

Article

Blockade of Human $\alpha 7$ Nicotinic Acetylcholine Receptor by α -Conotoxin ImI Dendrimer: Insight from Computational Simulations

Xiaoxiao Xu ^{1,2}, Jiazhen Liang ^{1,2}, Zheyu Zhang ¹, Tao Jiang ^{1,2} and Rilei Yu ^{1,2,3,*} 

¹ Key Laboratory of Marine Drugs, Chinese Ministry of Education, School of Medicine and Pharmacy, Ocean University of China, Qingdao 266003, China; 21170831073@stu.ouc.edu.cn (X.X.); 11180822010@stu.ouc.edu.cn (J.L.); zzy8617@stu.ouc.edu.cn (Z.Z.); jiangtao@ouc.edu.cn (T.J.)

² Laboratory for Marine Drugs and Bioproducts of Qingdao National Laboratory for Marine Science and Technology, Qingdao 266003, China

³ Innovation Center for Marine Drug Screening & Evaluation, Qingdao National Laboratory for Marine Science and Technology, Qingdao 266003, China

* Correspondence: rlyu@ouc.edu.cn

Received: 23 April 2019; Accepted: 17 May 2019; Published: 23 May 2019



Abstract: Nicotinic acetylcholine receptors (nAChRs) are ligand-gated ion channels that are involved in fast synaptic transmission and mediated physiological activities in the nervous system. α -Conotoxin ImI exhibits subtype-specific blockade towards homomeric $\alpha 7$ and $\alpha 9$ receptors. In this study, we established a method to build a 2 \times ImI-dendrimer/h (human) $\alpha 7$ nAChR model, and based on this model, we systematically investigated the molecular interactions between the 2 \times ImI-dendrimer and h $\alpha 7$ nAChR. Our results suggest that the 2 \times ImI-dendrimer possessed much stronger potency towards h $\alpha 7$ nAChR than the α -ImI monomer and demonstrated that the linker between α -ImI contributed to the potency of the 2 \times ImI-dendrimer by forming a stable hydrogen-bond network with h $\alpha 7$ nAChR. Overall, this study provides novel insights into the binding mechanism of α -ImI dendrimer to h $\alpha 7$ nAChR, and the methodology reported here opens an avenue for the design of more selective dendrimers with potential usage as drug/gene carriers, macromolecular drugs, and molecular probes.

Keywords: 2 \times ImI-dendrimer; h $\alpha 7$ nAChR; linker; binding affinity; molecular dynamics simulation; MMGB/SA

1. Introduction

Nicotinic acetylcholine receptors (nAChRs) are cation-selective pentameric ligand-gated ion channels that belong to the Cys-loop receptor family, which also includes γ -aminobutyric acid type A (GABAA), glycine, and serotonin (5-HT₃) receptors [1,2]. It consists of three parts, an extracellular domain, a transmembrane domain, and an intracellular domain (Figure 1A). Up to now, more than 10 different neuronal nAChR subtypes have been discovered, including $\alpha 7$, $\alpha 9\alpha 10$, $\alpha 3\beta 2$, and $\alpha 4\beta 2$ [3]. Each subtype is closely related to a series of pathophysiological functions, such as Parkinson's disease, Alzheimer's disease, epilepsy, and so on [4–6]. For instance, disorders of $\alpha 7$ nAChR can cause schizophrenia and Alzheimer's disease [7]. Therefore, nAChR inhibitors with high potency and low toxicity can be potentially developed into drugs for the treatment of these major diseases [8,9].

Conotoxins derived from the venom of *Conus* snails are pharmacologically valuable peptides with potency at various ion channels [10–13]. Most of the reported conotoxins targeting nAChRs are α -conotoxins, which belong to the most widely studied conotoxin class [12]. α -Conotoxin ImI (α -ImI) features a short α -helix and two disulfide bonds that link cysteines I–III and II–IV (Figure 1B). It comprises 12 residues and is C-terminal amidated (indicated by * in the sequence) (Figure 1C).

α -ImI binds specifically to the human (h) $\alpha 7$ and $\alpha 3\beta 2$ nAChR with IC_{50} of 595 nM and 40.8 nM, respectively [13,14]. Currently, α -conotoxins are receiving increased attention from researchers due to their potential medicinal value or potential use as molecular probes for neuropharmacology study.

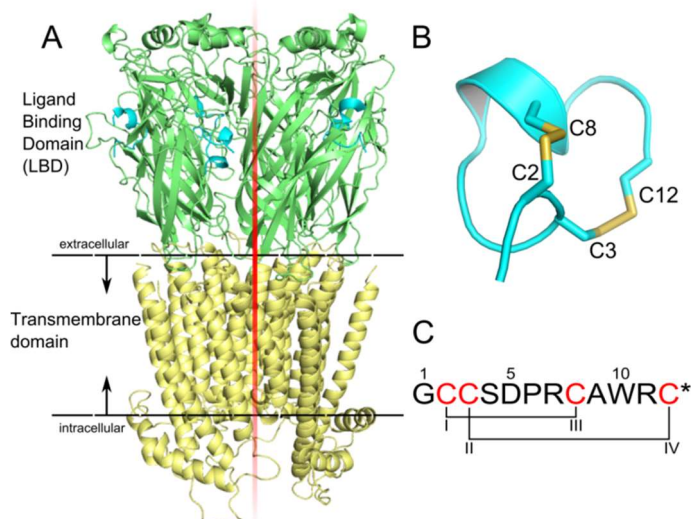


Figure 1. Structures of a nicotinic acetylcholine receptor (nAChR) and α -ImI. (A) $h\alpha 7$ nAChR bound with α -ImI. nAChRs are ligand-gated ion channels. The structure of nAChR consists of a ligand binding domain (green), a transmembrane domain (yellow), and an intracellular domain (purple). Five α -ImI (light blue) bound to the acetylcholine binding sites. The α -ImI/ $h\alpha 7$ -nAChR complex structure was built using the crystal structure of $\alpha 1$ subunit (Protein data bank (PDB) code: 2q1) and AChBP/ImI (PDB code: 2c9t) as templates. (B,C) α -ImI comprises 12 residues and is C-terminal amidated (indicated by *). The structure features a short α -helix and two disulfide bonds that link cysteines I–III and II–IV. The cysteines are highlighted in red.

Dendrimers with polyvalent structures, first developed in the 1980s [15,16], have been widely regarded as useful carriers for small molecular drugs and gene delivery [17,18]. By integrating the merits of dendrimers with bioactive peptides, peptide-decorated dendrimers (PDDs) have been extensively fabricated to generate vaccines [19–24], antiviral agents [25,26], and antitumor therapeutics [27–32] due to their multivalency effects. In particular, dendrimeric peptides have shown interesting properties for enhancing overall binding affinity and specificity compared with monovalent ligands. For instance, the α -ImI dimer showed substantially enhanced potency at $h\alpha 7$ nAChR [33], and in 3–5% *w/w* SPL7013 gels, a dendrimer with a polyanionic outer surface was effective in blocking vaginal transmission of simian/HIV-1 virus (SHIV) in macaques [34]. Despite its promising applications, rational design of dendrimeric peptides to achieve optimal bioactivity has proven to be challenging [35,36]. Hence, it is a prerequisite to establish a computational method for the design of dendrimeric peptides *in silico* prior to chemical synthesis in the laboratory. For this purpose, we used a computational modeling method to build models of α -ImI dendrimer bound with $h\alpha 7$ nAChR and calculated its binding energy. The simulation results shed light on the interaction mechanism between α -ImI dendrimer and $h\alpha 7$ nAChR.

2. Results and Discussion

2.1. Comparing the Binding Mode of α -ImI Monomer and α -ImI Dimer at $h\alpha 7$ nAChR

The α -ImI monomer and α -ImI dimer possessed similar binding modes at $h\alpha 7$ nAChR (Figure 2A,B and Figure S1). The critical residues conferring α -ImI specificity for $h\alpha 7$ nAChR were clustered at one site of α -ImI, which is consistent with a previous NMR structural study of α -ImI [37]. Comparing the conformations of α -ImI before and after molecular dynamics (MD) simulations, it was found that the

conformations of D5, R7, and W10 were well maintained, while R11 demonstrated a slight orientation change (Figure 2A,B). Results from a previous mutagenesis study and computational modeling suggested that D5, R7, and W10 in α -ImI contribute most to the binding affinity of α -ImI [38,39], which is in line with the results from our modeling of α -ImI/ $h\alpha 7$ -nAChR monomers and 2 \times ImI-dendrimer/ $h\alpha 7$ -nAChR in the current study (Figure 2A,B). The overall results suggest that conformations for these critical residues in each α -ImI of the dimer were maintained after MD simulations, and the linker had minor effects on α -ImI binding to the $h\alpha 7$ nAChR.

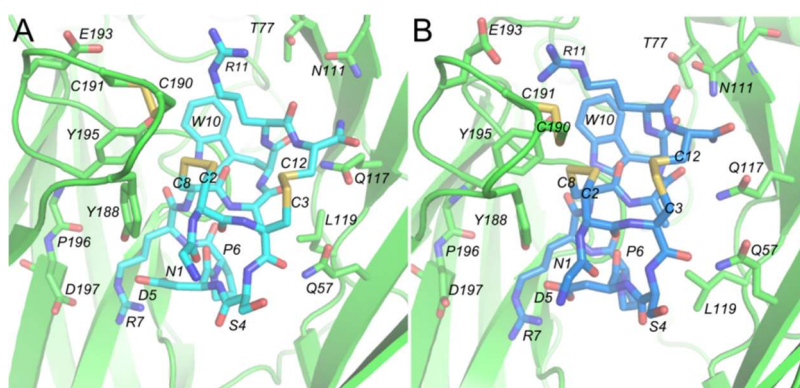


Figure 2. Binding mode of the α -ImI monomer and dimer. (A) the binding mode of the α -ImI monomer (light blue). (B) the binding mode of α -ImI of the 2 \times ImI-dendrimer in the same pocket as (A) (blue). The $h\alpha 7$ nAChR is shown in cartoon, while α -ImI and the residues of the binding site are shown in stick form.

2.2. Effects of the Linker to the Binding of 2 \times ImI-Dendrimer with $h\alpha 7$ nAChR

2.2.1. Conformation of α -ImI in the 2 \times ImI-Dendrimer

Conformation of α -ImI was not impacted by the linker in the dimer. Comparison between the root mean square deviation (RMSD) for α -ImI as a monomer and a dimer showed that the conformation of α -ImI maintained stable over the MD simulations (Figure 3A). Indeed, polyethylene glycol (PEG), as the main component of the linker, provided a spacer segment to vary flexibility, length, and accessibility of α -ImI [33].

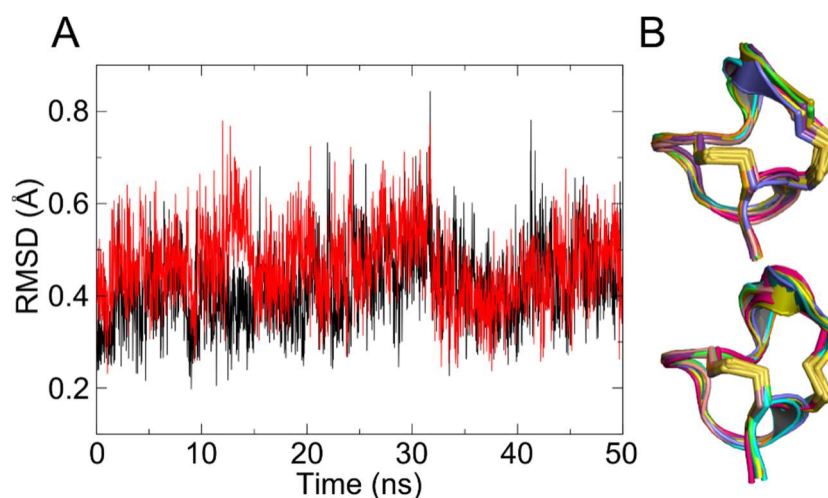


Figure 3. The conformation of the two α -ImI in the dimer. (A) Evolution of the root mean square deviation (RMSD) for each α -ImI in the dimer in the 50 ns molecular dynamics (MD) simulations. (B) Superposition diagram of the averaged extracted 8 frames (in varied colors) from the last 10 ns and the α -ImI initial frame (in blue).

The secondary structure of each α -ImI in the 2 \times ImI-dendrimer was maintained. Comparing the secondary structure of each α -ImI in the 2 \times ImI-dendrimer in the last 20 ns of the MD simulation and the two α -ImI monomers, we found that the linker had no significant effect on the secondary structure of α -ImI, especially in the last 10 ns (Figure S2A,B). Alignment of the 8 frames extracted from the last 10 ns MD with even time intervals with the α -ImI initial frame revealed that the secondary structure of each α -ImI in the 2 \times ImI-dendrimer was not significantly changed (Figure 3B). Together, the linker was flexible, and it did not impact the conformation of α -ImI in the dendrimeric form. Each α -ImI in the dimer was structurally intact and free to interact with $\text{h}\alpha 7$ nAChR independently.

2.2.2. The Opening of the C-Loop

A peripheral loop in nAChR (Figure 4A), called the C-loop, behaves as a ligand-triggering lid, effectively closing and opening the ligand-binding pocket [40]. Given that the measurement of the C-loop opening is an indicator for the characterization of the effect of the ligands acting on nAChRs [41,42], such measurements have been made to characterize the conformational change of the binding site of the 2 \times ImI-dendrimer. The results show that the opening of the C-loop in each binding pocket was maintained at about 19Å throughout the whole MD simulation, which was comparable to the values from our previous study [39] (Figure 4B), indicating that the linker between the two α -ImI of the 2 \times ImI-dendrimer neither entered the binding pocket nor participated in the interaction with the residues at the binding site.

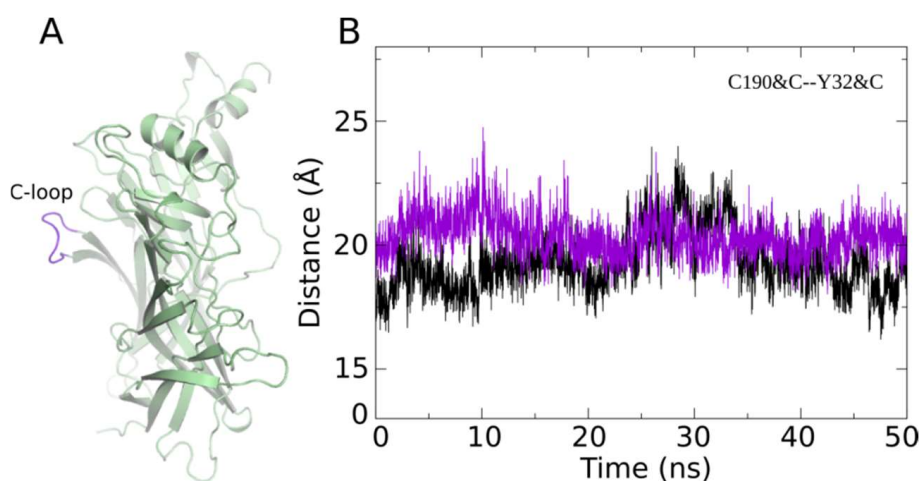


Figure 4. The opening of the C-loop in two adjacent binding sites. (A) Side view of the $\text{h}\alpha 7$ nAChR subunit. A peripheral loop highlighted in purple represents the C-loop. (B) C-loop opening measurement in the MD simulation. It was measured by calculating the distance between the CA atom of C190 and the CA atom of Y32 in $\text{h}\alpha 7$ nAChR over time. Purple and black represent the distance variation of two different binding sites, respectively.

2.2.3. Interacting with $\text{h}\alpha 7$ nAChR

In the design of the 2 \times ImI-dendrimer, the PEG linker not only links the two α -ImI, but also enhances the dendrimer solubility. From the above analysis, we confirmed that the linker was free from the binding site, neither affecting the interaction of α -ImI to the receptor nor interacting with the residues of the binding sites. We were interested in the conformational states of the linker in the MD simulation. Here, we extracted 25 conformations from 1 to 50 ns and 10 conformations in the first 1 ns with even time intervals to observe the conformational change of the linker. Through cluster analysis, we found that the dynamics of the linker evolved from the non-equilibrated and fluctuated state (Figure S3A,B) to the equilibrated and relevantly stable state (Figure 5A). At the beginning of the MD simulation, the linker showed substantial fluctuation from 0 to 14 ns, whereas its flexibility gradually

decreased from 14 to 34 ns. Afterward, the linker showed a certain degree of stability (Figure 5A, orange and blue rectangle). The improved stability for the linker originated from its interactions with the region of the receptor between the two adjacent subunits.

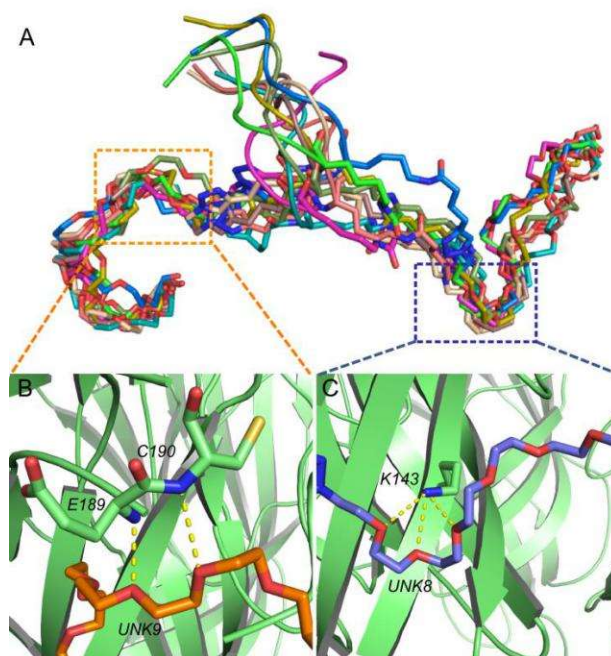


Figure 5. Conformation and binding modes of the linker. (A) The average extraction frames from 34th ns to 50th ns. Linker was divided into two parts, named UNK8 and UNK9 (Figure 7). (B) Binding mode of the left half of linker (UNK9) at hα7-nAChR; (C) Binding mode of the right half of linker (UNK8) at hα7-nAChR. hα7 nAChR is shown in green, and the two parts of the linkers are colored in orange (UNK9) and purple (UNK8), respectively.

Being stabilized by the local residues, the left and right (Figure 5A) fragments of the linker maintained regular curving conformation in the MD simulation. To study the specific role played by the two parts of the linker, we performed cluster analysis to identify the most populated conformations and used these to identify possible interaction partners. According to the above conclusion, the linker reached equilibrium at 34–50 ns, and during this period, we extracted frames with 1 ns intervals to perform a cluster analysis and analyzed the linker conformation change to identify possible interaction partners (Figure S4). Overall, conformations and interactions formed by the right half of linker (UNK8) were significantly more stable than those of UNK9. For UNK8, the U-shape was relatively stable, especially at the last 5 ns. UNK9, however, was in a less stable state.

As shown by Figure S4, the linker was most stable in the last 5 ns, and we extracted the last frame to analyze the interactions in detail between the linker and hα7 nAChR. The two-dimensional (2D) interaction diagrams (Figure S5) that were obtained using Schrödinger (Maestro, Version 9.0) showed comprehensive interactions between the linker and the receptor. The three-dimensional (3D) interaction diagrams (Figure 5B,C) of these main interactions showed that the oxygen atoms of UNK8 formed three hydrogen bonds with the three hydrogen atoms of the nitrogen atom on the side chain of K143. Three oxygen atoms surrounded the nitrogen atoms on the side chain of K143 to present a “U” shape, forming an extremely stable hydrogen-bond network. On the other side, UNK9 formed two hydrogen bonds with E189 and C190, respectively. Distance analysis (Figure S6) indicated that these hydrogen bonds were stable in the MD simulation. Overall, our simulation results suggested that the linker was directly involved in interactions with the receptor but without interference to the interactions between α-ImI and hα7 nAChR.

2.3. Binding Energy Calculation and Decomposition

In general, the molecular mechanics–generalized Born surface area (MMGB/SA) method is able to give more accurate predictions of the ligand binding affinity than the molecular mechanics–Poisson–Boltzmann surface area (MMPB/SA) method because of the approximations introduced in the MMGB/SA method [39,43]. Indeed, the MMGB/SA performed better than MMPB/SA in several studies [44–46]. Here, the MMGB/SA was used to explain why the 2×ImI-dendrimer could significantly enhance the binding free energy in comparison with the native α -ImI monomer.

At the thermodynamic level, the binding affinity was determined by the magnitude of the Gibbs free energy (ΔG). Our calculation results indicate that the binding affinity of the 2×ImI-dendrimer is stronger than that of the α -ImI monomer (Table 1), which is consistent with the experimental results [33]. Each α -ImI of the 2×ImI-dendrimer can be accessible at the $h\alpha 7$ nAChR binding site and collectively cause a multivalency effect. Unlike the monomers, the multivalent α -ImI density at the surface increases, which can strengthen ligand receptor binding probability and improve the targeting of attached components [47].

Table 1. Energy contribution of the α -ImI monomer and dimer.

Ligands	ΔG (Kcal/mol)	ΔH (Kcal/mol)	$T\Delta S$ (Kcal/mol)
α -ImI	−30.68	−73.70	−43.02
2×ImI-dendrimer	−78.46	−233.85	−155.39

ΔG is a function of only two terms, the enthalpy (ΔH) and the entropy (ΔS). The influence of enthalpy change (ΔH) can be from dehydration of polar groups of ligands and receptors, hydrogen bond and Van der Waals interactions, etc. As the enthalpy and entropy contribute to the binding energy in an additive fashion ($\Delta G = \Delta H - T\Delta S$), it is clear that reduced enthalpy is beneficial to increase the binding free energy. The ΔH of the 2×ImI-dendrimer was approximately 3-fold lower than its monomeric counterparts (Table 1), suggesting that the interaction between the 2×ImI-dendrimer and $h\alpha 7$ nAChR is stronger than that of the monomer. According to the binding mode (Figure 5B,C), the linker in the 2×ImI-dendrimer also contributed substantially to its enthalpy. Overall, the linker and dual α -ImI jointly prompted favorable enthalpy.

Although the enthalpy of the 2×ImI-dendrimer was approximately 3-fold lower than its monomeric counterparts, the entropy loss (ΔS) of the dimer was 3-fold more than that of the monomer (Table 1). The conformational entropy change usually reflects a loss of conformational degrees of freedom between the ligands and the protein. Consequently, in terms of the loss of conformational degrees of freedom, the loss of the 2×ImI-dendrimer was much greater than that of the monomer. The reason might lie in the PEG spacer units, which is part of the linker. It was flexible prior to binding with the receptor, whereas its conformational constraint increased substantially when the linker interacted with the receptor (Figure 5B,C), therefore, making it an unfavorable term.

In a strategy to obtain the contribution of the linker to α -ImI dimer binding affinity, the binding energy contribution from UNK8 and UNK9 was calculated using MMGB/SA. The calculation results show that the linker made a beneficial contribution to the binding energy. Interestingly, the energy contribution of UNK8 was higher than that of UNK9 (Table 2), indicating that the two parts (UNK8 and UNK9) play different roles in binding with $h\alpha 7$ nAChR. These calculated results are consistent with the results given by the binding mode analysis. The cartoon diagram of the 2×ImI-dendrimer/ $h\alpha 7$ -nAChR is shown in Figure 6A. The linker had two main effects on binding energy, adverse entropy contribution, and beneficial enthalpy contribution. If the linker was too short, only one α -ImI of the 2×ImI-dendrimer' could bind to $h\alpha 7$ nAChR, and the linker could not closely interact with $h\alpha 7$ nAChR (Figure 6B). Consequently, the $\Delta H'$ and the $\Delta S'$ both decreased compared with those of the 2×ImI-dendrimer with a reasonable length of linker. Under these circumstances, the potency of the 2×ImI-dendrimer' was comparable to that of the monomer ($\Delta G' = \Delta G$). If the linker was too long, both α -ImI of

the 2×ImI-dendrimer” could simultaneously bind to hα7 nAChR, whereas the multivalency effects were significantly decreased due to the overly long linker (Figure 6C). Thus, compared with the 2×ImI-dendrimer with a reasonable length of linker, the $\Delta H''$ either decreased or did not change, whereas the $\Delta S''$ decreased. In this case, the potency of the 2×ImI-dendrimer” was comparable to that of the monomer or the 2×ImI-dendrimer ($\Delta G'' = \Delta G$).

Table 2. Energy contribution of two segments of the linker.

Ligands	$\Delta G'''$ (Kcal/mol)
UNK8	−22.32
UNK9	−13.12

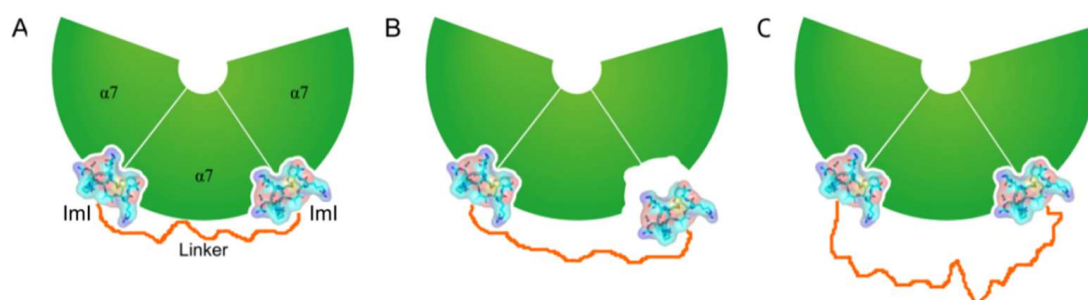


Figure 6. The 2×ImI-dendrimer/hα7-nAChR model with different lengths of linkers. hα7 nAChR, α-ImI, and the linker are labeled. (A) The 2×ImI-dendrimer model with a linker of reasonable length. Its enthalpy change, entropy change, and binding energy were expressed as ΔH , ΔS , and ΔG . (B) The 2×ImI-dendrimer model with a linker that was too short (2×ImI-dendrimer’). Its enthalpy change, entropy change, and binding energy were expressed as $\Delta H'$, $\Delta S'$, and $\Delta G'$. (C) The 2×ImI-dendrimer model with an overly long linker (2×ImI-dendrimer”). Its enthalpy change, entropy change, and binding energy were expressed as $\Delta H''$, $\Delta S''$, and $\Delta G''$.

Overall, our computational studies suggest that the 2×ImI-dendrimer interaction with hα7 nAChR is enthalpy-driven binding and an appropriate linker is necessary to obtain full activity. If the selected linker is too long or too short, one can expect an increase/decrease in the flexibility of the linker potentially affecting the bioactivity. Our findings provide guidance for the design of functional peptide dendrimers and suggest that the linker length, flexibility, and hydrophilicity (e.g., with an appropriate number of hydrogen bond acceptors or donors) should be carefully considered.

3. Conclusions

In this study, we established a computational method for the simulation of the interactions between the 2×ImI-dendrimer and hα7 nAChR and statistically analyzed the relationship between the linker, α-ImI, and hα7 nAChR. We found that the 2×ImI-dendrimer maintains its tertiary peptide structure and is free to interact with hα7 nAChR. There were several critical interactions between the linker and hα7 nAChR, which suggested that the multivalent effects are closely related to the linker length and flexibility.

In summary, such a computational method is not only useful to explain the potency of conotoxin dendrimers, but also for the rational design of other peptide dendrimers and small molecular copolymers to improve their potency and specificity. Our work will provide guidance for the design of other dendrimers used as drug/gene carriers, macromolecular drugs, and molecular probes.

4. Materials and Methods

4.1. α-ImI/hα7-nAChR Complex

In the absence of a crystal structure of hα7 nAChR, hα7 nAChR ligand binding domain (LBD) combined with α-ImI was modeled using a comparative approach [39,48–50]. In this study, the structure

of AChBP in complex with α -ImI (PDB code: 2c9t) was employed as a structural template to orient the five α 7 subunits in the pentamer. The orientations of the side chains were modeled according to the extracellular domain of the α 1 nAChR subunit (PDB code: 2qc1). The multiple sequence alignment between AChBP, α -ImI/h α 7-nAChR, and the α 1 nAChR subunit was generated using MUSCLE [51] and manually adjusted based on structural superimpositions of the AChBP and α 1 nAChR subunit. MODELLER (Version 9v14) [52] was then employed to generate 100 3D structural models of the α -ImI/h α 7-nAChR complex. The model selected according to the discrete optimized protein energy (DOPE) score [53] was analyzed using MolProbity [54], and more than 94% of residues were in the favorable region of the Ramachandran plot, which is acceptable for a comparative model [53].

4.2. 2 \times ImI-dendrimer/h α 7-nAChR Complex

Figure S5 illustrates the procedures of the methodology of building the 2 \times ImI-dendrimer/h α 7-nAChR model. In the first stage, UNK8 and UNK9 were constructed by Discovery Studio 3.5 and ChemDraw, and the peptide fraction was generated using the sequence command included in xLEaP. Afterwards, Antechamber and Amber were used to generate parameters for the UNK8/UNK9 and peptide segments, respectively. Next, all the parameters of UNK8/UNK9, UNK8/UNK9.PDB, and the α -ImI.PDB were loaded into xLEaP. The 2 \times ImI-dendrimer and 2 \times ImI-dendrimer/h α 7-nAChR (one 2 \times ImI-dendrimer with five α 7 subunits) were constructed successively in the editing window of xLEaP. Clearing both tasks, the MD simulation was carried out.

4.2.1. The Building of the 2 \times ImI-dendrimer

The structure of the linker consisted of two PEG spacer units (UNK8 and UNK9) and a peptide fragment (Lys-Gly-(Arg)₄-Gly) (Figure 7). The molecule building module of Discovery Studio 3.5 was used to generate UNK8/UNK9 at the N terminal of α -ImI in the two adjacent binding pockets of h α 7 nAChR. The locations of both ends of the linker were determined based on the two N terminals of α -ImI. The rough conformation of the linker was determined based on the concave–convex degree of the h α 7 nAChR surface between the two adjacent binding sites. Then, the linker was positioned on the surface of the receptor by carefully checking the heavy atoms distances between the linker and the receptor to avoid atom collisions.

The forcefield used by Discovery Studio 3.5 to construct the linker was CHARMM, which was incompatible with the forcefield used, AMBER. ChemDraw was used here to convert the CHARMM PDB format structures into a PDB format that was compatible and readable with Antechamber. First, ChemDraw 2D was used to construct the two-dimensional structure of UNK8, and then, ChemDraw 3D was used to generate the three-dimensional structure (named UNK8.PDB). UNK8.PDB with modified atomic names can be imported into Antechamber to generate parameters. The procedure for generating parameters for UNK9.PDB was the same as that for UNK8.PDB.

We used AMBER forcefield ff14SB for the peptide fraction, and general AMBER force field GAFF parameters for UNK8 and UNK9. Parameters for UNK8 and UNK9 (Table S1) were generated using the Antechamber module embedded in AmberTools in AMBER16 package [55]. Atom partial charges for UNK8 and UNK9 were produced using the R.E.D Tools [56].

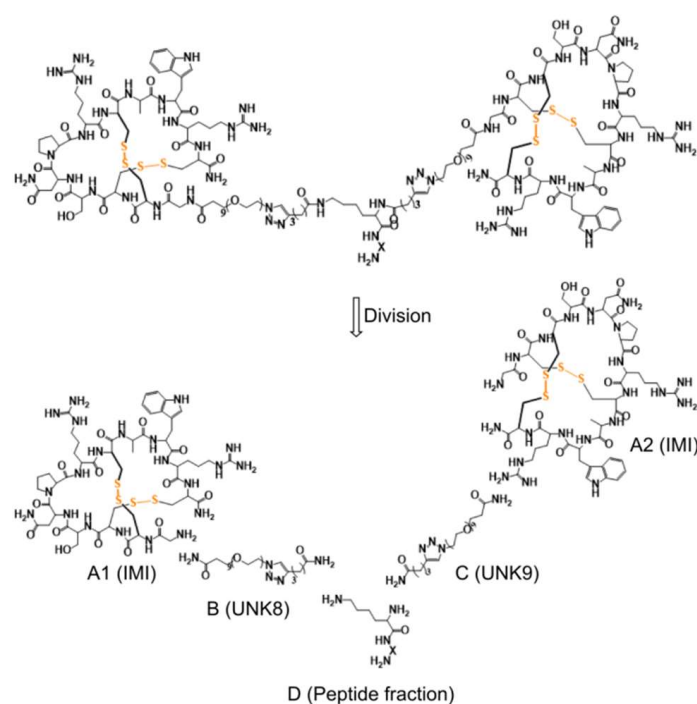


Figure 7. The structure diagram of the ligand and the linker. (A1) and (A1) represent α -ImI. (B) and (C) are the polyethylene glycol (PEG) spacer units, which were named UNK8 and UNK9 respectively. (D) represents the peptide fraction, and the “X” represents 6 amino acid residues (Gly-Arg-Arg-Arg-Arg-Gly).

4.2.2. Molecular Dynamics Simulation

The $2\times$ ImI-dendrimer/ $\alpha 7$ -nAChR complex that we simulated contained one α -ImI-dendrimer and five $\alpha 7$ subunits. The $2\times$ ImI-dendrimer/ $\alpha 7$ -nAChR model was solvated in a cubic box with 49,498 water molecules, and 13 Na⁺ were added to simulate and neutralize the system. The ff14SB forcefield [57] was applied to the protein and peptide, and the GAFF was used for the linker region. Once we built the whole system in xLeaP of AMBER16, minimization before the MD simulation was performed to remove the Van der Waals contacts between the α -ImI dendrimer and $\alpha 7$ nAChR. The first was constrained optimization, which was the steepest descent method optimization of 2000 steps and the conjugate gradient method optimization of 3000 steps, and the solute binding force was 100 kcal mol. After completing the first round of energy optimization, the binding force was removed from the solute molecules, unconstrained optimization was performed, and the entire system was optimized using the same parameters as above. The MD simulations were carried out after minimization using methods as described previously [58]. Additionally, MD simulations of two α -ImI monomers bound with five $\alpha 7$ subunits were also performed.

4.2.3. Binding Energy Calculations

MMGB/SA [59] was applied to calculate the binding affinities of the $2\times$ ImI-dendrimer and the parts of the linker (UNK8 and UNK9) against $\alpha 7$ nAChR. The energies were averaged on the 50 frames extracted from the last 10 ns of the MD simulation.

The values of the binding free energy ($\Delta G_{\text{binding}}$) for each model were calculated based on the following equation:

$$\Delta G_{\text{binding}} = G_{\text{complex}} - G_{\text{ligand}} - G_{\text{receptor}}. \quad (1)$$

The free energy can be decomposed into three components (complex, receptor, and ligand):

$$G = \langle G_{\text{solute}} \rangle + \langle G_{\text{epol}} \rangle + \langle G_{\text{SA}} \rangle, \quad (2)$$

where G_{solute} is the solute Gibbs free energy, G_{epol} represents the polar contribution to the solvation energy, and GSA represents non-polar contribution to the solvation energy. The internal dielectric and external dielectric constants were set to 2.0 and 80.0, respectively. A probe radius of 1.4 Å, a grid spacing of 0.5 Å, and ionic strength of 0.15 mol/L were set up for the calculations. Other parameters of the energy calculation were described previously in [39].

The entropy can be divided into solvation and configuration entropy. The configuration entropy is a measure of the entropy in the solute (protein–ligand complex) in solution and is the only entropy element calculated explicitly [60]. Oehme et al. calculated the entropy used the NMODE module to explain the effect of entropy on binding free energies [61]. They found that the entropy estimates correlate with the solvent-accessible surface area (SASA) of the ligands. In this work, estimates of the entropy contribution to the binding free energy ($-\Delta S$) used the NMODE module of AMBER. The calculation condition was limited to structures every 100 ps (200 snapshots over the 5 ns trajectory) from 34th ns to 50th ns. To find a balance between accuracy and efficiency, 12 Å was kept, and the other less important residues were truncated. We used a notation of $\Delta G''$ to indicate binding energies without the inclusion of entropy, whereas ΔG refers to the binding energy inclusive of entropy.

Supplementary Materials: The following are available online at <http://www.mdpi.com/1660-3397/17/5/303/s1>.

Author Contributions: R.Y. conceived of and designed the experiments. R.Y., X.X., J.L., and Z.Z. performed the experiments. R.Y. and X.X. analyzed the data. R.Y. and T.J. contributed materials/analysis tools. R.Y. and X.X. wrote the paper.

Funding: This work was supported by the Fundamental Research Funds for the Central Universities (201762011, 201941012), with grants from the National Natural Science Foundation of China (NSFC) (No. 81502977, No. 41830535), the National Laboratory Director Fund (QNL201709), and the Taishan Scholars Program of Shandong, China. We thank for the support from the Center for High Performance Computing and System Simulation, Pilot National Laboratory for Marine Science and Technology

Conflicts of Interest: The authors declare no conflicts of interest.

References

1. Hogg, R.C.; Raggenbass, M.; Bertrand, D. Nicotinic acetylcholine receptors: from structure to brain function. *Rev. Physiol. Biochem. Pharmacol.* **2003**, *147*, 1–46.
2. Changeux, J.-P. The nicotinic acetylcholine receptor: the founding father of the pentameric ligand-gated ion channel superfamily. *J. Biol. Chem.* **2012**, *287*, 40207–40215. [[CrossRef](#)]
3. Albuquerque, E.X.; Pereira, E.F.R.; Alkondon, M.; Rogers, S.W. Mammalian nicotinic acetylcholine receptors: from structure to function. *Physiol. Rev.* **2009**, *89*, 73–120. [[CrossRef](#)] [[PubMed](#)]
4. Isaias, I.U.; Spiegel, J.; Brumberg, J.; Cosgrove, K.P.; Marotta, G.; Oishi, N.; Higuchi, T.; Küsters, S.; Schiller, M.; Dillmann, U.; et al. Nicotinic acetylcholine receptor density in cognitively intact subjects at an early stage of Parkinson's disease. *Front. Aging Neurosci.* **2014**, *6*, 213. [[CrossRef](#)]
5. Lombardo, S.; Maskos, U. Role of the nicotinic acetylcholine receptor in Alzheimer's disease pathology and treatment. *Neuropharmacology* **2015**, *96*, 255–262. [[CrossRef](#)] [[PubMed](#)]
6. Becchetti, A.; Aracri, P.; Meneghini, S.; Brusco, S.; Amadeo, A. The role of nicotinic acetylcholine receptors in autosomal dominant nocturnal frontal lobe epilepsy. *Front. Physiol.* **2015**, *6*, 22. [[CrossRef](#)]
7. Brumwell, C.L.; Johnson, J.L.; Jacob, M.H. Extrasynaptic alpha 7-nicotinic acetylcholine receptor expression in developing neurons is regulated by inputs, targets, and activity. *J. Neurosci.* **2002**, *22*, 8101–8109. [[CrossRef](#)] [[PubMed](#)]
8. Posadas, I.; López-Hernández, B.; Ceña, V. Nicotinic receptors in neurodegeneration. *Curr. Neuropharmacol.* **2013**, *11*, 298–314. [[CrossRef](#)]
9. Taly, A.; Corringer, P.-J.; Guedin, D.; Lestage, P.; Changeux, J.-P. Nicotinic receptors: allosteric transitions and therapeutic targets in the nervous system. *Nat. Rev. Drug Discov.* **2009**, *8*, 733–750. [[CrossRef](#)] [[PubMed](#)]
10. Kaas, Q.; Westermann, J.-C.; Halai, R.; Wang, C.K.L.; Craik, D.J. ConoServer, a database for conopeptide sequences and structures. *Bioinformatics* **2008**, *24*, 445–446. [[CrossRef](#)]
11. Kaas, Q.; Yu, R.; Jin, A.-H.; Dutertre, S.; Craik, D.J. ConoServer: Updated content, knowledge, and discovery tools in the conopeptide database. *Nucleic Acids Res.* **2012**, *40*, D325–D330. [[CrossRef](#)]

12. Azam, L.; McIntosh, J.M. Alpha-conotoxins as pharmacological probes of nicotinic acetylcholine receptors. *Acta Pharmacol. Sin.* **2009**, *30*, 771–783. [[CrossRef](#)]
13. Ellison, M.; Gao, F.; Wang, H.-L.; Sine, S.M.; McIntosh, J.M.; Olivera, B.M. Alpha-conotoxins ImI and ImII target distinct regions of the human alpha7 nicotinic acetylcholine receptor and distinguish human nicotinic receptor subtypes. *Biochemistry* **2004**, *43*, 16019–16026. [[CrossRef](#)]
14. Servent, D.; Thanh, H.L.; Antil, S.; Bertrand, D.; Corringer, P.J.; Changeux, J.P.; Ménez, A. Functional determinants by which snake and cone snail toxins block the alpha 7 neuronal nicotinic acetylcholine receptors. *J. Physiol. Paris* **1998**, *92*, 107–111. [[CrossRef](#)]
15. Posnett, D.N.; Mcgrath, H.; Tam, J.P. A novel method for producing anti-peptide antibodies. Production of site-specific antibodies to the T cell antigen receptor beta-chain. *J. Biol. Chem.* **1988**, *263*, 1719–1725.
16. Tam, J.P. Synthetic peptide vaccine design: synthesis and properties of a high-density multiple antigenic peptide system. *Proc. Nat. Acad. Sci. U. S. A.* **1988**, *85*, 5409–5413. [[CrossRef](#)]
17. Coles, D.J.; Toth, I. Dendritic peptide-based carriers for gene delivery. *Curr. Drug Deliv.* **2009**, *6*, 338–342. [[CrossRef](#)]
18. Zhang, C.; Pan, D.; Luo, K.; She, W.; Guo, C.; Yang, Y.; Gu, Z. Peptide dendrimer-Doxorubicin conjugate-based nanoparticles as an enzyme-responsive drug delivery system for cancer therapy. *Adv. Healthc. Mater.* **2014**, *3*, 1299–1308. [[CrossRef](#)]
19. De Oliveira, E.; Villén, J.; Giralt, E.; Andreu, D. Synthetic approaches to multivalent lipopeptide dendrimers containing cyclic disulfide epitopes of foot-and-mouth disease virus. *Bioconjug. Chem.* **2003**, *14*, 144–152. [[CrossRef](#)]
20. Nardin, E.H.; Calvo-Calle, J.M.; Oliveira, G.A.; Nussenzweig, R.S.; Schneider, M.; Tiercy, J.M.; Loutan, L.; Hochstrasser, D.; Rose, K. A totally synthetic polyoxime malaria vaccine containing Plasmodium falciparum B cell and universal T cell epitopes elicits immune responses in volunteers of diverse HLA types. *J. Immunol.* **2001**, *166*, 481–489. [[CrossRef](#)]
21. Schellinger, J.G.; Danan-Leon, L.M.; Hoch, J.A.; Kassa, A.; Srivastava, I.; Davis, D.; Gervay-Hague, J. Synthesis of a trimeric gp120 epitope mimic conjugated to a T-helper peptide to improve antigenicity. *J. Am. Chem. Soc.* **2011**, *133*, 3230–3233. [[CrossRef](#)] [[PubMed](#)]
22. Skwarczynski, M.; Zaman, M.; Urbani, C.N.; Lin, I.-C.; Jia, Z.; Batzloff, M.R.; Good, M.F.; Monteiro, M.J.; Toth, I. Polyacrylate dendrimer nanoparticles: a self-adjuvanting vaccine delivery system. *Angew. Chem. Int. Ed. Engl.* **2010**, *49*, 5742–5745. [[CrossRef](#)]
23. Veprek, P.; Hajdúch, M.; Dzubak, P.; Kuklík, R.; Polakova, J.; Bezouska, K. Comblike dendrimers containing Tn antigen modulate natural killing and induce the production of Tn specific antibodies. *J. Med. Chem.* **2006**, *49*, 6400–6407. [[CrossRef](#)] [[PubMed](#)]
24. Bay, S.; Cantacuzene, D.; Leclerc, C.; Lo-Man, R. Multiple antigen glycopeptide carbohydrate, vaccine comprising the same and use thereof 2010. US Patent US7696326B2, 3 May 2007.
25. Tarallo, R.; Carberry, T.P.; Falanga, A.; Vitiello, M.; Galdiero, S.; Galdiero, M.; Weck, M. Dendrimers functionalized with membrane-interacting peptides for viral inhibition. *Int. J. Nanomed.* **2013**, *8*, 521–534.
26. Hatano, K.; Matsubara, T.; Muramatsu, Y.; Ezure, M.; Koyama, T.; Matsuoka, K.; Kuriyama, R.; Kori, H.; Sato, T. Synthesis and influenza virus inhibitory activities of carbosilane dendrimers peripherally functionalized with hemagglutinin-binding Peptide. *J. Med. Chem.* **2014**, *57*, 8332–8339. [[CrossRef](#)] [[PubMed](#)]
27. Zhang, X.; Zhang, Z.; Xu, X.; Li, Y.; Li, Y.; Jian, Y.; Gu, Z. Bioinspired therapeutic dendrimers as efficient peptide drugs based on supramolecular interactions for tumor inhibition. *Angew. Chem. Int. Ed. Engl.* **2015**, *54*, 4289–4294. [[CrossRef](#)]
28. Bonnal, S.; Vigevani, L.; Valcárcel, J. The spliceosome as a target of novel antitumour drugs. *Nat. Rev. Drug Discov.* **2012**, *11*, 847–859. [[CrossRef](#)]
29. Henning, L.M.; Bhatia, S.; Bertazzon, M.; Marczyneke, M.; Seitz, O.; Volkmer, R.; Haag, R.; Freund, C. Exploring monovalent and multivalent peptides for the inhibition of FBP21-tWW. *Beilstein. J. Org. Chem.* **2015**, *11*, 701–706. [[CrossRef](#)]
30. Varamini, P.; Rafiee, A.; Giddam, A.K.; Mansfeld, F.M.; Steyn, F.; Toth, I. Development of New Gonadotropin-Releasing Hormone-Modified Dendrimer Platforms with Direct Antiproliferative and Gonadotropin Releasing Activity. *J. Med. Chem.* **2017**, *60*, 8309–8320. [[CrossRef](#)] [[PubMed](#)]
31. Yim, C.-B.; Dijkgraaf, I.; Merckx, R.; Versluis, C.; Eek, A.; Mulder, G.E.; Rijkers, D.T.S.; Boerman, O.C.; Liskamp, R.M.J. Synthesis of DOTA-conjugated multimeric [Tyr3]octreotide peptides via a combination of

- Cu(I)-catalyzed “click” cycloaddition and thio acid/sulfonyl azide “sulfo-click” amidation and their in vivo evaluation. *J. Med. Chem.* **2010**, *53*, 3944–3953. [[CrossRef](#)]
32. Livant, D. Compounds for, and methods of, treating cancer and inhibiting invasion and metastases. U.S. Patent 20120077755 A1, 29 March 2012.
 33. Wan, J.; Huang, J.X.; Vetter, I.; Mobli, M.; Lawson, J.; Tae, H.-S.; Abraham, N.; Paul, B.; Cooper, M.A.; Adams, D.J.; et al. α -Conotoxin dendrimers have enhanced potency and selectivity for homomeric nicotinic acetylcholine receptors. *J. Am. Chem. Soc.* **2015**, *137*, 3209–3212. [[CrossRef](#)]
 34. Jiang, Y.-H.; Emau, P.; Cairns, J.S.; Flanary, L.; Morton, W.R.; McCarthy, T.D.; Tsai, C.-C. SPL7013 gel as a topical microbicide for prevention of vaginal transmission of SHIV89.6P in macaques. *AIDS Res. Hum. Retroviruses* **2005**, *21*, 207–213. [[CrossRef](#)]
 35. Wan, J.; Mobli, M.; Brust, A.; Muttenthaler, M.; Andersson, Å.; Ragnarsson, L.; Castro, J.; Vetter, I.; Huang, J.X.; Nilsson, M. Synthesis of Multivalent [Lys8]-Oxytocin Dendrimers that Inhibit Visceral Nociceptive Responses. *Au. J. Chem.* **2017**, *70*. [[CrossRef](#)]
 36. Wan, J.; Brust, A.; Bholra, R.F.; Jha, P.; Mobli, M.; Lewis, R.J.; Christie, M.J.; Alewood, P.F. Inhibition of the norepinephrine transporter by χ -conotoxin dendrimers. *J. Pept. Sci.* **2016**, *22*, 280–289. [[CrossRef](#)]
 37. Maslennikov, I.V.; Shenkarev, Z.O.; Zhmak, M.N.; Ivanov, V.T.; Methfessel, C.; Tsetlin, V.I.; Arseniev, A.S. NMR spatial structure of α -conotoxin ImI reveals a common scaffold in snail and snake toxins recognizing neuronal nicotinic acetylcholine receptors 1. *FEBS Lett.* **1999**, *444*, 275–280. [[CrossRef](#)]
 38. Quiram, P.A.; Jones, J.J.; Sine, S.M. Pairwise Interactions between Neuronal α 7 Acetylcholine Receptors and α -Conotoxin ImI. *J. Biol. Chem.* **1999**, *274*, 19517–19524. [[CrossRef](#)] [[PubMed](#)]
 39. Yu, R.; Craik, D.J.; Kaas, Q. Blockade of neuronal α 7-nAChR by α -conotoxin ImI explained by computational scanning and energy calculations. *PLoS Comput. Biol.* **2011**, *7*, e1002011. [[CrossRef](#)] [[PubMed](#)]
 40. Cheng, X.; Wang, H.; Grant, B.; Sine, S.M.; McCammon, J.A. Targeted Molecular Dynamics Study of C-Loop Closure and Channel Gating in Nicotinic Receptors. *PLoS Comput. Biol.* **2006**, *2*, e134. [[CrossRef](#)] [[PubMed](#)]
 41. Brams, M.; Pandya, A.; Kuzmin, D.; van Elk, R.; Krijnen, L.; Yakel, J.L.; Tsetlin, V.; Smit, A.B.; Ulens, C. A Structural and Mutagenic Blueprint for Molecular Recognition of Strychnine and d-Tubocurarine by Different Cys-Loop Receptors. *PLoS Biol.* **2011**, *9*, e1001034. [[CrossRef](#)] [[PubMed](#)]
 42. Ma, Q.; Tae, H.-S.; Wu, G.; Jiang, T.; Yu, R. Exploring the Relationship between Nicotinic Acetylcholine Receptor Ligand Size, Efficiency, Efficacy, and C-Loop Opening. *J. Chem. Inf. Model.* **2017**, *57*, 1947–1956. [[CrossRef](#)]
 43. Tsui, V.; Case, D.A. Theory and applications of the generalized born solvation model in macromolecular simulations. *Biopolymers* **2000**, *56*, 275–291. [[CrossRef](#)]
 44. Rastelli, G.; Rio, A.D.; Degliesposti, G.; Sgobba, M. Fast and accurate predictions of binding free energies using MM-PBSA and MM-GBSA. *J. Comput. Chem* **2010**, *31*, 797–810. [[CrossRef](#)]
 45. Zhang, X.; Li, X.; Wang, R. Interpretation of the Binding Affinities of PTP1B Inhibitors with the MM-GB/SA Method and the X-Score Scoring Function. *J. Chem. Inf. Model.* **2009**, *49*, 1033–1048. [[CrossRef](#)] [[PubMed](#)]
 46. Hou, T.; Wang, J.; Li, Y.; Wang, W. Assessing the performance of the molecular mechanics/Poisson Boltzmann surface area and molecular mechanics/generalized Born surface area methods. II. The accuracy of ranking poses generated from docking. *J. Comput. Chem.* **2011**, *32*, 866–877. [[CrossRef](#)]
 47. da Silva Santos, S.; Igne Ferreira, E.; Giarolla, J. Dendrimer Prodrugs. *Molecules* **2016**, *21*, 686. [[CrossRef](#)]
 48. Le Novère, N.; Grutter, T.; Changeux, J.-P. Models of the extracellular domain of the nicotinic receptors and of agonist- and Ca²⁺-binding sites. *Proc. Natl. Acad. Sci. U. S. A.* **2002**, *99*, 3210–3215. [[CrossRef](#)] [[PubMed](#)]
 49. Costa, V.; Nistri, A.; Cavalli, A.; Carloni, P. A structural model of agonist binding to the α 3 β 4 neuronal nicotinic receptor. *Br. J. Pharmacol.* **2003**, *140*, 921–931. [[CrossRef](#)]
 50. Pérez, E.G.; Cassels, B.K.; Zapata-Torres, G. Molecular modeling of the α 9 α 10 nicotinic acetylcholine receptor subtype. *Bioorg. Med. Chem. Lett.* **2009**, *19*, 251–254. [[CrossRef](#)]
 51. Edgar, R.C. MUSCLE: A multiple sequence alignment method with reduced time and space complexity. *BMC Bioinf.* **2004**, *5*, 113. [[CrossRef](#)] [[PubMed](#)]
 52. Šali, A.; Blundell, T.L. Comparative Protein Modelling by Satisfaction of Spatial Restraints. *J. Mol. Biol.* **1993**, *234*, 779–815. [[CrossRef](#)]
 53. Morris, A.L.; MacArthur, M.W.; Hutchinson, E.G.; Thornton, J.M. Stereochemical quality of protein structure coordinates. *Proteins* **1992**, *12*, 345–364. [[CrossRef](#)] [[PubMed](#)]

54. Chen, V.B.; Arendall, W.B.; Headd, J.J.; Keedy, D.A.; Immormino, R.M.; Kapral, G.J.; Murray, L.W.; Richardson, J.S.; Richardson, D.C. MolProbity: All-atom structure validation for macromolecular crystallography. *Acta Crystallogr. D. Biol. Crystallogr.* **2010**, *66*, 12–21. [[CrossRef](#)]
55. Case, D.A.; Cerutti, D.S.; Cheatham, T.E., III; Darden, T.A.; Duke, R.E.; Giese, T.J.; Gohlke, H.; Goetz, A.W.; Greene, D. *Amber 2017 Reference Manual*; University of California: San Francisco, CA, USA, 2017.
56. Dupradeau, F.-Y.; Pigache, A.; Zaffran, T.; Savineau, C.; Lelong, R.; Grivel, N.; Lelong, D.; Rosanski, W.; Cieplak, P. The R.E.D. tools: advances in RESP and ESP charge derivation and force field library building. *Phys. Chem. Chem. Phys.* **2010**, *12*, 7821–7839. [[CrossRef](#)]
57. Maier, J.A.; Martinez, C.; Kasavajhala, K.; Wickstrom, L.; Hauser, K.E.; Simmerling, C. ff14SB: Improving the Accuracy of Protein Side Chain and Backbone Parameters from ff99SB. *J. Chem. Theory Comput.* **2015**, *11*, 3696–3713. [[CrossRef](#)] [[PubMed](#)]
58. Chen, F.; Huang, W.; Jiang, T.; Yu, R. Determination of the μ -Conotoxin P111A Specificity Against Voltage-Gated Sodium Channels from Binding Energy Calculations. *Mar. Drugs* **2018**, *16*, 153. [[CrossRef](#)] [[PubMed](#)]
59. Wittayanarakul, K.; Hannongbua, S.; Feig, M. Accurate prediction of protonation state as a prerequisite for reliable MM-PB(GB)SA binding free energy calculations of HIV-1 protease inhibitors. *J. Comput. Chem.* **2010**, *29*, 673–685. [[CrossRef](#)]
60. Dunitz, J.D. Win some, lose some: enthalpy-entropy compensation in weak intermolecular interactions. *Chem. Biol.* **1995**, *2*, 709–712. [[CrossRef](#)]
61. Oehme, D.P.; Brownlee, R.T.C.; Wilson, D.J.D. Effect of atomic charge, solvation, entropy, and ligand protonation state on MM-PB(GB)SA binding energies of HIV protease. *J. Comput. Chem.* **2012**, *33*, 2566–2580. [[CrossRef](#)]



© 2019 by the authors. Licensee MDPI, Basel, Switzerland. This article is an open access article distributed under the terms and conditions of the Creative Commons Attribution (CC BY) license (<http://creativecommons.org/licenses/by/4.0/>).