

RSA in Spine: A Review

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Abstract

Study Design: Systematic review of literature.

Objectives: This systematic review was conducted to investigate the accuracy of radiostereometric analysis (RSA), its assessment of spinal motion and disorders, and to investigate the limitations of this technique in spine assessment.

Methods: Systematic review in all current literature to investigate the role of RSA in spine.

Results: The results of this review concluded that RSA is a very powerful tool to detect small changes between 2 rigid bodies such as a vertebral segment. The technique is described for animal and human studies for cervical and lumbar spine and can be used to analyze range of motion, inducible displacement, and fusion of segments. However, there are a few disadvantages with the technique; RSA percutaneous procedure needs to be performed to implant the markers (and cannot be used preoperatively), one needs a specific knowledge to handle data and interpret the results, and is relatively time consuming and expensive.

Conclusions: RSA should be looked at as a very powerful research instrument and there are many questions suitable for RSA studies.

Keywords

radiostereometric analysis, RSA, radiological assessment of the spine, RSA in spine

Introduction

Radiostereometric analysis (RSA) is an accurate radiographic technique of measuring 3-dimensional (3D) movements between 2 bodies *in vivo*.¹⁻¹⁰

The principle of RSA is that when radio-opaque markers are inserted in the skeleton in 2 different bodies with the use of stereography and specialized computer software, the 3D position and any relative change in relation between these labelled bodies can be detected.¹¹ The relative change in distance between the markers reflects the relative movement between the 2 different marked bodies.¹² RSA was first developed by Goran Selvik, a Swedish mathematician in 1972 in Lund, Sweden. RSA remained in the laboratories as a research tool for many years before entering into the clinical study mainly in orthopedics and trauma. Spinal motion assessment was the first clinical application of RSA.¹¹ Joint arthroplasty is one of the main fields where RSA is established as the main method of assessment of implant migration and loosening.^{13,14} Fracture, osteotomies, and knee joint assessment are the other RSA applications in orthopedics and trauma.¹⁵⁻¹⁹

Spinal fusion, scoliosis surgery, spondylolisthesis treatment, and intervertebral disc arthroplasty are the main spinal

conditions where RSA is used. Hindmarsh reported the first scoliosis treatment assessment by RSA in 1973, followed by Olsson and colleagues reporting, in 1976, the first analysis of lumbosacral spine fusion studied with RSA.^{11,20}

This systematic review was conducted to investigate the accuracy of RSA, its assessment of spinal motion and disorders, and to investigate the cause of why RSA still not commonly used in the clinical assessment of spine after about 30 years since its first use in spine.

Materials and Methods

To establish the evidence that supports the use of RSA in the assessment of spinal motion, we conducted a systemic search in

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the literature. The literatures were reviewed by searching through the most common available databases:

- PubMed (to December 2015)
- Medline (1966 to December 2015)
- Embase (1980 to December 2015)
- Cochrane database (to December 2015)

The search strings were the same in all databases (“radiostereometric analysis,” “radiostereometry,” “roentgen stereophotogrammetric analysis,” “RSA”) and are shown in the following table.

Search Strings	PubMed	Medline	Embase	Cochrane
Radiostereometric analysis	405	154	271	154
Radiostereometry	495	138	170	84
Roentgen stereophotogrammetric analysis	266	256	151	36
RSA	5247	3967	3832	302
Combination	102	84	53	15
Total				254

Results

The total number of articles in the combined searches was 254. PubMed combined search resulted in 102 references, which was the highest number, while Medline, Embase, and Cochrane gave 84, 53, and 13, respectively.

The inclusion criteria were the following:

1. Published article in which spinal motion was assessed by RSA
2. Clear documentation of the accuracy of RSA
3. An article in English

The exclusion criteria were the following:

1. Nonspinal RSA study
2. No clear documentation about the accuracy of RSA
3. Not an article in English
4. Review papers

A total of 213 references were excluded because they were irrelevant or not fitting the inclusion criteria. The remaining 41 studies were included in this review study (Table 1).

The Precision and Accuracy of RSA in the Reviewed Articles

The accuracy of RSA varies in the literatures and it depends on several factors. The accuracy is the closeness of the measurements obtained to the actual movement.⁴⁴ The stability and security of beads fixation, the number of the beads inserted, and the distribution of the beads in each rigid body are the most important factors in determining the precision of the RSA setup and assessment (Figure 1).^{29,45} The accuracy can be adversely

affected by the instability of the beads in the rigid body.⁴⁴ This can be improved by using a very tight hole in the bone and avoiding oversized drilling, which keeps the beads loose or by delaying the assessment for 14 days, especially in metabolically active bone (children) to allow for initial instability to settle.⁴⁵ The alternative way to improve the instability is by using glue materials such as bone wax to provide temporary stabilization. The higher the number and the wider the distribution of the beads, the better the accuracy of the RSA assessment.^{11,45} The precision of RSA is the closeness of the measurements obtained from repeated examination to that of the first examination usually measured by testing and retesting of all of the sample of patients and defined as the standard deviation from the repeated measurements.^{32,33,45,46}

The accuracy is often expressed as a value and any movement above this value is considered significant. A movement below this value is considered insignificant as it is within the RSA setup error range. Table 2 shows summary of the reported precision figures of the RSA setup in the reviewed articles. Articles with unclear documentations of the accuracy and precision or using range of accuracy were excluded from this table. The mean translational accuracy in millimeters was (0.44, 0.5, 0.72) in the (*x*, *y*, and *z* axes), respectively, and rotational accuracy in degrees was (1.89, 1.92, and 1.13) in the (*x*, *y*, and *z* axes), respectively. This may suggest that we should aim for accuracy figures close to these values.

Application of RSA and Analysis of Reviewed Papers

RSA has been used for studying of (1) inducible displacement of vertebral segments and (2) spinal deformation over time. Inducible displacement should be understood as the positional difference between 2 vertebral bodies resulting from positional changes, such as supine to standing and also flexion/extension. These changes are ultimately described in translations and rotations in 3 dimensions. Areas studied are degenerative changes,³⁶⁻³⁸ spondylolisthesis,^{27,34,35,48,50} pseudarthrosis,²² fusion healing,^{20-23,28-33,39,47,51} and disc replacement.^{39-43,49,52} Spinal deformation is the changes in segmental position over time, such as a segment that collapses into kyphosis during fusion healing²⁹ and scoliosis.²⁴ To fully study the fusion process, *repeated* provocations are needed (inducible displacement), which allows studies of both mobility (provocation) and deformation (comparison of repeated examinations).

Inducible Displacement

Cervical Spine. Lee et al performed a pioneering work in the cervical spine in a cadaveric setup in 1993.²⁶

In a study conducted by Nabhan et al, RSA was used to compare cervical disc arthroplasty and fusion.⁴⁹ Although the clinical outcome of both groups was the same, there was significant loss of intervertebral motion in the fusion group compared with disc replacement when looked at 3, 6, 12, and 24 weeks after surgery. However, the segmental motion decreased

Table 1. Summary of All the Studies Included in This Review.

No.	Author	Journal	Year	Subject	Number	Area	Diagnosis	Operation	Aim of RSA	Result	Accuracy
1	Olsson	<i>Acta Radiol Diagn (Stockh)</i>	1976	Pig	5	Lumbar	Induced fusion	Fusion	Stability	Fusion/nonfusion	No
2	Olsson	<i>Invest Radiol</i>	1976	Human	2	Lumbar	DD	Fusion	Stability	Nonfusion detected with RSA	Range
3	Olsson	<i>Acta Radiol Diagn (Stockh)</i>	1976	Human	3	Lumbar	DD	Fusion	Stability	Stiffening of non-instrumented Fusion starts within 174 days	Yes
4	Olsson	<i>Acta Radiol Diagn (Stockh)</i>	1977	Human	3	T-L spine	Scoliosis	Fusion	Displacement	RSA is good in the assessment of residual curve movement after scoliosis surgery	No
5	Olsson	<i>Clin Orthop Relat Res</i>	1977	Human	12	Lumbar	DD or spondylolisthesis	Fusion	Stability	Fusion takes place within 180 days	Yes
6	Johnsson	<i>Spine</i>	1990	Human	11	Lumbar	Spondylolisthesis	Fusion	Stability	RSA not in correlation with X-ray (supine) in assessing fusion	No
7	Axelsson	<i>Spine</i>	1992	Human	7	Lumbar	DD	Fusion	Stability	Lumbosacral orthosis restricts motion, including hip: no further effect	No
8	Lee	<i>J Spinal Disord</i>	1993	Cadaver	45	Cervical	Cadveric spine	No operation	ROM	Accuracy determined	Yes
9	Lee	<i>Spine</i>	1994	Human	2	Cervical	DD	Fusion	Stability	Studies of fusion, few pats	No
10	Axelsson	<i>Spine</i>	1997	Human	6	Lumbar	Spondylolisthesis	Adjacent segment	Juxtartused segment	Hypermobility in the juxtartused segment	Yes
11	Johnsson	<i>Eur Spine J</i>	1997	Human	11	Lumbar	Low back pain	Fusion	Stability	Transfacet biodegradable rods increases fusion speed	Yes
12	Leivseth	<i>Spine</i>	1998	Human	8	Lumbar	Trauma	Fusion	Stability	RSA is superior to distortion-compensated Roentgen analysis	Yes
13	Zoega	<i>Eur Spine J</i>	1998	Human	18	Cervical	Disc herniation	Fusion cage w/o plate	Stability/displacement	Plate prevents kyphosis during fusion healing	Yes
14	Johnsson	<i>Spine</i>	1999	Human	12	Lumbar	DD	Fusion	Stability	Screws and plates provide rigid fixation	Yes
15	Axelsson	<i>Spine</i>	2000	Human	16	Lumbar	Spondylolisthesis	No operation	ROM	Low-grade spondylolisthesis (grade II) gives no instability	Yes
16	Gunnarsson	<i>Eur Spine J</i>	2000	Human	14	Lumbar	DD	Fusion	Stability	Rods and plates provide good stability for 1- or 2-level fusion	Yes
17	Lofgren	<i>Spine</i>	2000	Human	45	Cervical	Disc herniation	Fusion	Stability	Cloward fusion: Autograft = allograft = xenograft	Yes
18	Ryd	<i>Acta Orthop Scand</i>	2000	Human	36	Cervical	Disc herniation	Fusion	Accuracy	Accuracy studied	Yes
19	Johnsson	<i>Spine</i>	2002	Human	20	Lumbar	Spondylolisthesis	Fusion	Stability	Autologous bone = BMP-7	Yes
20	Pape	<i>Spine</i>	2002	Human	10	Lumbar	Spondylolisthesis	Fusion	Stability	RSA reliable for assessing fusion	Yes
21	Zoega	<i>Eur Spine J</i>	2003	Human	45	Cervical	Disc herniation	Fusion	Stability	Fusion; RSA superior to conventional X-ray bending films	Yes
22	Axelsson	<i>Eur Spine J</i>	2004	Human	18	Lumbar	LBP/DD	No operation	Inducible displacement	Disc height <50% → natural stabilization begins	Yes
23	Axelsson	<i>Spine</i>	2005	Human	12	Lumbar	Normal	Temporary external fixation	ROM	Supine to sitting gives largest changes	Yes
24	Halldin	<i>Int Orthop</i>	2005	Human	24	Lumbar	Disc herniation	Discectomy	Inducible displacement	No change in independent displacement after conventional discectomy over 5 years	No
25	Halldin	<i>Int Orthop</i>	2005	Human	21	Lumbar	Disc herniation	Discectomy	Inducible displacement	Early postoperative increase of inducible displacement; predicts poor outcome at 5 years	Yes
26	Krijnen	<i>Clin Orthop Relat Res</i>	2006	Goat	28	Lumbar	Normal	Fusion	Stability	Titanium cage = bioabsorbable cage	No
27	Axelsson	<i>Acta Orthop</i>	2007	Human	9	Lumbar	Adjacent segment	Adjacent fusion	ROM	No difference in ROM at adjacent segment; preoperative to 5 years postoperative	Yes
28	Lind	<i>Spine</i>	2007	Human	11	Cervical	Disc herniation	Disc prosthesis	Stability/ROM	Prosthesis stable in bone = bony ingrowth good; ROM	Yes
29	Nabhan	<i>J Long Term Eff Med Implants</i>	2007	Human	24	Lumbar	DD	Fusion/prosthesis	Stability/ROM	Prosthesis provides segmental motion	No
30	Nabhan	<i>Eur Spine J</i>	2007	Human	25	Cervical	DD	Fusion/prosthesis	Stability/ROM	Prosthesis provides segmental motion; decrease of segmental motion with time	Yes

(continued)

Table 1. (continued)

No.	Author	Journal	Year	Subject	Number	Area	Diagnosis	Operation	Aim of RSA	Result	Accuracy
31	Nabhan	<i>Spine</i>	2007	Human	41	Cervical	DD	Fusion/prosthesis	Stability/ROM	Cervical spine disc prosthesis preserves motion within the first 1 year after surgery	No
32	Nabhan	<i>Zentralbl Neurochir</i>	2007	Human	37	Cervical	DD	Fusion cage w/o plate	Stability	Anterior plate fixation did not improve the progress of fusion in one-level ACDF	No
33	Park	<i>Spine</i>	2009	Human	16	Cervical	DD	Fusion	Stability	RSA correlation well with flexion/extension films in the assessment of fusion	No
34	Park	<i>J Spinal Disord Tech</i>	2009	Human	10	Lumbar	DD	Prosthesis	ROM	Cobb method = QMA, RSA differs	No
35	Fayyazi	<i>J Spinal Disord</i>	2010	Human	6	Lumbar	Spondylolisthesis	Dynesys instrumentation	ROM	The Dynesys dynamic instrumentation system seems to stabilize degenerative spondylolisthesis	No
36	McDonald	<i>Spine J</i>	2010	Cadaver	1	Cervical	Cadaveric spine	Motion	ROM	RSA is an accurate method of assessment of ROM of spine	No
37	Boustani	<i>Clin Biomech (Bristol, Avon)</i>	2012	Finite	1	Lumbar	Finite	Fusion	ROM	Two postures flexion while standing and extension in a lying position are most suited for the assessment of spinal fusion when using RSA	No
38	Park	<i>Int J Spine Surg</i>	2012	Human	16	Lumbar	DD	PLIF vs dynamic stabilization versus discectomy alone	ROM	Lower amount of motion was seen after dynamic stabilization and PLIF when compared with discectomy	Yes
40	Humadi	<i>Evid Based Spine Care J</i>	2013	Sheep	9	Lumbar	Normal	Fusion	Accuracy	RSA as good as fine cut CT scan in assessment of fusion	No
41	Skeppholm	<i>J Neurosurg Spine</i>	2015	Human	28	Cervical	DD	Fusion vs arthroplasty	ROM	Arthroplasty showed intrinsic mobility several years after implantation	No

Abbreviations: RSA, radiostereometric analysis; DD, degenerative disc; ROM, range of motion; ACDF, anterior cervical discectomy and fusion; QMA, quantitative motion analysis; PLIF, posterior lumbar interbody fusion; CT, computed tomography.

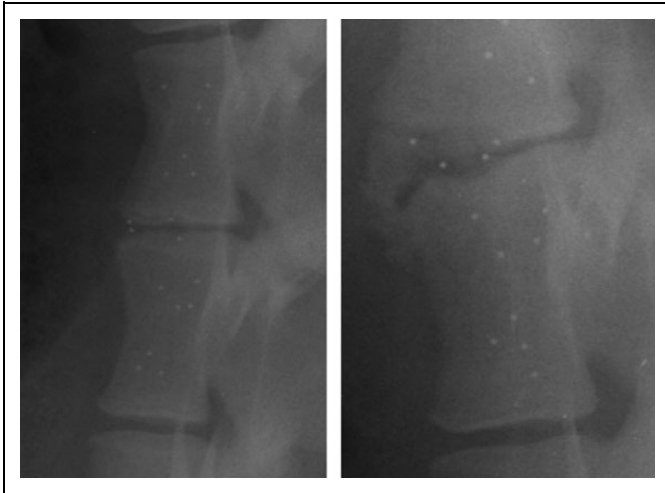


Figure 1. X-rays of lumbar spine in sheep showing the widely distributed RSA beads.

gradually in both groups over time, and further follow-up is recommended to verify the long-term outcome of this study.

Lumbar Spine. In the lumbar area, inducible displacement measured with RSA has been used to study the effect of lumbosacral orthosis,²⁵ stability in low-grade spondylolisthesis,⁴⁸ after discectomy,^{37,38} in different stages of degenerative disc disease,³⁶ and motion over disc replacement segments.^{40,42,49}

In 1992, Axelsson et al found that lumbosacral orthosis inhibits trunk mobility rather than lumbar mobility.²⁵ Extension to the hip did not add further stability. In a later study, Axelsson et al could rule out instability in low-grade L5/S1 isthmic spondylolisthesis compared to radiologically normal segments.⁴⁸

In 2004, Axelsson et al used RSA to study the stages of progressive degenerative process in the lumbar spine.³⁶ The authors assessed the intervertebral mobility for the 2 most-distal lumbar disc levels in 18 adult patients with low back pain, different stages of radiological disc degeneration, and no prior spinal surgery. RSA was used to measure the relative inducible displacement through the disc segments by changing position from supine to sitting. They concluded that the inducible displacement through the studied discs changes throughout the degenerative process and the stage of natural stabilization begins when disc height is reduced by 50%. The same authors studied inducible displacement over segments adjacent to lumbar fusion and found no difference preoperatively compared to 5 years later.⁵

The effect of lumbar discectomy on intervertebral motion over a period of 5 years was studied by Halldin et al.³⁸ Twenty-four patients with lumbar disc prolapse were treated by lumbar discectomy at the L4-L5 or L5-S1 level. The treated level was compared with the corresponding untreated level, which means that patients who had discectomy at L5-S1 were used as control for patients who had a discectomy at L4-L5 and vice versa. At the L4-L5 level they found no significant difference between the operated and control levels at discharge or 5 years postoperatively, whereas there at the L5-S1 level there was a

statistically significant motion reduction in the sagittal plane compared to the controls. Furthermore, 21 L4-5 or L5-S1 discectomy patients were studied in a prospective cohort study.³⁷ RSA was done postoperatively and 5 years after surgery. The results suggested that increased vertebral displacement in the early postoperative phase after discectomy is associated with a high risk of recurrence of back pain in the future.

Nabhan et al conducted a prospective study using RSA to compare lumbar spine disc replacement versus fusion for single-level degenerative disc disease.⁴¹ They divided the patients into 2 groups, 13 patients who underwent disc replacement and 11 patients who had fusion procedures. They followed-up their patients with serial RSAs up to 12 months after surgery and found significant segmental motion in the disc replacement group in comparison to the lumbar fusion group.

RSA has been found to be very accurate and enables assessment of range of motion (ROM) in 3 dimensions both in terms of translation (AP and lateral directions) and rotations (around the x , y , and z axes).^{5,8,10,26,27,48} This particular advantage of RSA over other radiological tools made RSA the preferred method of assessment of ROM of disc arthroplasty.^{8,40-42,49}

Spinal Deformation

Scoliosis. Olsson et al studied spinal correction of scoliosis prospectively as early as 1977. They presented data on deformation of the residual curve up to 1 year postoperatively.²⁴

Cervical Spine. The first RSA randomized controlled trial on cervical spine by Zoega et al was a comparison of anterior cervical discectomy and fusion (ACDF) techniques where plate fixation added to crest graft prevented kyphosing during healing, which, however, did not affect the postoperative outcome.²⁹ Lofgren et al found similar fusion rates for ACDF regardless of the use of allograft, autograft, or xenograft.³²

Lumbar Fusion. Assessment of lumbar fusion healing was the first and is the most common topic for RSA in spine. RSA has the advantage of being dynamic and accurate. The disadvantage and limitations of other radiological methods like dynamic flexion extension plain X-ray films and computed tomography (CT) scan pushed researchers and surgeon to use RSA. Dynamic plain X-ray films are the most common method used in most clinical practice. There are several studies that showed this method as nonaccurate and that there is significant inter-observer error.^{9,53,54} CT scan has the disadvantage of being nondynamic and the risk of exposing the body to high X-ray radiation doses, which subsequently increase the risk of malignancies.⁵⁵⁻⁶¹ Leivseth et al compared RSA to distortion compensation roentgen analysis (DCRA) in monitoring spinal motion. The authors found DCRA is inferior to RSA, with a higher measurement error. They describe 1° and 1 mm as limitation for DCRA to detect. If higher precision is important, as in spinal fusion assessment, RSA is recommended. In addition, RSA measures rotation and translation in 3 dimensions, while

Table 2. Accuracy as Reported in the Literature.

Study	Levels	Year	Accuracy					
			Translation			Rotation		
			Transverse (x) (mm)	Vertical (y) (mm)	Sagittal (z) (mm)	Transverse (x) (°)	Vertical (y) (°)	Sagittal (z) (°)
Olsson ²³		1977	0.1			0.3	0.2	0.1
Johnsson ⁶		1990	0.3	0.6	0.7			
Axelsson ²⁵		1992	0.3	0.6	0.7			
Lee ²⁶		1993	0.115	0.094	0.13	0.22	0.11	
Axelsson ²⁷		1997	0.3	0.6	0.7			
Johnsson ⁴⁷		1997	0.3	0.6	0.7			
Leivseth ²⁸		1998	0.7	0.16	0.22			
Zoega ²⁹		1998	0.43	0.34	0.85	4	3.7	2
Johnsson ³⁰		1999	0.3	0.6	0.7			
Axelsson ⁴⁸		2000	0.3	0.6	0.7			
Gunnarsson ³¹		2000	0.3	0.6	0.7			
Lofgren ³²		2000				1		
Ryd ³³		2000	0.12			0.36		
Johnsson ³⁴		2002	0.5	0.5	0.7	0.2	0.5	0.9
Pape ³⁵		2002	0.3	0.5	0.7			
Zoega ⁹	1-level	2003	0.56	0.27	0.81	3.6	4.2	1.3
	2-level		0.43	0.34	0.85	4	3.7	2
Axelsson ³⁶		2004	0.5	0.5	0.7			
Axelsson ¹⁰		2005	0.5	0.5	0.7			
Halldin ³⁸		2005	0.95	0.61	0.93	2.74	0.88	1.08
Axelsson ⁵		2007	0.5	0.5	0.7			
Lind ⁴⁰		2007	1.53	1.1	1.5	0.16	0.08	0.12
Nabhan ⁴⁹		2007	0.45	0.3	0.65	4.2	3.9	1.5
Mean			0.44	0.5	0.72	1.89	1.92	1.13

DCRA just measures rotation around the transverse axis and translation in the sagittal plane.^{28,62-64}

Although there are many published studies about the clinical application of RSA in spinal surgery, there are several limitations to this investigation tool.

1. The main reason why RSA cannot be used in high numbers is because it consumes too much time and resources and demands an operation expertise and specific knowledge that is possessed only by a few people. It means that it needs to be performed at the university level with special facilities and economical resources for research. Quantitative motion analysis (QMA) and quantitative fluoroscopy (QF) are other techniques that use computer technology to assess the ROM across segments of the spine.⁶⁵ This technique is used more frequently in spine clinical and research practice compare to RSA. The accuracy of QF may not be the same as RSA, but the practicality and the noninvasiveness of this technique makes its future promising when compared with RSA.⁶⁶
2. There is no universally accepted figure (degree of rotation or millimeter of translation) below which the tested segment is considered fused and above which it is considered nonfused. Most of the studies considered any movement above the precision figure as significant because it is above the error limit of this tool. It is not clear whether there are still some movements across

successfully fused discs due to the plasticity of the fusion mass, especially in the early stages of fusion. If we consider that there is no movement across successful fusion then any movement above the error limit of the RSA setup is consistent with pseudarthrosis. For all of this RSA needs to be validated by the use of an animal model, which allows the comparison of RSA results to histopathology as the gold standard in the assessment of different stages of fusion. This type of study may be able to give us an idea about how accurate RSA is in the assessment of fusion and more importantly may quantify the diagnosis of fusion.

3. RSA may be considered an invasive procedure. The beads can be inserted via an open technique during the surgical exposure to perform the index surgery and this may require further dissection or exposure. The new development of bead insertion instruments and the insertion of the beads at the time of surgical operation where the spine is already exposed makes it less invasive. Percutaneous insertion of the beads has been described and used as separate procedure with potential risks.⁴⁸ As a result of this invasive nature of the procedure, human clinical study using RSA requires obtaining informed consent as an additional procedure.
4. The accuracy of RSA varies in the literatures and it depends on several factors. The accuracy means the closeness of the measured value to the true one.⁴⁴ The

stability and security of beads fixation, the number of the beads inserted, and the distribution of the beads in each rigid body are the most important factors in determining the accuracy of the RSA setup and assessment.^{29,45} The accuracy can be adversely affected by the instability of the beads in the rigid body.⁴⁴ This can be improved by using a very tight hole in the bone and avoiding oversize drilling, which keeps the beads loose, or by delaying the assessment for 14 days, especially in metabolically active bone (children) to allow for the initial instability to settle.⁴⁵ The alternative way to improve the instability is by using gluing materials like bone wax. The higher the number and the wider the distribution of the beads, the better the accuracy of the RSA assessment.^{11,45} The accuracy of RSA is usually measured by testing and retesting of all of the sample of patients and is defined as the standard deviation from the repeated measurements.^{32,33,45,46}

5. The precision of RSA is the ability to achieve the same measurements by repeating the test. It can be measured only by repeating the test or by pair examination. Since RSA involves X-ray radiation, repeating the test exposes the patient to extra or double the radiation of a single testing. This is one of the disadvantages of RSA. The advantage of knowing the precision of the RSA testing usually outweighs the risk of radiation exposure, but careful explanation of the risk to the patient is mandatory.
6. Risk of RSA beads migration into spinal canal, soft tissue, and blood vessel of distant sites is another concern of the clinical use of RSA, especially in patients with poor bone quality. Extraosseous beads migration into the soft tissue was studied by Lawrie et al in the setting of total hip replacement RSA study.⁶⁷

Unfortunately, the accuracy and precision of assessment were not mentioned properly in several studies included in this review, and this questions the reliability of these assessments. In some studies, the accuracy was calculated from only the instability of the markers in the rigid bodies, which is inadequate as the number and distribution of the markers play a very important role as discussed above. Most of the studies agreed that the precision of RSA can be detected by repeating the assessment. This has been not uniformly applied. Some studies repeated the RSA assessment in all of the patients included in the study. Other studies repeated the test in a sample of the patients. In a few studies included in this review, the authors used the precision of prior study conducted with the same RSA setup as a reference precision of their new study. The precision and accuracy of RSA need a uniform clear definition to avoid any mix up. Measuring the precision of the study by repeating the RSA in a small sample of patients or by using that of prior study is not without risk. This can result in misleading figures and may affect the overall results of the study.

Although this review gives us a rough figure about the average accuracy of RSA from previous works, which is translation

accuracy in mm (0.45, 0.5, and 0.75) in the (*x*, *y*, and *z* axes), respectively, and rotational accuracy in degrees (1.89, 1.92, and 1.13) in the (*x*, *y*, and *z* axis), respectively, these figures are only rough and cannot be taken as exact due to various factors that could affect accuracy in RSA.

The accuracy of RSA did not improve with time as expected for any other radiological assessment tool and this may be because the earlier studies were animal studies, which makes it easier to justify putting a higher number of beads in a wider distribution. Although some recent studies are finite or cadaveric,⁶⁸ most are clinical human studies, which make it more difficult to widely distribute the RSA beads in the spine without causing unnecessary dissection and potential harm.⁶⁹

Despite all the above-mentioned limitations of RSA, it has been agreed by most researchers that RSA is an accurate method of assessment of spinal range of motion, inducible displacement, and spinal fusion. Humadi et al had tested the accuracy of RSA compared to fine-cut CT scan in an animal study using sheep as a model. They concluded that RSA is as accurate as CT scan with minimal radiation exposure.⁶³ They also suggested using a special awl in creating the holes for RSA beads and gluing the beads into the hole using bone wax to improve the stability of the beads and improve the accuracy of the assessment.⁶³

RSA can be used in assessment of scoliosis and in response to surgical correction in terms of derotation as RSA may be able to quantify the amount of derotation achieved postoperatively. RSA can also be used to follow-up traumatic injury of the spine and evaluate loss of position or progressive collapse of these injuries. Kyphoplasty is another area where RSA can be used to guide and follow-up the correction after this procedure. Assessment of ROM following the application of dynesys dynamic posterior stabilization system for treatment of degenerative lumbar spine has been reported using RSA.^{70,71}

Resorbable radio-opaque bioactive glass markers have shown adequate potential for RSA assessment due to their bone-bonding properties for marker stability and sufficient radio-opacity.⁷² It is too early to decide whether this potential marker can replace tantalum beads for RSA assessment, and further preclinical comparison between the 2 markers is suggested by Madanat et al.⁷²

Conclusion

RSA is a very powerful tool to detect small changes between 2 rigid bodies such as a vertebral segment. The technique is described for animal and human studies for cervical and lumbar spine and can be used to analyze ROM, inducible displacement, and fusion of segments. The accuracy and precision of RSA is superior to other techniques of assessment of motion and inducible displacement like QMA and QF. However, there are a few disadvantages with this technique. RSA is an invasive technique and percutaneous surgical procedure is needed to implant the markers. It is a labor-intensive process requiring trained personnel with specific knowledge to handle data and interpret the results, and it is relatively time consuming and

expensive. In conclusion, RSA should be looked at as a very powerful research instrument that can be applied in limited clinical spine work, and there are many clinical questions suitable for RSA studies.

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References

- Onsten I, Berzins A, Shott S, Sumner DR. Accuracy and precision of radiostereometric analysis in the measurement of THR femoral component translations: human and canine in vitro models. *J Orthop Res*. 2001;19:1162-1167.
- Borlin N, Thien T, Karrholm J. The precision of radiostereometric measurements. Manual vs. digital measurements. *J Biomech*. 2002;35:69-79.
- Valstar ER, Vrooman HA, Toksvig-Larsen S, Ryd L, Nelissen RG. Digital automated RSA compared to manually operated RSA. *J Biomech*. 2000;33:1593-1599.
- Resnick DK, Choudhri TF, Dailey AT, et al. Guidelines for the performance of fusion procedures for degenerative disease of the lumbar spine. Part 4: radiographic assessment of fusion. *J Neurosurg Spine*. 2005;2:653-657.
- Axelsson P, Johnsson R, Stromqvist B. Adjacent segment hypermobility after lumbar spine fusion: no association with progressive degeneration of the segment 5 years after surgery. *Acta Orthop*. 2007;78:834-839.
- Johnsson R, Selvik G, Strömquist B, Sundén G. Mobility of the lower lumbar spine after posterolateral fusion determined by roentgen stereophotogrammetric analysis. *Spine (Phila Pa 1976)*. 1990;15:347-350.
- Nabhan A, Pape D, Pitzen T, et al. Radiographic analysis of fusion progression following one-level cervical fusion with or without plate fixation. *Zentralbl Neurochir*. 2007;68:133-138.
- Park SA, Fayyazi AH, Ordway NR, Sun MH, Fredrickson BE, Yuan HA. Correlation of radiostereometric measured cervical range of motion with clinical radiographic findings after anterior cervical discectomy and fusion. *Spine (Phila Pa 1976)*. 2009;34:680-686.
- Zoega B, Karrholm J, Lind B. Mobility provocation radiostereometry in anterior cervical spine fusions. *Eur Spine J*. 2003;12:631-636.
- Axelsson P, Karlsson BS. Standardized provocation of lumbar spine mobility: three methods compared by radiostereometric analysis. *Spine (Phila Pa 1976)*. 2005;30:792-797.
- Karrholm J, Gill RH, Valstar ER. The history and future of radiostereometric analysis. *Clin Orthop Relat Res*. 2006;448:10-21.
- Valstar ER, Gill R, Ryd L, Flivik G, Börllin N, Kärrholm J. Guidelines for standardization of radiostereometry (RSA) of implants. *Acta Orthop*. 2005;76:563-572.
- Therbo M, Lund B. Roentgenographic stereogrammetric analysis after total knee arthroplasty [in Danish]. *Ugeskr Laeger*. 2009;171:888-890.
- Mjoberg B, Selvik G, Hansson LI, Rosenqvist R, Onnerfält R. Mechanical loosening of total hip prostheses. A radiographic and roentgen stereophotogrammetric study. *J Bone Joint Surg Br*. 1986;68:770-774.
- Bey MJ, Kline SK, Tashman S, Zauel R. Accuracy of biplane x-ray imaging combined with model-based tracking for measuring in-vivo patellofemoral joint motion. *J Orthop Surg*. 2008;3:38. doi:10.1186/1749-799X-3-38.
- Downing MR, Ashcroft PB, Johnstone AJ, Bach O, Mackenzie S, Ashcroft GP. Assessment of inducible fracture micromotion in distal radial fractures using radiostereometry. *J Orthop Trauma*. 2008;22(8 suppl):S96-S105.
- Smith C, Hull ML, Howell SM. Roentgen stereophotogrammetric analysis methods for determining ten causes of lengthening of a soft-tissue anterior cruciate ligament graft construct. *J Biomech Eng*. 2008;130:041002. doi:10.1115/1.2904897.
- Madanat R, Moritz N, Aro HT. Three-dimensional computer simulation of radiostereometric analysis (RSA) in distal radius fractures. *J Biomech*. 2007;40:1855-1861.
- Pape D, Adam F, Seil R, Georg T, Kohn D. Fixation stability following high tibial osteotomy: a radiostereometric analysis. *J Knee Surg*. 2005;18:108-115.
- Olsson TH, Selvik G, Willner S. Kinematic analysis of posterolateral fusion in the lumbosacral spine. *Acta Radiol Diagn (Stockh)*. 1976;17:519-530.
- Olsson TH, Selvik G, Willner S. Kinematic analysis of posterior spinal fusions in pigs. *Acta Radiol Diagn (Stockh)*. 1976;17:369-384.
- Olsson TH, Selvik G, Willner S. Kinematic analysis of spinal fusions. *Invest Radiol*. 1976;11:202-209.
- Olsson TH, Selvik G, Willner S. Mobility in the lumbosacral spine after fusion studied with the aid of roentgen stereophotogrammetry. *Clin Orthop Relat Res*. 1977;129:181-190.
- Olsson TH, Selvik G, Willner S. Postoperative kinematics in structural scoliosis. *Acta Radiol Diagn (Stockh)*. 1977;18:75-86.
- Axelsson P, Johnsson R, Stromqvist B. Effect of lumbar orthosis on intervertebral mobility. A roentgen stereophotogrammetric analysis. *Spine (Phila Pa 1976)*. 1992;17:678-681.
- Lee S, Harris KG, Nassif J, Goel VK, Clark CR. In vivo kinematics of the cervical spine. Part I: development of a roentgen stereophotogrammetric technique using metallic markers and assessment of its accuracy. *J Spinal Disord*. 1993;6:522-534.
- Axelsson P, Johnsson R, Stromqvist B. The spondylolytic vertebra and its adjacent segment. Mobility measured before and after posterolateral fusion. *Spine (Phila Pa 1976)*. 1997;22:414-417.
- Leivseth G, Brinckmann P, Frobin W, Johnsson R, Strömquist B. Assessment of sagittal plane segmental motion in the lumbar spine. A comparison between distortion-compensated and stereophotogrammetric roentgen analysis. *Spine (Phila Pa 1976)*. 1998;23:2648-2655.
- Zoega B, Karrholm J, Lind B. Plate fixation adds stability to two-level anterior fusion in the cervical spine: a randomized study using radiostereometry. *Eur Spine J*. 1998;7:302-307.
- Johnsson R, Axelsson P, Gunnarsson G, Strömquist B. Stability of lumbar fusion with transpedicular fixation determined by

- roentgen stereophotogrammetric analysis. *Spine (Phila Pa 1976)*. 1999;24:687-690.
31. Gunnarsson G, Axelsson P, Johnsson R, Strömqvist B. A method to evaluate the in vivo behaviour of lumbar spine implants. *Eur Spine J*. 2000;9:230-234.
 32. Lofgren H, Johannsson V, Olsson T, Ryd L, Levander B. Rigid fusion after Cloward operation for cervical disc disease using autograft, allograft, or xenograft: a randomized study with radiostereometric and clinical follow-up assessment. *Spine (Phila Pa 1976)*. 2000;25:1908-1916.
 33. Ryd L, Yuan X, Lofgren H. Methods for determining the accuracy of radiostereometric analysis (RSA). *Acta Orthop Scand*. 2000; 71:403-408.
 34. Johnsson R, Stromqvist B, Aspenberg P. Randomized radiostereometric study comparing osteogenic protein-1 (BMP-7) and autograft bone in human noninstrumented posterolateral lumbar fusion: 2002 Volvo Award in clinical studies. *Spine (Phila Pa 1976)*. 2002;27:2654-2661.
 35. Pape D, Fritsch E, Kelm J, et al. Lumbosacral stability of consolidated anteroposterior fusion after instrumentation removal determined by roentgen stereophotogrammetric analysis and direct surgical exploration. *Spine (Phila Pa 1976)*. 2002;27: 269-274.
 36. Axelsson P, Karlsson BS. Intervertebral mobility in the progressive degenerative process. A radiostereometric analysis. *Eur Spine J*. 2004;13:567-572.
 37. Halldin K, Zoëga B, Kärrholm J, Lind BI, Nyberg P. Is increased segmental motion early after lumbar discectomy related to poor clinical outcome 5 years later? *Int Orthop*. 2005;29:260-264.
 38. Halldin K, Zoëga B, Nyberg P, Kärrholm J, Lind BI. The effect of standard lumbar discectomy on segmental motion: 5-year follow-up using radiostereometry. *Int Orthop*. 2005; 29:83-87.
 39. Krijnen MR, Helder MN, Doulabi BZ, Bank RA, Wuisman PI, Klein-Nulend J. Does bioresorbable cage material influence segment stability in spinal interbody fusion? *Clin Orthop Relat Res*. 2006;448:33-38.
 40. Lind B, Zoega B, Anderson PA. A radiostereometric analysis of the Bryan cervical disc prosthesis. *Spine (Phila Pa 1976)*. 2007; 32:885-890.
 41. Nabhan A, Al-Yhary A, Ishak B, Steudel WI, Kollmar O, Steimer O. Analysis of spinal kinematics following implantation of lumbar spine disc prostheses versus fusion: radiological study. *J Long Term Eff Med Implants*. 2007;17:207-216.
 42. Nabhan A, Ahlhelm F, Shariat K, et al. The ProDisc-C prosthesis: clinical and radiological experience 1 year after surgery. *Spine (Phila Pa 1976)*. 2007;32:1935-1941.
 43. Phillips FM, Allen TR, Regan JJ, et al. Cervical disc replacement in patients with and without previous adjacent level fusion surgery: a prospective study. *Spine (Phila Pa 1976)*. 2009;34:556-565.
 44. Selvik G. Roentgen stereophotogrammetry. A method for the study of the kinematics of the skeletal system. *Acta Orthop Scand Suppl*. 1989;232:1-51.
 45. Kärrholm J. Roentgen stereophotogrammetry. Review of orthopedic applications. *Acta Orthop Scand*. 1989;60:491-503.
 46. Cai R, Yuan X, Rorabeck C, Bourne RB, Holdsworth DW. Development of an RSA calibration system with improved accuracy and precision. *J Biomech*. 2008;41:907-911.
 47. Johnsson R, Axelsson P, Stromqvist B. Posterolateral lumbar fusion using facet joint fixation with biodegradable rods: a pilot study. *Eur Spine J*. 1997;6:144-148.
 48. Axelsson P, Johnsson R, Stromqvist B. Is there increased intervertebral mobility in isthmic adult spondylolisthesis? A matched comparative study using roentgen stereophotogrammetry. *Spine (Phila Pa 1976)*. 2000;25:1701-1703.
 49. Nabhan A, Ahlhelm F, Pitzen T, et al. Disc replacement using Pro-Disc versus fusion: a prospective randomised and controlled radiographic and clinical study. *Eur Spine J*. 2007; 16:423-430.
 50. Pape D, Adam F, Fritsch E, Müller K, Kohn D. Primary lumbosacral stability after open posterior and endoscopic anterior fusion with interbody implants: a roentgen stereophotogrammetric analysis. *Spine (Phila Pa 1976)*. 2000;25:2514-2518.
 51. Lee S, Harris KG, Goel VK, Clark CR. Spinal motion after cervical fusion. In vivo assessment with roentgen stereophotogrammetry. *Spine (Phila Pa 1976)*. 1994;19:2336-2342.
 52. Nabhan A, Steudel WI, Nabhan A, Pape D, Ishak B. Segmental kinematics and adjacent level degeneration following disc replacement versus fusion: RCT with three years of follow-up. *J Long Term Eff Med Implants*. 2007;17:229-236.
 53. Santos ER, Goss DG, Morcom RK, Fraser RD. Radiologic assessment of interbody fusion using carbon fiber cages. *Spine (Phila Pa 1976)*. 2003;28:997-1001.
 54. Cook SD, Patron LP, Christakis PM, Bailey KJ, Banta C, Glazer PA. Comparison of methods for determining the presence and extent of anterior lumbar interbody fusion. *Spine (Phila Pa 1976)*. 2004;29:1118-1123.
 55. Heggie JC. Patient doses in multi-slice CT and the importance of optimisation. *Australas Phys Eng Sci Med*. 2005;28:86-96.
 56. John V, Ewen K. Comparative studies on the patient's exposure to radiation in case of spinal thin-layer computed tomography and of conventional radiologic examination methods [in Danish]. *Strahlentherapie*. 1983;159:180-183.
 57. Ngaile JE, Msaki P, Kazema R. Towards establishment of the national reference dose levels from computed tomography examinations in Tanzania. *J Radiol Prot*. 2006;26:213-225.
 58. Hall EJ, Brenner DJ. Cancer risks from diagnostic radiology. *Br J Radiol*. 2008;81:362-378.
 59. Iakovou I, Karavida N, Kotzassarlidou M. The computerized tomography scans and their dosimetric safety. *Hell J Nucl Med*. 2008;11:82-85.
 60. Mayo JR. Radiation dose issues in longitudinal studies involving computed tomography. *Proc Am Thorac Soc*. 2008;5:934-939.
 61. Tarin TV, Sonn G, Shinghal R. Estimating the risk of cancer associated with imaging related radiation during surveillance for stage I testicular cancer using computerized tomography. *J Urol*. 2009;181:627-632.
 62. Leivseth G, Kolstad F, Nygaard OP, Zoega B, Frobin W, Brinckmann P. Comparing precision of distortion-compensated and stereophotogrammetric Roentgen analysis when monitoring fusion in the cervical spine. *Eur Spine J*. 2006;15:774-779.

63. Humadi A, Freeman BJ, Moore RJ, et al. A comparison of radiostereometric analysis and computed tomography for the assessment of lumbar spinal fusion in a sheep model. *Evid Based Spine Care J.* 2013;4:78-89.
64. McDonald CP, Bachison CC, Chang V, Bartol SW, Bey MJ. Three-dimensional dynamic in vivo motion of the cervical spine: assessment of measurement accuracy and preliminary findings. *Spine J.* 2010;10:497-504.
65. du Rose A, Breen A. Relationships between lumbar intervertebral motion and lordosis in healthy adult males: a cross sectional cohort study. *BMC Musculoskelet Disord.* 2016; 17:121.
66. Park SA, Ordway NR, Fayyazi AH, Fredrickson BE, Yuan HA. Comparison of Cobb technique, quantitative motion analysis, and radiostereometric analysis in measurement of segmental range of motions after lumbar total disc arthroplasty. *J Spinal Disord Tech.* 2009;22:602-609.
67. Lawrie DF, Downing MR, Ashcroft GP, Gibson PH. Insertion of tantalum beads in RSA of the hip: variations in incidence of extra-osseous beads with insertion site. *Acta Orthop Scand.* 2003;74:404-407.
68. Boustani HN, Rohlmann A, van der Put R, Burger A, Zander T. Which postures are most suitable in assessing spinal fusion using radiostereometric analysis? *Clin Biomech (Bristol, Avon).* 2012; 27:111-116.
69. Skeppholm M, Svedmark P, Noz ME, Maguire GQ Jr, Olivecrona H, Olerud C. Evaluation of mobility and stability in the discover artificial disc: an in vivo motion study using high-accuracy 3D CT data. *J Neurosurg Spine.* 2015;23:383-389.
70. Fayyazi AH, Ordway NR, Park SA, Fredrickson BE, Yonemura K, Yuan HA. Radiostereometric analysis of postoperative motion after application of dynesys dynamic posterior stabilization system for treatment of degenerative spondylolisthesis. *J Spinal Disord.* 2010;23:236-241.
71. Park SA, Fayyazi AH, Yonemura KS, Fredrickson BE, Ordway NR. An in vivo kinematic comparison of dynamic lumbar stabilization to lumbar discectomy and posterior lumbar fusion using radiostereometric analysis. *Int J Spine Surg.* 2012;6:87-92.
72. Madanat R, Moritz N, Vedel E, Svedström E, Aro HT. Radio-opaque bioactive glass markers for radiostereometric analysis. *Acta Biomater.* 2009;5:3497-3505. doi:10.1016/j.actbio.2009.05.038.