

## Research Article

# Molecular Imaging, Pharmacokinetics, and Dosimetry of $^{111}\text{In}$ -AMBA in Human Prostate Tumor-Bearing Mice

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Molecular imaging with promise of personalized medicine can provide patient-specific information noninvasively, thus enabling treatment to be tailored to the specific biological attributes of both the disease and the patient. This study was to investigate the characterization of DO3A-CH<sub>2</sub>CO-G-4-aminobenzoyl-Q-W-A-V-G-H-L-M-NH<sub>2</sub> (AMBA) *in vitro*, MicroSPECT/CT imaging, and biological activities of  $^{111}\text{In}$ -AMBA in PC-3 prostate tumor-bearing SCID mice. The uptake of  $^{111}\text{In}$ -AMBA reached highest with  $3.87 \pm 0.65\%$  ID/g at 8 h. MicroSPECT/CT imaging studies suggested that the uptake of  $^{111}\text{In}$ -AMBA was clearly visualized between 8 and 48 h postinjection. The distribution half-life ( $t_{1/2\alpha}$ ) and the elimination half-life ( $t_{1/2\beta}$ ) of  $^{111}\text{In}$ -AMBA in mice were 1.53 h and 30.7 h, respectively. The  $C_{\max}$  and AUC of  $^{111}\text{In}$ -AMBA were 7.57% ID/g and 66.39 h\*% ID/g, respectively. The effective dose appeared to be 0.11 mSv/MBq<sup>-1</sup>. We demonstrated a good uptake of  $^{111}\text{In}$ -AMBA in the GRPR-overexpressed PC-3 tumor-bearing SCID mice.  $^{111}\text{In}$ -AMBA is a safe, potential molecular image-guided diagnostic agent for human GRPR-positive tumors, ranging from simple and straightforward biodistribution studies to improve the efficacy of combined modality anticancer therapy.

## 1. Introduction

Prostate cancer is estimated to rank first in number of cancer cases and second in number of deaths due to cancer among men in the Western world [1]. Gastrin-releasing peptides (GRPs), including Bombesin-like peptides (BLPs), are involved in the regulation of a large number of biological processes in the gut and central nervous system (CNS) [2]. They mediate their action on cells by binding to members of a superfamily of G protein-coupled receptors [3]. There are four known subtypes of BN-related peptide receptors, namely, gastrin-releasing peptide receptor (GRPR, BB2, BRS-2), neuromedin B receptor (NMBR, BB1, BRS-1), orphan receptor (BRS-3), and amphibian receptor (BB4-R) [4]. Except the BB4-R, all the receptors were widely distributed, especially in the gastrointestinal (GI) tract and central nervous system (CNS). The receptors have a large range of effects in both normal physiology and pathophysiological conditions [5]. GRPRs are normally

expressed in nonneuroendocrine tissues of the pancreas, breast, and neuroendocrine cells of the brain, GI tract, lung, and prostate, but are not normally expressed by epithelial cells in the colon, lung, or prostate [6, 7].

Molecular imaging enables the visualization of the cellular function and the followup of the molecular process in living organisms without perturbing them [8]. The radionuclide molecular imaging technique is the most sensitive and can provide target-specific information. The radiotracer could also be used for radionuclide therapy. Thus, the development of a personalized theranostic (image and treat) agent would allow greater accuracy in selection of patients who may respond to treatment, and assessing the outcome of therapeutic response [9]. Gastrin-releasing peptide receptors (GRPRs) are overexpressed in several primary human tumors and metastases [5]. Markwalder and Reubi reported that GRPRs are expressed in invasive prostate carcinomas and in prostatic intraepithelial neoplasms at high

density, whereas normal prostate tissue and hyperplastic prostate tissue were predominantly GRPR negative [10]. These findings suggest that GRPR may be used as a molecular basis for diagnosing and staging prostate cancer, further for imaging-guided personalized medicine using radiolabeled bombesin analogues.

Previous studies have evaluated the  $^{111}\text{In}$ -radiolabeled BN analogues which bind rapidly into GRP receptor-positive tumor cells, including PC-3, CA20948, and AR42J using gamma camera imaging after administration [11–14]. AMBA (DO3A-CH<sub>2</sub>CO-G-(4-aminobenzoyl)-QWAVGHLM-NH<sub>2</sub>) (Figure 1), a BBN-related peptide agonist, has a DO3A structure that can chelate tripositive lanthanide isotopes, such as  $^{68}\text{Ga}$ ,  $^{90}\text{Y}$ ,  $^{111}\text{In}$ , and  $^{177}\text{Lu}$ . Thus, it can formulate many kinds of radiolabelled probes for various purposes [15]. Indium 111 emits  $\gamma$ -photons of two energies (172 and 245 keV) as well as Auger and internal conversion electrons.  $^{111}\text{In}$ -AMBA was initially used for diagnostic purposes but remains the potential for radiotherapy. Auger electron, with a maximum energy of <30 keV, is a high linear energy transfer (LET) radiation with subcellular pathlength (2–500 nm) in tissues [16]. For imaging the presence or absence of GRPR, the  $^{111}\text{In}$ -AMBA could be used for patient selection for further radiotherapy ( $^{177}\text{Lu}$ -AMBA), chemotherapy (BLP antagonists), or therapeutic response monitoring as imaging-guided personalized medicine. Although  $^{111}\text{In}$ -AMBA has been evaluated as an imaging agent [17–20], the pharmacokinetics and dosimetry of the agent have not been reported yet. In this study,  $^{111}\text{In}$ -AMBA was designed as an image-guided diagnostic agent for human GRPR-positive tumors, which only retain the last eight amino acids (Q-W-A-V-G-H-L-M-NH<sub>2</sub>) from native BN. The pharmacokinetics, biodistribution, dosimetry, and micro-SPECT/CT imaging of  $^{111}\text{In}$ -AMBA were evaluated in human androgen-independent PC-3 prostate tumor-bearing SCID mice.

## 2. Materials and Methods

**2.1. Chemicals.** Protected N $^{\alpha}$ -Fmoc-amino acid derivatives were purchased from Calbiochem-Novabiochem (Laufelfingen, Switzerland), Fmoc-amide resin and coupling reagent were purchased from Applied Biosystems Inc. (Foster City, CA, USA), and DOTA-tetra (tBu) ester was purchased from Macrocylics (Dallas, TX, USA). Fmoc-4-abz-OH was obtained from Bachem (Chauptstrasse, Switzerland). Bombesin was purchased from Fluka (Buchs, Switzerland).

**2.2. Synthesis of AMBA.** AMBA was synthesized by solid phase peptide synthesis (SPPS) using an Applied Biosystems Model 433A full automated peptide synthesizer (Applied Biosystems, Foster City, CA, USA) employing the Fmoc (9-fluorenylmethoxy-carbonyl) strategy. Carboxyl groups on Fmoc-protected amino acids were activated by (2-( $^1\text{H}$ -benzotriazol-1-yl)-1,1,3,3-tetramethyluronium hexafluorophosphate (HBTU), forming a peptide bond with the N-terminal amino group on the growing peptide, anchored *via* the C-terminus to the resin, provided

for stepwise amino acid addition. Rink Amide resin (0.25 mmole) and Fmoc-protected amino acids (1.0 mmole), with appropriate side-chain protections, and DOTA-tetra (tBu ester) were used for SPPS of the BBN conjugates. Side chain protecting groups in the synthesis were Trt for Gln and His, and Boc for Trp.

The protected peptide-resin was cleaved and deprotected with mixture of 50% trifluoroacetic acid (TFA): 45% chloroform, 3.75% anisole, and 1.25% 1, 2-ethanedithiol (EDT) for 4 h at room temperature (RT). The crude peptide was isolated by precipitating with cool diethyl ether. After centrifugation, the collected precipitate was dried under vacuum. The crude peptide sample was purified by reverse phase high-performance liquid chromatography (HPLC) using a column of XTerra prep, MSC18, 5  $\mu\text{m}$ , 18  $\times$  50 mm (Waters Corp., MA, USA) with an acetonitrile/water gradient consisting of solvent A (0.1% TFA in H<sub>2</sub>O) and solvent B (0.1% TFA in acetonitrile), with a 14.8% yield; flow: 6 mL/min; gradient: 20%–40% B for 20 min. The molecular weight was determined with a MALDI-TOF Mass Spectrometer (Bruker Daltonics Inc, Germany). *M/z* determined for the peptide was AMBA, 1,502.6 [M+H].

**2.3. Radiolabeling of  $^{111}\text{In}$ -AMBA.** AMBA was radiolabeled with  $^{111}\text{In}$  as previously described by Zhang et al. [21]. Briefly, AMBA was labeled with  $^{111}\text{In}$  ( $^{111}\text{InCl}_3$ , Institute of Nuclear Energy Research (INER), Taoyuan (Taiwan), 16430 MBq/mL in 0.05 N HCl, pH 1.5–1.9) by reaction of  $6.66 \times 10^{-4}$   $\mu\text{mole}$  (1  $\mu\text{g}$ ) peptide in 95  $\mu\text{L}$  0.1 M NH<sub>4</sub>OAc (pH 5.5) with 64.75 MBq  $^{111}\text{InCl}_3$  in 5  $\mu\text{L}$  0.04 N HCl for 10 min at 95°C. The specific activity of  $^{111}\text{In}$ -AMBA was  $9.72 \times 10^4$  MBq/ $\mu\text{mole}$ . The radiolabeling efficiency was analyzed using instant thin-layer chromatography (ITLC SG, Pall Corporation, New York, USA) with 0.1 M Na-citrate (pH 5.0) as solvent (indium citrate and  $^{111}\text{InCl}_3$ : Rf = 0.9~1.0, peptide-bound  $^{111}\text{In}$ : Rf = 0~0.1) [22]. Radio high-performance liquid chromatography (Radio-HPLC) analysis was performed using a Waters 2690 chromatography system with a 2996 photodiode array detector (PDA), a Bioscan radiodetector (Washington, DC, USA), and an FC 203B fraction collector by Gilson (Middleton, WI, USA).  $^{111}\text{In}$ -AMBA was purified by an Agilent (Santa Clara, CA, USA) Zorbax bonus-RP HPLC column (4.6  $\times$  250 mm, 5  $\mu\text{m}$ ) eluted with a gradient mixture from 10% B to 40% B in 40 min. Flow rate was 1 mL/min at RT, and the retention time for  $^{111}\text{In}$ -AMBA was 22.5 min. After purification by HPLC, 100% ethanol was used instead of acetonitrile by solvent exchange with Waters Sep-Pak Light C18 cartridge (Milford, MA, USA). Normal saline was added after evaporation, and pH value was at the range 7~7.5.

**2.4. Receptor Cold Competition Assay.** Cold competition binding assay was studied using human bombesin 2 receptor expressed in HEK-293 cells as the source of GRP receptors (PerkinElmer, Boston, MA, USA). Assays were performed using FC96 plates and the Multiscreen system (Millipore, Bedford, MA). Binding of  $^{125}\text{I}$ -Tyr<sup>4</sup>-Bombesin (PerkinElmer,



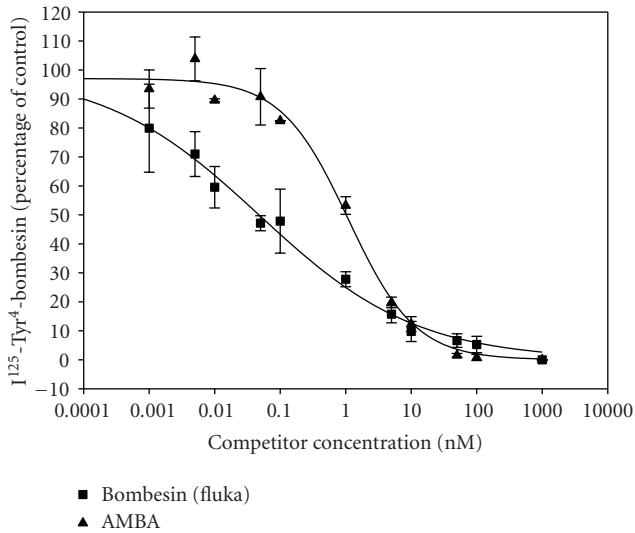


FIGURE 2: Competitive binding assay of AMBA versus  $^{125}\text{I-Tyr}^4$ -Bombesin with human bombesin 2 receptors.

of injected activity per g (% IA/g) for the organs in mice was extrapolated to uptake in organs of a 70-kg adult using the following formula [24]:

$$\left[ \left( \frac{\% \text{IA}}{g_{\text{organ}}} \right)_{\text{animal}} \times \left( \text{Kg}_{\text{TB weight}} \right)_{\text{animal}} \right] \times \left( \frac{g_{\text{organ}}}{\text{Kg}_{\text{TB weight}}} \right)_{\text{human}} = \left( \frac{\% \text{IA}}{\text{organ}} \right)_{\text{human}} \quad (1)$$

The extrapolated values (% IA) in the human organs at 1, 4, 8, 24, and 48 h were fitted with exponential biokinetic models and integrated to obtain the number of disintegrations in the source organs. This information was entered into the OLINDA/EXM computer program. The integrals (MBq-s) for 15 organs, including heart contents (blood), brain, muscle, bone, heart, lung, spleen, pancreas, kidneys, liver, and remainder of body were evaluated and used for dosimetry evaluation. The code also displays contributions of different source organs to the total dose of target organs. For the estimation of the tumor absorbed dose, it was assumed that once the radiopharmaceutical is inside the tumor, there is no biological elimination.

### 3. Results

**3.1. Radiolabeling and In Vitro Receptor Binding Assay.** The radiolabeling efficiency of  $^{111}\text{In-AMBA}$  was  $95.43 \pm 1.37\%$  ( $n = 11$ ). The *in vitro* competitive binding assays were determined in the human bombesin 2 receptor using  $^{125}\text{I-Tyr}^4$ -Bombesin as the GRP-R specific radiotracer, and unlabeled AMBA and native BN as competitors. The  $\text{IC}_{50}$  of the AMBA and native BN in human bombesin 2 receptor (Figure 2) is  $0.82 \pm 0.41$  nmol/L and  $0.13 \pm 0.10$  nmol/L, respectively, in a single, direct, nanomolar range, demonstrating high specificity and affinity for the GRP receptor.

The  $\text{K}_i$  of AMBA and native BBN were  $0.65 \pm 0.32$  nmol/L and  $0.10 \pm 0.08$  nmol/L, respectively.

**3.2. Biodistribution.**  $^{111}\text{In-AMBA}$  accumulated significantly in tumor, adrenal, pancreas, small intestine, and large intestine (Table 1). Fast blood clearance and fast excretion from the kidneys were observed. High levels of radioactivity were found in the kidneys before 24 h, indicating that the radioactivity was excreted rapidly in the urine within 24 h. The levels of radioactivity reached the highest with  $3.87 \pm 0.65$  % ID/g at 8 h and then declined rapidly. The highest tumor/muscle ratio (Tu/Mu) of  $^{111}\text{In-AMBA}$  was 11.79 at 8 h after injection and decreased progressively to 4.82 and 5.16 at 24 and 48 h after administration, respectively. Other GRPR-positive organs (small intestine and large intestine) also showed the specific binding of  $^{111}\text{In-AMBA}$  (Table 1). The tumor/muscle ratios were decreased conspicuously at 4 and 24 h postadministration.

**3.3. Pharmacokinetic Studies.** The radioactivity declined to under detection limit after 24 h. The pharmacokinetic parameters derived by a two-compartment model [27] indicated that the distribution half-life ( $t_{1/2\alpha}$ ) and distribution half-life ( $t_{1/2\beta}$ ) of  $^{111}\text{In-AMBA}$  were  $1.53 \pm 0.69$  h and  $30.73 \pm 8.56$  h, respectively (Table 2).

**3.4. Micro-SPECT/CT Imaging.** Micro-SPECT/CT imaging of  $^{111}\text{In-AMBA}$  indicated significant uptake in the tumors at 8 and 24 h after intravenous injection (Figure 3). The longitudinal micro-SPECT/CT imaging showed high accumulation of  $^{111}\text{In-AMBA}$  in pancreas and gastrointestinal tract at 4, 8, 24, and 48 h after intravenous injection.

**3.5. Radiation Absorbed Dose Calculation.** The radiation-absorbed dose projections for the administration of  $^{111}\text{In-AMBA}$  to humans, determined from the residence times in mice, are shown in Table 3. The highest absorbed doses appear in the lower large intestine ( $0.12$  mSv/MBq $^{-1}$ ), upper large intestine ( $0.13$  mSv/MBq $^{-1}$ ), kidneys ( $0.12$  mSv/MBq $^{-1}$ ), osteogenic cells ( $0.22$  mSv/MBq $^{-1}$ ), and pancreas ( $0.25$  mSv/MBq $^{-1}$ ). The effective dose appears to be approximately  $0.11$  mSv/MBq $^{-1}$ . The red marrow absorbed dose is estimated to be  $0.09$  mSv/MBq $^{-1}$ . For a 2-g tumor, the unit density sphere model was used and the estimated absorbed dose was  $8.09$  mGy·MBq $^{-1}$ .

### 4. Discussion

Growth factor receptors are involved in all steps of tumor progression, enhancing angiogenesis, local invasion, and distant metastases. The overexpression of growth factor receptors on the cell surface of malignant cells might be associated with a more aggressive behavior and a poor prognosis. For these reasons, tumor-related growth factor receptors can be taken as potential targets for therapeutic intervention. Over the last two decades, GRP and other BLPs may act as a growth factor in many types of cancer. GRPR antagonists have been developed as anticancer candidate

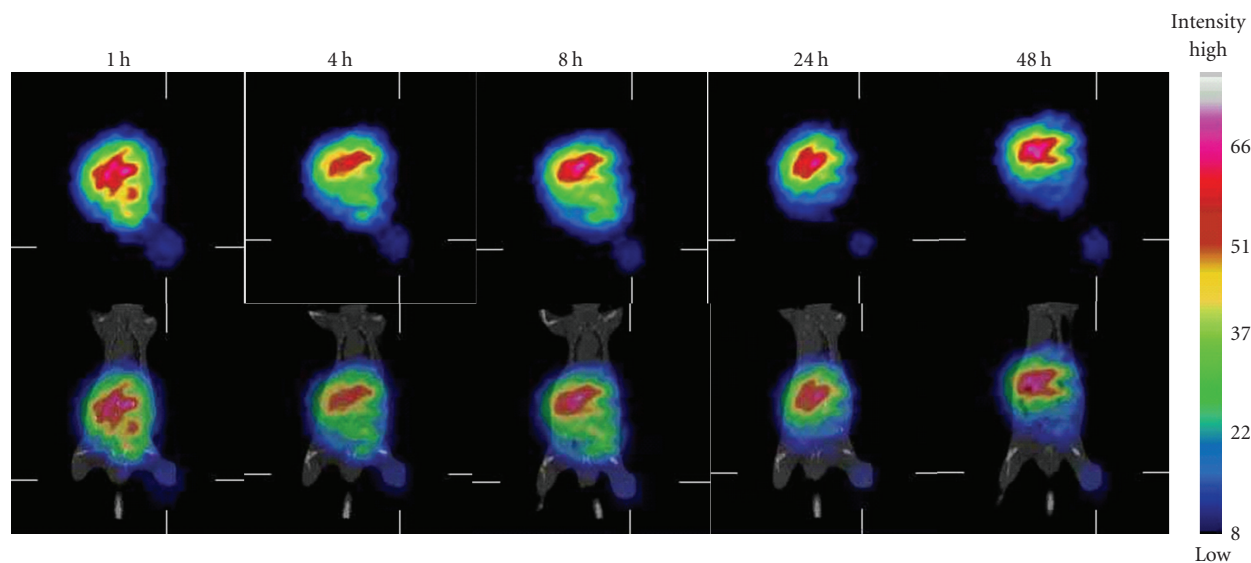


FIGURE 3: MicroSPECT/CT images of  $^{111}\text{In}$ -AMBA targeting PC-3 tumors xenograft SCID mice.  $12.2 \text{ MBq}/4 \mu\text{g}$   $^{111}\text{In}$ -AMBA was administered to each mouse by intravenous injection. The images were acquired at 1, 4, 8, 24, and 48 h after injection. The energy window was set at  $173 \text{ keV} \pm 10\%$  and  $247 \text{ keV} \pm 10\%$ ; the image size was set at  $80 \times 80$  pixels. The color map shows the SPECT pixel values from 0 to the maximum expressed with an arbitrary value of 100.

TABLE 1: Biodistribution of  $^{111}\text{In}$ -AMBA after intravenous injection in PC-3 prostate tumor-bearing SCID mice.

Organ	1 h	4 h	8 h	24 h	48 h
Blood	$0.95 \pm 0.09$	$0.50 \pm 0.06$	$0.42 \pm 0.02$	$0.19 \pm 0.03$	$0.09 \pm 0.02$
Brain	$0.06 \pm 0.01$	$0.05 \pm 0.01$	$0.05 \pm 0.00$	$0.02 \pm 0.00$	$0.03 \pm 0.00$
Skin	$0.99 \pm 0.22$	$0.60 \pm 0.16$	$0.55 \pm 0.02$	$0.36 \pm 0.02$	$0.28 \pm 0.02$
Muscle	$0.57 \pm 0.19$	$0.33 \pm 0.14$	$0.33 \pm 0.02$	$0.21 \pm 0.04$	$0.14 \pm 0.02$
Bone	$1.02 \pm 0.18$	$0.92 \pm 0.21$	$1.57 \pm 0.18$	$0.90 \pm 0.13$	$0.60 \pm 0.07$
Heart	$0.62 \pm 0.09$	$0.48 \pm 0.04$	$0.56 \pm 0.08$	$0.41 \pm 0.05$	$0.32 \pm 0.04$
Lung	$1.78 \pm 0.23$	$1.88 \pm 0.46$	$1.70 \pm 0.65$	$0.60 \pm 0.17$	$0.26 \pm 0.03$
Adrenals	$5.79 \pm 1.21$	$7.08 \pm 1.22$	$17.8 \pm 4.65$	$7.41 \pm 1.99$	$5.20 \pm 1.11$
Spleen	$2.80 \pm 1.49$	$6.90 \pm 1.87$	$8.90 \pm 2.34$	$4.41 \pm 0.58$	$2.19 \pm 0.51$
Pancreas	$6.14 \pm 0.99$	$12.9 \pm 2.44$	$54.9 \pm 2.51$	$15.9 \pm 1.94$	$9.80 \pm 2.21$
Kidney	$3.56 \pm 0.15$	$4.23 \pm 0.28$	$3.92 \pm 0.91$	$4.10 \pm 0.72$	$2.74 \pm 0.30$
Liver	$7.26 \pm 0.53$	$8.22 \pm 1.05$	$7.04 \pm 0.24$	$8.64 \pm 1.31$	$6.59 \pm 1.83$
Bladder	$7.63 \pm 2.94$	$1.75 \pm 0.75$	$1.07 \pm 0.12$	$0.64 \pm 0.06$	$0.46 \pm 0.10$
Stomach	$0.81 \pm 0.09$	$0.80 \pm 0.07$	$3.97 \pm 1.15$	$0.97 \pm 0.29$	$0.47 \pm 0.05$
SI	$1.67 \pm 0.22$	$1.56 \pm 0.17$	$4.42 \pm 0.61$	$1.48 \pm 0.27$	$0.74 \pm 0.10$
LI	$1.77 \pm 0.25$	$3.42 \pm 1.10$	$7.04 \pm 1.48$	$2.39 \pm 0.38$	$0.99 \pm 0.16$
Tumor (PC-3)	$2.24 \pm 0.66$	$1.86 \pm 0.71$	$3.87 \pm 0.65$	$1.02 \pm 0.09$	$0.75 \pm 0.08$
Tumor/muscle	3.89	5.69	11.79	4.82	5.16

Values are expressed as % ID/g, mean  $\pm$  SEM ( $n = 4\text{-}5$  at each time point). SI: small intestine; LI: large intestine.

compounds, exhibiting impressive antitumoral activity both *in vitro* and *in vivo* in various murine and human tumors [28, 29]. Clinical trials with GRPR antagonists in cancer patients are in its initial phase as anticipated by animal toxicology studies and preliminary evaluation in humans [29]. Presently, efforts at the identification of the most suitable candidates for clinical trials and at improving drug formulation for human use are considered priorities. It may also be anticipated that GRPRs may be exploited as

potential carriers for cytotoxins, immunotoxins, or radioactive compounds. Thus, the visualization of these receptors through molecular image-guided diagnostic agents may become an interesting tool for tumor detection and staging in personalized medicine.

The present study showed the highest accumulation of  $^{111}\text{In}$ -AMBA in pancreas in mice (Table 1). However, interspecies differences in structure and pharmacology of human and animal GRP receptors have been reported [30].

TABLE 2: Pharmacokinetic parameters of plasma in PC-3 tumor-bearing mice after intravenous injection of  $10 \mu\text{Ci}/\text{mouse}$   $^{111}\text{In}$ -AMBA (mean  $\pm$  SEM,  $n = 5$ ).

Parameter	Unit	Value
A	% ID/g	$6.15 \pm 0.69$
B	% ID/g	$1.43 \pm 0.61$
$\alpha$	1/h	$1.19 \pm 0.85$
$\beta$	1/h	$0.03 \pm 0.01$
$\text{AUC}_{0-168\text{h}}$	$\text{h} \times (\% \text{ID}/\text{g})$	$66.4 \pm 17.3$
$t_{1/2\alpha}$	h	$1.53 \pm 0.69$
$t_{1/2\beta}$	h	$30.7 \pm 8.56$
$C_{\text{max}}$	% ID/g	$7.37 \pm 0.64$

A, B,  $\alpha$ ,  $\beta$ : macro rate constants;  $t_{1/2\alpha}$ ,  $t_{1/2\beta}$ : distribution and elimination half-lives;  $\text{AUC}_{0-168\text{h}}$ : area under concentration of  $^{111}\text{In}$ -AMBA versus time curve;  $C_{\text{max}}$ : maximum concentration in plasma.

TABLE 3: Radiation dose estimates for  $^{111}\text{In}$ -AMBA in humans.

Organ	Estimated dose (mSv/MBq $^{-1}$ )*
Adrenals	$1.5E - 01$
Brain	$3.1E - 02$
Breasts	$7.7E - 02$
Gallbladder Wall	$1.5E - 01$
LLI Wall	$1.2E - 01$
Small Intestine	$1.3E - 01$
Stomach Wall	$1.1E - 01$
ULI Wall	$1.3E - 01$
Heart Wall	$7.2E - 02$
Kidneys	$1.2E - 01$
Liver	$2.0E - 01$
Lungs	$7.4E - 02$
Muscle	$7.0E - 02$
Ovaries	$1.2E - 01$
Pancreas	$2.5E - 01$
Red Marrow	$8.8E - 02$
Osteogenic Cells	$2.2E - 01$
Skin	$5.8E - 02$
Spleen	$1.2E - 01$
Testes	$5.9E - 02$
Thymus	$9.0E - 02$
Thyroid	$9.2E - 02$
Urinary Bladder Wall	$1.1E - 01$
Uterus	$1.3E - 01$
Total Body	$9.2E - 02$
Effective Dose	$1.1E - 01$

\* Radiation-absorbed dose projections in humans were determined from residence times for  $^{111}\text{In}$ -AMBA in SCID mice and were calculated by use of OLINDA/EXM version 1.0 computer program.

Because the pancreas is the primary normal tissue in these animals that expresses a high density of bloodstream-accessible GRPRs, the accumulation of  $^{111}\text{In}$  in the pancreas is a direct reflection of the efficacy of radiolabeled BN analogs for *in vivo* targeting of cell-surface-expressed GRPRs [31]. Retention of  $^{111}\text{In}$ -AMBA in the pancreas may be due to the

characteristic of a radioagonist with effective internalization and cell retention. Waser et al. reported that in contrast to the strongly labeled GRPR-positive mouse pancreas with  $^{177}\text{Lu}$ -AMBA, the human pancreas did not bind  $^{177}\text{Lu}$ -AMBA unless chronic pancreatitis was diagnosed [32].

The majority of research efforts into the design of bombesin-based radiopharmaceuticals have been carried out using GRPR agonists. The main reason for using agonists is that they undergo receptor-mediated endocytosis enabling residualization of the attached radiometal within the targeted cell [33]. Micro-SPECT/CT imaging is a noninvasive imaging modality that can longitudinally monitor the behavior of GRPR expression in the same animal across different time-points before and during therapy. In the present study, tumor targeting and localization of  $^{111}\text{In}$ -AMBA was clearly imaged with micro-SPECT/CT after 1 to 48 h of administration, suggesting that micro-SPECT/CT imaging with  $^{111}\text{In}$ -AMBA is a good tool for studying the tumor targeting, distribution, and real-time therapeutic response *in vivo*.

The effective dose projected for the administration of  $^{111}\text{In}$ -AMBA to humans ( $0.11 \text{ mSv}/\text{MBq}^{-1}$ ) (Table 3) is comparable to that for  $^{111}\text{In}$ -pentetreotide ( $0.12 \text{ mSv}/\text{MBq}^{-1}$ ) [34], the only  $^{111}\text{In}$ -labeled peptide receptor-targeted radiotherapeutic agent to be used clinically [35, 36]. The intestines, osteogenic cells, kidneys, and pancreas appear to receive absorbed doses around  $0.2 \text{ mSv}/\text{MBq}^{-1}$  of  $^{111}\text{In}$ -AMBA. At a maximum planned administration of 111 MBq for diagnostic imaging, the total radiation-absorbed dose to these organs kidneys would be about 12 mSv. The use of animal data to estimate human doses is a necessary first step, but such studies give only an estimate of radiation doses to be expected in human subjects. More accurate human dosimetry must be established with imaging studies involving human volunteers or patients. The dosimetry data presented here will be valuable in the dose planning of these studies, and for application of  $^{111}\text{In}$ -AMBA to Investigational New Drug (IND) research.

Clinically, primary prostate cancer and the metastases may be heterogeneous, demonstrating a spectrum of phenotypes from androgen-sensitive to androgen-insensitive.  $^{177}\text{Lu}$ -AMBA, a conjugated bombesin compound for imaging and systemic radiotherapy, is now in phase I clinical trials [15].  $^{177}\text{Lu}$ -AMBA has been evaluated in early stages of prostate cancer represented by the androgen-dependent, prostate-specific antigen-secreting hormone-sensitive prostate cancer cell line LNCaP [6], derived from a lymph node metastasis, and also in PC-3 cell line, derived from bone metastasis, is androgen-independent and is thought to represent late-stage hormone-refractory prostate cancer (HRPC) [37].  $^{177}\text{Lu}$ -AMBA will be clinically efficacious as a single-agent radiotherapeutic for heterogeneous metastatic prostate cancer and be a valuable adjunct to traditional chemotherapy. Thus, the visualization of GRPR receptors through  $^{111}\text{In}$ -AMBA as an image-guided agent may contribute to the use of radiotherapeutic,  $^{177}\text{Lu}$ -AMBA, and other traditional chemotherapy in personalized medicine.

Targeted therapeutic and imaging agents are becoming more prevalent and are used to treat increasingly smaller

population of patients. This has led to dramatic increases in the costs for clinical trials. Biomarkers have great potential to reduce the numbers of patients needed to test novel targeted agents by predicting or identifying nonresponse early on and thus enriching the clinical trial population with patients more likely to respond. GRPRs are expressed on prostate tumor cells, making it a potential biomarker for cancer. The imaging of  $^{111}\text{In}$ -AMBA indicated the stage of prostate cancer for determining the therapeutic approach to prostate cancer and for monitoring the therapeutic efficacy. The expression of GRPR will vary from patient to patient due to the stages and individual difference. If such patients could be prescreened with  $^{111}\text{In}$ -AMBA to identify those with higher tumor expression of GRPR, then it would be possible to select cases for receiving BLPs-specific treatment, while cases with low tumor expression of GRPR can consider other treatment options. Consequently, the proposed approaches enable optimized and individualized treatment protocols and can enhance the development of image-guide personalized medicine.

By visualizing how well drug targeting systems deliver pharmacologically active agents to the pathological site,  $^{111}\text{In}$ -AMBA furthermore facilitates “personalized medicine” and patient individualization, as well as the efficacy of combination regimens. Regarding personalized medicine, it can be reasoned that only in patients showing high levels of target site uptake with high expression of GRPR should treatment be continued; otherwise, alternative therapeutic approaches should be considered.

## 5. Conclusion

$^{111}\text{In}$ -AMBA showed a characteristic of agonist, a good bioactivity *in vitro* and uptake in human GRPR-expressing tumors *in vivo*. The molecular image-guided diagnostic agent can be used for various different purposes, ranging from simple and straightforward biodistribution studies to extensive and elaborate experimental setups aiming to enable “personalized medicine” and to improve the efficacy of combined modality anticancer therapy.

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