


 Cite this: *RSC Adv.*, 2025, 15, 223

Meniran (*Phyllanthus niruri* L.) embedded zeolitic imidazolate framework (ZIF-8) nanoparticle for cancer chemotherapy: supported molecular docking analysis†

 Fasih Bintang Ilhami,^{ID}*^a Sari Edi Cahyaningrum,^{ID}^b Andika Pramudya Wardana,^b Noto Susanto Gultom,^c Hasan Subekti,^a Astrid Rahmawati^d and Sapti Puspitarini^{*a}

Cancer is among the leading causes of mortality worldwide. Natural bioactive compounds like Meniran (*Phyllanthus niruri* L.) have been the focus of extensive research due to their potent anticancer properties. Nevertheless, drug delivery strategies may be necessary to encapsulate bioactive compounds, thereby reducing their toxicity and enhancing their stability. Herein, we successfully synthesized Meniran extract incorporated zeolitic imidazolate framework (ZIF-8) nanoparticles for anticancer therapy. Meniran-incorporated ZIF-8 nanoparticles possess unique advantages including well-distributed nanoparticles with rhombic dodecahedrons and excellent pH-responsiveness. *In vitro* analysis showed that Meniran-incorporated ZIF-8 nanoparticles have anticancer activity towards HeLa cells. Interestingly, computational simulations offer valuable insights into the molecular-level interaction mechanisms between ZIF-8 and specific proteins under cancer cells. As far as we are aware, this is the first report of natural bioactive compounds derived from Meniran encapsulated into nanoparticles as a drug delivery system, marking a significant advancement in the development of novel biomaterials for cancer treatment.

 Received 4th September 2024
 Accepted 21st December 2024

DOI: 10.1039/d4ra06399f

rsc.li/rsc-advances

Introduction

Conventional cancer treatments are widely utilized but suffer from several drawbacks, including inadequate, solubility of the drug, lack of specificity towards the target, and notable adverse effects.^{1,2} Drug delivery system-based nanoparticles present promising alternatives as therapeutic agents, with the potential to substantially enhance cancer treatment efficacy. Drug-loaded nanoparticles possess the capability to pass through the vascular network of tumors owing to the Enhanced Permeability and Retention (EPR) effect. This phenomenon extends the amount of time that anticancer drugs stay in bloodstream, subsequently improving drug bioavailability and therapeutic efficacy while reducing the occurrence of side effects.³⁻⁷ The EPR effect has been substantiated in multiple tumor models,

wherein nanoparticle-drug conjugates achieve drug concentrations 10- to 100-fold higher than free drugs within tumor tissues. This targeted drug delivery mechanism could have been the driving force of the EPR effect exclusive to tumor tissues and was not observed in normal tissues.⁸⁻¹⁰ The primary objective of cancer research has been the successful delivery of targeted drugs to specific areas of the body, to minimize adverse effects and maximize therapeutic potential.

To date, the focus on plant-derived natural compounds has garnered attention due to their phytochemicals for therapeutics. *Phyllanthus niruri* L., referred to known as Meniran is a medicinal plant that commonly thrives in humid and rocky regions especially Indonesia. The plant comprises a diverse array of chemical components, including as lignans, tannins, polyphenols, alkaloids, flavonoids, terpenoids, and steroids.¹¹ Nurcholis and coworkers¹² mentioned that Meniran is notably rich in phenolic compounds. Most importantly, Meniran has been investigated as an anticancer agent in several cancer cell lines, such as Lewis cells line,^{13,14} HL-60 cells line,¹⁵ HepG2 cells line,¹⁶ 143B cell line,¹⁷ and A549 cells line.^{14,18} Thus, Meniran has pharmacological efficacy due to its bioactive components such as hepatoprotective, reducing blood sugar levels, anticancer, antimicrobial, preventing oxidative damage, and cardioprotective.¹⁹ However, despite the notable advantages of plant-derived natural compounds, there are still various obstacles to overcome in terms of their biomedical application

^aDepartment of Natural Science Faculty of Mathematics and Natural Science, Universitas Negeri Surabaya, Surabaya 60231, Indonesia. E-mail: fasihilhami@unesa.ac.id; saptipuspitarini@unesa.ac.id

^bDepartment of Chemistry, Faculty of Mathematics and Natural Sciences, Universitas Negeri Surabaya, Surabaya 60231, Indonesia

^cDepartment of Physics, Universitas Padjadjaran, Bandung 45363, Indonesia

^dDepartment of Applied Chemistry, Osaka Institute of Technology, Osaka 535-8585, Japan

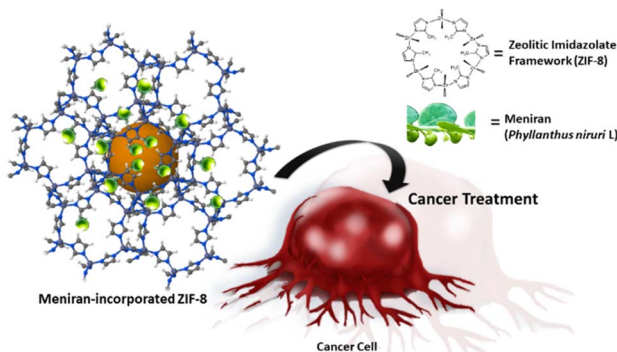
† Electronic supplementary information (ESI) available: LC-HRMS analysis, loading content, binding affinity results are provided. See DOI: <https://doi.org/10.1039/d4ra06399f>



including their solubility and stability in water, as well as potential harmful effects within the body.²⁰ As a possible approach to tackle these issues, we hypothesized that incorporating plant-derived natural compounds into smart materials might have a significant alter on their solubility and stability in water.

Metal–Organic Frameworks (MOF) represent a continuously expanding crystalline materials classification consists metal ions and an organic component known as the linker.²¹ MOF possess numerous attractive characteristics including their significant porosity (which exceeds 50% of the crystal volume), large surface area (ranging from about 1000 to 10 000 m² g⁻¹), and the ability to precisely adjust their properties by altering either the reaction conditions or the reactants. MOF have been applied in a diverse array of fields, including catalysis, gas storage, adsorbents for separation processes, sensors, biomedical imaging, and drug delivery.^{22–27} Zeolitic Imidazolate Framework (ZIF-8) is a very notable metal–organic framework known for its remarkable properties, mostly attributed to its significant pore width of 11.6 Å and nanosized. These properties include facile synthesis at room temperature, economically viable precursors, excellent stability, high surface area, and the potential for further enhancements through chemical modification of the linker which promising candidate for drug delivery systems.^{28–33} ZIF-8 has a unique characteristic of pH-responsive drug release, whereby pharmaceuticals are released at a faster rate at acidic pH levels (5.5–6), which align with the internal conditions of cancer cells, namely inside endosomes and lysosomes. As a consequence, this leads to more targeted drug release, thereby minimizing the side effects associated with the carried drugs.^{28,34,35}

Herein, we create plant-derived natural compounds of extract Meniran incorporated into ZIF-8 nanoparticles for a potential approach to cancer therapy. These materials clearly showed well-distribution nanoparticles with strong activity towards cancer cells. Moreover, computational simulations provide insight into the interaction mechanisms of ZIF-8 with specific proteins at the molecular level. To the best of our knowledge, this is the first report on the incorporation of bioactive compounds from extract Meniran into ZIF-8 nanoparticles for cancer therapy. Therefore, this study could offer



Scheme 1 Graphical illustration Meniran-incorporated ZIF-8 nanoparticles and release within cancer cells to provide toxicity.

valuable insights into the development of innovative strategies based on plant-derived natural compound nanoparticles for cancer treatment Scheme 1.

Results and discussion

The Meniran extract was obtained through the extraction method, which employed methanol as the solvent, subsequently obtained through column separation following solvent evaporation. First, the LC-HRMS was conducted to confirm the qualitative results of compounds isolated within Meniran. As shown in Table S1†, the bioactive compound analysis presented that Meniran contains several bioactive compounds which include flavonoid, tannin, and phenol group. These results indicate that the combination extract contains bioactive compounds that have pharmacological effects as anticancer. The therapeutic and pharmacological effects of plant-derived natural chemicals are attributed to their active components, such as phenol and flavonoid groups, which have been scientifically shown to possess anticancer properties.^{38–40} Next, we also performed interaction prediction between Meniran compounds and proteins by *in silico* study. Meniran extract is anticipated to potentially suppress cancer cell proliferation due to its active components, which include quercetin, rutin, and quercetin 3-beta-D-glucoside (Isoquercitrin). Although it is possible that these compounds work synergistically in their function as alternative herbs. However, perhaps the mechanism of action of these compounds can be evaluated through predictions of interactions between compounds *in silico*. As illustrated in Fig. S1,† these compounds interact with many proteins associated with cell proliferation, including EGFR and CASP3. Numerous studies indicate that EGFR activation may be suppressed by quercetin,⁴¹ rutin,⁴² and quercetin 3-beta-D-glucoside⁴³ which these compounds have been shown to activate Caspase.⁴⁴

Furthermore, we introduced bioactive components of Meniran into ZIF-8 nanoparticles at ambient temperature and evaluated them using a spectrophotometer with absorbance at 285 nm to precisely quantify of encapsulation efficiency. Meniran contains bioactive compounds such as flavonoids, tannins, and phenolic groups, which are capable of forming weak coordination interactions with Zn²⁺ in an aqueous system.^{45,46} As illustrated in Table S2†, the Meniran-incorporated ZIF-8 at a weight ratio of 2:1 attained the maximum drug-loading content (DLC) of 5.01 ± 0.85%. These results consistent with previous studies that MOF including ZIF-8 has high payload capacity.^{47–49}

The structure of ZIF-8, Meniran and Meniran-incorporated ZIF-8 was initially examined by Fourier Transform Infra-Red (FTIR) and X-ray diffraction (XRD). As shown in Fig. 1a, the distinctive peaks from IR spectroscopy of ZIF-8 are located in the 900–1350 cm⁻¹ (bending of the imidazole ring inside the plane), <800 cm⁻¹ (bending of the imidazole ring out of the plane) and peak around 420 cm⁻¹, implying the existence of a chemical bond between the metal and the ligand. The primary peaks of Meniran extract are seen at 3305 cm⁻¹ (O–H stretching), 2942 cm⁻¹ (CH₂– stretching), 2854 cm⁻¹ (–CH₃ stretching),

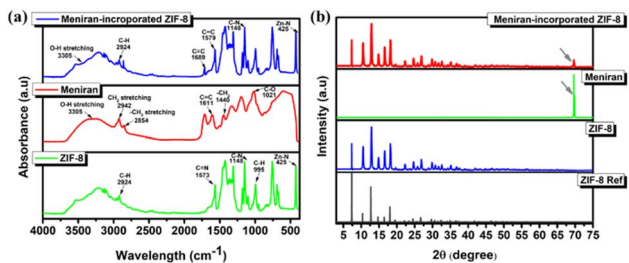


Fig. 1 Characteristic of ZIF-8, Meniran, and Meniran-incorporated ZIF-8 under (a) FTIR spectra and (b) XRD pattern.

1611 cm^{-1} (C=C bonds), 1440 cm^{-1} and 1332 cm^{-1} ($-\text{CH}_3$ twisting and wagging), and 1021 cm^{-1} (C-O stretching in secondary alcohols). The Meniran-incorporated ZIF-8 has similar peaks to pristine ZIF-8, indicating that are several overlapping peak locations between Meniran and ZIF-8. Moreover, the X-ray powder diffraction (XRD) patterns verified that samples were crystalline ZIF-8 in the $I43m$ space group, exhibiting distinct and intense diffraction peaks that align with previous studies^{50–52} (Fig. 1b). The diffractogram of Meniran indicates that partly amorphous structure with highest peak at $2\theta = 69.6^\circ$, while Meniran-incorporated ZIF-8 did not exhibit any altered peak from the diffractogram of pure ZIF-8 thereby enabling the MOF to preserve its intrinsic structural characteristics. Notably, a small peak was noticed at about $2\theta = 69.6^\circ$ (shown by a grey arrow), which suggests the existence of Meniran within ZIF-8.

To examine the surface structure of the samples, a field emission scanning electron microscopy (FE-SEM) was performed equipping with an energy dispersive spectroscopy at a working voltage of 20 kV. As shown in Fig. 2a, the morphology of ZIF-8 is well-distribution as nanostructure with rhombic dodecahedrons, polyhedrons with 12 faces, 24 edges and 14 vertices as agreement with previous studies.⁴⁹ Interestingly, Meniran-incorporated ZIF-8 has almost unchanged the

morphology, indicating that ZIF-8 maintained the morphology of nanostructure (Fig. 2b). Furthermore, TEM analysis confirmed that the Meniran-incorporated ZIF-8 exhibited rhombic dodecahedron shapes and were slightly larger than the pristine ZIF-8 nanoparticles[†]. The particle size is a critical element in the effectiveness of tumor cell therapies, ZIF-8 nanoparticles with a size of 70 nm can successfully internalize towards tumor cells.⁵³ To verify these results, we further evaluated the particle size distribution by DLS. As shown in Fig. 2c, the particle size of ZIF-8 nanoparticles is 76.2 ± 1.98 , while Meniran-incorporated ZIF-8 nanoparticles exhibited particle size slightly higher of 85.1 ± 1.05 . These findings indicate that the increasing particle size might be due to Meniran already payload into ZIF-8 nanoparticles. Next, to clearly understand of surface area of the ZIF-8 nanoparticles and Meniran-incorporated ZIF-8 nanoparticles, we examined by Brunauer-Emmett-Teller BET analysis of nitrogen adsorption isotherms. As shown in Fig. 2d, the surface area of ZIF-8 nanoparticles was determined to be $1021 \text{ m}^2 \text{ g}^{-1}$ and pore volume $0.43 \text{ cm}^3 \text{ g}^{-1}$, which is consistent with other reports with a range from 960 to $1820 \text{ m}^2 \text{ g}^{-1}$.⁵⁴ However, upon the incorporation of Meniran into ZIF-8 nanoparticles, the surface area significantly decreased up to $403 \text{ m}^2 \text{ g}^{-1}$ with pore volume $0.11 \text{ cm}^3 \text{ g}^{-1}$, indicating that may be attributed to Meniran occupying the adsorption sites of the ZIF-8 nanoparticles while the smaller change may be attributed to the specific adsorption mechanism involved. These results are in excellent agreement with SEM and TEM result.

Based on previous reports ZIF-8 has pH-responsive properties that have inspired us to investigate the *in vitro* drug release kinetics under PBS conditions. As depicted in Fig. 3a, under pH 7.4 of Meniran-incorporated ZIF-8 nanoparticles only 28% released after 36 h. Importantly, under pH 5.0 Meniran was rapidly released reached 70% and restrained release after 36 h. The Meniran-incorporated ZIF-8 exhibits pH-responsive release capacity due to the coordination bond disruption between zinc ions and imidazolate at lower pH levels.⁵⁵ Thus, the acidic environment surrounding malignancy can provide the stimulation to trigger the rapid release of Meniran from the carriers.

Furthermore, we performed a cytotoxicity assay of ZIF-8, Meniran, and Meniran-incorporated ZIF-8 nanoparticles toward HeLa cells due a stable and reproducible results across multiple experiments by MTT method. As shown in Fig. 3b, the

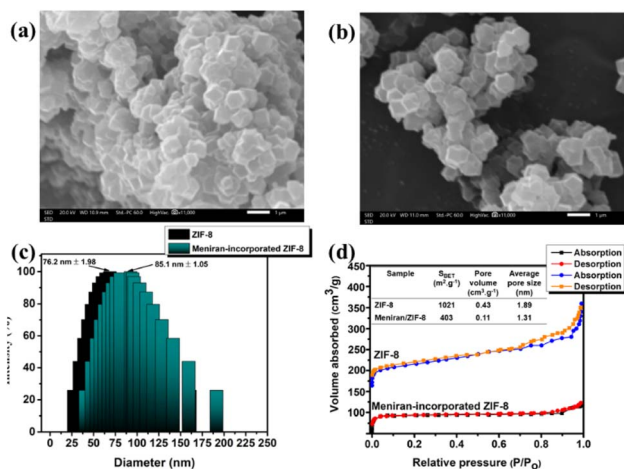


Fig. 2 SEM images of (a) ZIF-8 and (b) Meniran-incorporated ZIF-8, (c) DLS spectra, and (d) BET analysis of ZIF-8 and Meniran-incorporated ZIF-8.

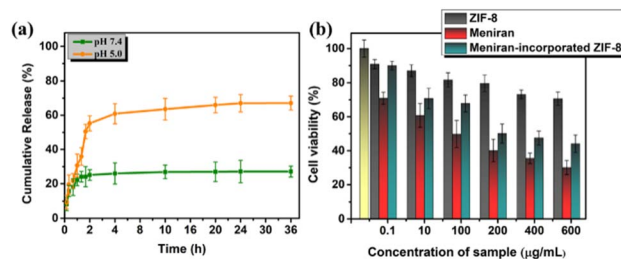


Fig. 3 (a) *In vitro* drug release of Meniran-incorporated ZIF-8 nanoparticles under different pH values. (b) MTT analysis of ZIF-8, Meniran, and Meniran-incorporated ZIF-8 under HeLa cells.

cells viability only slightly decreases following incubation with ZIF-8 nanoparticles and without any IC_{50} value, suggesting that these nanocarriers are biocompatible. Surprisingly, Meniran-incorporated ZIF-8 exhibited rapidly released and cell viability significantly decreased with $IC_{50} = 205.41 \pm 3.09 \mu\text{g mL}^{-1}$, compared with pure Meniran $IC_{50} 102.37 \pm 2.89 \mu\text{g mL}^{-1}$ indicating that the time required for Meniran to be released from ZIF-8 nanoparticles and consequently delayed of Meniran internalization towards the cells. Therefore, these findings confirm that bioactive compound from Meniran extract incorporated into ZIF-8 nanoparticles potent cytotoxicity in cancer cells and improve efficacy chemotherapy.

To confirm the adsorption of ZIF-8 could has interact with protein target for anticancer, molecular docking calculations were implemented. As shown in Table S3†, the docking results for AKT-1, EGFR, or MDM2 with ZIF-8 demonstrated higher binding affinities to AKT-1 and EGFR compared to a known inhibitor, with affinities of $-10.8 \text{ kcal mol}^{-1}$ versus AZD5363's $-9.1 \text{ kcal mol}^{-1}$ for AKT-1, and $-8.5 \text{ kcal mol}^{-1}$ versus MTX-531's $-8.2 \text{ kcal mol}^{-1}$ for AKT-1. However, in MDM2, ZIF-8 is potentially bound with binding affinities of $-9.4 \text{ kcal mol}^{-1}$, compared inhibitor (Imidazole, $-9.6 \text{ kcal mol}^{-1}$). Furthermore, we conducted an investigation focused on assessing the alignment of the compounds with the protein active site owing to crucial for evaluating the potential of these nanoparticle to inhibit the proteins effectively. The molecular docking analysis revealed that ZIF-8 nanoparticles could bind to a similar region

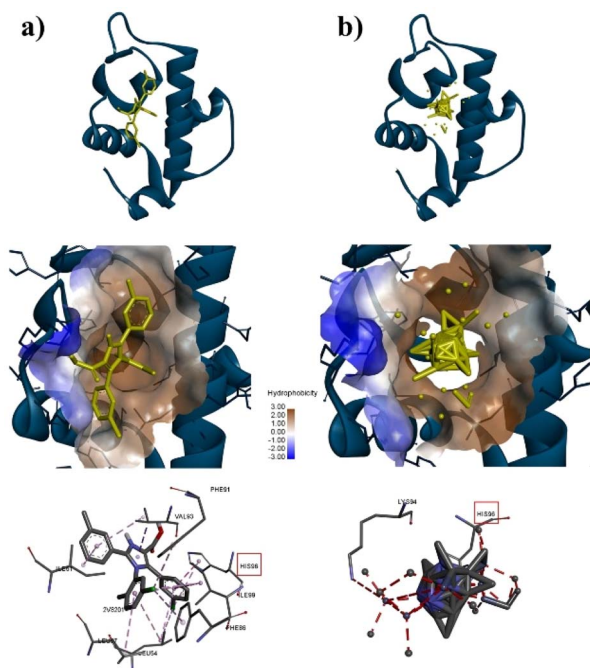


Fig. 4 Interaction between MDM2 and (a) imidazole or (b) ZIF-8. At the top, MDM2 is depicted as a blue-ribbon structure, with ligands shown in yellow. At the centre, a hydrophobicity surface map of the MDM2 active site is shown, with the ligands highlighted in yellow. At the bottom, interactions between the ligands and the amino acid residues of the protein are illustrated with red box as marker the same amino acid residue.

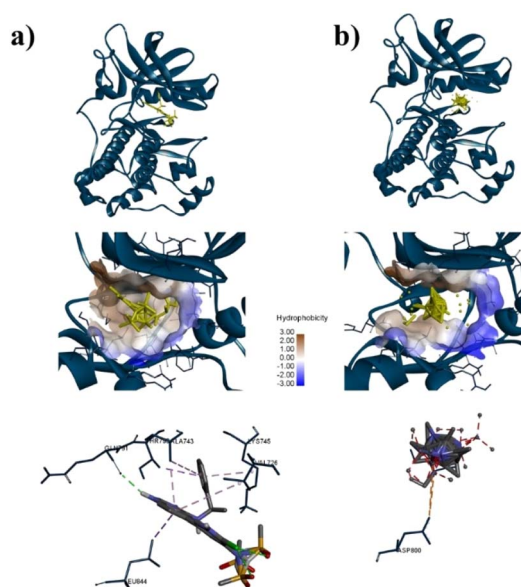


Fig. 5 Interaction between AKT-1 and (a) AZD5363 or (b) ZIF-8. At the top, AKT-1 is depicted as a blue-ribbon structure, with ligands shown in yellow. At the centre, a hydrophobicity surface map of the AKT-1 active site is shown, with the ligands highlighted in yellow. At the bottom, interactions between the ligands and the amino acid residues of the protein are illustrated with red box as marker the same amino acid residue.

as the inhibitor (Fig. 4–6). However, only in the cases of MDM2 and AKT-1 did ZIF-8 exhibit comparable amino acid residue interactions to those of the control ligand (Fig. 4 and 5). The ZIF-8 nanoparticles binding to HIS96 is comparable to that of the native inhibitor when interacting with the MDM2 protein (Fig. 4). Similarly, ZIF-8 binding to GLU234 and GLU278 mirrors the native inhibitor's interactions with the MDM2 protein (Fig. 5).

Nanoparticles (NPs) often exhibit distinct magnetic, thermal, optical, and electrical properties due to their large surface area and significant quantum mechanical effects. They are frequently designed and employed as drug carriers, facilitating the targeted delivery of chemotherapeutic agents to tumor tissues while reducing damage to healthy organs.⁵⁶ ZIF-8 is a type of nanoparticle, composed of zinc metal and 2-methyl imidazole (MIM) ligand, are one of the most widely used types of ZIFs owing to their inherent properties, such as the low toxicity of zinc metal, relatively large cavities, high thermal and chemical stability, ultrahigh surface area, and high crystallinity.⁵⁷ Moreover, the LD50 (the dosage at which 50% of the animal population is killed) for ZIF-8 has been documented as 1400 mg mL^{-1} .^{57,58} This research aimed to assess the effectiveness of ZIF-8 as a drug nanocarrier for anticancer agents by molecular docking analysis.

Next, our study used three specific proteins, namely AKT-1, MDM2, and EGFR which are implicated in cancer pathways, such as regulating cell proliferation, angiogenesis, and apoptosis. Several studies have concentrated on targeting these proteins in cancer therapy.^{59–63} Based on Table S3†, ZIF-8 nanoparticles have potential to binding with three proteins

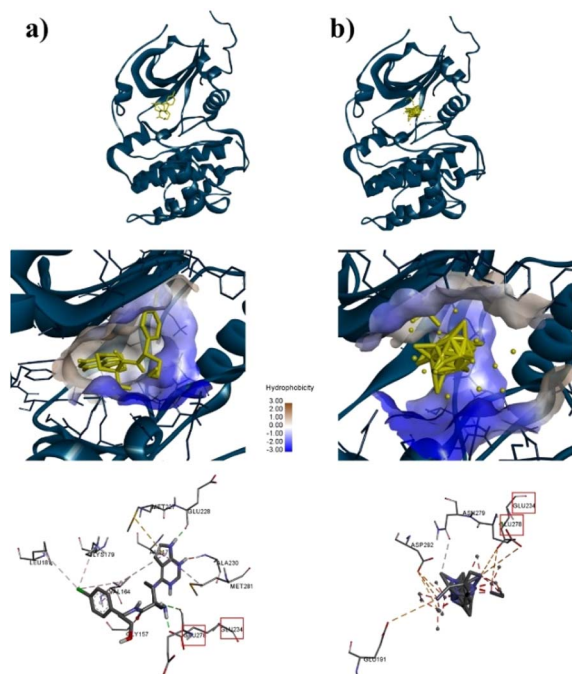


Fig. 6 Interaction between EGFR and (a) MTX-31 or (b) ZIF-8. At the top, EGFR is depicted as a blue-ribbon structure, with ligands shown in yellow. At the centre, a hydrophobicity surface map of the EGFR active site is shown, with the ligands highlighted in yellow. At the bottom, interactions between the ligands and the amino acid residues of the protein are illustrated.

above which binding affinity as same as the native inhibitor. Then, ZIF-8 nanoparticles have comparable interactions with amino acid residues when compared to the control ligand. These interactions play a role in the anticancer pathway by inhibiting AKT-1, MDM2, and EGFR. Suppression of both proteins may result in reduced cell growth and formation of new blood vessels, which can ultimately lead to cell death (Fig. 7). Hence, further *in vitro* study is required to validate the efficacy of the drugs being studied.

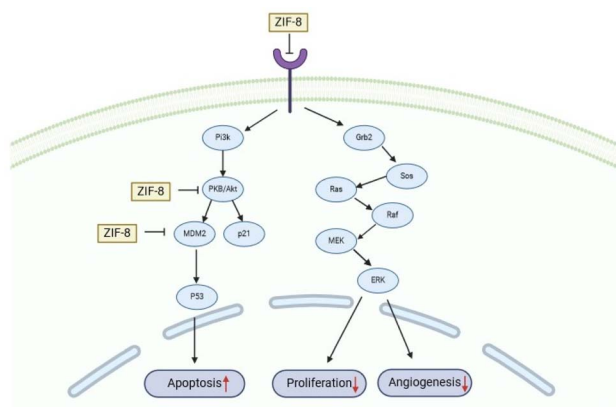


Fig. 7 ZIF-8 role in anticancer pathway through inhibition of AKT-1, MDM2, and EGFR. Inhibition of both proteins may lead to decreased cell proliferation and angiogenesis, which may lead to apoptosis.

Conclusion

The bioactive compound was extracted from the leaves of Meniran (*Phyllanthus niruri* L.) using methanol and successfully identified through LC-HRMS analysis. Subsequently, Meniran was incorporated into ZIF-8 to form nanoparticles, and FTIR and XRD analyses were conducted to confirm the chemical structure. The resulting Meniran-incorporated ZIF-8 nanoparticles successfully maintained their chemical and crystalline structure, compared to pure ZIF-8. Moreover, the shape of Meniran-incorporated ZIF-8 nanoparticles shows well-distribution nanoparticles with rhombic dodecahedrons which provide to internalize towards cancer cells. The Meniran-incorporated ZIF-8 nanoparticles showed rapidly release under acidic environment while slowly release under normal condition. Interestingly, *in vitro* analysis showed that Meniran-incorporated ZIF-8 nanoparticles has anticancer activity towards HeLa cells. To support these results, computational simulations clearly demonstrated that ZIF-8 as nanocarrier has molecular-level interaction with EGFR, AKT-1, MDM-2 under cancer cells. Thus, this study provides new insight to development of bioactive compounds encapsulated into nanoparticles as cancer treatment.

Experimental section

Materials

Phyllanthus niruri (Meniran) was sourced from a local plant in East Java, Indonesia. Zinc nitrate hexahydrate ($\text{Zn}(\text{NO}_3)_2 \cdot 6\text{H}_2\text{O}$, 98%), 2-methylimidazole ($\text{C}_4\text{H}_6\text{N}_2$, 99%) were purchased from Sigma-Aldrich (USA). Ultrapure water, purified using Milli-Q Plus 185 equipment, was consistently utilized in all experimental procedures throughout this study.

Meniran extraction process

Phyllanthus niruri L. (Meniran) leaves were obtained from Mount Lawu at an altitude of 914 masl with coordinates $7^\circ 34'00''\text{S } 111^\circ 13'16''\text{E}$. A total of ± 1 kg of dry leaf powder of Meniran was extracted by maceration method using methanol (1:3 b/v). Extraction was carried out for 1×24 hours and repeated 3 times. The extract of Meniran was concentrated with a rotary vacuum evaporator at 45°C (Buchi Rotavapor R-100).

Synthesis ZIF-8 nanoparticles

ZIF-8 nanoparticles were synthesized following the methodology outlined in a previous report.^{36,37} 2-Methylimidazole (5.67 g) was dissolved in 20 mL of water, while zinc nitrate hexahydrate (0.29 g) was dissolved in 2 mL of water. Subsequently, the aqueous zinc nitrate solution (0.29 g, 2 mL) was added to the aqueous 2-methylimidazole solution and stirred vigorously for 4 h at room temperature. Finally, the milky white precipitates were washed several times with water through centrifugation at 12 500 rpm. The resulting product was then dried in an oven at 40°C for 24 h.

Preparation incorporation of Meniran into ZIF-8 nanoparticle

A mixture of 30 mg of Meniran extract and 10 mg of ZIF-8 in 5 mL of methanol was stirred for 48 h at room temperature, with the vial kept sealed to prevent methanol evaporation. The powder was dried at room temperature for 24 h. The supernatant obtained after centrifugation was used to quantify the amount of Meniran loaded.

Active compound analysis using liquid chromatography high resolution mass spectrometry (LC-HRMS)

LC-HRMS analysis was performed at the Central Laboratory of Life Sciences, Brawijaya University. Sample preparation was carried out by dissolving the combination of extracts in water solvent. The clear extract solution was injected into LC-HRMS (Thermo Scientific Dionex Ultimate 3000 RSLCnano with microflow meter). The mobile phase consisted of (A) 0.1% formic acid in water and (B) 0.1% formic acid in acetonitrile. Chromatographic separation was performed with a Hypersil GOLD aQ analytical column particle size of $50 \times 1 \text{ mm} \times 1.9 \mu\text{m}$ with an analytical flow rate of $40 \mu\text{L min}^{-1}$. The column temperature was set at $40 \text{ }^\circ\text{C}$, and the running time was 30 minutes. The polarity was adjusted to either positive or negative. Full scan at a resolution of 70 000, and data-dependent MS2 was at a resolution of 17 500. Data processing using Compound Discoverer (Thermo Scientific) with McCloud MS/MS Library.

Release of Meniran from Meniran-incorporated ZIF-8 nanoparticles under different pH

A standard release system was prepared in PBS solution at varying pH levels of 7.4 and 5.0. The release system was subsequently maintained at $25 \text{ }^\circ\text{C}$ with continuous stirring, and 3 mL of the release medium was withdrawn at each designated time point. The supernatant was collected through centrifugation and utilized to quantify the concentration of released Meniran using UV-vis spectroscopy with absorbance at 285 nm.

Characterization

X-ray diffraction (XRD). The X-ray diffraction (XRD) patterns were acquired using a Miniflex-600 X-ray diffractometer (Rigaku, Japan) across an angular range of $0\text{--}80$ degrees, utilizing $\text{Cu K}\alpha$ radiation ($\lambda = 1.5419 \text{ \AA}$) at an operating voltage of 30 kV and a current of 10 mA.

Scanning electron microscopy (SEM). Sample solutions were applied onto silicon wafers *via* spin-coating and subsequently examined using a high-resolution field-emission scanning electron microscope (JSM-6500F SEM, JEOL, Tokyo, Japan).

Transmission electron microscopy (TEM). The transmission electron microscope (TEM, JEOL, JEM-2000FXII, Japan) was utilized at an acceleration voltage of 120 kV. For the preparation of the TEM specimen, a sample dispersion was placed onto a carbon-coated copper grid and allowed to dry in air. Finally, the sample was observed by TEM at 200 kV.

Dynamic light scattering (DLS). The hydrodynamic particle size distribution of ZIF-8 and Meniran-incorporated ZIF-8

nanoparticles in were measured using a DLS instrument (Nano Brook 90Plus PALS, Brookhaven, USA).

Brunauer–Emmett–Teller (BET). The Brunauer–Emmett–Teller (BET) surface area and pore volume were assessed at a relative pressure between 0.05 and 0.25.

Cytotoxicity test

HeLa cells were seeded into 96-well plates at a density of 1×10^5 cells per well in 100 μL of medium. The medium was substituted with a fresh one containing pristine ZIF-8 and Meniran-incorporated ZIF-8 at various concentrations, subsequently culture for 24 h. Then, 20 μL of MTT reagent was introduced into each well and incubated for 4 h. Finally, 100 μL of DMSO was added to each well to dissolve the formazan generated by MTT and measured using an ELISA microplate reader.

Computational simulations

Macromolecules and ligands preparation. The macromolecules were used MDM2 and AKT1 proteins, which retrieved from Protein Data Bank (PDB) database (<https://www.rcsb.org/>) with ID 4gv1 for AKT1, 8sc7 for EGFR, and 4oq3 for MDM2. The ligands were used ZIF-8 as nanoparticle, Imidazole as MDM2 inhibitor, MTX-531 as EGFR inhibitor, and AZD5363 as AKT1 inhibitor. The 3D structure of ZIF-8 was construed by ChemDraw, while Imidazole, MTX-531 and AZD5363 were obtained from PDB which linked with the protein.

Molecular docking. Interactions between macromolecules and ligands were examined using AutoDock Vina integrated with PyRx. This docking method was employed to assess binding affinities and to explore molecular mechanisms, following established protocols. The docking process involved treating receptors as rigid and ligands as flexible within the active site. The outcomes of the docking and binding interactions were analyzed using BIOVIA Discovery Studio.

Pathway analysis. Pathway analysis for MDM2, EGFR, and AKT1 was conducted using the Kyoto Encyclopedia of Genes and Genomes (KEGG; <https://www.genome.jp/kegg/>). This database includes various pathways that serve as references for understanding gene or protein functions within a cell.

Data availability

The authors confirm that the data supporting the findings of this study are available within the article and its ESI.† Raw data that support the findings of this study are available from the corresponding author, upon reasonable request.

Conflicts of interest

The authors declare no competing financial interest.

Acknowledgements

This study was supported financially by Ministry of Research, Technology, and Higher Education Republic of Indonesia (DRTPM) (contract no. B/61648/UN38.III.1/LK.04.00/2024).

References

- 1 Y. Octavia, C. G. Tocchetti, K. L. Gabrielson, S. Janssens, H. J. Crijns and A. L. Moens, *J. Mol. Cell. Cardiol.*, 2012, **52**, 1213–1225.
- 2 Y. Cui, J. Sui, M. He, Z. Xu, Y. Sun, J. Liang, Y. Fan and X. Zhang, *ACS Appl. Mater. Interfaces*, 2016, **8**, 2193–2203.
- 3 Y. B. Lim, K. S. Moon and M. Lee, *Chem. Soc. Rev.*, 2009, **38**, 925–934.
- 4 J. S. Lee and J. Feijen, *J. Controlled Release*, 2012, **161**, 473–483.
- 5 Z. Zhang, X. Chen, L. Chen, S. Yu, Y. Cao, C. He and X. Chen, *ACS Appl. Mater. Interfaces*, 2013, **5**, 10760–10766.
- 6 X. Guo, D. Li, G. Yang, C. Shi, Z. Tang, J. Wang and S. Zhou, *ACS Appl. Mater. Interfaces*, 2014, **6**, 8549–8559.
- 7 H. Li, Y. Cui, J. Sui, S. Bian, Y. Sun, J. Liang, Y. Fan and X. Zhang, *ACS Appl. Mater. Interfaces*, 2015, **7**, 15855–15865.
- 8 J. Fang, H. Nakamura and H. Maeda, *Adv. Drug Delivery Rev.*, 2011, **63**, 136–151.
- 9 D. Jiang, W. Mu, X. Pang, Y. Liu, N. Zhang, Y. Song and S. Garg, *ACS Appl. Mater. Interfaces*, 2018, **10**, 37797–37811.
- 10 S. Ganta, H. Devalapally, A. Shahiwala and M. Amiji, *J. Controlled Release*, 2008, **126**, 187–204.
- 11 D. A. T. ATEŞ, *ÖZLEM Turkish Journal of Biology*, 2003, **27**, 157–162.
- 12 W. Nurcholis, B. P. Purwakusumah, E. D. Purwakusumah, T. Katayama and T. Suzuki, *J. Kim. Valensi*, 2012, **2**, 501–510.
- 13 S.-T. Huang, R.-C. Yang, L.-J. Yang, P.-N. Lee and J.-H. S. Pang, *Life Sci.*, 2003, **72**, 1705–1716.
- 14 H.-H. Tseng, P.-N. Chen, W.-H. Kuo, J.-W. Wang, S.-C. Chu and Y.-S. Hsieh, *Integr. Cancer Ther.*, 2011, **11**, 267–278.
- 15 S.-T. Huang, R.-C. Yang, M.-Y. Chen and J.-H. S. Pang, *Life Sci.*, 2004, **75**, 339–351.
- 16 N. Chudapongse, M. Kamkhunthod and K. Poompachee, *J. Ethnopharmacol.*, 2010, **130**, 315–319.
- 17 H.-Y. Wu, T.-K. Lin, H.-M. Kuo, Y.-L. Huang, C.-W. Liou, P.-W. Wang, J.-H. Chuang and S.-T. Huang, *J. Evidence-Based Complementary Altern. Med.*, 2012, **2012**, 925824.
- 18 S. H. Lee, I. B. Jaganath, R. Manikam and S. D. Sekaran, *BMC Compl. Alternative Med.*, 2013, **13**, 271.
- 19 M. Geethangili and S. T. Ding, *Front. Pharmacol.*, 2018, **9**, 1109.
- 20 J. Voigt, *Food/Nahrung*, 1993, **37**, 185.
- 21 W. Liang, P. Wied, F. Carraro, C. J. Sumby, B. Nidetzky, C.-K. Tsung, P. Falcaro and C. J. Doonan, *Chem. Rev.*, 2021, **121**, 1077–1129.
- 22 L. Jiao, J. Y. R. Seow, W. S. Skinner, Z. U. Wang and H.-L. Jiang, *Mater. Today*, 2019, **27**, 43–68.
- 23 H. D. Lawson, S. P. Walton and C. Chan, *ACS Appl. Mater. Interfaces*, 2021, **13**, 7004–7020.
- 24 N. V. de Almeida Ferraz, W. Silva Vasconcelos, C. Santos Silva, S. Alves Junior, C. G. Amorim, M. da Conceição, B. S. M. Montenegro and M. C. da Cunha Areias, *Sens. Actuators, B*, 2020, **307**, 127636.
- 25 J. Rosário, L. L. da Luz, R. Geris, J. G. S. Ramalho, A. F. da Silva, S. A. Júnior and M. Malta, *Sci. Rep.*, 2019, **9**, 7302.
- 26 S. G. F. de Assis, G. C. Santos, A. B. S. Santos, E. H. L. Falcão, R. da Silva Viana and S. A. Junior, *J. Solid State Chem.*, 2019, **276**, 309–318.
- 27 E. Aghazadeh Asl, M. Pooresmaeil and H. Namazi, *Mater. Chem. Phys.*, 2023, **293**, 126933.
- 28 Q. Wang, Y. Sun, S. Li, P. Zhang and Q. Yao, *RSC Adv.*, 2020, **10**, 37600–37620.
- 29 X. Dou, M. Keywanlu, R. Tayebbe and B. Mahdavi, *J. Mol. Liq.*, 2021, **329**, 115557.
- 30 I. B. Vasconcelos, T. G. d. Silva, G. C. G. Militão, T. A. Soares, N. M. Rodrigues, M. O. Rodrigues, N. B. d. Costa, R. O. Freire and S. A. Junior, *RSC Adv.*, 2012, **2**, 9437–9442.
- 31 J. S. F. Silva, J. Y. R. Silva, G. F. de Sá, S. S. Araújo, M. A. G. Filho, C. M. Ronconi, T. C. Santos and S. A. Júnior, *ACS Omega*, 2018, **3**, 12147–12157.
- 32 L. R. de Moura Ferraz, A. É. G. A. Tabosa, D. D. S. da Silva Nascimento, A. S. Ferreira, V. de Albuquerque Wanderley Sales, J. Y. R. Silva, S. A. Júnior, L. A. Rolim, J. J. de Souza Pereira and P. J. Rolim-Neto, *Sci. Rep.*, 2020, **10**, 16815.
- 33 S. Feng, X. Zhang, D. Shi and Z. Wang, *Front. Chem. Sci. Eng.*, 2021, **15**, 221–237.
- 34 C.-Y. Sun, C. Qin, X.-L. Wang, G.-S. Yang, K.-Z. Shao, Y.-Q. Lan, Z.-M. Su, P. Huang, C.-G. Wang and E.-B. Wang, *Dalton Trans.*, 2012, **41**, 6906–6909.
- 35 H. Ren, L. Zhang, J. An, T. Wang, L. Li, X. Si, L. He, X. Wu, C. Wang and Z. Su, *Chem. Commun.*, 2014, **50**, 1000–1002.
- 36 J. Redfern, L. Geerts, J. W. Seo, J. Verran, L. Tosheva and L. H. Wee, *ACS Appl. Nano Mater.*, 2018, **1**, 1657–1665.
- 37 T. Imae, A. Rahmawati, A. M. Berhe and M. A. Kebede, *ACS Appl. Nano Mater.*, 2022, **5**, 16842–16852.
- 38 O. Aung Myo, N. Mohd Nasir Mat, L. Ohn Mar and S. Nordin, *Asian Journal of Medicine and Biomedicine*, 2022, **6**, 17–31.
- 39 D. Tungmunthum, A. Thongboonyou, A. Pholboon and A. Yangsabai, *Medicine*, 2018, **5**, 93.
- 40 N. Q. Nguyen, L. V. Minh, L. H. Trieu, L. M. Bui, T. D. Lam, V. Q. Hieu, T. V. Khang and L. N. Y. Trung, *IOP Conf. Ser.:Mater. Sci. Eng.*, 2020, **736**, 062017.
- 41 A. B. Firdous, G. Sharmila, S. Balakrishnan, P. RajaSingh, S. Suganya, N. Srinivasan and J. Arunakaran, *Food Funct.*, 2014, **5**, 2632–2645.
- 42 J. Lee, J. Lee, W. Sim, J. H. Kim, C. Choi and J. Jeon, *BMB Rep.*, 2023, **56**, 594–599.
- 43 N. Lotfi, Z. Yousefi, M. Golabi, P. Khalilian, B. Ghezlbash, M. Montazeri, M. H. Shams, P. Z. Baghbadorani and N. Eskandari, *Front. Immunol.*, 2023, **14**, 1077531.
- 44 Q. Chen, P. Li, P. Li, Y. Xu, Y. Li and B. Tang, *Oncol. Rep.*, 2023, **49**, 6.
- 45 L. Xing, H. Zheng, Y. Cao and S. Che, *Adv. Mater.*, 2012, **24**, 6433–6437.
- 46 F. Novio, J. Simmchen, N. Vázquez-Mera, L. Amorin-Ferré and D. Ruiz-Molina, *Coord. Chem. Rev.*, 2013, **257**, 2839–2847.
- 47 K. Jiang, L. Zhang, Q. Hu, X. Zhang, J. Zhang, Y. Cui, Y. Yang, B. Li and G. Qian, *Microporous Mesoporous Mater.*, 2019, **275**, 229–234.

- 48 G. Chen, J. Luo, M. Cai, L. Qin, Y. Wang, L. Gao, P. Huang, Y. Yu, Y. Ding, X. Dong, X. Yin and J. Ni, *Molecules*, 2019, **24**, 3369.
- 49 W. Cai, J. Wang, C. Chu, W. Chen, C. Wu and G. Liu, *Advanced Science*, 2019, **6**, 1801526.
- 50 K. Qiu, Y. Shu, J. Zhang, L. Gao and G. Xiao, *Catal. Lett.*, 2022, **152**, 172–186.
- 51 D. W. Lewis, A. R. Ruiz-Salvador, A. Gómez, L. M. Rodríguez-Albelo, F.-X. Coudert, B. Slater, A. K. Cheetham and C. Mellot-Draznieks, *CrystEngComm*, 2009, **11**, 2272–2276.
- 52 M. He, J. Yao, Q. Liu, K. Wang, F. Chen and H. Wang, *Microporous Mesoporous Mater.*, 2014, **184**, 55–60.
- 53 X. Liu, Y. Li, Y. Ban, Y. Peng, H. Jin, H. Bux, L. Xu, J. Caro and W. Yang, *Chem. Commun.*, 2013, **49**, 9140–9142.
- 54 J. Zhuang, C.-H. Kuo, L.-Y. Chou, D.-Y. Liu, E. Weerapana and C.-K. Tsung, *ACS Nano*, 2014, **8**, 2812–2819.
- 55 D. N. Ta, H. K. D. Nguyen, B. X. Trinh, Q. T. N. Le, H. N. Ta and H. T. Nguyen, *Can. J. Chem. Eng.*, 2018, **96**, 1518–1531.
- 56 F.-S. Liao, W.-S. Lo, Y.-S. Hsu, C.-C. Wu, S.-C. Wang, F.-K. Shieh, J. V. Morabito, L.-Y. Chou, K. C. W. Wu and C.-K. Tsung, *J. Am. Chem. Soc.*, 2017, **139**, 6530–6533.
- 57 X. Yu, I. Trase, M. Ren, K. Duval, X. Guo and Z. Chen, *J. Nanomater.*, 2016, **2016**, 1087250.
- 58 M. Ahmadi, M. Khoramjoui, S. Dadashzadeh, E. Asadian, M. Mosayebnia, P. Geramifar, S. Shahhosseini and F. Ghorbani-Bidkorpeh, *J. Drug Delivery Sci. Technol.*, 2023, **81**, 104249.
- 59 M. A. Elaziz, N. S. Abdelrahman, N. A. Hassan and M. O. Mohamed, *Math. Probl. Eng.*, 2022, **2022**, 3029932.
- 60 L. Chibaya, B. Karim, H. Zhang and S. N. Jones, *Proc. Natl. Acad. Sci. U. S. A.*, 2021, **118**, e2003193118.
- 61 Z. Tóthová, M. Šemeláková, Z. Solárová, J. Tomc, N. Debeljak and P. Solár, *Int. J. Mol. Sci.*, 2021, **22**, 7682.
- 62 B. George, B. Gui, R. Raguraman, A. M. Paul, H. Nakshatri, M. R. Pillai and R. Kumar, *Cells*, 2022, **11**, 2290.
- 63 T. L. Wargasetia, H. Ratnawati, N. Widodo and M. H. Widyananda, *Cancer Inf.*, 2021, **20**, 11769351211031864.