

CELL BIOLOGY

Receptor dimer stabilization by hierarchical plasma membrane microcompartments regulates cytokine signaling

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The interaction dynamics of signaling complexes is emerging as a key determinant that regulates the specificity of cellular responses. We present a combined experimental and computational study that quantifies the consequences of plasma membrane microcompartmentalization for the dynamics of type I interferon receptor complexes. By using long-term dual-color quantum dot (QD) tracking, we found that the lifetime of individual ligand-induced receptor heterodimers depends on the integrity of the membrane skeleton (MSK), which also proved important for efficient downstream signaling. By pair correlation tracking and localization microscopy as well as by fast QD tracking, we identified a secondary confinement within ~300-nm-sized zones. A quantitative spatial stochastic diffusion-reaction model, entirely parameterized on the basis of experimental data, predicts that transient receptor confinement by the MSK meshwork allows for rapid reassociation of dissociated receptor dimers. Moreover, the experimentally observed apparent stabilization of receptor dimers in the plasma membrane was reproduced by simulations of a refined, hierarchical compartment model. Our simulations further revealed that the two-dimensional association rate constant is a key parameter for controlling the extent of MSK-mediated stabilization of protein complexes, thus ensuring the specificity of this effect. Together, experimental evidence and simulations support the hypothesis that passive receptor confinement by MSK-based microcompartmentalization promotes maintenance of signaling complexes in the plasma membrane.

INTRODUCTION

Signal transduction across the plasma membrane (PM) frequently involves the association of transmembrane receptors to dimeric or oligomeric complexes. These complexes are formed by reversible, noncovalent interactions and thus continuously associate and dissociate. Nanoscale hierarchical organization of the PM caused by the cortical actin meshwork [membrane skeleton (MSK)], membrane microdomains (lipid rafts), and protein-protein interactions (1–8) has been speculated to play an important role in the assembly and dynamics of signaling complexes (9–14). In particular, dimerization of receptor tyrosine kinases and related receptors has been suspected of being highly regulated by PM compartmentalization (15–17). However, the function of transient confinement by nanoscale membrane domains in sustaining individual, functional signaling complexes has remained largely speculative (18).

Here, we have explored the assembly and dynamics of the type I interferon (IFN) receptor by single quantum dot (QD) tracking and localization microscopy (TALM). The IFN receptor comprises two subunits, IFNAR1 and IFNAR2, which are expressed at low cell surface densities (typically a few 100 copies per cell) (19). IFNAR1 and IFNAR2 are dimerized by simultaneous interaction with IFN via independent binding epitopes (19–21). IFNAR2 binds IFN α 2 with an equilibrium dissociation constant of ~5 nM and a complex lifetime of ~100 s (22), whereas the affinity toward IFNAR1 is three orders of magnitude lower, and the complex dissociates about 100-fold faster

(20, 23). Different members of the IFN family bind IFNAR1 with distinct binding affinities and kinetics, which has been correlated with their differential cellular activities (24, 25). By exploiting recent progress in nanoparticle monofunctionalization and receptor cell surface labeling (26), we unraveled here the diffusion and interaction dynamics of individual receptor dimers in the PM of living cells by single QD tracking (27–32), enabling long-term observation of individual IFNAR signaling complexes with very high spatial and temporal resolution (Fig. 1A). On the basis of spatiotemporal correlation analyses of single complex trajectories, we identified transient dissociation and reassociation of complexes within MSK nanostructures. Integrating our comprehensive experimental data with quantitative spatial stochastic models suggests that hierarchical, two-tiered PM compartmentalization governs efficient reassociation of receptor dimers, implicating a sensitive interplay of MSK-based diffusion barriers and receptor dimerization dynamics.

RESULTS

Dimerization of IFNAR1 and IFNAR2 is induced by IFN

IFNAR dimerization and the lifetime of receptor dimers at the PM were explored by single-molecule localization microscopy using QD labeling, ensuring high photostability and long-term imaging with the highest spatial and temporal resolution (27). For site-specific, orthogonal labeling with QDs, IFNAR1 and IFNAR2 were fused to the HaloTag and the SNAP tag, respectively, and stably expressed in IFNAR2-deficient U5A cells at physiological levels (~5 to 10 copies/ μm^2). Full functional integrity of this complemented cell line with respect to IFN signaling was recently demonstrated (33), making it a viable model for our studies. On the basis of sequential, tag-specific biotinylation, IFNAR1 and IFNAR2 were labeled with monobiotinylated QDs via bivalent streptavidin (bSAV) (Fig. 1A) (26), thus excluding bias by multivalent interactions. A typical labeling

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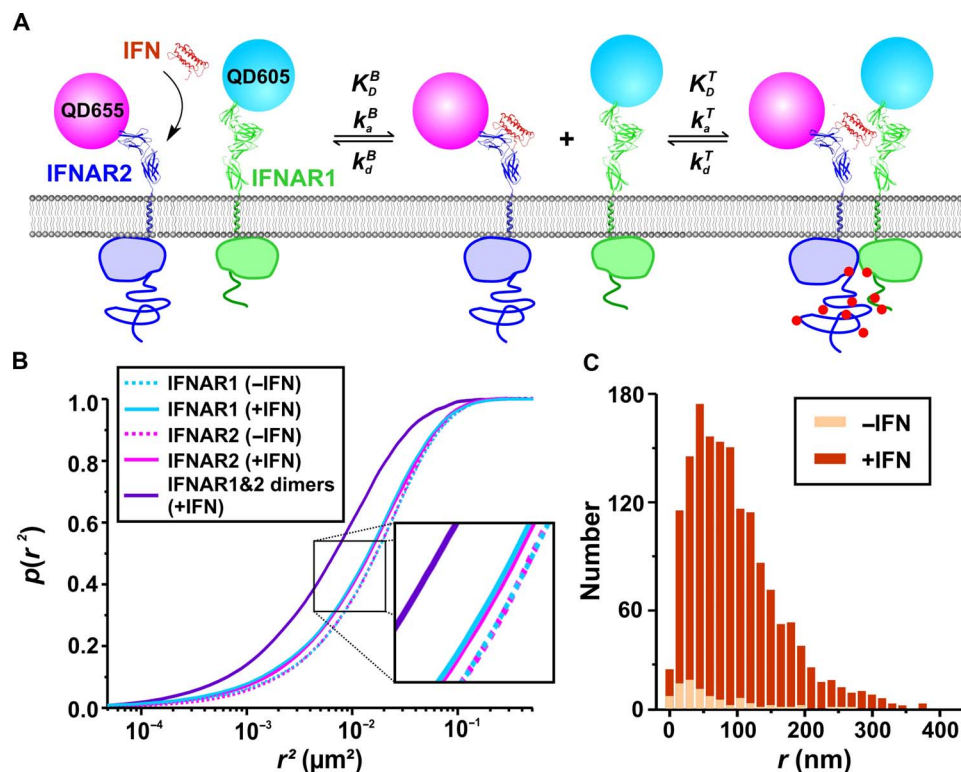


Fig. 1. Spatiotemporal dynamics of IFNAR assembly in the PM. (A) IFNAR1 and IFNAR2 stably expressed in U5A cells at physiological levels were labeled orthogonally with monofunctional QD605 and QD655. Rate constants involved in a two-step receptor dimerization mechanism, which can be assumed owing to the highly asymmetric properties of IFN interaction with the two receptor subunits: After IFN capturing from the solution by the high-affinity subunit IFNAR2, IFNAR1 is recruited within the membrane to form the ternary signaling complex. The dynamic equilibrium between binary and ternary complexes in the PM is described by the 2D rate constants k_a^T and k_d^T as well as the 2D equilibrium dissociation constant K_D^T . (B) Cumulative probability plot of QD-labeled IFNAR1 and IFNAR2 square displacements in the absence (dashed lines) and in the presence (solid lines) of 50 nM IFN α 2 as obtained from >10,000 individual displacements. The square displacements were determined for a lag time of 160 ms (five frames). The IFN α 2 concentration ensured saturation of all IFNAR2 at the cell surface. For comparison, the square displacements observed for IFNAR1/IFNAR2 dimers are included (violet line). Diffusion constants obtained by two-component mean square displacement (MSD) analyses are provided in table S1. (C) Histogram of the displacements of IFNAR1-IFNAR2 dimers identified by colocomotion analysis in the absence and in the presence of IFN α 2 ($N = 81$ without IFN α 2 versus $N = 1492$ with IFN α 2) for a lag time of 160 ms.

degree of ~16% with high orthogonality and negligible background labeling was achieved (movies S1 and S2 and fig. S4). Statistical analysis of displacements (within five frames, that is, 160 ms), obtained from more than 10,000 individual displacements, revealed highly similar diffusion kinetics of IFNAR1 and IFNAR2 (Fig. 1B). Upon the addition of IFN α 2, a small yet significant reduction in the average diffusion could be detected, suggesting ligand-induced receptor dimerization (Fig. 1B). Single-molecule colocomotion analysis based on tracking of colocalized molecules over multiple steps revealed that only after the addition of the ligand could a substantial amount of IFNAR1/IFNAR2 dimers be detected (Fig. 1C and movie S3). The mobility of these receptor dimers was substantially decreased, as compared to the unliganded receptor subunits (Fig. 1B and table S1). The association and dissociation of individual receptor dimers could be discerned in the presence of IFN α 2 (movie S4 and Fig. 2, A and B), corroborating the model of reversible receptor dimerization, as depicted in Fig. 1A. From the relative number of colocomotion trajectories after IFN α 2 stimulation (6.6%) in combination with the estimated QD labeling degree of ~16%, we infer that ~40% of receptors were recruited into ternary complexes. In comparison, ~2% receptor dimers were observed in the absence of ligand, which is characterized by very low mobility and can be ascribed to nonspecific background binding and/or aggregation of QD. These results

highlight the efficient IFN α 2-induced dimerization of IFNAR1 and IFNAR2 and the formation of a dynamic equilibrium between binary and ternary complexes in the PM.

Lifetime and effector activation of receptor dimers depend on MSK integrity

Even though individual ternary complexes could be readily identified by colocomotion analysis, insufficient tracking fidelity due to QD blinking impeded the reliable quantification of lifetimes of individual complexes from the length of cotrajectories. We therefore devised a method to filter the data sets according to time-lapse particle correlation (fig. S5), yielding much longer and largely unbiased colocomotion trajectories. On the basis of this method, we analyzed the lifetime of several hundred individual receptor dimers, yielding an exponential distribution with an average complex lifetime $\tau = 15.2 \pm 1.7$ s (Fig. 3, A and B). In contrast, the lifetime of ternary complexes in artificial membranes *in vitro* was found to be ~3 s (34), that is, fivefold lower than that of ternary complexes in the PM.

Potentially, transient confinement of receptor dimers in sub-microscopic MSK corrals (<100 nm in diameter) could be responsible for enhancing the probability that dissociated receptor subunits rapidly reassociate. To test this hypothesis, we investigated the role of the MSK in confining IFNAR1 and IFNAR2 and in the apparent

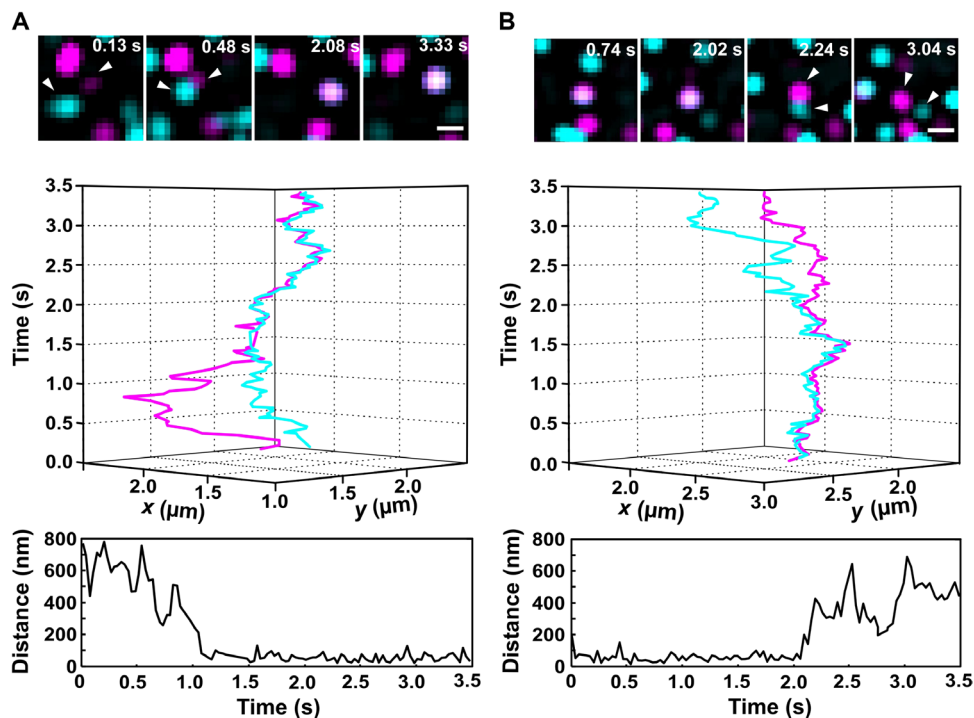


Fig. 2. Dynamic equilibrium of receptor dimerization observed at the single-molecule level. Assembly (A) and dissociation (B) of individual IFNAR1 (cyan) and IFNAR2 (magenta) heterodimers observed in the presence of IFN α 2: time series of images (top), 3D trajectories (middle), and distances between receptors as a function of time (bottom). White arrowheads mark the dimerized receptors. Scale bars, 1 μ m.

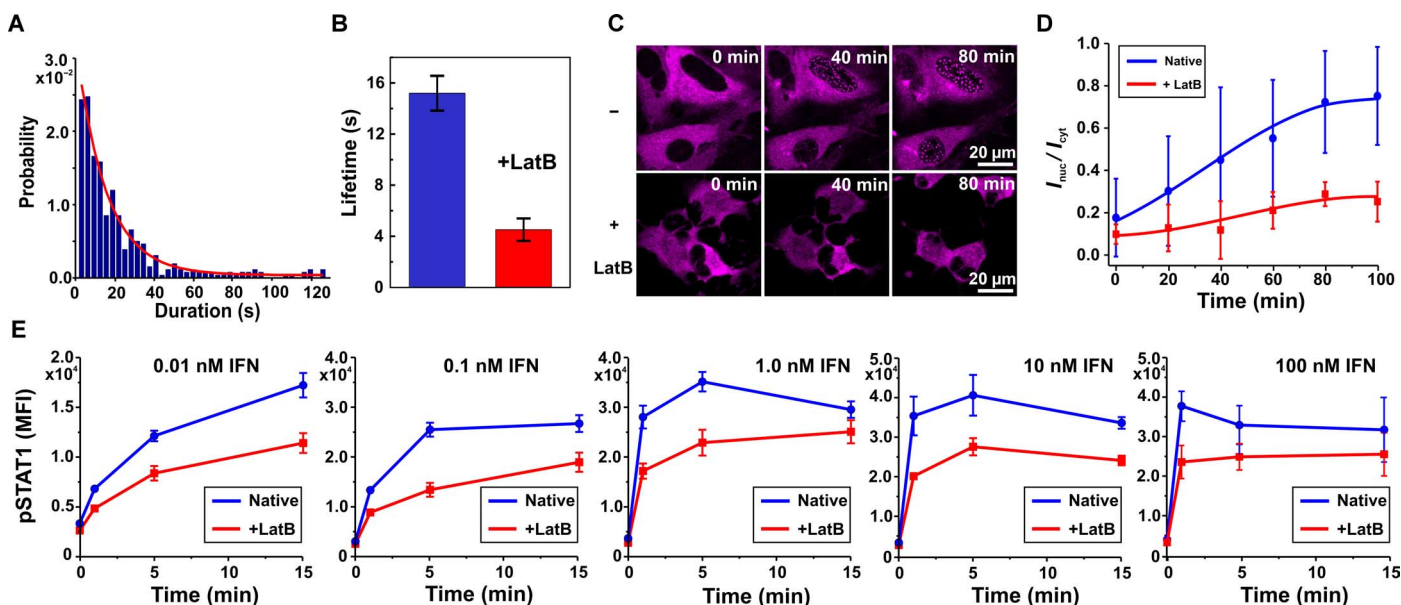


Fig. 3. Lifetime of receptor dimers and IFN signaling activity depend on MSK integrity. (A and B) Ternary complex lifetime in the native PM obtained from a colocomotion trajectory length histogram (390 individual tracked colocomotion events). An average lifetime of 15.2 ± 1.7 s (mean \pm SD) was obtained by an exponential fit. (B) Complex lifetimes obtained from trajectory length histograms in the absence and in the presence of LatB. (C and D) IFN α 2-stimulated translocation of STAT2 in the absence and in the presence of LatB. (C) Translocation of STAT2-TagRFP stably expressed in HeLa cells, visualized by confocal laser scanning microscopy. (D) Time-dependent STAT2 translocation monitored by the ratio of fluorescence intensity of STAT2-TagRFP in the nucleus to that in the cytoplasm. Data are presented as means \pm SD from seven cells connected by lines to guide the eye. (E) Kinetics of STAT1 phosphorylation at different IFN α 2 concentrations in the absence and in the presence of LatB. HeLa cells were stimulated with the indicated concentrations of IFN α 2, and pSTAT1 was quantified at various time points by phosphoflow cytometry. Data are means \pm SE from four independent replicates.

lifetime of individual ternary complexes. Upon treatment of cells with Latrunculin B (LatB) to inhibit actin polymerization, thus destabilizing the MSK (35), approximately twofold increased diffusion constants for both IFNAR1 and IFNAR2 were detected (fig. S6 and table S1). Strikingly, increased receptor mobility upon LatB treatment was accompanied by a decrease in the stability of receptor dimers (Fig. 3B). Under these conditions, a lifetime of 4.4 ± 0.8 s was obtained, corroborating the fact that the MSK contributes to stabilizing signaling complexes.

Because the lifetime of signaling complexes may be critical for downstream signaling, we examined the role of MSK integrity in the activation of signal transducer and activator of transcription 1 (STAT1) and STAT2, which are hallmark effector proteins of IFN signaling (36, 37). STAT1 and STAT2 are phosphorylated by the IFN signaling complex to form, together with interferon regulatory factor 9, the transcription factor ISGF3, a key regulator of IFN-stimulated gene expression (36, 38). ISGF3 is formed upon phosphorylation of STAT1 and STAT2 by the IFN signaling complex, resulting in the nuclear translocation of these proteins (39). Functional studies were performed in HeLa cells, in which IFN downstream signaling is more robust than in the complemented U5A cell line, whereas both cell lines display similar receptor density, diffusion, and signaling dynamics (33, 40). In a first step, we quantified IFN-stimulated nuclear translocation of STAT2 by fluorescence microscopy in living cells. In native HeLa cells stably expressing STAT2 fused to TagRFP (STAT2-TagRFP), time-dependent translocation of STAT2 into the nucleus was observed after treatment with IFN α 2 (Fig. 3C), yielding characteristic subnuclear accumulation (41). In contrast, a much weaker nuclear translocation was observed for the same experiment carried out after LatB treatment (Fig. 3, C and D). STAT2 translocation was still detectable after LatB treatment, confirming that IFN signaling was still possible in these cells but with decreased efficacy. To pinpoint the cause of reduced ISGF3 translocation, we explored how LatB treatment affects STAT phosphorylation. Kinetic analysis of STAT1 phosphorylation by phosphoflow cytometry confirmed the functional relevance of actin cytoskeleton integrity for IFN signaling (Fig. 3E). The concentration dependence and time dependence of STAT1 phosphorylation suggest that LatB treatment affects the rate of STAT1 phosphorylation. Because phosphorylated STAT1 is required for ISGF3 formation and nuclear translocation, this observation can explain delayed STAT2 translocation upon LatB treatment. These results suggest that the actin cytoskeleton is involved in the activation of IFN effector proteins, possibly as a scaffold of PM compartmentalization, contributing to stabilizing IFNAR1/IFNAR2 dimers. However, other cellular functions of actin polymerization (for example, in receptor endocytosis and trafficking) could also be responsible for this effect.

A spatial stochastic MSK model reproduces IFNAR diffusion properties

We therefore further explored our hypothesis that confinement by the nanoscale MSK meshwork, as proposed by the “picket fence” model (42), may promote rapid reassociation of the same receptor subunits. Because a diameter of <100 nm for the MSK confinement zone has been reported, the temporal and spatial resolution applied in the cotracking experiments did not allow us to resolve these events (3). To better understand the effect of MSK compartments on reassociation and the apparent stability of ternary complexes, we set up a high-resolution spatial stochastic computer model of receptor diffusion in the PM. Our model was parameterized using

experimental molecular kinetics and diffusion data obtained with IFNAR reconstituted using artificial membranes (23, 34, 43) (see the Supplementary Materials for a detailed model description). An MSK-like compartmentalization was introduced by means of a triangular mesh with an average length scale of 70 nm (Fig. 4A and fig. S7). This length scale, corresponding to the mean square root of the compartment area, had been previously reported for HeLa cells (3, 6), which yielded very similar diffusion properties of IFNAR1 and IFNAR2 compared to U5A cells (33, 40). Hop diffusion between MSK compartments was specified by the associated hop probability p_{MSK} , whereas the diffusion constants inside the corral were set at values obtained for the transmembrane proteins and the ternary complex reconstituted into artificial membranes (compare Table 1) (43, 44). As it turned out, this model could robustly reproduce the experimentally observed step length histograms in the absence and in the presence of LatB (Fig. 4B and fig. S8).

MSK-dependent complex reassociation events are predicted by the model

On the basis of the p_{MSK} values obtained by fitting the experimental data (Table 1), we simulated the interaction dynamics of individual complexes using the molecular association and dissociation rate constants k_a^T and k_d^T , respectively (compare Fig. 1A), previously determined for IFNAR1 and IFNAR2 reconstituted into artificial membranes (23, 34, 43). The experimental k_a^T was converted into an on-rate probability p_{on} , assuming an association radius $r_{\text{on}} = 5$ nm estimated from the structure of the ternary complex (21). In comparison with experiments, a p_{on} value of 0.0068 was obtained, highlighting the fact that the recruitment of IFNAR1 by the IFN α 2/IFNAR2 complex is far from being diffusion-controlled in homogeneous membranes. The average lifetime of the complex τ_{mol} was set to 3 s in accordance with k_d^T , the IFNAR1 dissociation rate constant from the IFNAR2/IFN α 2 complex (34). To determine the apparent complex lifetime in the MSK meshwork (τ_{MSK}), we initiated simulations with a single receptor dimer that was randomly placed inside the compartmentalized membrane domain. During diffusion in the MSK meshwork, the dissociation of the complex was stochastically initiated according to the average molecular lifetime τ_{mol} , and reassociation was allowed on the basis of p_{on} . Although these simulations were carried out with a 5- μ s time resolution and a <5-nm spatial resolution, the positions of the complex and the two receptor subunits were recorded every 0.032 s to mimic the experimental acquisition rate. A complex was considered fully dissociated once IFNAR2 and IFNAR1 were localized in non-neighboring MSK compartments (compare the Supplementary Materials). These simulations revealed substantial reassociation within individual MSK compartments for hopping probabilities of an intact MSK (movie S5, Fig. 4C, and fig. S10). A histogram of these apparent complex lifetimes obtained from 100 individual complexes is shown in Fig. 4D, yielding an approximately threefold increase in the average complex lifetime ($\tau = 9.4$ s), as compared to the τ_{mol} of noncompartmentalized, artificial membranes. In contrast, only minor apparent stabilization of the ternary complex was observed in simulations with hopping rates corresponding to the presence of LatB ($\tau = 4.1$ s; Fig. 4D), matching the experimentally observed complex lifetimes very well. The robustness of these results was corroborated by extensive control simulations with altered local diffusion properties of the receptor (fig. S11). Likewise, variation in r_{on} did not yield significant changes in the complex stability, given that p_{on} was adjusted according to the in vitro association kinetics (fig. S12).

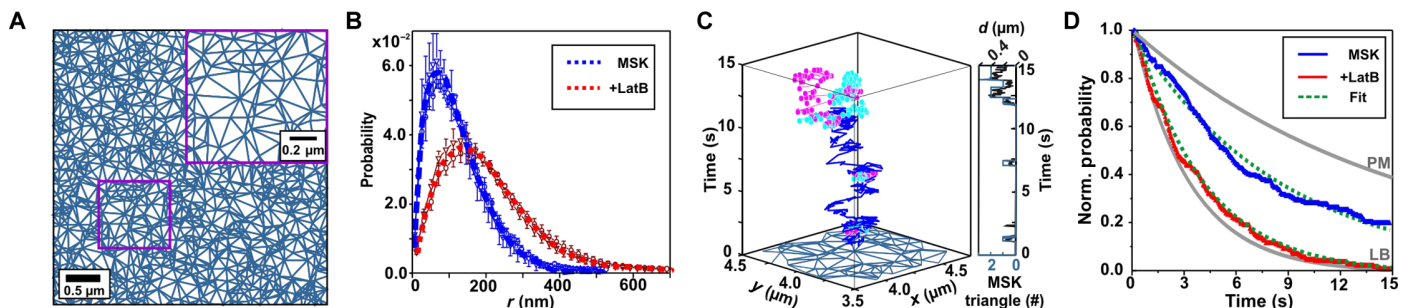


Fig. 4. Modeling of diffusion and interaction in the context of a stochastic MSK meshwork. (A) Model of the MSK mesh with an average 70-nm length scale. Inset is a 2 \times magnification of the region highlighted by the rectangle. (B) Displacement probability density of the diffusing receptors (IFNAR1, circle; IFNAR2, triangle) in the PM of native cells (blue) and LatB-treated cells (red). Fitting the experimental data sets (dotted lines) with the MSK hop diffusion model yielded experimental hopping probability values summarized in Table 1. (C) Representative spatial stochastic simulation of an individual complex within MSK microcompartments, revealing transient dissociation and reassociation of receptor dimers (time lapse, 0.032 s; IFNAR1, cyan; binary IFNAR2/IFNAR2 complex, magenta; ternary complex, blue). (D) Experimental lifetimes of ternary complexes measured in solid supported lipid bilayers (LB) and in the PM, compared to simulated ternary complex lifetimes based on receptor confinement by the MSK in native cells (blue) and in LatB-treated cells (red).

Table 1. Key experimental parameters and the associated constants derived by simulations. Molecular diffusion constants of receptors in an artificial lipid bilayer D_{mol} (mean value \pm SD) (43); diffusion constants in the PM D_{cell} obtained from 160 ms squared displacement analysis (mean values \pm SD) (table S1); simulated hop probabilities p_{MSK} ; simulated apparent lifetime of complexes within the MSK τ_{MSK} ; hop probability across SC barriers p_{SC} . NA, not applicable.

Cell status	Species	D_{mol} ($\mu\text{m}^2/\text{s}$)	τ_{mol} (s)	D_{cell} ($\mu\text{m}^2/\text{s}$)	τ_{cell} (s)	p_{MSK}	τ_{MSK} (s)	p_{SC}	τ_{MSK+SC} (s)
Native	Receptor subunits	1.1 ± 0.2	NA	0.043 ± 0.002	NA	0.00095	NA	0.0025	NA
	Ternary complex	0.7 ± 0.2	3	0.022 ± 0.001	15.2 ± 1.7	0.0006	9.4	0.0018	12.1
+LatB	Receptor subunits	1.1 ± 0.2	NA	0.068 ± 0.004	NA	0.0036	NA	NA	NA
	Ternary complex	0.7 ± 0.2	3	0.053 ± 0.002	4.4 ± 0.8	0.002	4.1	NA	NA

Receptor diffusion is confined by hierarchical, MSK-dependent microdomains

These results fostered our hypothesis that reassociation due to passive confinement by the MSK can increase the apparent stability of ternary complexes in the PM. However, our compartmentalization model could not match the experimentally observed ternary complex lifetimes in wild-type cells. We therefore explored in more detail the sub-microscopic spatiotemporal organization of IFNAR1 and IFNAR2 in the PM. For this purpose, we used TALM (45), a robust method that we recently developed for identifying and characterizing transient confinement zones (40). Superresolution TALM images, reconstructed by localizing individual receptor subunits over a period of 25 s, revealed substantial local confinement of the receptors (Fig. 5A). To selectively quantify the dimension of the spatiotemporal organization of ternary complexes, we applied pair correlation TALM (pcTALM), which clearly identified transient confinement zones with an average diameter of 250 ± 30 nm (Fig. 5, B and C). Notably, these secondary confinement zones could not be detected in the presence of LatB (fig. S13), suggesting that these larger-scale microcompartments also depend on the cortical actin skeleton.

Upon closer inspection of individual colocomotion trajectories, distances between IFNAR1 and IFNAR2 above the noise level were detected (Fig. 5, D to F, and movie S6), which is indicative of transient dissociation and reassociation events within these larger membrane compartments. Our analyses revealed an average of 1.7 reassociation

events per trajectory with a significant intersubunit separation distance of >200 nm. We further characterized the properties of these secondary confinement zones by QD tracking with submillisecond time resolution (2000 frames per second) using a scientific complementary metal-oxide semiconductor (sCMOS) camera. A typical trajectory obtained at this 66-fold increased acquisition rate is shown in Fig. 5G, clearly exhibiting highly confined diffusion properties (Fig. 5H, fig. S14, and movie S7). Confinement zones were identified and quantified using a spatiotemporal cluster algorithm (Fig. 5I), yielding an average diameter of 270 nm and an average dwell time of 0.43 s (fig. S15). Characterization of the diffusion properties by MSD analysis confirmed nested confinement zones (Fig. 5H, fig. S14, and table S4). Upon the addition of LatB, secondary confinement was largely abrogated, which agrees with the pcTALM analysis very well.

Comprehensive spatial stochastic model reproduces experimental complex lifetimes

We therefore refined our membrane model to include additional microcompartmentalization as a secondary, passive transient confinement zone. To this end, we introduced hierarchical confinement with each secondary compartment (SC) set to be composed of a number of interconnected MSK compartments, as observed in the experiments (Fig. 6A and fig. S16). Inner (MSK-based) and outer (SC-based) barriers were assigned distinct hop probabilities (p_{MSK}

and p_{SC} , respectively) according to the experimentally observed diffusion properties (fig. S17). On the basis of this refined spatial stochastic diffusion model, we simulated the dissociation of ternary complexes (compare the Supplementary Materials). By applying this two-tiered membrane compartmentalization model, a further increase of the apparent complex stability was obtained ($\tau = 12.1$ s), more closely

matching the experimentally observed complex stability (Fig. 6B). On the basis of this model, we reassessed our trajectory length analysis by terminating cotrajectories at an intersubunit distance threshold of 200 nm, which was chosen on the basis of the experimentally observed intersubunit distance distribution (Fig. 5F). Under these conditions, a lifetime of 8.8 s was obtained (fig. S18), which is in excellent agreement

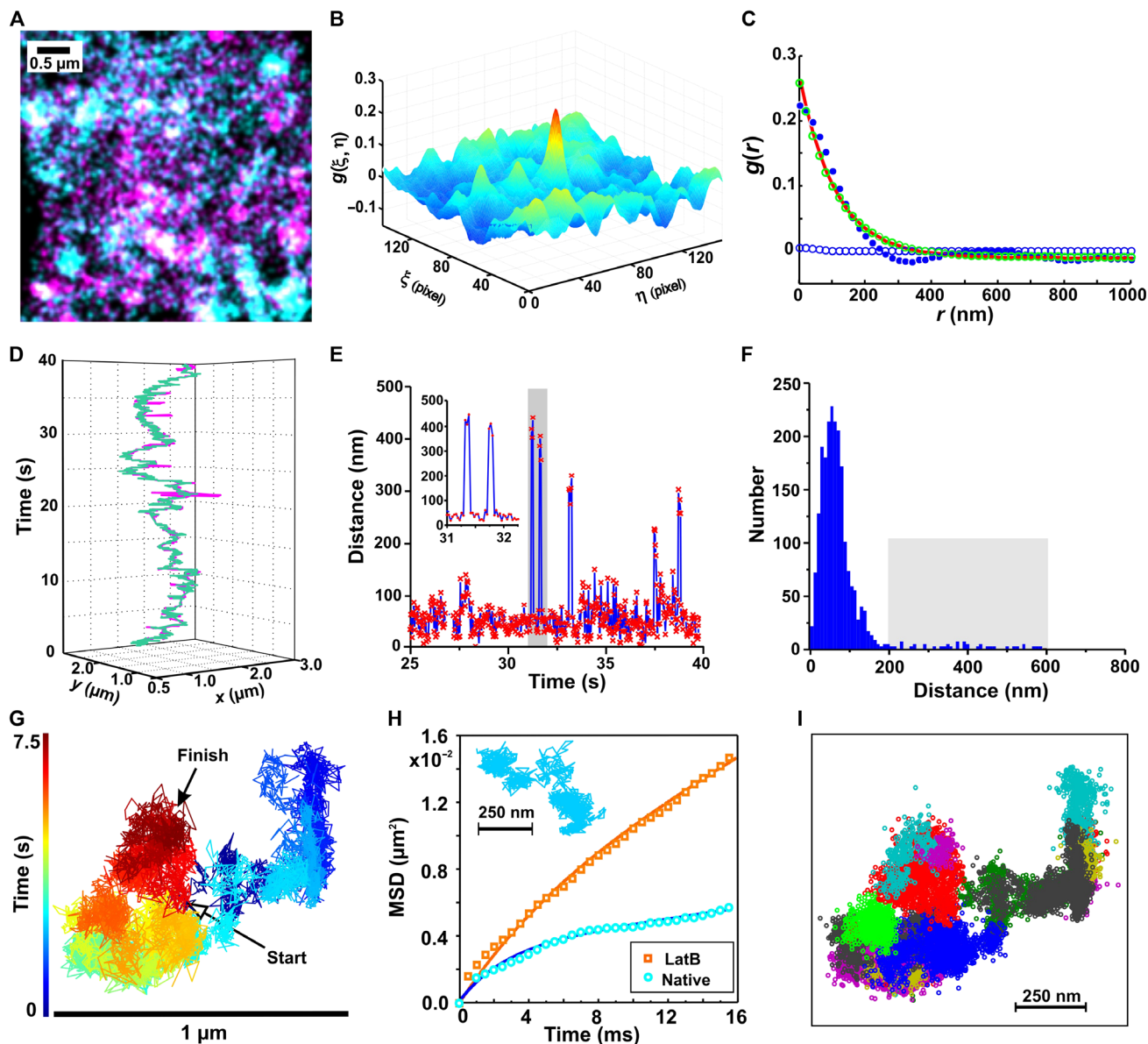


Fig. 5. Secondary compartmentalization of IFNAR complexes. (A to C) Identification of secondary confinement zones by dual-color TALM and pcTALM. (A) TALM images of IFNAR1 (cyan) and IFNAR2 (magenta) in the presence of IFN α 2. (B) Image cross-correlation and (C) pair correlation analyses. The pair correlation curve (blue dots) was deconvolved into the contributions of free (blue circles) and confined (green circles) diffusion components by fitting Eq. 3 (Materials and Methods). (D to F) Transient dissociation events observed within experimental colocomotion trajectories. (D) Localizations of IFNAR1 (cyan) and IFNAR2 (magenta) within an individual colocomotion trajectory. (E) IFNAR1-IFNAR2 distance map within an individual cotrajectory (red dots connected by a blue line) showing dissociation and reassociation events within secondary confinement dimensions. Two characteristic dissociation events highlighted by the gray bar are enlarged in the inset. (F) Histogram of IFNAR1-IFNAR2 distances yielding a significant fraction (2.3%) of distances of >200 nm, which correspond to transient dissociation events (highlighted by the gray rectangle). The total number of displacements $N = 1560$ was obtained from 24 trajectories yielding an average of 1.5 reassociation events per trajectory. (G and H) Detection of secondary confinement zones by fast QD tracking. (G) Trajectory of an individual particle covering 15,000 frames. Color coding according to the acquisition time indicated by the time bar. (H) MSD analysis of fast QD tracking in native cells and after the addition of LatB. A typical trajectory from native cells is shown in the inset. MSD data obtained from more than 1000 trajectories. (I) Identification of domains (depicted in different colors) by DBSCAN analysis.

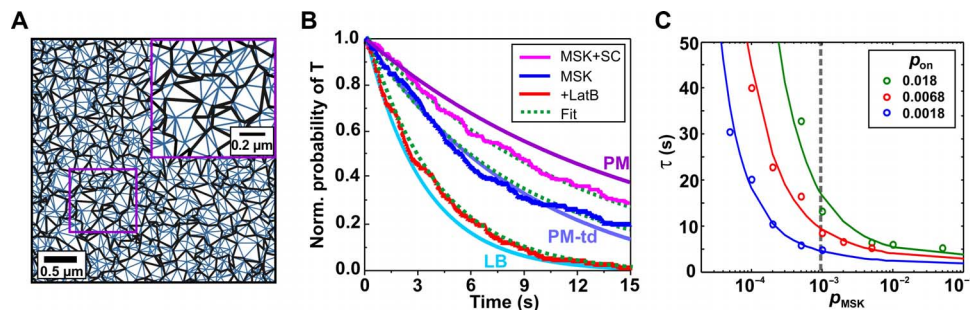


Fig. 6. Complex reassociation in hierarchical confinement zones. (A) Spatial organization of confinement zones used for the model. Thin and bold lines correspond to hopping probabilities p_{MSK} and p_{SC} , respectively. Inset is a magnification of the region highlighted by the rectangle. (B) Comparison of apparent complex stability obtained by simulations with experimentally observed lifetimes plotted as exponential decay curves [LB, molecular kinetics determined with artificial membranes in vitro; PM, complex lifetimes observed in the PM; PM-td, complex stability considering transient dissociation of dimers above a 200-nm intersubunit distance threshold chosen on the basis of the experimentally observed intersubunit distance distribution (Fig. 5F)]. (C) Role of association kinetics and hopping probability p_{MSK} for stabilizing complexes, as measured by their lifetime (with respect to our selected metric).

with the lifetime obtained by the basic (single compartmentalization) MSK model (Fig. 6B).

Having identified a set of biologically realistic parameters describing complex reassociation, we further investigated whether cells could have developed a regulatory mechanism to exploit or control the stabilizing effect of receptor confinement. Two key parameters were taken into account: (i) the molecular two-dimensional (2D) association rate constant k_a^{2D} , which determines the reassociation probability of transiently confined interaction partners, and (ii) the MSK hop probability p_{MSK} , which determines the confinement of receptors in the MSK. We systematically explored how MSK-induced complex stabilization depends on the binding probability along with MSK hop probabilities (Fig. 6C). As expected, an approximately threefold increase of the binding probability results in an even longer apparent complex lifetime. Upon threefold reduction of the binding probability (and, hence, k_a^{2D}) from the experimentally determined value, stabilization by the MSK could no longer be observed at this hopping probability. A similar effect could be obtained with a fourfold increase of the hop probability, which is in line with our experimental observations upon LatB treatment.

DISCUSSION

Hierarchical organization models of the PM predict an interplay of molecular interactions and confinement into membrane microdomains. Using single-molecule localization techniques in combination with spatial stochastic modeling, we obtained evidence that MSK-based diffusion barriers play an important role in maintaining signaling complexes by facilitating reassociation of the same receptor subunits, thus ensuring sustained “signaling bursts” (18). We successfully reproduced the experimentally observed complex stabilization in a spatial stochastic model of receptor dynamics by incorporating passive diffusion barriers. All parameters used for these simulations were directly derived from experimental data, corroborating the validity of the model. Our analyses suggest that secondary confinement beyond the 70-nm MSK meshwork substantially contributed to further stabilizing the complex, which could be experimentally resolved. A similar hierarchical confinement has been recently observed for epidermal growth factor receptor dimerization (31), suggesting more general features of PM compartmentalization, the underlying molecular and cellular bases of which remain to be investigated. According to our simulations, both levels of compartmentalization are required

to enhance rapid complex reassociation to a level matching the experimentally observed lifetime of individual complexes. Transient dissociation events within SCs could be resolved experimentally, thus confirming the relevance of these structures in maintaining receptor dimers. Whereas receptor stabilization by transient confinement had been previously hypothesized (18, 31), we here quantified its molecular and cellular determinants on the basis of a fully quantitative model.

Our simulations suggest that the molecular 2D association rate constant of IFNAR1 recruitment into the ternary complex is just large enough for the complex to experience a moderate increase in apparent lifetime, through repeated reassociation of its subunits. Thus, it appears that MSK permeability may have evolved to a level that supports efficient reassociation of receptor interactions with sufficiently high on-rates. Given that molecular association rate constants substantially higher than those reported for the IFNAR1-IFN α 2 complex are frequently observed, even stronger MSK effects on the reassociation of receptor dimers are possible. However, for the cell, this reassociation of dynamic signaling complexes seems to establish another regulatory control mechanism because the lifetime of a functional signaling complex is defined not only by molecular interaction dynamics but also by cellular context. We found that MSK integrity is important for efficient downstream signaling by the IFN receptor, implicating a key role of receptor dimer stability in effector activation. IFN β binds IFNAR1 with an approximately 100-fold higher binding affinity and complex stability than IFN α 2, a feature that has been correlated with distinct cellular activities of IFN β (46). These differential activities of IFN α 2 and IFN β strongly depend on the cellular context (47), which may relate to a differential degree of MSK compartmentalization (3, 6). Thus, the regulation of complex stability via the MSK permeability emerges as an important regulatory determinant of the functional plasticity of cytokine receptors and receptor tyrosine kinases, a prominent feature of signal transduction based on receptor dimerization.

MATERIALS AND METHODS

Materials

Poly(ethylene glycol) (PEG)-amino functionalized QDs (QD605 and QD655; cat. no. Q21501MP and Q21521MP, respectively) were purchased from Invitrogen and were functionalized as monovalent biotin QDs, as recently described (26). Poly-L-lysine-graft-(PEG) functionalized with an RGD peptide (PLL-PEG-RGD) (48) for minimizing

nonspecific binding of QDs on the surface was synthesized, as recently detailed (40). Bovine serum albumin (BSA) (essentially fat acid-free) was purchased from Sigma-Aldrich. Halo-PEG₄-biotin ligand (HTL-biotin) was purchased from Promega (cat. no. G859). Benzylguanine-biotin (SNAP-biotin) was purchased from New England Biolabs (cat. no. S9110S). Glucose oxidase and glucose were purchased from Sigma, and glucose catalase was from Roche Applied Science. LatB from *Latrun-culia magnifica* was purchased from Sigma-Aldrich (L5288). If not specified otherwise, all other materials were purchased from Sigma-Aldrich.

Protein expression and purification

IFN α 2 was expressed and purified as previously described (22). bSAV was prepared by fractionation of streptavidin tetramers that were obtained by refolding a mixture of dead and alive streptavidin monomers, as previously described (49). Expression plasmids for dead and alive streptavidin monomers were based on vectors obtained from A. Ting (Massachusetts Institute of Technology, Cambridge, MA) but included a tobacco etch virus (TEV) cleavage to allow the removal of the His tag (50). After incubation with the TEV protease, bSAV was purified by immobilized metal ion affinity chromatography.

Plasmids and cell culture

Plasmids for the expression of IFNAR1 fused to the HaloTag (51) and of IFNAR2 fused to the optimized SNAP tag (52) were generated as follows: The genes of full-length IFNAR1 and IFNAR2 without the N-terminal signal sequences were inserted into pDisplay (Invitrogen) via the Bgl II and Pst I restriction sites, respectively. Subsequently, genes coding for the HaloTag and the SNAP tag were inserted via the Bgl II site. The constructs, including the signal sequence of the pDisplay vector (immunoglobulin κ chain leader sequence), were transferred by restriction with Eco RI and Not I into modified versions of pSems-26m (Covalys Biosciences), linking the open reading frame to a neomycin or puromycin resistance cassette, respectively, via an internal ribosomal entry site. STAT2 fused to a C-terminal TagRFP (STAT2-TagRFP) was cloned into the pSEMS-26m vector (Covalys Biosciences) by cassette cloning, as recently described (53).

Cells were cultured at 37°C and 5% CO₂ in Earle's minimum essential medium (MEM) with stable glutamine (FG0325, Biochrom AG) supplemented with 10% fetal bovine serum (S0615, Biochrom AG), 1% nonessential amino acids (M11003, PAA Laboratories GmbH), and 1% Hepes buffer without the addition of antibiotics. U5A cells stably transfected with HaloTag-IFNAR1 and SNAP-IFNAR2c were generated in two steps: In a first step, U5A cells were transfected by HaloTag-IFNAR1 via G418 selection. Transfected cells were selected for stable neomycin resistance by cultivation in the presence of G418 (800 μ g/ml; 345810, Calbiochem). A cell clone with homogeneous and moderate expression of HaloTag-IFNAR1 was chosen and proliferated. In a second step, SNAP-IFNAR2c was transfected and selected via Puromycin resistance at 0.4 μ g/ml (D00123816, Calbiochem). After transfection with STAT2-TagRFP, HeLa cells stably expressing STAT2-TagRFP were selected on the basis of the neomycin resistance.

Quantification of STAT2 translocation and STAT1 phosphorylation

IFN-stimulated STAT2 translocation in the nucleus was monitored by confocal laser scanning microscopy (IX81, Olympus, equipped with an Olympus FluoView 1000 LSM unit) at room temperature. HeLa cells stably expressing STAT2-TagRFP were cultivated on microscope coverslips. IFN α 2 (20 nM) was added in the solution after

the cell sample was mounted on the microscope. Fluorescence intensity of STAT2-TagRFP per pixel for the selected region of interest (ROI) in the nucleus and cytosol was obtained as $F_{\text{nuc}}(t)$ and $F_{\text{cyto}}(t)$, respectively. To calculate the relative fluorescence intensity (F_R), an ROI outside the cell was chosen, with its intensity used as reference (F_{ref}): $F_R(t) = [F_{\text{nuc}}(t) - F_{\text{ref}}] / [F_{\text{cyto}}(t) - F_{\text{ref}}]$. To explore the effect of MSK to STAT2 translocation, 10 μ M LatB was added for 10 min at room temperature before the addition of IFN α 2.

Phosphorylation of STAT1 in the HeLa cells was analyzed by flow cytometry, as previously described (54). The HeLa cells were stimulated with 0.01, 0.1, 1, and 10 nM IFN α 2. Intracellular staining of pSTAT1 was performed after the permeabilization of cells with ice-cold methanol [100% (v/v)]. Alexa Fluor 488-conjugated antibodies specific for pSTAT1 were purchased from BD Biosciences and used at a 1:50 dilution. After staining, pSTAT1 was quantified by flow cytometry using an Accuri C6 flow cytometer. The extent of STAT1 phosphorylation was calculated by subtracting the mean fluorescence intensity (MFI) of pSTAT1 of the stimulated samples from that of the unstimulated samples. To evaluate the effect of destruction of the cell MSK, the same experiments were carried out after a 10-min treatment with 10 μ M LatB.

QD labeling in living cells

Before labeling, cells were transferred onto glass coverslips precoated with PLL-PEG-RGD to minimize nonspecific binding of dyes and QDs on the surface, as recently detailed (40). PEG-amino functionalized QDs (QD605 and QD655, Invitrogen) were monobiotinylated (^{BT}QD), as previously described (26). U5A cells stably expressing HaloTag-IFNAR1 and SNAP-IFNAR2 were seeded on PLL-PEG-RGD-coated glass coverslips for 48 hours before labeling. Cell surface receptors were labeled by monobiotinylated QDs in two steps. First, the HaloTag was biotinylated by incubating 1 μ M HTL-biotin for 45 min at room temperature. The cells were washed three times with phosphate-buffered saline (PBS)-BSA buffer (PBS containing 1% essentially fat acid-free BSA) and then incubated with 500 nM His tag-free bSAV for 10 min, followed by washing three times with PBS-BSA. Subsequently, 20 nM ^{BT}QD605 in PBS-BSA was added and incubated for 10 min. The cells were then washed twice with MEM containing an additional 0.1 mM biotin to block the remaining biotin-binding sites and washed two more times with MEM alone. The SNAP tag was then biotinylated by incubating 400 nM SNAP-biotin ligand for 10 min, followed by washing three times with PBS-BSA. Subsequent reactions with bSAV and ^{BT}QD655 were performed as described above. After the second QD labeling step, the cell sample was washed three times with MEM without phenol red for microscopy experiments.

Single-molecule fluorescence microscopy

Single-molecule fluorescence imaging was carried out with an inverted total internal reflection fluorescence (TIRF) microscope (Olympus IX71), equipped with a dual-line TIRF illumination condenser (Olympus) and a back-illuminated electron-multiplied (EM)-charge-coupled device (CCD) camera (iXon DU897D, Andor Technology). An image acquisition rate of 30 Hz was set for the EM-CCD camera. A 488-nm solid-state laser (200 mW Sapphire, Coherent) was coupled into the microscope through polarization-maintaining mono-mode fibers (kineFLEX, Point Source). Laser light was reflected by a quad-line dichroic beam splitter (Di R405/488/561/647, Semrock) and passed through an objective of high numerical aperture (NA) (150 \times TIRF objective UAPO; NA, 1.45; Olympus). A typical excitation

power of 800 μW was measured at the objective. For simultaneous dual-color detection of QD605 and QD655, a DualView microimager (Optical Insight) was used together with a 640 DCXR dichroic beam splitter (Chroma) in combination with the band-pass filters FF01-585/40 and FF01 670/30 (Semrock), respectively. Typical time series of 2000 to 20,000 frames were recorded at 30 Hz (~ 1 to 10 min). To minimize photooxidation of QDs over a long period, an oxygen scavenging system containing glucose oxidase (0.5 mg ml^{-1}), catalase (40 mg ml^{-1}), and 5% (w/v) glucose was added. Under these conditions, no photooxidation of QDs was observed during the experimental period (~ 10 min of continuous illumination).

All live cell images were acquired at room temperature. Receptor dimerization was initiated by incubating 50 nM IFN $\alpha 2$, thus ensuring very rapid saturation of cell surface IFNAR2 by the ligand. Imaging was performed in the presence of IFN $\alpha 2$. For inhibition of actin polymerization, 10 μM LatB was added for 10 min at room temperature before imaging. For all dual-color single-molecule fluorescence imaging experiments, the overlay of the two channels was calibrated by imaging fluorescent microbeads (TetraSpeck microspheres 0.1 μm , T7279, Invitrogen), which were used for calculating a transformation matrix. After channel alignment based on the transformation matrix, the deviation between the channels was found to be $7.3 \pm 4.0 \text{ nm}$ (fig. S19).

For fast image acquisition, an sCMOS camera (ORCA-Flash 4.0 V2, Hamamatsu) was mounted on the same microscope setup. In combination with the 150 \times TIRF objective, an effective pixel size of 43 nm was obtained. Imaging was limited to areas of 2048 \times 102 pixels, yielding a frame readout rate of 2000 Hz upon operating the camera in the frame transfer mode. During the fast QD imaging experiments, the typical output laser power at the objective was set to be 20 mW for detection of individual QDs in each frame. The typical imaging time was 15 s, which corresponds to 30,000 frames altogether.

Colocalization analysis and single-particle tracking

To localize and track individual QD-labeled receptors, a 2D Gaussian mask for localization of single emitters was used (55, 56). For colocalization analysis, particle coordinates from the two channels were aligned by a projective transformation using a transformation matrix. The transformation matrix was calculated on the basis of a calibration measurement with multicolor fluorescent beads (TetraSpeck microspheres 0.1 μm , Invitrogen) that are visible in both spectral channels (*cp2iform* of type "affine," MATLAB, MathWorks). An average alignment precision of $7.3 \pm 4.0 \text{ nm}$ was obtained between the two channels (fig. S19). Particles colocalized within a distance of 50 nm were selected for colocomotion analyses.

Single-molecule trajectories were reconstructed using the multitarget tracing algorithm (57). Colocomotion trajectories were obtained by applying the same algorithm to the data set of colocalized molecules. The detected trajectories were evaluated with respect to their step length distribution to determine the diffusion constants. To minimize the effect of long-range perturbations and misconnections, we focused on local displacements in five steps (0.16 s). Hence, only trajectories observed for at least six consecutive frames were used.

Calculated displacements r were pooled for analysis. The cumulative probability of squared displacement $p(r^2)$ was nonlinear least squares fitted by a two-component equation (31, 58, 59) as

$$p(r^2) = 1 - \left[f \cdot \exp\left(-\frac{r^2}{4D_1 t}\right) + (1-f) \cdot \exp\left(-\frac{r^2}{4D_2 t}\right) \right] \quad (1)$$

Here, D_1 and D_2 correspond to diffusion constants of a fast and a slow mobility component, respectively, and f is the fraction of the first component. For each fitting, we pooled ~ 1000 to 4000 trajectories recorded within 2000 frames (64 s). To exclude biases in our analyses of diffusion properties and colocalization, immobile particles were identified by the DBSCAN (density-based spatial clustering of applications with noise) algorithm (60), as recently described (44). Using optimized parameters, the detected localizations with very high spatiotemporal correlation (that is, immobile over very long times) were grouped and filtered out.

Time-lapse particle correlation

To increase cotracking fidelity, we used spatiotemporal particle correlation. A filtering program that employs particle correlation in a time-lapse manner was developed for selecting colocalized particles with coordinates of (x_i, y_i, t_i) , according to the following equation

$$(x_i - \bar{x}_i)^2 + (y_i - \bar{y}_i)^2 < 4Dt, \quad i = 1 \text{ to } N \quad (2)$$

Here, the left part is the square displacement of each particle relative to the averaged position; \bar{x}_i and \bar{y}_i denote the mean values of x and y coordinates of all colocalized particles; N is the total number of colocalized particles. D is the diffusion constant of QD-labeled receptors, which is $0.06 \mu\text{m}^2/\text{s}$ (table S1); t is 20 frames (0.64 s), defined as t_{conf} , a reliable time window for particle correlation in which colocalized QD pairs are considered to not have disappeared because of blinking. It was found that when the observation window is longer than 20 frames, the cumulative probability of observing the QD pairs is higher than 0.9 (fig. S20). By shifting the as-defined time window frame by frame, colocalization noise can be distinguished from true colocomotion events by spatial correlation because random colocalizations are not spatially correlated, and QD blinking can be overcome by temporal correlation (fig. S5B). After processing the time-lapse particle correlation, the noise-filtered, blinking-inhibited colocalizations were obtained. They were connected to colocomotion trajectories according to the highest connection possibility based on the same protocol previously published (9, 31).

Tracking and localization microscopy

Superresolution images of the QD-labeled receptors were obtained on the basis of TALM, as previously described (45). To generate super-resolution images, a 2D Gaussian mask for localization of single emitters was used in each frame of an image stack (55, 56). The localization precision in two dimensions was determined as previously described by Thompson *et al.* (55). To render TALM images, the position of each molecule localized within the image stack was cumulatively plotted as a Gaussian blurred spot with the SD of its point spread function (PSF) set to the averaged localization precision (20 nm). Typical frame numbers are between 300 and 3000 frames (~ 10 - to 96-s integrated imaging time). To explore the dynamics of superresolved structures, a subset of TALM images within a fixed time span (observation window) was reconstructed. The observation window was sliding along the whole TALM image stack in a time-lapse manner to generate time-lapse TALM (40). The typical observation window was 30 to 1000 frames in size (~ 1 - to 32-s integrated imaging time).

pcTALM was carried out as recently described in detail (40). For the characterization of transient confinement zones, TALM images were generated from 800 frames with a time lapse of 256 ms. In the first step, a conventional image correlation spectroscopy (ICS) analysis (61, 62) was applied to the Gaussian-blurred TALM images. For

pair correlation of the TALM images, the Cartesian coordinates of the ICS function were converted into polar coordinates to yield the pair correlation $g(r)$, which was fitted by a two-component model (63)

$$g(r) = g(r)^{\text{free}} + g(r)^{\text{confine}} = A \exp\left(-\frac{r^2}{4\sigma^2}\right) + B \exp\left(-\frac{r}{\lambda}\right) \quad (3)$$

where A is the amplitude of free diffusion, σ is the SD of the PSF of the Gaussian-blurred TALM images ($\sigma = 20$ nm), B is the amplitude of confined diffusion, and λ is the average radius of the randomly shaped confinement zones. Fitting $g(r)$ by Eq. 3 yields λ , A , and B , as shown in fig. S13C. The confinement probability (cp) for describing the chance of the diffusive particle to be confined in the analyzed area was calculated as

$$\text{cp} = \frac{B}{A + B} \quad (4)$$

Confinement and cluster analysis

QD-labeled receptors in TIRF images acquired with an sCMOS camera at an acquisition rate of 2000 Hz were localized and tracked as described above. MSD analysis according to the published methods (42, 64–66) was used to identify transiently confined receptor diffusion. Anomalous diffusion was described as

$$\text{MSD}(t) = 4Dt^\alpha \quad (5)$$

where α is the anomalous diffusion coefficient: $\alpha = 1$, Brownian diffusion; $0 \leq \alpha < 1$, anomalous diffusion. α was determined by plotting MSD/t versus t and fitting of the equation

$$\log(\text{MSD}/t) = (\alpha - 1)\log(t) \quad (6)$$

The effect of membrane compartmentalization on the diffusion in the short term (<32 ms) was identified by fitting a hop diffusion model (65)

$$\text{MSD}(t) = \left(\frac{L^2}{3}\right) \left[1 - \exp\left(\frac{-12D_{\text{micro}}t}{L^2}\right)\right] + 4D_{\text{MACRO}}t + c \quad (7)$$

where L , D_{micro} , and D_{MACRO} denote the diameter of compartment, the local diffusion constant, and the macroscopic diffusion constant, respectively, and c is a constant offset related to the spatial localization precision. The residence time within the compartment τ_{comp} was calculated according to (3)

$$\tau_{\text{comp}} = \frac{L^2}{4D_{\text{MACRO}}} \quad (8)$$

The time it takes for the molecule to experience the effect of the barrier of the confinement τ_{barrier} was calculated according to (66)

$$\tau_{\text{barrier}} = \frac{L^2}{12D_{\text{micro}}} \quad (9)$$

Confinement zones were further identified by spatiotemporal cluster analysis of the fast TALM images with an average localization precision of 15 nm, which were rendered from 15,000 frames acquired in 7.5 s.

Cluster analysis of the TALM images was based on the method of DBSCAN (60), which defines clusters relying solely on the principle of density reachability. For the quantification of the secondary confinement, the reported 70 nm as the average mesh diameter of the MSK in HeLa cells (3) was chosen to determine the density reachability. After points were classified into clusters, the residence time was quantified by counting the time span of the first point to the last point in each cluster. The MATLAB function *kmeans* was used to determine their sizes. All sizes and residence times of clusters were subjected to histogram analysis (fig. S15).

Simulations of diffusion and interaction dynamics in a compartmentalized PM

All simulations of the interaction dynamics of IFNAR1 (R1), IFNAR2: IFN (R2), and the ternary complex (T) were performed using the computer program *Smoldyn* (67). The parameter values for (i) the diffusion constants of all three species, (ii) the rate at which the complex T dissociates, and (iii) the association radius were directly obtained from experimental measurements (34, 43, 68). The parameter value for (iv) the probability of binding was fitted with irreversible binding dynamics obtained from the experiments and depended on the simulation time step. The latter was set to ensure nanometer resolution below the binding radius. MSK compartmentalization of the membrane was introduced as a random triangulation of the 2D plane. The (v) distribution of compartment sizes defined as the square roots of triangle areas and (vi) the median length scale were chosen to match those reported from experiments on representative cell lines (3). The diffusive jump of a molecule from one triangular compartment to another was accepted with a prespecified (vii) hop probability. In a second step, a higher-level (secondary) compartmentalization was established by dividing all triangles into separate groups. The outer boundaries of these larger compartments were assigned a distinct hop probability. All hop probabilities were fitted using experimentally obtained jump length distributions and, in the case of the model with SCs, MSK dwell times. Detailed information on the modeling and simulation can be found in section S1.

SUPPLEMENTARY MATERIALS

Supplementary material for this article is available at <http://advances.sciencemag.org/cgi/content/full/2/12/e1600452/DC1>

section S1. Description of the spatial stochastic models and the simulations

table S1. Measured IFN receptor diffusion constants under different conditions.

table S2. Calculated binding probability p_{on} for different microscopic diffusion constant D_{micro} .

table S3. Parameter scenarios ($D_{R1/R2}$, Δt , r_{on} , and p_{on}) and mean lifetimes τ for fitting hop probabilities.

table S4. Experimental properties of primary and SCs.

fig. S1. Comparison of non-colocalization criteria.

fig. S2. Effect of the binding probability on the simulated receptor complex lifetime.

fig. S3. Simulation of ternary complex lifetime in the hierarchical plasma membrane model.

fig. S4. Orthogonal labeling of IFNAR1 and IFNAR2 with monovalent QD.

fig. S5. High-fidelity colocomotion analysis.

fig. S6. Role of the MSK for receptor diffusion.

fig. S7. Model of the stochastic MSK meshwork used for simulations.

fig. S8. Fitting of hop probabilities of the MSK model.

fig. S9. Fitting of association probabilities.

fig. S10. Sample simulations of ternary complex dissociation and reassociation.

fig. S11. Dependency of simulated receptor complex lifetime on MSK hop probability.

fig. S12. Effect of the reaction radius on the simulated receptor complex lifetime.

fig. S13. TALM and pTALM analyses of receptor confinement.

fig. S14. Primary and secondary confinement confirmed by tracking receptors at 2000 Hz.

fig. S15. Compartment size and dwell time determined by DBSCAN analysis of fast TALM images.

fig. S16. Spatial stochastic model for simulating hierarchical confinement zones.

fig. S17. Fitting of hop probabilities in the refined MSK model.
 fig. S18. Experimental trajectory length histograms for different colocalization cutoffs.
 fig. S19. Channel alignment for colocalization analysis.
 fig. S20. Determination of the observation window for time-lapse pcTALM.
 movie S1. Controls confirming the labeling specificity.
 movie S2. Dual-color single-molecule imaging of QD-labeled IFNAR1 and IFNAR2 in a live cell.
 movie S3. Characterization of receptor diffusion before and after IFN stimulation.
 movie S4. Assembly and dissociation of ternary complexes revealed by single-molecule tracking.
 movie S5. Diffusion, dissociation, and reassociation of an individual ternary complex in the MSK meshwork, as obtained from spatial simulations.
 movie S6. Experimentally observed receptor rebinding events.
 movie S7. Transient receptor confinement at the native cell PM observed by fast TALM.
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