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ORIGINAL ARTICLE

Quantitative determination of residual 1,4-dioxane in three-dimensional printed bone scaffold



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(2)

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KEYWORDS

headspace gas chromatography mass spectrometry; three-dimensional printing porous scaffold; 1,4-dioxane **Summary** Background/Objective: A novel porous scaffold poly (lactide-co-glycolide) and tricalcium phosphate (PLGA/TCP) was developed by three-dimensional printing technology for bone defect repair. As a Class 2 solvent with less severe toxicity, content of residual 1,4-dioxane in this newly developed scaffold should be rigorously controlled when it is translated to clinical use. In this study, a headspace gas chromatography-mass spectrometric (HS-GC-MS) method and related testing protocol were developed for quantitative determination of 1,4-dioxane in the PLGA/TCP composite scaffolds. *Methods:* Matrix effect analysis was used to optimise the pretreatment method of the scaffolds. Then, the procedure for testing 1,4-dioxane using HS-GC-MS was set up. The accuracy, precision, and robustness of this newly developed quantitative method were also validated

before quantification of 1,4-dioxane in the scaffolds with different drying procedures. *Results*: Dimethyl formamide (DMF) was the optimal solvent for dissolving scaffolds for GC-MS with proper sensitivity and without matrix effect. Then, the optimised procedure was determined as: the scaffolds were dissolved in DMF and kept at 90°C for 40 minutes, separated on a HP-5MS column, and detected by mass spectroscopy. Recovery experiments

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gave 97.9–100.7% recovery for 1,4-dioxane. The linear range for 1,4-dioxane was determined as 1–40 ppm with linear correlation coefficient \geq 0.9999. Intraday and interday precision was determined as being within relative standard deviation of below 0.68%. The passable drying procedure was related to lyophilising (-50°C, 50 Pa) the scaffolds for 2 days and drying in vacuum (50 Pa) for 7 days.

Conclusion: This is the first quantitative method established to test 1,4-dixoane in a novel scaffold. This method was validated with good accuracy and reproducibility, and met the methodological requirements of the Guideline 9101 documented in the Chinese Pharmacopoeia 2015 Edition.

The translational potential of this article: This quantitative method for determination of residual 1,4-dioxane in the novel scaffolds is a key technical method during its translation into clinical use because this method is an important and indispensable file in the enterprise standard when the porous scaffold is registered as a Class III implanted medical device for bone defect repair, which is used to guarantee the safety of the scaffolds. It is also applied to optimise the drying process of scaffolds and to monitor the quality of scaffolds in the industrialisation process. Further, this method provides references for other solvents quantitative determination in porous scaffolds or materials.

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Introduction

Steroid-associated osteonecrosis (SAON) is one of the most difficult diseases to treat as it largely occurs in large joints leading to articular surface collapse and expensive joint replacement [1-3]. The prognosis of joint replacement in SAON patients is poor due to osteolysis and impaired osteogenesis [4,5]. Accordingly, research and development of osteopromotive scaffolds ready for implantation, which would be capable of activating host cells to differentiate into angiogenic and osteogenic lineage, would be desirable [6,7].

Low-temperature deposition manufacturing (LDM) is a unique rapid prototype technology [8,9] that provides accurate point-to-point control of liquid moulding materials to form scaffolds with a gradient pore structure [10,11]. In some studies, series of porous poly(lactic-*co*-glycolic acid) and tricalcium phosphate (PLGA/TCP) scaffold were fabricated using the LDM technique [12]. The PLGA/TCP scaffolds exhibited osteoconductive activity and could also be used as a drug carrier [11,13–20].

In the process of scaffold fabrication, 1,4-dioxane was optimised as a necessary solvent used for dissolving PLGA due to its low melting point, liposolubility and highly volatile nature. However, with two oxygen atoms, 1,4-dioxane has been shown to be carcinogenic to animals and humans [21-24]. Furthermore, 1,4-dioxane may also be toxic to liver, lungs, kidneys, and the central nervous system [25]. 1,4-dioxane was defined as a Class 2 solvent associated with less severe toxicity, which should be limited to below 380 ppm according to international regulations, such as Chinese Pharmacopoeia [26], International Conference on Harmonization of Technical Requirements for Registration of Pharmaceuticals for Human Use [27], and United States Pharmacopoeia [28]. Therefore, it is mandatory to test residual 1,4-dioxane for PLGA/TCP scaffolds and this testing is also necessary for registration and guality control of novel scaffolds.

To date, established testing methods for 1,4-dioxane have been used for quantification analysis in liquid or liquid-like samples, such as drinking water, waste water, vaccines, and cosmetics. These samples were usually processed with double distilled water [29,30]. For scaffolds, the pretreatment is a necessary step to select a proper solvent before analysis.

It was reported that 1,4-dioxane was determined reliably in water by various techniques including direct aqueous injection, purge and trap gas chromatographymass spectrometric (GC-MS), and GC-MS analysis of continuous liquid—liquid extraction extracts [30]. Conventional purge and trap GC-MS is strictly limited by poor purge efficiency of 1,4-dioxane whose detection limit is about 100 times higher than those efficiently purged volatile organic compounds [30]. Headspace GC-MS (HS-GC-MS) was used commonly in the determination of poorly purged organic solvents in cosmetics [31] as it could reach the target compound to eliminate the background interference in special boiling point of volatile organic compounds. Therefore, HS-GC-MS was chosen as an analysis method for scaffolds to simplify the pretreatment process and acquire high quantity chromatogram or spectrum.

The purpose of this investigation was to develop a selective, rapid, yet simple and robust method for the determination of 1,4-dioxane in PLGA/TCP porous scaffolds by HS-GC-MS. The procedure included pretreatment of the scaffolds, sample enrichment by headspace apparatus, separation from other components by GC, and identification by MS. The method was validated and applied to optimise the drying process of scaffolds during fabrication that could also be generalised as standard and/or guideline for wide applications.

Experimental

Standards and reagents

1,4-dioxane (99.9%, GC grade) and dimethyl sulphoxide (GC grade) were obtained from Aladdin (Shanghai, China).

Dimethyl formamide (DMF; HPLC grade) was obtained from J&K Scientific Corporation (Beijing, China).

Raw material of scaffolds

PLGA: The ratio of lactic acid to glycolic acid was 75:25. Molecular weight was 250,000 Da and provided by Shandong Institute of Medical Instruments (Shandong, China).

TCP: Low temperature β -tricalcium phosphate. Range of particle size was 0.1–5 μ m. It was obtained by chemical precipitation and purchased from Shanghai Bio-lu Bio-materials Co., Ltd. (Shanghai, China).

Fabrication and surface morphologies of PLGA/TCP scaffolds

Porous scaffolds PLGA/TCP were made by threedimensional (3D) printing based on LDM technique (Figure 1A). Before the samples were fabricated, PLGA was dissolved in 1,4-dioxane at a ratio of 1:5 (weight/volume). TCP was mixed with the solution at a ratio of 1:4 (weight/ weight) (TCP:PLGA). Homogenous slurries were controlled to be deposited into specific positions according to the model predesigned by computer animated design. The fabrication temperature in the refrigerator was -30° C. Subsequently, the scaffolds were lyophilised to remove the solvent during fabrication. Matrix blank scaffolds were fabricated followed by the process of sample, except that PLGA was dissolved in dimethylsulphoxide instead of in 1,4dioxane. The surface morphologies of the prepared scaffold sections were observed by scanning electron microscopy (SEM, JEOL JSM-6390, Tokyo, Japan) at 15 kV and 5.0 m.

One scaffold weighed 2 g and was lyophilised at -50° C, 50 Pa for 2 days; then, it was cut into five 0.3 g of scaffolds separately, and dried at room temperature for 0 days, 3 days, 6 days, 7 days, and 9 days in vacuum drying oven with the pressure of 50 Pa for selecting the best freeze-drying process.

Preparation of standard solutions

Standard solutions of DMF were used for the calibration curve: 0.4 mL, 0.2 mL, 0.1 mL, and 0.05 mL of standard stock solution (1000 ppm) were transferred to five 10 mL volumetric flasks with DMF, separately, diluted with DMF to volume and mixed. Subsequently, 1 mL of 10 ppm of standard solution was transferred to a 10 mL volumetric flask, diluted with DMF to volume, and then mixed to obtain 1 ppm standard solution.

Standard solutions of Na₂CO₃ solution used for calibration curve: 2.5 mL, 1.25 mL, 0.625 mL, 0.3125 mL, and 0.128 mL of standard stock solution (400 ppm) were transferred to five 10 mL volumetric flasks with Na₂CO₃, separately, diluted with Na₂CO₃ solution (0.3 g/mL) to volume, and mixed.

Standard solutions including matrix blank scaffolds: 0.3 g of matrix blank scaffolds, which were cut into pieces of $0.2 \times 0.2 \times 0.2 \text{ cm}^3$ were transferred to a headspace vial, and five parallels were prepared. Then, 4 mL of five different concentrations of standard solutions of DMF or Na₂CO₃ solution used for the calibration curve were transferred into five headspace vials one by one.

All of the standard solutions described above (4 mL) were transferred to each vial and the vials were closed immediately. After heating the vial for 40 minutes at 90° C,



Figure 1 Porous properties of our novel three-dimensional printed scaffolds. (A) Photo of poly (lactide-*co*-glycolide) and tricalcium phosphate (PLGA/TCP) porous scaffold. (B–F) Representative scanning electron microscopy images of porous PLGA/TCP scaffold at different magnifications [(B) $20\times$; (C) $200\times$; (D) $250\times$; (E) $500\times$; (F) $2000\times$].

the HS-GC-MS of the gas in the sample vial was performed for optimisation of solutions.

Quantitation

A 0.3 g sample was weighed accurately and cut into pieces of $0.2 \times 0.2 \times 0.2 \text{ cm}^3$ in a headspace vial. DMF (4 mL) was transferred to this vial, and the vial was closed immediately. After heating the vial for 40 minutes at 90°C, the HS-GC-MS of the gas in the sample vial was performed in the selective ion (masses 88) mode. The sample was quantified by the external standard method. Calibration curves were determined at the beginning of sample set in 1 day. Blanks and check standards were run for each sample set. Overall, blanks and check standards comprised a minimum of 30% of the total samples analysed during any given analysis sequence to ensure the stability of the method.

GC/MS analysis

HS-GC tandem MS was used to identify and quantify 1,4dioxane. An Agilent (California, USA) 7890B GC was used for all separations. The GC was equipped with a 30m \times 0.25 mm \times 0.25 μ m HP-5 MS column (California, USA). The GC was coupled to an Agilent 7697A headspace for injection and an Agilent 5977 mass spectrometer (MS) operated in electric ionisation mode while using the selective ion monitoring mode. Optimised parameters of GC-MS are as followed in Table 1.

Method validation

Specificity

Specificity described the ability of an analytical method to separate the analysts of interest accurately from other components expected to be present in samples. The guiding principle 9101 [26] entitled "The validation guidelines of drug quality standard analytical method" provides identification requirements and criteria for specificity testing. Blank, sample, and 100 ppm of standard solution were prepared following the preparation protocol and detected.

Accuracy

According to Chinese Pharmacopoeia 2015 Edition guideline 9101 [26], accuracy can be evaluated with spiking recovery experiments. Matrix blank can be used to evaluate recovery as described in the guideline. In our sample preparation process, 0.3 g scaffold was dissolved with 4 mL DMF. According to Chinese Pharmacopoeia [26], International Conference on Harmonization of Technical Requirements for Registration of Pharmaceuticals for Human Use [27], and United States Pharmacopoeia [28], 1,4-dioxane in the products should be no more than 380 ppm. We convert the concentration of 1,4-dioxane in 0.3 g scaffold (i.e. 380 ppm) into the concentration in 4 mL DMF according to the following formula: 380 ppm \times weight of the scaffold (0.3 g)/the weight of DMF = 380 ppm \times 0.3g/(volume \times density) of DMF = 380 ppm \times 0.3g/(4 mL \times 0.9487 g/L) = 30 ppm. This means the concentration of 1,4-dioxane in 0.3 g scaffold in 4 mL DMF should be less than 30 ppm. So, 20 ppm, 25 ppm, and 30 ppm of 1,4-dioxane standard solutions Table 1Optimised parameters of HS-GC-MS for determining 1,4-dioxane in novel porous scaffolds.

Content	Item	Parameter
Instrument	HS	Agilent 7697A
	GC	Agilent 7890
	MS	Agilent 5977A
Parameters of	Temperature	90°C
Headspace	Time	40 min
Parameters of GC	Column	HP-5MS
	Process of Column	40°C (5 min)
	Temperature	320°C (5 min)
	Process of post run	
	Gas mode	Velocity
	Velocity	36.262 cm/sec
	Inlet mode	split
	Split ratio	50:1
Parameters of MS	Temperature of source	230°C
	Temperature of inlet	220°C
	Quantifier ion	88
	Quantifier ion	58
	Scan mode	SIM

GC = gas chromatography; HS = head space; MS = mass spectrometry; SIM = selected ion monitoring.

were prepared with matrix blank scaffolds in DMF; triplicate samples of each concentration were prepared. The recovery was calculated as follows: (actual concentration/ theoretical concentration) \times 100%.

Precision

The method precision can be determined using standard preparations [29]. Method repeatability expresses the precision of the analytical method including system precision and sample preparation under the described operating conditions. Two standards of 25 ppm were processed by two different research assistants in 2 days for determination of both intra- and inter-day precision using the same method. Every sample was analyzed six times. Relative standard deviation (RSD%) was used for the evaluation of precision.

Limit of detection and limit of quantitation

The limit of detection (LOD) is the lowest amount that can be detected, but not necessarily quantified. According to the guideline [26], it is defined as the concentration required to give a signal to noise ratio (S/N) of 3:1. The limit of quantification (LOQ) is the lowest amount that can be quantified accurately, defined as the concentration required to give a signal to noise ratio (S/N) of 10:1.The noise ratio was calculated automatically by a Mass Selective Detector (MSD) chemstation of Agilent after the target peak was integrated. A serial sample of low concentrations (100 ppb, 10 ppb, 1 ppb, 0.1 ppb) were detected and analysed.

Linearity

Series concentrations of standards of 1,4-dioxane of 1-40 ppm were prepared as per the preparation protocol described earlier. Calibration curves were constructed for each analyst, plotting (peak area of quantifier ion) versus

62

concentration (ppm). Slope, intercept, and correlation coefficient were calculated using linear regression analysis.

Robustness of the method

Robustness can be described as the ability to reproduce the (analytical) method under different circumstances. When a small change exists, a robust test is set up to evaluate the robustness of a method. Special factors changed in GC-MS detection were columns of different brands or batch numbers, different solid phase, different types of supports, flow rate of carrier gas, temperature of column, inlet, and detection [26]. In this validation, we used two different columns (HP-5ms and DB-624) to detect the same sample for evaluating the robustness. Each column detected samples in triplicate.

Application in optimising the drying procedure

Scaffolds dried at 37°C in 0 days, 3 days, 6 days, 7 days, and 9 days in vacuum drying oven were quantified by optimised conditions. The content of 1,4-dioxane was compared with different scaffolds processed in different drying procedures.

Statistical analysis

The peak areas of 1,4-dioxane in different extracts were presented as means \pm standard deviation of three repeated

experiments. T test was performed using SPSS 16.0 software (Chicago, IL, USA) for comparison with statistical significance at p < 0.05.

Results

Porous property of 3D printing PLGA/TCP scaffolds

The photo of 3D printing porous scaffold is shown in Figure 1A. From the SEM images, we found that the scaffolds had well interconnected macropore structures (Figure 1B), and numerous micropores were observed on the wall surface of the scaffold framework, with pore sizes ranging from 5 μ m to 50 μ m (Figures 1C–1F).

DMF was the optimal solvent for dissolving scaffolds for GC-MS.

In this investigation, two solvents (double distilled H₂O, DMF) and two sodium solutions (NaCl solution and Na₂CO₃ solution) were chosen as optimising solvents for sample preparation (Figure 2A). The order of the peak area of 1,4-dioxane was: double distilled Na₂CO₃-H₂O > NaCl-H₂O > H₂O > DMF (p < 0.01 vs. H₂O, n = 3) (Figure 2B). However, the area of 1,4-dioxane in each concentration of the calibration curves without matrix were twice that of those in which matrix was dissolved with Na₂CO₃-H₂O. These differences were not found between the calibration curves with or without matrix blank scaffolds dissolved with DMF



Figure 2 Optimisation of the solvent in pretreatment process. (A) Standard solution of 25 ppm dissolved with different solutions. (B) Quantified area of 1,4-dioxane in different solutions using the same head space gas chromatography mass spectrometry parameter. ** p < 0.01 (n = 3), vs. ddH₂O. (C) Matrix effect of standards dissolved with Na₂CO₃-H₂O or dimethyl formamide (DMF). The concentrations of standard dissolved with Na₂CO₃-H₂O were 6.25 ppm, 12.5 ppm, 25 ppm, 50 ppm, and 100 ppm. The concentrations of the standard dissolved with DMF were 1 ppm, 5 ppm, 10 ppm, 20 ppm, and 40 ppm. AB*S = abundance × second ; dd = double distilled; ppm = parts per million.

(Figure 2C), indicating that the matrix effect of samples significantly existed when dissolved with $Na_2CO_3-H_2O$. Thus, DMF was the optimal solvent for dissolving scaffolds for GC-MS.

Validation of the method

System suitability

The 70 eV electron ionization mass spectral ions from 1,4dioxane include the molecular ion, m/z 88 ([M]⁺, quantifier ion) and fragment ions, m/z 58 ([M-CH₂O]⁺, qualifier ion). The retention time of the target mass was 3.266 min. There was 100% chromatographic resolution of the peaks (resolution, (RS) > 1.5) (Figure 3). The tailing factor of this target peak was 2.26, and the number of theoretical plates was 36,954.

Specificity

The results showed that the method was specific as there was no other peak to interfere with the peak of interest, and as for the retention time no significant difference was observed from the standard components (Figure 4).

Accuracy, precision, robustness, and linearity

The accuracy, precision, robustness, and linearity of the method are summarised in Table 2. Recovery experiments gave 97.9-100.7% recovery for 1.4-dioxane (Table S1). The repeatability of the method was expressed as % RSD of five continuous standards, and the %RSD of peak area was 0.6%. %RSD of retention time and peak area that described intraday precision were 0.01% and 0.58%, respectively (n = 6). Interday precision was calculated to describe intermediate precision of retention time and peak area, which were 0.02% and 0.62% (n = 12), respectively (Table S2). The linear range for 1,4-dioxane was determined as 1-40 ppm. The calibration curves were linear for all the standard components with correlation coefficient \geq 0.9999. LOD and LQD for 1,4-dioxane were 1 ppb and 5 ppb, respectively. The results showed that the resolution, tailing factor, and the number of theoretical plates when the column was changed to DB-624 met the system suitability requirements. %RSD of six samples was 1.6% between Hp-5ms and DB-624 (Table S3), implying that the area of target peak had little changes. All of the results met the requirement of the guideline 9101 described in the Chinese Pharmacopoeia 2015 Edition [26] (Table 2).



Figure 3 Chromatography and spectrum for the determination of 1,4-dioxane. (A) Extract ion gas chromatography mass spectrometry (GC-MS) of 1,4-dioxane of sample. (B) Extract ion GC-MS of 1,4-dioxane of standard. (C) Mass spectrum of 1,4-dioxane of sample. (D) Mass spectrum of 1,4-dioxane of standard.



Figure 4 The method shows good specificity. (A) There is no peak in the selected ion monitoring (SIM) chromatography of blank. The same retention time (min) of 1,4-dioxane in the SIM chromatography of sample (B) and SIM chromatography of 25 ppm standard (C) without other peaks to interfere.

Items		Tested value		Accepted range [26]
Linearity		R ²	0.99999	/
·		Range (ppm)	1-40	/
Accuracy (Recovery)		20 ppm	97.9% ± 3.76	90-108%
		25 ppm	$100.7\%\pm2.41$	
		30 ppm	98.9% ± 1.18	
Precision (RSD)	Repeatability $(n = 6)$	RT	0.01%	< 3%
		Area	0.58%	
	Intermediate precision	RT	0.02%	< 6%
	(n = 12)			
		Area	0.62%	
Robustness (RSD)		1.60%		1

RSD = relative standard deviation; RT = retention time

Application in the translation of PLGA/TCP porous scaffolds

The established method has been used to monitor the drying process and control the quality of the scaffolds. The

result showed that 1,4-dioxane in the scaffolds lyophilised $(-50^{\circ}C, 50 \text{ Pa})$ for 2 days and then dried in vacuum (25°C, 50 Pa) for 7 days were below 380 ppm. Extension of freeze drying time to 9 days did not reduce the content of 1,4-dioxane (Figure 5). According to the data above, the



Figure 5 Optimisation of freeze-drying process. Scaffolds were lyophilised for 2 days and dried at 37° C in 0 days, 3 days, 6 days, 7 days, and 9 days in vacuum drying oven. ppm = parts per million.

scaffolds should be freeze-dried for 2 days and then dried in vacuum more than 7 days to control the content of 1,4-dioxane to satisfy the safety limit.

Discussion

Three-dimensional printing porous scaffolds are promising regenerative strategies for bone defect repair in orthopaedics [6,7]. As a newly developed medical product, safety issues are considered as the most important ones. As a Class 2 solvent with less severe toxicity, content of residual 1,4-dioxane in the novel 3D printing PLGA/TCP scaffolds should be rigorously controlled [26]. We first developed an HS-GC-MS method for testing 1,4-dioxane in PLGA/TCP porous scaffolds. This method utilised a reproducible and highly recovery sample preparation process, a more efficient separation technology, and a specific singleion monitoring mass detection to quantify 1,4-dioxane in PLGA/TCP porous scaffolds.

Different from the liquid or liquid-like sample [29,30], 1,4-dioxane should be extracted from the solid scaffold at the first step. Four solutions were used; as a result, the detected amount of 1,4-dioxane was exactly inversely related to its solubility in different solution, and Na₂CO₃ solution showed the highest sensitivity due to the saltingout effect [32]. However, as the first method to test the gas from a solid porous structure, we further investigated the matrix effects of the different solutions. There were two different extraction systems, one in Na₂CO₃ solution, retaining the porous structure of the scaffolds, and the other in DMF solution without any porous structures. In DMF solution, the scaffolds were dissolved into powders, and 1,4-dioxane was distributed in solution phase and gas phase. The detected amount was determined by its solubility in DMF, so the detected amount of 1,4-dioxane were the same in DMF with or without matrix blank scaffolds. In Na₂CO₃ solution with the matrix blank scaffold, 1,4dioxane was distributed in three phases: scaffold, solution, and gas, and the detected amount was determined not only the solubility in Na₂CO₃ but also the attachment in the porous scaffolds. Thus, the detected amount of 1,4dioxane in Na₂CO₃ solution only was more than that in the Na2CO3 solution with matrix blank scaffolds (Figure 2C). The fabricated porous scaffolds had both regular macropores, with the size among 300 μ m to 500 μ m, as well as irregular micropores with size from 5 μ m to 50 μ m pores (Figure 1B–1F) [11,13], which might be the cause of matrix effects. Thus, we selected DMF to extract 1.4-dioxane from the scaffolds as the pretreatment process of the GC-MS methods. The following method's validation results further confirmed the feasibility of this procedure.

This method was validated with good accuracy and reproducibility and met the methodological requirements of the guideline 9101 described in the Chinese Pharmacopoeia 2015 edition. It is one of the indispensable files in medical device approval and registration. We used this established method to monitor the drying process of scaffolds to guarantee the residual 1,4-dioxane less than 380 ppm, according to Chinese Pharmacopoeia [26]. Our results showed that 1,4-dioxane in the scaffolds lyophilised $(-50^{\circ}C, 50 \text{ Pa})$ for 2 days and then dried in vacuum (25°C, 50 Pa) for 7 days were below 380 ppm (Figure 4). After examining the three-phase diagram of 1,4-dioxane, we found that the conditions of $-50^{\circ}C$ and 50 Pa for lyophilising are not efficient for removing 1,4-dioxane (Figure S1) because in this environment 1,4-dioxane prefers solid rather than gas; therefore, we will further optimise the drying process by lowering the pressure or increasing the temperature to improve the freeze-dry efficiency. Our newly established guantitative method will also be used to verify this hypothesis.

In fact, when we used this established method to test 1,4-dioxane in the PLGA raw material from different suppliers, we detected chloroform in some batches (Figure S2). However, if we want to accurately quantify the chloroform or dichloromethane, the pretreatment (extract) process is commonly used, while the parameters of GC-MS should be specifically tuned for each target solvent to meet the requirements of method validation.

Conclusion

In this investigation, the HS-GC-MS method was firstly developed for testing 1,4-dioxane in PLGA/TCP porous scaffolds. This method was validated to meet the requirements in the Chinese Pharmacopoeia 2015 Edition, which provided residual 1,4-dioxane test methods in the PLGA/TCP scaffolds for CFDA registration. First, we resolved the method of pretreatment of the solid scaffold to eliminate matrix effect in the development process. The analysis method had been used to optimise the process of drying of scaffolds to satisfy the product requirement. In addition, it is an important tool for quality control of the composite scaffolds.

Translational significance

Three-dimensional printing porous scaffolds are promising regenerative strategies for bone defect repair in orthopaedics [6,7]. As a newly developed medical product, safety issues are considered as the most important ones. As a Class 2 solvent with less severe toxicity, content of residual 1,4-dioxane in the novel 3D printing PLGA/TCP scaffolds should be rigorously controlled according to international regulations, such as Chinese Pharmacopoeia [26], International Conference on Harmonization of Technical Requirements for Registration of Pharmaceuticals for Human Use [27] and United States Pharmacopoeia [28]. In this work, we firstly developed an HS-GC-MS method for testing 1,4-dioxane in PLGA/TCP porous scaffolds. It is an important file in medical device approval and registration. It has been applied as an enterprise standard to optimise the drying process of scaffolds and monitor the quality of scaffolds in the industrialisation process.

Conflicts of interest

The authors declare no conflicts of interest in this work.

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Appendix A. Supplementary data

Supplementary data related to this article can be found at http://dx.doi.org/10.1016/j.jot.2017.06.004.

References

- [1] Griffith JF, Antonio GE, Kumta SM, Hui DSC, Wong JKT, Joynt GM, et al. Osteonecrosis of hip and knee in patients with severe acute respiratory syndrome treated with steroids. Radiology 2005;235:168–75.
- [2] Zhang G, Sheng H, He YX, Xie XH, Wang YX, Lee KM, et al. Continuous occurrence of both insufficient neovascularization and elevated vascular permeability in rabbit proximal femur during inadequate repair of steroid-associated osteonecrotic lesions. Arthritis Rheum-US 2009;60:2966–77.
- [3] Xie XH, Wang XL, Yang HL, Zhao DW, Qin L. Steroid-associated osteonecrosis: epidemiology, pathophysiology, animal model, prevention, and potential treatments (an overview). J Orthop Translat 2015;3:58–70.
- [4] Nair MB, Kretlow JD, Mikos AG, Kasper FK. Infection and tissue engineering in segmental bone defects—a mini review. Curr Opin Biotechnol 2011;22:721–5.
- [5] Cao HJ, Guan HF, Lai YX, Qin L, Wang XL. Review of various treatment options and potential therapies for osteonecrosis of the femoral head. J Orthop Translat 2016;4:57–70.
- [6] Wang XL, Xie XH, Zhang G, Chen SH, Yao D, He K, et al. Exogenous phytoestrogenic molecule icaritin incorporated into a porous scaffold for enhancing bone defect repair. J Orthop Res 2013;31:164–72.
- [7] Li Y, Chen SK, Li L, Qin L, Wang XL, Lai YX. Bone defect animal models for testing efficacy of bone substitute biomaterials. J Orthop Translat 2015;3:95–104.
- [8] Lee CH, Cook JL, Mendelson A, Moioli EK, Yao H, Mao JJ. Regeneration of the articular surface of the rabbit synovial joint by cell homing: a proof of concept study. Lancet 2010; 376:440-8.
- [9] Stevens B, Yang YZ, Mohandas A, Stucker B, Nguyen KT. A review of materials, fabrication to enhance bone regeneration in methods, and strategies used engineered bone tissues. J Biomed Mater Res B 2008;85B:573–82.
- [10] Fedorovich NE, Alblas J, Hennink WE, Oner FC, Dhert WJA. Organ printing: the future of bone regeneration? Trends Biotechnol 2011;29:601–6.
- [11] Chen SH, Zheng LZ, Xie XH, Wang XL, Lai YX, Chen SK, et al. Comparative study of poly (lactic-co-glycolic acid)/tricalcium phosphate scaffolds incorporated or coated with osteogenic growth factors for enhancement of bone regeneration. J Orthop Translat 2014;2:91–104.
- [12] Lai YX, Li L, Chen SK, Zhang M, Wang XL, Zhang P, et al. A Novel magnesium composed PLGA/TCP porous scaffold fabricated by 3D printing for bone regeneration. J Orthop Translat 2014;2:218–9.
- [13] Qin L, Yao D, Zheng LZ, Liu WC, Liu Z, Lei M, et al. Phytomolecule icaritin incorporated PLGA/TCP scaffold for steroid-associated osteonecrosis: proof-of-concept for prevention of hip joint collapse in bipedal emus and mechanistic study in quadrupedal rabbits. Biomaterials 2015;59: 125-43.
- [14] Duan CG, Liu J, Yuan Z, Meng GL, Yang XM, Jia SJ, et al. Adenovirus-mediated transfer of VEGF into marrow stromal cells combined with PLGA/TCP scaffold increases

vascularization and promotes bone repair in vivo. Arch Med Sci 2014;10:174-81.

- [15] Chen SH, Lei M, Xie XH, Zheng LZ, Yao D, Wang XL, et al. PLGA/TCP composite scaffold incorporating bioactive phytomolecule icaritin for enhancement of bone defect repair in rabbits. Acta Biomater 2013;9:6711–22.
- [16] Xie XH, Wang XL, Zhang G, He YX, Wang XH, Liu Z, et al. Structural and degradation characteristics of an innovative porous PLGA/TCP scaffold incorporated with bioactive molecular icaritin. Biomed Mater 2010;5.
- [17] Sherwood JK, Riley SL, Palazzolo R, Brown SC, Monkhouse DC, Coates M, et al. A three-dimensional osteochondral composite scaffold for articular cartilage repair. Biomaterials 2002;23: 4739-51.
- [18] Yu D, Li Q, Mu X, Chang T, Xiong Z. Bone regeneration of critical calvarial defect in goat model by PLGA/TCP/rhBMP-2 scaffolds prepared by low-temperature rapid-prototyping technology. Int J Oral Max Surg 2008;37:929–34.
- [19] Chen SH, Wang XL, Xie XH, Zheng LZ, Yao D, Wang DP, et al. Comparative study of osteogenic potential of a composite scaffold incorporating either endogenous bone morphogenetic protein-2 or exogenous phytomolecule icaritin: an in vitro efficacy study. Acta Biomater 2012;8:3128–37.
- [20] Klenke FM, Liu YL, Yuan HP, Hunziker EB, Siebenrock KA, Hofstetter W. Impact of pore size on the vascularization and osseointegration of ceramic bone substitutes in vivo. J Biomed Mater Res A 2008;85A:777–86.
- [21] IARC Working Group on the Evaluation of Carcinogenic Risks to Humans. Overall evaluations of carcinogenicity : an updating of IARC monographs volumes 1 to 42. In: IARC monographs on the evaluation of carcinogenic risks to humans. Lyon, France: World Health Organization; 1987.
- [22] National Cancer Institute. In: Carcinogenicity technical report. Bethesda: National Cancer Institute; 1978.
- [23] Fishbein L. Potential industrial carcinogens and mutagens. Elsevier Science. Available at: https://www.elsevier.com/

books/potential-industrial-carcinogens-and-mutagens/ author/978-0-444-41777-0. [Accessed January 1, 1979].

- [24] Lundberg I, Hogberg J, Kronevi T, Holmberg B. Three industrial solvents investigated for tumor promoting activity in the rat liver. Cancer Lett 1987;36:29–33.
- [25] United States Environmental Protection Agency. In: Technical fact sheet-1,4-dioxane. United States Environmental Protection Agency; 2014.
- [26] Chinese Pharmacopoeia Commission. In: The Pharmacopoeia of the People's Republic of China 2015. China Medical Science Press; 2015.
- [27] International Conference on Harmonisation (ICH) of Technical Requirements for the Registration of Pharmaceuticals for Human Use. ICH Harmonised Tripartite guideline, step 4. In: International Conference on Harmonisation (ICH) of technical requirements for the registration of pharmaceuticals for human use; 2011.
- [28] The United States Pharmacopeial Convention. United States Pharmacopeial, USP 39–NF 34. In: The United States Pharmacopeial Convention; 2015.
- [29] Armstrong BL, Senyurt AF, Narayan V, Wang X, Alquier L, Vas G. Stir bar sorptive extraction combined with GC-MS/MS for determination of low level leachable components from implantable medical devices. J Pharm Biomed Anal 2013;74: 162-70.
- [30] Draper WM, Dhoot JS, Remoy JW, Perera SK. Trace-level determination of 1,4-dioxane in water by isotopic dilution GC and GC-MS. Analyst 2000;125:1403–8.
- [31] Rastogi SC. Headspace analysis of 1,4-dioxane in products containing polyethoxylated surfactants by GC-MS. Chroma-tographia 1990;29:441–5.
- [32] Marusic Radovcic N, Vidacek S, Janci T, Medic H. Characterization of volatile compounds, physico-chemical and sensory characteristics of smoked dry-cured ham. J Food Sci Technol 2016;53:4093–105.