# **SPECIAL ISSUE INSIGHT**

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# Check for updates

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Continuous intra-abdominal pressure: is it

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Abdominal contents are primarily fluid in character so that pressure within this compartment follows Pascal's hydrostatic law. Intra-abdominal pressure (IAP) is the steady state pressure within the abdominal cavity and changes during respiration with an inspiratory increase [1]. Mean perfusion pressure (MPP) is the difference between mean arterial pressure (MAP) and central venous pressure (CVP). Similarly abdominal perfusion pressure (APP) is calculated as the difference between MAP and IAP. MPP has been seen to be associated with progression of organ system injury [2].

## **Consensus definition**

The reference standard for intermittent IAP measurements is via the bladder with a maximal instillation volume of 25 mL of sterile saline. IAP should be expressed in mmHg and measured at end-expiration in the supine position after ensuring abdominal muscle contractions are absent and with the transducer zeroed at the level where the midaxillary line crosses the iliac crest and is approximately 5–7 mmHg in healthy and 10 mmHg in critically ill adults. IAH is defined by a sustained or repeated elevation in IAP  $\geq$  12 mmHg. ACS is defined as a sustained IAP > 20 mmHg that is associated with new organ dysfunction/failure [3].

## Pathophysiology

There are four factors affecting IAP: gravity, uniformity of compression, shear stress and deformation, and presence

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ACS and guide treatment. The kidneys are very vulnerable to raised IAP and some suggest they are the canary in the coalmine for IAH and elevated renal parenchymal and venous pressures are the main causes for AKI. Subsequently, raised IAP decreases chest wall compliance and in combination with the cranial shift of the diaphragm this results in reduced lung volumes causing compression atelectasis, hypoxia and hypercarbia. In addition, the negative effects of increased IAP on the cardiovascular system are explained by significant changes in preload, afterload, and contractility. As a result, reduced cardiac output leads to low blood pressure followed by poor organ perfusion and eventually worsening of IAH. A summary of the effects of raised IAP on other end-organs are shown in Fig. 1 Panel A [3, 5, 6]. Intermittent intra-abdominal pressure measurement Measuring IAP via the bladder is currently the most

of abdominal muscle contraction [1, 4]. However, in the critically ill patient the abdomen often behaves as a

hydraulic system. Raised IAP affects multiple organ sys-

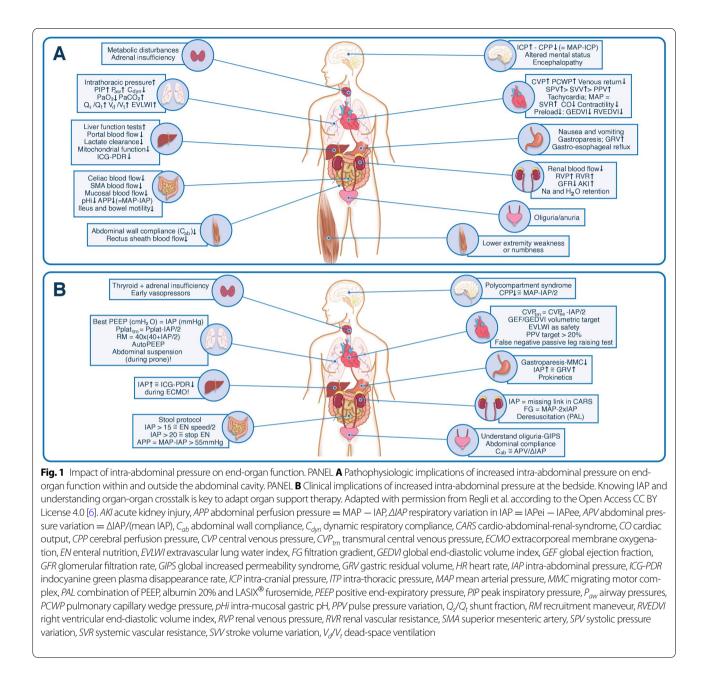
tems within and outside the abdominal cavity and under-

standing the pathophysiology can prevent impending

widely accepted technique due to its simplicity, reliability, user-friendliness, and reproducibility with the added benefits of low cost minimal invasiveness and low complication risks [5]. This technique was originally described by Kron and later modified by Iberti, Cheatham and Malbrain [1] (ESM Fig. 1) to a closed system using a pressure transducer that allowed for multiple IAP measurements [7]. IAP measurements can also be performed via the height of the urine column with a Foley manometer [1] (ESM Fig. 2). Particularly in patients with bladder trauma, neurogenic bladder dysfunction, outflow obstruction, or pelvic hematomas where measurements via the bladder might be unreliable and/or contraindicated, the stomach







can then be used as an alternative route (ESM Fig. 3 and 4) [1]. Coca et al. reported data from 205 kidney transplant patients where intermittently measured high IAP was common and associated with delayed graft function, postoperative complications, and absence of graft function recovery [8]. In addition, IAP is a prognostic marker when measured during exploratory laparotomy in surgical patients, with higher numbers associated with mortality, a higher SOFA score and prolonged ileus. Fifty five percent of patients having cardiac surgery were found to have IAH (IAP 12 or more in mmHg) when measured

intermittently and a further 24% had higher pressures during the first two hours of ICU stay. Even though routine intermittent IAP measurement suggests that high IAP is uncommon, it should be considered postoperatively in patients with obesity. Other factors associated with development of IAH in cardiac surgery would be prolonged cardiopulmonary bypass or surgical time, and need for vasopressor support.

# Continuous intra-abdominal pressure measurement

Intermittent IAP measurements via the bladder in symptomatic patients or those with a high clinical suspicion of developing abdominal compartment syndrome (ACS) every 4 to 6 h is widely accepted as routine practice. Today different techniques are available for continuous intraabdominal pressure (CIAP) measurement and estimation. CIAP can be measured directly via the peritoneum (this is the technique used during laparoscopy to limit insufflation pressures to 14 mmHg, or chronic ambulatory peritoneal dialysis), however the use of direct intraperitoneal pressure measurement has not been advocated in critically ill patients because its invasiveness, infection risk and complications. The use of balloon-tipped abdominal catheters has also been described [1]. CIAP can also be estimated in critically ill patients via the bladder using a 3-way Foley with continuous irrigation. In the near future another device will become available that can be connected to an existing Foley (Serenno Medical, Yokeneam Illit, Israel). Finally, CIAP can be estimated via a balloon-tipped nasogastric tube (Spiegelberg, Hamburg, Germany) [9]. Recently, the Accuryn Monitoring System (Potrero Medical, Hayward, California, USA) using a special urinary catheter with an extra airfilled balloon at the tip has been FDA cleared for measuring IAP, urinary output (UO), and core body temperature. A significant advantage of this system is near-continuous, high-fidelity and high-resolution IAP monitoring as shown in a recent study in cardiac surgery patients observing persistent increases in IAP that had previously not been shown with traditional spot-check measurements [10]. One more consideration when measuring IAP at high frequency is the signal to noise factor. Applying a 10-min running median and resampling data at longer intervals every 15 min may help mitigate the effect of patient position and factors that induce rapid sudden changes in IAP such as diaphragmatic contraction with a coughing [10].

### Less invasive techniques

Less invasive techniques include the use of a strain gauge, respiratory inductance plethysmography, or abdominal tensiometer, as well as the application of ultrasoundbased techniques for IAP monitoring (like tonometry, abdominal wall thickness, Doppler, or laser), bio-electrical impedance analysis, microwave reflectometry, digital image correlation and finally, the use of a wireless motility capsule [11]. Recently, IAP was measured noninvasively in an in vitro model with an advanced abdominal wall phantom using a transient radar method.

# Is continuous intra-abdominal pressure measurement the future?

Continuous intra-abdominal pressure has many possibilities: first, an IAP trend allows to assess the effect of treatment, to visualize the interaction between physiologic variables in real time. Second, CIAP allows the user to obtain a continuous APP trend as a potential better resuscitation target and for early identification of impending ACS. Third, CIAP allows automation via computer analysis and calculation of the area under the curve (AUC) and the time above a threshold as in analogy to ICP where the pressure time-burden may be of prognostic value. Fourth, CIAP allows to diagnose poly-compartment syndrome and prediction of acute kidney injury (AKI) and cardioabdominal-renal syndrome (CARS) earlier than via the intermittent measurement technique. While most prediction models for kidney injury feature urine output in conjunction with other parameters, very few feature IAP, and those that do have used IAP as an intermittent tool in clinically at risk patients. Specifically, the use of CIAP allowed prediction of AKI with a higher precision and recall compared to the use of urinary output alone, and up to 28 h before the event [12]. Fifth, it allows to calculate abdomino-thoracic and thoraco-abdominal pressure transmission which is important to understand organorgan crosstalk phenomena (ESM Fig. 5) [4, 13-15]. Sixth, it helps us understand problems during ventilation and weaning, for example forced expiration in COPD, ventilator asynchrony, increased transdiaphragmatic pressures and work-of-breathing. Seventh, it might help us to select lung protective ventilation, driving pressure, recruitment maneuver, and optimal PEEP (in  $cmH_2O$ ) setting equal to IAP (in mmHg) [6]. Finally, it provides us with an idea of abdominal wall compliance  $(C_{ab})$  with the respiratory abdominal variation test (RAVT), where the higher abdominal pressure variation (APV) and respiratory variations ( $\Delta$ IAP) the lower the  $C_{\rm ab}$  [4]. Analysis of the raw IAP data signal not only gives us information on absolute values of IAP (with end inspiratory and end expiratory value), but also delta ( $\Delta$ ) IAP (IAP<sub>ei</sub> minus IAP<sub>ee</sub>), APV ( $\Delta$ IAP/mean IAP), which can be used to assess  $C_{ab}$  and splanchnic perfusion. Furthermore, this data can be combined with heart rate, respiratory rate, and relative stroke volume and pulse pressure variation data (ESM Fig. 6, Panels A-D). Medical management options are summarized and listed in ESM Fig. 7.

#### Supplementary Information

The online version contains supplementary material available at https://doi. org/10.1007/s00134-022-06780-4.

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#### Declarations

#### **Conflicts of interest**

MLNGM is a Professor of Critical Care Research at the 1st Department of Anaesthesiology and Intensive Therapy, Medical University of Lublin, Poland. He is co-founder, past-President and current Treasurer of WSACS (The Abdominal Compartment Society, http://www.wsacs.org). He is a member of the medical advisory Board of Pulsion Medical Systems (part of Getinge group), Serenno Medical, Potrero Medical, and Baxter, and consults for BBraun, Becton Dickinson, ConvaTec, Spiegelberg, and Holtech Medical. He is the co-founder and President of the International Fluid Academy (IFA). The IFA (http://www. fluidacademy.org) is integrated within the not-for-profit charitable organization iMERiT. International Medical Education and Research Initiative, under Belgian law. AKK is a paid consultant for and chairs the steering committee for the Predict AKI group for Potrero Medical and also consults for Edwards Lifesciences, Philips North America, GE Healthcare, Hill-Rom, and Caretaker Medical. His institution has grant funding from Caretaker Medical for ongoing investigations on portable hemodynamic monitoring. AKK is on the executive advisory board for Medtronic and Retia Medical. AKK receives support from the Wake Forest CTSI via NIH/NCATS KL2 for a trial of continuous portable hemodynamic and saturation monitoring on hospital wards. The other author has no potential conflicts of interest in relation to the contents of this paper. The payment of the Open Access fee was kindly supported by an unrestricted educational grant from Potrero Medical.

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Received: 11 April 2022 Accepted: 5 June 2022 Published: 4 August 2022

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