Surface and buildup dose characteristics for 6, 10, and 18 MV photons from an Elekta Precise linear accelerator

Eric E. Klein,* Jacqueline Esthappan,[†] and Zuofeng Li[‡]

Division of Physics, Department of Radiation Oncology, Washington University School of Medicine, Campus Box 8224, 660 S. Euclid Ave., St. Louis, Missouri 63110-1093

(Received 31 July 2002; accepted for publication 20 September 2002)

Understanding head scatter characteristics of photon beams is vital to properly commission treatment planning (TP) algorithms. Simultaneously, having definitive surface and buildup region dosimetry is important to optimize bolus. The Elekta Precise linacs have unique beam flattening filter configurations for each photon beam (6, 10, and 18 MV) in terms of material and location. We performed a comprehensive set of surface and buildup dose measurements with a thin window parallel-plate (PP) chamber to examine effects of field size (FS), source-to-skin distance (SSD), and attenuating media. Relative ionization data were converted to fractional depth dose (FDD) after correcting for bias effects and using the Gerbi method to account for chamber characteristics. Data were compared with a similar vintage Varian linac. At short SSDs the surface and buildup dose characteristics were similar to published data for Varian and Elekta accelerators. The FDD at surface (FDD₀) for 6, 10, and 18 MV photons was 0.171, 0.159, and 0.199, respectively, for a 15×15 cm², 100 cm SSD field. A blocking tray increased FDD₀ to 0.200, 0.200, and 0.256, while the universal wedge decreased FDD₀ to 0.107, 0.124, and 0.176. FDD₀ increased linearly with FS ($\sim 1.16\%$ /cm). FDD₀ decreased exponentially for 10 and 18 MV with increasing SSD. However, the 6 MV FDD₀ actually increased slightly with increasing SSD. This is likely due to the unique distal flattening filter for 6 MV. The measured buildup curves have been used to optimize TP calculations and guide bolus decisions. Overall the FDD₀ and buildup doses were very similar to published data. Of interest were the relatively low 10 MV surface doses, and the 6 MV FDD₀'s dependence on SSD. © 2003 American College of Medical Physics. [DOI: 10.1120/1.1520113]

PACS number(s): 87.53.-j, 87.66.-a

Key words: buildup region, surface dose, Elekta, radiotherapy

INTRODUCTION

Understanding head scatter characteristics of photon beams is important to properly commission and test treatment planning (TP) algorithms. Most modern commercial TP systems (TPS) either use model-based or analytical methods to calculate dose distributions in the buildup region. In either case it is vital to measure buildup curves accurately in order to evaluate the accuracy of TPS calculations. Simultaneously, having definitive dosimetry at the surface and buildup region is important to optimize bolus thickness required to enhance surface dose, in clinical cases such as inflammatory breast disease. Finally, it is imperative to describe the effect of scattering (wedge, collimating jaws, etc.) and immobilization (polyurethane foam, treatment tables, etc.) media on surface dose.

Comprehensive data sets in the buildup and build-down (exit) regions have been published for vintage Varian¹⁻⁴ and Siemens⁵ linacs, and for modern day Varian⁶⁻⁹ or Elekta¹⁰ linacs. In these publications, it is evident that subtle differences in the unique beam delivery systems can affect dose to the buildup region. These include the beam monitor chamber and flattening filter construc-



FIG. 1. Photon delivery system for Elekta Precise linacs. (a) 6 MV system that is unique by virtue of the x-low flattening filter relatively distal from the primary filter. (b) Expanded view of the 18 MV system unique by virtue of the relatively proximal steel difference filter.

tion. In addition, support devices such as treatment tables or polyurethene immobilization platforms can also influence surface dose.^{2,8,9,11,12} The Elekta Precise linear accelerators (Elekta, Norcross, GA) have unique beam flattening filter configurations for each photon beam (6, 10, and 18 MV) in terms of material and location. The filter configurations for the 6 and 18 MV photon beams are shown in Fig. 1.

We performed a comprehensive set of surface and buildup dose measurements on the Precise linacs with a thin window parallel-plate chamber to examine effects of field size (FS), source-to-skin distance (SSD), and attenuating media.

METHODS AND MATERIALS

The Elekta Precise linacs in our clinic deliver 6, 10, and 18 MV photons with PDD₁₀ of 68.3%, 73.1%, and 79.5%, respectively. Measurements were performed with a parallel plate (PP) ionization chamber (PS-033, Capintec, Ramsey, NJ) possessing an entry window thickness of 0.5 mg/cm^2 , a plate separation of 2 mm, and a collecting diameter of 16.2 mm. For each measurement point, the relative ionization was acquired by dividing the charge collected at depth, via a modified Keithley electrometer (Modified K602, CNMC Co., Nashville, TN), by the charge at the depth of d_{max} and then corrected to PDD by correcting for bias effects and using the Gerbi method to account for chamber characteristics.¹³ This was accomplished in the following method: *Bias Correction*: All ionization readings were corrected by first accounting for bias effects where,

(i)

$$\frac{M^+ + M^-}{2} = M, \tag{1}$$

where M^+ and M^- are the collected positive and negative charges, respectively. The uncorrected percent depth ionization (PDI) is calculated from the uncorrected bias averaged ionization readings.

(ii)

$$PDI = \frac{M(d)}{M(d_{\text{max}})}.$$
(2)

The PDI was then corrected to PDD by accounting for chamber (Capintec Parallel-Plate) characteristics according to the Gerbi method.

3 Klein, Esthappan, and Li: Surface and buildup dose characteristics ...

(iii)

$$PDD = PDI - \xi(0, E) l e^{-\alpha (d/d_{\max})}, \tag{3}$$

where

 $\xi(0,E) =$ energy dependent chamber corrections,

$$\xi(0,E) = [-1.666 + (1.982 \text{IR})] \times [C - 15.8),$$

where

IR= ionization ratio (6 MV=0.675, 10 MV=0.728, 18 MV=0.783) C= sidewall-collector distance (mm)=6 α = constant of 5.5.

Buildup region data were measured for field sizes ranging from 5 to 40 cm, SSDs ranging from 80 to 140 cm, and for depths from surface to just beyond d_{max} . Field sizes were defined by the collimator setting (100 cm SSD). In addition, surface doses were measured with the Elekta *Universal* wedge and a 9 mm lexan block tray in place. Data were compared with a similar vintage Varian linac.

RESULTS

A. Surface dose characteristics

At short SSDs (≤ 100 cm) the surface and buildup dose characteristics were similar to previously published data. The data are reported in fractional depth dose data (PDD/100), as this was the reporting method in prior publications. The fractional depth dose (FDD) at surface (FDD₀) for open 6, 10, and 18 MV photon beams was 0.171, 0.159, and 0.199, respectively, for a 15×15 cm², 100 cm SSD field. The blocking tray increased FDD₀ to 0.200, 0.200, and 0.256, while the universal wedge decreased FDD₀ to 0.107, 0.124, and 0.176 for the 6, 10, and 18 MV photons, respectively. Table I summarizes this data along with a comparison to Varian data. The wedge data in each case were measured without the respective block trays in place. The Elekta wedge is the *Universal* wedge with its proximal surface located at 18.6 cm from the source; and the Elekta block tray is a 9 mm lexan tray, located at 64.7 cm from the source. The Varian wedge is a 45° lead wedge (located at 49.2 cm from the source); and the Varian block tray is a 6 mm lexan tray, located at 61.6 cm from the source.

B. Dependence on field size

We found that the surface dose, reported as FDD, increased nearly linearly with FS ($\sim 1.16\%$ /cm). The graph in Fig. 2 depicts this trend.

C. Dependence on SSD

The FDD₀ decreased exponentially for 10 and 18 MV with increasing SSD. However, the 6 MV FDD₀ actually increased slightly with increasing SSD. This is likely due to the unique distal "x-ray" flattening filter for 6 MV. The graph in Fig. 3 summarizes these results.

TABLE I. Elekta precise fractional surface dose: 15×15 cm² field size, 100 cm SSD. Values in parentheses are for a Varian 2100C accelerator.

Absorber/Energy	6 MV	10 MV	18 MV
Open	0.171 (.205)	0.159	0.199 (0.215)
Block Tray	0.200 (.226)	0.200	0.256 (0.223)
Universal Wedge (Varian 45° wedge)	0.107 (.179)	0.124	0.176 (0.136)



FIG. 2. Fractional surface dose as a function of energy and field size at a constant SSD of 100 cm, without a block tray in place.



FIG. 3. Fractional surface dose as a function of energy and SSD with a constant collimating field size of 15×15 cm, and without a block tray in place.

D. Buildup data

Figures 4 graphically represent the buildup curves for each of the photon energies. The buildup curves are normalized to the respective d_{max} FDD values.

The 15×15 cm² data for each energy were extracted for comparison. Once again data are normalized to each respective d_{max} value. The results are displayed in Fig. 5.

DISCUSSION AND CONCLUSIONS

The measured buildup curves have been used to validate TP calculations and guide bolus decisions. Overall the FDD at surface (FDD_0) and buildup doses were very similar to published data. One point of interest is the relatively low 10 MV surface doses. This is most likely due to the two-tier flattening filter system employed for the 10 MV beam. Also of special interest was the 6



FIG. 4. (a) Fractional depth dose as a function of depth and field size at a constant for 6 MV photons, without a block tray in place. (b) Fractional depth dose as a function of depth and field size at a constant for 10 MV photons, without a block tray in place. (c) Fractional depth dose as a function of depth and field size at a constant for 18 MV photons, without a block tray in place.



FIG. 5. Fractional depth dose as a function of depth and energy for a 15×15 cm field size, without a block tray in place.

MV dependence of FDD_0 on SSD. The constant FDD_0 , independent of SSD, is likely a reflection of the distal location of the 6 MV flattening filter, placing the source of scattered electrons and photons further from the target and thereby creating a smaller solid angle of head scatter. In terms of dependence on attenuation devices, it is of interest that the influence of the block tray on surface was minimal for 6 MV beams compared with prior reports, with only a minimal increase (3% absolute increase), but was consistent compared with prior reports for 18 MV photons (6% absolute increase). This is due to the relatively thick (9 mm) lexan tray compared with other machines' 6 mm trays. This thick tray absorbs a greater percentage of low energy scattered electrons and photons for 6 MV photons compared to the 18 MV beam. This same scenario is even more evident for the steel universal wedge whereby the wedge acts as both an generator and absorber of head scatter. The result is a greater absorption for 6 MV compared with 18 MV photons. In general, the Precise linac delivers lower surface dose for 6 and 18 MV photons compared with a similar vintage Varian machine, with the exception of attenuated 18 MV photons.

- *Email address: klein@radonc.wustl.edu
- [†]Email address: esthappan@radonc.wustl.edu
- [‡]Email address: zuofeng@radonc.wustl.edu
- ¹C. W. Coffey, J. L. Beach, D. J. Thompson, and M. Mendiondo, "X-ray beam characteristics of the Varian Clinac-6/100 linear accelerator," Med. Phys. **7**, 716–722 (1980).
- ²G. Krithivas and S. H. Rao, "A study of the characteristics of radiation contaminants within a clinically useful photon beam," Med. Phys. **12**, 764–768 (1985).
- ³J. A. Purdy, "Buildup/surface dose and exit dose measurements for a 6-MV linear accelerator," Med. Phys. **13**, 259–262 (1986).
- ⁴D. E. Velkey, D. J. Manson, J. A. Purdy, and G. D. Oliver, "Build-up region of megavoltage photon radiation sources," Med. Phys. **2**, 14–19 (1975).
- ⁵J. L. Horton, "Dosimetry of the Siemens Mevatron 67 linear accelerator," Int. J. Radiat. Oncol., Biol., Phys. 9, 1217–1233 (1983).
- ⁶M. J. Butson, T. Cheung, P. K. Yu, and B. Webb, "Variations in skin dose associated with linac bed materials at 6 MV x-ray energy," Phys. Med. Biol. **47**, N25–30 (2002).
- ⁷J. Carl and A. Vestergaard, "Skin damage probabilities using fixation materials in high-energy photon beams," Radiother. Oncol. **55**, 191–198 (2000).
- ⁸E. E. Klein and J. A. Purdy, "Entrance and exit depth doses for the Clinac 2100C," Int. J. Radiat. Oncol., Biol., Phys. **27**, 429–435 (1993).
- ⁹A. Lamb and S. Blake, "Investigation and modeling of the surface dose from linear accelerator produced 6 and 10 MV photon beams," Phys. Med. Biol. **43**, 1133–1146 (1998).
- ¹⁰A. R. Hounsell and J. M. Wilkinson, "Electron contamination and build-up doses in conformal radiotherapy fields," Phys. Med. Biol. 44, 43–55 (1999).

7 Klein, Esthappan, and Li: Surface and buildup dose characteristics ...

- ¹¹D. E. Mellenberg, "Dose behind various immobilization and beam-modifying devices," Int. J. Radiat. Oncol., Biol., Phys. **32**, 1193 (1995).
- ¹²D. P. Fontenla, J. J. Napoli, M. Hunt, D. Fass, B. McCormick, and G. J. Kutcher, "Effects of beam modifiers and immobilization devices on the dose in the build-up region," Int. J. Radiat. Oncol., Biol., Phys. **30**, 211–119 (1994).
- ¹³B. J. Gerbi and F. M. Khan, "Measurement of dose in the buildup region using fixed-separation plane-parallel ionization chambers," Med. Phys. 17, 17–26 (1990).