REVIEW



Radiomics in liver diseases: Current progress and future opportunities

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Abstract

Liver diseases, a wide spectrum of pathologies from inflammation to neoplasm, have become an increasingly significant health problem worldwide. Noninvasive imaging plays a critical role in the clinical workflow of liver diseases, but conventional imaging assessment may provide limited information. Accurate detection, characterization and monitoring remain challenging. With progress in quantitative imaging analysis techniques, radiomics emerged as an efficient tool that shows promise to aid in personalized diagnosis and treatment decision-making. Radiomics could reflect the heterogeneity of liver lesions via extracting high-throughput and high-dimensional features from multi-modality imaging. Machine learning algorithms are then used to construct clinical target-oriented imaging biomarkers to assist disease management. Here, we review the methodological process in liver disease radiomics studies in a stepwise fashion from data acquisition and curation, region of interest segmentation, liver-specific feature extraction, to task-oriented modelling. Furthermore, the applications of radiomics in liver diseases are outlined in aspects of diagnosis and staging, evaluation of liver tumour biological behaviours, and prognosis according to different disease type. Finally, we discuss the current limitations of radiomics in liver disease studies and explore its future opportunities.

Abbreviations: AFP, α-fetoprotein; ALB, serum albumin; ALT, serum alanine aminotransferase; AST, aspartate aminotransferase; AUC, area under the curve; CA 19-9, carbohydrate antigen 19-9; CB, conjugated bilirubin; CNN, convolution neural network; CT, computed tomography; DL, deep learning; HBsAg, hepatitis B virus surface antigen; HCC, hepatocellular carcinoma; ICC, intrahepatic cholangiocarcinoma; MRI, magnetic resonance imaging; NASH, nonalcoholic steatohepatitis; PD-1, anti-programmed cell death protein; PD-L1, anti-programmed cell death ligand 1; PIVKA-II, prothrombin induced by vitamin K absence-II; PLT, platelet count; PT, prothrombin time; ROI, region of interest; SWE, shear wave elastography; TACE, transcatheter arterial chemoembolization; TB, Serum total bilirubin.

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KEYWORDS

data science, liver diseases, machine learning, precision medicine, radiologic technology

1 | INTRODUCTION

Liver diseases, a wide spectrum of pathologies from inflammation to neoplasm, have become a major health problem worldwide. Noninvasive imaging plays a critical role in the characterization and monitoring of liver diseases. Conventional ultrasound, computed tomography (CT) and magnetic resonance imaging (MRI) are widely used for qualitative evaluation of liver morphology and blood supply.¹⁻³ Tremendous progress is still being made in liver imaging with introduction of advanced techniques, including metabolic imaging, molecular imaging, and multi-parametric functional MRI, etc, allowing improved evaluation of liver diseases and assisting personalized medical decision making.⁴⁻⁶

With accumulation of scalable liver imaging data, radiomics emerges as a novel radiological technique that comprehensively utilizes large-scale medical imaging into the process of liver disease management via artificial intelligence techniques.^{7,8} It enables extraction of high-throughput quantitative imaging features beyond inspections of naked human eyes and converting encrypted medical imaging into minable numerical data.⁸ Combined with clinical, pathological, or genetic information, radiomics would assist in lesion characterization, preoperative diagnosis, treatment efficacy evaluation, as well as prognosis prediction in various clinical settings.⁹⁻¹¹

Quantitative imaging traits were proved to be associated with global gene expression programmes, and could reconstruct 78% of the global gene expression profiles in liver cancer.¹² This groundbreaking result laid a foundation and greatly encouraged researchers to explore the potential of quantitative imaging tool in preoperative genetic/pathological outcome prediction. Hence, a great deal of radiomics studies have been conducted using multi-parametric and multi-modality imaging in terms of liver disease diagnosis and treatment decision making.¹³⁻⁴⁸ In certain scenarios, this artificial intelligence-based technique could even compete pathological gold standard, providing new ways for unsolved clinical problems in the paradigm of liver disease management.¹⁶ Nevertheless, it still requires further multi-centre and prospective validation for the validity of radiomics. The interpretability and the correlation with biological/pathological underpinnings also represent substantial obstacles for the translation of artificial intelligence into real clinical practice.

Here, we review the basic concepts of radiomics methodologies specific for liver studies from data acquisition, liver/lesion segmentation, feature design, to model construction (Figure 1). Meanwhile, representative clinical applications of radiomics in liver diseases regarding diagnosis, staging, evaluation of liver tumour biological behaviours, and prognosis are also within the scope of this study. Finally, we summarize the current challenges and limitation of radiomics, and explore its future directions in liver diseases.

Key points

- Radiomics as an emerging technique based on medical imaging analysis is more commonly used in liver disease studies.
- Inter-personal heterogeneity could be revealed via extracting high-dimensional quantitative imaging features and analysed by artificial intelligence algorithms.
- Radiomics can be applied in the diagnosis, treatment effect evaluation and prognosis prediction in liver diseases.

2 | METHODOLOGY OF RADIOMICS IN LIVER DISEASES

2.1 | Data acquisition and curation

Data used in radiomics studies can be single-centre or multi-centre, and retrospective or prospective. Here, we searched PubMed (8 October 2019) for radiomics studies on liver diseases using terms (liver diseases AND radiomics), and found 36 clinical target-oriented published work.¹³⁻⁴⁸ Most (33 out of 36) studies were performed on single-centre with retrospective cohort, while only two studies were performed on multi-centre and prospective cohort (Table 1). And the most commonly used imaging modality was CT (18 studies), followed by MRI (12 studies), positron emission tomography (PET) (two studies) and ultrasonography (US) (four studies) (Table 1).

Considering the effect of inconsistent imaging acquisition protocol and reconstruction procedure in multi-centres via multi brand manufactories, preprocessing of the collected imaging data is required. Currently, the most commonly used methods conclude resampling and intensity normalization. Image resampling is used to improve image quality and eliminate bias introduced by non-uniform imaging resolution.^{49,50} Image intensity normalization is utilized to correct inter-subject intensity variation by transforming all images from original greyscale into a standard greyscale.^{51,52} Park et al normalized liver signal intensity according to the spleen signal on hepatobiliary phase (HBP) images to extract high-order textural features and revealed the improved diagnostic value as compared with non-normalized data.²⁹

In addition to imaging data, clinical factors were also involved in radiomics analysis, including patient age, gender, Child-Pugh stage, histologic grading, BCLC stage, cirrhosis and its cause, etc.¹³⁻⁴⁸ Laboratory examination indexes comprise serum α -fetoprotein (AFP) level, prothrombin induced by vitamin K absence-II (PIVKA-II) level, carbohydrate



FIGURE 1 Workflow of radiomics methodological process

antigen 19-9 (CA 19-9) level, hepatitis B virus surface antigen (HBsAg), serum alanine aminotransferase (ALT), aspartate aminotransferase (AST), serum total bilirubin (TB), conjugated bilirubin (CB), serum albumin (ALB), prothrombin time (PT), platelet count (PLT), etc.¹³⁻⁴⁸

2.2 | Region of interest segmentation

Segmentation of region of interest (ROI) could be divided into manual segmentation and semiautomatic/automatic segmentation. Most radiomics studies on liver disease applied manual segmentation. Only six studies performed semiautomatic/automatic segmentation.^{17,30,39,46,53,54}

Manual segmentation is performed by radiologists to annotate the location and precise boundary of the lesion. Another way of manual segmentation is realized by placing a rectangular/circle box via deep learning analysis. Wang et al conducted a squared ROI segmentation as the input of convolution neural network (CNN) and achieved satisfying performance in liver fibrosis stage prediction.¹⁶ Naganawa et al applied similar segmentation approach with a 2-cm diameter circular ROI covering the lesion while excluding intrahepatic vessels.¹⁵ Considering the discrepancy of subjective judgement in manual segmentation, segmentations by multi-clinicians, of multi-time point, and using computer perturbation are required to decrease the intra- and inter-reader variability.³² Feature reproducibility and robustness are generally evaluated through calculation of intra-class correlation coefficient and concordance correlation coefficient.^{36,56,57}

Automatic segmentation aims to annotate ROIs by computer automatically, whereas semiautomatic segmentation still needs

partial manual intervention to mark the centre of the lesion before automatic segmentation. Several classic segmentation algorithms showed good performance in liver lesion annotation.⁵⁸⁻⁶¹ These methods can be generally divided into three categories: (a) algorithms based on intensity thresholds and region (global thresholding, local thresholding, region growing, and region splitting and merging methods), (b) algorithms based on statistical approach (statistical parametric mapping and maximization segmentation algorithm), clustering (k-means clustering and fuzzy clustering) and deformable model approach (Snake model and geometric active contour model), (c) algorithms incorporating empirical knowledge into the segmentation process (Atlas Guided Approach and Artificial Neural Network).

2.3 | Feature extraction

Radiomic features are divided into manual engineered features and deep learning (DL) features. Manual engineered features include shape/histogram/texture-based features. Shape-based features describe the geometric attributes of the ROIs. Histogram features capture the first-order statistic characteristics of liver parenchyma or liver lesion. Textural features, extracted from a series of high-order textural matrixes, describe the granular textural pattern of the ROIs. In addition, filtered features are extracted from ROI preprocessed by wavelet, Laplacian and Gaussian filters from multiple dimensions.⁶² Commonly used manual engineered features are shown in Table 2. Another type of engineered features is defined as empirical features or semantic features that are designed by experience and knowledge of radiologists. Fu et al designed "peer-off" features with hypothesis that

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Reference	Zhou et al ¹³	Cozzi et al ¹⁴	Naganawa et al ¹⁵	Wang et al 16	ŗ	Peng et al ¹⁷	Peng et al ¹⁷ Reimer et al ¹⁸	Peng et al ¹⁷ Reimer et al ¹⁸ Akai et al ¹⁹	Peng et al ¹⁷ Reimer et al ¹⁸ Akai et al ¹⁹ Li et al ²⁰	Peng et al ¹⁷ Reimer et al ¹⁸ Akai et al ¹⁹ Li et al ²⁰ Hui et al ²¹	Peng et al ¹⁷ Reimer et al ¹⁸ Akai et al ¹⁹ Li et al ²⁰ Hui et al ²¹ Kim et al ²²	Peng et al ¹⁷ Reimer et al ¹⁸ Akai et al ¹⁹ Li et al ²⁰ Hui et al ²¹ Kim et al ²² Liu et al ²³	Peng et $al^{1/}$ Reimer et $al^{1/9}$ Akai et $al^{1/9}$ Li et al^{20} Liu et al^{22} Liu et al^{23} Wu et al^{24}	Peng et $al^{1/}$ Reimer et $al^{1/9}$ Akai et $al^{1/9}$ Li et al^{21} Kim et al^{21} Liu et al^{22} Uu et al^{23} Wu et al^{24} Yao et al^{25}	Peng et $al^{1/}$ Reimer et al^{19} Akai et al^{19} Li et al^{20} Hui et al^{21} Li u et al^{22} Wu et al^{24} Yao et al^{26} Hu et al^{26}	Peng et $al^{1'}$ Reimer et al^{18} Akai et al^{19} Li et al^{20} Hui et al^{21} Kim et al^{22} Li u et al^{23} Wu et al^{24} Yao et al^{25} Hu et al^{26}	Peng et $al^{1/}$ Reimer et $al^{1/8}$ Akai et $al^{1/9}$ Li et al^{20} Hui et al^{21} Kim et al^{22} Liu et al^{23} Wu et al^{24} Yao et al^{24} Hu et al^{26} Hu et al^{26} Sheng et al^{28}	Peng et $al^{1'}$ Reimer et al^{19} Akai et al^{19} Li et al^{20} Hui et al^{21} Kim et al^{22} Li u et al^{23} Wu et al^{24} Yao et al^{26} Hu et al^{26} Klaassen et al^{27} Sheng et al^{28} Park et al^{29}	Peng et al ¹⁷ Reimer et al ¹⁹ Akai et al ¹⁹ Li et al ²⁰ Hui et al ²¹ Kim et al ²² Liu et al ²³ Yao et al ²⁵ Hu et al ²⁶ Klaassen et al ²⁶ Rlaassen et al ²⁶ Park et al ²⁸ Park et al ²⁹	Peng et $al^{1'}$ Reimer et al^{18} Akai et al^{19} Li et al^{20} Hu i et al^{21} Kim et al^{21} Liu et al^{23} Wu et al^{24} Yao et al^{24} Yao et al^{26} Hu et al^{26} Hu et al^{26} Rlaassen et al^{28} Park et al^{29} Park et al^{29} Chen et al^{30}
Number	Ţ	2	с	4	5		Ŷ	6	8 J Ç	9 8 4 6	6 9 8 10	6 8 110 11	6 8 11 12 12	6 9 11 12 13	6 8 11 12 13 13	6 9 11 12 13 15	6 8 11 12 13 14 15 15	6 8 11 11 13 13 15 15 17 17	6 8 8 11 12 13 13 15 15 15 17 17 17	6 8 8 110 112 113 113 115 115 115 117 117 117 118

TABLE 1 Summary of published radiomics studies on liver diseases

(Continues)

	ence in HCC	ctomy Liver	ılar carcinoma na	lar invasion	orectal Liver	ence in HCC	ence in HCC	ence in arcinoma	in hcc after liver	sure and patient n	cological	lar invasion	iltrating CD8 + T	:ype HCC	م مد میشما
linical Characteristics	rediction of early recur	rediction of Posthepate Failure in HCC	rediction of hepatocellı and hepatic haemangio	rediction of microvascu	rognostic model for col Metastasis	rediction of early recur	rediction of early recur	rediction of early recur intrahepatic cholangioc	rediction of recurrence transplantation	rediction of portal pres outcome in hypertensic	rediction of immune-or characteristics	rediction of microvascu	valuation of Tumour-Inf Cells	iagnosis of dual-pheno	nnroved nrognosticatio
Imaging Modality C	CT P	CT P	AR	CT	PET P	CT	MR	MR	CT	CT	MRI	CT P	PET E	MRI	CT Ir
Statistical analysis (feature selection and modelling)	LASSO	LASSO, Logistic	Variance threshold, LASSO, Decision tree, Random forest, K nearest neighbors, Logistic	Multivariable logistic regression	Univariate and multivariate	MRMR, LASSO, Cox	LASSO	Wilcoxon signed-rank test, Logistic	Lasso	LASSO	Binary logistic regression analysis	LASSO + BPNet	linear elastic-net model	LASSO	Multivariate cox propotional
No. and type of radiomic features	1044 (histogram, wavelet, texture)	713 (intensity, texture, wavelet, shape and size)	1029 (first-order, shape, texture, high-order)	7260 radiomic features	41 (histogram)	647 (intensity, texture, wavelet, shape and size)	385 (histogram, texture)	396 (histogram, texture, Haralick, morphological)	853 radiomic features	1474 radiomic features	218 radiomic features	1044 textural features	57 radiomic features	First order statistical, shape, textural, and higher order statistical features	114 radiomic features
No. of patients	156	125	369	495	52	184	155	47	133	169	48	206	142	100	102
Study design (retrospective/ prospective, single or multi- centre study)	Retrospective, single-centre study	Retrospective, single-centre study	Retrospective, single-centre study	Retrospective, single-centre study	Retrospective, single-centre study	Retrospective, single-centre study	Retrospective, single-centre study	Retrospective, single-centre study	Retrospective, single-centre study	Retrospective, single-centre study	Retrospective, single-centre study	Retrospective, single-centre study	Retrospective, single-centre study	Retrospective, single-centre study	Retrospective: single-centre study
Reference	Shan et al ³³	Cai et al ³⁴	Wu et al ³⁵	Xu et al ³⁶	Rahmim et al ³⁷	Yuan et al ³⁸	Zhang et al ³⁹	Zhao et al ⁴⁰	Guo et al ⁴¹	Tseng et al ⁴²	Hectors et al ⁴³	Ni et al ⁴⁴	Liao et al ⁴⁵	Huang et al ⁴⁶	Shur et al ⁴⁷
Number	21	22	23	24	25	26	27	28	29	30	31	32	33	34	35

TABLE 1 (Continued)

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tumour grows from inside to outside.⁶³ By splitting the tumour into 10 peel-off layers and extracting corresponding statistical features and its ratio, it can reflect tumour growth pattern and spatial heterogeneity. They found the feature - POF_entropy showed satisfactory value for predicting the progress-free survival following liver resection and transarterial chemoembolization. This feature exactly represented the texture randomness or irregularity of the innermost layer.

Compared with manual engineered features, DL network could extract supplementary high-dimensional features that are hard to depict by observers.^{55,64-66} The DL network encodes medical image into shape information and abstract textural information via shallow and deep layers respectively. Wang et al proposed a novel method to automatically extract DL features from MR imaging using CNN.⁶⁴ They found that DL features outperformed textural features in predicting the malignancy of HCC. Chaudhary et al used unsupervised auto-encoder framework to extract DL features.⁶⁶ Features extracted from the bottleneck layer showed predictive ability for the survival risk of liver cancer.

2.4 | Task-oriented modelling

Generally, the methods for feature selection conclude filter-based, wrapper-based, and model-embedded methods.⁶⁷ Filter-based methods produce a selected feature set according to the correlation between features and the classifying labels. Commonly used filterbased methods include calculation of mutual information, correlation coefficient and uni-variable analysis (ie Mann-Whitney U test and Chi-squared test), etc.⁶⁸⁻⁷⁰ Wrapper-based methods take into account the weighing of feature subsets, and are combined with an appointed classifier. It selects features that could improve the accuracy of the prediction to the maximum extend and removes the features that contribute less to the prediction until the specified feature number is reached. Model-embedded methods perform feature selection in the process of model construction. An example of this method is the least absolute shrinkage and selection operator (LASSO) algorithm.⁷¹ LASSO aims to minimize the residual sum of squares, subjected to the sum of the absolute value of the coefficients being less than a tuning parameter. It forces specified coefficients to zero and thus effectively produce a simpler model. Among the aforementioned methods, filter-based methods require less computation time than the other two methods but with lower prediction accuracy. Thus, they are most commonly used as a primary selection method to initially reduce features.^{23,55}

Regarding modelling strategy, radiomics studies on liver disease mostly utilized supervised learning modelling. LASSO logistic regressing modelling was commonly used, demonstrating satisfying performance particularly in small sample size based studies.^{22,31,72} Support vector machine and random forest were also used in published liver disease radiomics studies.^{19,23,27,32} Notably, Li et al compared six types of machine-learning algorithms in predicting liver fibrosis, including adaptive boosting, decision tree, logistic regression, neural network, random forest and support vector machine.²⁰ Their result indicated that adaptive boosting, random forest and support vector machine stood out as superior modelling methods with improved accuracy for fibrosis prediction.

3 | RADIOMICS IN THE DIAGNOSIS AND STAGING OF LIVER DISEASES

For clinical application, radiomics plays a pivotal role in the diagnosis, staging and grading of several liver diseases, of which most efforts focused on hepatic malignancies and liver diffuse diseases (Figure 2).

3.1 | Hepatic malignancies

Hepatocellular carcinoma (HCC) is currently the most common primary liver cancer.⁷³ However, many non-HCC malignancies (eg small duct type intrahepatic cholangiocarcinoma [ICC] and combined hepatocellular-cholangiocarcinoma) and other atypical benign focal liver lesions (eg haemangioma and hepatic adenoma) can mimic HCC, making the diagnosis challenging via current imaging techniques.^{74,75}

Radiomics demonstrated great potential in differentiating focal liver lesions.^{25,76,77} Li et al primarily investigated texture features of focal hepatic lesions on spectral attenuated inversion-recovery T2 weighted MRI, and found that the radiomics signatures can help classify hepatic haemangioma, hepatic metastases and HCC with satisfying diagnostic performances (area under the curve [AUC]: 0.83-0.91).⁷⁶ Trivizakis et al reported that the three-dimensional convolutional neural network features on diffusion-weighted MR images achieved an accuracy of 83% for discriminating primary and metastatic liver tumours.⁷⁷ In addition to MR imaging, radiomics analysis on multi-modal ultrasound images also demonstrated diagnostic ability for benign and malignant focal liver lesion classification (AUC: 0.94, 95%CI: 0.88-0.98) and malignant subtyping (AUC: 0.97, 95%CI: 0.93-0.99).²⁵

3.2 | Liver diffuse diseases

Besides hepatic malignancies, radiomics also showed potential in characterization of liver diffuse diseases including fatty liver diseases and liver fibrosis. The first study evaluating the performance of CT-based texture features for predicting nonalcoholic steatohepatitis (NASH) was conducted by Naganawa et al, which included 88 retrospective suspected NASH patients.¹⁵ They reported that the AUC reached up to 0.94 in patients without suspected fibrosis, but dropped significantly in patients with suspicion of fibrosis (AUC: 0.60). Tang et al further explored the relationship between a quantitative ultrasound-based machine learning model and histopathology scoring in a rat model.⁷⁸ Their results demonstrated that combining quantitative ultrasound parameters with conventional shear wave elastography significantly improved the classification accuracy of steatohepatitis, liver steatosis, inflammation and fibrosis.

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Other than fatty liver diseases, more studies focused on liver fibrosis staging and associated complications. A prospective multi-centre study by Wang et al revealed that DL radiomics of shear wave elastography (SWE) significantly improved the accuracy of liver fibrosis staging, with AUCs of 0.97, 0.98 and 0.85 for cirrhosis (F4), advanced fibrosis (\geq F3) and significant fibrosis (\geq F2) respectively.¹⁶ Similar results have been reported by another prospective study, in which the machine-learning-based multi-parametric ultrasomics model achieved remarkably improved power for significant fibrosis (\geq F2).²⁰

CT-based radiomics was also utilized for noninvasive assessment of liver fibrosis. Choi et al retrospectively developed a DL system on portal venous phase CT images in 7461 patients and validated it in an independent data sets comprising 891 patients.⁷⁹ The accuracy was of 79.4% in the validation sets, with AUC of 0.96, 0.97 and 0.95 for \geq F2, \geq F3 and F4 respectively. Regarding portal hypertension, Liu et al reported in their multi-centre prospective study that the radiomics signature on portal venous phase CT images accurately detected portal hypertension with the C-index of 0.889, 0.800, 0.917 and 0.827 in four external validation cohorts respectively.²³

4 | RADIOMICS IN THE EVALUATION OF LIVER TUMOUR BIOLOGICAL BEHAVIOURS AND PROGNOSIS

Beyond diagnosis and staging, radiomics enables quantitative assessment of liver tumour biological behaviours, as well as prediction of prognosis and antitumoral treatment effect (Figure 2).

4.1 | HCC

4.1.1 | Measurement of tumour differentiation and proliferation

Histologic grade was one of the most important risk factors for postoperative recurrence in HCC.⁸⁰⁻⁸³ Recently, two MRI-based studies investigated radiomic features for HCC aggressiveness characterization, demonstrating the potential of radiomics as indicative biomarkers for HCC grade.^{24,84} Regarding Ki-67 level, Ye et al reported that radiomics analysis can evaluate the tumour Ki-67 level preoperatively with good accuracy (C-index: 0.936) in a prospective study.⁸⁵

4.1.2 | Assessment of tumour vascular invasion

Preoperative discrimination between neoplastic and bland portal vein thrombosis and detection of microvascular invasion in HCC is critically important.^{86,87} Canellas et al explored the role of CT texture features for differentiating neoplastic and bland portal vein thrombosis. They found that mean value of positive pixels and

entropy can characterize portal vein thrombosis.⁸⁸ Recent studies have shown promising results of CT and ultrasound-based radiomics signatures for preoperative microvascular invasion prediction, all with high diagnostic accuracy.^{17,89}

4.1.3 | Prediction of treatment efficacy and prognosis

Radiomics analysis permits accurate prediction of prognosis and effective diverse therapy evaluation.^{73,90} Several studies were conducted for hepatic resection evaluation, and one study was for liver transplantation evaluation.^{13,19,21,28,91-93} Furthermore, Li et al found that texture analysis of CT images can be helpful not only in prognosis prediction, but also in treatment selection between liver resection and transcatheter arterial chemoembolization (TACE).⁸¹ For HCC patients with prominent vascular invasion and/or extrahepatic spread (BCLC stage C), systematic treatment is the standard of care recommended by current guidelines from different geographical regions.^{36,90} Mulé et al retrospectively investigated 92 advanced HCC patients from two centres and reported that the contrast-enhanced CT texture feature entropy was correlated with tumour heterogeneity by manual visualization, and entropy on portal venous phase images was an independent predictor for OS.⁹⁴

Radiomics analysis also yielded promising results in predicting response for patients treated with immunotherapies. Sun et al retrospectively generated a contrast-enhanced CT-based radiomics signature of tumour-infiltrating CD8 cells and investigated its performances in predicting tumour immune phenotype (immune-inflamed vs immune-desert) and response to anti-programmed cell death protein (PD)-1 or anti-programmed cell death ligand 1 (PD-L1) monotherapies.⁹⁵ Another study by Chen et al explored the capacity of radiomics analysis on gadoxetic acid-enhanced MR imaging in predicting immunoscore, a new prognostic biomarker for immunotherapy revealing tumour infiltrating lymphocytes density.⁹⁶

4.2 | ICC

ICC is an aggressive primary hepatic cancer arising from the bile duct epithelium.⁹⁷ However, unlike HCC, surgical resection is currently the only curative treatment for ICC patients.⁹⁸ A recent single-centre retrospective study reported that the radiomics signature on preoperative arterial-phase contrast-enhanced MR images can be used to predict early recurrence of ICC after partial hepatectomy with the AUC of 0.82 and 0.77 in the training and validation cohort respectively.⁵⁵ Ji et al constructed a radiomics signature from portal venous CT to predict lymph node metastasis in biliary tract caners.⁹⁹ They found good discrimination of the signature in both training (AUC: 0.81) and validation cohort (AUC: 0.80).⁹⁹

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	Gray Level Dependence Matrix (GLDM) Features (n = 14)	Small Dependence Emphasis (SDE)	Large Dependence Emphasis (LDE)	Gray Level Non- Uniformity (GLN)	Dependence Non- Uniformity (DN)	Dependence Non- Uniformity Normalized (DNN)	Gray Level Variance (GLV)	Dependence Variance (DV)	Dependence Entropy (DE)	Low Gray Level Emphasis (LGLE)	High Gray Level Emphasis (HGLE)	Small Dependence Low Gray Level Emphasis (SDLGLE)	Small Dependence High Gray Level Emphasis (SDHGLE)	(Continues)
	Neighbouring Gray Tone Difference Matrix (NGTDM) Features (n = 5)	Coarseness	Contrast	Busyness	Complexity	Strength								
	Gray Level Size Zone Matrix (GLSZM) Features (n = 16)	Small Area Emphasis (SAE)	Large Area Emphasis (LAE)	Gray Level Non- Uniformity (GLN)	Gray Level Non- Uniformity Normalized (GLNN)	Size-Zone Non- Uniformity (SZN)	Size-Zone Non- Uniformity Normalized (SZNN)	Zone Percentage (ZP)	Gray Level Variance (GLV)	Zone Variance (ZV)	Zone Entropy (ZE)	Low Gray Level Zone Emphasis (LGLZE)	High Gray Level Zone Emphasis (HGLZE)	
	Gray Level Run Length Matrix (GLRLM) Features (n = 16)	Short Run Emphasis (SRE)	Long Run Emphasis (LRE)	Gray Level Non-Uniformity (GLN)	Gray Level Non-Uniformity Normalized (GLNN)	Run Length Non- Uniformity (RLN)	Run Length Non- Uniformity Normalized (RLNN)	Run Percentage (RP)	Gray Level Variance (GLV)	Run Variance (RV)	Run Entropy (RE)	Low Gray Level Run Emphasis (LGLRE)	High Gray Level Run Emphasis (HGLRE)	
Textural features (n = 75)	Gray Level Co-occurrence Matrix (GLCM) Features (n = 24)	Autocorrelation	Joint Average	Cluster Prominence	Cluster Shade	Cluster Tendency	Contrast	Correlation	Difference Average	Difference Entropy	Difference Variance	Joint Energy	Joint Entropy	
	Histogram features (n = 19)	Energy	Total Energy	Entropy	Minimum	10th percentile	90th percentile	Maximum	Mean	Median	Interquartile Range	Range	Mean Absolute Deviation (MAD)	
	Shape-based 2D features (n = 16)	Mesh Surface	Pixel Surface	Perimeter	Perimeter to Surface ratio	Sphericity	Spherical Disproportion	Maximum 2D diameter	Major Axis Length	Minor Axis Length	Elongation			
	Shape-based 3D features (n = 16)	Mesh Volume	Voxel Volume	Surface Area	Surface Area to Volume ratio	Sphericity	Compactness	Spherical Disproportion	Maximum 3D diameter	Maximum 2D diameter (Slice)	Maximum 2D diameter (Column)	Maximum 2D diameter (Row)	Major Axis Length	
		1	2	с	4	2	9	7	∞	6	10	11	12	

TABLE 2 Radiomic features used in radiomics studies on liver diseases

<u> </u>	WILEY-LIVE	IONAL											
	Gray Level Dependence Matrix (GLDM) Features (n = 14)	Large Dependence Low Gray Level Emphasis (LDLGLE)	Large Dependence High Gray Level Emphasis (LDHGLE)										
	Neighbouring Gray Tone Difference Matrix (NGTDM) Features (n = 5)												63
	Gray Level Size Zone Matrix (GLSZM) Features (n = 16)	Small Area Low Gray Level Emphasis (SALGLE)	Small Area High Gray Level Emphasis (SAHGLE)	Large Area Low Gray Level Emphasis (LALGLE)	Large Area High Gray Level Emphasis (LAHGLE)								-
	Gray Level Run Length Matrix (GLRLM) Features (n = 16)	Short Run Low Gray Level Emphasis (SRLGLE)	Short Run High Gray Level Emphasis (SRHGLE)	Long Run Low Gray Level Emphasis (LRLGLE)	Long Run High Gray Level Emphasis (LRHGLE)								
Textural features (n = 75)	Gray Level Co-occurrence Matrix (GLCM) Features (n = 24)	Informational Measure of Correlation (IMC) 1	Informational Measure of Correlation (IMC) 2	Inverse Difference Moment (IDM)	Maximal Correlation Coefficient (MCC)	Inverse Difference Moment Normalized (IDMN)	Inverse Difference (ID)	Inverse Difference Normalized (IDN)	Inverse Variance	Maximum Probability	Sum Average	Sum Entropy	Sum of Squares
	Histogram features (n = 19)	Robust Mean Absolute Deviation (rMAD)	Root Mean Squared (RMS)	Standard Deviation	Skewness	Kurtosis	Variance	Uniformity					
	Shape-based 2D features (n = 16)												
	Shape-based 3D features (n = 16)	Minor Axis Length	Least Axis Length	Elongation	Flatness								
		13	14	15	16	17	18	19	20	21	22	23	24

Filtered features extracted from images preprocessed by wavelet filter, Laplacian of Gaussian filter, etc, including the shape/histogram/texture-based radiomic features.

TABLE 2 (Continued)





Metastatic hepatic malignancies 4.3

In addition to primary liver cancers, radiomics also showed promise in the evaluation of several metastatic hepatic malignancies. Lubner et al found that pretreatment portal venous phase CT texture features of the colorectal liver metastases were significantly associated with tumour grade, KRAS mutation and OS.¹⁰⁰ Another retrospective study investigated the ratio between the texture of colorectal liver metastases and the surrounding liver, and found that it may reflect tumour aggressiveness, chemotherapy response and OS.¹⁰¹ However, Lee et al reported that texture features from liver parenchyma on portal venous phase CT cannot be used to

predict the development of hepatic metastasis in colorectal cancer patients.¹⁰² Apart from colorectal cancer, emerging evidence suggests that the CT-based radiomics signature of esophagogastric liver metastases can help predict treatment response to chemotherapy.²⁷

5 | FUTURE CHALLENGES AND **OPPORTUNITIES**

Current published studies revealed the potential of radiomics analysis in liver disease diagnosis, tumour biological property profiling, and prognosis estimation. However, although MR imaging can provide the multi-parametric information regarding hepatic function and microenvironment with higher tissue resolution, most studies to date have focused on radiomics analyses of CT.¹⁰³⁻¹⁰⁶ In addition, a large number of studies were retrospective in design and lack independent external validation across different geographical areas and races, which may limit the generalizability and applicability of the current findings. Different prevalence of disease may also influence the accuracy of the algorithm (*eg* positive and negative predictive values). Moreover radiomics results are extremely sensitive to the various technical acquisition parameters, especially among different vendors. Therefore, more large scale multi-centre prospective studies with standardized acquisition, segmentation and imaging postprocessing are needed to ensure further development of radiomics in liver diseases.

6 | CONCLUSIONS

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Radiomics as a newly emerged quantitative technique is burgeoning in liver disease management with consistently developing methodology. Previous studies, although mainly retrospective in design and based on single imaging modality, have revealed its potential in diagnosis, treatment evaluation and prognosis prediction of several liver diseases. Nevertheless, further multi-centre and prospective validation is still needed to valid its clinical usefulness, especially in prognosis-related targets.

Current main obstacles for the application of radiomics in liver disease rely on high-quality data collection and mechanism explanation on the biological basis. Multi-institutional data sharing and intensive collaborations on data cleansing and labelling offer appeal in filling this gap. Artificial intelligence algorithms with improved accuracy and interpretability meanwhile need to be developed to facilitate broader translation and clinical adoption.

7 | FINANCIAL INFORMATION

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CONFLICT OF INTEREST

None.

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