ Briefly, 5-FU (20 mg) was dissolved in Milli-Q water (5 mL) added drop by drop into the CH (100 mg) in acetic acid (1% v/v) solution. The obtained NP

suspensions were collected by centrifugation at 10,000 rpm for 15 min, resuspended in Milli-Q water, washed three times and filtered through a 0.45 μm membrane. The obtained NPs were stored at 2°C–8°C.

Preparation of HA–CH–IRN/5-FU NPs

PLGA–CH hybrid NPs (CH–IRN/5-FU NPs) were prepared as follows: 5-FU (20 mg) was mixed with CH (100 mg) in acetic acid (1% v/v) solution and then added drop by drop into the IRN NP suspensions.

HA–CH–IRN/5-FU NPs (Figure 1A) was fabricated by adding HA solution drop by drop into the CH–IRN/5-FU NP suspensions.³⁰ The obtained CH–IRN/5-FU NP and HA–CH–IRN/5-FU NP suspensions were collected by centrifugation at 10,000 rpm for 15 min, resuspended in Milli-Q water, washed three times and filtered through a 0.45 μm membrane. The obtained NPs were stored at 2°C–8°C.

Blank HA- and CH-containing NPs not including IRN and 5-FU (HA–CH NPs) were prepared by the same procedure without adding the two drugs.

Characterization of NPs

Transmission electron microscopy (TEM) was used to investigate the morphology of HA–CH–IRN/5-FU NPs, using JEM-1200EX transmission electron microscope

(JEOL, Tokyo, Japan).³¹ One drop of HA–CH–IRN/5-FU NPs was placed onto a copper grid and air-dried. A drop of 2% aqueous solution of sodium phosphotungstate was applied as a negative stain, and the NPs were then examined under the microscope.

Mean particle size (volume mean diameter), polydispersity index (PDI) and zeta potential of NPs were characterized using photon correlation spectroscopy with a Zetasizer 3000 (Malvern Instruments, Malvern, UK) as described in our previous study.³²

The IRN and 5-FU entrapment efficiency (EE) in NPs was determined by high-performance liquid chromatography (HPLC; LC-20A; Shimadzu, Tokyo, Japan). 5-FU content was quantified using 250 \times 4.6 mm C18 column.²⁹ The mobile phase (flow rate 0.6 mL/min) was KH_2PO_4 0.05 M triethylamine 0.1%, and ultraviolet detection was set at 266 nm. Quantitative analysis of IRN was carried out by spectrophotometric assay (UV-1800, UV-VIS spectrophotometer; Shimadzu) at 370 nm.³³ The EE of the NPs was calculated according to the following equation: EE (%) = drug amount in NPs/drug feeding \times 100.

Serum stability of HA–CH–IRN/5-FU NPs and single drug-loaded NPs was evaluated in phosphate-buffered saline (PBS) containing 10% FBS (v/v) at 37°C for 72 h. At times 0, 2, 4, 8, 24, 48 and 72 h, 1 mL of each sample was diluted with

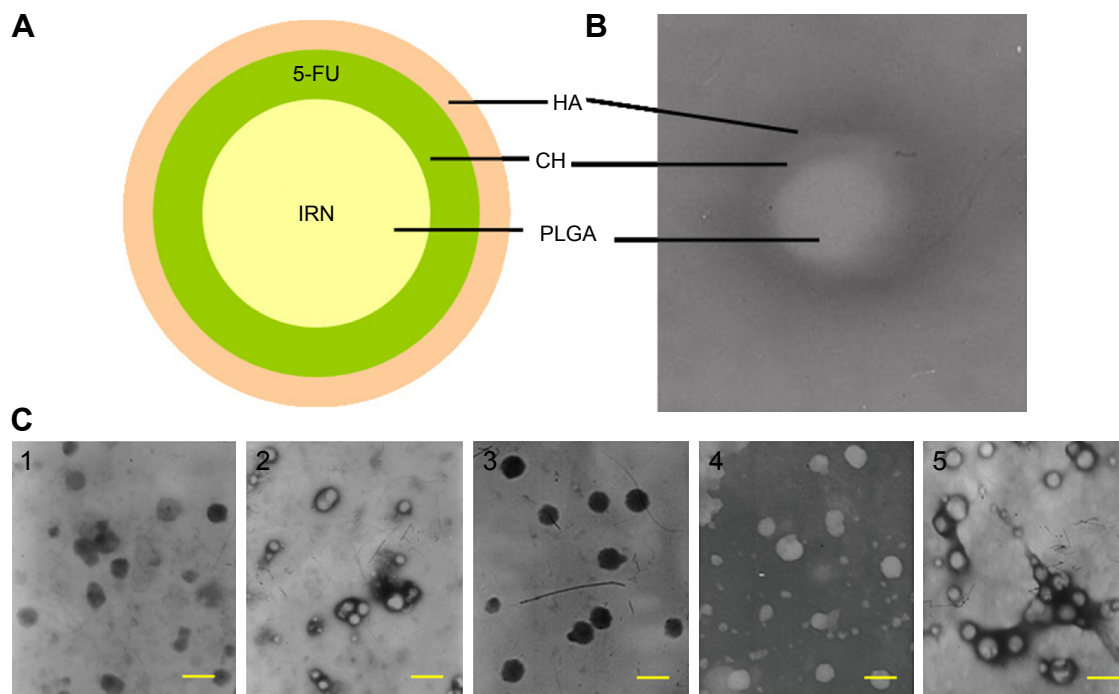


Figure 1 Scheme graph and TEM images of HA-CH-IRN/5-FU NPs and other NPs.

Notes: (A) Scheme graph of the structure of HA–CH–IRN/5-FU NPs. (B) TEM image of HA–CH–IRN/5-FU NPs. (C) TEM images of HA–CH–IRN/5-FU NPs (1), CH–IRN/5-FU NPs (2), IRN NPs (3), 5-FU NPs (4) and HA–CH NPs (5) (yellow scale bars represent 200 nm).

Abbreviations: HA, hyaluronic acid; CH, chitosan; IRN, irinotecan; 5-FU, 5-fluorouracil; NP, nanoparticle; PLGA, poly(D,L-lactide-co-glycolide); TEM, transmission electron microscopy.

2 mL of triethylamine and the mixture was bath sonicated for 5 min, followed by centrifugation at 10,000 rpm for 5 min. The variation trends of the particle size were evaluated.

In vitro drug release studies

In vitro drug release studies were performed on IRN and/or 5-FU-co-loaded NPs.³⁴ Briefly, 50 mg of NPs were resuspended in 10 mL of PBS and placed at 37°C in a shaker incubator shaking at the speed of 100 rpm. At predetermined times (1, 2, 4, 8, 12, 24, 48 and 72 h), the suspension was centrifuged at 12,000 rpm for 10 min, the supernatant was harvested and the amount of IRN and 5-FU was quantified by the method mentioned in the “characterization of NPs” section. The pellets of NPs were resuspended in fresh PBS in the original tube for further incubation.

Cellular uptake studies

The uptake rates of IRN and/or 5-FU-co-loaded NPs by MGC803 cells were tested using coumarin 6 as a model fluorescent molecule, which can be encapsulated into various NPs for quantitative investigation.³¹ Kinds of coumarin 6-loaded NPs were prepared by the same method as described in the “Preparation of IRN-loaded PLGA NPs”, “Preparation of 5-FU-loaded CH NPs” and “Preparation of HA-CH-IRN/5-FU NPs” sections, with the adding of 20 mg coumarin 6 along with the drugs into each formula. Coumarin 6-loaded NPs were added at concentrations of 200 mg/mL into MGC803 cells equilibrated with Hank’s buffered salt solution (HBSS) at 37°C. After incubation for 24 and 72 h, the medium was removed and the wells were washed three times with cold PBS solution. Then, cells were washed once with 1 mL of PBS; detached with trypsin/EDTA, centrifuged at 1,500 rpm, 4°C for 5 min; resuspended in 300 µL of PBS and directly introduced to a flow cytometer.

In vitro cytotoxicity assays

In vitro cytotoxicity of NPs was estimated in MGC803 cells using MTT assay.³⁵ Briefly, MGC803 cells were seeded in 96-well plates at a density of 2,000 cells/well and incubated for 24 h. IRN- and/or 5-FU-contained solutions or NPs were added at various concentrations for 48 h. MTT was then added to the media at a concentration of 5 mg/mL and incubated for 4 h. The formazan crystals were dissolved in 100 µL dimethyl sulfoxide (DMSO), and optical absorbance was recorded at 570 nm with a Model 680 Microplate Reader (Bio-Rad Laboratories Inc., Hercules, CA, USA). Cell viability was calculated as percentage of the untreated control.

Synergistic effect evaluation and selection of the ratio of drugs

To evaluate the synergistic effects and select the suitable ratio of drug co-loaded in the NPs, the combination index (CI) was measured according to the Chou and Talalay’s method.^{36,37} Based on the cell viability results calculated in the “Cellular uptake studies” section, the median inhibitory concentration (IC₅₀) values were calculated using Origin 8.0 (OriginLab, Northampton, MA, USA). CI was calculated by the equation: $CI = [(C)_{IRN}/(C_{50})_{IRN}] + [(C)_{5-FU}/(C_{50})_{5-FU}]$. (C)_{IRN} and (C)_{5-FU} represents the concentration of IRN and 5-FU in the combination system at the IC₅₀ value. (C₅₀)_{IRN} and (C₅₀)_{5-FU} represent the IC₅₀ value of IRN alone and 5-FU alone, respectively. CI < 1, CI = 1 and CI > 1 indicate synergism, additive effect and antagonism, respectively.

Tumor induction

Tumors were induced in mice by subcutaneous injection of MGC803 cells (10⁷ cells suspended in 100 µL normal saline) into the right and left flanks on the dorsal side of the Balb/c nude mice.³⁸ The measurements were taken in two perpendicular dimensions, and tumor volumes were calculated by the following equation: tumor volume (mm³) = (longest diameter × shortest diameter²)/2. When the volume of the tumor reached ~50 mm³ (~1 day), the GC-bearing mice were divided into eight groups (with eight mice in each group) that were ready for the treatment.

In vivo tissue distribution study

The GC-bearing mice model was used to investigate the in vivo tissue distribution of IRN- and/or 5-FU-contained solutions or NPs.³⁹ The mice were divided into several groups and administered 1 mL of solutions or NPs through the tail vein separately. At predetermined time intervals, mice were sacrificed and the heart, liver, spleen, lung, kidney, stomach, colon and tumor of mice were collected. The tissues were cut into small pieces and homogenized with physiological saline. After appropriate dilution of supernatants, the content of IRN and 5-FU was quantified by the method mentioned in the “Characterization of NPs” section.

In vivo antitumor effect and system toxicity evaluation

In vivo antitumor effect and system toxicity of the NPs were evaluated in terms of tumor volume and body weight changes.⁴⁰ The mice were divided into several groups and administered IRN- and/or 5-FU-contained solutions or NPs every other day for 3 weeks. Tumor sizes and mouse body

weights were measured. Tumor volumes were calculated using the equation presented in the “Synergistic effect evaluation and selection of the ratio of drugs” section.

Statistical analysis

The level of significance in all statistical analyses was set at a probability of $P < 0.05$. Experiments were performed at least three times ($n=3$) and expressed as mean \pm SD. Statistical differences were determined using Student's *t*-test for comparison of two groups and one-way ANOVA for multiple groups.

Results

Characterization of HA–CH–IRN/5-FU NPs

Morphology of HA–CH–IRN/5-FU NPs exhibited an LBL type of spherical particle (Figure 1B). It appeared as a white core, a gray first layer over the core and a darker outside second layer. Morphology of other NPs is presented in Figure 1C. Mean particle size, PDI and zeta potential were also tested (Table 1). The size of NPs was increased from 91 to 153 along with the LBL formation procedure, indicated that the coating of CH and HA layer enlarged the particles. Zeta potential of the NPs varied due to the positive or negative charges of the materials used. The EE of IRN- and/or 5-FU-loaded NPs was $>90\%$. Changes in size in the presence of serum are described in Figure 2. The NPs tested were stable up to 72 h without any significant size changes.

In vitro drug release

In vitro release of IRN and 5-FU from NPs was in a sustained behavior (Figure 3). The release behavior of 5-FU (Figure 3B) from the NPs was faster than that of IRN (Figure 3A). The release rate of HA–CH–IRN/5-FU NPs was the slowest. The release rate of drugs from CH–IRN/5-FU NPs was slower than that of IRN NPs. 5-FU released from 5-FU NPs was more slower than from the CH–IRN/5-FU NPs.

Cellular uptake

Cellular uptake efficiency of the NPs was tested. As shown in Figure 4, cellular uptake efficiency of HA–CH–IRN/5-FU NPs and HA–CH NPs was significantly higher than other NPs, reached $>80\%$ at 72 h post treatments ($P < 0.05$). Cellular uptake efficiency of CH–IRN/5-FU NPs, IRN NPs and 5-FU NPs showed no obvious difference compared with each other.

In vitro cytotoxicity

In vitro cytotoxicity of IRN- and/or 5-FU-contained solutions or NPs was investigated using MGC803 cells. Following incubation with samples for 48 h, cell viability was summarized (Figure 5). HA–CH–IRN/5-FU NPs exhibited the most effective tumor cell inhibition ability among all samples tested. The results illustrated that the drug-loaded NPs were more efficient than free drug solutions ($P < 0.05$). Double drugs contained NPs, and the solution also had a higher cytotoxicity than single drug-contained NPs and solution ($P < 0.05$).

Synergistic effect and selection of the ratio of the two drugs

Dual drug-co-loaded NPs with various IRN to 5-FU weight ratios were applied to MGC803 cells using MTT assay to determine the synergistic effect and selection of the ratio of the two drugs (Table 2). The combination therapy showed synergistic effect when IRN to 5-FU ratio was 2:1. The CI_{50} values for HA–CH–IRN/5-FU NPs, CH–IRN/5-FU NPs and IRN/5-FU solutions were 0.521, 0.884 and 0.787, respectively. The IRN to 5-FU weight ratio of 2:1 exhibited stronger synergism in both NPs and solution formulations; thus, this ratio was determined in this study. So the ration of 2:1 (IRN to 5-FU, w/w) was used for all the in vitro and in vivo studies.

In vivo tissue distribution

In vivo tissue distribution of HA–CH–IRN/5-FU NPs, CH–IRN/5-FU NPs and IRN/5-FU solution was investigated

Table 1 Characterization of NPs

Formulations	HA–CH–IRN/5-FU NPs	CH–IRN/5-FU NPs	IRN NPs	5-FU NPs	HA–CH NPs
Particle size (nm)	153.8 \pm 5.6	127.3 \pm 4.8	91.4 \pm 3.6	86.9 \pm 3.9	155.1 \pm 5.2
Size distribution (PDI)	0.187 \pm 0.021	0.164 \pm 0.018	0.118 \pm 0.012	0.147 \pm 0.016	0.184 \pm 0.025
Zeta potential (mV)	-13.7 \pm 1.9	+17.5 \pm 2.6	-16.9 \pm 2.2	+25.8 \pm 3.7	-15.2 \pm 2.4
EE of IRN (%)	94.5 \pm 2.3	93.6 \pm 2.1	92.8 \pm 2.8	N/A	N/A
EE of 5-FU (%)	91.4 \pm 3.1	92.3 \pm 2.9	N/A	93.4 \pm 3.2	N/A

Abbreviations: NPs, nanoparticles; HA, hyaluronic acid; CH, chitosan; IRN, irinotecan; 5-FU, 5-fluorouracil; PDI, polydispersity index; EE, entrapment efficiency; N/A, not applicable.

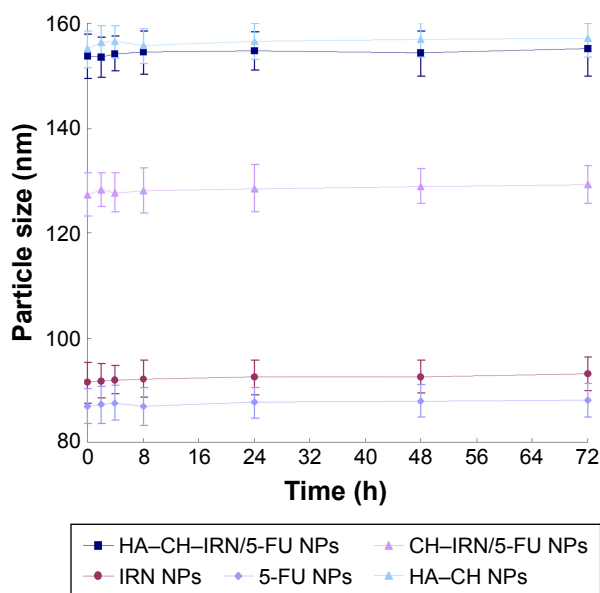


Figure 2 Changes in size in the presence of serum.

Note: Data are presented as mean \pm SD ($n=3$).

Abbreviations: HA, hyaluronic acid; CH, chitosan; IRN, irinotecan; 5-FU, 5-fluorouracil; NPs, nanoparticles.

in GC-bearing mice model (Figure 6). IRN and 5-FU distributions of HA-CH-IRN/5-FU NPs were higher in the tumor tissue than those of CH-IRN/5-FU NPs and IRN/5-FU solution ($P<0.05$). Drugs loaded in NPs had relatively lower accumulation in heart and kidney than drugs' solution ($P<0.05$).

In vivo antitumor effect and system toxicity

In vivo antitumor efficiency was evaluated in GC-bearing mice model (Figure 7A). The most obvious tumor inhibition was clearly observed in the HA-CH-IRN/5-FU NPs group; the tumor growth was prominently delayed, which attained $\sim 217 \text{ mm}^3$ on 21-day posttreatment. The 0.9% saline control group had a tumor volume of $1,530 \text{ mm}^3$ on day 21. Tumor growth was more significantly inhibited by drug-loaded NPs than free drug solutions ($P<0.05$). Dual drug-co-loaded NPs and solutions showed better tumor suppression efficacy than the single drug containing NPs and solutions ($P<0.05$).

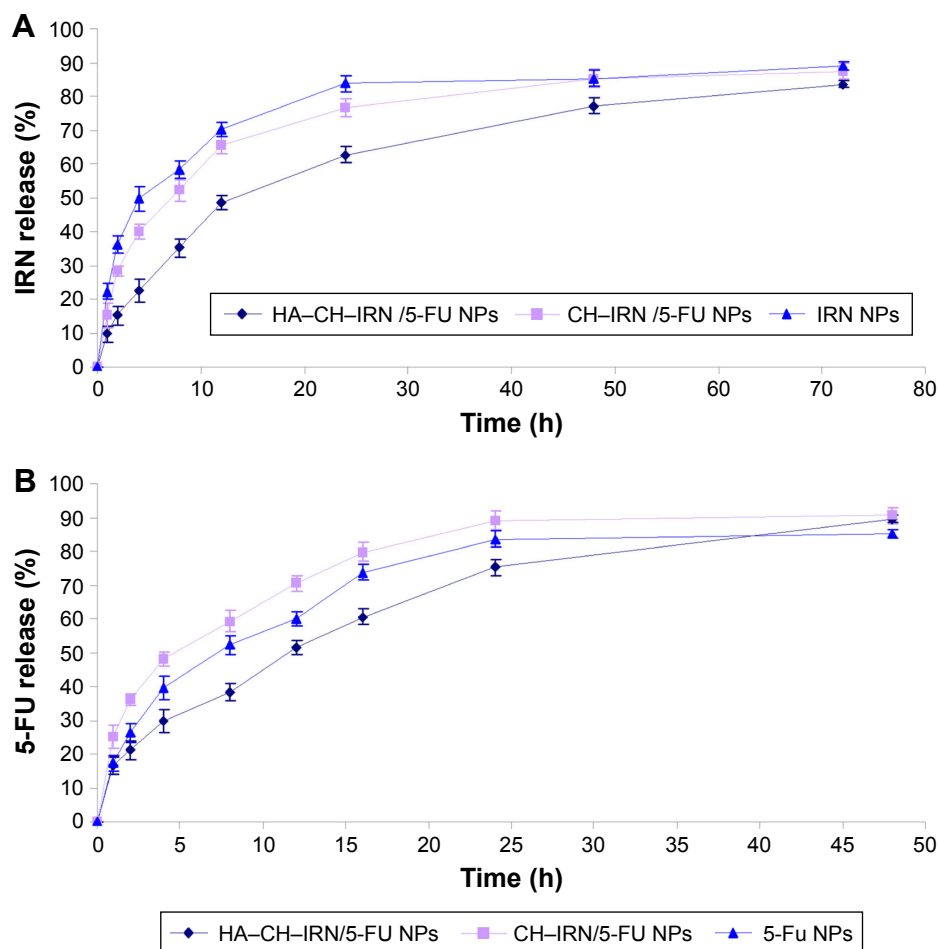


Figure 3 In vitro release of IRN (A) and 5-FU (B) from NPs.

Note: Data are presented as mean \pm SD ($n=3$).

Abbreviations: IRN, irinotecan; 5-FU, 5-fluorouracil; NPs, nanoparticles; HA, hyaluronic acid; CH, chitosan.

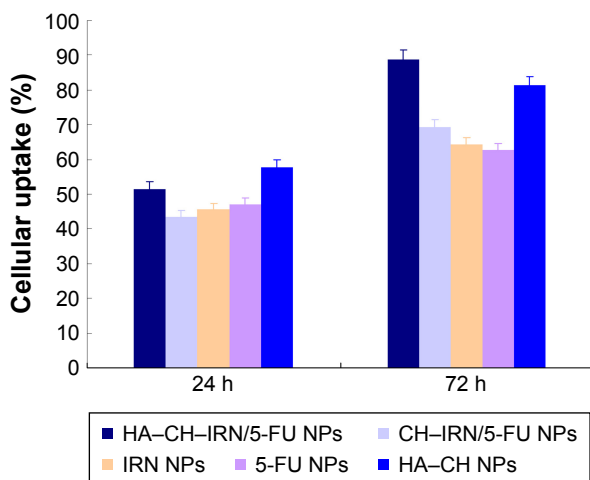


Figure 4 Cellular uptake efficiency of the NPs.

Note: Data are presented as mean \pm SD (n=3).

Abbreviations: NPs, nanoparticles; HA, hyaluronic acid; CH, chitosan; IRN, irinotecan; 5-FU, 5-fluorouracil.

HA-CH-IRN/5-FU NPs exhibited better tumor inhibition ability than non-modified CH-IRN/5-FU NPs ($P < 0.05$). The obvious emaciation could be observed in the free drug solution groups, with an obvious decrease in the body weight (Figure 7B). The NP groups did not cause a significant difference in body weight changes. A significant body weight increase was found in the 0.9% saline control group.

Discussion

LBL assembly techniques are promising strategies for incorporating various agents with different physicochemical

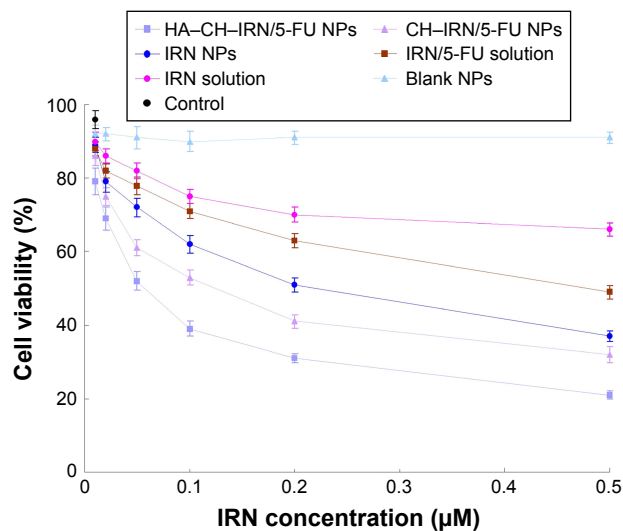


Figure 5 In vitro cytotoxicity of IRN and/or 5-FU-contained solutions or NPs investigated in MGC803 cells.

Note: Data are presented as mean \pm SD (n=3).

Abbreviations: IRN, irinotecan; 5-FU, 5-fluorouracil; NPs, nanoparticles; HA, hyaluronic acid; CH, chitosan.

Table 2 Synergistic effect evaluation and selection of the ratio of drugs by CI calculation

Formulations	IRN/5-FU ratio (w/w)	IC ₅₀ IRN (µM)	IC ₅₀ 5-FU (µM)	CI ₅₀
IRN NPs	N/A	0.261	N/A	N/A
5-FU NPs	N/A	N/A	0.123	N/A
CH-IRN/5-FU NPs	4/1	0.242	0.061	1.423
CH-IRN/5-FU NPs	2/1	0.112	0.056	0.884
CH-IRN/5-FU NPs	1/1	0.096	0.096	1.148
HA-CH-IRN/5-FU NPs	2/1	0.066	0.033	0.521
IRN solution	N/A	1.961	N/A	N/A
5-FU solution	N/A	N/A	1.162	N/A
IRN/5-FU solution	2/1	0.837	0.419	0.787

Abbreviations: CI, combination index; IRN, irinotecan; 5-FU, 5-fluorouracil; IC₅₀, median inhibitory concentration; NPs, nanoparticles; N/A, not applicable; CH, chitosan; HA, hyaluronic acid.

properties, and LBL-based NPs could be engineered as the targeted drug delivery system to provide enhanced stability, cellular uptake, regulation of drug release and targeting capabilities.⁴¹ In this study, we used the LBL technique to develop multilayer NPs by the electrostatic interaction of oppositely charged HA (negative) and CH (positive). Moreover, because of the specific binding between HA and CD44, our NPs can be used for targeted delivery of anticancer drugs into GC that are commonly overexpressed with CD44.

Electrostatic interactions are widely reported to be the main driving force for the multilayer formation process between two oppositely charged polyelectrolytes for the LBL technique.^{42,43} Morphology, size and zeta potential of NPs are often characterized to determine whether an additional layer could be successfully formulated onto the previous carriers. Figure 1B illustrates the layered core-shell structure of HA-CH-IRN/5-FU NPs; this could be the evidence that the system was successfully assembled. Moreover, the increased particle size indicated that the coating of CH and HA layers enlarged the particles. Zeta potential of the NPs was reversed due to the positive or negative charged materials used. The NPs tested were stable up to 72 h without any significant size changes in serum and suggest in a period of time that this formulation may be stable when intravenously administrated.

Sustained release behavior of IRN and 5-FU from NPs could significantly improve the therapeutic efficacy of the drugs loaded.²⁷ Faster release behavior of 5-FU from the NPs than that from IRN could be explained by stating that the 5-FU was loaded in the outer layer of the NPs and the IRN was loaded in the inner core. More slowly release of 5-FU from 5-FU NPs than from the CH-IRN/5-FU NPs may be due to the preparation of 5-FU NPs using a large amount of CH that may stuck the 5-FU release.

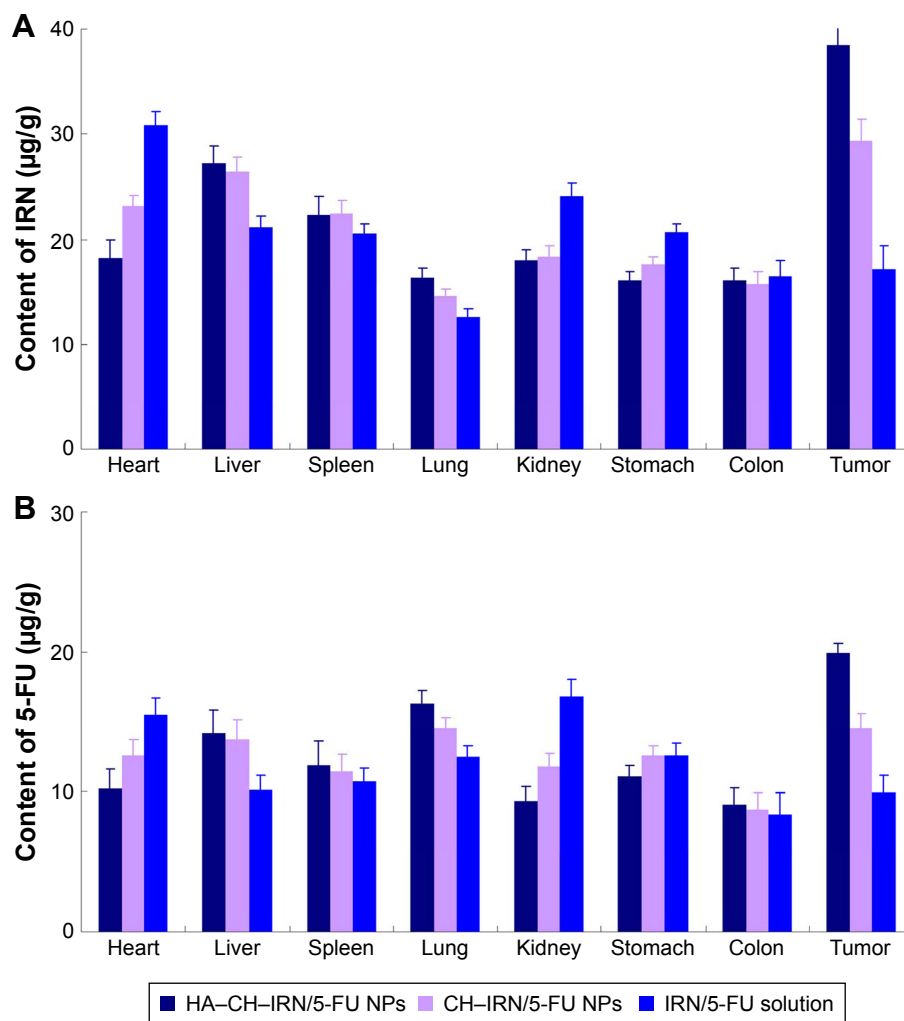


Figure 6 In vivo tissue distribution of IRN (A) and 5-FU (B) investigated in GC-bearing mice model.

Note: Data are presented as mean ± SD (n=8).

Abbreviations: IRN, irinotecan; 5-FU, 5-fluorouracil; GC, gastric cancer; HA, hyaluronic acid; CH, chitosan; NPs, nanoparticles.

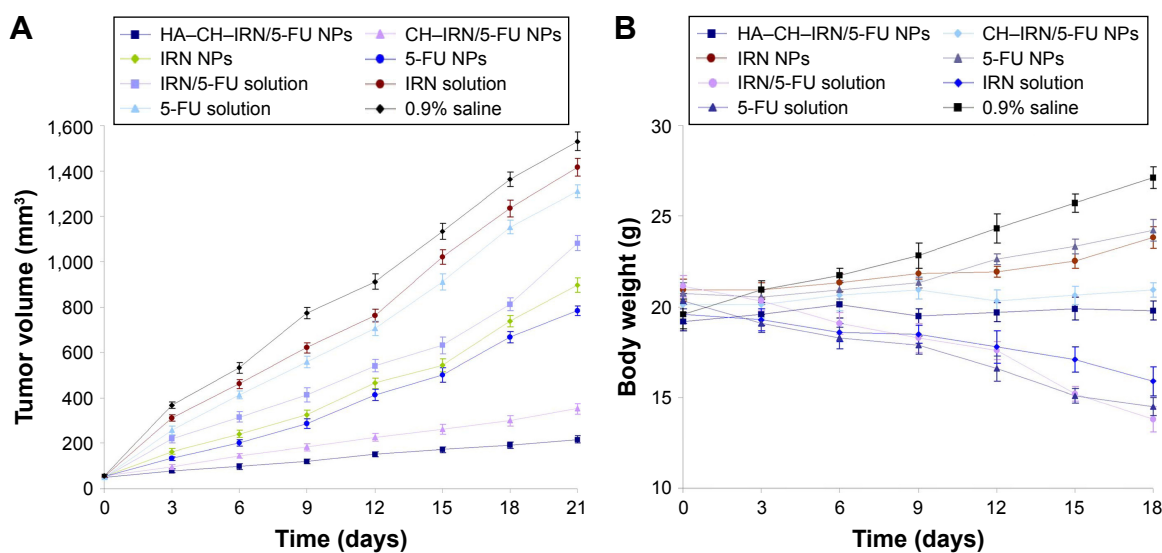


Figure 7 In vivo antitumor effect and system toxicity of the NPs evaluated in terms of tumor volume (A) and body weight changes (B).

Note: Data are presented as mean ± SD (n=8).

Abbreviations: NPs, nanoparticles; HA, hyaluronic acid; CH, chitosan; IRN, irinotecan; 5-FU, 5-fluorouracil.

The therapeutic effects of the NPs would depend on internalization of the NPs to the cancer cells. Coumarin 6, a fluorescent probe, was used to represent the drug in the NP formulation to analyze cellular uptake of the NPs. Cellular uptake efficiency of HA-CH-IRN/5-FU NPs was significantly higher than other NPs. This could be attributed to enhanced cancer cell-specific adherence of the HA ligands. This behavior may improve the activity and overcome drug resistance.³¹ In order to investigate the cytotoxicity and synergistic effect of dual drug-co-loaded NPs, we have performed a cell viability study using MGC803 cells in an in vitro MTT assay. Evaluation of drug-drug interaction is important in all areas of medicine and particularly in combination cancer chemotherapy.⁴⁴ Chou and Talalay⁴⁵ in 1983 introduced the term CI for quantification of synergism or antagonism for two drugs. If the CI value is < 1 , synergism is indicated, and if the CI value is 1 to infinity, antagonism is indicated.⁴⁶ When IRN to 5-FU weight ratio was 2:1, the CI_{50} values for HA-CH-IRN/5-FU NPs, CH-IRN/5-FU NPs and IRN/5-FU solution were < 1 . This section confirmed the synergistic effect and the best IRN to 5-FU ratio of the two drug-containing systems.

In vivo drug distribution of NPs was higher in the tumor tissue and lower in heart and kidney, which could decrease the side effects during the tumor therapy.⁴⁷ On the contrary, the drug solution samples mainly distributed in heart and kidney. This may lead to systemic toxicity. Higher drug distribution of NPs formulations in tumor might be due to the sustained release behavior and targeted ability of the NPs thus prolonged the blood circulation time and could better target the tumor site.

It was observed that in vivo antitumor efficiency of the dual drugs could be better after loading in the NPs because of the higher tumor volume suppression. The higher antitumor efficiency of drugs after co-loaded in HA-CH-IRN/5-FU NPs than non-modified CH-IRN/5-FU NPs is related to the targeted ability of HA.⁴⁸ Based on the healthy body weight of NP-treated mice, the NPs constructed were proposed as safe carriers for the delivery of anticancer drugs. Minimizing the toxicity and side effects of drugs could prove the targeting efficiency of NPs. The in vivo antitumor results suggested the best anti-tumor effect of folate decorated double drugs contained NLCs due to the synergetic effect of the two drugs, and the least systemic toxic side effect of the NLC formulations for the head and neck cancer treatment.

Conclusion

HA-CH-IRN/5-FU NPs consisting of PLGA and IRN as the core, CH and 5-FU as a shell on the core and HA as

the outmost layer were prepared. HA-CH-IRN/5-FU NPs displayed enhanced antitumor activity in vitro and in vivo than non-modified NPs, single drug-loaded NPs and drug solutions. The results demonstrate that HA-CH-IRN/5-FU NPs can achieve impressive antitumor activity and the novel targeted drug delivery system offers a promising strategy for the treatment of GC.

Disclosure

The authors report no conflicts of interest in this work.

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