Research Article

Oxygenator Is the Main Responsible for Leukocyte Activation in Experimental Model of Extracorporeal Circulation: A Cautionary Tale

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In order to assess mechanisms underlying inflammatory activation during extracorporeal circulation (ECC), several small animal models of ECC have been proposed recently. The majority of them are based on home-made, nonstandardized, and hardly reproducible oxygenators. The present study has generated fundamental information on the role of oxygenator of ECC in activating inflammatory signaling pathways on leukocytes, leading to systemic inflammatory response, and organ dysfunction. The present results suggest that experimental animal models of ECC used in translational research on inflammatory response should be based on standardized, reproducible oxygenators with clinical characteristics.

1. Introduction

Extracorporeal circulation (ECC) is essential for cardiopulmonary bypass (CPB) during conventional cardiac surgery and extracorporeal membrane oxygenation (ECMO) during extracorporeal life support [1].

Systemic inflammation after ECC is believed to contribute to various pathophysiological outcomes, including renal, pulmonary, and myocardial damage [2]. The underlying mechanism is likely to be multifactorial, involving operative trauma, hemodilution and endothelial damage by edema, ischemia/reperfusion of organs, and contactactivation of blood components during ECC [2, 3]. The latter is known to have a pivotal role even after recent improvements in materials and techniques. Despite these insights, the mechanisms that control systemic inflammatory response during ECC remain poorly characterized at the molecular level. To address this issue several experimental animal models have been described [4–10]. The rat model of ECC is more accessible and less expensive compared to large animal models. Indeed it allows large availability of assay also with transgenic, knock-out, and syngenic species. Most of the models currently described in literature are based on homemade oxygenators [4–10]. We have recently reported the validation of a rat model of ECC with a miniaturized hollow fiber oxygenator with current clinical standards produced by one of the leading companies in the clinical field [11].

In the present study we aimed to assess the role of oxygenator, manufactured with industrial standards and clinical characteristics, in the development of leukocyte activation and systemic inflammation in a rat model of ECC.

2. Methods

After institutional animal care committee approval, 20 male Wistar rats (400–450 g; Harlan, Udine, Italy) housed under standard laboratory conditions were anesthetized (sodium pentobarbital, 30 mg/kg intraperitoneally) and intubated through the oropharynx with a 14-gauge polyethylene tube. They were mechanically ventilated with a rodent respirator (Harvard Apparatus Inc., Holliston, Massachusetts). The tidal volume was 7 mL/kg and the respiratory rate was 50 to 60 breaths/min with an air-oxygen mixture (inspired oxygen fraction = 0.5). Ventilation was adjusted to keep an arterial carbon dioxide tension of 35 to 45 mmHg. Rats were secured supine on a heating board to maintain rectal temperature at 37°C during the surgical procedure before the initiation of ECC. The left femoral artery was cannulated with a heparinized 24-gauge Teflon catheter to monitor systemic arterial pressure and to collect arterial blood for gas analysis. Central cannulation was performed as previously described [11, 12]. In brief, after complete sternotomy, a venous cannula (a modified 4-hole 16-gauge Angiocath catheter) was advanced into the right atrium using a right transsuperior vena cava approach, allowing excellent drainage. The left common carotid artery was cannulated using an 18-gauge catheter advanced to the aortic arch. Another 18-gauge catheter was inserted into the right femoral vein and advanced into inferior vena cava.

Full heparinization (500 IU/kg) was assured after surgical preparation and immediately before ECC initiation to reduce overall blood loss. ECC was set up as previously described [11, 12]. The setup consisted of a venous reservoir, a roller pump, a hollow fiber oxygenator (Sorin, Mirandola, Italy), and a vacuum regulator with an applied pressure of $-30 \text{ mm H}_2\text{O}$ to facilitate venous drainage, all connected by 1.6-mm internal diameter plastic tubing. Total priming volume was 10.5 mL, gas exchange surface was 450 cm², and heat exchange surface was 15.8 cm².

2.1. Study Design. Rats were randomized into two groups. The first group received the blood returned from the ECC circuit into the cannula positioned into the left common carotid artery.

In the second group of animals the oxygenator was not present in the ECC circuit and the blood was returned from the ECC circuit into the cannula allocated into the right femoral vein.

ECC was instituted in both groups at a flow rate of 120 mL/kg/min for 60 minutes. After the experiment, animals were humanely killed by anesthetic overdose.

2.2. Measurements. To access the inflammation induced by ECC in the two groups studied, blood samples were collected before and after ECC.

One hundred microliters of whole blood in ethylenediaminetetraacetic acid was determined by color immunofluorescent flow-cytometry analysis (FACSCalibur/BD CellQuest Pro software; Becton Dickinson, Tokyo, Japan).

Whole blood samples were incubated with Becton Dickinson (Franklin Lakes, NJ) lyse/fix buffer (containing phosphatase inhibitors) for 10 minutes at 37°C. Leukocytes were then isolated by centrifugation (300 g for 5 minutes) and washed once with phosphate-buffered saline. Cells were resuspended in 0.5 mL prechilled Becton Dickinson Perm Buffer III, vortexed, and incubated on ice for 30 minutes. After this, cells were washed twice with phosphate-buffered saline and resuspended in 0.5 mL Becton Dickinson Stain-Buffer (fetal bovine serum) before incubation for 30 minutes (at room temperature) with PE-Cy7- or PE-conjugated antibodies that recognized Ser529 phosphorylated RelA (p65; NF- κ B) or Thr180/Tyr182 phosphorylated p38 or isotype-matched controls, with subsequent washing and analysis by flow-cytometry (Becton Dickinson). Fluorescence of PE-conjugated p65 and PE-Cy7-conjugated p38 MAP kinase antibodies was quantified in granulocytes or mononuclear cells (identified by forward and side scatter plots) using Summit 4.3 software (Dako, Glostrup, Denmark).

The levels of TNF- α (Thermo scientific, Rockford, IL, USA), IL-6 (Thermo scientific, Rockford, IL, USA), and neutrophil elastase (NE, cloud-clone, Houston, TX, USA) were determined by Enzyme Linked Immunoadsorbent Assay (ELISA) kits, according to the manufacturer's instruction.

To access the inflammation in organ tissue, right lung was harvested immediately after euthanasia. Therefore it was fixed in 4% paraformaldehyde at 4°C overnight. Paraffinembedded sections (3 μ m) were stained with hematoxylin and eosin (H&E) and examined by microscope analysis by a pathologist blinded to the experimental groups. The severity of lung injury was scored using a 5-point scale according to combined assessment of alveolar congestion, haemorrhage, accumulation of neutrophils in the airspace or vessel wall, and the thickness of alveolar wall/hyaline membrane formation with minimal 0 for normal lung histology and maximum 5 for most injured lung [13].

2.3. Statistic. Statistical analysis was performed using SPSS 11.0 software (SPSS Inc., USA). Results are reported as mean \pm standard error (SE). Comparison between groups at a specific time point was determined by the Student *t* test. A *P* value < 0.05 was considered significant.

3. Results

3.1. Hemodynamic Parameters. All the animals in both groups survived through the experiment. Table 1 displays the hemodynamic and physiological parameters recorded before and after ECC. No differences between the two groups were demonstrated.

3.2. Inflammatory Signalling Pathways Activation on Leukocytes. The kinetics of leukocyte activation were determined by measuring p38 phosphorylation and NF- κ B phosphorylation in leukocytes. Intracellular staining and flow-cytometry demonstrated that ECC induced phosphorylation of both p38 (Figure 1(a)) and NF- κ B (Figure 1(b)) in mononuclear cells and granulocytes after ECC. Moreover the amount of leukocyte activation was significantly higher in ECC + oxygenator group.

Figure 2 shows representative flow-cytometry analysis before ECC and after ECC in each group. A significant depletion of mononuclear cells and granulocytes after ECC + oxygenator is evident.

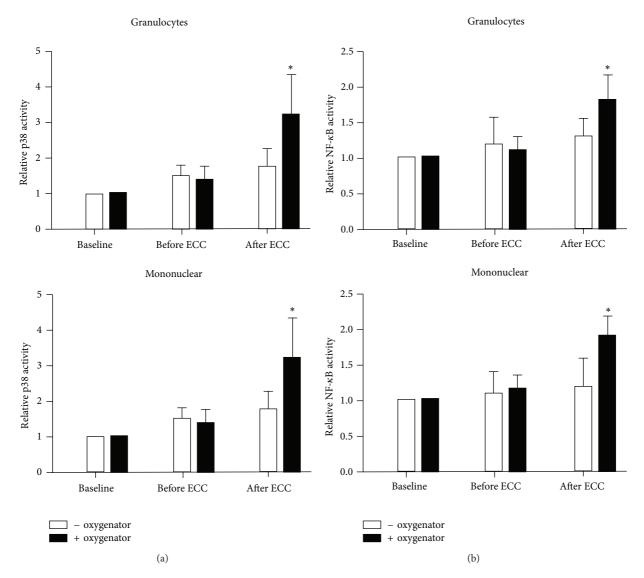


FIGURE 1: P38 and NF- κ B activation in leukocytes in response to ECC was significantly higher in presence of oxygenator. Peripheral blood samples were collected at baseline, before and after ECC. Leukocytes were fixed and permeabilized before intracellular staining using Alexa Fluor 568-conjugated antibodies that recognize (a) Thr180/Tyr182 phosphorylated p38 or (b) Ser529 phosphorylated NF- κ B or with isotypematched antibodies as a control. After lysis of red blood cells, fluorescence of granulocytes or mononuclear cells was quantified by flowcytometry (after gating of cells by size and granularity). Mean fluorescence levels were calculated after subtracting values from isotype-control antibodies. Mean values are shown with standard deviations. *P < 0.05 between the two groups at the same time point.

3.3. Inflammatory Response and Organ Injury. Plasma levels of TNF- α (Figure 3(a)), neutrophil elastase (NE) (Figure 3(b)), and IL-6 (Figure 3(c)) increased after ECC in both groups. However they were significantly higher in ECC + oxygenator compared to ECC – oxygenator (P < 0.01).

Rats receiving ECC + oxygenator demonstrated a recognized feature of pulmonary injury, characterized by edema, hemorrhage, increased thickness of alveolar wall, and inflammatory cells into alveolar spaces (Figure 4(a)). The lung injury scores were therefore significantly higher in ECC + oxygenator (4.50 ± 0.50) than in ECC – oxygenator ($3.0 \pm$ 1.0; P < 0.001) (Figure 4(b)).

4. Discussion

The present study has generated fundamental information on the role of oxygenator of ECC in activating inflammatory signalling pathways on leukocytes. By the use of a previously reported and validated rat model of ECC [11, 12], we have demonstrated for the first time that oxygenator has a pivotal role in triggering leukocyte activation and subsequent inflammatory response.

Given the recognized role of p38 and NF- κ B in the transcriptional induction of proinflammatory molecules [14–16], we have demonstrated that ECC + oxygenator leads to a significant phosphorylation (i.e., activation) of both p38 and

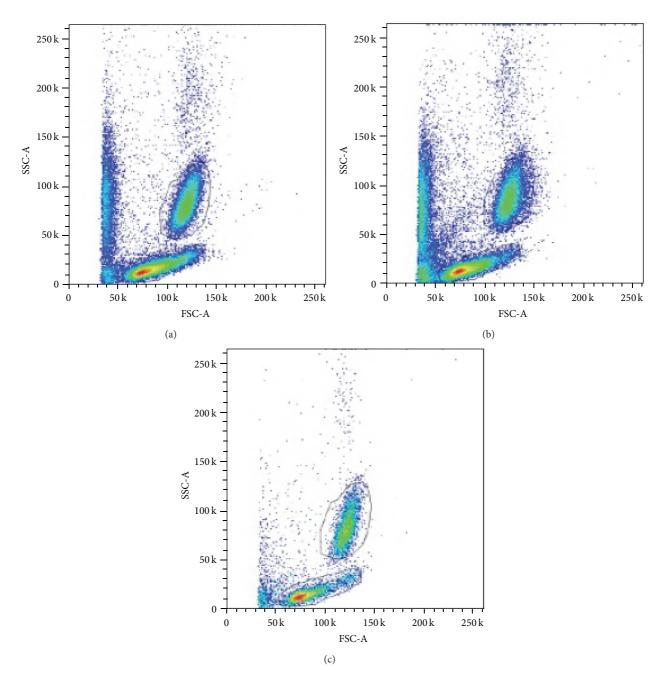


FIGURE 2: Representative flow-cytometry analysis at baseline (a), after ECC without oxygenator (b) and after ECC with oxygenator (c). A significant depletion of mononuclear cells and granulocytes after ECC + oxygenator is evident.

NF- κ B in leukocytes. The underlying mechanism may involve contact-activation of blood components [17, 18]. Therefore it is possible to argue that the contact-activation between blood components and ECC surfaces is mainly produced in the oxygenator. The latter is indeed an essential component of ECC circuits in clinical setting [19]. Both CPB and ECMO are based on the performance of oxygenator to support circulatory and respiratory functions during cardiac surgery operations or critical cardiorespiratory diseases, respectively [20].

Surface coating of ECC circuits, oxygenator included, with heparin or phosphorylcholine has been proved to reduce

the inflammatory response [21–24]. This is detectable not only on the basis of laboratory results but also by clinical parameters like reduced respiratory index and improved pulmonary and coagulation function in pediatric patients [21– 23]. Therefore coated ECC equipment has become a clinical standard since beginning of 2000. However surface coating with either heparin or phosphorylcholine has not resolved the clinical problem of inflammatory response induced by ECC [24].

Many rat models of ECC have been proposed recently in order to assess molecular mechanisms responsible for

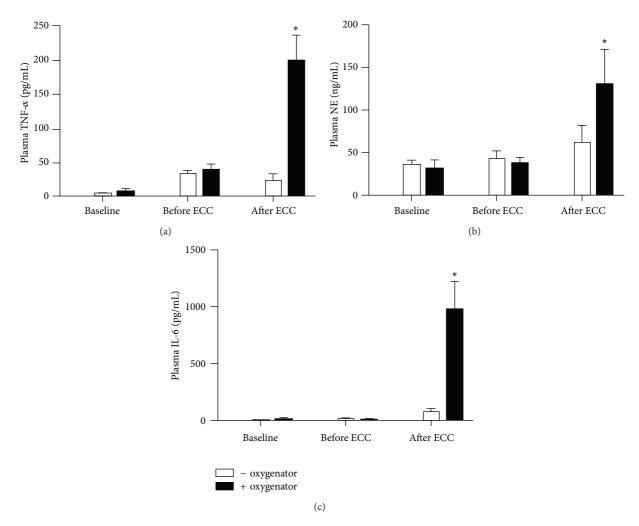


FIGURE 3: Systemic inflammatory response assessed by TNF- α (a), neutrophil elastase (NE) (b), and IL-6 (c) levels in plasma. *P < 0.01 versus the other group at the same time point.

	Before ECC		After ECC	
	 oxygenator 	+ oxygenator	 oxygenator 	+ oxygenator
Heart rate (bpm)	287 ± 5	292 ± 8	314 ± 11	304 ± 10
MAP (mmHg)	58.3 ± 9.0	60.3 ± 8.3	50.5 ± 8.0	55.1 ± 9.7
Haematocrit (%)	34.5 ± 1.1	33.5 ± 1.8	11.2 ± 6.1	10.2 ± 5.8
Haemoglobin (g/dL)	12.8 ± 0.6	13.0 ± 0.9	4.8 ± 1.2	5.2 ± 0.9
WBC ($\times 10^3$ /mm ³)	6.2 ± 1.8	5.5 ± 0.7	3.1 ± 0.4	2.7 ± 0.5
SaO ₂ (%)	98.2 ± 0.5	97.9 ± 0.4	95.2 ± 0.6	96.0 ± 1.1
PaO ₂ (mmHg)	72.3 ± 5.8	75.0 ± 4.1	69.0 ± 3.0	70.2 ± 9.0
PaCO ₂ (mmHg)	40.3 ± 5.9	43.0 ± 7.0	39.9 ± 4.0	42.3 ± 6.5
рН	7.32 ± 0.05	7.38 ± 0.04	7.22 ± 0.12	7.14 ± 0.20
BE (mmol/L)	-4.3 ± 1.2	-3.1 ± 1.5	-10.1 ± 4.7	-11.7 ± 6.2
HCO ₃ (mmol/L)	24.1 ± 7.8	22.0 ± 6.1	11.0 ± 10.1	16.1 ± 9.8

TABLE 1: Hemodynamic and ph	ysiological parameters.
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WBC = white blood cells; bpm = beats per minute; MAP = mean arterial pressure; SaO₂ = arterial oxygen saturation; PaO₂ = partial pressure of arterial oxygen; PaCO₂ = partial pressure of arterial carbon dioxide; BE = base excess; HCO₃ = standard bicarbonate. Data represent means ± SE.

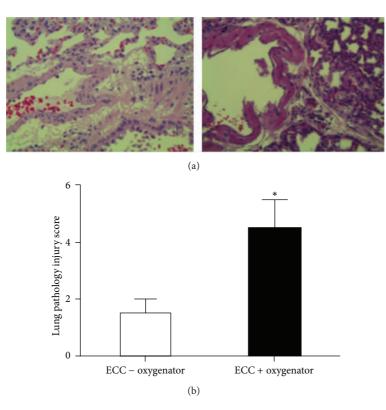


FIGURE 4: Lung injury. Representative histological images (magnification 40x) of right lung fixed in formaldehyde, sectioned, and stained with haematoxylin and eosin (a). The acute lung injury score was calculated (b). *P < 0.01.

activation of inflammatory response during ECC and to study possible therapeutic interventions [4–10]. All of these models are based on different home-made oxygenators. We have previously proposed a validated model of ECC in rat with a miniaturized hollow fiber oxygenator with clinical characteristics and manufactured with industrial standards by one of the leading producers of clinical oxygenators [11]. The present work demonstrated that a clinical relevant oxygenator has a major impact on leukocyte activation and systemic inflammatory response with implications in organ dysfunction. Therefore experimental studies aimed at investigating inflammatory response during ECC should be based on models with a standardized, reproducible, and clinical relevant oxygenator.

5. Conclusions

Oxygenator has a major role in leukocyte activation, inflammatory response, and organ dysfunction during ECC.

The present results suggest that experimental animal models of ECC used in translational research on inflammatory response should be based on standardized, reproducible oxygenators with clinical characteristics.

Conflict of Interests

The authors declare that there is no conflict of interests regarding the publication of this paper.

Authors' Contribution

Alessio Rungatscher and Maddalena Tessari contributed equally.

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References

- J. Börgermann, R. J. Scheubel, A. Simm, R. E. Silber, and I. Friedrich, "Inflammatory response in on- versus off-pump myocardial revascularization: is ECC really the culprit?" *Thoracic and Cardiovascular Surgeon*, vol. 55, no. 8, pp. 473–480, 2007.
- [2] S. Wan, J.-L. Leclerc, and J.-L. Vincent, "Inflammatory response to cardiopulmonary bypass: mechanisms involved and possible therapeutic strategies," *Chest*, vol. 112, no. 3, pp. 676–692, 1997.
- [3] P. Biglioli, A. Cannata, F. Alamanni et al., "Biological effects of off-pump vs. on-pump coronary artery surgery: focus on inflammation, hemostasis and oxidative stress," *European Journal of Cardio-thoracic Surgery*, vol. 24, no. 2, pp. 260–269, 2003.
- [4] Y. Hiramatsu, N. Gikakis, J. H. Gorman III et al., "A baboon model for hematologic studies of cardiopulmonary bypass," *Journal of Laboratory and Clinical Medicine*, vol. 130, no. 4, pp. 412–420, 1997.
- [5] W. G. Kim, H. J. Moon, T. H. Won, and H. K. Chee, "Rabbit model of cardiopulmonary bypass," *Perfusion*, vol. 14, no. 2, pp. 101–105, 1999.

- [6] G. B. Mackensen, Y. Sato, B. Nellgård et al., "Cardiopulmonary bypass induces neurologic and neurocognitive dysfunction in the rat," *Anesthesiology*, vol. 95, no. 6, pp. 1485–1491, 2001.
- [7] C. Wittnich, M. P. Belanger, W. J. Wallen, S. M. Torrance, and S. Juhasz, "A long-term stable normothermic cardiopulmonary bypass model in neonatal swine," *Journal of Surgical Research*, vol. 101, no. 2, pp. 176–182, 2001.
- [8] R. Günzinger, S. M. Wildhirt, H. Schad et al., "A rat model of cardiopulmonary bypass with cardioplegic arrest and hemodynamic assessment by conductance catheter technique," *Basic Research in Cardiology*, vol. 102, no. 6, pp. 508–517, 2007.
- [9] F. Doguet, P.-Y. Litzler, F. Tamion et al., "Changes in mesenteric vascular reactivity and inflammatory response after cardiopulmonary bypass in a rat model," *Annals of Thoracic Surgery*, vol. 77, no. 6, pp. 2130–2137, 2004.
- [10] A. Janata, I. A. M. Magnet, T. Drabek et al., "Extracorporeal versus conventional cardiopulmonary resuscitation after ventricular fibrillation cardiac arrest in rats: a feasibility trial," *Critical Care Medicine*, vol. 41, no. 9, pp. e211–e222, 2013.
- [11] G. D. Cresce, B. H. Walpoth, D. Mugnai et al., "Validation of a rat model of cardiopulmonary bypass with a new miniaturized hollow fiber oxygenator," *ASAIO Journal*, vol. 54, no. 5, pp. 514– 518, 2008.
- [12] A. Rungatscher, D. Linardi, A. Giacomazzi et al., "Cardioprotective effect of δ -opioid receptor agonist vs mild therapeutic hypothermia in a rat model of cardiac arrest with extracorporeal life support," *Resuscitation*, vol. 84, no. 2, pp. 244–248, 2013.
- [13] B. Kabay, Z. Teke, F. O. Aytekin et al., "Pyrrolidine dithiocarbamate reduces lung injury caused by mesenteric ischemia/reperfusion in a rat model," *World Journal of Surgery*, vol. 31, no. 8, pp. 1707–1715, 2007.
- [14] M. S. Hayden and S. Ghosh, "Signaling to NF-κB," Genes and Development, vol. 18, no. 18, pp. 2195–2224, 2004.
- [15] A. Mócsai, Z. Jakus, T. Vántus, G. Berton, C. A. Lowell, and E. Ligeti, "Kinase pathways in chemoattractant-induced degranulation of neutrophils: the role of p38 mitogen-activated protein kinase activated by Src family kinases," *The Journal of Immunology*, vol. 164, no. 8, pp. 4321–4331, 2000.
- [16] A. Cloutier, T. Ear, E. Blais-Charron, C. M. Dubois, and P. P. McDonald, "Differential involvement of NF-kappa B and MAP kinase pathways in the generation of inflammatory cytokines by human neutrophils," *Journal of Leukocyte Biology*, vol. 81, no. 2, pp. 567–577, 2007.
- [17] S. Zahler, P. Massoudy, H. Hartl, C. Hähnel, H. Meisner, and B. F. Becker, "Acute cardiac inflammatory responses to postischemic reperfusion during cardiopulmonary bypass," *Cardiovascular Research*, vol. 41, no. 3, pp. 722–730, 1999.
- [18] O. Liangos, S. Domhan, C. Schwager et al., "Whole blood transcriptomics in cardiac surgery identifies a gene regulatory network connecting ischemia reperfusion with systemic inflammation," *PLoS ONE*, vol. 5, no. 10, Article ID e13658, 2010.
- [19] L. K. von Segesser, P. Tozzi, I. Mallbiabrrena, D. Jegger, J. Horisberger, and A. Corno, "Miniaturization in cardiopulmonary bypass," *Perfusion*, vol. 18, no. 4, pp. 219–224, 2003.
- [20] A. Rungatscher, S. Hallström, A. Giacomazzi et al., "Role of calcium desensitization in the treatment of myocardial dysfunction after deep hypothermic circulatory arrest," *Critical Care*, vol. 17, article R245, 2013.
- [21] F. De Somer, K. François, W. van Oeveren et al., "Phosphorylcholine coating of extracorporeal circuits provides natural protection against blood activation by the material surface,"

European Journal of Cardio-Thoracic Surgery, vol. 18, no. 5, pp. 602–606, 2000.

- [22] E. A. Grossi, K. Kallenbach, S. Chau et al., "Impact of heparin bonding on pediatric cardiopulmonary bypass: a prospective randomized study," *Annals of Thoracic Surgery*, vol. 70, no. 1, pp. 191–196, 2000.
- [23] T. Ozawa, K. Yoshihara, N. Koyama, Y. Watanabe, N. Shiono, and Y. Takanashi, "Clinical efficacy of heparin-bonded bypass circuits related to cytokine responses in children," *The Annals* of *Thoracic Surgery*, vol. 69, no. 2, pp. 584–590, 2000.
- [24] A. Böning, J. Scheewe, T. Ivers et al., "Phosphorylcholine or heparin coating for pediatric extracorporeal circulation causes similar biologic effects in neonates and infants," *Journal of Thoracic and Cardiovascular Surgery*, vol. 127, no. 5, pp. 1458– 1465, 2004.