



# Use of X-Ray Fluorescence Microscopy for Studies on Research Models of Hepatocellular Carcinoma

Tatjana Paunesku<sup>1</sup>, Andrew C. Gordon<sup>2</sup>, Sarah White<sup>3</sup>, Kathleen Harris<sup>2</sup>, Olga Antipova<sup>4</sup>, Evan Maxey<sup>4</sup>, Stefan Vogt<sup>4</sup>, Anthony Smith<sup>1</sup>, Luiza Daddario<sup>1</sup>, Daniele Procissi<sup>2</sup>, Andrew Larson<sup>2</sup> and Gayle E. Woloschak<sup>1\*</sup>

<sup>1</sup> Radiation Oncology Department, Feinberg School of Medicine, Northwestern University, Chicago, IL, United States,

<sup>2</sup> Radiology Department, Feinberg School of Medicine, Northwestern University, Chicago, IL, United States, <sup>3</sup> Department of Radiology, Division of Interventional Radiology, Medical College of Wisconsin, Milwaukee, WI, United States, <sup>4</sup> X-Ray Sciences Division, Advanced Photon Source, Argonne National Laboratory, Argonne, IL, United States

## OPEN ACCESS

### Edited by:

Dörthe Schae, UCLA David Geffen School of Medicine, United States

### Reviewed by:

Christina Strell, Vienna University of Technology, Austria  
Bohic Sylvain, INSERM, France

### \*Correspondence:

Gayle E. Woloschak  
g-woloschak@northwestern.edu

### Specialty section:

This article was submitted to Radiation and Health, a section of the journal Frontiers in Public Health

**Received:** 18 May 2021

**Accepted:** 26 July 2021

**Published:** 20 August 2021

### Citation:

Paunesku T, Gordon AC, White S, Harris K, Antipova O, Maxey E, Vogt S, Smith A, Daddario L, Procissi D, Larson A and Woloschak GE (2021) Use of X-Ray Fluorescence Microscopy for Studies on Research Models of Hepatocellular Carcinoma. *Front. Public Health* 9:711506. doi: 10.3389/fpubh.2021.711506

**Introduction:** TheraSphere® microspheres containing yttrium <sup>90</sup>Y are among many radioembolization agents used clinically to reduce liver tumor burden, and their effects on cancer volume reduction are well-established. At the same time, concerns about off target tissue injury often limit their use. Deeper investigation into tissue distribution and long-term impact of these microspheres could inform us about additional ways to use them in practice.

**Methods:** Healthy rat liver and rabbit liver tumor samples from animals treated with TheraSpheres were sectioned and their elemental maps were generated by X-ray fluorescence microscopy (XFM) at the Advanced Photon Source (APS) synchrotron at Argonne National Laboratory (ANL).

**Results:** Elemental imaging allowed us to identify the presence and distribution of TheraSpheres in animal tissues without the need for additional sample manipulation or staining. Ionizing radiation produced by <sup>90</sup>Y radioactive contaminants present in these microspheres makes processing TheraSphere treated samples complex. Accumulation of microspheres in macrophages was observed.

**Conclusions:** This is the first study that used XFM to evaluate the location of microspheres and radionuclides in animal liver and tumor samples introduced through radioembolization. XFM has shown promise in expanding our understanding of radioembolization and could be used for investigation of human patient samples in the future.

**Keywords:** radioembolization of liver malignancies, X-ray fluorescence microscopy, rabbit (Lagomorph), yttrium 90 microspheres, hepatocellular carcinoma

## INTRODUCTION

Cancers affecting liver tissue are among the most difficult to treat, regardless of their origin. Primary liver cancers account for more than 700,000 deaths per year worldwide and show an annual 2% increase among causes of mortality over the last 13 years (1). As much as 70–90% of primary liver cancer cases are attributed to hepatocellular carcinoma (HCC) (2). In cases when surgical

resection is impossible, HCC treatments include the use of “small molecules” such as sorafenib (3) or external beam radiation such as stereotactic body radiotherapy (SBRT) (4). While the liver blood supply is primarily venous, the HCC blood supply is arterial (5) and this peculiarity allows use of intra-arterial HCC therapies such as chemoembolization and radioembolization (6–9). Each one of these treatments also has its own set of possible complications. Sorafenib, for example, can cause skin toxicity that is severe enough to necessitate dose reduction or discontinuation of therapy (10). Radiotoxicity can be an outcome of either external beam radiotherapy or radioembolization and careful calculation of allowable doses makes up a part of any treatment regimen (6, 11). Despite the fact that radiopharmaceutical therapy is generally considered effective for treatment of many types of cancer (12), liver cancer radioembolization is discontinued just prior to treatment in as many as one third of all patients due to a variety of concerns (13). New approaches for safer radioembolization or combination treatments are needed. To this end, detailed evaluation in animal models of liver cancer treatments needs to be developed beyond current capabilities.

In order to investigate the feasibility of different treatment combinations and approaches, the use of animal models is extremely important for evaluation of radioembolization. Among them, the rabbit VX2 liver cancer model is one of the most valuable as the size of these animals permits use of diagnostic and treatment approaches similar to those used in human patients. Clinically used agents for chemoembolization (5) and radioembolization (14) were explored in this model for a long while. More recently, this model is used for testing of novel therapeutic and diagnostic agents such as nanoparticles (15–19) and targeted nanoparticles (20, 21), both alone and in combination with radionuclides (22–24). VX2 cells are a rabbit cell line, originally induced by cottontail rabbit papilloma virus (25), that grows well in immunologically competent animals. The tumors generated by VX2 implantation are well-vascularized and, in liver, similar to HCC. We have used this animal model for different types of studies for more than 15 years (14, 20, 23, 26–31). Over the same period, we have also worked on introducing a unique imaging technique, x-ray fluorescence microscopy (XFM), into pathology (20, 32–36). Although we have previously used XFM to image liver VX2 samples (20), this is the very first study where we have developed and implemented necessary sample preparation techniques to process radioactive tissue samples and make them suitable for XFM imaging. In this work, we were able to identify individual TheraSpheres used for radioembolization both by their silica and yttrium content. At the same time, we could see the tissue and cell outlines through their biological element content, as 2D features in phosphorus, sulfur, iron, zinc etc. This approach has great promise for evaluation of processes ongoing in tissues containing radionuclides. Due to natural elemental content, XFM maps of biological samples are analogous to images of hematoxylin-and-eosin (H&E) stained samples, while radionuclides and other inorganic materials present in tissues can be registered and quantified.

## METHODS

### Animals

This study used New Zealand white rabbits weighing between 12 and 20 lbs, used as either donor rabbits or liver-cancer animals (with VX2 tumors implanted into the liver under ultrasound guidance). The institutional animal care and use committee of Northwestern University approved all work in this study. As mentioned in the introduction, our work with VX2 rabbits has been extensive over the past 15 years, in different studies we used VX2 tumor bearing rabbits for a wide variety of endpoints (6, 14, 20, 23, 26–31).

VX2 cells, originally procured from National Cancer Institute (NCI, Frederick, MD, USA) were injected in the hind limb of a donor rabbit and allowed to grow for 3–4 weeks. Tumor growth was checked by palpation and the donor animals were sacrificed when the tumors reached 2–3 cm. These tumors were excised and dissected, and the viable tumor tissue was then cut into small sections and suspended in sterile Hank's solution (Sigma).

Recipient liver cancer rabbits were anesthetized by intramuscular injection of ketamine at 44 mg/kg and xylazine 3–5 mg/kg, and the rabbit was maintained under inhalational isoflurane at 2–3% during the procedure. Rabbit's abdomen was shaved and a preliminary ultrasound (Mindray M7, Mindray Medical Intl Ltd.) was done with a L14-6S transducer. A millimeter long incision in the skin above liver was done under aseptic conditions and a coaxial introducer was inserted into the liver under direct ultrasound guidance. Several small tumor fragments were pushed through the introducer into the liver and a final ultrasound was performed to assess for complications including bleeding. The anesthetic was reversed with yohimbine 0.5 mg/kg (Lloyd Laboratories). Meloxicam 0.2 mg/kg (Norbrook Laboratories Ltd., Newry, Northern Ireland) was administered for pain. After tumor implantation procedure the rabbits were monitored daily for pain, lethargy, appetite and mobility. Two weeks after surgery, the tumor growth was monitored using 7T magnetic resonance imaging. This work followed procedures used routinely in the past (14, 26–31, 37).

### Radioembolization

For these experiments we used clinical microspheres TheraSphere<sup>®</sup> (BTG Interventional Medicine) containing yttrium <sup>90</sup>Y. The beads were made of glass, 20–30 μm in diameter with specific gravity of 3.6 g/cc. The use of glass <sup>90</sup>Y microspheres for research was approved and monitored by the Radiation Safety Office of the Northwestern University.

Rabbit treatments with microspheres were done in animals with liver tumor growth confirmed by MRI imaging. Microspheres were injected using a microcatheter (Renegade HI-FLO, Boston Scientific) and microwire (Glidewire<sup>®</sup> GT; 0.018", 180 cm) used under fluoroscopic guidance (OEC 9800 Plus mobile C-arm and vascular platform workstation, GE Medical Systems) in order to approach the left hepatic artery *via* celiac artery and femoral artery. Digital subtraction angiography (Omnipaque, GE Healthcare) was used to identify the anatomy and confirm the target treatment volume, native arterial flow, and reflux. Radioembolization was done with 9 mg of microspheres

**TABLE 1** | Administered activity (primarily  $^{90}\text{Y}$ , for additional explanation see **Table 2**) on the day of animal treatment.

| Animal        | Administered activity (Bq) | Date     |
|---------------|----------------------------|----------|
| Rabbit 843382 | 80,586,899.58              | 10/25/15 |
| Rabbit 827185 | 92,169,487.58              | 8/23/15  |
| Rabbit 827186 | 69,696,624.87              | 8/23/15  |
| Rabbit 762071 | 84,036,896.28              | 11/9/14  |
| “Rat 21”      | 33,881,260.94              | 10/25/15 |

**TABLE 2** | MDS Nordion measurement of by-products at 60 days post-calibration for TheraSphere with Calibration dates after January 1, 2010.

| Isotope                       | Half-life | Energy line(s) | Average activity per unit mass |                 |
|-------------------------------|-----------|----------------|--------------------------------|-----------------|
|                               | Days      | keV            | Bq/mg                          | SD ( $n = 13$ ) |
| Y-91                          | 58.51     | 1,204.7        | 2,504                          | 271             |
| Y-88                          | 106.65    | 898            | 895                            | 64              |
| Cr-51                         | 27.7      | 320.1          | 78.9                           | 9.1             |
| Total for all other nuclides: |           |                | 81                             | 7.5             |

( $\sim 1$  GBq) per animal, followed by 30–40 ml of sterile 0.9% saline over 3–5 min. Finally, the femoral artery was ligated and the animals were maintained for 2–3 more weeks depending on their health status. The rabbits were monitored daily for pain, lethargy, appetite and mobility.

TheraSpheres treatments of healthy animals were done with healthy Sprague-Dawley rats (Charles River Laboratories, Wilmington, MA), 450–500 g of weight. Catheterization of hepatic lobe in a rat required a surgical procedure where the animal's abdomen was opened, mesenteric venous drainage was used to select the right portal vein and a catheter was used to inject 9 mg of TheraSpheres and 6–8 ml of sterile 0.9% saline over 1–2 min. In this case partially decayed microspheres (day 5 after calibration to 1 GBq, corresponding to 0.2738GBq) were used. Ligation was done after infusion, the bowel was returned into the abdominal cavity, and the abdomen was closed in two layers. Animals were monitored daily and sacrificed 2 months after this procedure.

Administered activity on the day of animal treatment is provided in **Table 1**. While activity indicated in **Table 1** came primarily from  $^{90}\text{Y}$ , several other radionuclides are also present in TheraSpheres. Some of them have a significantly longer half-life than  $^{90}\text{Y}$  (**Table 2**), and this generated additional concerns with sample processing and handling.

## Sample Preparation

At necropsy, the livers were separated into pieces suitable for freezing in molds with optimum cutting temperature solution (Tissue-Tek<sup>®</sup> O.C.T. Compound, Sakura<sup>®</sup> Finetek). Frozen samples were stored in a  $-80^{\circ}\text{C}$  freezer and allowed to decay before further use.

Samples for X-ray fluorescence microscopy were prepared from livers of four rabbits (each with a VX2 tumor) and one rat,

(example of “radio-surgery”) treated with TheraSpheres. Seven-micrometer-thick frozen tissue sections were prepared on a Leica cryostat dedicated to work with radioactive samples, placed on Ultralene membrane (SPEX Sample Prep, LLC, 15 Liberty St., Metuchen, NJ, USA) and allowed to air dry. Radioactivity of these samples was followed with a hand-held Geiger counter in order to monitor possible contamination during processing. Once dried, these samples were positioned on an in-house 3D printed PLA sample support, Ultralene membrane backing was glued onto the PLA frame and trimmed. Samples were wrapped with the Ultralene membrane and the entire assembly secured with Kapton tape (Kapton Tape Com.) in order to prevent potential radioactive contamination of X-ray fluorescence microscope.

## X-Ray Fluorescence Microscopy

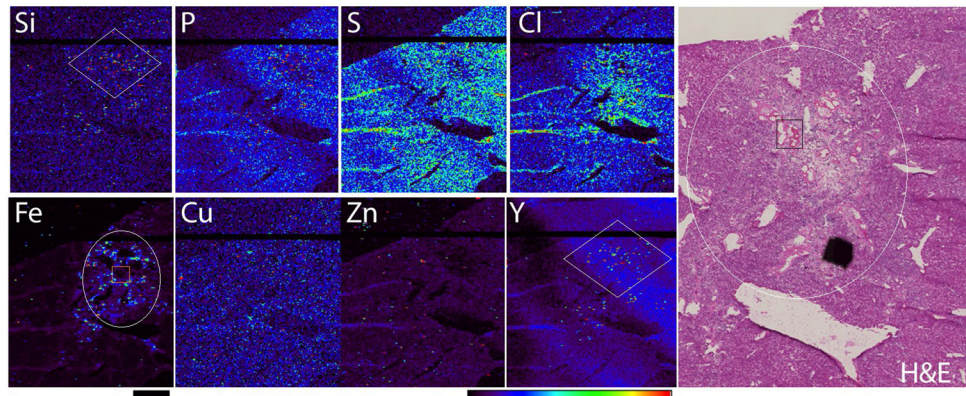
Elemental mapping was done at the Advanced Photon Source Synchrotron at two different instruments: X-ray microprobe at Sector 2, beamline station 2ID-E; and with the “large area instrument” at the Sector 8 bending magnet beamline 8BM-B). At the large area instrument, at the beamline station 8BMB, KB mirror are used to obtain a 30 micron beam spot size for a high throughput overview of elemental distribution in tissues. Spectra were collected with a SII Vortex ME4 4-element silicon drift detector (SII NanoTechnology USA, Northridge, CA). For calibration we used thin film AXO standards (Applied X-ray Optics, Dresden, Germany) and the peaks were deconvoluted using MAPS software (38). Per pixel counts were converted to elemental concentrations ( $\mu\text{g}/\text{cm}^2$ ). Hard X-rays energy of 21 and 15 keV were both used for scanning at 8BM-B station. While K line of Y was imaged at 21 keV, scanning at 15 keV was also used in order to increase yield of fluorescent signals from biologically relevant elements. At this combination of energies all elemental components of interest were detected by their K alpha fluorescence. This included not only “native biological elements,” but also silica—major component of glass microspheres and yttrium itself.

For higher resolution scans at the Sector 2-ID-E samples were raster-scanned with a beam focused to 0.3 micron using Fresnel Zone Plates. At this station only hard X-rays of 21 keV were used. Silicon drift energy dispersive detector positioned was used to collect the fluorescence signal from samples, at  $90^{\circ}$  to the incident beam. Per pixel elemental concentration was obtained by comparison with the thin-film standards NBS-1832 and NBS-1833 from the National Bureau of Standards (Gaithersburg, MD), and the analysis was done using MAPS software (38) as detailed in other studies (20, 34–36).

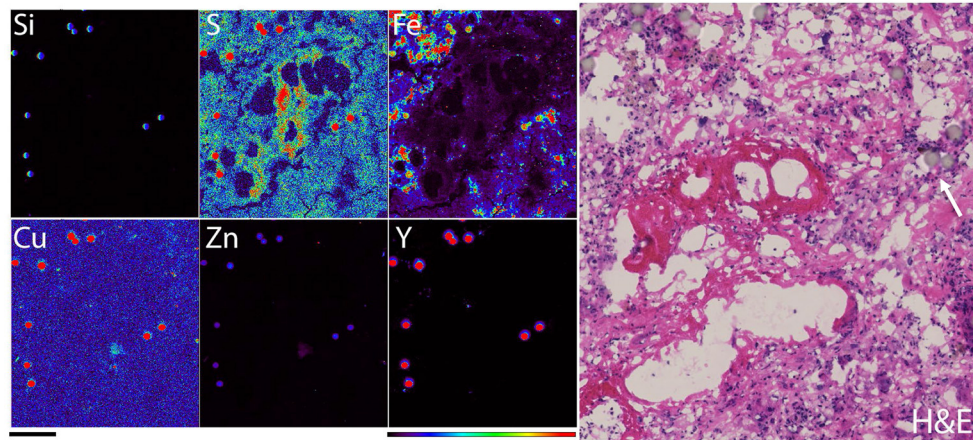
## RESULTS

### “Radio-Surgery” of Healthy Rat Liver

The distribution of TheraSpheres was investigated in four rabbit VX2 liver cancer samples and a single rat with tumor free liver, all exposed to TheraSpheres as a means of “radio-surgery” (see **Table 1**). One additional rabbit treated with cold TheraSpheres was included in the analysis (**Supplementary Figure 1**, obtained at station 2-ID-E with X-ray energy of 21 keV). This sample allowed us to see how much of the XFM yttrium signal can



**FIGURE 1** | Rat liver tissue elemental map obtained with 30 micron spot size scanning, X-ray energy 15 keV (Station 8BM-B). Elemental maps were obtained simultaneously while sample was moved by rapid raster scanning (so called: “fly scans”) through the X-ray beam. Scale bar—2 mm, color bar indicates elemental quantity as represented by false colors, from black (no signal) to red (highest signal). Hematoxylin and eosin (H&E) staining of the same region in one of the adjacent tissue sections is shown in the right-hand panel. White diamonds in Si and Y maps correspond to a TheraSpheres rich area; white circle indicates fibrotic area in Fe map and H&E image. Orange rectangle in Fe image and black rectangle in H&E image correspond to areas shown in **Figure 2** (due to imaging setup, in **Figure 2** these areas are horizontally flipped).



**FIGURE 2** | Elemental map of a detail of rat liver tissue obtained with 300 nanometer spot size (station 2ID-E), X-ray energy 21 keV. At this x-ray energy fluorescence produced by yttrium overwhelms signals of most biological elements and the spheres “appear in all elemental channels.” Elemental maps were obtained simultaneously while sample was moved by rapid raster scanning (so called: “fly scans”) through the X-ray beam. Scale bar—200 microns, color bar indicates elemental quantity as represented by false colors, from black (no signal) to red (highest signal). Elemental signal maxima in micrograms per cm square for different elements were: 804 for Si, 14.5 for S, 0.499 for Cu, 37.1 for Fe, 7.79 for Zn and 774 for Y. Hematoxylin and eosin staining of the same region in one of the adjacent tissue sections is shown in the right hand panel; white arrow points to a TheraSphere. Please note that the same areas were scanned at lower magnification in **Figure 1**, as explained.

be ascribed to the “overflow” of the very strong Si signal. In samples treated with cold and hot TheraSpheres Si signal maxima were comparable (191 and 227 micrograms per square centimeter) while signal maxima for artifact Y signal vs. true Y signal differed 1,000-fold (0.56 vs. 515 micrograms per square centimeter).

For sample prep for XFM, tissues were frozen in optimum cutting temperature (O.C.T.), sectioned at 7 microns on a cryostat and placed onto an Ultralene membrane to be scanned by X ray fluorescence microscopy (XFM). XFM images of the rat liver were obtained with different X-ray energies. We first

obtained a large overview image shown in **Figure 1** with 15 keV energy X-rays at 8BM-B beamline (30 micron spot size). The XFM technique gives simultaneous maps for biological elements P, S, Cl, K, Ca, Mn, Fe, Cu, Zn, as well as elements that make the TheraSphere microparticles—Si and Y (in scans at 21 keV). It should be noted that the sample area with the highest Si signals (dots in red color which represents the highest signal) is outlined by a white diamond. This region of the sample also has the highest Fe signal. We have noticed in other tissue samples that accumulation of fibroblasts (fibrosis) is associated with an increase in iron accumulation. Fibrotic area in Fe signal and H&E

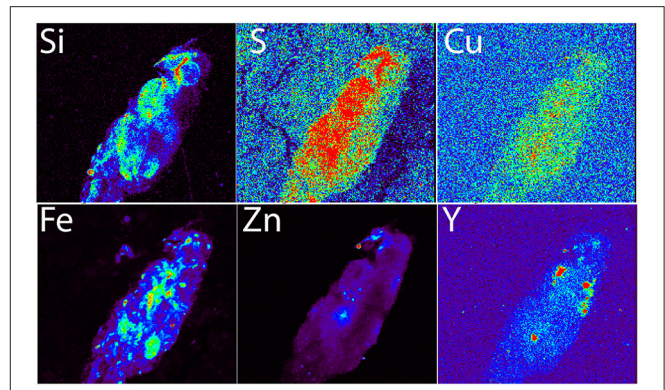
images are outlined by white ovals. Weak staining in the necrotic area of the H&E image corresponds with the development of fibrosis in the same area of the sample. Subsequent high-resolution imaging of the same sample at 21 keV energy was done in a sub-area of this tissue, labeled in **Figure 1** as described in the **Figure 1** legend.

A closer look into the same area (**Figure 2**) was obtained by conducting XFM at the 2ID-E beamline where the sample was scanned with a beam size of 300 nm and at an X-ray energy of 21 keV (optimal for K alpha excitation of yttrium). **Figure 2** shows a spread of microspheres (strong Si and Y signals of clearly spherical, 20–30 micron beads) surrounding an area with little iron and high sulfur signals, matching a region of necrotic changes where cell debris and extracellular matrix create a dense protein mesh (proteins are the major source of S in XFM images) with gradually accumulating fibrosis (Fe rich signal outside of the microsphere rich area). H&E image of the same sample region in one of the subsequent tissue sections shows the appearance of TheraSpheres in visible light images. Their identification is difficult and depends mostly on the appearance of the spherical shape itself.

In **Figure 1** we can note that the microsphere rich area of the sample has the occasional “spots” with concentrated Zn signal that are independent from spots in Si and Y which correspond to microspheres. A closer investigation of one such Zn high region (**Figure 3**) has shown an accumulation of mostly “crushed” microspheres (although at least one found in the upper middle portion of the image retained its’ spherical shape). The ratio of Zn and Fe in the same area of **Figure 3** was an order of magnitude greater than Zn and Fe concentration in the overall region of microsphere spread (e.g., **Figure 2**). At the same time, concentration of yttrium within this region was smaller than in intact microspheres (Y maximum in **Figure 2** in 774 vs. only 0.635 microgram per cm square in **Figure 3**). This suggests that the zinc rich structure in **Figure 3** is a macrophage that has ingested several microspheres and damaged them structurally which led to a decreased Y concentration compared to Y maxima in intact microspheres.

## Radioembolization of VX2 Tumors in Rabbits

In rabbit liver embolization experiments, the same quantity of microspheres (in terms of glass/silica content, although not with respect to  $^{90}\text{Y}$ , see **Table 1**) was injected as in rats. Therefore, much fewer microspheres were noted in rabbit liver samples compared to rat liver (**Figure 4**). A “lacey-like” tissue consistency of tumor tissue in rabbits was notable, elemental concentration for chlorine was the greatest in the same region of the sample. The most dynamic region of tumor growth and the region with the best vasculature was found at the border between tumor and healthy liver parenchyma. In this region of the tissue, the concentration of iron was the highest as well as the concentration of copper Cu. No comparative modulation of copper was seen in rat liver tissue and it is possible that this increase in Cu is driven by the presence of the tumor. It is known that Cu is one of the elements that shows intense redistribution during angiogenesis



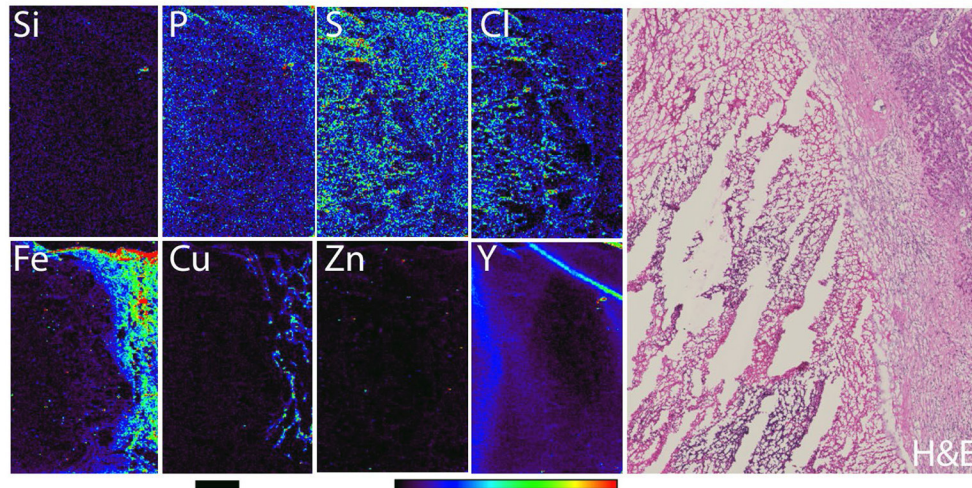
**FIGURE 3** | A detail of rat liver tissue elemental map obtained with 300 nanometer spot size (station 2ID-E), X-ray energy 21 keV. Scale bar –100 microns, color bar indicates elemental quantity as represented by false colors, from black (no signal) to red (highest signal). Signal maxima in micrograms per cm square for different elements were: 125 for Si, 5.45 for S, 0.199 for Cu, 50.9 for Fe, 23.7 for Zn, and 0.635 for Y.

(39). Considering that VX2 tumors are hypervascular, it is possible that increased Cu signal corresponds to the area of the tissue with the most active growth of tumor blood vessels.

## DISCUSSION AND CONCLUSIONS

Use of XFM in investigation of biological samples has rapidly grown over the past decade with the development of third generation synchrotrons with beamlines and endstations dedicated to biological samples (34, 37, 40–45). While some of these capacities existed at the Advanced Photon Source since early 2,000 s, only recently could they be utilized for samples with large areas of interest such as pathology samples. This possibility opened after development of rapid scanning protocols and introduction of new detectors. While these new developments enabled tomographic imaging of single cells or whole small organisms such as zebrafish embryos (46–49), they have also allowed rapid screening of large sample areas. Today, the samples as large as few centimeters can be imaged at sub-micrometer resolution. In this work we used XFM to investigate animal liver tissue samples and evaluate elemental distribution of native biological elements as well as materials introduced into this organ by injection of TheraSpheres, glass microspheres containing radioactive  $^{90}\text{Y}$  for radioembolization and radio-lobectomy.

While different approaches can be used to follow distribution of TheraSpheres *in vivo* (6, 14), these methods lack the resolution necessary to establish micro-dosimetry in *ex vivo* samples. It is conceivable that different patterns of TheraSphere distribution could be correlated to different treatment outcomes. While cytotoxicity is the primary reason for use of TheraSpheres, it has been observed in some patient cases that the healthy liver remnant may initiate liver regeneration after TheraSphere treatment. If this type of beneficial development can be correlated with specific TheraSphere distribution patterns, this could be exploited to improve HCC care.



**FIGURE 4** | Rabbit liver with VX2 tumor necrotic region (left half of the sample) and VX2 viable part of the tumor (right-hand side of the sample). Elemental map was obtained with 30 micron spot size scanning, at X-ray energy 15 keV (station 8BM-B). Scale bar—2 mm, color bar indicates elemental quantity as represented by false colors, from black (no signal) to red (highest signal). Hematoxylin and eosin staining of the same region in one of the adjacent tissue sections is shown in the right hand panel.

In addition, by using XFM to evaluate TheraSphere treated samples, it may be possible to monitor the process of neoangiogenesis by focusing on Cu accumulation and redistribution in viable regions of the tumor. This may be of particular importance for investigation of HCC because of its hypervascularity. In fact, tumor microvasculature density can be used as a predictor of recurrence in surgically treated patients (50). Because of HCC hypervascularity, therapies that target neoangiogenesis have long been considered as a good approach for treatment of HCC. For example, anti-angiogenesis coupled with the antiproliferative drug sorafenib, the current standard of care for HCC, inhibits the receptor tyrosine kinases vascular endothelial growth factor receptor 2 (VEGFR-2), platelet-derived growth factor receptor-beta 1/2 (PDGFR- $\beta$ ), and the kinase RAF (51). Use of XFM for screening of HCC samples would allow us to monitor the response to sorafenib or other anti-angiogenesis treatments. It should be noted that radioembolization is also often used in combination with sorafenib (8, 52) therefore, XFM investigation of HCC samples from such patients could be doubly interesting.

Finally, investigation of radio-lobectomy by XFM was also shown to be informative. Investigation of a liver sample from a TheraSphere treated but otherwise healthy, rat demonstrates elemental changes caused by necrosis and fibrotic changes in this organ caused by the cytotoxic effect of TheraSpheres. In addition, presence of broken microspheres leached from most of the yttrium in the rat sample suggest that macrophages may be capable of redistributing the TheraSpheres. In HCC treatment such involvement of the macrophages would be detrimental to therapy.

In conclusion, this is an early pilot study that established operating procedures for imaging of highly radioactive

samples by XFM. Next, this work also documented that tissue elemental mapping at different energies (15 and 21 keV) provides informative data both about the biological elements and the TheraSpheres. Nevertheless, much more work is still needed in order to fully develop procedures for tomographic and high throughput imaging of these samples. Some of the work could be done with samples generated with cold TheraSpheres. For example, procedures for tomographic imaging of samples that contained only silica and approaches for precise quantification of silica would support the work with samples generated from tissues exposed to radioactive TheraSpheres in the distant past. On the other hand, addition of complementary approaches for imaging of radioactive samples such as use of high-resolution beta-microimagers (e.g., from Biospace Lab) or 3D autoradiography (53) would complement studies conducted with fresh samples prepared soon after treatments with radiolabeled TheraSpheres. In short—many possible avenues are opened for continuation of these studies and deeper evaluation of TheraSphere treatments.

## DATA AVAILABILITY STATEMENT

The original contributions presented in the study are included in the article/**Supplementary Material**, further inquiries can be directed to the corresponding author/s.

## ETHICS STATEMENT

The animal study was reviewed and approved by Northwestern University Animal Care and Use Committee.

## AUTHOR CONTRIBUTIONS

TP: project conception, experimental work and data interpretation, and manuscript preparation. ACG and DP: experimental work and data interpretation. SW, KH, OA, and EM: experimental work. SV and AL: data interpretation. AS and LD: manuscript preparation. GEW: project conception and manuscript preparation. All authors contributed to the article and approved the submitted version.

## FUNDING

This study was supported by Northwestern University Multi-PI Basic Science Synergy Research Grant and NIH Training Grant R25CA132822. Work at Argonne National Laboratory was supported by the U.S. Department of Energy, Office of Science, Office of Basic Energy Sciences, Contract No. DE-AC02-06CH11357. Imaging work performed at Northwestern

University Cell Imaging Facility was supported by NCI CCSG P30 CA060553 Grant awarded to the Robert H. Lurie Comprehensive Cancer Center.

## ACKNOWLEDGMENTS

MRI imaging was performed at the Center for Translational Imaging (CTI) at Northwestern University. Tissue processing and sectioning were done by the Northwestern University Pathology core <http://cancer.northwestern.edu/pathcore/index.cfm>. The authors especially wish to thank Bernice Frederick for excellent support with sample preparation.

## SUPPLEMENTARY MATERIAL

The Supplementary Material for this article can be found online at: <https://www.frontiersin.org/articles/10.3389/fpubh.2021.711506/full#supplementary-material>

## REFERENCES

- Mejia JC, Pasko J. Primary liver cancers: intrahepatic cholangiocarcinoma and hepatocellular carcinoma. *Surg Clin North Am.* (2020) 100:535–49. doi: 10.1016/j.suc.2020.02.013
- Torre LA, Bray F, Siegel RL, Ferlay J, Lortet-Tieulent J, Jemal A. Global cancer statistics, 2012. *CA Cancer J Clin.* (2015) 65:87–108. doi: 10.3322/caac.21262
- Llovet JM, Ricci S, Mazzaferro V, Hilgard P, Gane E, Blanc JF, et al. Sorafenib in advanced hepatocellular carcinoma. *N Engl J Med.* (2008) 359:378–90. doi: 10.1056/NEJMoa0708857
- Tsai CL, Hsu FM, Cheng JC. How to improve therapeutic ratio in radiotherapy of HCC. *Liver cancer.* (2016) 5:210–20. doi: 10.1159/000367767
- Geschwind JF, Artemov D, Abraham S, Omdal D, Huncharek MS, McGee C, et al. Chemoembolization of liver tumor in a rabbit model: assessment of tumor cell death with diffusion-weighted MR imaging and histologic analysis. *J Vasc Interv Radiol.* (2000) 11:1245–55. doi: 10.1016/S1051-0443(07)61299-8
- Young JY, Rhee TK, Atassi B, Gates VL, Kulik L, Mulcahy ME, et al. Radiation dose limits and liver toxicities resulting from multiple yttrium-90 radioembolization treatments for hepatocellular carcinoma. *J Vasc Interv Radiol.* (2007) 18:1375–82. doi: 10.1016/j.jvir.2007.07.016
- Rammohan A, Sathyanesan J, Ramaswami S, Lakshmanan A, Senthil-Kumar P, Srinivasan UP, et al. Embolization of liver tumors: past, present and future. *World J Radiol.* (2012) 4:405–12. doi: 10.4329/wjr.v4.i9.405
- Sacco R, Conte C, Tumino E, Parisi G, Marceglia S, Metrangola S, et al. Transarterial radioembolization for hepatocellular carcinoma: a review. *J Hepatocell Carcinoma.* (2016) 3:25–9. doi: 10.2147/JHC.S50359
- Lee EJ, Chung HW, Jo JH, So Y. Radioembolization for the treatment of primary and metastatic liver cancers. *Nucl Med Mol Imaging.* (2019) 53:367–73. doi: 10.1007/s13139-019-00615-9
- Chen AP, Setser A, Anadkat MJ, Cotliar J, Olsen EA, Garden BC, et al. Grading dermatologic adverse events of cancer treatments: the common terminology criteria for adverse events version 4.0. *J Am Acad Dermatol.* (2012) 67:1025–39. doi: 10.1016/j.jaad.2012.02.010
- Wondergem M, Smits ML, Elschot M, de Jong HW, Verkooijen HM, van den Bosch MA, et al. <sup>99m</sup>Tc-macroaggregated albumin poorly predicts the intrahepatic distribution of <sup>90</sup>Y resin microspheres in hepatic radioembolization. *J Nucl Med.* (2013) 54:1294–301. doi: 10.2967/jnumed.112.117614
- Sgouros G, Bodei L, McDevitt MR, Nedrow JR. Radiopharmaceutical therapy in cancer: clinical advances and challenges. *Nat Rev Drug Discov.* (2020) 19:589–608. doi: 10.1038/s41573-020-0073-9
- Masthoff M, Schindler P, Harders F, Heindel W, Wilms C, Schmidt HH, et al. Analysis of failed therapy evaluations in radioembolization of primary and secondary liver cancers. *J Cancer Res Clin Oncol.* (2021) 147:1537–45. doi: 10.1007/s00432-020-03443-z
- Gupta T, Virmani S, Neidt TM, Szolc-Kowalska B, Sato KT, Ryu RK, et al. MR tracking of iron-labeled glass radioembolization microspheres during transcatheter delivery to rabbit VX2 liver tumors: feasibility study. *Radiology.* (2008) 249:845–54. doi: 10.1148/radiol.2491072027
- Duan X, Li H, Han X, Ren J, Li F, Ju S, et al. Antitumor properties of arsenic trioxide-loaded CalliSpheres<sup>®</sup> microspheres by transarterial chemoembolization in VX2 liver tumor rabbits: suppression of tumor growth, angiogenesis, and metastasis and elongation of survival. *Am J Transl Res.* (2020) 12:5511–24.
- Shi Q, Lu Y, Huang S, Zhou C, Yang C, Liu J, et al. Apatinib-loaded callispheres beads for embolization in a rabbit VX2 liver tumor: characterization *in vitro*, pharmacokinetics and tumor response *in vivo*. *Drug Deliv.* (2020) 27:1301–7. doi: 10.1080/10717544.2020.1818881
- Gaba RC, Khabbaz RC, Muchiri RN, Morrison JD, Elkhadrady L, Totura WM, et al. Conventional versus drug-eluting embolic transarterial chemoembolization with doxorubicin: comparative drug delivery, pharmacokinetics, and treatment response in a rabbit VX2 tumor model. *Drug Deliv Transl Res.* (2021) doi: 10.1007/s13346-021-00985-8. [Epub ahead of print].
- Kim D, Lee JH, Moon H, Seo M, Han H, Yoo H, et al. Development and evaluation of an ultrasound-triggered microbubble combined transarterial chemoembolization (TACE) formulation on rabbit VX2 liver cancer model. *Theranostics.* (2021) 11:79–92. doi: 10.7150/thno.45348
- Liu L, Xu X, Liang X, Zhang X, Wen J, Chen K, et al. Periodic mesoporous organosilica-coated magnetite nanoparticles combined with lipiodol for transcatheter arterial chemoembolization to inhibit the progression of liver cancer. *J Colloid Interface Sci.* (2021) 591:211–20. doi: 10.1016/j.jcis.2021.02.022
- Refaat T, West D, El Achy S, Parimi V, May J, Xin L, et al. Distribution of iron oxide core-titanium dioxide shell nanoparticles in VX2 tumor bearing rabbits introduced by two different delivery modalities. *Nanomaterials (Basel, Switzerland).* (2016) 6:143. doi: 10.3390/nano6080143
- Liu X, Xie Y, Qi X, Xu K. Transcatheter arterial chemoembolization (TACE) with iRGD peptide in rabbit VX2 liver tumor. *J Cancer Res Ther.* (2020) 16:1703–9. doi: 10.4103/jcrt.JCRT\_1411\_20
- Kobeiter H, Georgiades CS, Leakakos T, Torbenson M, Hong K, Geschwind JF. Targeted transarterial therapy of Vx-2 rabbit liver tumor with Yttrium-90 labeled ferromagnetic particles using an external magnetic field. *Anticancer Res.* (2007) 27:755–60.
- Gordon AC, White SB, Yang Y, Gates VL, Procissi D, Harris KR, et al. Feasibility of combination intra-arterial yttrium-90 and irinotecan

- microspheres in the VX2 rabbit model. *Cardiovasc Intervent Radiol.* (2020) 43:1528–37. doi: 10.1007/s00270-020-02538-x
24. Bastiaannet RC, Bastiaannet R, van Nimwegen SA, Barten-van Rijbroek AD, Van Es RJJ, Rosenberg A, et al. Feasibility of CT quantification of intratumoural (166)Ho-microspheres. *Eur Radiol Exp.* (2020) 4:29. doi: 10.1186/s41747-020-00157-2
  25. Shope RE, Hurst EW. Infectious papillomatosis of rabbits: with a note on the histopathology. *J Exp Med.* (1933) 58:607–24. doi: 10.1084/jem.58.5.607
  26. Sato KT, Larson AC, Rhee TK, Salem RA, Nemcek AA, Mounajjed T, et al. Real-time MRI monitoring of transcatheter hepatic artery contrast agent delivery in rabbits. *Acad Radiol.* (2005) 12:1342–50. doi: 10.1016/j.acra.2005.06.019
  27. Larson AC, Rhee TK, Deng J, Wang D, Sato KT, Salem R, et al. Comparison between intravenous and intraarterial contrast injections for dynamic 3D MRI of liver tumors in the VX2 rabbit model. *J Magn Reson Imaging.* (2006) 24:242–7. doi: 10.1002/jmri.20623
  28. Virmani S, Wang D, Harris KR, Ryu RK, Sato KT, Lewandowski RJ, et al. Comparison of transcatheter intraarterial perfusion MR imaging and fluorescent microsphere perfusion measurements during transcatheter arterial embolization of rabbit liver tumors. *J Vasc Interv Radiol.* (2007) 18:1280–6. doi: 10.1016/j.jvir.2007.07.008
  29. Virmani S, Harris KR, Szolc-Kowalska B, Paunesku T, Woloschak GE, Lee FT, et al. Comparison of two different methods for inoculating VX2 tumors in rabbit livers and hind limbs. *J Vasc Interv Radiol.* (2008) 19:931–6. doi: 10.1016/j.jvir.2008.02.019
  30. Deng J, Virmani S, Yang GY, Tang R, Woloschak G, Omary RA, et al. Intraprocedural diffusion-weighted PROPELLER MRI to guide percutaneous biopsy needle placement within rabbit VX2 liver tumors. *J Magn Reson Imaging.* (2009) 30:366–73. doi: 10.1002/jmri.21840
  31. White SB, Chen J, Gordon AC, Harris KR, Nicolai JR, West DL, et al. Percutaneous ultrasound guided implantation of VX2 for creation of a rabbit hepatic tumor model. *PLoS ONE.* (2015) 10:e0123888. doi: 10.1371/journal.pone.0123888
  32. Jansen SA, Paunesku T, Fan X, Woloschak GE, Vogt S, Conzen SD, et al. Ductal carcinoma *in situ*: X-ray fluorescence microscopy and dynamic contrast-enhanced MR imaging reveals gadolinium uptake within neoplastic mammary ducts in a murine model. *Radiology.* (2009) 253:399–406. doi: 10.1148/radiol.2533082026
  33. Barrea RA, Gore D, Kujala N, Karanfil C, Kozyrenko S, Heurich R, et al. Fast-scanning high-flux microprobe for biological X-ray fluorescence microscopy and microXAS. *J Synchrotron Radiat.* (2010) 17:522–9. doi: 10.1107/S0909049510016869
  34. Paunesku T, Wanzer MB, Kirillova EN, Muksinova KN, Revina VS, Lyubchansky ER, et al. X-ray fluorescence microscopy for investigation of archival tissues. *Health Phys.* (2012) 103:181–6. doi: 10.1097/HP.0b013e31824e7023
  35. Poropatich K, Paunesku T, Zander A, Wray B, Schipma M, Dalal P, et al. Elemental Zn and its binding protein zinc- $\alpha$ 2-glycoprotein are elevated in HPV-positive oropharyngeal squamous cell carcinoma. *Sci Rep.* (2019) 9:16965. doi: 10.1038/s41598-019-53268-1
  36. Kumthekar P, Ko CH, Paunesku T, Dixit K, SonabendAM, Bloch O, et al. A first-in-human phase 0 clinical study of RNA interference-based spherical nucleic acids in patients with recurrent glioblastoma. *Sci Transl Med.* (2021) 13:eabb3945. doi: 10.1126/scitranslmed.abb3945
  37. Paunesku T, Vogt S, Lai B, Maser J, Stojicevic N, Thurn KT, et al. Intracellular distribution of TiO<sub>2</sub>-DNA oligonucleotide nanoconjugates directed to nucleolus and mitochondria indicates sequence specificity. *Nano Lett.* (2007) 7:596–601. doi: 10.1021/nl0624723
  38. Vogt S. MAPS: a set of software tools for analysis and visualization of 3D X-ray fluorescence data sets [Article; Proceedings Paper]. *J Phys IV.* (2003) 104:635–8. doi: 10.1051/jp4:20030160
  39. Finney L, Mandava S, Ursos L, Zhang W, Rodi D, Vogt S, et al. X-ray fluorescence microscopy reveals large-scale relocalization and extracellular translocation of cellular copper protein during angiogenesis [Research Support, U.S. Gov't, Non-P.H.S.]. *Proc Natl Acad Sci USA.* (2007) 104:2247–52. doi: 10.1073/pnas.0607238104
  40. Bohic S, Simionovici A, Snigirev A, Ortega R, Devès G, Heymann D, Schroer CG. Synchrotron hard x-ray microprobe: fluorescence imaging of single cells. *Appl Phys Lett.* (2001) 78:3544. doi: 10.1063/1.1366362
  41. Paunesku T, Rajh T, Wiederrecht G, Maser J, Vogt S, Stojicevic N, et al. Biology of TiO<sub>2</sub>-oligonucleotide nanocomposites. *Nat Mater.* (2003) 2:343–6. doi: 10.1038/nmat875
  42. Chwiej J, Szczerbawska-Boruchowska M, Lankosz M, Wojcik S, Falkenberg G, Stegowski Z, et al. Preparation of tissue samples for X-ray fluorescence microscopy. *Spectrochimica Acta B.* (2005) 60:1531–7. doi: 10.1016/j.sab.2005.10.002
  43. McRae R, Bagchi P, Sumalekshmy S, Fahrni CJ. *In situ* imaging of metals in cells and tissues. *Chem Rev.* (2009) 109:4780–27. doi: 10.1021/cr900223a
  44. Ortega R, Devès G, Carmona A. Bio-metals imaging and speciation in cells using proton and synchrotron radiation X-ray microspectroscopy. *J R Soc Interface.* (2009) 6:S649–58. doi: 10.1098/rsif.2009.0166.focus
  45. De Samber B, De Schampelaere KA, Janssen CR, Vekemans B, De Rycke R, Martinez-Criado G, et al. Hard X-ray nanoprobe investigations of the subtissue metal distributions within *Daphnia magna*. *Anal Bioanal Chem.* (2013) 405:6061–8. doi: 10.1007/s00216-013-7019-6
  46. Alderden RA, Mellor HR, Modok S, Hall MD, Sutton SR, Newville MG, et al. Elemental tomography of cancer-cell spheroids reveals incomplete uptake of both platinum(II) and platinum(IV) complexes [Research Support, Non-U.S. Gov't Research Support, U.S. Gov't, Non-P.H.S.]. *J Am Chem Soc.* (2007) 129:13400–1. doi: 10.1021/ja076281t
  47. Yuan Y, Chen S, Paunesku T, Gleber SC, Liu WC, Doty CB, et al. Epidermal growth factor receptor targeted nuclear delivery and high-resolution whole cell X-ray imaging of Fe<sub>3</sub>O<sub>4</sub>@TiO<sub>2</sub> nanoparticles in cancer cells. *ACS Nano.* (2013) 7:10502–17. doi: 10.1021/nn4033294
  48. Bourassa D, Gleber S-C, Vogt S, Yi H, Will F, Richter H, et al. 3D imaging of transition metals in the zebrafish embryo by X-ray fluorescence microtomography. *Metallomics.* (2014) 6:1648–55. doi: 10.1039/C4MT00121D
  49. Chen S, Deng J, Yuan Y, Flachenecker C, Mak R, Hornberger B, et al. The Bionanoprobe: hard X-ray fluorescence nanoprobe with cryogenic capabilities. *J Sync Rad.* (2014) 21:66–75. doi: 10.1107/S1600577513029676
  50. Poon RT, Ng IO, Lau C, Yu WC, Yang ZF, Fan ST, et al. Tumor microvessel density as a predictor of recurrence after resection of hepatocellular carcinoma: a prospective study. *J Clin Oncol.* (2002) 20:1775–85. doi: 10.1200/JCO.2002.07.089
  51. Hora C, Romanque P, Dufour JF. Effect of sorafenib on murine liver regeneration. *Hepatology (Baltimore, Md).* (2011) 53:577–86. doi: 10.1002/hep.24037
  52. Mahvash A, Murthy R, Odisio BC, Raghav KP, Girard L, Cheung S, et al. Yttrium-90 resin microspheres as an adjunct to sorafenib in patients with unresectable hepatocellular carcinoma. *J Hepatocell Carcinoma.* (2016) 3:1–7. doi: 10.2147/JHC.S62261
  53. Nguyen MP, Ramakers RM, Kamphuis C, Koustoulidou S, Goorden MC, Beekman FJ. EXIRAD-3D: Fast automated three-dimensional autoradiography. *Nuclear Med Biol.* (2020) 86–87:59–65. doi: 10.1016/j.nucmedbio.2020.06.001

**Conflict of Interest:** The authors declare that the research was conducted in the absence of any commercial or financial relationships that could be construed as a potential conflict of interest.

**Publisher's Note:** All claims expressed in this article are solely those of the authors and do not necessarily represent those of their affiliated organizations, or those of the publisher, the editors and the reviewers. Any product that may be evaluated in this article, or claim that may be made by its manufacturer, is not guaranteed or endorsed by the publisher.

Copyright © 2021 Paunesku, Gordon, White, Harris, Antipova, Maxey, Vogt, Smith, Daddario, Procissi, Larson and Woloschak. This is an open-access article distributed under the terms of the Creative Commons Attribution License (CC BY). The use, distribution or reproduction in other forums is permitted, provided the original author(s) and the copyright owner(s) are credited and that the original publication in this journal is cited, in accordance with accepted academic practice. No use, distribution or reproduction is permitted which does not comply with these terms.