Leveraging Chlorination-Based Mechanism for Resolving Subcellular Hypochlorous Acid

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Abstract:

Hypochlorous acid (HOCI) is crucial for pathogen defense, but an imbalance in HOCI levels can lead to tissue damage and inflammation. Existing HOCI indicators employ an oxidation approach, which may not truly reveal the chlorinative stress environment. We designed a suite of indicators with a new chlorinationbased mechanism, termed HOCISense dyes, to resolve HOCI in sub-cellular compartments. HOCISense dyes allow the visualization of HOCI with both switch-on and switch-off detection modes with diverse emission colors, as well as a unique redshift in emission. HOCISense features a minimalistic design with impressive sensing performance in terms of HOCI selectivity, and our design also facilitates functionalization through click chemistry for resolving subcellular HOCI. As a proof of concept, we targeted plasma membrane and lysosomes with HOCISense for subcellular HOCI mapping. With utilizing HOCISense, we discovered the STING pathway-induced HOCI production and the abnormal HOCI production in Niemann-Pick diseases. To the best of our knowledge, this is the first chlorination-based HOCI indicator series for resolving subcellular HOCI.

Introduction

Hypochlorite (HOCI) is a potent reactive oxygen species (ROS) that plays a critical role in the immune response to defend against pathogens. When bacteria invade cells, neutrophils detect the foreign material, elicit a downstream immune response, then capture and break down these materials via NETosis (extracellular) and phagocytosis (intracellular).¹ HOCI is the key component in killing pathogens as it is membrane permeable.² It originates from myeloperoxidase (MPO) in lysosomes, which rapidly catalyzes H_2O_2 and CI^- to produce HOCI.³ During respiratory burst, HOCI is generated to eliminate pathogens through the oxidative and chlorinative mechanisms. The imbalance of HOCI causes oxidative and chlorinative damage to host tissues, responsible for tissue injury and inflammatory diseases, such as rheumatoid arthritis,⁴ cancer,⁵ and atherosclerosis.⁶

To detect and visualize HOCI, existing HOCI indicators have predominantly relied on modulating fluorescence intensity via the oxidation of specific fluorophore motifs, such as pyrroles,^{7,8} thiols,⁹⁻¹¹ oximes/¹²⁻¹⁴ catechols,^{15,16} chalcogens¹⁷⁻¹⁹ and oxidative bond cleavages.²⁰⁻²⁵ In addition to its oxidative properties, HOCI plays a crucial role in chlorinating biomolecules such as amino acids, nucleic acids, lipids, and carbohydrates.²⁶⁻³¹ These chlorination reactions contribute to a form of cellular stress known as chlorinative stress, which can significantly disrupt cellular signaling pathways. This disruption influences critical processes such as cell survival and apoptosis, and modulates immune responses, thereby linking chlorinative stress to inflammation³²⁻³⁴ and age-related diseases.³⁵ This highlights the importance of studying chlorinative stress to better understand its impact on cellular function and disease progression. Existing HOCI indicators employ an oxidation approach that may not truly reveal the chlorinative stress environment.^{31,35,36} A chlorination-based HOCI indicator capable of "capturing" chlorine from HOCI would be ideal for detecting HOCI and chlorinative stress. It also minimizes potential

interference from other ROS or reactive nitrogen species (RNS). However, chlorination-based HOCI detection is challenging because halides are generally known to quench fluorophores,^{37,38} and non-selective chlorination often lead to fluorescence quenching.³⁹

HOCI is a weak acid with a pKa of 7.6, meaning that its equilibrium with hypochlorite ions (OCI⁻) depends on the pH. At pH values below 7.6, the stronger oxidant HOCI predominates, whereas above 7.6, OCI⁻ is predominant, indicating that pH determines which form of HOCI is more prevalent and consequently influences its impact on biomolecules and cells.⁴⁰ On the other hand, cell compartmentalization allows different organelles to maintain distinct internal pH environments, enabling them to carry out specialized functions. Therefore, a HOCI indicator that can selectively label specific cellular compartment for subcellular HOCI imaging is crucial to study the chlorinative stress. However, the cellular distribution of existing HOCI indicators mainly relies on their intrinsic property of the molecules, which might require a lengthy synthetic modification to change the subcellular localization of the HOCI indicators. Furthermore, multi-spectral imaging is often employed in chemical biology where sensors with different emission options are preferred but the existing HOCI indicators lack diverse emission options and fine-tuning capabilities, which limits their practical use in imaging studies. Hence, there is a pressing need for HOCI indicators that can detect HOCI via chlorination, offer emission at different wavelengths, and be functionalized for subcellular imaging to advance studies of HOCI.

This work presents the design and synthesis of a novel series of HOCI indicators, termed HOCISense, which detect HOCI through a unique mechanism involving the chlorination of fluorophores. HOCISense indicators exhibit high selectivity and responsiveness to HOCI, enabling both switch-on and switch-off modes of detection, accompanied by a fluorescence emission redshift. This innovative mechanism confers HOCISense with remarkable versatility, allows tuning of emission properties for multispectral imaging and facilitates functionalization for organelle-selective HOCI imaging. The effectiveness of HOCISense is further demonstrated by its facile synthesis, efficient subcellular targeting, and robust performance across a range of biological applications. The structure-activity relationship study provides critical insights into the detection mechanism, while the ability of HOCISense dyes to monitor HOCI levels has been validated through in-cell HOCI calibration and the assessment of LPS-stimulated HOCI production. HOCISense was also used to investigate the hyper-production of HOCI following PAMPs stimulation in pharmacologically induced NP-A/B and NP-C cell models. Additionally, we observed elevated basal HOCI production in primary cells derived from NP-C patients. These discoveries demonstrate the immediate practical relevance of this tool to the research community for studying chlorinative stress.

Results

Novel HOCI-detecting mechanism of HOCISense detects HOCI through chlorination

BODIPY emerges as a promising dye for cellular imaging due to its notable high brightness and cellular permeability.⁴¹ The photophysical properties of BODIPY with various modifications have been thoroughly investigated.⁴²⁻⁴⁴ It was reported that BODIPY dyes free of substituents at the 2,6-positions can undergo electrophilic substitution reactions in the presence of chlorosulfonic acid, while other electrophiles can be introduced in an analogous manner for further synthetic modification.⁴⁵ For the synthesis of the chlorinated BODIPY, trichloroisocyanuric acid was used for BODIPY chlorination.^{46,47} Trichloroisocyanuric acid serves as a disinfectant, algicide, and bactericide, offering versatility and efficiency in chlorination and oxidation reactions. Similarly, HOCI acts as a primary disinfectant agent and a powerful ROS,

inducing both oxidation and chlorination reactions. Furthermore, the quantum yield and the maximum emission wavelength of BODIPY has been previously observed to change upon 2,6-dichlorination.⁴⁶ We hypothesized that HOCI has the potential to chlorinate BODIPY dye, leading to a red-shift in its fluorescence emission spectrum and change in its quantum yield. In other words, the BODIPY core that free of substituents at the 2,6-positions could function as chlorination-based HOCI-sensing fluorophores.

Firstly, **1a** was synthesized^{46,48} and its ability to detect HOCI was investigated. Upon addition of sodium hypochlorite (NaOCI), which served as the source of HOCI, **1a** exhibited a red-shifted emission in a physiological buffer with its emission wavelength changing from 512 nm to 546 nm (Fig. 1b, Supplementary Figure 40). The fluorescence intensity of **1a** decreased significantly in the presence of HOCI, making **1a** a "Turn-Off" probe for HOCI detection. The UV-Vis absorption spectra also showed the shift in absorption peak maximum from 510 nm to 540 nm, suggesting **1a** reacted with HOCI and formed a new compound with different absorption, causing the red-shift change in excitation and emission (Supplementary Figure 40). The results of high-resolution mass spectroscopy (HRMS) further validate the hypothesis that HOCI can chlorinate **1a** (Supplementary Figure 41). Notably, **1a** can detect HOCI in a pH-independent manner, as evidenced by the fluorescence intensity of **1a** across a pH range of 4 to 8. (Supplementary Figure 42).

To design a HOCI-sensing fluorophore with a fluorescence "Turn-On" signal, this was proceeded by methylating **1a** to form **1b**. It has been reported that the robust fluorescence characteristic of pyridyl-BODIPY, such as **1a**, is suppressed upon protonation or coordination of the pyridine nitrogen atom.⁴⁹⁻⁵¹ Furthermore, the fluorescence intensity of *N*-methylpyridinium BODIPY is significantly quenched due to the photoinduced electron transfer.⁵² Consequently, we hypothesized that **1b** would initially exhibit weak fluorescence and become bright upon chlorination by HOCI. As anticipated, **1b** exhibited weak fluorescence, whereas **1b** demonstrated robust fluorescence with an emission red-shift from 525 nm to 555 nm upon addition of HOCI (Fig. 1b-d, Supplementary Figure 40). Remarkably, the "Turn-On" fluorescence response of **1b**, characterized by a red-shift emission, manifested a higher fold-change (170-fold) when excited at 540 nm as opposed to 490 nm (Supplementary Figure 44).

To develop HOCI-sensing fluorophores with distinct emission wavelengths, *N*-methylated(pyridyl)-BODIPY compounds were synthesized with different pyridyl groups at the 8-position of the BODIPY chromophore (**2a–3b**, Fig. 1a). Both **2a** and **3a** exhibited an emission of around 515 nm and a "Turn-Off" response towards HOCI, which is similar to that of **1a** (Supplementary Figure 40). Upon addition of HOCI, the emissions of **2a** and **3a** decreased significantly and red-shifted. **2b** displayed an emission shift from 537 nm to 555 nm with a reasonable increase in fluorescence. Notably, **3b** displayed an emission at 594 nm, which shifted to 600 nm with enhanced emission in the presence of HOCI (Fig. 1b, Supplementary Figure 40). In other words, by replacing the pyridyl group at the 8-position of the BODIPY chromophore from *meso-(N*-methyl-3-pyridyl)-BODIPY (**2b**) to *meso-(N*-methyl-4-pyridyl)-BODIPY (**3b**), the emission of the HOCI-sensing fluorophore was tuned to the orange emission range. These results demonstrate that the novel HOCI detection mechanism not only enables both switch-off and switch-on modes of detection but also offers diverse emission options suitable for multispectral imaging, with the emission shift response further enhancing the signal-to-noise ratio for improved detection sensitivity.

in vitro characterization of HOCI-sensing fluorophore

Among all the dyes evaluated, **1b** showed the highest emission change with the bathochromic shift of around 30 nm upon reaction with HOCI in the testing conditions, compared to **2b** with around 18 nm emission red-shift and **3b** with *ca*. 6 nm emission red-shift. **1b** also showed fast kinetic response to HOCI,

responding within minutes (Supplementary Figure 43, video S1). Hence, **1b** was chosen for further characterization due to the favorable fluorescent change. As seen in the fluorescence intensity of the titration curve (Fig. 1c-d, Supplementary Figure 44), **1b** showed gradual fluorescence enhancement with an excitation of 490 nm. To confirm that the emission enhancement of **1b** is triggered by HOCI, ROS scavengers were added. The emission enhancement of **1b** in the presence of HOCI was significantly reduced when *N*-acetyl cysteine, GSH, GSSG, and NADPH were introduced, as the majority of the highly oxidizing HOCI reacted with these biologically relevant reductants (Fig. 1e, Supplementary Figure 45). The impact of physiological ions on **1b** was also investigated. The HOCI detecting ability of **1b** was not affected by the presence of physiological ions (Na⁺, K⁺, Ca²⁺, Mg²⁺) and trace ions (Zn²⁺, Mn²⁺, and Cu²⁺), but was greatly reduced in the presence of ferrous ions (Fe²⁺), which was possibly due to the Fenton type redox reactions (Fig. 1f, Supplementary Figure 46).^{53,54} **1b** recognized HOCI and exhibited a high fluorescence in physiological pH range 4.0–7.0, which is useful for HOCI detection in different cellular organelles (Fig. 1g, Supplementary Figure 47).

There are numerous types of ROS produced in cells. ROS/RNS are known for their high reactivity with short lifetimes⁵⁵ which could cause quenching of fluorophores or no response. Therefore, a selective HOCI indicator is important to study HOCI-involved biological processes. The peak-to-peak emission was enhanced by about 150-fold in the presence of HOCI upon 540 nm excitation while the other ROS/RNS (including H_2O_2 , O_2 , D_2 , $^{t}BuOOH$, 'OH, 'NO, ROOR', ROO' and ONOO') showed no fluorescence enhancement and no bathochromic shift. These results indicate that our design in **1b** achieved a high selectivity towards HOCI and displayed a unique emission red-shift of 30 nm from original 525 nm to 555 nm (Fig. 1h, Supplementary Figure 48).

Validation of new HOCI detection mechanism

NMR titration was performed to further validate the HOCI detecting mechanism of 1b. The NMR titration of **1b** showed a gradual downfield shift (labeled as proton e in Fig. 2a) of β -hydrogen at the 2,6-positions of the pyrrole moiety from ~6.7 ppm to ~7.0 ppm after the addition of HOCI. The peak integration decreased from two to one (Fig. 2a), as the structure transitioned from the non-chlorinated reactant (labeled as proton e) to mono-chlorinated product (labeled as proton e'), suggesting the substitution of the β -hydrogen on pyrrole by a electron-withdrawing CI atom. As **1b** and its reaction product with HOCI contain a +1 charge, HRMS served as an effective way to verify the detection mechanism. The reaction mixture showed the peaks $[M-H+CI]^+$ with m/z = 374.1403 and $[M-2H+2CI]^+$ with m/z = 408.1015, corresponding to mono-chlorinated product and di-chlorinated product respectively (Fig. 2b-c). Similar chlorination products were also observed in the other two methylated BODIPYs 2b and 3b (Supplementary Figure 49) as well as the non-methylated BODIPYs 1a, 2a and 3a (Supplementary Figure 41). In addition, the m/z peaks corresponding to the **1b** remained unchanged in the presence of both HOCI and the scavengers (Supplementary Figure 50). The results of the HRMS and NMR data are consistent with the proposed HOCI detecting mechanism that HOCI chlorinates the BODIPY core of 1ab, 2a-b and 3a-b, leading to a red-shift in its fluorescence emission spectrum and a change in its quantum yield.

To further understand the design principles of this new class of HOCI-sensing fluorophores, several structures with variations at the 2,6-positions were synthesized to mask the β -hydrogens on the pyrroles. The HOCI detecting ability of these variations (**1c**-**f**) were investigated to determine the structure-activity relationship. The β -hydrogen were replaced by ethyl substituents, resulting in the formation of disubstituted **1d** and mono-substituted **1f**. When the β -hydrogen on pyrroles were absent in **1d**, addition of

HOCI resulted in disappearance of the characteristic BODIPY absorption peak. (Supplementary Figure 40). HRMS analysis of the reaction mixture (**1d** with HOCI) suggested structural decomposition including demethylation and non-selective chlorination (Supplementary Figure 51). In such way, the d-PeT is not able to switch off and results in fluorescence quenching. For mono-substituted **1f**, the reaction mixture showed a peak corresponding to the chlorinated product $[M-H+CI]^+$ with m/z = 402.1719 (Supplementary Figure 52). These results demonstrate that the β -hydrogens at the 2,6-positions of the pyrrole core can direct a selective chlorination to produce the characteristic "Turn-On, red-shift" fluorescence response. In other words, the absence of substituents at the 2- or 6-positions of the BODIPY core in **1b** is essential for HOCI-induced chlorination, which subsequently alters the emission wavelength and fluorescence intensity of **1b**.

in cellulo HOCI calibration of HOCISense dyes

HOCISense dyes were assessed for their effect on cell viability. 1a, 1b, and 3b exhibited almost no cytotoxicity up to 100 µM (Supplementary Figure 53). These dyes were selected for cell imaging applications based on their favorable fluorescence response, high specificity towards HOCI, and minimal cytotoxicity. RAW 264.7 cells were incubated with the dyes for 30 min (referred to as the 'pulse'), washed the cells, and then allowed them to grow in complete medium for 1 h (referred to as the 'chase'). The fluorescence intensity of 1b-labeled cells was significantly higher than that of the unlabeled cells. The uptake experiment results demonstrated that **1b** effectively labeled RAW 264.7 cells (Supplementary Figure 54). The intracellular HOCI-sensing abilities of 1a, 1b, and 3b in HOCI-clamped RAW 264.7 cells were then investigated (Supplementary Figure 55). Upon cell fixation, the dyes distributed throughout the cytosol. The intracellular HOCI calibration result is consistent with the *in vitro* experiments, showing a dose-dependent response to [HOCI] for 1a, 1b, and 3b (Fig. 2d-e, Supplementary Figure 56-58). The fluorescence intensity of 1b- and 3b- labeled cells increased with increasing concentration of clamped HOCI. Conversely, 1a detected HOCI with a "Turn-Off" response, as the intracellular fluorescence intensity decreased with increasing [HOCI]. These results indicate that 1a, 1b, and 3b, which detect HOCI through a novel chemical mechanism, are capable of monitoring intracellular HOCI production at physiological concentrations (20 to 400 µM).56,57

Functionalization of HOCISense dyes for extracellular HOCI detection

The pyridinium design of HOCISense dyes also supported chemical functionalization, as the pyridine of HOCISense dyes was PEGylated with azide-PEG₃-iodide through an S_N2 reaction to form **1b-azide** (Fig. 3d). The resulting **1b-azide** was conjugated with different organelle-targeting groups or carriers through strain-promoted azide-alkyne cycloaddition. This modification did not extensively alter the pyridinium BODIPY structure, and the conjugation by click reaction did not significantly affect the fluorescence characteristics of HOCISense dyes. For proof of concept, we targeted the plasma membrane with HOCISense to evaluate extracellular HOCI exposure as HOCI serves as a biomarker for chronic inflammatory conditions,⁵⁸ and elevated extracellular levels of HOCI have been associated with necrotic cell death.⁵⁷ A reported plasma-membrane-labeling ligand **mb**^{59,60} was utilized to prepare **DBCO-mb**, a ligand for efficient labeling via click reaction. **mb** was confirmed to target the plasma membrane, guiding the BODIPY dye to specifically label the membrane instead of the entire cell (Fig. 3b-c, Supplementary Figure 59a-d). By clamping the cells with HOCI, it was shown that **1b-mb** effectively detects HOCI around the membrane, consistent with in-cell HOCI calibration of **1b** (Fig. 3f, Supplementary Figure 60-61). PAMPs, including lipopolysaccharides (LPS) and phorbol 12-myristate 13-acetate (PMA), are known to induce HOCI production. By incubating LPS and PMA with RAW 264.7 macrophages, we successfully

employed **1b-mb** to monitor the resultant HOCI levels, demonstrating the probe's efficacy in detecting extracellular HOCI. A significantly higher pseudo-color intensity was observed across the cell membrane when the cells were stimulated with PAMPs (Fig. 3e-g, Supplementary Figure 62). These results demonstrated that **1b-mb** could monitor the extracellular HOCI exposure of the plasma membrane.

Functionalization of HOCISense dyes for lysosomal HOCI detection

MPO is localized in lysosomes, which are central to various metabolic pathways. Elevated HOCI levels in lysosomes are associated with numerous diseases and may reflect cellular integrity and functionality. Therefore, measuring lysosomal HOCI levels, without triggering an immune response, can serve as a valuable indicator of lysosomal integrity and overall cellular health. To detect lysosomal HOCI production without stimulating the immune response, **1b** was conjugated to 10k molecular weight dextran (Fig. 4a), which can be taken up by cells through fluid-phase endocytosis and reach the endolysosomes (Fig. 4b).⁶¹⁻ ⁶³ Dextran-1b was prepared via a two-step functionalization and click chemistry (Fig. 4a). The DBCO linker was conjugated to amino-dextran to form **DBCO-dextran**, and then conjugated it with **1b-azide** to form dextran-1b. Using dextran-1b, we measured lysosomal HOCI production in RAW 264.7 cells following PAMP stimulation and observed an increase in lysosomal fluorescence intensity. To confirm that this increase was due to MPO-produced HOCI, cells were treated with 50 µM MPO inhibitor aminobenzoic acid hydrazide (4-ABAH). The decreased lysosomal fluorescence intensity upon inhibitor treatment confirmed that the fluorescence increase was due to MPO-dependent HOCI production (Fig. 4c-d). After validating the lysosomal HOCI-monitoring ability of dextran-1b, we aimed to determine if the STING pathway induces HOCI production, given that STING pathway is a key component of the innate immune system that recognizes bacterial secondary messengers and has recently been implicated in various neurodegenerative diseases.⁶⁴ Upon STING activation with DMXAA, a significant increase in lysosomal fluorescence intensity was observed (Fig. 4e-f). Cells pre-treated with H-151, a potent STING antagonist that inhibits STING palmitoylation, showed a reduction in **dextran-1b** signal. This reduction indicates that the increased signal is directly attributable to STING activation. The observed HOCI generation upon STING activation highlights a compelling correlation between the STING signaling axis and the resulting HOCI production.

Basal HOCI production in Niemann–Pick diseases

Niemann-Pick (NP) disease is a lysosomal storage disorder sub-classified into three types: A, B, and C. Types A and B are caused by mutations of acid sphingomyelinase (ASM), while type C results from mutations of NPC1 or NPC2 protein.^{62,65} These mutations lead to abnormal accumulation of lysosomal cargos. Elevated ROS levels is also observed in NP phenotype cells due to altered mitochondrial and peroxisomal function.⁶⁶ Therefore, dextran-1b was utilized to assess the lysosomal HOCI level in Niemann-Pick diseases. To prepare the pharmacologically induced NP-A/B and NP-C cell models, cells were pre-incubated with amitriptyline hydrochloride (AH) and U18666A, which are inhibitors of ASM and NPC1, respectively, to mimic the deficiency of these lysosomal proteins. Without any PAMPs stimulation, the lysosomal HOCI levels in both NP-A/B and NP-C models were higher than those in WT cells (Fig. 5ab). The NP-A/B model exhibited a two-fold increase in lysosomal fluorescence intensity, while the NP-C model displayed a four-fold increase in lysosomal fluorescence intensity. Upon PAMPs stimulation, enhanced lysosomal fluorescence intensity was observed in both NP-A/B and NP-C models, with a marked hyperproduction of HOCI in the NP-C model (Fig. 5a-b). Based on the results from the NP cell models, whether patient samples exhibit elevated basal levels of HOCI production was investigated. Dextran-1b was utilized to evaluate the HOCI level of primary cells derived from normal healthy individuals and NP-C patients. Our results showed that NP-C patient fibroblasts had a higher average HOCI level than normal healthy individuals (Fig. 5c-d) and these results were consistent with the observed elevated basal HOCI production in the pharmacologically induced NP-A/B and NP-C cell models. Given that inflammation is a significant driver of NPC pathology, this previously unreported basal HOCI production provides novel insights into the mechanisms underlying the disease.

Discussion

Through a strategic methylation/alkylation design, we effectively overcame four critical challenges simultaneously, providing robust and precise chemical tools for resolving subcellular HOCI. The water solubility of pyridyl BODIPYs was greatly enhanced through the methylation/alkylation because of bearing +1 charge. After the methylation/alkylation, the fluorescence of pyridinium BODIPYs (**1b**, **2b** and **3b**) switched to a "turn-on" response towards HOCI based on the d-PeT mechanism while most fluorophores including pyridyl BODIPY (**1a**, **2a** and **3a**) feature a "turn-off" response. In addition, the extended glycol linker in **1b-azide** facilitated easy functionalization, enabling the installation of organelle-targeting properties. As a result, membrane-targeting **1b-mb** and lysosome-targeting **dextran-1b** were successfully prepared and demonstrated for subcellular HOCI imaging. Finally, changing the *N*-methylated-3-pyridyl group to *N*-methylated-4-pyridyl group at the 8-position of the BODIPY shifted the emission of the HOCI-sensing fluorophores from yellow to orange. Furthermore, it is noteworthy that fluorescence 'turn-on' response with a peak shift is particularly useful for imaging, as it enables the monitoring of fluorescence intensity at the shifted emission peak, resulting in minimal background signal in the absence of the target analyte and a significantly higher fold change upon its presence (Supplementary Figure 45).

The new chlorination-based HOCI detection mechanism allows us to have a universal method to functionalize the developed HOCISense dyes for subcellular imaging. For proof of concept, we targeted plasma membrane and lysosomes with HOCISense for monitoring extracellular HOCI exposure and lysosomal HOCI production. The capability of HOCISense for subcellular HOCI mapping was also demonstrated by monitoring PAMPs-induced lysosomal HOCI. The lysosomal HOCI production upon STING pathway activation was then visualized, marking the first report of STING signaling-induced HOCI production. It demonstrated the capability of HOCISense dyes to monitor HOCI distribution, enabling the study of its impact on various cellular compartments.

HOCI overproduction was also observed in Niemann–Pick disease samples using our lysosome-labeling HOCI indicator. Our findings indicate that hyper-HOCI-production is present in pharmacologically induced NP-A/B and NP-C cell models upon PAMPs stimulation. Additionally, an increased basal HOCI production was detected even in the absence of PAMPs stimulation, a phenomenon also observed in primary cells from NPC patients. To the best of our knowledge, this is the first report of abnormal higher HOCI basal level in NP diseases. These findings suggest that elevated basal HOCI production may contribute to the pathology of Niemann–Pick disease. Given that inflammation is a significant driver of NPC pathology,^{67,68} this unreported basal HOCI production provides novel insights into the mechanisms underlying the disease.

In conclusion, a series of HOCISense dyes were developed and featured a novel chlorination-based detection mechanism. It is promising that the minimalistic design of HOCISense dyes also allows for tuning the emission, adjusting detection mode and functionalizing at the same time, which greatly shortens the time for synthesis and further modification. All these properties make these dyes ideal for multispectral imaging. Structural activity relationship of HOCISense dyes was studied and we discovered that β -hydrogen on the pyrrole of BODIPY is essential for the directed chlorination by HOCI. The strategic

alkylation design is beneficial to modulate the cellular distribution of HOCISense by click conjugation. As a proof of concept, we targeted plasma membrane and lysosomes with HOCISense for monitoring extracellular HOCI exposure and lysosomal HOCI production. Our tools successfully monitor the PAMPsinduced extracellular and lysosomal HOCI, find out the HOCI production induced by STING activation, and discovered the elevated basal HOCI production in drug-induced NP disease cell models and primary fibroblast samples from NP patients.

Declaration of interests

The authors declare no competing financial interests.

Resources availability

We are delighted to provide our developed tools upon request.

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Author contributions

F.T., L.T., and K.L. wrote the manuscript. F.T., L.T., wrote the supporting information with the input of all authors. All authors discussed the results and commented on the manuscript. F.T., L.T., and K.L. designed the project. Compounds **1a-1f**, **2a-b**, **3a-b**, **1b-N**₃ were synthesized by F.T., L.T., N.P., and M.S. **DBCO-NHS**, **DBCO-mb** were synthesized by M.R.N. and M.A. The *in vitro* characterization, NMR titration, mass spectrometry, cellular distribution, *in cellulo* HOCI clamping, HOCI imaging were performed by F.T. and L.T. HOCI production during STING activation was evaluated by C.H. J.M performed the cell viability assay and provide imaging supporting.

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Figure 1. HOCISense dyes, a series of selective HOCI indicators with diverse emission options and detection mode.

a, Molecular structure of HOCISense dyes.

b, Multispectral fluorescent response of HOCISense dyes (1a, 1b, 2b, and 3b) to HOCI.

c, Emission spectra of **1b** (5 μ M) in the presence of HOCI (0–8 equiv.). Conditions: water containing 0.5% DMF, λ_{ex} = 490 nm.

d, Fluorescence intensity of **1b** (5 μ M) in the presence of HOCI (0–8 equiv.). Conditions: water containing 0.5% DMF, λ_{ex} = 490 nm, λ_{em} = 560 nm.

e, Fluorescence intensity at 560 nm of **1b** (5 μ M) in the presence of various ROS scavengers (300 μ M *N*-Acetyl Cysteine, 1 mM GSH, 1mM GSSG and 100 μ M NADPH) with and without HOCI (10 equiv.). Conditions: water containing 0.5% DMF, λ_{ex} = 540 nm, λ_{em} = 560 nm.

f, Fluorescence intensity of **1b** (5 μ M) in the presence of different metal ion (20 μ M for Mn²⁺, Fe²⁺, Co²⁺, Ni²⁺, Cu²⁺, Zn²⁺, and 100 mM for Na⁺, K⁺, Ca²⁺, Mg²⁺) with and without HOCI (10 equiv.). Conditions: water containing 0.5% DMF. λ_{ex} = 490 nm, λ_{em} = 560 nm.

g, Fluorescence intensity of **1b** (5 μ M) at 560 nm in the presence and absence of HOCI (10 equiv.) at different pH. Conditions: citrate-phosphate buffer (10 mM) containing 0.5 % DMF, λ_{ex} = 490 nm, λ_{em} = 560 nm, n = 3.

h, Fluorescence intensity of **1b** (5 μ M) in the presence of different ROS/ RNS (10 equiv.) with and without HOCI (10 equiv.). Photo taken under UV light. Conditions: phosphate buffer (60 mM, pH 7.2) containing 0.5% DMF, λ_{ex} = 540 nm, λ_{em} = 560 nm.

Error bars indicate the mean ± standard error of mean (s.e.m.) of three independent measurements.



Figure 2. HOCISense detects HOCI based on fluorophore chlorination.

a, **1b** undergoes chlorination with HOCI. Stacked ¹H NMR spectrum for **1b** with the titration of increasing amounts of NaOCI.

b–**c**, Mass spectral characterization of HOCI chlorinated products from **1b**. Diagram of HRMS (+ve ESI) spectrum of **1b** after the addition of HOCI, showing the **b**, chlorination and **c**, dichlorination reaction product.

d, In-cell HOCI calibration. Representative fluorescence images of **1b**-labelled RAW 264.7 cells clamped at the indicated [HOCI].

e, Histogram for the whole cell intensity of 1b-labeled cells at the indicated [HOCI].

Imaging experiments were performed in triplicate.



Scale = 20 µm

Figure 3. Functionalization of HOCISense dye for plasma membrane labeling and extracellular HOCI mapping.

a, Structures for BODIPY-azide and BODIPY-mb.

b-c, Representative fluorescence images of RAW 264.7 cells labeled with **BODIPY-azide** or **BODIPY-mb** respectively.

d-f, Functionalization of 1b for plasma membrane labeling.

d, Synthesis scheme of **1b-mb**.

f, In-cell HOCI calibration. Representative fluorescence images of **1b-mb**-labelled cells clamped at the indicated [HOCI].

e, Schematic diagram illustrating 1b-mb response to HOCI.

g, **1b-mb** detects PAMP-stimulated HOCI production. Representative fluorescence image of **1b-mb**-labelled RAW 264.7 cells upon stimulation of LPS and PMA.

Experiments were performed in triplicate.



Figure 4. Functionalization of HOCISense dyes for lysosomal HOCI imaging.

a, Synthesis scheme of **dextran-1b**. By reacting the **1b-azide** with DBCO-functionalized amino dextran, **dextran-1b** is synthesized, combining the fluorescent properties of **1b** with the lysosome-labeling capabilities of dextran.

b, Trafficking of **dextran-1b** through endocytosis pathway (EE, early endosome; LE, late endosome; LY, lysosome).

c-d, dextran-1b detects PAMP-stimulated lysosomal HOCI production.

c, Representative fluorescence images of **dextran-1b**-labelled RAW 264.7 cells showing the enhanced fluorescence intensity upon PMAPs stimulation while the enhanced signal was reduced upon treatment of MPO inhibitor 4-ABAH.

d, Quantification of endolysosomal fluorescence intensity of **dextran-1b**-labelled RAW 264.7 cells at the indicated conditions.

Experiments were performed in triplicate. The median value of each trial is given by a square, circle, and triangle symbol (n = number of lysosomes).

e-f, STING activation induces HOCI production.

e, Representative fluorescence images of **dextran-1b**-labelled RAW 264.7 with or without murine STING stimulator dimethylxanthenone acetic acid (DMXAA, 30 μ M) and STING inhibitor H151 (15 μ M).

f, Quantification of whole cell fluorescence intensity of **dextran-1b**-labelled RAW 264.7 cells at the indicated conditions.

Experiments were performed in triplicate. The median value of each trial is given by a square, circle and triangle symbol, and median of whole experiment represented by line (n = number of cells).



Figure 5. HOCISense dye detects the basal lysosomal HOCI production in Niemann–Pick diseases.

a-b, HOCISense dyes detects basal lysosomal HOCI production in pharmacologically induced NP A/B and C cell models.

a, Representative fluorescence images of **dextran-1b**-labelled RAW 264.7 cells treated with 65 µM amitriptyline (AH) or 20 µM U18666A with and without stimulation of LPS and PMA.

b, Quantification of lysosomal fluorescence intensity in indicated condition.

c-d HOClSense dye detects the basal lysosomal HOCl production in primary skin fibroblast divided from NP-C patients.

c, Representative fluorescence images of **dextran-1b**-labeled primary skin fibroblast from apparently healthy individuals and NP-C patients.

d, Quantification of lysosomal fluorescence intensity of fibroblast samples from apparently healthy individuals and NP-C patients.

Experiments were performed in triplicate for each cell line sample. The median value of each trial is given by square, circle, and triangle symbols. Error bars indicate the mean \pm standard error of the mean (s.e.m.) of nine independent measurements. ****P* < 0.001. One-way analysis of variance (ANOVA) followed by Dunnett's test for multiple comparison.