

Review



2018; 8(7): 1824-1849. doi: 10.7150/thno.22172

# Metal-based NanoEnhancers for Future Radiotherapy: Radiosensitizing and Synergistic Effects on Tumor Cells

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Received: 2017.07.31; Accepted: 2018.01.05; Published: 2018.02.12

#### Abstract

Radiotherapy is one of the major therapeutic strategies for cancer treatment. In the past decade, there has been growing interest in using high Z (atomic number) elements (materials) as radiosensitizers. New strategies in nanomedicine could help to improve cancer diagnosis and therapy at cellular and molecular levels. Metal-based nanoparticles usually exhibit chemical inertness in cellular and subcellular systems and may play a role in radiosensitization and synergistic cell-killing effects for radiation therapy. This review summarizes the efficacy of metal-based *NanoEnhancers* against cancers in both *in vitro* and *in vivo* systems for a range of ionizing radiations including gamma-rays, X-rays, and charged particles. The potential of translating preclinical studies on metal-based nanoparticles-enhanced radiation therapy into clinical practice is also discussed using examples of several metal-based *NanoEnhancers* (such as CYT-6091, AGulX, and NBTXR3). Also, a few general examples of theranostic multimetallic nanocomposites are presented, and the related biological mechanisms are discussed.

Key words: tumor, radiation therapy, metal-based nanoparticles, NanoEnhancers, radiosensitization, synergistic chemo-radiotherapy

## Introduction

Radiation therapy (RT) is one of the most effective modalities for the treatment of primary and metastatic solid tumors, microscopic tumor extensions, as well as regional lymph nodes. Alone or combined with other modalities, RT is effective at eliminating cancer cells including stem cells [1] and is used in the treatment of more than half of cancer patients. Radiations (X-rays, y-rays, electrons, neutrons, and charged particles) utilized in RT could damage cells by directly interacting with critical targets or indirectly through free radical production such as hydroxyl radicals [2]. The evolving computer-aided and information-based radiotherapy

techniques are capable of locally delivering ionizing radiation to the tumor by precise external irradiation or brachytherapy while minimizing normal tissue injury. These techniques include the state-of-the-art 3D-conformal image-guided radiotherapy (IGRT) imaging, with intensity-modulated in-room radiotherapy (IMRT) with dynamically controlled multileaf collimators (MLCs) and particle therapy (protons and carbon ions) with reverse depth dose profile. The clinical applications of RT can benefit from the technology improvements, but increasing the radiation dose is insufficient to significantly improve tumor control probability (TCP) for many

radioresistant tumors. To further widen the therapeutic window, biological and chemical strategies using individual biomarkers to predict, evaluate and manage responsiveness to specific therapies should be properly integrated with the advanced RT techniques [3]. Another main challenge of RT is that tumors are often located near normal tissues and organs at risk (OARs), limiting the radiation doses delivered to the target volumes. Therefore, agents preferentially sensitizing tumors to ionizing radiation, termed radiosensitizers, have attracted great interest in radiation oncology [4]. Also, radioprotectors, agents that have radioprotective effects, have been employed to reduce normal tissue complication probability (NTCP). Almost all these agents have been developed for interactions with specific biological targets (the pathway/signaling cascade) at levels from molecules to cells to organs to the whole organism, modulating the responses that occur after radiation exposure (Fig. 1). Thus, in the era of precision medicine, new advances in technology and cancer biology will further improve the

therapeutic outcome of RT at the individual patient level.

Nanomedicines can improve therapeutic benefits by reducing systemic side effects and/or increasing drug accumulation inside tumors by using nanomaterials based on organic, inorganic, protein, lipid, glycan compounds, synthetic polymers, and viruses [5]. The physicochemical properties (size, shape, coating and functionalization, etc.) of nano-agents influence their pharmacokinetics, bioavailability, biodistribution, as well as targeting and intracellular delivery. The nano-agents can achieve specific tumor targeting *via* passive targeting utilizing the enhanced permeability and retention (EPR) effect due to the leaky vasculature of cancerous tissues, active targeting (through high-affinity targeting molecules), and stimuli-responsive triggered release to endogenous or exogenous stimuli. However, a variety of real challenges, such as poor biocompatibility and lack of targeting specificity, hamper the development of ideal nanomedicines.

	Level (target)	Potential <mark>sensitizer</mark> or protector
	Reactive oxygen species Radicals	UROD RNAi, amifostine, pyridoxamine
	DNA damage response Double-stranded break recognition Homologous recombination repair NHEJ repair PARP	Mirin, ATM/ATR inhibitors (e.g., KU-55933), DT01 RS-1, RI-1, modulators of RAD51 expression DNA-PK inhibitors (e.g., NU7441, salvicine) veliparib, olaparib
₹KS&	Chromatin organization HDAC	Vorinostat, belinostat, panobinostat
	<b>Cellular response</b> Cell cycle arrest Mitogen signaling Pro-death signaling	Chk1/Chk2 inhibitors, CDK4/6 inhibitors Cetuximab Pifithrin, GSK-3β inhibitors, anti-ceramide, cytochrome c/cardiolipin complex inhibitors
00	Tumor microenvironment Inflammatory products Tumor stem cells Hypoxia	Statins Salinomycin, thioridazine, homologous recombination inhibitors Carbogen, efaproxiral, tirapazamine, motexafin gadolinium, EZN-2968
	Effects at tissue level Angiogenesis Immune effects Gene therapy Cell repopulation	Bevacizumab Anti-CTLA-4, anti-PD-1, IL-2 + SBRT TNFerade, HSV-tk, G207 Palifermin

Figure 1. Potential radiosensitizers (red) and radioprotectors (green) that may be useful in modulating radiation effects. Reproduced with permission from reference [4], copyright 2013 American Association for the Advancement of Science.



Figure 2. Schematic illustration of metal-based NanoEnhancer radiosensitization process. (Upper-left) Following administration of NanoEnhancers, radiation therapy is carried out after a certain time interval. (Upper-right) Probable biological mechanisms include oxidative stress, cell cycle arrest, DNA repair inhibition, autophagy, ER stress, etc. Besides ionizing radiation-induced fluctuations in biological systems, the metal-based NanoEnhancers internalized by tumor cells can elicit significant cellular biochemical changes prior to, during, and following irradiation. (Lower-left) Classical radiosensitization process, which typically consists of physical dose enhancement, chemical contribution and biological phase, resulting in lethal cellular damage. The primary targets depending on cellular and subcellular distribution and location of metal-based NanoEnhancers include cell membrane, cytoplasm, nucleus, mitochondria, endoplasmic reticulum (ER), and other organelles. Specifically, photoelectrons and Auger electrons generated from the irradiated metal-based nanoparticles could contribute to the dose enhancement directly through the interactions with critical targets or indirectly through free radical production (mostly ROS (reactive oxygen species)), which can be assessed by DCFH-DA (2',7'-dichlorofluorescein diacetate) in living cell models and 3-CCA (coumarin-3-carboxylic acid) in aqueous buffered solutions. In addition, the production of hydroxyl radical in the radiosensitization processes of metal-based nanoparticles could be attributed to the catalytic-like mechanism/surface-catalyzed reaction (e.g., in IONs (iron oxide nanoparticles) this is the surface-catalyzed Haber-Weiss cycle and Fenton reaction). (Lower-right) Patterns of cell death in radiosensitization, such as apoptosis, necrosis, mitotic catastrophe, autophagic death, and senescence. Consequently, the enhanced cell-killing effects might result from the complicated physical, chemical and biological effects induced by the complex action of metal-ba

It is of note that high Z (atomic number) materials, especially metals, usually exhibit chemical inertness, which could decrease potential health hazards in cellular and subcellular systems, an attribute that is critical for clinical use [6]. Another factor that can help reduce the side effects of nano-agents is local intratumoral or superselective intra-arterial injection and tumor bed deposition during surgery for localized solid tumors, lowering the volume of distribution. In 1980, Matsudaira et al. first demonstrated that iodine contrast medium could sensitize cultured cells to X-rays [7]. Subsequently, numerous studies investigating the radiosensitizing and synergistic effects of metal-based nanoparticles for radiotherapy, termed "NanoEnhancers", have been reported in the past decades [8]. Photoelectrons and Auger electrons generated from the irradiated metal-based nanoparticles could contribute to the dose enhancement and subsequent radiobiological enhancement [9, 10]. The classical radiosensitization processes consist of physical dose enhancement,

chemical contribution and biological phase (Fig. 2, lower-left) which cells undergo as the time progresses from nanoseconds to days. Specifically, the electrons, emitted along the primary tracks of the incident ionizing particles, are capable of inducing inner shell ionization of the metal atoms, and the Auger electrons are emitted from the metal-based nanoparticles with the relaxation of the excited core [11]. Subsequently, the electrons can damage cells directly through the interactions with critical targets or indirectly through free radical production. Furthermore, adding free radical scavengers such as DMSO (dimethyl sulfoxide) or NAC (N-acetyl cysteine) in the biological systems would be helpful in evaluating the separate roles for direct and indirect effects in the metal-based NanoEnhancer radiosensitization process. Based on the experimental results, we previously concluded that the production of hydroxyl radical in the radiosensitization processes of metal-based nanoparticles might be attributed the to surface-catalyzed reaction, especially for high-energy

charged particles [12-14]. Additionally, other pharmacological effects of metal-based nanoparticles cannot be excluded for their radiosensitizing/ synergistic effects.

In this review, we discuss the advancements in NanoEnhancers to augment the efficacy of radiation therapy in both in vitro and in vivo systems for a range of ionizing radiation types including  $\gamma$ -rays, X-rays, and charged particles based on the type of metallic element. Furthermore, we introduce the potential of translating these preclinical studies of several probable metal-based NanoEnhancers (mainly AGuIX and NBTXR3) into clinical practice. Some general examples of theranostic multimetallic nanocomposites are presented. We also address the underlying biological mechanisms for the radiosensitizing and synergistic effects of metal-based nanoparticles. We only briefly discuss the use of gold-based nanoparticles as many review articles are available on this subject, and we mainly focus on metal-based nanoparticles other used for radiotherapy. The metal-based nanoparticles containing unstable radionuclides are excluded from this review.

# Metal-based *NanoEnhancers* for ionizing radiation

## **Gold-based nanoparticles**

Numerous publications have shown the utility of gold nanoparticles (AuNPs) for diagnostic and therapeutic applications in cancer therapy [15], especially in radiotherapy, because gold has a high atomic number, good biocompatibility, and relatively strong photoelectric absorption coefficient [12]. In 2000, Herold et al. reported that gold microspheres produce biologically effective could dose enhancement for kilovoltage X-rays [16]. And, in 2004, Hainfeld et al. described an improvement in X-ray therapy in tumor-bearing mice following delivery of AuNPs to tumors [17]. Thereafter, other studies, using in vitro assays as well as xenografts, focused on the synergistic or sensitizing effect of AuNPs in radiation therapy using X-rays, y-rays, electron beams and high-energy charged protons/carbon ions [18, 19].

The size, shape, functionalization, concentration, and intracellular distribution of AuNPs can influence their effect on radiation [20-23]. Recently, our group published a series of papers in which we presented our studies using gold-based nanoparticles for synergistic chemo-radiotherapy (**Fig. 3**). We found that AuNPs could significantly improve the hydroxyl radical production and the cell-killing effects of X-rays and fast carbon ions [12]. We also synthesized the reductive thioctyl tirapazamine (TPZs)-modified AuNPs (TPZs-AuNPs) and showed their ability for radiation enhancement [24]. We further proposed that ionizing radiation exposure was cell cvcle phase-dependent for cellular uptake of gold nanoclusters (AuNCs). Additionally, our results demonstrated that the radiation-induced delay of cell division could enhance the retention of AuNCs in the parent tumor cells [25]. Koonce et al. also reported that when combined with X-rays, the novel nanomedicine AuNPs CYT-6091 pegylated incorporating tumor necrosis factor-a (TNF) (CytImmune, http://www.cytimmune.com/) could inhibit in vivo tumor growth [26]. Because CYT-6091 has passed phase 1 trials (NCT00356980 and NCT00436410), the work shows great promise for

clinical translation. The biological mechanisms for radiosensitizing and synergistic effects by AuNPs will be further discussed below in section **Biological contributions** of metal-based *NanoEnhancers* in RT.

## Platinum-based nanoparticles

Platinum-based agents consisting of platinum complexes (cisplatin, carboplatin, and oxaliplatin, etc.), have been widely used as anticancer drugs in chemotherapy and chemo-radiotherapy [27]. However, these compounds are nonselective for tumor cells. Hence, platinum-based nanoparticles (PtNPs) were used for cancer treatment exploiting the EPR effect. Functionalization of these particles could help to lower the volume of distribution and to reduce side effects, thus improving therapeutic efficacy [28].

Relatively few studies have investigated the radiosensitizing and synergistic effects of PtNPs for ionizing radiations. Le Sech et al. found that tuning the synchrotron X-ray energy to the L<sub>III</sub> edge of the platinum atom bound to DNA could increase the number of double-strand breaks (DSBs) in DNA under dry conditions [29]. Also, Kobayashi et al. reported that chloroterpyridine platinum (PtTC) bound to plasmid DNA could enhance the X-ray-induced breaks in DNA in aqueous solution [30]. Their results suggested that the enhancement in breaks was mainly mediated by hydroxyl radical (OH), which originated from the inner-shell excitation of platinum atoms. Corde et al. showed that irradiation above or below the platinum K-shell edge did not enhance the cell death after treating cancer cells with cis-platinum. However, photoactivation of cis-platinum (PAT-Plat) was able to enhance the slowly repairable DSBs while inhibiting the DNA-protein kinase activity, dramatically relocalizing RAD51, hyperphosphorylating BRCA1 (breast cancer 1), and activating the proto-oncogenic cellular Abelson (c-Abl) tyrosine kinase [31, 32]. In

another study, Porcel et al. presented the prominent radiosensitization platinum of nanoparticles compared to dispersed platinum atoms with fast carbon ions  $(C^{6+})$  where these nanoparticles (NPs) strongly enhanced the breaks in DNA, especially DSBs [33]. Furthermore, their results demonstrated that the production of water radicals in the radiosensitization process further damaged DNA as an indirect effect, while the direct effect played a minor role. Also, Porcel et al. reported that platinum nanoparticles could enhance the breaks in DNA with low energy X-rays, y-rays, and fast helium ions (He<sup>2+</sup>)[34, 35]. That platinum nanoparticles were capable of augmenting the radiation effects of fast protons (150 MeV H<sup>+</sup>) for plasmid DNA was shown by Schlathölter et al. [36]. In other studies, Li et al. found that the enhanced carcinostatic effect on human esophageal squamous cell carcinoma (ESCC)-derived cell line, KYSE-70, resulted from apoptosis when the cancer cells were treated with platinum nanocolloid (Pt-nc) in combination with  $\gamma$ -rays, and Pt-nc had an enhancing effect on human normal esophageal epithelial cells (HEEpiC) with irradiation [37, 38].

However, the investigation by Jawaid et al. showed that platinum nanoparticles could greatly decrease the production of reactive oxygen species (ROS) induced by X-rays, subsequent Fas expression, loss of mitochondrial membrane potential, and apoptosis in human lymphoma U937 cells [39]. They also found that platinum nanoparticles attenuated the apoptotic pathway, which was mediated by helium-based cold atmospheric plasma-induced ROS [40].

Drug delivery systems (DDS) including liposomes and other lipid-based carriers, macromolecules such polymer-based as nanoparticles, biodegradable materials, and protein-based systems could be used to improve therapeutic benefit by reducing systemic side effects and/or enhancing pharmacological properties [41-44]. In this context, Charest et al. reported that Lipoplatin<sup>TM</sup>, a liposomal formulation of cisplatin, improved the cellular uptake of cisplatin and showed a radiosensitizing effect on F98 glioma cells with  $\gamma$ -rays [45]. Recently, compared to cisplatin, cisplatin-polysilsesquinoxane (PSQ) nanoparticle (Cisplatin-PSQ NP) comprised of PSQ polymer crosslinked by a cisplatin prodrug was described by Della Rocca et al. that could improve therapeutic efficacy in chemoradiotherapy in a murine model of non-small cell lung cancer [46].

### Silver-based nanoparticles

According to previous investigations [47, 48], silver nanoparticles (AgNPs) exhibit important antimicrobial activity [49] and could also be used as potential anticancer therapeutic agents [50, 51] because of their intrinsic therapeutic properties. In cancer therapy, anti-proliferative effects of AgNPs might result from different underlying mechanisms, including induction of apoptosis [52-54], production of ROS [55], inhibitory action on the efflux activity of drug-resistant cells [56], and reactivity with glutathione (GSH) molecules [57].

Many studies demonstrated that AgNPs could as radiosensitizers and enhancers for serve radiotherapy. Gu's group observed that AgNPs (20 nm and 50 nm) sensitized glioma cells in vitro and concluded that the release of Ag<sup>+</sup> cations from the silver nanostructures inside cells might result in the radiosensitizing effect [58]. Furthermore, following delivery of AgNPs to tumors, they could improve X-ray therapy for rats bearing C6 glioma [59] and mice bearing U251 glioma [60]. Similarly, Huang et al. showed that biocompatible Ag microspheres improved the cell-killing effects of X-rays on gastric cancer MGC803 cells [61]. Lu and coworkers synthesized AgNPs using egg white and observed marked X-ray irradiation enhancement on human breast adenocarcinoma MDA-MB-231 cells [62]. Significant cytotoxic and radiosensitizing effects of AgNPs on triple-negative breast cancer (TNBC) cells in vitro and in vivo were demonstrated by Swanner et al. [63]. AgNPs also induced elevated DNA damage, increased expression of Bax/caspase-3 leading to apoptosis, decreased expression of Bcl-2, and reduction of catalase (CAT), superoxide dismutase (SOD), and total GSH contributing to the enhancement in radiosensitivity of human hepatocellular carcinoma HepG2 cells [64]. The results indicated no accumulation of cells in the sensitive  $G_2/M$  phase. Elshawy et al. observed enhancement by AgNPs of the cell-killing effects of  $\gamma$ -rays on human breast cancer MCF-7 cells, which might result from the inhibition of proliferation, increased activity of lactate dehydrogenase (LDH) and caspase-3, and altered expression of caspase-3, Bax, and Bcl-2 genes [65].

The above results illustrate that though silver is cheaper than gold, AgNPs are less inert and biocompatible than AuNPs and the biological mechanisms for radiosensitization and synergistic effects by AgNPs could be more complicated.



AuNCs concentration for incubation (µg/mL)

Figure 3. (A-C) Radiation enhancement effect of gold nanoparticles (AuNPs) [12]. (A) AuNPs improve the cell-killing effects of X-rays and fast carbon ions. (B) AuNPs improve the hydroxyl radical production of X-rays (assessed by 3-CCA). (C) AuNPs improve the hydroxyl radical production of carbon ions (assessed by 3-CCA). (D-E) Synergistic radiosensitizing effect of the reductive thioctyl trapazamine (TPZs)-modified AuNPs (TPZs-AuNPs) [24]. (D) The radiation enhancement mechanism of TPZs-AuNPs proposed in this study. (E) The fluorescence images of ROS with DCFH-DA in human hepatocellular carcinoma HepG2 cells after X-ray irradiation in the presence of TPZs-AuNPs. Scale bar = 200 µm. (F-G) Dynamically-enhanced retention of gold nanoclusters (AuNCs) in human cervical carcinoma HeLa cells following X-ray exposure [25]. (F) Schematic illustration of our strategy for improving cellular uptake of nanoparticles. (G) The fluorescence intensities of cell samples after 24 h incubation with the as-prepared luminescent AuNCs used as both "nano-agents" and fluorescent trafficking probes (control and following 2.0 Gy X-ray irradiation). Reproduced with permission from references: [12], copyright 2015 Elsevier; [24], copyright 2016 Dove Medical Press; [25], copyright 2016 Elsevier.

#### Gadolinium-based nanoparticles

Gadolinium (Gd, rare earth (lanthanide) metal) chelates have been commonly used as magnetic resonance imaging (MRI) contrast agents for T<sub>1</sub> contrast [66]. Hence, for a more precise and accurate irradiation, Gd chelates have been applied in MRI-guided radiotherapy. In 1996, Young et al. found that Gd (III) texaphyrin (Gd-tex<sup>2+</sup>), a porphyrin-like complex, could serve as an efficient radiosensitizer [67]. In tumor-bearing mice, MRI scanning confirmed the selective localization of Gd-tex<sup>2+</sup> in tumors. Motexafin gadolinium (MGd), a metallotexaphyrin, can catalyze the oxidation of intracellular reducing metabolites and generate ROS. Several large studies demonstrated that MGd was capable of potentially enhancing the cytotoxic effects of radiation through several mechanisms as well as selectively inhibiting tumor cell growth by itself [68]. Consequently, great Gd-based agents show promise for multifunctional theranostic (diagnostic and therapeutic) applications in clinical practice. In addition to its application as a positive MRI T<sub>1</sub> contrast agent [69], gadolinium-based nanoparticles (GdNPs) have been identified as valuable theranostic sensitizers for radiation therapy [70, 71](Table 1). More importantly, GdNPs, such as AGuIX (Activation and Guidance of Irradiation by X-ray) [87], exhibit diminished or no toxicity in preclinical studies employing mice and monkeys and are eliminated rapidly via the kidneys [88, 89]. In contrast, the release of free Gd (III) from acyclic chelates constituting commonly used conventional Gd-based MRI contrast agents in the acidic conditions of the kidneys can be responsible for the high frequency of serious and sometimes fatal nephrogenic systemic fibrosis (NSF) observed in patients with renal failure.

Among the lanthanide elements, Gd is of great theoretical and practical interest to researchers focusing on neutron capture therapy (NCT) because of the high neutron capture cross-section of nonradioactive <sup>157</sup>Gd [90]. Tokumitsu et al. have shown that as-prepared biodegradable gadopentetic acid (Gd-DTPA)-loaded chitosan microparticles could emit  $\gamma$ -rays in the thermal neutron irradiation test, suggesting that the particles could be used in gadolinium neutron-capture therapy (Gd-NCT)[72]. Subsequent in vitro and in vivo studies demonstrated that Gd-loaded chitosan nanoparticles were possible agents for Gd-NCT [73-76]. Studies evaluating other types of GdNPs, including calcium phosphatepolymeric micelles, Gd<sub>2</sub>O<sub>3</sub> cores/polysiloxane shell, and gadoteridol/liposome, reported similar results [77, 78, 80, 85].

**Table 1.** Application of theranostic GdNPs to radiotherapy

NP/core type	Coating	Size	Functionalization	Radiation/energy	Cells & tumor models	Function	Refs
Gd-DTPA-loaded -microparticles	Chitosan	4.1 μm 3.3 μm	None	Thermal neutron	None	Gd-NCT ( <i>in vitro</i> γ-ray emission)	[72]
Gd-DTPA-loaded -nanoparticles	Chitosan	430 nm 452 nm 391 nm 214 nm	None	Thermal neutron	C57BL/6 mice with B16F10 (malignant melanoma)	Gd-NCT	[73-7 5]
Gd-DTPA-loaded -nanoparticles	Chitosan	430 nm	None	None	(MFH) Nara-H cells (human sarcoma)	MRI	[76]
Gd-DTPA-loaded -nanoparticles	Calcium phosphate-polyme ric micelle	55 nm	None	Thermal neutron	C26 cells (colon adenocarcinoma) BALB/c mice with C26	MRI Gd-NCT	[77, 78]
Gd <sub>2</sub> O <sub>3</sub>	Polysiloxane shell	sub-45 nm	None	50 keV monochromatic synchrotron X-ray 45 MeV proton	CT26 cells (colon adenocarcinoma)	Improve ROS yields	[79]
Gd <sub>2</sub> O <sub>3</sub>	Polysiloxane shell	~7.3 nm	Pentafluorophenyl ester-modified PEG	Thermal neutron	EL4 and EL4-Luc cells (lymphoma)	Fluorescence imaging MRI Gd-NCT	[80]
Gd <sub>2</sub> O <sub>3</sub>	Polysiloxane shell	sub-5 nm	DTPA	660 keV γ-ray (source of <sup>137</sup> Cs) 6 MV X-ray X-ray microbeam (~72 Gy s <sup>-1</sup> mA <sup>-1</sup> )	U87 cells (human glioblastoma) SQ20B cells (human head and neck squamous cell carcinoma) LTH cells (Human T Lymphocytes) Fischer 344 rats with 9L cells (glioma)	MRI Radiosensitization	[81-8 3]
$Gd_2O_3$	Polysiloxane shell	3 nm	DOTA	X-ray microbeam (~72 Gy s <sup>-1</sup> mA <sup>-1</sup> )	Fischer 344 rats with 9L	MRI Radiosensitization	[84]
Gadoteridol (C17H29GdN4O7)	Coatsome EL-01-N liposome	N/A	None	Thermal neutron	BALB/c mice with C26	MRI Gd-NCT	[85]
Gd <sub>2</sub> O <sub>3</sub>	Withania somnifera extract	25-35 nm	None	660 keV γ-ray (source of <sup>137</sup> Cs)	Swiss albino mice with EAC cells (Ehrlich ascites carcinoma)	Radiosensitization	[86]

DOTA: 1,4,7,10-tetraazacyclododecane-N,N',N'',N'''-tetraacetic acid; DTPA: diethylenetriaminepentaacetic acid; Gd-NCT: gadolinium neutron-capture therapy; MRI: magnetic resonance imaging; PEG: polyethylene glycol; ROS: reactive oxygen species.

The radiosensitizing and synergistic effects of GdNPs when combined with other ionizing radiation types, such as  $\gamma$ -rays, X-rays, and charged particles (protons and heavy ions), have been well established. Mowat et al. found that Gd<sub>2</sub>O<sub>3</sub>-based nanoparticles could be used as sensitizing agents to improve the killing effects of both γ-rays and X-rays [81]. Furthermore, Le Duc et al. showed that the GdNP improved the survival of rats bearing aggressive brain tumors by means of microbeam radiation therapy (MRT) while applied to MRI [82](Fig. 4). Therefore, this sub-5 nm GdNP consisting of a polysiloxane network surrounded by Gd chelates (cyclic, not acyclic) was named "AGuIX" [91](Table 2). As described by Mignot et al., these small rigid platforms (SRP) were synthesized by an original top-down process, which consists of gadolinium oxide (Gd<sub>2</sub>O<sub>3</sub>) core formation, encapsulation by a polysiloxane shell DOTAGA (1,4,7,10-tetraazacyclografted with dodecane-1-glutaric anhydride-4,7,10-triacetic acid) ligands, Gd<sub>2</sub>O<sub>3</sub> core dissolution following chelation of Gd<sup>3+</sup> by DOTAGA ligands, and polysiloxane fragmentation [84]. AGuIX nanoparticles exhibit potential as a theranostic drug for radiation therapy, including MRI contrast, radiosensitization, and

adapted biodistribution due to the EPR effect [93, 94, 96, 99-101]. A phase 1 trial (NCT02820454) is in progress in France by the AGuIX group (NH TherAguix, http://nhtheraguix.com/). It was reported that the first in human injection of AGuIX was carried out at Grenoble hospital in July 2016.

#### Iron-based nanoparticles

In addition to GdNPs, iron-based nanoparticles have been investigated as theranostic magnetic nanoparticles [106, 107], including inorganic paramagnetic iron oxide (or magnetite) nanoparticles, or superparamagnetic iron oxide nanoparticles (SPIONs) [108]. However, instead of T<sub>1</sub> contrast like GdNPs, iron oxide nanoparticles (IONs) have been used as negative T<sub>2</sub> MRI contrast agents [109]. Furthermore, IONs are considered ideal agents for diagnosis, treatment, and treatment monitoring of cancers because of their excellent properties, such as facile synthesis, biocompatibility, and biodegradability [110]. In particular, IONs have potential applications not only as MRI contrast agents photothermal but also in therapy (PTT), photodynamic therapy magnetic (PDT), hyperthermia, and chemo/biotherapeutics [111-113].



Figure 4. Ultrasmall gadolinium-based nanoparticles (GdNPs) induce both a positive contrast for magnetic resonance imaging (MRI) and a radiosensitizing effect. (A) Transmission electron microscopy (TEM) phase-contrast imaging at low spatial resolution of  $Gd_2O_3$  cores after encapsulation in a polysiloxane shell (insets show projected potential calculations of  $Gd_2O_3$  after and before polysiloxane formation (top and bottom, respectively)). (B) MRI T<sub>1</sub>-weighted images of the brain of a 9L glioma-bearing rat before and after intravenous injection of GdNPs. (C) T<sub>1</sub>-weighted images of a slice including a kidney (K) and the bladder (B) of a rat before and after intravenous injection of GdNPs. (C) T<sub>1</sub>-weighted images of a series of successive transverse slices including the right and left kidneys (RK and LK, respectively) and the bladder (B) of a 9L glioma-bearing rat. The images were recorded before and after the intravenous injection of GdNPs. (E) Survival curve comparison obtained on 9L glioma-bearing rats without treatment (black dashed curve), only treated by microbeam radiation therapy (MRT)(blue curve), and treated by MRT 5 min (red curve) and 20 min (green curve) after GdNP intravenous injection during 103 days after tumor implantation. Reproduced with permission from reference [82], copyright 2011 American Chemical Society.

#### Table 2. Application of AGulX<sup>a</sup> to radiotherapy

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Radiation/energy	Cells & tumor models	Function	Refs
220 kVp & 6 MV X-ray	HeLa cells (human cervical carcinoma)	Radiosensitization	[91]
250 kV & 320 kV X-ray	SQ20B, FaDu and Cal33 cells (human head and neck squamous cell carcinoma) Athymic nude mice with SQ20B	Radiosensitization	[92]
X-ray microbeam (62 Gy s <sup>-1</sup> mA <sup>-1</sup> )	Fischer 344 rats with 9L	MRI Radiosensitization	[93]
200 keV X-ray	NMRI nude mice with H358-Luc cells (human non-small cell lung cancer)	MRI Radiosensitization	[94]
220 kVp & 6 MV X-ray	Panc1 cells (human pancreatic cancer)	MRI Radiosensitization	[95]
220 kV & 320 kV X-ray	B16F10 cells C57BL/6J mice with B16F10	MRI Radiosensitization	[96]
90 keV X-ray X-ray microbeam (~72 Gy s <sup>-1</sup> mA <sup>-1</sup> )	F98 cells (glioma) Fischer 344 rats with 9L	Radiosensitization MRI Radiosensitization	[97] [98]
220 kVp & 6 MV X-ray	Capan-1 cells (human pancreatic adenocarcinoma) CrTac: NCr- <i>Fox1nu</i> mice with Capan-1 Cynomolgus monkeys ( <i>macaca</i> <i>fascicularis</i> )	MRI Radiosensitization	[99]
6 MV X-ray	Fischer 344 rats with 9L-ESRF cells (glioma)	MRI Radiosensitization	[100]
6 MV X-ray	Capan-1 cells CrTac: NCr- <i>Fox1nu</i> mice with Capan-1	MRI Radiosensitization	[101]
1.25 MeV γ-ray (source of <sup>60</sup> Co)	U87 cells	Radiosensitization	[102]
1.25 MeV γ-ray (source of <sup>60</sup> Co) 25-80 keV monochromatic synchrotron X-ray	F98 cells	Radiosensitization	[103]
150 MeV proton	None	Improve SSB & DSB yields	[104]
150 MeV/uma He <sup>2+</sup> (LET = 2.33 keV/μm) 270 MeV/uma C <sup>6+</sup> (LET = 13 keV/μm)	CHO cells (Chinese hamster ovary)	Radiosensitization	[105]

<sup>a</sup>AGuIX: Activation and Guidance of Irradiation by X-ray, the sub-5 nm GdNPs based on a polysiloxane network surrounded by Gd chelates. DSB: double-strand break; SSB: single-strand break.

Another promising application of IONs is as radiosensitizers/enhancers. Although the atomic number of iron (Fe, Z = 26) is relatively low, IONs are mostly used in combination with low-linear energy transfer (LET) kV and MV X-rays. In an orthotopic rat model of prostate cancer following intratumoral injection of an aminosilane-type shell-coated SPION with a core diameter of 15 nm, a combination of thermotherapy and X-ray irradiation was shown to more effectively reduce tumor growth than radiation alone [114]. This result might be attributed in part to the radiosensitizing and synergistic effects by magnetic nanoparticles. Other studies also reported notable in vitro radiosensitization of prostate cancer cells by X-rays in conjunction with IONs [115, 116]. Also, it has been demonstrated that IONs could sensitize other tumor cells both in vitro and in vivo. For instance, Huang et al. showed that cross-linked dextran-coated IONs (CLIONs) were internalized by HeLa cells and EMT-6 mouse breast cancer cells and improved the killing effects of X-ray irradiation [117]. Recently, several groups have presented similar results [118] showing the application of IONs together with MRI [119]. Other studies indicated that X-ray radiosensitization by IONs might be attributed to the production of ROS owing to IONs' surface-catalyzed Haber-Weiss cycle and Fenton reaction [120-122]. Furthermore, in other studies, the IONs-mediated radiosensitization was observed in combination with monoenergetic synchrotron X-ray radiation [123, 124]. Kleinauskas et al. reported that IONs enhanced the efficacy of monochromatic Fe K-edge synchrotron X-rays more significantly than conventional broadband X-rays [115]. Considering the limitations of conventional proton therapy (PT), Kim et al. evaluated the effect of IONs for PT and demonstrated the radiosensitizing effects of IONs in vitro and in vivo [125]. The follow-up studies also provided evidence for this promising application of IONs [126-128]. It was also reported that IONs were able to enhance radiation cytotoxicity of  $\gamma$ -rays [129]. In addition to IONs, other types of iron based-nanoparticles have shown radiosensitizing effects [130].

Although a number of ION formulations have been approved by the FDA, many studies have shown the toxic effects of IONs [110]. To overcome this disadvantage, surface modification and functionalization with various molecules and ligands would be helpful in addressing clearance from the circulation and retention in the mononuclear phagocyte system (MPS) as well as improving tissue targeting, biocompatibility, and stability [131]. Currently, IONs remain as the ideal platform for cancer theranostics.

#### Hafnium-based nanoparticles

Hafnium oxide (hafnia, HfO<sub>2</sub>) has been shown to possess photo-luminescent properties [132] and HfO<sub>2</sub> nanoparticles (HfO<sub>2</sub> NPs) exhibit chemical inertness in cellular and subcellular systems [133-135]. Hence, owing to the high atomic number, electron density, and chemical stability of hafnium/hafnia, HfO<sub>2</sub> NPs show promising potential as sensitizers for radiation therapy as well as X-ray contrast agents [136].

NBTXR3, the functionalized HfO<sub>2</sub> NPs developed by Nanobiotix (http://www.nanobiotix. com/\_en/), are 50-nm-sized crystalline nanoparticles bearing a negative surface charge. NBTXR3 were designed for direct local intratumoral injection and subsequent radiosensitization [6, 137]. Subsequently, it has been demonstrated by Monte Carlo simulation

that NBTXR3 crystalline nanoparticles exposed to high-energy photons could promote a significant radiation dose enhancement, and the obvious radiosensitizing effects of NBTXR3 in vitro and in vivo were presented [138-140]. Also, nonclinical toxicology evaluation of this agent showed a good tolerance. Many clinical trials (7 records) were carried out using NBTXR3 crystalline nanoparticles-RT combination (Table 3). The phase 1 trial of NBTXR3 (NCT01433068) started in 2011 and completed in 2015. It was shown that human injection (22 sarcoma patients in France) was well tolerated until 10% of tumor volume with preoperative external beam radiotherapy and did not result in leakage of these nanoparticles into the adjoining healthy tissues, while NBTXR3 NPs were used as a medical device to reduce the tumor size before surgery (performed 6-8 weeks after RT completion) [141-144]. Currently, several multinational phase 1/2 trials and one phase 2/3 trial are ongoing and recruiting participants for the treatment of head and neck cancer (squamous cell carcinoma), rectal cancer, hepatocellular carcinoma (liver cancer), prostate cancer, and adult soft tissue sarcoma.

 Table 3.
 Clinical trials investigating NBTXR3<sup>a</sup> crystalline nanoparticle-RT combination (records in https://clinicaltrials.gov/)

ClinicalTrials.go v Identifier	Star t	Phas e	Indication	Numbe r of	Country & region	Status
NCT01433068	year 201 1	Ι	Adult soft tissue sarcoma	22	France	Complete d
NCT01946867	201 3	Ι	Head and neck cancer	48	France, Spain	Recruiting
NCT02379845	201 5	п/ш	Adult soft tissue sarcoma	180	Australia, Belgium, France, Germany, Hong Kong, Hungary, Italy, Norway, Philippine s, Poland, Romania, South Africa, Spain	Recruiting
NCT02465593	201 5	I/II	Rectal cancer	42	Taiwan	Recruiting
NCT02721056	201 5	I/II	Hepatocellula r carcinoma; liver cancer	200	France	Recruiting
NCT02805894	201 6	I/II	Prostate cancer	96	United States	Recruiting
NCT02901483	201 6	I/II	Head and neck squamous cell carcinoma	42	Taiwan	Recruiting

 $^{\rm a}\text{NBTXR3},$  50-nm-sized crystalline  $\text{HfO}_2$  nanoparticles bearing a negative surface charge.

Chen et al. synthesized hafnium-doped hydroxyapatite nanoparticles (Hf:HAp NPs) by wet chemical precipitation and showed marked  $\gamma$ -ray irradiation enhancement of Hf:HAp NPs, probably resulting from intracellular ROS formation, for human non-small cell lung cancer A549 cells using *in vitro* assay as well as xenografted tumors [145]. A rational design of nanoscale metal organic frameworks (NMOFs) composed of hafnium (Hf<sup>4+</sup>) and tetrakis (4-carboxyphenyl) porphyrin (TCPP) was also described with significant radiosensitizing effects of pegylated Hf-TCPP NMOFs exhibiting efficient clearance from the body when combined with X-rays [146].

# Other types of metallic element-based nanoparticles

A considerable number of nanoparticles based on other metallic elements have demonstrated efficiency in radiosensitization or synergistic cell-killing effects for radiation therapy with single functionality or multifunctionality. These elements include bismuth, titanium, tantalum, cerium, germanium, zinc, and tungsten and were evaluated in several studies.

Due to the strong absorption of X-rays, bismuth nanoparticles (BiNPs) were employed as contrast agents for X-ray imaging [147]. Also, BiNPs led to higher dose enhancement than AuNPs and PtNPs for diagnostic X-rays, attributed to both photoelectrons and Auger electrons with respect to the cell and the nucleus [10]. The synthesized NPs mainly comprise Bi<sub>2</sub>Se<sub>3</sub>, Bi<sub>2</sub>S<sub>3</sub>, and Bi<sub>2</sub>O<sub>3</sub> NPs stabilized by different ligands and molecules. Hossain and coworkers used BiNPs conjugated with folic acid to selectively detect circulating tumor cells (CTCs) combined with collimated X-rays, and showed the improved killing of localized CTCs with the dose of primary X-rays Other investigators also reported that [148]. biocompatible Bi<sub>2</sub>Se<sub>3</sub> NPs exhibited diminished toxicity and the potential to function as theranostic agents for radiation therapy, including multimodal imaging, radiosensitization, and PTT [149, 150]. Moreover, several studies have revealed that Bi<sub>2</sub>S<sub>3</sub> and Bi2O3 NPs could serve as radiosensitizers and enhancers for radiotherapy [151-156]. Algathami et al. validated and quantified the radiation dose enhancement of Bi<sub>2</sub>S<sub>3</sub> and Bi<sub>2</sub>O<sub>3</sub> NPs using phantom cuvettes and novel 3D phantoms and found that the radiation enhancement was greater when irradiating with kV X-rays compared to MV X-rays [157]. Nevertheless, a recent study showed that Bi<sub>2</sub>Se<sub>3</sub> NP, also the catalytic topological insulator, could be used as a potential radioprotective agent due to its ability to scavenge free radicals [158].

Titanium-based nanoparticles can also function as NanoEnhancers. Titanium dioxides (titania, TiO<sub>2</sub>), sometimes used as a disinfectant, is employed to eradicate cancer cells using photocatalytic chemistry [159]. It has been reported that two human glioblastoma cells, SNB-19 and U87MG, were radiosensitized following incubation with titanate nanotubes (TiONts)[160]. Also, titania nanoparticles modified with polyacrylic acid (PAA) and H<sub>2</sub>O<sub>2</sub> (PAA-TiO<sub>2</sub>/H<sub>2</sub>O<sub>2</sub> NPs) enhanced the cell-killing effects of X-rays mediated through the generation of ROS/hydroxyl radicals, which was assessed by colony forming assays and xenografts [161]. Interestingly, this PAA-TiO<sub>2</sub>/H<sub>2</sub>O<sub>2</sub> NP was also capable of releasing H<sub>2</sub>O<sub>2</sub> molecules from the NP surface [162]. It was suggested that Čerenkov radiation (CR) contributes to the radiation enhancement in the presence of TiO<sub>2</sub> NPs [163].

Tantalum-based NPs can play a role in radiosensitizing or synergistic cell-killing effects for radiation therapy. Using plasmid DNA, Cai et al. demonstrated that secondary electrons emitted from the soft X-ray-exposed tantalum surface induced DNA damage more efficiently than X-ray alone [164]. Subsequently, it was shown that tantalum pentoxide nanoceramics/ceramic nanostructured particles (Ta<sub>2</sub>O<sub>5</sub> NSPs) exposed to MV X-ray photons could promote an obvious radiation dose enhancement in 9L glioma cells [165]. Several relevant follow-up studies concerning Ta2O5 NSP radiosensitization have been published [166-169]. Considering the lower oxygen partial pressure (pO2) inside tumors and advantages of multifunctional nanotheranostics, a series of modified and functionalized tantalum oxide nanoparticles (TaOx NPs) have been synthesized, and their diagnostic and therapeutic application in radiotherapy has been demonstrated [170-173].

Numerous studies have investigated cerium (another high-Z lanthanide rare earth element) oxide (ceria, CeO<sub>2</sub>) nanoparticles and demonstrated their diverse applications, such as radioprotection, radiosensitization, anticancer therapeutics, and antioxidation [174-178]. Tarnuzzer et al. found that ceria NPs protected the normal human breast CRL-8798 epithelial cells but not the human breast cancer MCF-7 cells from radiation-induced cell death [179]. Subsequently, other groups presented detailed investigations of the effects of CeO2 NPs [180-184]. It was also confirmed that CeO<sub>2</sub> NPs could enhance the cytotoxic effects of radiation therapy. Cerium oxide nanoparticles could sensitize pancreatic cancer cells to kV X-rays by improving ROS production, as shown by in vitro assays as well as xenografts [185]. Other groups also reported similar results when evaluating X-rays, electrons, and protons [186-188]. Thus, like

PtNPs and Bi<sub>2</sub>Se<sub>3</sub> NPs, CeO<sub>2</sub> NPs have dual effects on radiotherapy. These results suggest that metal-based nanoparticles act not only as radiosensitizers but also as radioprotectors in radiation therapy [189]. It is, therefore, important to investigate the underlying mechanisms of metal-based nanoparticles-induced dual effects.

In addition to the metallic elements listed above, other nanoparticles also show promise as effective *NanoEnhancers* for future radiotherapy. For example, inorganic germanium nanoparticles (GeNPs) could enhance the radiosensitivity of cells [190]. Similarly, the potential of zinc oxide (ZnO) nanoparticles [191, 192] for radiosensitization is obvious from both *in vitro* and *in vivo* studies, and tungsten-based nanoparticles have also been reported as probable radiosensitizers [193-196] (**Fig. 5**).

## Theranostic multimetallic nanocomposites for future RT

As discussed, given the advantages of multifunctional theranostics in radiation oncology, a large number of hybrid nanomaterials based on multimetallic elements (e.g., bimetallic and trimetallic) have been prepared and might help to improve therapeutic benefits for future radiation therapy. In this section, we present some general examples of these theranostic nanoparticles (**Table 4**), and discuss the advancements in *NanoEnhancers*.

Broadly, several factors determine the functions and applications of the multimetallic nanocomposites (**Fig. 6**) including types of elements, their sizes, structures, shapes, coatings, functionalizations, and drugs to be delivered. As reviewed in previous sections, most high Z metallic elements were applied for radiosensitization including X-ray contrast and computed tomography (CT)[198]. Magnetic metals, such as Gd and Fe, were utilized for MRI contrast [202, 205], and concurrent chemotherapy was achieved in the presence of Pt and its complexes [197, 203].

Multimetallic nanocomposites are well-designed metal-based hybrid materials with diverse structures and shapes consisting of at least two metals. Besides their radiosensitizing and synergistic effects as well as CT and MR imaging capabilities, multimetallic nanocomposites have exhibited a variety of additional functions in drug delivery [209], PTT [210, 212], PDT [208], PA (photoacoustic) imaging [211, 213], and monitoring and evaluation during treatment [199, 200]. In particular, the multimetallic nanocomposites nanoparticles termed upconversion (UCNPs) containing rare earth elements [214] have attracted great interest in radiation oncology [215]. Overall, UCNPs can generate cytotoxic ROS [216]. Moreover, it was demonstrated that UCNPs could play a role in PTT [217] and diagnostic imaging [218]. Besides the above-mentioned NPs, a variety of metallic, non-metallic, and metallio-organic nanocomposites have been formulated and studied as promising multifunctional theranostic *NanoEnhancers* [219-221].

## **Biological contributions of metal-based** *NanoEnhancers* in **R**T

As described above. the metal-based NanoEnhancers show promising efficacy against cancers in both in vitro and in vivo systems for a range of ionizing radiation types including  $\gamma$ -rays, X-rays, and charged particles. However, the predicted enhancement in physical absorbed doses based on the Monte Carlo simulations often differed from the observed biological enhancement, with the former being less than the latter [222]. Hence, the amplification of cell-killing effects for ionizing radiation not only results from the increase in physical dose, but also mainly from other fluctuations or responses in biological systems. In addition to the

major role of oxygen radicals in metal-based NanoEnhancer radiosensitization [223, 224], numerous investigations have suggested the existence of complicated processes in the biological phase. It appears that other possible mechanisms underlie the sensitizing and synergistic effects of metal-based NanoEnhancers in radiotherapy, which may vary based on the metallic element of the NanoEnhancer. Moreover, the enhancement depends on cellular and subcellular distribution and location of metal-based NanoEnhancers with respect to the cell and the nucleus [10, 225, 226] (Fig. 2, lower-left). Also, metal-based NanoEnhancers in tumor cells or organelles, such as mitochondria and endoplasmic reticulum (ER) [227], can elicit unidentified cellular biochemical changes [228-230] leading to their radiosensitizing and synergistic effects in combination with ionizing radiations. Thus, the enhanced cell-killing effects might result from the complicated physical, chemical, and biological effects induced by the complex action of metal-based nanoparticles and ionizing radiation exposure [8, 231].



Figure 5. Tungsten sulfide (WS<sub>2</sub>) quantum dots (QDs) as multifunctional nanotheranostic agents for *in vivo* dual-modal image-guided photothermal/radiotherapy synergistic therapy. (A) Schematic illustration of WS<sub>2</sub> QDs for dual-mode computed tomography (CT)/photoacoustic (PA) imaging and photothermal therapy (PTT)/radiation therapy (RT) synergistic therapy. (B) Atomic force microscopy (AFM) topography images of the as-prepared WS<sub>2</sub> QDs. (C) Temperature change of WS<sub>2</sub> QD solution at a concentration of 100 ppm over four laser on/off cycles. (D) PA images of BEL-7402 human hepatocellular carcinoma-bearing mice before and after the intravenous injection of WS<sub>2</sub> QDs. (E) CT images of tumor before and after the intravenous of BEL-7402 human hepatocellular carcinoma-bearing mice after different groups of BEL-7402 human hepatocellular carcinoma-bearing mice after different administrations at the end of PTT and RT. Repreduced with permission from reference [194], copyright 2015 American Chemical Society.

NP type	Metal 1	Metal 2	Metal 3	Coating	Size (nm)	Functionalization & delivered drug	Radiation/ene rgy	Cells & tumor models	Function	Refs
Spheres	Au	Pt (cisplatin)	None	None	50	MUA	660 keV γ-ray (source of <sup>137</sup> Cs)	S1, S2, and SP56 cells (human glioblastoma multiforme)	Chemotherapy Radiosensitization	[197]
Dendrites	Au	Pt	None	PEG	30	None	X-ray	4T1 cells (breast cancer)	CT imaging Radiosensitization PTT	[198]
Spheres	Au	Gd (chelates)	None	None	N/A	DTDTPA	660 keV γ-ray (source of <sup>137</sup> Cs) X-ray microbeam (~72 Gy s <sup>-1</sup> mA <sup>-1</sup> )	U87 cells Sprague-Dawley rats with osteosarcoma Fischer 344 rats with 9LGS cells (glioma)	MRI Radiosensitization Monitoring and evaluation	[199]
Polymeric micelles	Au	Fe (SPIONs)	None	PEG-PCL	100	None	150 kVp X-ray	HT1080 cells (human fibrosarcoma) Nu/nu mice with HT1080	MRI Radiosensitization Monitoring and evaluation	[200]
Spheres	Au (core)	Mn (MnO <sub>2</sub> , shell)	None	PEG	~100	None	160 keV X-ray	4T1 cells BALB/c mice with 4T1	MRI Radiosensitization	[201]
Spheres	Au (core)	Mn (MnS, shell)	Zn (ZnS, shell)	PEG	~110	None	X-ray	4T1 cells BALB/c mice with 4T1	MRI Radiosensitization	[202]
Spheres	Pt	Fe	None	Cysteami ne	3	None	6 MV X-ray	HEK293T cells (human embryonic kidney) HeLa cells	Chemotherapy Radiosensitization	[203]
Spheres	Ag	Fe (SPIONs)	None	None	~102	Epidermal growth factor receptor-specific antibody	X-ray	CNE cells (human nasopharyngeal carcinoma)	MRI Radiosensitization	[204]
Flakes	Gd (Gd (III), doped)	W (WS2, base)	None	C <sub>18</sub> PMH- PEG	~0.268	None	X-ray	4T1 cells BALB/c mice with 4T1	CT imaging MRI PA imaging Radiosensitization PTT	[205]
Clusters	Gd	W	None	BSA	3.5	None	X-ray	BALB/c mice with MDA-MB-231 (human breast adenocarcinoma) BALB/c mice with BEL-7402 (human hepatocellular carcinoma)	CT imaging MRI Radiosensitization PTT	[206]
Particles/f ragments	Gd (AGuIX, silica-base	Bi (Bi (III), entrapped)	None	None	sub-5	DOTAGA DOTA-NHS	220 kVp & 6 MV X-ray	A549 cells (human non-small cell lung cancer)	CT imaging MRI Radiosensitization	[207]
Spheres	a) Gd/ Eu (doped)	Zn (ZnO, base)	None	None	9	None	200 kVp X-ray 1.25 MeV γ-ray (source of <sup>60</sup> Co)	PC3 cells (human prostate carcinoma) L929 cells (fibroblast) HeLa cells	CT imaging MRI Radiosensitization PDT	[208]
Spheres	Fe (SPIONs, core)	Zn (ZnO, shell)	None	None	< 200	Transferrin receptor antibody Doxorubicin	6 MeV X-ray	SMMC-7721 cells (human hepatocellular carcinoma) BALB/c mice with SMMC-7721	MRI Chemotherapy Radiosensitization	[209]
"Bullet-lik e″	Bi (Bi <sub>2</sub> Se <sub>3</sub> , shell)	Mn (MnSe, core)	None	PEG	Length: 132 Width: 111	None	140 keV X-ray	4T1 cells BALB/c mice with 4T1	CT imaging MRI Radiosensitization PTT	[210]
Sheets	Bi (Bi <sub>2</sub> S <sub>3</sub> )	Mo (MoS <sub>2</sub> )	None	PEG	~300	None	X-ray	L929 cells BALB/c mice with 4T1	CT imaging PA imaging Radiosensitization PTT	[211]

BSA: bovine serum albumin; C<sub>18</sub>PMH: poly(maleic anhydride-alt-1-octadecene); CT: computed tomography; DOTAGA: 1,4,7,10-tetraazacyclododecane-1-glutaric anhydride-4,7,10-triacetic acid; DTDTPA: dithiolated derivative of the diethylenetriaminepentacetic acid; MUA: mercaptoundecanoic acid; NHS: *N*-hydroxysuccinimide; PA: photoacoustic; PCL: polycaprolactone; PDT: photodynamic therapy; PTT: photothermal therapy.



Figure 6. Ultrasmall silica-based bismuth gadolinium nanoparticles (gadolinium-based AGulX (Activation and Guidance of Irradiation by X-ray) nanoparticles with entrapped Bi (III)) for dual magnetic resonance/CT image-guided radiotherapy (IGRT). (A) These agents were synthesized by an original top-down process, which consists of Gd<sub>2</sub>O<sub>3</sub> core formation, encapsulation by polysiloxane shell grafted with DOTAGA (1,4,7,10-tetraazacyclododecane-1-glutaric anhydride-4,7,10-triacetic acid) ligands, Gd<sub>2</sub>O<sub>3</sub> core dissolution following chelation of Gd (III) by DOTAGA ligands, and polysiloxane fragmentation. Moreover, at the final stage of the synthesis, DOTA (1,4,7,10-tetraazacyclododecane-N,N',N'',N'''-tetraacetic acid)-NHS (N-hydroxysuccinimide) ligands were grafted to the surface to entrap free Bi<sup>3+</sup> atoms into the final complex. (B) MRI (relaxivity) and CT (Hounsfield units) linear relation with concentration of nanoparticles (metal) in aqueous solution. (C) Qualitative representation of γ-H2AX and 53BP1 (p53-binding protein 1) foci formation, with and without 4 Gy irradiation, with and without nanoparticles, 15 min post-irradiation. (D) Biodistribution study performed by ICP-MS (inductively coupled plasma-mass spectrometry) in animals after intravenous injection of nanoparticles. (E) Experimental timeline based on a current clinical workflow for MRI-guided radiotherapy. (F) Fusion of the CT and MRI images. Yellow arrows indicate the inceased contrast in the tumor. (G) Dosimetry study performed for a single fraction of 10 Gy irradiation delivered from a clinical linear accelerator (6 MV). (H) Dose-volume histogram showing the radiation dose distribution in the tumor and in the 2017 American Chemical Society.

Although a comprehensive understanding of the biological mechanisms involved in radiosensitization of metal-based NanoEnhancer is crucial for their correct design and clinical application, relatively limited information is available on this subject. The existing investigations mainly focused on the radiosensitizing and synergistic effects of AuNPs and AgNPs [232, 233]. The underlying mechanisms for radiosensitization with conventional chemical and biological agents as well as metal-based NanoEnhancers mainly consist of ROS generation, targeting of DNA damage response and repair, inhibition of cell cycle checkpoint machinery, modification of the tumor microenvironment, antiangiogenesis, and immune modulation [234]. As

displayed in **Fig. 2** (upper-right), probable biological mechanisms mainly consist of oxidative stress, cell cycle arrest, DNA repair inhibition, autophagy, and ER stress, which are discussed separately in this section.

# Oxidative stress and mitochondrial dysfunction

Oxidative stress could damage cells through the interactions between critical biological targets or reducing substances and generated ROS in the presence of ionizing radiations and metal-based *NanoEnhancers* [235]. The primary targets and reducing substances mainly comprise cellular membrane structures, DNA, proteins, lipids, and

GSH. Also,  $pO_2$  inside tumors has a prominent role during the course of RT and the hypoxic tumor microenvironment weakens ROS production and oxygen fixation reaction, decreasing the RT efficacy [225]. Mitochondria are believed to be the amplifiers of radiation-induced ROS production [236] and, as the "energy powerhouse of the cell", are unavoidable early targets in the design of next generation metal-based NanoEnhancers with organelle-targeting capability [237-239]. Mitochondrial dysfunction, which includes mitochondrial DNA (mtDNA) damage, mobilization of cytochrome c, and other significant effects of oxidative stress, could trigger the cell death such as apoptosis. Taggart et al. provided the first evidence for the involvement of mitochondria in the AuNPs-mediated radiosensitizing effect [240]. The same group recently identified mitochondria as a probable driver for the radiosensitization by AuNPs outside the nucleus when irradiating cytoplasm with a very low-energy ultrasoft X-ray microbeam (278 eV carbon K-shell X-rays) without causing nuclear damage [241]. In addition, protein disulphide isomerase (PDI) residing in or on the ER/nucleus/mitochondria/cytosol/cell surface as well as mitochondrial oxidation were identified as novel targets during radiosensitization by AuNPs [242]. Nevertheless, the nucleus has been proven to be one of the most sensitive and major targets for metal-based NanoEnhancers.

Interestingly, in contrast to the above results, some previous studies have demonstrated that metal-based *NanoEnhancers* could diminish DNA repair efficiency as well as result in accumulation of cells in the sensitive  $G_2/M$  phase. However, when combined with X-rays, no notable enhancement in ROS production [160, 243] was observed, and even reduction in both endogenous and radiation-generated ROS was reported [187].

## Cell cycle arrest/redistribution

Ionizing radiation exposure has been demonstrated to delay mammalian cell cycle progression by inducing G1 or G2 phase arrest [244, 245]. As part of the complex cellular responses to DNA damage, these cell cycle checkpoint activations involve DNA repair. Therefore, inhibition of the cell cycle checkpoint machinery is considered a promising way to sensitize tumors to ionizing radiations. The cell cycle phase at the time of irradiation is equally important and can influence the radiosensitivity of cancer cells. The cells in late S phase are most radioresistant, while the cells in  $G_2/M$  phase are most radiosensitive (radiosensitivity:  $G_2/M > G_1 > early S$ > late S)[246, 247]. Consequently, chemotherapy (such as paclitaxel (PTX) and docetaxel (DTX))

followed by radiotherapy and multifraction radiotherapy (e.g., conventional fractionation (CF), 1.8-2.5 Gy daily fractions, Monday to Friday treatment), might synchronize cells at sensitive phases ( $G_2/M$  and  $G_1$  phase) for RT, and could partially help to improve the therapeutic benefit.

The metal-based NPs induce cell cycle arrest [248-250], which can be exploited to increase radiosensitivity as well as chemosensitivity of cancer cells. Roa et al. reported that glucose-capped AuNPs played a role in radiosensitizing the radioresistant human prostate carcinoma DU-145 cells [251]. Additionally, the authors analyzed the effect of AuNPs on the cell cycle distribution of cancer cells with flow cytometry. The results indicated that pretreatment with AuNPs led to accumulation of cancer cells at the most radiosensitive  $G_2/M$  phase of the cell cycle due to the activation of the cyclin-dependent kinases (CDK). Likewise, data from other groups suggested that AuNPs-induced G<sub>2</sub>/M phase arrest might contribute to the radiation enhancement when combined with AuNPs [252-256]. In contrast, we and several other groups showed that treatment with AuNPs did not result in accumulation of cells in the radiosensitive  $G_2/M$  phase [12, 225, 257, 258]. In this respect, AgNPs [259-262] and GdNPs [103] were also reported to arrest cancer cells at the  $G_2/M$  phase.

Also, as mentioned earlier in subsection **Gold-based nanoparticles**, we have previously shown that exposure to ionizing radiation could delay the division of tumor cells, and improved the subsequent cellular uptake of nano-agents in cells.

## **DNA** repair inhibition

Radiotherapy is known to elicit various types of DNA damage [263]. After sensing DNA damage, cellular DNA damage-response (DDR) machinery executes DNA repair by homologous recombination (HR), nonhomologous end-joining (NHEJ) for DSBs, as well as other pathways. Failure to repair the damage would cause cell death. Thus, in combination with RT, inhibition of DNA repair can augment the killing of tumor cells [264].

Typically, ionizing radiation-induced DNA damage modes include single-strand breaks (SSBs), DSBs, DNA-protein cross-links, and base damages. Among them, DSBs are considered the principal lethal type for radiation-induced lesions due to their more irreparable nature [265]. Some studies have shown that metal-based *NanoEnhancers* could increase the number of initial DSBs in DNA following irradiation when employing plasmid DNA and agarose gel electrophoresis [20]. In spite of this, along with time progress, the variation in DNA repair (in terms of dvnamic changes in DNA damage) during radiosensitization can also be evaluated by comet blotting, assay, Western or immunostaining. Phosphorylated histone variant v-H2AX (phosphorylation at serine 139) and p53-binding protein 1 (53BP1) (DNA repair protein) are considered to be the earliest sensitive markers of DSBs and the conserved DSBs sensor, respectively [266]. Therefore, immunostaining to monitor the dynamic DSBs number, the kinetics of y-H2AX and 53BP1 foci were employed to assess the effect of metal-based NanoEnhancers on the subsequent DNA repair after DSBs damage in RT [267].

As reviewed in previous sections, TiONts and germanium oxide (germania, GeO<sub>2</sub>) have been shown to decrease efficiency of DNA repair following irradiation. then sensitize cells [160. 243]. Quantification of indirect y-H2AX and 53BP1 foci through immunofluorescence assays revealed the impact of AuNPs on the DNA repair processes following X-ray exposure [225, 268]. However, other reports suggested that AuNPs did not influence the DNA repair [258, 269]. A recent study indicated that gadolinium-based AGuIX NPs affected neither the level of DSBs nor the kinetics or efficiency of their repair, while eliciting marked radiosensitizing and synergistic effects probably attributed to the NPs' location in the cytoplasm rather than the nucleus [270]. Furthermore, repair of X-ray-induced DNA damage in human hepatocellular carcinoma HepG2 cells was shown to be delayed in the presence of AgNPs, while X-ray-induced initial DNA damage was not affected. [271].

# Autophagy, ER stress, and other biological mechanisms

Among the biological mechanisms underlying radiation enhancement in the presence of metal-based *NanoEnhancers* are autophagy and ER stress.

Autophagy plays a major role during cellular and environmental stress by facilitating nutrient recycling via lysosome-mediated degradation of damaged and dysfunctional organelles, proteins, and other cytoplasmic constituents and helps in maintaining the intracellular homeostasis [272, 273]. This conserved catabolic process possesses both positive and negative regulatory capabilities and can promote tumor progression [274]. Inhibition of autophagic responses in neoplastic cells induces the antineoplastic effect [275, 276]. The inhibitors of autophagy include chloroquine (CO)and hydroxychloroquine (HCQ), which are being used in many active and recently completed clinical trials, especially in combination with other therapeutic

modalities such as radiotherapy (NCT01469455, NCT01575782, NCT02432417, NCT02378532, and NCT01727531). Others include 3-methyladenine (3-MA) and wortmannin for established tumors. Radiation-induced autophagy represents one of the radioprotective mechanisms in cancer cells, while inducing autophagy in RT can also increase cell death [277]. We also found that high-LET carbon ions could induce significant autophagy in tumor cells and CQ or 3-MA sensitized cancer cells to carbon ions, probably through inhibition of autophagic responses [278].

In the past decade, most studies indicated that metal-based NPs could be exploited as efficient activators for autophagy due to the cellular defense mechanism against NPs-induced stress [279]. On the other hand, very few studies reported that the metal-based NPs were capable of mediating the inhibitory effects for autophagy. Herein, a few general examples of relevant studies on metal-based *NanoEnhancers* are presented with regard to inhibition and induction of autophagy.

Liang's group reported that, similar to CQ alkalinization of lysosomal pH, AuNPs could block autophagy flux through size-dependent NPs uptake lvsosome impairment and resulting in autophagosome accumulation [280](Fig. 7). Later, using in vitro assays and tumor-bearing mice, Wen's group verified that inhibition of AgNPs-induced improved autophagy in cancer cells their antineoplastic effect [281]. Most interestingly, Gu's group recently described the important role of autophagy AgNPs-induced in the AgNPs' radiosensitization. Their studies implied that autophagy played a protective role in glioma cells treated with AgNPs, and inhibiting the protective autophagy led to the elevated levels of ROS and cell death (apoptosis)[282, 283]. These results have important implications for the application of metal-based NanoEnhancers in RT.

stress, originating ER from the endogenous/exogenous insults resulting in impaired protein folding, is considered another kind of cytoprotective pathway to re-establish ER homeostasis by the activation of unfolded protein response (UPR) [284]. If ER stress cannot be reversed, cellular functions often deteriorate, finally leading to cell death [285]. Therefore, targeting ER stress is considered a potential approach to cancer therapy [286, 287]. Furthermore, the links between ER stress and autophagy have been substantiated [288, 289], and our laboratory has also presented some related data in our recent publications [290, 291].



**Figure 7. AuNPs induce autophagosome accumulation through size-dependent nanoparticle uptake and lysosome impairment. (A)** Effect of AuNPs on lysosome pH (representative fluorescence pictures of NRK cells (normal rat kidney) treated with AuNPs, then stained with LysoSensor Green DND-189 for evaluation of lysosomal acidity). Scale bar = 50 µm. (B) Vacuoles induced by AuNP treatment are enlarged lysosomes (inset: close-up of the enlarged lysosomes). Scale bar = 10 µm. (C) DQ-BSA (derivative-quenched bovine serum albumin, a self-quenched lysosome degradation indicator) analysis of lysosomal proteolytic activity. Accumulation of fluorescence signal, generated from lysosomal proteolysis of DQ-BSA, was much lower in AuNP-treated cells. Scale bar = 10 µm. (D) Formation of CFP (cyan fluorescent protein)-LC3 (microtubule-associated protein 1 light chain 3) dots (pseudocolored as green) in CFP-LC3 NRK cells treated with AuNPs. Left, confocal image; right, bright-field image. Scale bar = 10 µm. (E) LC3 turnover assay. The differences in LC3-I and LC3-II levels were compared by immunoblot analysis of cell lysates. (F) Degradation of the autophagy-specific substrate/polyubiquitin-binding protein p62/SQSTM1 (sequestosome I) was detected by immunoblotting. Reproduced with permission from reference [280], copyright 2011 American Chemical Society.

It has been reported that metal-based NPs such as AuNPs, AgNPs, and zinc oxide (ZnO) NPs could induce ER stress [292-297]. Various studies focused on using ER stress as a biomarker for nanotoxicological evaluation. However, Inanami's group evaluated the radiosensitizing potential of PEGylated nanogel containing AuNPs (GNG)[298, 299]. Their results suggested that GNG, which accumulated in the cytoplasm, sensitized murine squamous cell carcinoma SCCVII cells and human non-small cell lung cancer A549 cells to X-rays through induction of apoptosis and inhibition of DSB repair partly as a consequence of GNG-mediated ER stress. Also, in human breast cancer MCF-7 and T-47D cells, AgNPs elicited apoptosis, probably resulting from the irreparable AgNPs-induced ER stress [300]. Specifically, AgNPs caused accumulation and aggregation of misfolded proteins leading to ER stress and activation of UPR. On the other hand, non-cancerous human mammary epithelial MCF-10A cells were less sensitive to AgNPs. Also, no remarkable changes in the ER stress signaling pathway were observed in human hepatocellular

carcinoma HepG2 cells following treatment with AgNPs [301].

Recently, Kunjachan et al. reported that vessel-targeted AuNPs were able to disrupt tumor vascular by damaging the neo-endothelium and thus improving therapeutic efficacy of chemoradiotherapy while diminishing the toxicity of radiation and NPs [302]. At the tissue level, this is an indirect and superior therapeutic modality. Also, the bystander effect could affect the radiosensitizing and synergistic effects of metal-based *NanoEnhancers* through communication between cells *via* signaling molecules [233, 303]. Of note is the fact that metal-based *NanoEnhancers* can react with thiols, for instance GSH, decreasing cellular defenses against oxidative stress and resulting in persistent damage [11].

As illustrated in **Fig. 2**, the biological mechanisms for radiosensitization and synergistic effects of metal-based *NanoEnhancers* promote cell death by a variety of mechanisms, such as apoptosis, necrosis, mitotic catastrophe, autophagy, and senescence. No single process appears to dominate, rather a combination of these biological pathways

appears to determine the fate of sensitized cells. Furthermore, metal-based NPs have been shown to also directly modulate cellular activity, function, and behavior [304]. Developing innovative techniques and strategies, such as quantitative proteomics based on high-resolution mass spectrometry and systems biology, would be useful in evaluating biological contributions of metal-based NanoEnhancers in RT [305, 306]. As an example, at the Emira laboratory of the SESAME (Synchrotron-light for Experimental Science and Application in the Middle East) synchrotron in Jordan, Yousef et al. investigated the cellular biochemical changes in F98 glioma rat cells employing the combination of X-rays and AGuIX NPs [97, 307]. They determined the in situ chemical structure of biomolecules inside cells using Fourier transform infrared (FTIR) microspectroscopy. In this study, notable spectral signature alterations in DNA, protein, and lipid regions were detected, which indicated changes in cellular function including elevated apoptosis.

Thus, in contrast to conventional chemical and biological agents used as radiosensitizers or for synergistic chemo-radiotherapy with specific biological targets, it is uncertain what the most critical target for the radiosensitizing and synergistic effects of (high Z) metal-based nanoparticles/*NanoEnhancers* would be, because the primary targets depend on cellular and subcellular distribution and location of metal-based *NanoEnhancers* [118].

# **Conclusions and future perspectives**

Metal-based nanoparticles can be employed to preferentially sensitize tumors to ionizing radiation due to the strong photoelectric absorption coefficient for high atomic number metallic elements and relative chemical inertness in cellular and subcellular systems. Compared to conventional chemical and biological agents such as those containing cisplatin, nitroimidazoles, and iodinated DNA targeting agents, metal-based "NanoEnhancers" are gaining credence as more ideal sensitizing agents [308, 309]. The radiosensitizing and synergistic effects of NanoEnhancers are because of a multitude of physical, chemical, and biological parameters, such as the types of elements, the quantity and dose of ionizing radiation, as well as their size, shape, structure, coating, functionalization, concentration, pO2, and metal-based localization. Thus, nanoparticles, especially multimetallic nanocomposites, have shown great promise for multifunctional theranostic applications in radiation oncology.

The physical dose enhancement by the metal-based *NanoEnhancers* has been well described. However, experimentally observed sensitizer

enhancement ratio (SER) and radiation dose enhancement factor (DEF) values for metal-based NanoEnhancers determined by colony forming assays or xenografts are significantly higher than those attributed to photoelectrons and Auger electrons predicted by Monte Carlo simulations. As indicated in Fig. 2, the amplification of radiation dose enhancement is likely mediated by spatio-temporally distributed ROS (mainly OH), which are produced in the early stages and can be evaluated by DCFH-DA (2',7'-dichlorofluorescein diacetate) in living cell models and 3-CCA (coumarin-3-carboxylic acid) in aqueous buffered solutions. The complex biological processes underlying the sensitizing and synergistic effects of metal-based NanoEnhancers in radiotherapy include oxidative stress, cell cycle arrest, DNA repair inhibition, autophagy, and ER stress. So far, the biological synergies between radiotherapy and metal-based NanoEnhancers have not been well-addressed [310]. In the future, elucidation of the role of biological contributions including modification of the tumor microenvironment, immune modulation [311], and cellular biochemical changes elicited only by NanoEnhancers [257] during the radiosensitization process would be helpful in better designing metal-based NanoEnhancers. Additionally, novel simulation methods based on more accurate models should be further developed to better calculate the physical dose enhancement by the metal-based NanoEnhancers [312]. Although the excited electrons play a major role in inducing the production of ROS by ionizing water and oxygen molecules [313], the nanoscale mechanisms underlying metal-based NanoEnhancers-induced ROS production remain poorly understood. In recent years, surface-catalyzed reactions, including IONs' Haber-Weiss cycle and Fenton reaction, have been considered important induction mechanisms of the ROS cascade in the radiosensitization process of metal-based nanoparticles.

As for translating metal-based nanoparticles-enhanced radiation therapy into clinical practice, many interdisciplinary and multidisciplinary investigations in both in vitro and in vivo systems have provided promising results. However, at present, only two types of metal-based NanoEnhancers, multifunctional theranostic gadolinium-based AGuIX NPs and hafnia NBTXR3 NPs, are being specifically investigated for cancer radiotherapy in clinical trials. Although it has passed phase 1 trials, CYT-6091 pegylated AuNPs incorporating tumor necrosis factor-a has not been clinically investigated in combination with RT.

As discussed above, development of metal-based *NanoEnhancers* for clinical RT, especially

multifunctional theranostic nanocomposites, is facing numerous challenges [227, 314, 315]: physical & chemical characterizations, drug metabolism and pharmacokinetic (DMPK) screening, tissue targeting capability, biocompatibility and stability concerns, and regulatory, manufacturing, and immunogenic issues. For instance, the strategies of passive targeting suffer from some critical defects like the variation in tumor vascularization, vessel porosity, and drug expulsion [25]. Additionally, to minimize potential health risks originating from nonspecific accumulation as well as long-term metabolic decomposition in the body, elimination of metal-based NanoEnhancers containing heavy or toxic metals from the body is a serious concern [234]. So far, the assessment of metal-based NanoEnhancer toxicity has been inadequate. Detailed studies of biocompatibility and toxicity of these NPs are a must before they can be used in clinical practice [316].

It is increasingly being recognized that the lack and systematic experimental of established approaches principal is another obstacle for application of metal-based NanoEnhancers in cancer radiotherapy [20]. Availability of accredited standards and methodologies for assessing the radiosensitizing and synergistic effects of metal-based NanoEnhancers of would enable direct comparison these investigations undertaken by various groups. Furthermore, the ability of metal-based NanoEnhancers to integrate current clinical principles of radiation oncology, such as administration route and frequency during the course of RT, would determine their acceptance by different stakeholders including physicians and patients [6].

Sometimes serendipity, but not luck, may play a role in anti-cancer drug discovery [317]. Serendipitous discovery also requires scientific intuition, experience, knowledge, and critical thinking. Furthermore, an approach combining various disciplines of physics, biology, chemistry, pharmacology, medicine, and engineering as needed is necessary to remove the barriers and accelerate the difficult translation of preclinical studies on metal-based NanoEnhancers into new therapeutic strategies that would improve the outcome of RT at the individual patient level. This review was intended to provide an overview of the field as well as identify the areas to focus effort on.We hope that the continued efforts of both researchers and physicians will help design, develop, and apply the metal-based NanoEnhancers in cancer radiotherapy and will have a positive impact on therapeutic strategies for cancer treatment.

# Abbreviations

3-CCA: coumarin-3-carboxylic acid; 3-MA:

3-methyladenine; 53BP1: p53-binding protein 1; AFM: atomic force microscopy; AgNPs: silver nanoparticles; AGuIX: Activation and Guidance of Irradiation by X-ray; AuNCs: gold nanoclusters; AuNPs: gold nanoparticles; Bax: Bcl-2-associated X protein; Bcl-2: B-cell lymphoma-2; BiNPs: bismuth nanoparticles; BRCA1: breast cancer 1; BSA: bovine serum albumin; C18PMH: poly(maleic anhydride-alt-1-octadecene); c-Abl: cellular Abelson; CAT: catalase; CDK: cyclin-dependent kinases; CF: conventional fractionation; CFP: cyan fluorescent protein; CLIONs: cross-linked dextran-coated IONs; CQ: chloroquine; CR: Čerenkov radiation; CT: computed tomography; cells: CTCs: circulating tumor DCFH-DA: 2',7'-dichlorofluorescein diacetate; DDR: DNA damage-response; DDS: drug delivery systems; DEF: radiation dose enhancement factor; DMPK: drug metabolism and pharmacokinetic; DMSO: dimethyl sulfoxide; DOTA: 1,4,7,10-tetraazacyclododecane-N,N',N"',N"'-tetraacetic acid; DOTAGA: 1,4,7,10tetraazacyclododecane-1-glutaric anhydride-4,7,10triacetic acid; DQ-BSA: derivative-guenched bovine serum albumin; DSBs: double-strand breaks; DTDTPA: dithiolated derivative of the diethylenetriaminepentacetic DTPA: acid: diethylenetriaminepentaacetic acid; DTX: docetaxel; EPR: enhanced permeability and retention; ER: endoplasmic reticulum; ESCC: esophageal squamous cell carcinoma; FTIR: Fourier transform infrared; Gd-DTPA: gadopentetic acid; Gd-NCT: gadolinium neutron-capture therapy; GdNPs: gadolinium-based nanoparticles; Gd-tex2+: Gd (III) texaphyrin; GeNPs: germanium nanoparticles; GNG: PEGylated nanogel containing AuNPs; GSH: glutathione; HCO: hydroxychloroquine; HEEpiC: human normal esophageal epithelial cells; Hf:HAp NPs: hafnium-doped hydroxyapatite nanoparticles; HR: homologous recombination; ICP-MS: inductively coupled plasma-mass spectrometry; IGRT: image-guided radiotherapy; IMRT: intensity-modulated radiotherapy; IONs: iron oxide nanoparticles; LC3: microtubule-associated protein 1 light chain 3; LDH: lactate dehydrogenase; LET: linear energy transfer; MGd: motexafin gadolinium; MLCs: multileaf collimators; MPS: mononuclear phagocyte system; MRI: magnetic resonance imaging; MRT: microbeam radiation therapy; mtDNA: mitochondrial DNA; MUA: mercaptoundecanoic acid; NAC: *N*-acetyl cysteine; NCT: neutron capture therapy; NHEJ: nonhomologous end-joining; NHS: N-hydroxysuccinimide; NMOFs: nanoscale metal organic frameworks; NPs: nanoparticles; NSF: nephrogenic systemic fibrosis; NTCP: normal tissue complication probability; OARs: organs at risk; PA: photoacoustic; PAA: polyacrylic acid; PAT-Plat: photoactivation of *cis*-platinum: PCL: polycaprolactone; PDI: protein disulphide isomerase; PDT: photodynamic therapy; PEG: polyethylene glycol; pO<sub>2</sub>: oxygen partial pressure; PSO: polysilsesquinoxane; PT: proton therapy; Pt-nc: nanocolloid; PtNPs: platinum platinum-based nanoparticles; PTT: photothermal therapy; PtTC: chloroterpyridine platinum; PTX: paclitaxel; QDs: quantum dots; ROS: reactive oxygen species; RT: radiation therapy; SER: sensitizer enhancement ratio; SESAME: Synchrotron-light for Experimental Science and Application in the Middle East; SOD: superoxide dismutase; SPIONs: superparamagnetic iron oxide nanoparticles; SQSTM1: sequestosome 1; SRCT: synchrotron radiation computed tomography; SRP: small rigid platforms; SSBs: single-strand breaks; Ta<sub>2</sub>O<sub>5</sub> NSPs: tantalum pentoxide nanoceramics/ceramic nanostructured particles; TCP: control probability; tumor TCPP: tetrakis (4-carboxyphenyl) porphyrin; TEM: transmission electron microscopy; TiONts: titanate nanotubes; TNBC: triple-negative breast cancer; TNF: tumor necrosis factor-a; TPZs: thioctyl tirapazamine; UCNPs: upconversion nanoparticles; UPR: unfolded protein response.

#### Acknowledgements

This publication was jointly supported by the National Key Research and Development Program of the Ministry of Science and Technology of China (Grant No. 2016YFC0904600, Ministry of Science and Technology of China), the National Key Technology Support Program of the Ministry of Science and Technology of China (Grant No. 2015BAI01B11, Ministry of Science and Technology of China), the NSFC-CAS Joint Fund for Research Based on Large-scaled Scientific Facilities (Grant No. U1532264, National Natural Science Foundation of China), and CAS "Light of West China" Program (Grant to Yan Liu, Chinese Academy of Sciences). The authors acknowledge Dr. Iqbal U. Ali for proof reading.

## **Competing Interests**

The authors have declared that no competing interest exists.

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