Nucleic acid aptamers for targeting of shRNAbased cancer therapeutics

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Abstract: Aptamers are nucleic acid ligands which have been validated to bind to epitopes with a specificity similar to that of monoclonal antibodies. Aptamers have been primarily investigated for their direct function in terms of inhibition of protein targets; however, recent evidence gives reason to actively explore aptamers as targeting moieties for delivery of anticancer therapeutics. Many aptamers have been developed to bind to extracellular membrane domains of proteins overexpressed on cancer cells and have the potential to be modified for use in targeting cancer therapeutics. The use of DNA vector-based short hairpin RNA (shRNA) for RNA interference (RNAi) is a precise means for the disruption of target gene expression but its clinical usage in cancer is limited by obstacles related to delivery into cancer cells. Nucleic acid aptamers are attractive candidates for targeting of shRNA therapies. Their small size, ease of production and modification, and high specificity are valued attributes in comparison to other targeting moieties currently being tested. Here we review the development of aptamers directed to PSMA, Nucleolin, HER-3, RET, TN-C, and MUC1 and focus on their potential for use in targeting of shRNA-based cancer therapeutics.

Keywords: aptamer, tumor targeting, oligonucleotides therapeutics, cancer, shRNA, gene therapy

Introduction

Delivery vehicles optimal for shRNA delivery ideally are targeted in order to maximize biodistribution to the cancer cell population, thereby increasing their effectiveness in the clinical setting and minimizing potentially adverse off target (ie, nonmalignant) cell effects. Tumor cellular uptake at the target site(s) can be enhanced by conferring to the delivery vehicle the ability to recognize surface features of the target cells. This can be accomplished most readily by recognizing surface antigens or promoting receptor mediated endocytosis. Delivery vehicles can be complexed with monoclonal antibodies, peptides, small molecule ligands, and aptamers to recognize cell surface markers (Lu and Low 2002; Dyba et al 2004; Stefanidakis and Koivunen 2004; Hughes and Rao 2005).

Aptamers are noncoding nucleic acid oligomers made from either RNA or DNA. Much like tRNA, they fold through intramolecular bonds into varied tertiary structures. The folded structure of aptamers creates binding pockets that allow the molecules to interact with the three dimensional structure of specifi c domains on a protein's surface. Aptamers bind to epitopes with affinity comparable to that of monoclonal antibodies. Their dissociation constants are often in the picomolar to low nanomolar range. Because of their high surface area, the area in contact with the target is large, minimizing the chances of off target effects by increasing binding specificity. In some cases aptamers can inhibit the function of a target protein by binding to its active site, or inducing a conformational change, or inhibiting dimerization or DNA binding (Lupold et al 2002; Umehara et al 2004; Shi et al 2007).

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The idea of developing nucleic acid ligands for therapeutic purposes was born out of the study of activation of viral gene expression during HIV infection. There exists a nucleic acid ligand that binds specifically to a transactivator of human immunodeficiency virus type 1 (HIV-1) gene called Tat. The Tat protein normally binds to an RNA stem-loop structure called a trans-acting response element (TAR) which occurs within the first 60 nucleotides of all HIV-1 transcripts, thus activating expression of viral genes. A series of studies showed that overexpression of TAR sequence decoys conferred HIV-1 resistance to cells, presumably because the TAR oligonucleotides bound specifically to the Tat protein, thus inhibiting it from activating viral gene expression (Sullenger et al 1990; Sullenger et al 1991; Held et al 2006).

Since this initial discovery, a wide range of potential therapeutic applications for aptamers have been proposed and pursued (Bunka and Stockley 2006). Aptamers have been successfully developed against extracellular protein ligands, such as transforming growth factor receptors, platelet-derived growth factor, basic fibroblast growth factor, and vascular endothelial growth factor (VEGF) as well as intracellular proteins such as NFkb (Jellinek et al 1995; Golden et al 2000; Cassiday and Maher 2001; Pietras et al 2001; Ohuchi et al 2005, 2006; McCauley et al 2006). Pegaptanib, an aptamer that binds to and inhibits VEGF has been approved by the FDA for treatment of age related macular generation (Ng et al 2006). Aptamers that bind to blood coagulation factors VIIa and IXa are being investigated as anticoagulants (Rusconi et al 2002). A subset of aptamers that have been developed for therapeutic purposes have the potential to be used as targeting moieties for shRNA.

Aptamers represent an attractive alternative to traditional methods of targeting cancer gene therapy by circumventing many of the stumbling blocks that inhibit the effectiveness of these methods. Aptamers are smaller than monoclonal antibodies. With a molecular weight of 10–15 kDa they are one order of magnitude lighter than antibodies used for targeting, which have an average molecular weight of 150 kDa (White et al 2000). Aptamers are also less immunogenic than antibodies (Drolet et al 2000; Pestourie et al 2005; Apte et al 2007), making them more suited to systemic administration and long term therapy.

Aptamers can facilitate cell entry of an shRNA delivery vehicle in similar ways as traditional targeting moieties. Aptamers to the extracellular domains of transmembrane receptor proteins can penetrate the cell membrane by receptor mediated endocytosis (Hughes and Rao 2005). When aptamers bind to cell surface proteins they increase

the proximity of the delivery vehicle and the cell membrane. This facilitates charge interactions between a positively charged delivery vehicle and the negatively charged membrane that result in internalization of the payload. Here we will briefly review the process of aptamer development and then give examples of the current development of aptamers directed to good candidate proteins for tumor targeting.

Here we review the development of aptamers directed to PSMA, Nucleolin, HER-3, RET, TN-C, and MUC1 and focus on their potential for use in targeting of shRNA-based cancer therapeutics. Though most of these aptamers have not yet been used as shRNA targeting moieties in vivo this selection of aptamers represents a group that is well suited to the targeting shRNA-based cancer therapies thereby enhancing their efficiency and safety.

Aptamer production

RNA and DNA aptamers with specific binding properties can now be amplified in vitro from libraries through a streamlined, automated iterative selection process. Because of their small, relatively simple structure, the chemical modification of aptamers to increase serum stability or bioavailability can be accomplished readily. The production and modification of aptamers is very uncomplicated when compared to the production of monoclional antibodies, which require prokaryotic or eukaryotic expression systems. The chemical methods involved are well defined and easily conformable to good manufacturing process requirements, which has eased the transition of aptamers into the clinical setting.

Aptamers that bind to a specific target are isolated from a group of candidate oligonucleotides, either RNA or DNA, through 'systematic evolution of ligands by exponential enrichment' (SELEX) (Tuerk and Gold 1990). SELEX is an in vitro process that can be automated to allow the rapid production of aptamers (Cox et al 2002; Ellington et al 2005).

The SELEX process begins with a degenerate sequence library of $\geq 10^{15}$ molecules. With a library of this size it is likely that there is a molecule that will bind to almost any target (Ellington and Szostak 1990). The library is then treated with the target molecule at physiological pH and temperature. After some aptamers bind the aptamer-target complexes are partitioned from the nonbinding aptamers and bound species are regenerated and amplified by PCR in the case of DNA aptamers or RT-PCR in the case of RNA aptamers. The amplified molecules are then subjected to

another round of the selection process. Over this repetitive process of binding and amplification the pool is enriched for aptamers that bind most efficiently to the target (Gopinath 2007). SELEX can also be tailored by ligation and cleavage of small 10nt fixed primer sites before and after amplification. These smaller primer sequences allow the isolation of shorter aptamer sequences which can later be more readily synthesized chemically (Vater et al 2003).

Whole-cell SELEX is a procedure that has been developed for the selection of aptamers to extracellular matrix proteins and transmembrane proteins. It involves the introduction of cells overexpressing the protein target of interest to oligomer libraries. This procedure offers the advantage of selecting molecules more suited to recognizing their target in its natural glycosylation state under physiological conditions. Because of the great variety of proteins of the cell surface, a second set of traditional SELEX with the purified protein is sometimes necessary to obtain a purified specific aptamer product (Hicke et al 2001; Cerchia et al 2005; Ohuchi et al 2005). This method has been used to isolate aptamers that bind to human transforming growth factor-beta type III receptor displayed on cell surface (Ohuchi et al 2005, 2006).

Naked nucleotide oligomers are in general very unstable in the blood and are unsuitable for therapeutic or targeting applications. One study showed that an unmodified aptamer against thrombin had an in vivo serum half-life of only 108 seconds (Griffin et al 1993). A variety of chemical modifications can be applied to nucleic acid aptamers during and after the SELEX process in order to increase their suitability for systemic tumor targeting (Table 1). Natural nucleotides within aptamers can be substituted with 2' fluoro, O-methyl, or amino modified or 4' thio modified nucleotides that are poor substrates for nuclease degradation (Beigelman et al 1995; Gold et al 1995; Burmeister et al 2005; Kato et al 2005) $3'$ end caps can also be modified to confer nuclease resistance (Burmeister et al 2005). Aptamers can be bound to bulky lipids or polymers to reduce their renal clearance and increase their serum half-life (Boomer et al 2005). Aptamer intramolecular bonds can be altered to increase structural stability (Schmidt et al 2004). Beyond chemical modifications to increase stability, aptamers can also be modified with small functional groups to facilitate their attachment as targeting moieties to polymeric or lipid shRNA delivery vehicles. Amino groups have been added to aptamers in order to facilitate their conjugation to a nanoparticle composed of poly(lactic acid)-block-polyethylene glycol copolymer with a terminal carboxylic acid functional group (Farokhzad et al 2004).

Likely candidates for aptamer mediated cancer targeting

The following cell surface proteins are good candidates for tumor targeting. Aptamers are actively being developed for all of them, whether for therapeutic or for targeting purposes (Table 2).

Prostate-specific membrane antigen (PSMA)

The most extensively studied aptamer for cancer targeting binds to the prostate-specific membrane antigen (PSMA). PSMA is a well described protein that is expressed in prostate cancer epithelial cells (Israeli et al 1994; Murphy et al 1998). Its use in targeting of many different types of cancer therapeutics is a constantly developing field. In normal prostate epithelial cells, it is primarily expressed as the intracellular protein referred to as PSM' but in prostate carcinoma the splice variant termed PSMA is overexpressed. PSMA, which is more pertinent for targeting purposes, is a type 2 integral membrane glycoprotein folate carboxypeptidase expressed exclusively in prostate acinar epithelium (Su et al 1995). Increased PSMA expression has been documented in prostatic intraepithelial neoplasia, prostatic adenocarcinoma, and in tumor associated neovasculature. Its expression generally increases with disease progression and metastasis (Bostwick et al 1998).

PSMA was originally described as the target for mAb 7E11in the androgen-dependent LNCaP human prostatic adenocarcinoma cell line (Horoszewicz et al 1987). Antibodies that bind to the extracellular domain of the PSMA are used clinically for imaging and staging of prostate cancer (Freeman et al 2002) and are in clinical trials to determine therapeutic potential (Bander et al 2005). Monoclonal antibodies to PSMA have also been used to target delivery of gene therapy in vivo (Moffatt et al 2006).

The practicality of PSMA as a target for various kinds of anticancer therapies has placed it in center stage of aptamerbased cancer targeting research. The first reported RNA aptamers selected to bind a tumor-associated membrane antigen were two 2'-fluoro-pyrimidine RNA oligomers that bind to the extracellular domain of the PSMA. These two aptamers, called xPSM-A9 and xPSM-A10, which share no consensus sequences, bind to the PSMA at different extracellular epitopes. Aptamer xPSM-A9 was shown to inhibit the PSMA noncompetitively with an average K(i) of 2.1 nM, while aptamer xPSM-A10 inhibits the PSMA competitively with an average $K(i)$ of 11.9 nM (Lupold et al 2002).

Table 1 Common chemical modifications of aptamers for tumor targeting

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The nuclease resistant xPSMA-A10 aptamer has been exploited to target the delivery of various nanoparticulate drug delivery systems. It has peen particularly well studied as a targeting moiety for biodegradable nanoparticles conjugated with chemotherapeutics. In one study, the xPSMA-A10 aptamer was bound to a poly(lactic acid)-block-polyethylene glycol (PEG) copolymer with a terminal carboxylic acid functional group (PLA-PEG-COOH) and used to deliver rhodamine-labeled dextran as a model drug in vitro. This study showed that the targeted nanoparticles preferentially bind to and are taken up in vitro by LNCaP prostate epithelial cells which express PSMA, but not by PC3 prostate epithelial cells, which do not express detectable levels of the PSMA (Farokhzad et al 2004).

In a more recent study, $5'$ -NH₂ modified xPSMA-A10 aptamers were conjugated to poly(D,L-lactic-*co*-glycolic acid)-*block*-poly(ethylene glycol) nanoparticles with terminal carboxylic acid groups (PLGA-PEG-COOH).

These nanoparticles were then encapsulated with the chemotherapeutic docetaxel and tested in vitro and in vivo. The docetaxel-encapsulated nanoparticle-aptamer (Dtxl-NP-Apt) bioconjugates enhanced in vitro cellular toxicity with LNCaP prostate epithelial cells as compared with nanoparticles that lack the PSMA aptamer. After a single intratumoral injection of Dtxl-NP-Apt bioconjugates using a murine LNCaP xenograft model of prostate cancer, complete tumor reduction was noted in five of seven nude mice. 100% of the mice that received the Dtxl-NP-Apt bioconjugate survived the 109-day study. In contrast, only two of seven mice that received the non-targeted Dtxl-NP had complete tumor reduction and only 57% of the mice in this group survived the 109-day study. Only 14% of mice treated with Dtxl alone survived the 109-day study (Farokhzad et al 2006). A similar study tested PLGA-PEG-COOH-xPSMA-A10 conjugates encapsulating docetaxel and 14C labeled paclitaxel. It was found that the surface association of nanoparticles with targeting aptamer significantly enhanced delivery to tumors when compared to equivalent but nontargeted nanoparticles in a murine LNCaP xenograft model (Cheng et al 2007).

PSMA aptamers are particularly attractive as targeting moities for RNAi-based cancer therapeutics because the PSMA itself participates in membrane recycling, becoming internalized through ligand induced endocytosis, thus facilitating entry of the therapeutic payload into the cytoplasm (Ghosh and Heston 2004). This property of the PSMA has been exploited in the targeting of therapeutic siRNAs to prostate cancers using aptamer-siRNA chimeras and conjugates. In one study, a 27mer anti-Lamin siRNA was noncovalently bound to xPSMA-A9 aptamers using a modular streptavidin bridge and tested in vitro to transfect PC3 cells and LNCaP cells that naturally expressed the PSMA. The conjugates were successfully transfected with this method and inhibition of lamin expression was achieved. The conjugates displayed similar transfection efficiency to oligofectamine controls but better specificity, as they were only taken up by PSMA expressing LNCaP cells and not PSMA-negative PC3 cells (Chu et al 2006).

In another study, aptamer-siRNA chimeras were used to target prostate cancer cells and knock out expression of survival genes. Chimeras of the xPSMA-A10 aptamer and polo-like kinase 1 (PLK1) and BCL2 siRNAs were generated via in vitro transcription from DNA templates. The chimeras were shown be internalized and promote apoptosis preferentially in PSMA expressing LNCaP cells and not PC3 control cells. This specificity was retained in murine LNCaP xenograft tumor models where chimeras bearing PLK1

siRNAs mediated pronounced tumor regression while having no statistically significant effect on non-PSMA expressing PC3 xenografts (McNamara et al 2006).

Nucleolin

An aptamer (AS1411) that binds to the external domain of the membrane protein nucleolin is has been well characterized because of its therapeutic potential. Due to the properties of the aptamer and the properties of nucleolin itself AS1411 is an excellent candidate for aptamer mediated targeting of gene therapy.

Human nucleolin is an abundant multifunctional 76 kDa membrane associated phosphoprotein that has 707 amino acids in its sequence (Derenzini et al 1995; Sarcevic et al 1997). It is composed of three main domains, an acidic histone-like NH2 terminus, a central domain containing four RNA-binding sub-domains, and a carboxy terminal domain that contains its four sites of phosphorylation (Lapeyre et al 1987; Ginisty et al 1999). Though it was originally characterized as a nucleolar protein, nucleolin is also present on the external cell membrane where it functions as a signaling receptor of poorly defined function (Hovanessian et al 2000; Storck et al 2007).

Though its function on the surface of cancer cells has not been clearly defined, Nucleolin has been extensively investigated in the context of cancer. It has been shown to be associated with survival, growth and proliferation of cells, nuclear transport, transcription, packing and transport of rRNA, and replication and recombination of DNA (Srivastava and Pollard 1999). In addition, overexpression of nucleolin is related to poor clinical prognosis for some cancer types (Derenzini et al 1995; Derenzini 2000).

One pathophysiologic function of cell surface nucleolin that makes it ideal for targeting anticancer therapies is its involvement in internalization of specific ligands. Nucleolin has been shown to bind to and internalize the heparin-binding growth factor midkine (Said et al 2002), the iron-binding lycoprotein lactoferrin (Legrand et al 2004), acharan sulfate (Joo et al 2005), as well as the tumor-homing 34-amino acid peptide (F3) (Christian et al 2003).

The aptamer known as AS1411 was first developed as AGRO100 by Aptamera (Louisville, KY). It is an unmodified guanosine rich 26-mer, which binds to nucleolin. AS1411 was originally investigated because of observations that guanosine-rich oligonucleotides (GRO) had nonantisensebased in vitro antiproliferative properties against cancer cells (Bates et al 1999). These oligonucleotides were further studied and it was found that the unmodified DNA phosphodiester GRO analog GRO29A-OH, which retains the G quartet structure essential for nucleolin binding (Dapic et al 2003), displayed resistance against serum nuclease degradation (Dapic et al 2002). AS1411 is simply GRO29A-OH with its three 5′ thymidines cleaved.

A nontraditional aptamer because of its G quartet-based binding to its target, AS1411 has been shown to bind to cell surface nucleolin and inhibit growth of many cancer cell lines in vitro such as the prostate cancer cell line DU145, the breast cancer cell lines MDA-MB-231 and MCF-7, the lung cancer cell line A549, as well as the cervical cancer cell line HeLa (Bates et al 1999; Dapic et al 2002).

In anticipation of its use as a therapeutic, biodistribution studies were realized to characterize the in vivo pharmacodymanics, distribution, and metabolism of the aptamer following IV administration. AS1411 metabolism was studied in mice bearing lung and renal human tumor xenografts derived from A549 and A498 cells using IV administration of AS1411 radiolabeled with tritiated thymidine. Following 1, 10, and 25 mg/kg IV boluses of [3H]AS1411, 63% of the radiolabeled aptamer was excreted in urine within 5 hours while less than 1% of the injected dose was detected upon analysis of bile, thus suggesting that the main mode of metabolism is renal. This same study also showed that AS1411 displayed dose related pharmacokinetics with an elimination half life of 2 days in plasma and whole blood. Regardless of the dose administered, tumor/blood ratios were 4:6 for the renal carcinoma xenograft and 2:4 and for the lung carcinoma xenograft, showing that the aptamer effectively accumulated in tumor tissue (Ireson and Kelland 2006).

In vivo xenograft efficacy studies have collectively shown that AS1411 results in cytostasis rather than cytotoxicity. After treatment with AS1411 cells are blocked at S-phase. Because of this observation, there has been interest in combining AS1411 with nucleoside analogs such as gemcitabine, which act on cells during S-phase. Early in vitro and in vivo studies of AS1411 in combination with gemcitabine against PANC-1 pancreatic cancer cells have shown enhanced antitumor activity in comparison to either agent alone (Ireson and Kelland 2006).

Preclinical toxicology of AS1411 has been evaluated in rats and dogs with IV bolus dosages of up to 100 mg/kg in rats and 96-hour continuous IV infusions at doses up to 10 mg/kg/d . No significant toxicity was observed in either species, as determined by clinical observations, clinical pathology evaluation, and gross examination of tissues at necroscopy (Ireson and Kelland 2006).

AS1411 was the first nucleic acid-based aptamer approved for Phase I clinical testing for the treatment of cancer in humans. Results have been published on the progress of 17 patients with advanced solid tumors receiving AS1411 at the Brown Cancer Center in Louisville, KY (Laber et al 2005). This report describes a continuous IV infusion dose escalation study starting from 1 mg/kg/d and thus far reported up to 10 mg/kg/d. Fifteen patients received a 4 day infusion while 2 patients received a 7 day infusion. No serious toxicity related to AS1411 administration was observed. A patient with renal cancer achieved a sustained partial response at 16 months post-treatment and 41% of patients were reported to have stable disease at 2 months post-treatment. From these initial results the Phase I study has continued with a focus on renal and non–small cell lung cancers (Ireson and Kelland 2006; Laber et al 2006).

The extensive preclinical and burgeoning clinical data amassed about AS1411 makes it an ideal candidate for targeting of cancer gene therapy in humans.

Human epidermal growth factor receptor 3 (HER-3)

Human epidermal growth factor receptor 3 (HER-3) is a receptor tyrosine kinase that is overexpressed on the surface of many different cancer cells (Yokota et al 1988; Schneider et al 1989; Slamon et al 1989; Berchuck et al 1990; Dougall et al 1993). The extra-cellular domains of receptor tyrosine kinases are rational and accessible targets for anticancer therapies. The most prominent example of a therapy targeted to the extra-cellular domain of a receptor tyrosine kinase is Herceptin, a humanized monoclonal antibody that targets the extra-cellular domain of HER-2. This molecule has proved effective in the treatment of HER2-overexpressing breast cancers (Pegram et al 1999).

An aptamer to the extracellualar domain of HER-3, called A30, has been isolated using SELEX. A30 was demonstrated to have high binding specificity to HER-3, despite the sequence similarities shared by the extracellular domains of HER-2 and HER-3. In vitro, A30 inhibits the growth stimulatory effects of HER-3's natural ligand, heregulin, though it does not compete for its binding site. A30 also inhibits HER-3 from binding to HER-2 which is a necessary step in HER-mediated growth induction (Chen et al 2003).

Though A30 is still in the early stages of development and would likely need to undergo modifications to enhance its serum stability prior to its introduction in the clinical setting, it represents a possible future targeting moiety for shRNA delivery in the therapy of cancer.

RET

Another receptor tyrosine kinase for which an aptamer has been developed is the RET oncoprotein. Mutated forms of the RET Receptor tyrosine kinase are implicated as the cause of the dominant inherited cancer syndrome MEN2 (Hansford and Mulligan 2000). In MEN2, germline to 'missense mutations of the RET gene result in the conversion of cysteine 634 to tyrosine (RETC634Y), which causes cancers of the neuroendocrine organs. These mutations affect the cysteine rich extracellular domain of RET causing the loss of an intramolecular disulfide bond. The loss of this bond allows the formation dimmers of mutated RET monomers via an intermolecular disulfide bond. Dimerization results in a constitutively activated receptor (Iwashita et al 1999).

Using 16 cycles of whole-cell SELEX several RNA aptamers that bind to the extracellular domain of RETC634Y have been isolated. PC12 cells which expressed the mutant receptor were used for the selection procedure. The aptamer with the best signaling inhibition and the most nuclease resistance, termed D4, was selected for further development (Cerchia et al 2005).

An aptamer that binds specifically to RET could be useful for targeting of specific anticancer gene therapies and it also is another example of the use of whole-cell SELEX to effectively develop aptamers that bind to transmembrane proteins in their natural glycosylation states. This method could be employed to develop aptamers to other potential targets.

Tenascin-C (TN-C)

Tenascin-C is a hexameric extracellular matrix protein that is highly expressed during active tissue development processes including wound healing, angiogenesis, embryonic development, and tumor growth (Mackie et al 1988; Erickson and Bourdon 1989; Koukoulis et al 1991; Zagzag et al 1995). TN-C is an ideal candidate for targeting of anticancer shRNA therapy because it is highly expressed in tumor and in general its expression is expression is limited in normal tissues (Borsi et al 1992). High TN-C expression has been noted in osteosarcomas, lymphomas, glioblastomas, melanomas as well as carcinomas of breast, colon lung, and prostate (Chiquet-Ehrismann 2004; Orend 2005; Orend and Chiquet-Ehrismann 2006).

Using SELEX with TN-C expressing U251 glioblastoma cells RNA aptamers that bind to the extracellular fibrinogenlike domain of TN-C with high affinity were isolated. Several modifications were made to the aptamer in order to increase its usefulness as a targeting moiety. Its size was reduced in order to increase tissue penetration and efficiency of synthesis. It was $2'$ -OCH₃ substituted, and $3'$ capped in order to increase nuclease stability. A 5′ amine was also added to

serve as a conjugation site. After these modifications the resultant aptamer, termed TTA1, had an increased equilibrium Kd but the final value of 5×10^{-9} M still represents a very high affinity (Hicke et al 2001).

In a later experiment the potential of TTA1 to be used for *in vivo* drug delivery was evaluated. Uptake and tumor distribution of rhodamine red-X-labeled TTA1 was studied using fluorescence microscopy in a U251 human glioblastoma cell line xenograft nude mouse model. Within 10 minutes after IV injection of the fluorescently labeled aptamer, bright perivascular fluorescence was noted in the xenografts. The fluorescence then diffused throughout the tumor stroma over the following 3 hours (Hicke et al 2006).

Biodistribution and radioimaging studies were performed using (99m)Tc labeled TTA1 and glioblastoma (U251) and breast cancer (MDA-MB-435) tumor xenografts in nude mice. IV administered (99m)Tc labeled TTA1 showed rapid blood clearance with a serum half-life of less than 2 min, and rapid tumor penetration. TTA1 was cleared much more rapidly from the blood than from the tumor. Both renal and hepatobiliary clearance pathways were observed, but it is estimated that due to rapid nuclease degredation of the aptamer the clearance patterns observed were those of the aptamer metabolites. In these studies it was found that TTA1 affectively targeted a wide variety of TN-C expressing tumor types including colon (SW620), breast (MDA-MB-468, MDA-MB-435), glioblastoma (U251), rhabdomyosarcoma (A673). As a control TTA1 was also tested with a squamous cell carcinoma of the head and neck (KB) xenograft that did not express TN-C. As expected, KB xenografts did not display appreciable aptamer uptake (Hicke et al 2006).

The results of these studies are promising in terms of TTA1s potential use in tumor targeting. Before its use in targeting of shRNA-based cancer therapies it would probably need further modifications to increase its serum half life. While short half lives and rapid elimination are beneficial for minimizing potential toxicity, such a short serum half life may inhibit aptamer penetration in areas of the target tumor that are poorly perfused (Hicke et al 2006).

MUC1

MUC1 is a large, highly glycosylated transmembrane epithelial cell surface protein. Mucin proteins are expressed on the apical membrane of various epithelial cell types. They have many roles which facilitate the function of mucosal cells such as lubrication of epithelial cell surfaces, prevention of tissue dehydration, protection of cells from proteolytic degradation and provision of a barrier against infection (von Mensdorff-Pouilly et al 2000). Mucins also function as signal transduction receptors involved in triggering cellular responses such as proliferation, differentiation, and apoptosis (Taylor-Papadimitriou et al 1999; Hollingsworth and Swanson 2004). MUC1 overexpression has been well documented in many human adenocarcinomas including breast, pancreatic, ovarian, colorectal, lung, prostate, esophageal (Maeshima et al 1997; Aoki et al 1998; Zhang et al 1998; Hough et al 2000; Ginestier et al 2002; Kohlgraf et al 2003; Burjonrappa et al 2007). Its expression has also been documented in other types of tumors including astrocytoma, melanoma, neuroblastoma, as well as hematological malignancies (Oosterkamp et al 1997; Brossart et al 2001).

The cell surface expression pattern of MUC1 across human malignancies makes it an excellent and versatile target for cancer targeting with an aptamer. Using 10 rounds of in vitro SELEX, a group of DNA aptamers has been isolated that binds selectively to synthetic MUC1 peptides. This pool of aptamers, when fluorescently labeled has been verified to bind specifically to MUC1 expressing cancer cell lines in vitro (Ferreira et al 2006). In a later study this group of aptamers was demonstrated by radio-imaging to have good tumor penetration in a murine xenograft (Perkins and Missailidis 2007). These aptamers are in the early stages of development and before their transition into the clinic they would need further modification to minimize size and maximize nuclease resistance.

Conclusions

Aptamer development could ameliorate many of the traditional problems with the introduction of exogenous genetic material for therapeutic purposes. There is a wide range of experimentation occurring, from the laboratory to the preclinical setting, which has the potential to revolutionize the targeting of genebased therapy. The aptamers reviewed here represent the most promising areas of current development pertinent to aptamerbased targeting of shRNA cancer therapeutics and will likely be among the first to make transition to targeting in the clinic.

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