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# Saturation-pulse prepared heart-rate independent inversion-recovery (SAPPHIRE) biventricular T<sub>1</sub> mapping: inter-field strength, head-to-head comparison of diastolic, systolic and dark-blood measurements

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## Abstract

**Background:** To assess the feasibility of biventricular SAPPHIRE T<sub>1</sub> mapping in vivo across field strengths using diastolic, systolic and dark-blood (DB) approaches.

**Methods:** 10 healthy volunteers underwent same-day non-contrast cardiovascular magnetic resonance at 1.5 Tesla (T) and 3 T. Left and right ventricular (LV, RV) T<sub>1</sub> mapping was performed in the basal, mid and apical short axis using 4-variants of SAPPHIRE: diastolic, systolic, 0th and 2nd order motion-sensitized DB and conventional modified Look-Locker inversion recovery (MOLLI).

**Results:** LV global myocardial T<sub>1</sub> times (1.5 T then 3 T results) were significantly longer by diastolic SAPPHIRE (1283 ± 11|1600 ± 17 ms) than any of the other SAPPHIRE variants: systolic (1239 ± 9|1595 ± 13 ms), 0th order DB (1241 ± 10|1596 ± 12) and 2nd order DB (1251 ± 11|1560 ± 20 ms, all  $p < 0.05$ ). In the mid septum MOLLI and diastolic SAPPHIRE exhibited significant T<sub>1</sub> signal contamination (longer T<sub>1</sub>) at the blood-myocardial interface not seen with the other 3 SAPPHIRE variants (all  $p < 0.025$ ). Additionally, systolic, 0th order and 2nd order DB SAPPHIRE showed narrower dispersion of myocardial T<sub>1</sub> times across the mid septum when compared to diastolic SAPPHIRE (interquartile ranges respectively: 25 ms, 71 ms, 73 ms vs 143 ms, all  $p < 0.05$ ). RV T<sub>1</sub> mapping was achievable using systolic, 0th and 2nd order DB SAPPHIRE but not with MOLLI or diastolic SAPPHIRE. All 4 SAPPHIRE variants showed excellent re-read reproducibility (intraclass correlation coefficients 0.953 to 0.996).

**Conclusion:** These small-scale preliminary healthy volunteer data suggest that DB SAPPHIRE has the potential to reduce partial volume effects at the blood-myocardial interface, and that systolic SAPPHIRE could be a feasible solution for right ventricular T<sub>1</sub> mapping. Further work is needed to understand the robustness of these sequences and their potential clinical utility.

**Keywords:** T<sub>1</sub> mapping, Cardiovascular magnetic resonance, SAPPHIRE, MOLLI

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## Background

The myocardial longitudinal relaxation time, T<sub>1</sub> is a sensitive imaging biomarker for heart muscle disease, linked to both functional capacity and mortality [1–5].



Various techniques have been proposed to quantify  $T_1$  relaxation (Fig. 1), each with its own advantages and limitations [6]. One of the main issues of commonly-used  $T_1$  mapping techniques is the partial volume effect that can artifactually increase the myocardial  $T_1$  times of voxels located at the myocardial-blood pool interface due to confounding by the higher native  $T_1$  signal of the blood pool. This is most apparent in cross sectional imaging and its effects are especially detrimental to the study of thin-walled cardiac structures, notably the right ventricular (RV) free wall, atrial walls and the thinned myocardium in dilated cardiomyopathy [7, 8]. Partial volume effects are problematic because they reduce the accuracy and reproducibility of  $T_1$  mapping. To overcome this problem in the right and left ventricles (LV), systolic readouts have been proposed [9, 10], as it was hypothesized that the increased myocardial wall thickness during systole would increase the abundance of myocardial voxels that were free from partial volume effects. Systolic readouts collect data during a limited quiescent time window and therefore necessitate a shorter acquisition time to reduce temporal blurring, however this trade off could affect precision. In spite of this limitation, systolic  $T_1$  mapping approaches have potential advantages in arrhythmia and resulted in more evaluable images [9–11].

The modified Look-Locker inversion recovery (MOLLI) sequence is still the most commonly used  $T_1$  mapping approach in clinical practice due to its widespread availability across vendors and superior precision and reproducibility [12]. Being an inversion recovery-based approach, it is vulnerable to the aforementioned partial volume effects, as well as to off-resonance artifacts, and

confounding contributions by magnetisation transfer and  $T_2$  effects [11].

A  $T_1$  mapping sequence that combines saturation recovery and inversion recovery approaches, termed SAPPHIRE–SATuration Pulse Prepared Heart-rate independent Inversion REcovery–has recently been shown to have potential advantages in arrhythmia [13]. A further refinement to SAPPHIRE that provides blood suppression resulting in dark-blood (DB) native myocardial  $T_1$  mapping has shown additional promise at addressing the problem of myocardial signal contamination from the adjacent blood pool [8]. DB SAPPHIRE potentially measures more accurate  $T_1$  than the conventional diastolic SAPPHIRE because of less contamination from the blood pool signal, but this is at the expense of precision.

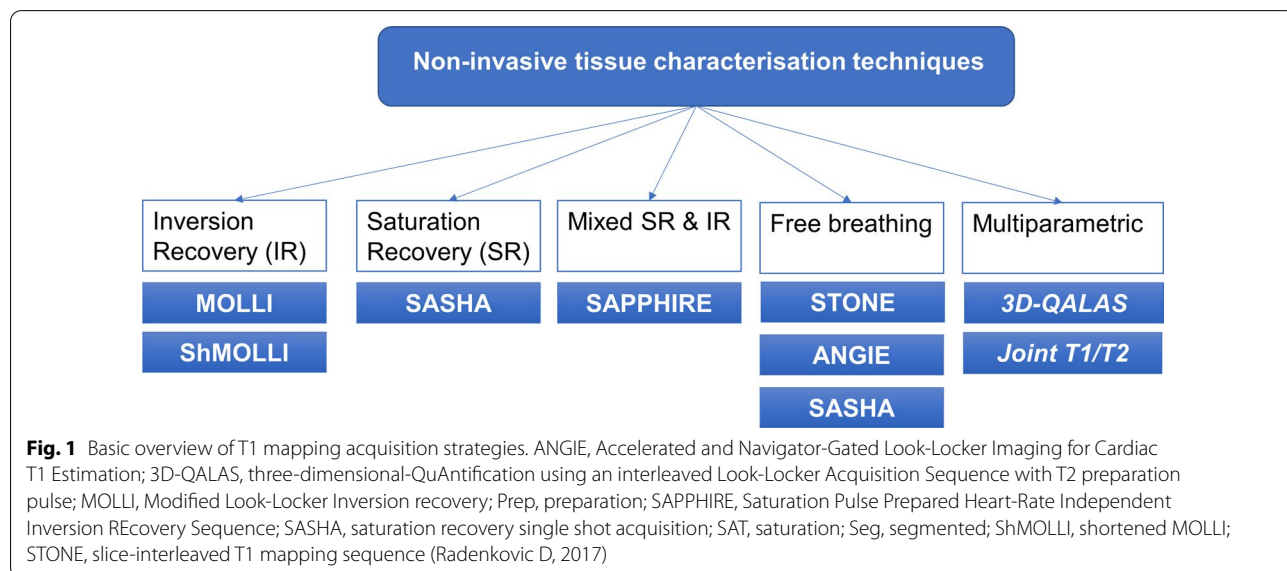
Here we undertake a head-to-head comparison of SAPPHIRE  $T_1$  mapping variants across field strengths. We assess the performance of LV and RV SAPPHIRE  $T_1$  mapping in vivo considering 4 variants: diastolic, systolic, 0th and 2nd order DB SAPPHIRE, and compare results to those obtained by conventional MOLLI across field strengths.

**Methods**

All subjects provided written informed consent. The study received ethical approval from the University College London (UCL) Research Ethics Committee (Project number 6782/001) and it conformed to the principles of the Helsinki Declaration.

**Study population and data collection**

In this prospective single-center observational study, 10 healthy volunteers underwent non-contrast cardiovascular



magnetic resonance (CMR) scanning at both field strengths on the same day at the UCL Bloomsbury Center for Clinical Phenotyping (London, UK). Volunteers had no prior cardiac history or known cardiac risk factors, were not on cardiovascular medications, had a normal resting electrocardiogram (ECG), and were free of conventional contraindications for CMR.

### Cardiovascular magnetic resonance

CMR studies were performed using two Siemens MR systems (Erlangen, Germany): MAGNETOM AERA 1.5 Tesla (T) operating VE11C-SP01 and MAGNETOM PRISMA 3 T operating VE11C-SP01, with 18-channel phased-array chest coils. The scan protocol was identical for the two field strengths and consisted of localizers, transaxial black blood HASTE anatomical stack, breath-held retrospectively ECG-gated balanced steady-state free precession (bSSFP) cines in standard long and short axis views [14], and then breath-held ECG-gated  $T_1$  mapping in the basal, mid and apical LV short axis slices (co-registered with the cines) using MOLLI with motion correction (MOCO), bright-blood diastolic SAPHIRE, bright-blood systolic SAPHIRE, 0th order DB SAPHIRE and 2nd order DB SAPHIRE in random order per scan. To minimize off-resonance artifacts with higher field strengths, the 3 T protocol additionally included frequency scouts and attention to volumetric shimming.

Typical imaging parameters for the  $T_1$  mapping sequences are summarised in Table 1.

### Cardiovascular magnetic resonance analysis

Images were analysed using CVI42 software (Circle Cardiovascular Imaging Inc. v.5.10.1, Calgary, Canada). Measurements were performed by two readers with over three years of advanced cardiac MRI experience (M.A., J.A.). LV volumes, LV ejection fraction (LVEF) and mass were determined according to standardized CMR methods [15] using a semiautomated threshold-based technique and body surface area (BSA) indexation where appropriate. Atrial volumes, LV maximal wall thickness, and mitral and tricuspid annular plane systolic excursions were determined as previously described [16–18].

For native  $T_1$  measurements in the LV, endo- and epicardial borders were manually drawn per segment according to the 16-segment American Heart Association model, in the 3 short axis slices (10% offset). Segmental  $T_1$  times were averaged to obtain the mean slice  $T_1$  and global  $T_1$  calculated as the mean of basal, mid and apical LV short axis slices.

As demonstrated in Fig. 2 the RV region of interest (ROI) measurements were obtained from the RV inferior wall or free wall in the basal or mid short axis slices if wall thickness  $\geq 5$  mm.

The transeptal myocardial  $T_1$  times for MOLLI and SAPHIRE variants were calculated in OsiriX MD using six evenly-spaced points along linear callipers transecting the mid-septal short axis slice on the  $T_1$  maps of each healthy volunteer.

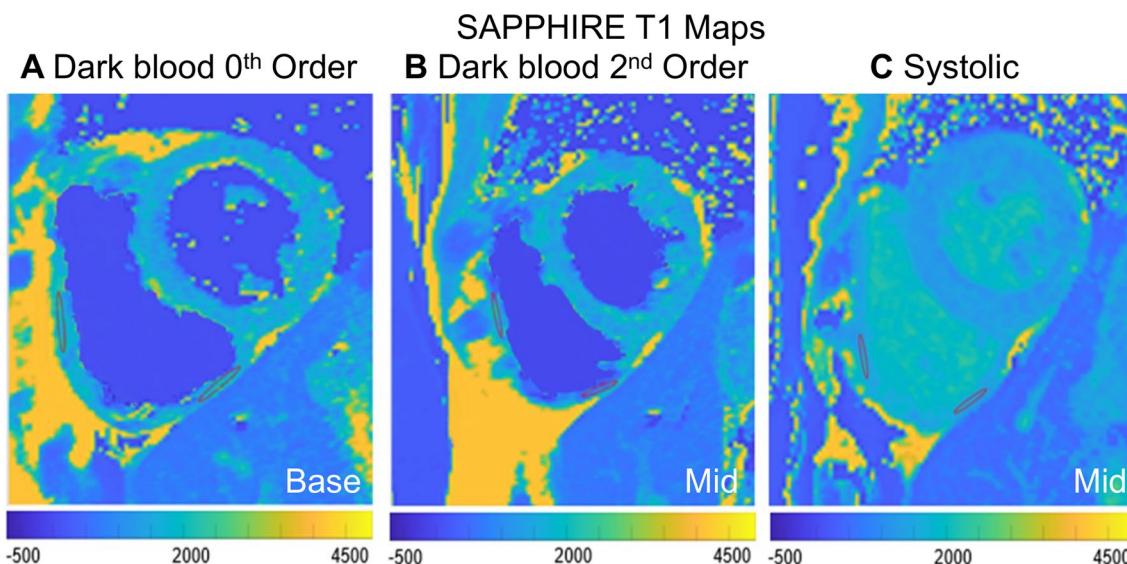
**Table 1** Typical imaging parameters for the SAPHIRE sequences

	TR/TE (ms)	TD (ms)	FA	TI (ms)	Matrix	Slice thickness (mm)	FOV (mm)	Pixel size (mm)	Acquisition window (ms)	
MOLLI	1.5 T	291.84/1.22	605	35°	~103–4035	256 × 192	8	300 × 225	1.171875 × 1.171875	4
	3 T	283.8/1.16	780	20°	~103–4438	256 × 192	8	300 × 225	1.171875 × 1.171875	4
Diastolic SAPHIRE	1.5 T	830/1.12	710	70°	~715	256 × 192	8	300 × 225	1.171875 × 1.171875	8
	3 T	856/1.12	778	68°	~740	256 × 192	8	300 × 225	1.171875 × 1.171875	8
Systolic SAPHIRE	1.5 T	830/1.12	315	70°	~335	256 × 192	8	300 × 225	1.171875 × 1.171875	9
	3 T	857/1.12	393	68°	~380	256 × 192	8	300 × 225	1.171875 × 1.171875	9
DB 0th order SAPHIRE <sup>†</sup>	1.5 T	800/1.28	678	70°	~670	256 × 192	8	300 × 225	1.171875 × 1.171875	7
	3 T	857/1.12	753	68°	~740	256 × 192	8	300 × 225	1.171875 × 1.171875	7
DB 2nd order SAPHIRE <sup>†</sup>	1.5 T	800/1.28	678	70°	~670	256 × 192	8	300 × 225	1.171875 × 1.171875	8
	3 T	857/1.12	750	68°	~740	256 × 192	8	300 × 225	1.171875 × 1.171875	8

DB, Dark blood; FA, flip angle; FOV, Field of view; MOLLI, Modified Look-Locker inversion recovery; SAPHIRE, SATuration Pulse Prepared Heart-rate independent Inversion Recovery; T, Tesla; TD trigger delay; TI inversion time; TR/TE, time between two consecutive excitations/ echo time

† 10 images acquired with 10 s breath-hold duration and 125 encoding steps for all sequences

† MSDE gradient amplitude 20 mT/m with preparation duration 10 ms



**Fig. 2** Right ventricular (RV)  $T_1$  times were determined by manually tracing regions of interest in the RV inferior wall or RV free wall on the basal (a) or mid-ventricular (b, c) short axis dark blood or systolic SAPPHIRE  $T_1$  map. Exemplar RV ROIs at 1.5 T are shown for 3 study participants. Other abbreviations as in Fig. 1

Intra- and inter-observer re-read variability was determined for measurements of average mid slice  $T_1$ , and mid septal ROI  $T_1$  in 5 randomly chosen CMR scans. Intra-observer variability was performed with one-month temporal interval between repeat analyses.

**Native SAPPHIRE  $T_1$  mapping sequences**

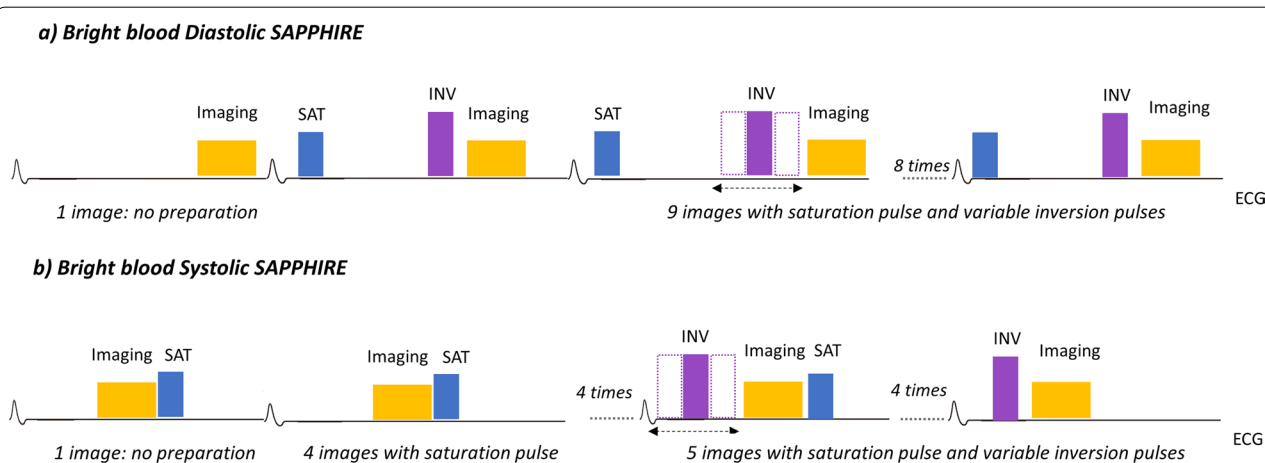
**Diastolic SAPPHIRE**

Conventional diastolic SAPPHIRE (without any attempt to suppress the blood signal, i.e. ‘bright blood’) consists of a combination of saturation and inversion

pulses. A saturation pulse is applied immediately after the R wave followed by an inversion pulse inserted in the same heartbeat prior to image acquisition (Fig. 3a). The first image acquisition is done without magnetisation preparation.

**Systolic SAPPHIRE**

Systolic SAPPHIRE also consists of saturation and inversion recovery magnetisation preparation hybrid and 10-ECG triggered readouts but data is acquired during systole, and with shorter acquisition windows than the



**Fig. 3** Sequence diagrams of the SAPPHIRE bright blood diastolic (a) and systolic (b)  $T_1$  mapping variants. The image acquisition window in systolic SAPPHIRE is shorter compared to diastole. ECG, Electrocardiogram; INV, Inversion pulse. Other abbreviations as in Fig. 1

diastolic SAPHIRE. Imaging in systole is challenging due to the short time window available between R waves resulting in a weak saturation recovery  $T_1$  mapping signal. As a fix, saturation is performed in the preceding heart-beat directly following the imaging pulses played in the previous heart-beat. Similar to diastolic SAPHIRE, the first image is acquired without magnetisation preparation. The remaining images are obtained with an extra inversion pulse with variable delay following the R wave (Fig. 3b).

**0th and 2nd Order dark blood diastolic SAPHIRE**

DB  $T_1$  mapping is achieved using a modified SAPHIRE technique [19]. For blood suppression, motion sensitized driven equilibrium (MSDE) preparation is inserted before the bSSFP imaging readout (Fig. 4a). The MSDE preparation consists of a  $90^\circ$  excitation tip-down pulse, a one or more  $180^\circ$  refocusing pulse, and a  $-90^\circ$  flip-back pulse to encode the spin dephasing in the longitudinal magnetisation (Fig. 4a). Strong motion sensitising gradients are also sandwiched in between the radiofrequency pulses to induce dephasing. Two kinds of motion sensitising gradients are employed, with nulling the gradient moment up to the 0th and 2nd order respectively. To achieve 0th order gradient nulling, identical trapezoidal gradients are played before and after the refocusing pulse.

Additionally, in this study advanced motion sensitising gradients were introduced. As illustrated in Fig. 4b, reverse bipolar gradient blips are inserted to achieve 0th and 2nd moment nulling.

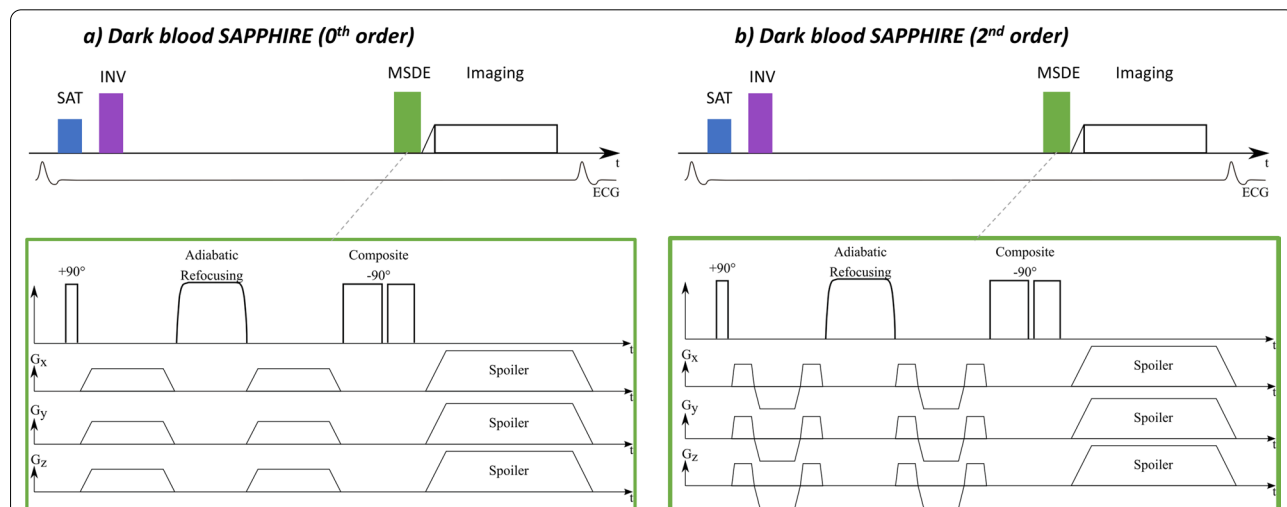
**Data analysis and statistics**

Statistical analysis was performed in R programming language (version 3.6.0, The R Foundation for Statistical Computing) and SPSS statistical software (version 26.0, IBM Corp., Armonk, NY, USA). Descriptive data are expressed as mean  $\pm$  standard deviation except where otherwise stated. The distribution of data was evaluated by histograms and Shapiro–Wilk test. Parametric and nonparametric continuous variables pertaining to participants were compared using student  $t$ -test or Mann–Whitney U test as appropriate. Categorical variables were compared by  $\chi^2$  or Fisher’s exact tests.

Linear mixed effect models were used to compare  $T_1$  times across SAPHIRE techniques (fixed effects: e.g. systolic vs. diastolic, 1.5 T vs. 3 T, slice level) accounting for repeatedness (random effect: subject ID). In addition, paired-samples  $t$ -test (parametric) or related-samples Wilcoxon signed rank test (non-parametric) were used for pairwise comparisons between MOLLI and SAPHIRE, and within SAPHIRE, across field strengths using Bonferroni correction.

Differences in transeptal  $T_1$  mapping profiles between sequences were assessed using two samples Anderson–Darling test as it gives more weight to the tails of the distribution (that is close to the blood-myocardial interface which was of particular interest to us). Two-sided  $p$ -values  $< 0.05$  were considered significant.

Intra- and inter-observer variability (absolute agreement) of  $T_1$  mapping times were assessed using two-way random, single measures intraclass correlation coefficient (ICC).



**Fig. 4** Sequence diagrams of the SAPHIRE dark blood  $T_1$  mapping variants with 0th (a) and 2nd (b) order flow sensitizing gradients. MSDE, Motion-sensitized driven equilibrium. Other abbreviations as in Figs. 1 and 3



**Table 2** Demographic and CMR characteristics of the healthy volunteers

Healthy volunteers (n = 10)	
<b>Demographics</b>	
Age, years	36 ± 10
Female	8 (80%)
Height, cm	168.4 ± 8.7
Weight, kg	71.6 ± 13.3
BSA, m <sup>2</sup>	1.8 ± 0.2
<b>CMR parameters</b>	
LAVi, mL/m <sup>2</sup>	11.0 ± 2.1
RAVi, mL/m <sup>2</sup>	11.3 ± 1.3
LVEDVi, mL/m <sup>2</sup>	74.6 ± 0.2
LVESVi, mL/m <sup>2</sup>	27.6 ± 0.2
LVEF, %	63 ± 5.1
MAPSE, mm	15.3 ± 2.7
LV MWT, mm	7.8 ± 1.0
LVMi, g/m <sup>2</sup>	48.3 ± 12.5
RVEDVi, mL/m <sup>2</sup>	75.1 ± 9.0
RVESVi, mL/m <sup>2</sup>	38.6 ± 9.9
RVEF, %	49 ± 10.2
RVMi, g/m <sup>2</sup>	25.8 ± 4
TAPSE, mm	25.3 ± 3.1

Data reported as mean ± 1SD or count (%) as appropriate

BSA, body surface area; CMR, cardiovascular magnetic resonance; LAVi, left atrial volume; LVEDVi, left ventricular end-diastolic volume indexed to body surface area; LVEF, left ventricular ejection fraction; LVESVi, left ventricular end-systolic volume indexed to body surface area; LVMi, left ventricular mass; MAPSE, mitral annular plane systolic excursion; MWT, maximum wall thickness; RAVi, right atrial volume; RVEDVi, right ventricular end-diastolic volume indexed to body surface area; RVEF, right ventricular ejection fraction; RVESVi, right ventricular end-systolic volume indexed to body surface area; SD, standard deviation; TAPSE, tricuspid annular plane systolic excursion

## Results

### Study population characteristics

Demographic and CMR characteristics of the 10 healthy volunteers (8 females, age 36 ± 10 years) are presented in Table 2.

### Feasibility in vivo

SAPPHERE T<sub>1</sub> mapping using all 4 variants was completed successfully in all subjects (Tables 3, 4). Each SAPPHERE T<sub>1</sub> map was acquired within a standard single breathold not dissimilar from a conventional MOLLI acquisition. ROI placement for RV T<sub>1</sub> mapping was not feasible using MOLLI or diastolic SAPPHERE because of insufficient wall thickness, but it was possible using systolic, 0th order and 2nd order DB SAPPHERE and results are reported in Table 4

### Inter-field strength differences

Healthy volunteer native myocardial T<sub>1</sub> times obtained by the 4 SAPPHERE variants and by MOLLI across field strengths are reported in Table 3, and global LV T<sub>1</sub> times provided in Fig. 5. As expected, for each sequence T<sub>1</sub> times were consistently higher at 3 T than at 1.5 T (all  $p < 0.005$ , Fig. 6).

### Differences between SAPPHERE variants and MOLLI

Native myocardial T<sub>1</sub> times by MOLLI for study members at either field strength matched the normal values by this sequence previously established at our center (reported in Table 3). As expected, from the known higher accuracy of saturation-based vs. inversion recovery-based T<sub>1</sub> mapping sequences [20], the 4 SAPPHERE variants measured longer global myocardial T<sub>1</sub> times than MOLLI (pairwise

**Table 3** Summary of LV T<sub>1</sub> mapping data by MOLLI and the 4 SAPPHERE variants across field strengths

Sequence	Field Strength	Basal SAX	Mid SAX	Apical SAX	Mid Septal ROI	Global T <sub>1</sub>	Non-apical Global T <sub>1</sub>
MOLLI*	1.5 T	1032 ± 23	1029 ± 26	1030 ± 21	1037 ± 28	1034 ± 7	1031 ± 2
	3 T	1297 ± 27	1297 ± 26	1311 ± 32	1310 ± 36	1298 ± 9	1295 ± 3
Diastolic SAPPHERE	1.5 T	1261 ± 45	1267 ± 33	1342 ± 60	1250 ± 79	1284 ± 11	1264 ± 3
	3 T	1637 ± 83	1596 ± 48	1593 ± 70	1603 ± 53	1601 ± 17	1612 ± 6
Systolic SAPPHERE	1.5 T	1286 ± 51	1225 ± 21	1239 ± 18	1225 ± 42	1239 ± 9	1253 ± 5
	3 T	1580 ± 41	1586 ± 44	1596 ± 43	1585 ± 48	1596 ± 13	1591 ± 4
DB 0th order SAPPHERE	1.5 T	1229 ± 57	1248 ± 30	1246 ± 55	1228 ± 78	1241 ± 10	1242 ± 3
	3 T	1571 ± 69	1595 ± 46	1608 ± 42	1597 ± 74	1596 ± 12	1584 ± 5
DB 2nd order SAPPHERE	1.5 T	1235 ± 46	1225 ± 61	1298 ± 51	1220 ± 111	1251 ± 11	1237 ± 5
	3 T	1550 ± 65	1555 ± 64	1569 ± 31	1503 ± 132	1561 ± 20	1561 ± 4

Values reported are mean ± 1SD

\*At our CMR Unit (the UCL Bloomsbury Center for Clinical Phenotyping) normal values for native myocardial T<sub>1</sub> by MOLLI in healthy volunteers are 1030 ± 32 ms at 1.5 T and 1280 ± 46 ms at 3 T

DB, Dark blood; MOLLI, Modified Look-Locker inversion recovery; ROI, region of interest; SAPPHERE, SATuration Pulse Prepared Heart-rate independent Inversion Recovery; SAX, short axis; T, Tesla. Other abbreviations as in Table 1

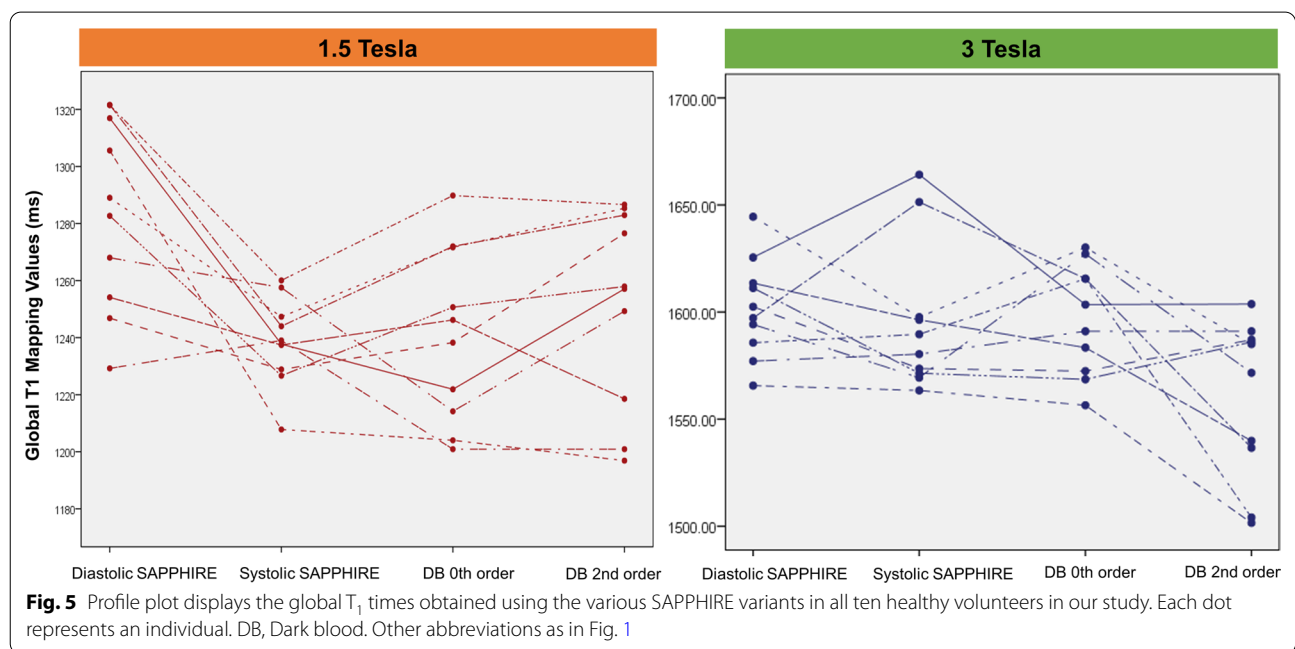
**Table 4** Summary of RV T<sub>1</sub> mapping times by MOLLI and the 4 SAPHIRE variants across field strengths

Sequence	Field Strength	Basal SAX (inferior or free wall)	Mid SAX (inferior wall)	Mid SAX (free wall)	Global T1ROI
MOLLI*	1.5 T	NA	NA	NA	NA
	3 T	NA	NA	NA	NA
Diastolic SAPHIRE*	1.5 T	NA	NA	NA	NA
	3 T	NA	NA	NA	NA
Systolic SAPHIRE	1.5 T	1531 ± 94	1479 ± 98	1422 ± 58	1477 ± 83
	3 T	1766 ± 14	1757 ± 51	1769 ± 31	1764 ± 32
DB 0th order SAPHIRE	1.5 T	1440 ± 67	1453 ± 122	1453 ± 104	1448 ± 98
	3 T	1724 ± 37	1681 ± 43	1689 ± 49	1698 ± 43
DB 2nd order SAPHIRE	1.5 T	1524 ± 44	1417 ± 82	1452 ± 54	1464 ± 60
	3 T	1684 ± 101	1667 ± 63	1658 ± 78	1670 ± 81

Values reported are mean ± 1SD

\*RV measurements were obtained only when the RV wall thickness ≥ 5 mm and this was not achievable with MOLLI or diastolic SAPHIRE

DB, Dark blood; MOLLI, Modified Look-Locker inversion recovery; ROI, region of interest; RV, right ventricle; SAPHIRE, SAturation Pulse Prepared Heart-rate independent Inversion REcovery; SAX, short axis; T, Tesla. Other abbreviations as in Table 1



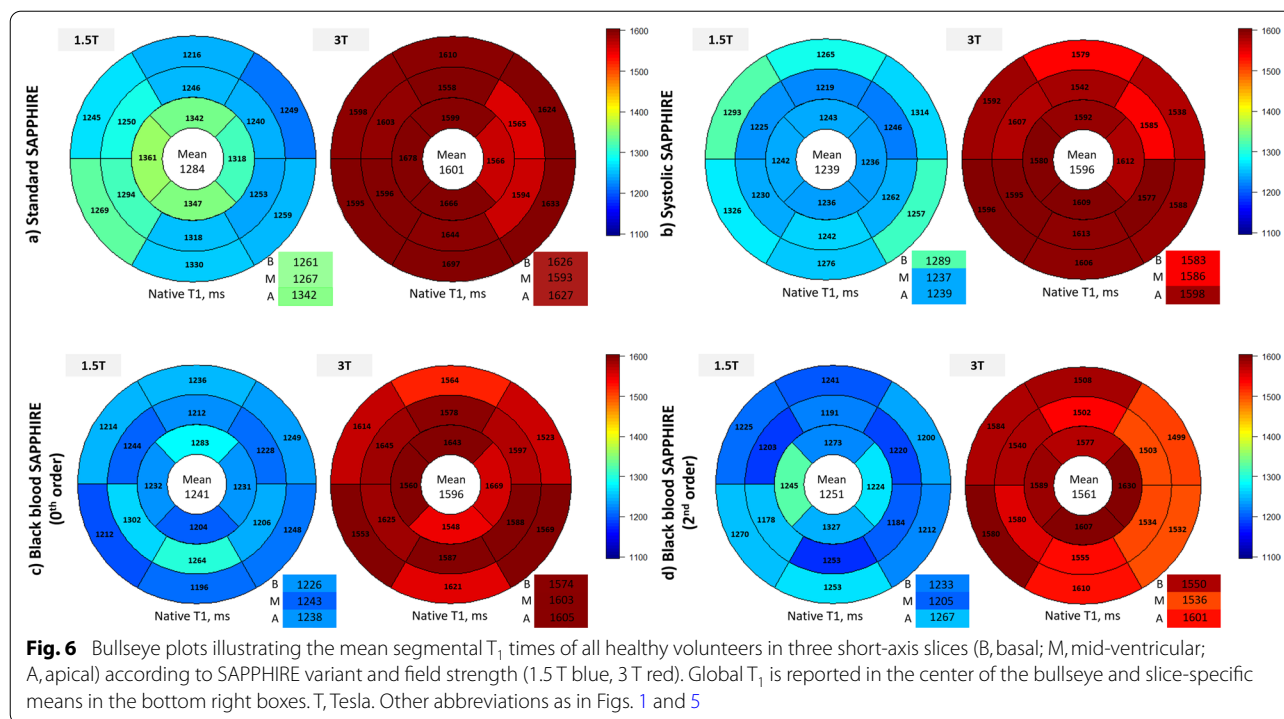
comparisons all  $p < 0.005$ , Additional file 1: Table S1). These differences persisted after removing the apical slice data (Additional file 1: Table S2,  $p < 0.005$ ).

**Differences between SAPHIRE variants**

Using linear mixed models to adjust for field strength, phase, slice location and subject, myocardial T<sub>1</sub> times by diastolic SAPHIRE were significantly longer than with systolic, 0th order DB and 2nd order DB SAPHIRE at 1.5 T and significantly longer than with systolic and 2nd order DB SAPHIRE at 3 T (all  $p < 0.05$ , Fig. 7a). After

excluding the apical slice the myocardial T<sub>1</sub> times by diastolic SAPHIRE were significantly longer than with systolic, 0th order DB and 2nd order DB SAPHIRE at both field strengths (all  $p < 0.05$ , Fig. 7b).

At 1.5 T pairwise comparisons for LV global T<sub>1</sub> showed that diastolic SAPHIRE measured significantly longer T<sub>1</sub> times than the 0th order DB SAPHIRE ( $p = 0.014$ , Additional file 1: Table S1) but not after excluding the apical slice data (Additional file 1: Table S2). Pairwise comparisons of RV T<sub>1</sub> times showed no differences between DB SAPHIRE variants (all  $p > 0.005$ , Additional



file 1: Table S3). At 3 T systolic SAPHIRE measured significantly longer RV  $T_1$  times than the 0th order and 2nd order SAPHIRE ( $p=0.028$  and  $0.001$ , respectively) but no such differences were observed at 1.5 T (all  $p>0.05$ ).

**Transmural  $T_1$  mapping profiles of MOLLI and SAPHIRE variants**

Figure 8a shows native  $T_1$  maps from MOLLI and the 4 SAPHIRE variants. Transmural  $T_1$  times (Fig. 8b) in the mid septum immediately adjacent to the LV and RV blood pools were longer by MOLLI and diastolic SAPHIRE when compared to systolic, 0th order DB and 2nd order DB SAPHIRE. Contamination from the high  $T_1$  of the blood pool appeared as an upsloping  $T_1$  profile near the edges of the septal profile for both MOLLI and diastolic SAPHIRE sequences, but not for the other SAPHIRE variants. Indeed, the profile distributions of transmural myocardial  $T_1$  times by the Anderson–Darling test differed significantly between MOLLI and all 4 SAPHIRE variants (diastolic  $p=0.0003$ ; systolic  $p=0.0003$ ; 0th order DB  $p=0.024$ ; 2nd order DB  $p=0.025$ ); between diastolic SAPHIRE and both DB variants (0th order DB  $p=0.0003$ ; 2nd order DB  $p=0.001$ ); and between systolic SAPHIRE and both DB variants (0th order DB  $p=0.0003$ ; 2nd order DB  $p=0.0005$ ). Furthermore, the dispersion of transmural  $T_1$  times across the mid septum for systolic ( $1233 \pm 22$  ms; interquartile range [IQR]=25.3 ms) and DB SAPHIRE variants (0th order:

$1206 \pm 46$  ms; IQR=71.0 ms | 2nd order:  $1178 \pm 52$  ms; IQR=72.9 ms) was narrower when compared to diastolic SAPHIRE ( $1263 \pm 86$  ms; IQR=142.8 ms), and the dispersion for systolic SAPHIRE narrower than of MOLLI ( $1054 \pm 42$  ms; IQR=56.4 ms).

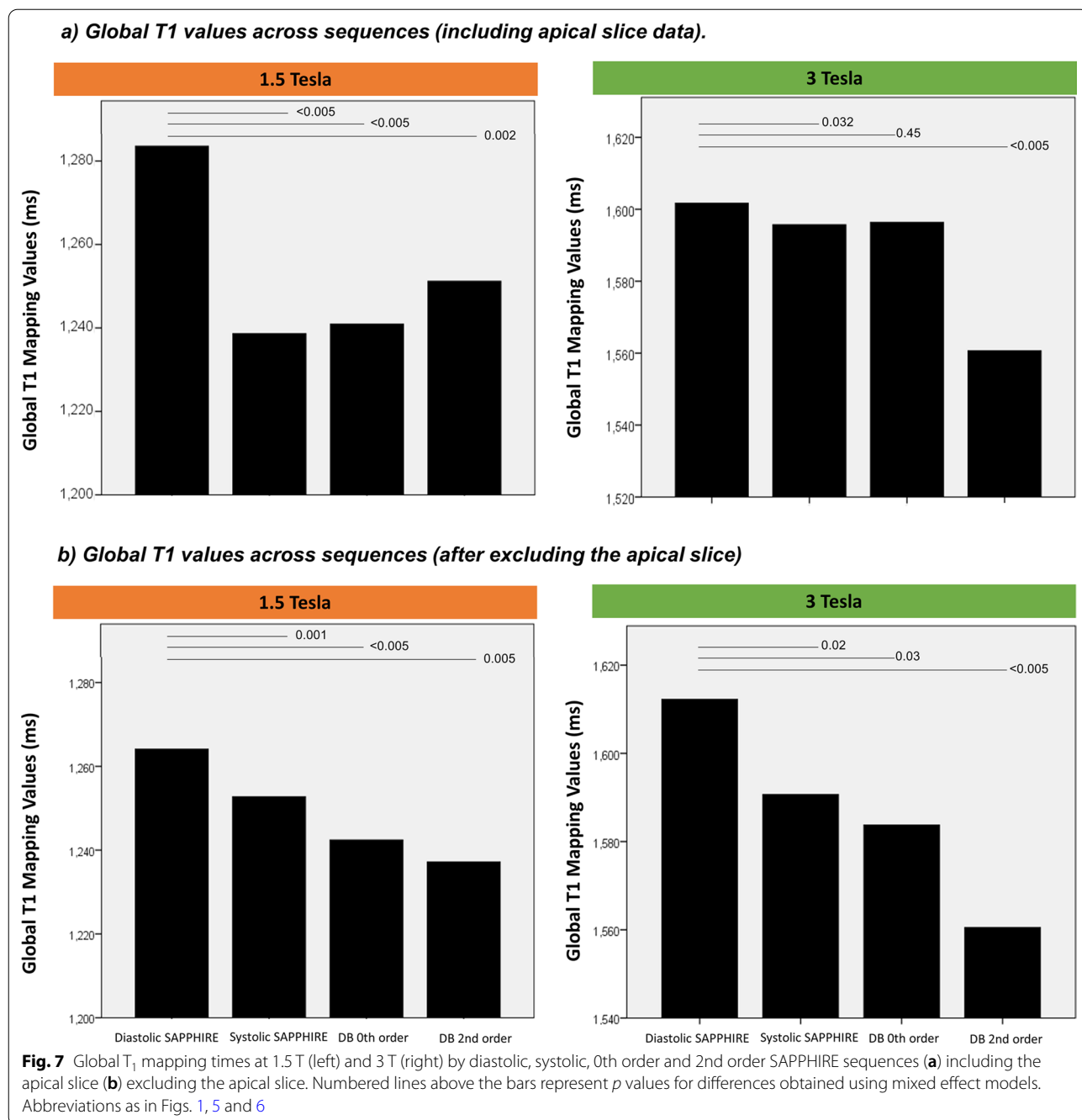
**Re-read variability of  $T_1$  mapping measurements**

Intra- and interobserver variability of myocardial  $T_1$  reads was excellent across all sequences tested with ICCs ranging from 0.953–0.996 (Table 5).

**Discussion**

This study assessed the feasibility of biventricular SAPHIRE  $T_1$  mapping in vivo across field strengths. We found that native  $T_1$  was significantly shorter by the systolic, 0th order DB and 2nd order DB SAPHIRE variants compared to diastolic SAPHIRE across field strengths. We show that systolic and DB SAPHIRE variants reduce the dispersion of trans-myocardial  $T_1$  times across the septum and abolish the artefactual  $T_1$  lengthening in voxels located at the blood-myocardial/epicardial boundaries that remains a visible problem for both MOLLI and diastolic SAPHIRE. Combined, these data suggest that systolic and DB SAPHIRE approaches may help counteract the problem of partial volume effects. According to these data, the 0th and 2nd order DB SAPHIRE sequences appear to be



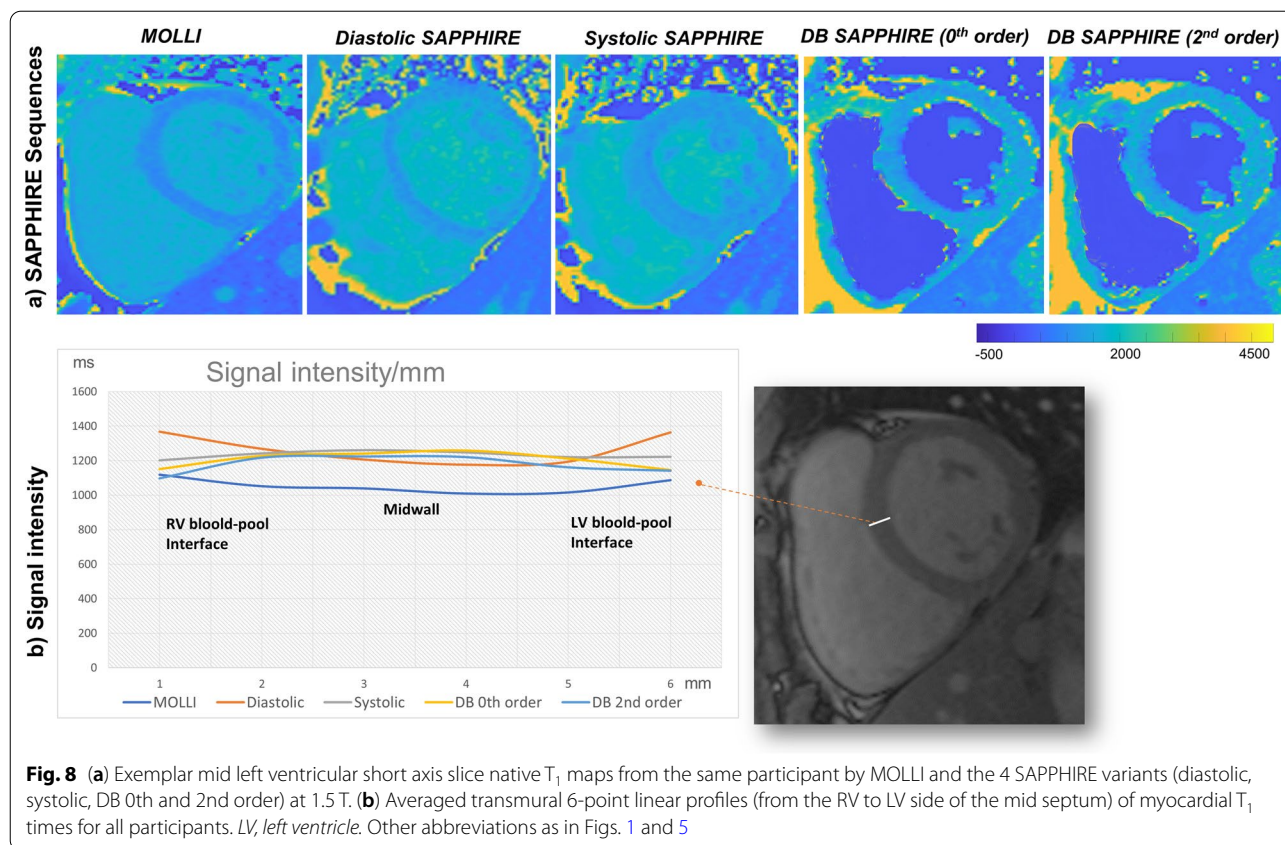


equivalent at preventing myocardial T<sub>1</sub> signal contamination by the adjacent blood pool. Systolic SAPHIRE was the sequence that produced the narrowest dispersion of myocardial T<sub>1</sub> times across the mid septum.

Previous work at 3 T has suggested that native myocardial T<sub>1</sub> in health lengthens progressively from base to apex [21, 22] and we observed a similar trend by MOLLI at 3 T but not at 1.5 T, and not with the majority of SAPHIRE variants used in this study. The most

likely explanation for the lengthening T<sub>1</sub> from base to apex is that partial volume effects are more prevalent in the thinner more apical segments, and exacerbated by the natural curvature of the apical cap.

Results from linear mixed model analysis showing that native T<sub>1</sub> was longer by diastolic than systolic SAPHIRE at both field strengths, are in agreement with previous work [9, 11, 23, 24]. It has been postulated that in systolic T<sub>1</sub> mapping these differences were due to reduced partial



**Fig. 8** (a) Exemplar mid left ventricular short axis slice native  $T_1$  maps from the same participant by MOLLI and the 4 SAPHIRE variants (diastolic, systolic, DB 0th and 2nd order) at 1.5 T. (b) Averaged transmural 6-point linear profiles (from the RV to LV side of the mid septum) of myocardial  $T_1$  times for all participants. *LV*, left ventricle. Other abbreviations as in Figs. 1 and 5

**Table 5** Re-read variability of  $T_1$  mapping measurements

Sequence	Region	Intra-observer ICC (95% CI)	Inter-observer ICC (95% CI)
MOLLI	Average mid	0.989 (0.91–0.99)	0.968 (0.76–0.99)
	Septal ROI	0.978 (0.78–0.99)	0.950 (0.53–0.99)
Diastolic SAPHIRE	Average mid	0.996 (0.45–0.99)	0.993 (0.82–0.99)
	Septal ROI	0.987 (0.89–0.99)	0.954 (0.52–0.99)
Systolic SAPHIRE	Average mid	0.957 (0.64–0.99)	0.953 (0.54–0.99)
	Septal ROI	0.964 (0.66–0.99)	0.982 (0.87–0.99)
0th order DB SAPHIRE	Average mid	0.994 (0.95–0.99)	0.984 (0.50–0.99)
	Septal ROI	0.991 (0.76–0.99)	0.986 (0.84–0.99)
2nd order DB SAPHIRE	Average mid	0.973 (0.78–0.99)	0.967 (0.47–0.99)
	Septal ROI	0.994 (0.79–0.99)	0.992 (0.88–0.99)

Agreement was considered excellent when ICC > 0.74, good when ICC = 0.60–0.74, fair when ICC = 0.40–0.59 and poor when ICC < 0.4  
 CI, confidence interval; ICC, intraclass correlation coefficient. Other abbreviations as in Tables 1 and 2

volume effects thanks to the increased LV wall thickness. The fact that 0th order and 2nd order DB SAPHIRE  $T_1$  times were significantly shorter than diastolic SAPHIRE suggests that blood pool suppression is another potential solution for the problem of partial volume effects.

We observed that the RV free wall was visible and indeed analysable on the short axis cine slices by systolic and DB SAPHIRE approaches but hardly visible at

all by conventional bright blood SAPHIRE or MOLLI. We found that RV  $T_1$  was significantly longer than LV  $T_1$  which might be due to residual partial voluming and/or the naturally higher collagen content of the RV [25]. The published literature provides conflicting data on the relationship between RV and LV  $T_1$ , with groups reporting higher RV  $T_1$  [26–28], lower RV  $T_1$  [29] or equivalent RV/LV  $T_1$  reads [30] in various cohorts, not all of which were

healthy controls as in our case. Although we took care to draw precise ROIs in the RV myocardium, partial voluming and contamination of RV  $T_1$  times from the inadvertent inclusion of voxels contaminated by blood pool or epicardial fat signals are plausible pitfalls that could have artefactually lengthened our native RV myocardial  $T_1$  times.

Overall, the evidence presented in this study suggests that systolic and DB approaches are less prone to partial volume effects than MOLLI and diastolic SAPPHIRE. The transeptal myocardial  $T_1$  times immediately adjacent to LV/RV blood pools recorded for 0th and 2nd order DB SAPPHIRE were significantly lower than those recorded for systolic SAPPHIRE (Fig. 8b) suggesting that blood pool nulling achieved by the DB  $T_1$  mapping approaches provides some additional benefit thanks to the reduced sensitivity to partial volume effects. Future work should continue to explore the potential clinical utility of DB SAPPHIRE  $T_1$  mapping for the study of thin-walled cardiac structures, such as the RV free wall, atria and apical slices.

We report excellent intra- and inter-observer re-read reproducibility for all the methods studied with all ICCs (>0.90) being well in line with previous reports [8, 21, 23, 24, 31–34].

In this study we also demonstrate the use of higher order gradient moment nulling for dark blood  $T_1$  mapping. In previous literature 0th order nulling was found to be susceptible to residual myocardial motion in some cases, necessitating fine tuning of the motion sensitising gradient moment. As the residual cardiac motion is less turbulent compared to blood flow, stronger motion sensitizing gradients may be applied when nulling the gradient moment up to the 2nd order. Even though quantification results were comparable between 0th and 2nd order DB SAPPHIRE in our experiments, 2nd order nulling may have the advantage of increased ease of use for clinical translation. Robustness of higher order gradient nulling for DB  $T_1$  mapping, thus, warrants further investigation in a patient cohort.

### Limitations

This small-scale single-center, single-vendor feasibility study includes a small number of healthy volunteers, the results hold promise to overcome some conventional  $T_1$  mapping limitations. Further work with larger cohorts in health and disease are needed to explore the robustness and validation. The establishment of normal values for  $T_1$  by SAPPHIRE was beyond the scope of this study.

Comparison to other  $T_1$  mapping sequences besides MOLLI was not undertaken and neither was post-contrast  $T_1$  mapping. Future work will need to examine the clinical utility of these SAPPHIRE sequences in patients with arrhythmia, cardiomyopathy and for the study of

other thin-walled cardiac structures such as the atria. RV  $T_1$  analysis was not possible on MOLLI or diastolic SAPPHIRE due to the RV thickness limitation. MOCO was used for MOLLI sequences but not for the SAPPHIRE  $T_1$  mapping sequences. Future work should seek to assess the impact of heart rate (HR) variability on the spin dynamic in the systolic SAPPHIRE sequence. This study was not specifically designed to examine the impact of HR on the quality of systolic data; nevertheless we had a broad range of resting HRs across study members (from 56 to 89 bpm). We observed good quality raw systolic images and reconstructed maps regardless of HR (Additional file 1: Figure S1).

Further testing and validation of the systolic SAPPHIRE sequence will be needed to understand its robustness in relation to RV  $T_1$  mapping, but our preliminary findings at least indicate that systolic SAPPHIRE  $T_1$  mapping permits placement of a decent-sized ROI in the RV free wall, otherwise impossible with conventional  $T_1$  mapping approaches.

### Conclusion

These small-scale preliminary healthy volunteer data suggest that DB SAPPHIRE has the potential to reduce partial volume effects at the blood-myocardial interface, and that systolic SAPPHIRE could be a feasible solution for right ventricular  $T_1$  mapping. Further work is needed to understand the robustness of these sequences and their potential clinical utility.

### Abbreviations

BSA: Body surface area; bSSFP: Balanced steady-state free precession; CI: Confidence interval; CMR: Cardiovascular magnetic resonance; CVI42: Circle Cardiovascular Imaging 42; DB: Dark-blood; ECG: Electrocardiogram; FA: Flip angle; HR: Heart rate; ICC: Intraclass correlation coefficient; LAVi: Left atrial volume indexed to body surface area; LV: Left ventricle; LVEDVi: Left ventricular end-diastolic volume indexed to body surface area; LVEF: LV ejection fraction; LVESVi: Left ventricular end-systolic volume indexed to body surface area; LVMI: Left ventricular mass indexed to body surface area; MAPSE: Mitral annular plane systolic excursion; MOCO: Motion correction; MOLLI: Modified look-locker inversion recovery; MSDE: Motion sensitized driven equilibrium; MWT: Maximum wall thickness; NIHR RD-TRC: National institute for health research rare diseases translational research collaboration; RAVi: Right atrial volume indexed to body surface area; ROI: Region of interest; RV: Right ventricle; RVEDVi: Right ventricular end-diastolic volume indexed to body surface area; RVEF: Right ventricular ejection fraction; RVESVi: Right ventricular end-systolic volume indexed to body surface area; SAPPHIRE: Saturation-pulse prepared heart-rate independent inversion-recovery; SAX: Short axis; SD: Standard deviation; T: Tesla; TAPSE: Tricuspid annular plane systolic excursion; TD: Trigger delay; TI: Inversion time; TR/TE: Time between two consecutive excitations/echo time; UCL: University College London.

### Supplementary Information

The online version contains supplementary material available at <https://doi.org/10.1186/s12880-022-00843-0>.

**Additional file 1.** Saturation-Pulse Prepared Heart-rate independent Inversion-Recovery (SAPPHIRE) Biventricular  $T_1$  Mapping: Inter-Field

Strength, Head-To-Head Comparison of Diastolic, Systolic and Dark-Blood Measurements. **Table S1.** Pairwise comparison of global T1 values across sequences (including apical slice data). **Table S2.** Pairwise comparison of global T1 values across sequences after excluding the apical slice. **Table 3.** Pairwise comparison of RV T1 values across sequences. **Figure s1.** Systolic SAPHIRE T1 mapping across a range of resting heart rates.

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### Author contributions

M.A. analysed the data, performed the statistical analysis and wrote the manuscript. J.B.A., K.D.K. and G.C. collected and acquisitioned the data. J.B.A., K.D.K., N.F., P.K.M. and S.W. contributed to data analysis and review of the manuscript. R.B., A.D.H. and J.C.M. have substantially revised the manuscript. G.C., S.W. and J.C.M. conceived of the project. All authors have read and approved the submitted version and all other substantially modified versions. All authors have agreed both to be personally accountable for their own contributions and to ensure that questions related to the accuracy or integrity of any part of the work, even ones in which the author was not personally involved, are appropriately investigated, resolved, and the resolution documented in the literature. All authors read and approved the final manuscript.

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### Availability of data and materials

The datasets used and/or analysed during the current study are available from the corresponding author on reasonable request.

### Declarations

#### Ethics approval and consent to participate

The study received ethical approval from the University College London (UCL) Research Ethics Committee. All subjects provided written informed consent.

#### Competing interests

The authors declare that they have no competing interests.

#### Consent for publication

Not applicable.

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