

Research article

Open Access

Fibrin and poly(lactic-co-glycolic acid) hybrid scaffold promotes early chondrogenesis of articular chondrocytes: an *in vitro* study

Munirah Sha'ban^{1,2}, Soon Hee Kim³, Ruszymah BH Idrus^{1,2} and Gilson Khang^{*3}

Address: ¹Department of Physiology, Faculty of Medicine, Universiti Kebangsaan Malaysia, Jalan Raja Muda Abdul Aziz, 50300 Kuala Lumpur, Malaysia, ²Tissue Engineering Laboratory, Universiti Kebangsaan Malaysia Hospital, 9th floor, Clinical Block, Jalan Yaacob Latif, 56000 Cheras, Kuala Lumpur, Malaysia and ³BK-21 Polymer BIN Fusion Research Team, Department of Polymer Science and Technology, Chonbuk National University, 664-14, Dukjin, Jeonju, 561-756, Seoul, Korea

Email: Munirah Sha'ban - munirahshaban@gmail.com; Soon Hee Kim - aofurwjr@hanmail.net; Ruszymah BH Idrus - ruszy@medic.ukm.my; Gilson Khang* - gskhang@chonbuk.ac.kr

* Corresponding author

Published: 25 April 2008

Received: 23 August 2007

Journal of Orthopaedic Surgery and Research 2008, 3:17 doi:10.1186/1749-799X-3-17

Accepted: 25 April 2008

This article is available from: <http://www.josr-online.com/content/3/1/17>

© 2008 Sha'ban et al; licensee BioMed Central Ltd.

This is an Open Access article distributed under the terms of the Creative Commons Attribution License (<http://creativecommons.org/licenses/by/2.0>), which permits unrestricted use, distribution, and reproduction in any medium, provided the original work is properly cited.

Abstract

Background: Synthetic- and naturally derived- biodegradable polymers have been widely used to construct scaffolds for cartilage tissue engineering. Poly(lactic-co-glycolic acid) (PLGA) are bioresorbable and biocompatible, rendering them as a promising tool for clinical application. To minimize cells lost during the seeding procedure, we used the natural polymer fibrin to immobilize cells and to provide homogenous cells distribution in PLGA scaffolds. We evaluated *in vitro* chondrogenesis of rabbit articular chondrocytes in PLGA scaffolds using fibrin as cell transplantation matrix.

Methods: PLGA scaffolds were soaked in chondrocytes-fibrin suspension (1×10^6 cells/scaffold) and polymerized by dropping thrombin-calcium chloride (CaCl_2) solution. PLGA-seeded chondrocytes was used as control. All constructs were cultured for a maximum of 21 days. Cell proliferation activity was measured at 1, 3, 7, 14 and 21 days *in vitro* using 3-(4,5-dimethylthiazole-2-yl)-2-, 5-diphenyltetrazolium-bromide (MTT) assay. Morphological observation, histology, immunohistochemistry (IHC), gene expression and sulphated-glycosaminoglycan (sGAG) analyses were performed at each time point of 1, 2 and 3 weeks to elucidate *in vitro* cartilage development and deposition of cartilage-specific extracellular matrix (ECM).

Results: Cell proliferation activity was gradually increased from day-1 until day-14 and declined by day-21. A significant cartilaginous tissue formation was detected as early as 2-week in fibrin/PLGA hybrid construct as confirmed by the presence of cartilage-isolated cells and lacunae embedded within basophilic ECM. Cartilage formation was remarkably evidenced after 3 weeks. Presence of cartilage-specific proteoglycan and glycosaminoglycan (GAG) in fibrin/PLGA hybrid constructs were confirmed by positive Safranin O and Alcian Blue staining. Collagen type II exhibited intense immunopositivity at the pericellular matrix. Chondrogenic properties were further demonstrated by the expression of genes encoded for cartilage-specific markers, collagen type II and aggrecan core protein. Interestingly, suppression of cartilage dedifferentiation marker; collagen type I was observed after 2 and 3 weeks of *in vitro* culture. The sulphated-glycosaminoglycan (sGAG) production in fibrin/PLGA was significantly higher than in PLGA.

Conclusion: Fibrin/PLGA promotes early *in vitro* chondrogenesis of rabbit articular chondrocytes. This study suggests that fibrin/PLGA may serve as a potential cell delivery vehicle and a structural basis for *in vitro* tissue-engineered articular cartilage.

Background

Autologous chondrocytes implantation (ACI) was first published by Brittberg et al. [1] in 1994. This technique is quickly becoming a successful and viable alternative treatment in orthopaedic surgery to total knee replacement, arthroscopy, and abrasion therapy. Two-step procedures are required for ACI. After cartilage is biopsied and cultured, the next procedure is to implant cultured chondrocytes arthroscopically. The second procedure is invasive and has all of the risks associated with open surgery. Future improvements could be shifting the arthrotomy to an arthroscopic procedure to help decrease the morbidity associated with arthrotomy. Therefore, we believed *in vitro* generation of 3D cartilage constructs can be utilized to overcome the drawback. In recent years, several promising recoveries of small full thickness lesions using *in vitro* 3D cartilage constructs have been discovered in rabbit [2-4], goat [5,6], and dog [7]. We have successfully performed autologous 'chondrocytes-fibrin' construct (ACFC) implantation in sheep model [8-10] with good results. However during implantation, we still performed arthrotomy and used periosteum to hold the implant since ACFC was too soft to hold into defect independently. Therefore, basic research is still necessary to develop its full potential. Our next aim is to improve the scaffolding material of our *in vitro* 3D cartilage construct.

Recently, various synthetic- and naturally-derived biodegradable polymers have been widely used to construct scaffolds for tissue engineering purposes [11,12]. Many trials have successfully cultured chondrocytes [13-15], reconstructed tissue engineered cartilage [16-19] and transplanted engineered cartilage into defect [3,8-10]. Thus, biocompatible scaffolds that afford cells proliferation and matrix accumulation have been widely investigated [2,20,21]. Advantages of synthetically-derived biodegradable polymers include controllable degradation rate, high reproducibility, and easy to fabricate into specific shapes. Whilst naturally-derived biodegradable polymers are usually mimicked the key elements of normal tissue [22].

Poly(lactic-co-glycolic acid) (PLGA) are bioresorbable and biocompatible synthetic polymer, rendering them as a promising tool for regenerative medicine and clinical application. Numerous attempts have been made for successful tissue reconstruction using PLGA-based scaffold either by PLGA itself [23,24] or in combination with natural polymers such as collagen [21,25], and extracellular matrices scaffolds, i.e. small intestinal submucosa [26,27] as well as demineralised bone particles [28]. Incorporation of bioactive molecules on PLGA surface is believed to mediate cells behavior, e.g. proliferation, differentiation and function [26-28]. To minimize cells lost during *in vitro* seeding procedure, we used fibrin to immobilize cells

and to provide homogenous cells distribution in PLGA scaffolds. Until this article is written, apart from similar approach conducted by the research group from Germany [29-31], there is limited information with regard to the use of fibrin as a cell transplantation matrix for articular chondrocyte in PLGA. Previously, the use of fibrin gel immobilization technique resulted in homogeneous distribution and promoted bone formation of human periosteum-derived progenitor cells in PLGA [29], PLGA-TCP composites [30] and PLGA-polydioxanone fleeces [31]. Fibrin has also been used for cartilage reconstruction purposes [8-10,13-20]. We hypothesized that fibrin would be an ideal cell carrier/transplantation matrix and to enhance *in vitro* chondrogenesis of rabbit articular chondrocytes by means of morphological, histological, biochemical and phenotypically similar to the normal hyaline cartilage.

Methods

Harvest of cartilage, chondrocytes isolation and monolayer culture expansion

Articular cartilage was aseptically dissected from the femoral condyles and patellae of 6 weeks-old New Zealand White rabbits (n = 6). Each sample was processed within 6 to 12 hours post-surgery. Cartilage was washed, minced and digested with 0.6% collagenase A (Roche Applied Science, Germany) at 37°C for 6 hours. Isolated chondrocytes were cultured at a density of 5,000 cells/cm² in F12 nutrient mixture (F12) and Dulbecco's Modified Eagle Medium (DMEM) (Gibco, Grand Island, NY) supplemented with 10% foetal bovine serum (FBS) (Gibco) with the presence of antibiotics and antimycotic (Gibco), 200 mM L-glutamine (Gibco) and 50 µg/ml of ascorbic acid (Sigma). All cultures were maintained in 5% CO₂ incubator (Optima Model 560, Optima Inc, USA) at 37°C with the medium changed every other day.

Preparation of microporous 3D PLGA scaffolds

PLGA copolymer (mole ratio 50:50, molecular weight 33,000 g/mole, Resomer RG 503 H) was purchased from Boehringer Ingelheim Pharma GmbH (Ingelheim, Germany). Micro-porous 3D PLGA scaffolds (0.2% w/v) were fabricated by the solvent casting/salt leaching technique using methylene chloride (CH₂Cl₂) (JT Baker, Baker Analyzed® A.C.S reagent, Malaysia) as previously described [26,32]. Sieved sodium chloride (NaCl) particles (90 and 180 µm) were dispersed in a polymer/solvent solution, which was then cast to make a scaffold using cylindrical silicone moulds (7 mm in diameter and 3 mm thickness). The salt particles were then leached out by continuous soaking in deionized water for 48 hours. The scaffolds were freeze-dried for 48 hours using freeze-dryer (IlShin Lab Co. Ltd, South Korea).

Formation of in vitro constructs

Each sample was assigned into two experimental groups – chondrocytes were seeded into (1) PLGA scaffolds with fibrin (fibrin/PLGA) and (2) PLGA without fibrin. Articular chondrocytes from primary passage (P0) were sub-cultured (P1) in 75 cm² culture flasks (Falcon). After confluence, cells were harvested, counted for total cell and viability. PLGA scaffolds were sterilized upon use by 70% ethanol. One million cells per scaffold was incorporated and resuspended with (1) fibrin glue kit from Greenplast® (Green Cross P. D. Company, Yongin, Korea) and (2) culture medium. PLGA scaffolds were soaked in 'chondrocytes-fibrin' admixture and polymerized within 5 minutes by dropping thrombin-CaCl₂ solution (Green Cross P. D. Company, Yongin, Korea). Chondrocytes suspension in culture medium was seeded directly into PLGA scaffolds. All constructs were cultured for 21 days *in vitro*. All constructs were evaluated at each time point of 1-, 2- and 3-weeks.

Measurement of cell proliferation activity of in vitro constructs

Cell proliferation activity and cells viability was measured using MTT assay at day 1, 3, 7, 14 and 21 *in vitro*. The tetrazolium compound MTT (0.5 mg/ml) (thiazolyl blue tetrazolium bromide, Sigma-Aldrich Inc., St Louis USA) was added to all constructs and incubated for 4 hours at 37°C. The resulted crystals were solubilised by dimethylsulfoxide (DMSO) (Sigma Chemical Co., St Louis, USA). The absorbance was read using E-Max ELISA plate reader (Molecular Device, USA) at 570 nm – yielding absorbance as a function of viable cell number. Data was expressed as mean ± standard error of the mean (SEM). Results were analyzed using Student's t-test and the difference are considered significance when $p < 0.05$.

Macroscopic observation, histology and immunohistochemistry analysis

Each construct was observed grossly at room temperature without any fixation and palpated with forceps to assess mechanical rigidity. After fixation with 10% formalin, specimens were processed and stained with Haematoxylin and Eosin (H&E) to assess tissue morphology, Safranin O to identify presence of proteoglycan-rich matrix and Alcian blue to detect accumulation of GAG. Immunohistochemistry (IHC) analysis was performed in accordance to the manufacturer's protocol (UltraTek HRP Kit, Immunotech, France) using monoclonal antibody (MAb) mouse anti-rabbit collagen type II (Calbiochem® EMD Biosciences, Inc. La Jolla) and MAb mouse anti-rabbit collagen type I (Sigma Aldrich).

Total RNA isolation, cDNA synthesis and conventional PCR

Total RNA was extracted from *in vitro* constructs at each time point of 1, 2 and 3 weeks using TRIzol reagent (Invitrogen, Carlsbad, CA) according to the manufacturer's protocol. Reverse transcription was carried out using Superscript™ II reverse transcriptase (Invitrogen, Carlsbad, CA) according to the manufacturer's protocol under the following conditions: 65°C for 5 minutes, 42°C for 2 minutes, 42°C and 70°C for 50 minutes and 15 minutes. Polymerase chain reaction was carried out using the Takara thermal cycler (Takara Bio Inc. Japan). Six- μ l of the amplified PCR products were separated by 1.5% agarose gel electrophoresis (SeaKem® LE Agarose, Cambrex Bio Science Rockland, Inc. USA), stained with SYBR® green nucleic acid gel stain (Cambrex Bio Science Rockland, Inc. USA) and visualized by UV transillumination using gel documentation system EDAS 290 Kodak (Viber Lourmat, France). All primer sequences were as follows: collagen type II: forward: 5'-gcaccatggacattggagg-3'/reverse: 5'-atgttttaaaaaatcgaag-3' [33]. Aggrecan core protein: forward: 5'-atcaacagagacctacgatgt-3'/reverse: 5'-gttaggtagag-gtagaccgt-3' [34]. Collagen type I: forward: 5'-gatcgcttcaggctcgagta-3'/reverse: 5'-ggcttcgggtggtcttga-3' [33]. Rabbit β -actin gene [34] was used as an endogenous control: forward: 5'-ccggcttcgcccgcgacg-3'/reverse: 5'-tcccggccagccaggtcc-3'. All primers were prepared by Genotech. Corp. (Daejeon, Korea).

Sulphated glycosaminoglycan (sGAG) production assay

All samples were digested with papain digestion solution (125 μ g/mL of papain, 5 mM L-cystein, 100 mM Na₂HPO₄, 5 mM EDTA, pH 6.8) at 60°C for 16 hours. Sulphated GAG contents were analyzed using a 1,9-dimethylmethylene blue (DMMB) assay [35]. Data was expressed as mean ± standard error of the mean (SEM). Results were analyzed using Student's t-test and the difference are considered significance when $p < 0.05$.

Results

Measurement of cell proliferation activity of in vitro constructs

Fibrin/PLGA hybrid construct and the PLGA group exhibited similar cell growth pattern *in vitro* (Figure 1). From the chart, cells proliferation was gradually increased from day-1 until day-7 with the fibrin/PLGA hybrid construct showed significantly higher cells proliferation activity ($p < 0.05$) compared to PLGA at day-3. Next, by day-14, cell proliferation activity in the fibrin/PLGA hybrid construct and PLGA constructs was significantly increased by 2.13-fold and 2.03-fold, respectively. However, the proliferation activity was then declined by day-21 in both groups. It has been indicated that the early stage of chondrogenesis involves the activity to establish cell-to-cell communication and cell-to-matrix interaction with regards to new

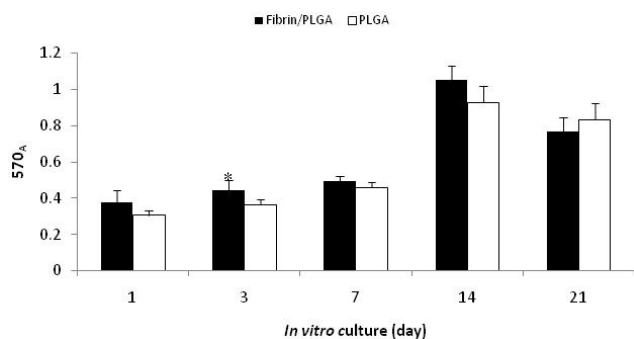


Figure 1
Measurement of cell proliferation activity of *in vitro* constructs. Fibrin/PLGA and PLGA construct exhibited similar growth pattern *in vitro*. Cells proliferation was gradually increased until day-14. Fibrin/PLGA showed a significant higher ($p < 0.05$) cells proliferation than PLGA at day-3 (*). Cells proliferation activity had declined by day-21.

cartilaginous tissue formation. We presumed at this stage the cellular proliferation has become less active. This could be one possible explanation in relation to the significant reduction of cell proliferation in fibrin/PLGA hybrid construct by 1.37-fold by the end of 21 days of *in vitro* culture.

Macroscopic observation of *in vitro* constructs

PLGA scaffold was designed in the shape of cylindrical disc with 7 mm diameter \times 3 mm height (Figure 2A). Scaffolds were prepared via solvent casting/salt leaching method. This selective dissolution technique produced highly porous polymer with pore sizes as same as the size of sieved NaCl granules (90 and 180 μ m). Morphological appearance of *in vitro* fibrin/PLGA hybrid constructs (Figure 2B) and PLGA construct (Figure 2C) was similar by day 7 in culture. However, at day 14, fibrin/PLGA hybrid construct (Figure 2D) exhibited slightly smooth and glistening morphology when compared to PLGA construct (Figure 2E). Both constructs showed no resisting compression when palpated with forceps. By the end of the third week, the *in vitro* fibrin/PLGA hybrid construct appeared whiter, smoother and glistening (Figure 2F), resembling morphology of cartilage-like tissue superior to PLGA construct (Figure 2G). In addition, fibrin/PLGA hybrid construct was slightly firmer than the PLGA construct.

Histological evaluation of *in vitro* constructs

At 2 weeks *in vitro*, when the fibrin/PLGA hybrid construct were stained using H&E, they predominantly showed superior histological features of normal cartilage compared to the PLGA group. The closely-packed cartilage-isolated cells were homogeneously distributed in the ECM and exhibited rounded morphology with lacunae embed-

ded in basophilic ground substance (Figure 3A). The pericellular and inter-territorial matrix region was strongly stained by the characteristic red of Safranin O, indicating presence of the proteoglycan-rich matrix (Figure 3B) corroborated with positive Alcian Blue staining (Figure 3C) confirming GAG accumulation. Next, the formation of cartilaginous tissue was remarkably evident by the third week of *in vitro* culture in the fibrin/PLGA hybrid construct. Cartilage-isolated cells with lacunae was well-distributed within the homogenous ECM (Figure 3G) in concert with the presence of specific histochemicals property of proteoglycan-rich matrix (Figure 3H) and GAG accumulation (Figure 3I). The difference between the fibrin/PLGA hybrid construct (Figure 3A, B, C and Figure 3G, H, I) and PLGA group (Figure 3D, E, F and Figure 3J, K, L) was clearly visible in term of overall cartilaginous tissue formation, cells organization and ECM distribution in all specimens. PLGA group exhibited few rounded chondrocytes cluster filling up several void spaces of the scaffold. For fibrin/PLGA hybrid construct, accumulation of proteoglycan-rich matrix and GAG at the core region was significant and was intensely stained at 2 weeks and greatest at 3 weeks when compared to PLGA construct. No sign of cartilaginous tissue formation in fibrin/PLGA hybrid construct and PLGA construct was observed at one week of *in vitro* culture.

Immunohistochemistry analysis of *in vitro* constructs

We analyzed collagen type II and collagen type I immunolocalization on the fibrin/PLGA hybrid construct, and we compared the results with the PLGA group. The specific cartilaginous ECM molecule, collagen type II exhibited strong immunopositivity at the pericellular and the inter-territorial matrix of the fibrin/PLGA hybrid constructs (Figure 4A). Minimal collagen type II expression was observed in PLGA specimens (Figure 4C). After 3 weeks, as shown in Figure 4E collagen type II marker maintained positive expression in the fibrin/PLGA hybrid construct, as did the chondrocytes cluster in PLGA construct (Figure 4G). Collagen type I expression demonstrated moderate immunopositivity throughout the ECM of both fibrin/PLGA hybrid constructs (Figure 4B, Figure 4F) and the PLGA group (Figure 4D, Figure 4H) at week 2 and week 3, respectively.

Cartilage-specific phenotypic expression analysis

When the mRNA expression of fibrin/PLGA hybrid construct and PLGA group were compared, no significant difference was observed between chondrocytes derived from both groups. The fibrin/PLGA hybrid construct and PLGA group showed comparable potential in sustaining the specific chondrogenic phenotypic expression at each time point of 1, 2 and 3 weeks. The expression of genes encoded the cartilage-specific markers; collagen type II and aggrecan core protein was steadily observed *in vitro*

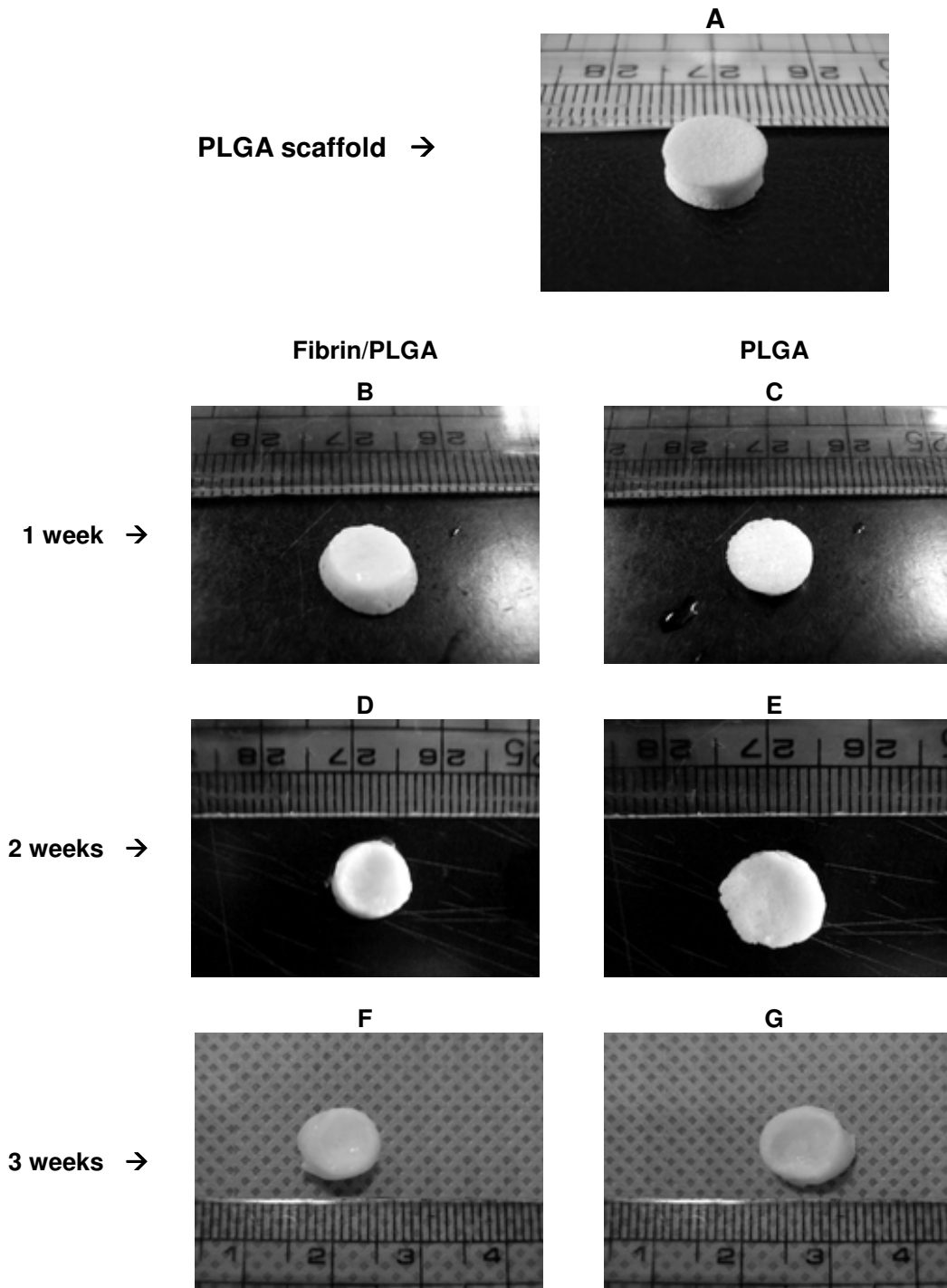


Figure 2

Macroscopic observation of *in vitro* constructs. Figure 2A represents PLGA scaffold which was designed in the shape of cylindrical disc. Fibrin/PLGA constructs (Figure 2B) and PLGA construct (Figure 2C) was morphologically similar after 7 days in culture. Fibrin/PLGA construct (Figure 2D) showed slightly smooth and glistening morphology when compared to PLGA (Figure 2E) after 14 days. By week 3, fibrin/PLGA construct appeared whiter, smoother and glistening (Figure 2F) than PLGA (Figure 2G).

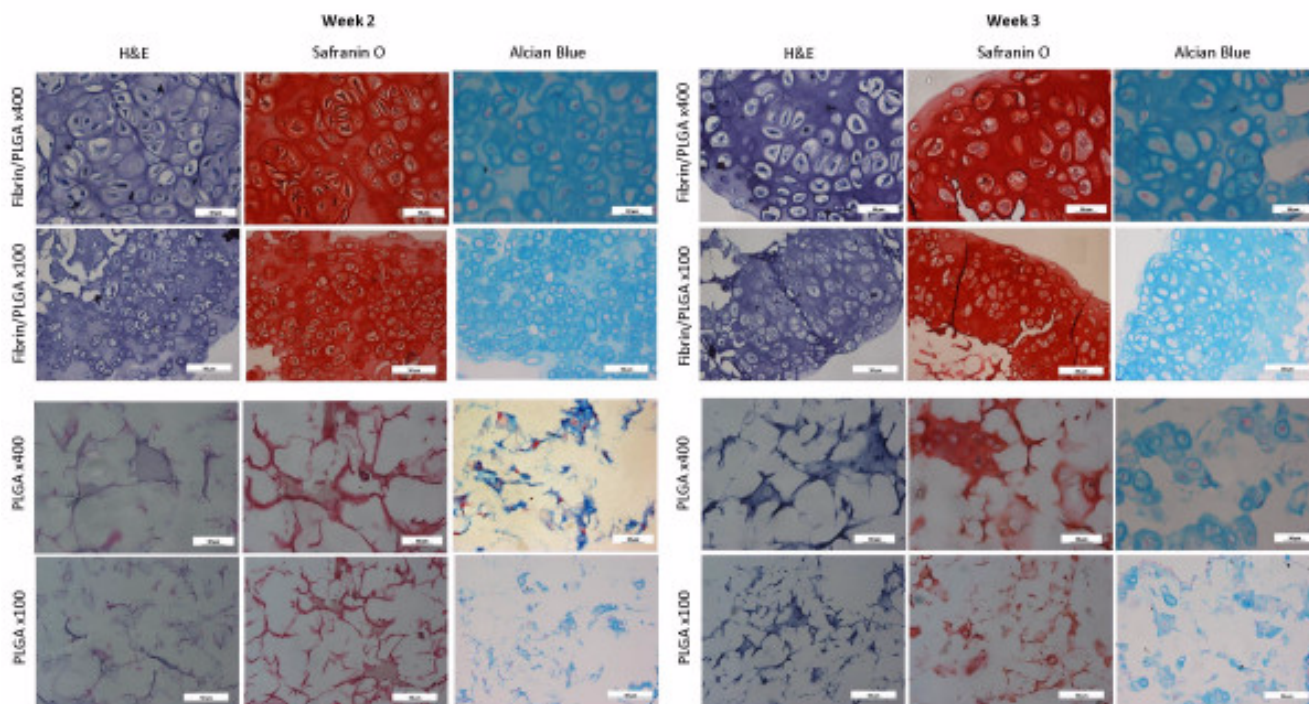


Figure 3

Histological evaluation of *in vitro* constructs. Fibrin/PLGA constructs showed superior histological features of cartilage-like tissue compared to PLGA. Differences between fibrin/PLGA (Figure 3A, B, C and Figure 3G, H, I) and PLGA (Figure 3D, E, F and Figure 3J, K, L) were clearly visible in term of overall cartilaginous tissue formation, cells organization and ECM distribution. The fibrin/PLGA constructs was intensely stained with Safranin O for accumulated proteoglycan and Alcian Blue for GAG at 2 weeks and greatest at 3 weeks.

culture, whereas collagen type I, the cartilage dedifferentiation marker exhibited down-regulation pattern after 2 and 3 weeks *in vitro*. The house-keeping gene, β -actin was steadily expressed in all specimens; to verify the two-step reverse-transcriptase PCR analysis was reliable and successful. Results were summarized in Figure 5.

Sulphated glycosaminoglycan (sGAG) production assay

The increment of average wet weight of fibrin/PLGA hybrid constructs (116.27 ± 4.65 mg, 137.25 ± 6.08 mg, 162.69 ± 7.12 mg) and PLGA group (116.88 ± 1.98 mg, 172.20 ± 8.78 mg, 241.33 ± 9.82 mg) was statistically significant ($p < 0.05$) from week 1, week 2 and week 3, respectively. After 2 and 3 weeks of *in vitro* culture, the PLGA group demonstrated significantly higher wet weight ($p < 0.05$) than fibrin/PLGA hybrid constructs by 1.25-fold and 1.48-fold, respectively (Figure 6A). As shown in Figure 6B, sGAG production in the fibrin/PLGA hybrid construct was definitely superior to the PLGA group at each time point. Normalized by the dried-weight of each sample, the relative sGAG content (%) was significantly higher ($p < 0.05$) in fibrin/PLGA hybrid constructs com-

pared to the PLGA group at 1 week and 3 week cultures. In particular, at week 1, with 0.223 ± 0.010 relative sGAG content, fibrin/PLGA hybrid constructs exhibited 1.92-fold higher sGAG production than the PLGA group; 0.116 ± 0.025 . At week 2, the relative sGAG content in fibrin/PLGA hybrid constructs; 0.197 ± 0.037 seemed higher than 0.113 ± 0.042 , the relative sGAG content in PLGA group; however the magnitude showed no significance difference between both groups. Next, by week 3, fibrin/PLGA hybrid constructs exhibited 0.296 ± 0.011 relative sGAG content, which was 1.67-fold higher than 0.177 ± 0.027 relative sGAG content in the PLGA group.

Discussion

Our aimed was to evaluate *in vitro* chondrogenesis of rabbit articular chondrocytes in PLGA scaffold utilizing fibrin as a cell transplantation matrix. Fibrin is biodegradable, biocompatible and non-immunogenic natural material [36], thus rendering this material as suitable scaffolding cell carriers [20] that helps provide homogenous cells distribution with no significant cells lost during the seeding process [29-31]. Immobilization of chondrocytes in fibrin

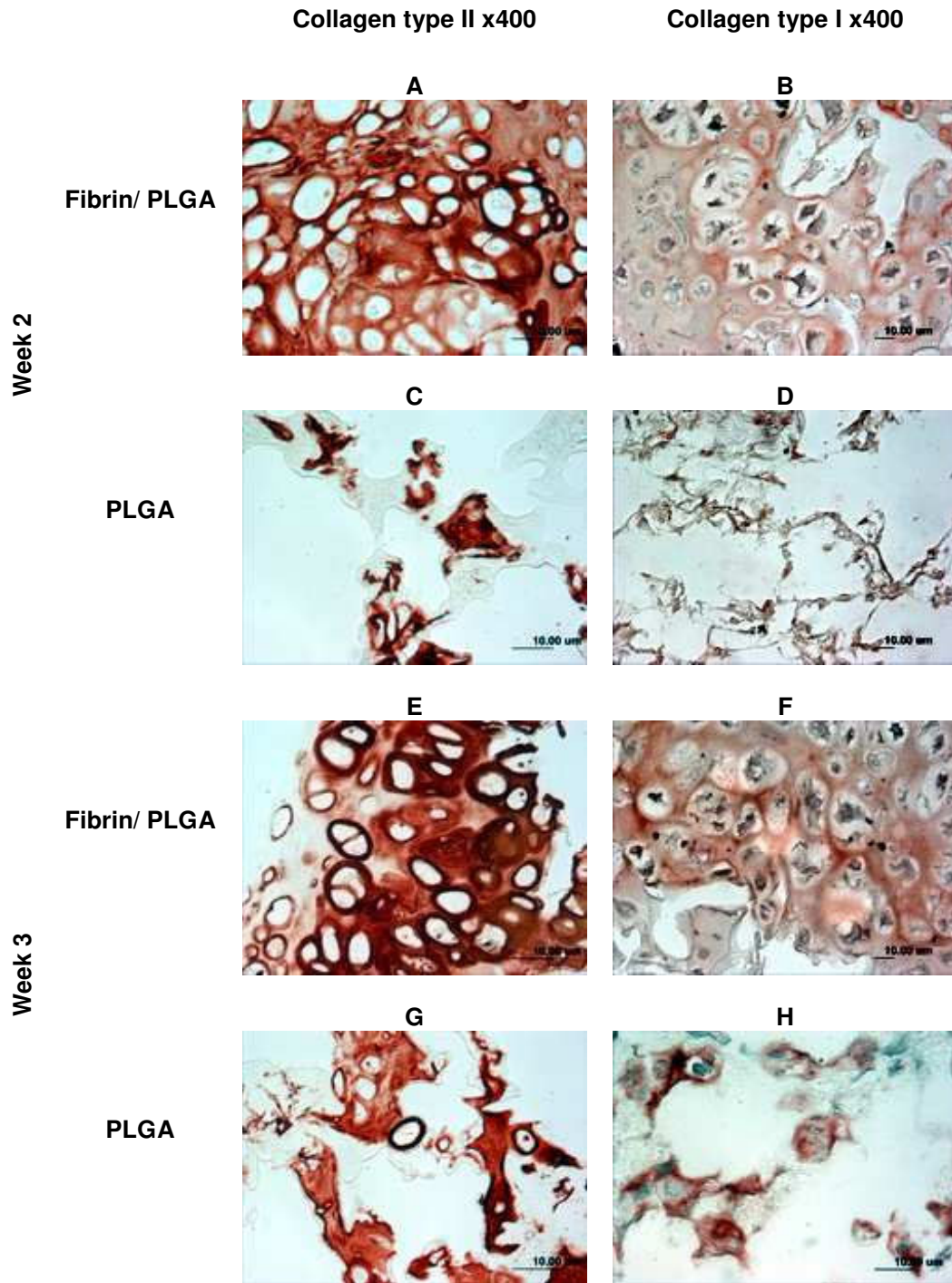


Figure 4

Immunohistochemistry analysis of *in vitro* constructs. As shown in Figure 4A, fibrin/PLGA exhibited strong immunopositivity of collagen type II which mainly localized at the pericellular and inter-territorial matrix. Minimal collagen type II expression could be observed in the PLGA construct (Figure 4C). After 3 weeks, collagen type II expression was maintained in fibrin/PLGA (Figure 4E) and PLGA (Figure G). Collagen type I in fibrin/PLGA constructs showed moderate immunopositivity at week-2 (Figure 4B) and week-3 (Figure 4F), as did PLGA (Figure 4D, Figure 4H).

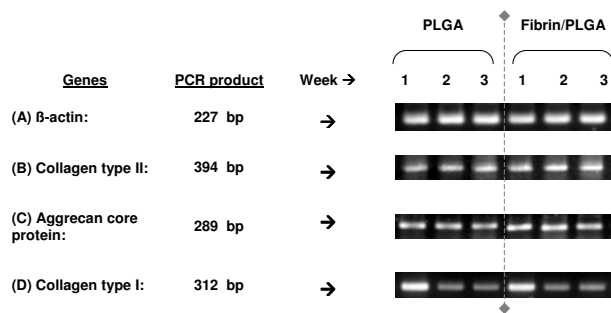
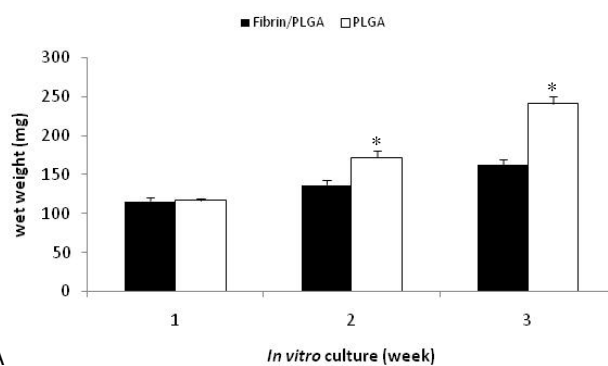


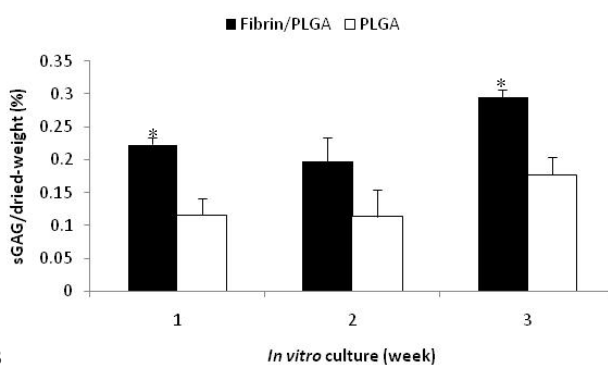
Figure 5
Cartilage-specific phenotypic expression analysis. The expression of genes encoded the cartilage-specific markers; collagen type II and aggrecan core protein was steadily expressed in fibrin/PLGA and PLGA. Interestingly, suppression of collagen type I was observed in fibrin/PLGA and PLGA at 2 weeks and 3 weeks. β -actin gene was steadily expressed in all samples to verify the analysis was reliable and successful.

resulted in homogenous cells distribution in PLGA scaffolds, easy to handle and deliver the cells [37]. Similar finding was reported in the previous assessment of osteogenic potential utilizing human periosteum-derived progenitor cells and fibrin gel immobilization technique in PLGA scaffold [29-31]. With regards to the present study, Lee et al. [37] also reported fibrin provided more uniform chondrocytes distribution during cell seeding via histology in macro-porous polyurethane scaffold.

Recently, Endres et al. [38] showed the 3D arrangement of human articular chondrocytes in human fibrin glue and resorbable PGA scaffolds cultured in the presence of human serum is an excellent system for the maturation of cartilage grafts in articular cartilage regeneration. It has been well documented that during growth in monolayer culture, chondrocytes adopt many of the phenotypic traits of fibroblast, as they become elongated and synthesize type I collagen rather than type II collagen. Thus, to induce the re-differentiation of expanded chondrocytes, the cells were first combined with fibrin glue as a temporary matrix and embedded in a resorbable felt structure to achieve a three-dimensional environment [38]. In this study, following cells seeding onto scaffolds, cells proliferated markedly in fibrin/PLGA and PLGA. Because of the growth, chondrocytes can secrete appropriate ECM molecules and develop chondrocyte-chondrocyte interaction to form clusters of various sizes as well as the 3D structure while preserving the original shape of the cell. By 2 weeks of culture period, histological differences between fibrin/PLGA and PLGA were obviously developed. Newly formed ECM was concentrated around the rounded cells, consistent with the established notion that a rounded



A



B

Figure 6
Sulphated-glycosaminoglycan (sGAG) production assay. The wet weight (Figure 6A) and sGAG production (Figure 6B) of the *in vitro* constructs were measured at 1, 2, and 3 weeks of culture, respectively. After 2 and 3 weeks *in vitro*, PLGA demonstrated significantly higher wet weight ($p < 0.05$) compared to fibrin/PLGA. The sGAG production in fibrin/PLGA construct was superior to PLGA. Relative sGAG contents (%) were significantly higher ($p < 0.05$) in fibrin/PLGA than PLGA at 1 week and 3 weeks.

morphology is an obligatory for the chondrocytic phenotype. Besides the histologically mature chondrocyte, extensive development of ECM indicated by presences of abundant proteoglycan-rich matrix and accumulated GAG in fibrin/PLGA was better than in PLGA. The expression of collagen type II, cartilage-specific ECM molecule was noticeably superior in fibrin/PLGA compared to PLGA. By day 21, fibrin/PLGA had significant cells-matrix organization and ECM deposition compared to PLGA group. Decline in growth rate by 21 days can be explained by a morphologically and structurally stable cells-matrix organization entering a steady state with no active cellular function at this stage. Clearly, the ECM production on fibrin/PLGA was superior to that of PLGA group. Lee et al. [37] suggested that the phenomenon may be due to higher cell-seeding efficiency and more homogeneous dis-

tribution of chondrocytes in the fibrin/PLGA hybrid construct. Similar criterion could be observed in PLGA-incorporated with collagen micro-sponges which was previously encountered as a promising 3D scaffold for articular cartilage tissue engineering [21,25].

Although there were remarkable histological differences in fibrin/PLGA hybrid scaffold and PLGA group, there was no significant variation in the semi-quantitative gene expression assessment for collagen type II, aggrecan core protein and collagen type I. Gene expression profiles showed that the chondrocyte phenotype was maintained in both groups. Interestingly, suppression of cartilage dedifferentiation marker, collagen type I can be observed in the *in vitro* constructs. Previously, although Lee et al. [37] reported the fibrin hydrogel-polyurethane hybrid scaffold system promoted higher levels of cartilage gene expression in the early stage of culture, the system still did not permit maintenance of the chondrocyte phenotype for the entire 4-week culture period. Accordingly, we suggest that fibrin would be an ideal cell carrier/transplantation matrix and enhance *in vitro* chondrogenesis of rabbit articular chondrocytes by mean of morphological, histological, biochemical and phenotypically similar to the normal hyaline cartilage. If this result is applicable for the clinical use, it is practically reliable for the reconstruction of clinical transplants for future orthopaedic surgery.

Conclusion

Fibrin/PLGA hybrid scaffold promotes early *in vitro* chondrogenesis of rabbit articular chondrocytes proven by means of morphology, histology, immunohistochemistry, chondrogenic gene expression and sGAG production. This study suggests that fibrin/PLGA hybrid scaffold may serve as a potential cell delivery vehicle and a structural basis for *in vitro* tissue-engineered articular cartilage construct. The *in vivo* experiment has been carried out and the results are currently written as a next chapter for this study.

Competing interests

The authors declare that they have no competing interests.

Authors' contributions

MS conceived the study, participated in its design, performed all the experiments and drafted the manuscript. SHK participated in the design of the study and conceived of the study. RBHI participated in the design of the study and conceived of the study. GK participated in the design of the study, conceived the study and drafted the manuscript. All authors read and approved the final manuscript.

Acknowledgements

This study was made possible by SCRC (SC3100) and KMOHW (0405-BO01-0204-0006). We thank Ms Youn Kyung Ko, Ms Hyun Jung Ha, Ms

Jung Won So and the BK-21 Polymer BIN Fusion Research Team, Department of Polymer Science and Technology, Chonbuk National University, South Korea who provided technical help for this study.

References

1. Brittberg M, Lindahl A, Nilsson A, Ohlsson C, Isaksson O, Peterson L: **Treatment of deep cartilage defects in the knee with autologous chondrocyte transplantation.** *N Engl J Med* 1994, **331(14)**:889-95.
2. Shao XX, Hutmacher DW, Ho ST, Goh JCH, Lee EH: **Evaluation of a hybrid scaffold/cell construct repair of high load bearing osteochondral defects in rabbits.** *Biomaterials* 2006, **27**:1071-80.
3. Willers C, Chen J, Wood D, Xu J, Zheng MH: **Autologous chondrocytes implantation with collagen bioscaffold for the treatment of osteochondral defects in rabbits.** *Tissue Eng* 2005, **11(7/8)**:1065-76.
4. Ito Y, Ochi M, Adachi N, Sugawara K, Yanada S, Ikada Y, Ronakorn P: **Repair of osteochondral defect with tissue engineered chondral plug in rabbit model.** *Arthroscopy* 2005, **21(10)**:1155-63.
5. Niederauer GG, Silva MA, Leatherbury NC, Korvick DL, Harroff HH, Ehler WC, Dunn CJ, Kiewsetter K: **Evaluation of multiphase implants for repair of focal osteochondral defects in goats.** *Biomaterials* 2000, **21**:2561-74.
6. van Susante JLC, Buma P, Schuman L, Homminga GN, Berg WB van den, Veth RPH: **Resurfacing potential of heterologous chondrocytes suspended in fibrin glue in large full-thickness defects of femoral articular cartilage: an experimental study in the goat.** *Biomaterials* 1999, **20**:1167-75.
7. Breinan HA, Minas T, Hsu HP, Nehrer S, Shortkroft S, Spector M: **Autologous chondrocytes implantation in a canine model: change in composition of reparative tissue with time.** *J Orthop Res* 2001, **19**:482-492.
8. Munirah S, Samsudin OC, Chen HC, Hussein SSS, Mohd Azam Khan GK, Aminuddin BS, Ruszymah BHI: **Articular cartilage restoration in load-bearing osteochondral defects by autologous chondrocytes-fibrin constructs implantation: an experimental study in sheep.** *J Bone Joint Surg (Br)* 2007, **89-B**:1099-1109.
9. Munirah S, Samsudin OC, Loqman MY, Siti Norhayati I, Chua KH, Aminuddin BS, Ruszymah BHI: **The potential of autologous cartilage implantation in ovine focal cartilage defects: a new option for articular cartilage restoration [Abstract].** *Tissue Eng* 2006, **12(4)**:1014.
10. Ruszymah BHI, Samsudin OC, Munirah S, Chen HC, Sharifah Salmah SH, Mohd Azam SGK, Aminuddin BS: **Repair of articular cartilage after implantation with autologous engineered cartilage made using autologous fibrin as the biomaterial: A fully autologous system [Abstract].** In *World Congress on Tissue Engineering & Regenerative Medicine* Pittsburgh, Pennsylvania Poster; 2006:268.
11. Kim SH, Ha HJ, Ko YK, Yoon SJ, Rhee JM, Kim MS, Lee HB, Khang G: **Correlation of proliferation, morphology and biological responses of fibroblasts on LDPE with different surface wettability.** *J Biomater Sci Polym Ed* 2007, **18(5)**:609-622.
12. Ko YK, Kim SH, Ha HJ, Yoon SJ, Rhee JM, Kim MS, Lee HB, Khang G: **Hybrid type of tissue-engineered biodisc using annulus fibrosus seeded PLGA scaffold and nucleus pulposus seeded MPEG-PCL hydrogel: Preliminary study.** *Key Engineering Mater* 2007, **342-343**:173-176.
13. Munirah S, Aminuddin BS, Samsudin OC, Badrul AHMY, Azmi B, Ruszymah BHI: **The significance of autologous human serum versus pooled human serum supplementation for the growth of human articular chondrocytes.** *J Orthop Surg (Hong Kong)* in press.
14. Munirah S, Aminuddin BS, Samsudin OC, Chua KH, Fuzina NH, Ruszymah BHI: **The re-expression of collagen type II, aggrecan and Sox9 in tissue engineered human articular cartilage.** *Tissue Eng Regen Med* 2005, **2**:347-55.
15. Munirah S, Aminuddin BS, Chua KH, Fuzina NH, Isa MR, Ruszymah BHI: **Tissue engineered human articular neocartilage using serial expanded chondrocytes.** *Med J Malaysia* 2004, **59(Suppl B)**:9-10.
16. Samsudin OC, Aminuddin BS, Munirah S, Chua KH, Fuzina NH, Isa MR, Azmi B, Badrul AHMY, Ruszymah BHI: **In vitro development of autologous tissue engineered human articular neocarti-**

- lage for orthopaedic surgery. *Med J Malaysia* 2004, **59(Suppl B)**:15-16.
17. Badrul AHMY, Aminuddin BS, Sharaf I, Samsudin OC, Munirah S, Ruszymah BHI: **The Effects of autologous human serum on the growth of tissue engineered human articular cartilage.** *Med J Malaysia* 2004, **59(Suppl B)**:11-12.
 18. Azmi B, Aminuddin BS, Sharaf I, Samsudin OC, Munirah S, Chua KH, Ruszymah BHI: **The significance of using pooled human serum in human articular cartilage tissue engineering.** *Med J Malaysia* 2004, **59(Suppl B)**:13-14.
 19. Munirah S, Aminuddin BS, Chua KH, Samsudin OC, Badrul AHMY, Azmi B, Fuzina NH, Ruszymah BHI: **Tissue-engineered human articular cartilage demonstrates intense immunopositivity for collagen type II.** *J Biosciences* 2006, **17(1)**:9-18.
 20. Eyrieh D, Brandl F, Appel B, Wiese H, Maier G, Wenzel M, Staudenmaier R, Goepferich A, Blunk T: **Long-term stable fibrin gels for cartilage engineering.** *Biomaterials* 2007, **28**:55-65.
 21. Chen G, Tanaka J, Tateishi T: **Osteochondral tissue engineering using a PLGA-collagen hybrid mesh.** *Materials Science and Engineering C* 2006, **26**:124-129.
 22. Khang G, Kim MS, Cho SH, Lee I, Rhee JM, Lee HB: **Natural scaffolds biomaterials for tissue regeneration.** *Tissue Eng Regen Med* 2004, **1(1)**:9-20.
 23. Park GE, Pattison MA, Park K, Webster TJ: **Accelerated chondrocyte functions on NaOH-treated PLGA scaffolds.** *Biomaterials* 2005, **26(16)**:3075-3082.
 24. Park GE, Park K, Webster TJ: **NaOH-treated PLGA scaffolds allow for greater articular chondrocyte functions.** *Bioengineering Conference. Proceedings of the IEEE 30th Annual Northeast* 2004:148-149 [<http://ieeexplore.ieee.org/iel5/9/104/28882/01300038.pdf?tp=&isnumber=&arnumber=1300038>]. Accessed online 25th July 2007
 25. Chen G, Sato T, Ushida T, Ochiai N, Tateishi T: **Tissue engineering of cartilage using a hybrid scaffold of synthetic polymer and collagen.** *Tissue Eng* 2004, **10(3/4)**:323-330.
 26. Kim SH, Yoon SJ, Choi B, Ha HJ, Rhee JM, Kim MS, Yang YS, Lee HB, Khang G: **Evaluation of various types of scaffold for tissue engineered intervertebral disc.** *Adv Exp Med Biol* 2006, **585**:169-181.
 27. Lee SJ, Lee I, Lee YM, Lee HB, Khang G: **Macroporous biodegradable natural/synthetic hybrid scaffolds as small intestine mucosa impregnated poly(lactide-co-glycolide) for tissue engineered bone.** *J Biomater Sci Polym Ed* 2004, **15(8)**:1003-1017.
 28. Jang JW, Park KS, Kim SH, Park CS, Kim MS, Han CW, Rhee JM, Khang G, Lee HB: **Tissue engineered bone regeneration using DBP-loaded PLGA scaffold in rabbit model.** *Tissue Eng Regen Med* 2005, **2(1)**:34-40.
 29. Zheng YX, Ringe J, Liang Z, Loch A, Chen L, Sittinger M: **Osteogenic potential of human periosteum-derived progenitor cells in PLGA scaffold using allogeneic serum.** *J Zhejiang Univ Sci B* 2006, **7(10)**:817-824.
 30. Arnold U, Lindenhayn K, Perka C: **In vitro-cultivation of human periosteum derived cells in bioresorbable polymer-TCP-composites.** *Biomaterials* 2002, **23(11)**:2303-2310.
 31. Perka C, Schultz O, Spitzer RS, Lindenhayn K, Burmester GR, Sittinger M: **Segmental bone repair by tissue-engineered periosteal cell transplants with bioresorbable fleece and fibrin scaffolds in rabbits.** *Biomaterials* 2000, **21(11)**:1145-1153.
 32. Khang G, Lee SJ, Han CW, Rhee JM, Lee HB: **Preparation and characterization of natural/synthetic hybrid scaffolds.** *Adv Exp Med Biol* 2003, **657**:235-245.
 33. Ha HJ, Kim SH, Yoon SJ, Ko YK, Lee EK, Son Y, Kim MS, Rhee JM, Khang G, Lee BH: **Characterization of annulus fibrosus and nucleus pulposus with sequential passage.** *Tissue Eng Regen Med* 2006, **3(4)**:416-422.
 34. Yamazaki S, Banes AJ, Weinhold PS, Tsuzaki M, Kawakami M, Minchew JT: **Vibratory loading decreases extracellular matrix and matrix metalloproteinase gene expression in rabbit annulus cells: one hundred sixty years ago in spine.** *Spine J* 2002, **2(6)**:415-420.
 35. Whitley CB, Ridnour MD, Draper KA, Dutton CM, Neglia JP: **Diagnostic test for mucopolysaccharidosis I. Direct method for quantifying excessive urinary glycosaminoglycan excretion.** *Clin Chem* 1989, **35**:374-9.
 36. Ruszymah BHI: **Autologous human fibrin as the biomaterial for tissue engineering.** *Med J Malaysia* 2004, **59(Suppl B)**:30.
 37. Lee CR, Grad S, Gorna K, Gogolewski S, Goessl A, Alini M: **Fibrin-polyurethane composites for articular cartilage tissue engineering: A preliminary analysis.** *Tissue Eng* 2005, **11(9/10)**:1562-157.
 38. Endres M, Neumann K, Schroder SEA, Vetterlein S, Morawietz L, Ringe J, Sittinger M, Kaps C: **Human polymer-based cartilage grafts for the regeneration of articular cartilage defects.** *Tissue Cell* 2007, **39(5)**:293-301.

Publish with **BioMed Central** and every scientist can read your work free of charge

"BioMed Central will be the most significant development for disseminating the results of biomedical research in our lifetime."

Sir Paul Nurse, Cancer Research UK

Your research papers will be:

- available free of charge to the entire biomedical community
- peer reviewed and published immediately upon acceptance
- cited in PubMed and archived on PubMed Central
- yours — you keep the copyright

Submit your manuscript here:
http://www.biomedcentral.com/info/publishing_adv.asp

