

# Field-measured drag area is a key correlate of level cycling time trial performance

James E. Peterman, Allen C. Lim, Ryan I. Ignatz, Andrew G. Edwards and William C. Byrnes

Department of Integrative Physiology, University of Colorado Boulder, Boulder, CO, USA

# **ABSTRACT**

Drag area  $(A_d)$  is a primary factor determining aerodynamic resistance during level cycling and is therefore a key determinant of level time trial performance. However,  $A_d$  has traditionally been difficult to measure. Our purpose was to determine the value of adding field-measured  $A_d$  as a correlate of level cycling time trial performance. In the field, 19 male cyclists performed a level (22.1 km) time trial. Separately, field-determined  $A_d$  and rolling resistance were calculated for subjects along with projected frontal area assessed directly  $(A_P)$  and indirectly (Est  $A_P$ ). Also, a graded exercise test was performed to determine  $\dot{V}O_2$  peak, lactate threshold (LT), and economy.  $\dot{V}O_2$  peak (l min<sup>-1</sup>) and power at LT were significantly correlated to power measured during the time trial (r = 0.83 and 0.69, respectively) but were not significantly correlated to performance time (r = -0.42 and -0.45). The correlation with performance time improved significantly (p < 0.05) when these variables were normalized to  $A_d$ . Of note,  $A_d$  alone was better correlated to performance time (r = 0.85, p < 0.001) than any combination of non-normalized physiological measure. The best correlate with performance time was field-measured power output during the time trial normalized to  $A_d$  (r = -0.92).  $A_P$  only accounted for 54% of the variability in  $A_d$ . Accordingly, the correlation to performance time was significantly lower using power normalized to  $A_P$  (r = -0.75) or Est  $A_P$  (r = -0.71). In conclusion, unless normalized to  $A_d$ , level time trial performance in the field was not highly correlated to common laboratory measures. Furthermore, our field-measured  $A_d$  is easy to determine and was the single best predictor of level time trial performance.

**Subjects** Biophysics, Anatomy and Physiology, Kinesiology, Orthopedics **Keywords** Drag coefficient, Power meter, Field testing, Power output, Predicting performance,
Exercise physiology

# INTRODUCTION

A cyclist's ability to produce and sustain mechanical power output is highly dependent upon physiological characteristics, particularly  $\dot{V}O_2$  max, lactate threshold (LT), and economy (*Coyle et al.*, 1988; *Coyle*, 1995). In the laboratory, where resistive forces are controlled or minimized, these physiological factors have been successfully used to predict simulated time trial performance (*Coyle et al.*, 1988; *Loftin & Warren*, 1994; *Coyle*, 1995; *Bishop et al.*, 2000; *Bentley et al.*, 2001; *Lamberts et al.*, 2012). However, in the field when

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Corresponding author William C. Byrnes, Byrnes@Colorado.edu

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cycling on level terrain at constant velocities (>40 km hr<sup>-1</sup>), more than 90% of the total resistance ( $R_{\rm TOT}$ ) impeding the forward motion of a bicycle-rider system is determined by aerodynamic resistance ( $R_a$ ) (Pugh, 1974; Di Prampero et al., 1979; Martin et al., 1998; Olds & Olive, 1999). Thus, measures of a cyclist's ability to supply mechanical power do not always predict performance time in time trial racing (Hoogeveen & Schep, 1997; Hometian Balmer, Hometian, Hometian Balmer, Hometian, Hometia

Measuring the aerodynamic resistance force ( $R_a$ ) during cycling can be complex. Direct measures include wind-tunnel tests (Davies, 1980; Kyle, 1991;  $Martin \ et \ al.$ , 1998), motorized towing ( $Di \ Prampero \ et \ al.$ , 1979;  $Capelli \ et \ al.$ , 1993), and coasting deceleration methods ( $De \ Groot$ ,  $Sargeant \ & Geysel$ , 1995;  $Candau \ et \ al.$ , 1999). Even though these direct measurements are accurate, they are impractical for most researchers and practitioners. For example, wind-tunnel testing facilities are inaccessible and costly. In addition, during wind tunnel testing, the bikes are not physically moving through the air and the pedaling motion introduces noise in the force measurement system during each pedal stroke. Motorized towing and coasting deceleration methods are also elaborate in their setup and execution meaning they are not an ideal substitute to a wind tunnel.

Because measuring the aerodynamic resistance force can be complex, it is sometimes assumed to be directly proportional to measures or estimates of the projected frontal area  $(A_P)$  of the bicycle and rider (Di Prampero et al., 1979; De Groot, Sargeant & Geysel, 1995; Olds & Olive, 1999; Heil, 2001; Anton et al., 2007). This assumes, though, that between individuals, aerodynamic resistance changes predictably with changes in  $A_P$ . However, evidence exists to the contrary. Previous research shows a lack of proportionality between an individual's measured  $A_P$  and aerodynamic resistance (Kyle, 1991; De Groot, Sargeant & Geysel, 1995). This discrepancy must be due to variability in the coefficient of drag ( $C_d$ , see equation (2)), which is influenced by the shape of the bicycle and rider, varies greatly between individuals, and does not change proportionally with changes in projected frontal area (Debraux et al., 2011).

Recently, it has been demonstrated that measuring mechanical power output and speed in the field with cycle mounted power meters is a viable and accessible technique for determining an individual's aerodynamic and rolling resistances (*Martin et al.*, 2006; *Debraux et al.*, 2011; *Lim et al.*, 2011). This technique, in combination with standard physiological profiling, could improve our ability to predict field performance since it has been argued that physical factors resisting forward motion play a larger role in performance outcome than physiological variables (*Jeukendrup & Martin*, 2001). *Anton et al.* (2007) have previously shown that projected frontal area alone is correlated to

Table 1 Mean  $\pm$  SD, minimum, and maximum descriptive information for all 19 subjects and values for the primary physiological performance measures assessed during the laboratory graded exercise stress test.

	Mean ± SD	Min	Max
Age (years)	$27.6 \pm 4.6$	20	36
Height (cm)	$174.0 \pm 6.0$	164	184
Body mass (kg)	$70.0 \pm 8.0$	59.5	87.3
Body fat (%)	$10.4 \pm 2.64$	6.0	16.5
Bone density (g cm $^{-2}$ )	$1.22\pm0.11$	1.03	1.41
Years racing	$8 \pm 5$	3	20
$VO_2$ peak (l min <sup>-1</sup> )	$4.67\pm0.40$	3.91	5.47
$VO_2$ peak (ml kg <sup>-1</sup> min <sup>-1</sup> )	$67.6 \pm 6.4$	54.2	76.5
Power at VO <sub>2</sub> peak (Watts)	$362 \pm 30$	308	410
Power to Mass at $VO_2$ peak (W kg <sup>-1</sup> )	$5.15 \pm 0.51$	4.21	5.95
LT 1 mM as % of VO <sub>2</sub> peak	$76 \pm 4.5$	65	82
Power at LT 1 mM (Watts)	$271\pm29$	230	331
Power to Mass at LT 1 mM (W kg <sup>-1</sup> )	$3.87 \pm 0.48$	3.03	4.53
Economy (W $1 O_2^{-1}$ )	$73.5 \pm 3.1$	69.1	78.9
Max heart rate (bpm)	$183 \pm 8$	168	197

performance time during a level time trial (r = -0.73). However, their estimated frontal area did not improve the prediction of level time trial performance compared to just maximal mechanical power output measured in the lab. As described above,  $A_P$  is not directly proportional to aerodynamic resistance. Thus, the aerodynamic characteristic of a cyclist (drag area ( $A_d$ )), which includes both  $A_P$  and  $C_d$ , may provide a better correlation for time trial performance.

Accordingly, the purpose of this study was to quantify physiological determinants of endurance performance in conjunction with physical factors that contribute to resistance during cycling. Correlations between the various determinants/factors and level time trial performance were then compared. We hypothesized a cyclist's physiological capacity or average power output would not predict level time trial performance time unless normalized to some representation of aerodynamic resistance. Additionally, we hypothesized that estimates of aerodynamic resistance, such as direct and indirect assessments of projected frontal area, would not correlate to performance as highly as the actual aerodynamic characteristic of the cyclist.

#### **METHODS**

# Subjects

Nineteen competitive male cyclists volunteered for this study. All subjects were licensed cyclists (United States Cycling Federation Category Pro/1/2 Road or Pro/Expert MTB) living, training, and racing in the Colorado, USA area for a minimum of two months. All tests were performed during the height of the local competitive cycling season. Descriptive characteristics of our nineteen subjects and the results from the laboratory testing are presented in Table 1. All subjects were informed of the risks involved with participation in

the study and gave written informed consent before participating. The Human Research Committee at the University of Colorado Boulder approved the protocol used for this study (reference number 0600.20).

#### Power measuring devices and calibration

All subjects utilized a rear hub power meter (CycleOps PowerTap, Madison, Wisconsin, USA) set to record external power output, ground velocity, cadence, and time measured at a frequency of 61 Hz with data averaged and recorded in epochs of 1.26 s for all variables. Heart rate was recorded using a CycleOps heart rate monitor chest strap that transmitted to the power meter computer. Nineteen distinct power meters were used throughout the study, one for each subject. Each subject used the same power meter for the time trial, laboratory testing, and aerodynamic/rolling resistance measures. Prior to commencing trials, all units used during testing were calibrated against a zero torque reference while pedals were stationary and unloaded as directed by the manufacturer.

# Laboratory measures and protocol

Laboratory measured endurance performance predictors including peak oxygen consumption ( $\dot{V}O_2$  peak), lactate threshold (LT), and economy (Watts l  $O_2^{-1}$  min<sup>-1</sup> at LT) were measured during a graded exercise test conducted within three days of the subject's time trial. Each test was performed on the subject's personal road bicycle attached to an electronically braked trainer (CompuTrainer<sup>®</sup>, Seattle, Washington, USA) with power measured using the rear hub power meter loaned to the subject at the beginning of the study. The protocol began at a power output between 100 and 150 watts and increased by approximately 30 watts every 4 min until volitional fatigue. All tests were conducted at an altitude of 1,625 m (5,330 ft) with an average barometric pressure, temperature, and humidity of 630.5  $\pm$  3.4 mm Hg, 22.9  $\pm$  1.4 °C, and 37.1  $\pm$  6.9%, respectively. Additionally, a fan was used to cool subjects throughout each exercise stress test.

Oxygen consumption and carbon dioxide production were averaged every 15 s through computer assisted indirect calorimetry using Parvomedics software and hardware to integrate input from a Validyne pressure tranducer and Perkin Elmer mass spectrometer. The pressure transducer was linked to a Hans Rudolph pneumotach measuring inspired ventilation and the Perkin Elmer mass spectrometer sampled from a 4-liter mixing chamber. Calibration procedures are summarized in Appendix S1.

Peak oxygen consumption was defined as the highest rate of oxygen consumption for a sampling interval of one minute during the graded exercise stress test. Subjects were vigorously encouraged to give a maximal effort and in all cases exceeded a respiratory exchange ratio of 1.15 and a blood lactate of 7 mM at volitional exhaustion. For the measure of economy, only the oxygen consumed over the last two minutes of each 4-minute stage was used to ensure steady state measures. Economy was measured as the ratio between power output and oxygen consumption (Watts  $1 O_2^{-1}$ ) at the lactate threshold from a regression of the oxygen consumption versus power relationship. In all subjects, the relationship between oxygen consumption and power output was linear (r > 0.99) through the penultimate stage.

Blood lactate concentration was measured at rest and over the last minute of each 4-minute stage. For each sample, approximately 50 µl of blood was drawn via finger pricks into a 75 µl capillary tube. Twenty-five µl was then mixed with a "cocktail" containing 50 µl of a buffer, lysing (Triton XL-100), and anti-glycolytic (sodium fluoride) solution. Lactate was finally analyzed using a YSI 2300 lactate analyzer (Yellow Springs, Ohio, USA). Before each test, the lactate analyzer was calibrated against a known standard, and re-calibrated every 15 min. The lactate threshold was defined as a point 1 mM above a baseline that included resting lactate (*Coyle et al.*, 1988). This process includes some subjective interpretation in determining the baseline values leaving room for potential human error. Thus, the average value for these points determined from eight independent observers was used in data analysis. No significant difference was found between observers.

Heart Rate during laboratory testing was measured using radio telemetry (Polar<sup>®</sup>, Lake Success, New York, USA) each minute while perceived exertion was measured using the Borg 6–20 scale 3 min into each stage. Within two days of the laboratory test, body composition was assessed using dual energy X-ray absorbtiometry (GE LUNAR DXA system, Fairfield, Connecticut, USA).

#### Time trial

The level time trial was conducted over two laps of a four-corner loop in Hygiene, Colorado. The total distance of the time trial was 22.1 km. Over the course of each lap, subjects gained and lost 79 m of elevation for a net elevation gain of 0 m. The layout of the course allowed the subjects to ride continuously with no stop signs or traffic lights impeding their effort. Subjects were allowed to utilize time trial bicycles equipped with time trial bars and an aerodynamic front wheel. Six subjects rode their standard road bike with no additional aerodynamic equipment. Another four subjects rode their standard road bike equipped with aerodynamic handlebars. The other nine subjects utilized a time trial bicycle equipped with aerodynamic handlebars with an aerodynamic deep dish or three-spoked front wheel.

Within two weeks prior to the time trial, subjects were asked to pre-ride the course to familiarize them with the route. All subjects had previous experience training on the selected course. Directly prior to the time trial, subjects performed their personal pre-competition warm-up. At this time, tires were inflated to 8.3 bar with the riders off the bicycle. Immediately before the time trial, the subject's individual mass ( $M_R$ ) and bicycle rider system mass ( $M_{BRS}$ ) were measured using an electronic scale previously calibrated against a laboratory balance scale (Detecto Scales, Webb City, Missouri, USA). At the start line, the on-board computers were cleared and the power meters calibrated against a zero load. During the time trial, subjects were blinded from viewing their power output but allowed to view speed, time, distance, cadence, and heart rate. In addition to the time measured by the on-board computer, performance time was also measured using an external stopwatch.

All time trials were held between 9 and 11 am. Air density was calculated from measures of ambient temperature, station pressure, and relative humidity collected with a Vantage Pro model weather instrument (Digital Instruments, Enterprise, Oregon, USA). Though

an attempt was made to schedule as many subjects as possible on the same day to control for wind, environmental conditions, and the competitive atmosphere, a total of ten separate time trials were performed with seven subjects performing the time trials alone and the others on one of three occasions. On days in which multiple subjects performed the time trial, enough time was given between the start of each subject so that subjects were not able to pace or draft off each other during the trial. During these separate occasions, the time trials were allowed to proceed as long as the wind did not exceed a 3 or a "gentle breeze" on the Beaufort Wind Scale. This is equivalent to a wind speed less than 19 km hr<sup>-1</sup> characterized by surroundings in which smoke rises vertically (0) to a wind velocity were leaves and small twigs constantly move (3).

## Data reduction and analysis

Immediately after the time trial, data collected from the CycleOps power meter and heart rate monitor was downloaded from the onboard computer to an Apple G4 computer. Downloaded data included time, power output, speed, cadence, and heart rate in 1.26-second intervals. Using Power Coach<sup>TM</sup> (Kochli Sport, Sonvilier, Switzerland) software operated by Apple G4 computers, the performance time measured by the external stopwatch was located on the data and isolated. The distance from this isolated data was then checked to ensure that it matched the actual distance of the course. The data isolated in this manner did not vary by more than 50 m ( $7.26 \pm 4.26 \, \text{s}$ ) from the actual distance of the course. Each line of data was also checked for any potential recording problems with any erroneous (loss of signal or supra-physiological) data interpolated between the adjacent data points. On average, approximately four seconds of data were interpolated in any given time trial (range = 0–24 s), with never more than 2 erroneous data points occurring in sequence. Finally, the statistics of interest were calculated using specific code written for Matlab<sup>®</sup> (Mathworks Inc., Berkeley, CA, USA).

# Field measured aerodynamic and rolling resistance profiling

Within three weeks of the time trial, aerodynamic and rolling resistances were determined from field measures of power and velocity (*Edwards & Byrnes*, 2007; *Lim et al.*, 2011). Using the methodology described by *Di Prampero et al.* (1979), drag area ( $A_d$ ) and rolling resistance ( $R_r$ ) were calculated for each subject (see Appendix S1).

#### Projected frontal area

Projected frontal area was determined based on the recommendations of *Olds & Olive* (1999). Digital photographs (Nikon Cool Pix 4300, Melville, New York, USA) of the subjects were taken while subjects sat in a riding position on the bicycle they used during the time trial, which was mounted on a stationary trainer. Photographs were analyzed using NIH Image 1.62 software. This software, after calibration against a known distance or area, automatically calculates the area of a given tracing. Projected frontal area was calculated from tracings of the subject's body and helmet only with the bicycle excluded. In addition to actual measures of projected frontal area, estimates of projected frontal area were also made. Numerous equations have been provided in the literature to either predict

Table 2 Primary determinants of aerodynamic and rolling resistance measured on the bicycle and body position used during the time trial.

	Mean ± SD	Min	Max
Air Density (kg m <sup>-3</sup> )	$1.00 \pm 0.02$	0.98	1.05
$k \text{ constant (N m}^{-2} \text{ s}^2)$	$0.170 \pm 0.028$	0.126	0.228
$A_d$ (m <sup>2</sup> )	$0.349 \pm 0.059$	0.258	0.462
$A_P$ (m <sup>2</sup> )	$0.338 \pm 0.050$	0.272	0.444
Est $A_P$ (m <sup>2</sup> ) (Olds et al., 1995)	$0.342 \pm 0.017$	0.32	0.375
Est $A_P$ (m <sup>2</sup> ) ( <i>Heil</i> , 2002)	$0.327 \pm 0.027$	0.293	0.386
$R_r(N)$	$4.88 \pm 1.27$	2.71	7.39
$C_r$ (dimensionless)	$0.006 \pm 0.002$	0.004	0.009
Total Mass (kg)	$80.33 \pm 9.42$	68.9	99.7

#### Notes.

Constant k, aerodynamic character of a cyclist;  $A_d$ , drag area;  $A_P$ , measured projected frontal area; Est  $A_P$ , estimated projected frontal area;  $R_r$ , rolling resistance;  $C_r$ , quality of the tire and road interface; total mass, mass of bicycle and rider

or account for some aspect of the aerodynamic drag or frontal area of cyclists (*Pugh*, 1974; *Davies*, 1980; *McLean*, 1993; *Olds*, *Norton & Craig*, 1993; *Olds et al.*, 1995; *Heil*, 2001; *Heil*, 2002). Some of the equations rely on the assumption that  $A_P$  is a constant fraction of body surface area (BSA), while others derive more complex algorithms to predict  $A_P$  based on various anthropometric qualities of a cyclist (i.e., height and weight). A total of ten different equations from previous research (*DuBois & DuBois*, 1916; *Pugh*, 1974; *Davies*, 1980; *McLean*, 1993; *Olds*, *Norton & Craig*, 1993; *Olds et al.*, 1995; *Heil*, 2001) were compared.

#### Statistical analyses

Bivariate correlations were performed to assess the relationship between physical, physiological, and normalized variables to time and average power measured during the time trial. In addition, stepwise multiple regressions were performed to locate the best single or combination of variables predictive of time and average power output. Differences between correlation coefficients were then located using the Hotelling test. The Pearson product-moment correlation coefficients were used to determine the relationship between actual and predicted values of  $A_p$  and  $A_d$ . Repeated-measure ANOVAs were run to determine if mean differences existed between actual and predicted values of  $A_p$ . If significance was found, the more conservative Scheffe post-hoc test was used to determine which variables differed. Significance for all calculations was set at p < 0.05. Descriptive data are reported as the mean, standard deviation, minimum, and maximum.

# **RESULTS**

The primary components of resistance during cycling are presented in Table 2. Because the  $A_P$  was calculated with the rider only while the  $A_d$  was calculated for the entire bicycle and rider system, it would be technically incorrect to calculate a  $C_d$  for the bicycle and rider system or rider alone. Still, dividing  $A_d$  by the  $A_P$  would give a estimated  $C_d$  of  $1.03 \pm 0.12$ . A correlation of 0.735 was found between  $A_P$  and  $A_d$ . No relationship, however, was found between  $A_P$  and the  $C_d$  (r = -.170, p = 0.486).

Table 3 Performance and environmental variables measured during the time trial.

	Mean ± SD	Min	Max
Total time (min:sec)	$31:24 \pm 2:15$	28:05:00	34:52:00
Temperature (°C)	$26.2 \pm 4.5$	20	35
Humidity (%)	$30.7 \pm 9.5$	14	50
Air pressure (mmHg)	$629.2 \pm 3.7$	626.4	638.3
Air density (kg $m^{-3}$ )	$0.97 \pm 0.02$	0.95	1
Average power (Watts)	$303 \pm 26$	259	354
Standard deviation of the power during the time trial (Watts)	$80 \pm 14$	61	113
Power (Watts kg <sup>-1</sup> )	$4.32 \pm 0.44$	3.27	4.98
Power (% of LT)	$112.4 \pm 9.2$	96.1	133
Power (% of VO <sub>2</sub> peak)	$84.1 \pm 5.9$	69.6	92.5
Heart rate (bpm)	$173 \pm 6$	161	183
Standard deviation of the heart rate during the time trial (bpm)	8 ± 2	4	11
Heart rate (% of LT HR)	$111.9 \pm 3.8$	101.5	117.6
Heart rate (% of Max $HR_r$ )	$95.5 \pm 1.1$	93.3	96.8
Max heart rate during the time trial (bpm)	$180 \pm 6.3$	167	192

The results of the time trial are presented in Table 3. Of the physiological variables measured,  $\dot{V}O_2$  peak ( $l \min^{-1}$ ) (r = 0.83, p < 0.001), power at  $\dot{V}O_2$  peak (r = 0.67, p < 0.001), and power at LT (r = 0.69, p < 0.001) were significantly correlated to field-measured power output during the time trial. These physiological measures, however, were not strongly or significantly related to time trial performance time ( $\dot{V}O_2$  peak r = -0.42, p = 0.08; power at  $\dot{V}O_2$  peak r = -0.43, p = 0.07; power at LT r = -0.45, p = 0.06). In addition, although significant, the field-measured power output during the time trial was correlated to performance time with an r-value of only -0.59. Thus, as hypothesized, non-normalized physiological measures were not strongly related to time trial performance time.

The correlation of physiological measures and performance time greatly increased when normalized to aerodynamics. When normalized to  $A_d$ , power at  $\dot{V}O_2$  peak (watts m $^{-2}$ ) (r=-0.92, p<0.001) and power at LT (r=-0.85, p<0.001) were better correlated to performance time (Fig. 1). Other normalized laboratory physiological performance measurements were either not significant or if significant were only moderately correlated. The correlation to performance time was best when mean field-measured power output was normalized to either k (r=-0.92, p<0.001) or  $A_d$  (r=-0.92, p<0.001). Figure 2 displays the relationship between performance time relative to the mean field-measured power output as well as mean field-measured power output normalized to body mass,  $A_P$ , and  $A_d$ . Rolling resistance alone or when used to normalize power or physiological measures was not related to performance time.

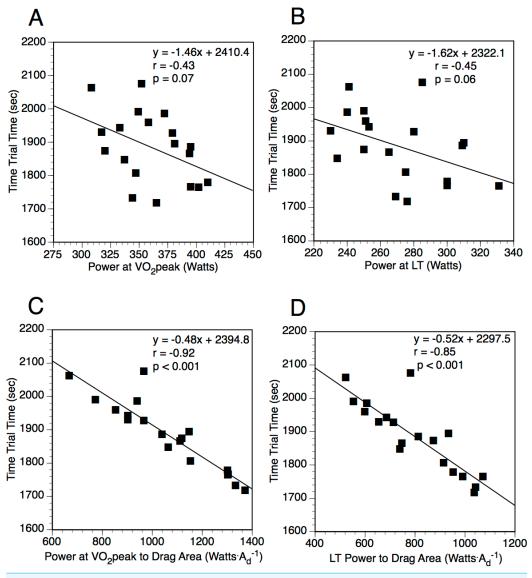


Figure 1 The relationship between time trial performance time relative to non-normalized and normalized laboratory measures. (A) Performance time relative to power at  $\dot{V}O_2$  peak. (B) Performance time relative to power at lactate threshold (LT). (C) Performance time relative to power at  $\dot{V}O_2$  peak normalized to field-determined drag area  $(A_d)$ . (D) Performance time relative to power at LT normalized to field-determined  $A_d$ .

Both k (r = -0.32, p = 0.18) and  $A_d$  (r = -0.32, p = 0.17) were not correlated to field-measured power output during the time trial. However, both k (r = 0.85, p < 0.001) and  $A_d$  (r = 0.85, p < 0.001) alone were significantly related to performance time. Although significant (p = 0.04), measured  $A_P$  alone had a lower correlation (r = 0.47) and no methods for determining Est  $A_P$  correlated with performance time (r = 0.010 to 0.099). Furthermore, field-measured power output normalized to  $A_P$  was only modestly correlated to performance time (r = -0.75).

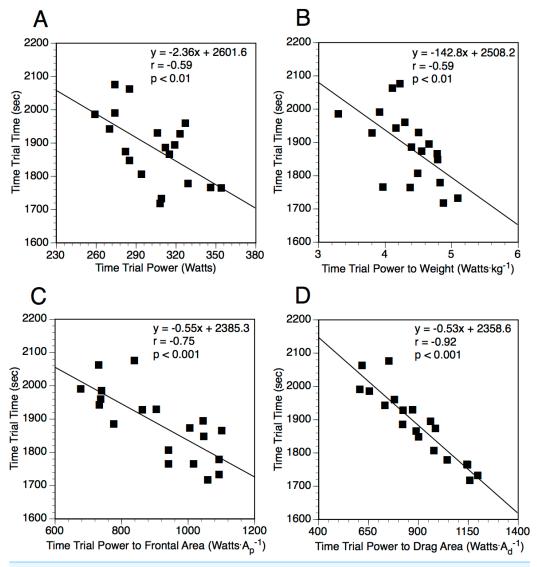


Figure 2 The relationship between time trial performance time relative to the non-normalized and normalized field-measured power output. (A) Performance time relative to mean field-measured power output. (B) Performance time relative to mean field-measured power output normalized to body mass. (C) Performance time relative to mean field-measured power output normalized to frontal area  $(A_P)$ . (D) Performance time relative to mean field-measured power output normalized to field-determined drag area  $(A_d)$ .

Assuming that all of the resistance faced by the cyclists during the time trial was due to aerodynamic and rolling resistance, estimates of power for each component are given. Aerodynamic power was calculated from the k measured for each subject's bicycle position while rolling resistance was assumed to be the remainder of the power. During the time trial, aerodynamic and rolling resistance accounted for 89.77% and 10.23% of the total power at  $272 \pm 23$  and  $31 \pm 12$  watts, respectively.

Except for the *Olds et al.* (1995) and *Heil* (2001) methods (P > 0.999 and 0.322, respectively), the mean value for  $A_P$  (0.338  $\pm$  0.049 m<sup>2</sup>) was significantly over predicted by

all other estimations of  $A_P$  as a percent of BSA (p < 0.001; Pugh (34), P = 0.011). The range for Est  $A_P$  as a percent of BSA was  $0.306 \pm 0.020$  m<sup>2</sup> to  $0.495 \pm 0.032$  m<sup>2</sup>. For predictions of  $A_P$  based on anthropometric algorithms, except for the *Heil* (2002) method (P = 0.983), all other methods significantly (P < 0.001) over predicted our digitized  $A_P$ . These Est  $A_P$  ranged from  $0.399 \pm 0.025$  m<sup>2</sup> to  $0.550 \pm 0.028$  m<sup>2</sup>. No correlation was found between total mass and  $A_P$  (P = 0.302, P = 0.208).

Stepwise regression was also performed to predict time trial performance time and power. In this multivariate analysis, the best correlates of level time were the mean field-measured power to  $A_d$  (r=-0.92, p<0.001,  $y=-0.53\times$  time trial power to drag area +2358.6). The correlation coefficient for this relationship was not significantly different from that for power to k (r=-0.92, p<0.001), which indicates that variations in ambient air density between the different time trial days was unlikely to have had much impact on performance time in our group of subjects. If power at  $\dot{V}O_2$  peak and LT are normalized to parameters that affect resistance, the best correlate of performance time was power at  $\dot{V}O_2$  peak normalized to  $A_d$  (r=-0.92, p<0.001,  $y=-0.48\times$  power at  $\dot{V}O_2$  peak to  $A_d+2394.8$ ). This correlation was not significantly different from that obtained using the mean field-measured power normalized to  $A_d$  or k. For power output during the time trial, the best correlate from all the variables measured in the laboratory is  $\dot{V}O_2$  peak ( $1 \text{ min}^{-1}$ ) (r=0.83, p<0.001,  $y=54.67\times\dot{V}O_2$  peak +48.8).

#### DISCUSSION

As hypothesized, a cyclist's mean field-measured power output normalized to our field-determined aerodynamic resistance (i.e., k or  $A_d$ ) was the best correlate of level time trial performance time (r=-0.92, p<0.001). These results demonstrate and confirm that aerodynamic resistance is the primary resistance that is faced when cycling on level terrain. Accordingly, lab-measured physiological indices of performance (e.g., power at  $\dot{V}O_2$  peak), though significantly correlated to field-measured power output (r=0.64), were not significantly related to performance time (r=-0.43), unless normalized to aerodynamic resistance (r=-0.92). Of note, our field-determined drag area alone was the single best correlation with performance time on the level (r=0.85, p<0.001), confirming that aerodynamic resistance in our population played the most significant role in level time trial performance. Further, our field-determined drag area improved correlations to performance time better than either  $A_P$  or Est  $A_P$ . In addition, rolling resistance was not a distinguishing predictor of performance reflecting its smaller contribution to the resistance to forward motion during cycling.

In agreement with *Balmer, Davison & Bird* (2000), we found the majority of laboratory measures were not significantly correlated to level time trial performance time. In contrast to our findings though, a number of investigators have shown stronger correlations between laboratory measures of performance and level time trial performance in the field (*Hawley & Noakes, 1992; Nichols, Phares & Buono, 1997; Smith, Dangelmaier & Hill, 1999; Anton et al., 2007*). It is likely that these conflicting findings are due to differences in the subject populations recruited. For example, in the study by Anton et al. (2007), the

subject population had a relatively homogenous frontal surface area  $(0.35 \pm 0.02 \,\mathrm{m}^2)$  and a relatively heterogeneous maximal mechanical power output  $(490 \pm 56 \,\mathrm{Watts})$  compared to the subjects from our study  $(0.34 \pm 0.05 \,\mathrm{and}\, 362 \pm 30, \mathrm{respectively})$ . This homogeneity in frontal surface area likely resulted in a greater correlation between laboratory measures and level time trial performance. Because level time trial performance is essentially a balance between resistive forces (primarily aerodynamic resistance) and propulsive forces (mechanical power output), homogeneity in one factor results in the other heterogeneous factor having a greater correlation. Furthermore, it is our belief that correlations in these previous studies would be stronger if the laboratory performance measures were normalized to the subject's actual aerodynamic drag area. For instance, in our study, power at LT had a correlation of -0.45 with performance time but when this same laboratory measure was normalized to  $A_d$ , the correlation became -0.85.

Our finding that level time trial performance time is best predicted by normalizing field-measured power output to either k or  $A_d$  (r=-0.92, p<0.001), while perhaps self-evident, underscores the significant absence of actual aerodynamic measures in studies attempting to predict cycling time trial performance in the field. *Martin et al.* (2006) found measured aerodynamic drag can be used to predict sprinting speed in cyclists. Our study furthers these findings, and is the first to highlight the importance of measured aerodynamics during longer duration events at slower speeds compared to those seen during sprinting. In our study, the mean field-measured power was significantly correlated to level time (r=-0.59, p<0.01) but only explained 35% of the variability in level time. However, when field-measured power was normalized to aerodynamics, 85% of the variability was explained by highlighting that differences in aerodynamics are a critical performance determinant.

We found aerodynamic drag alone represented as either k or  $A_d$ , was significantly correlated to performance time (r=0.85, p<0.001), explaining 72% of the variability in performance time. The heterogeneous equipment and positions subjects used in the time trial may have aided this finding. Out of our nineteen subjects, nine used time trial bicycles, four used standard road bicycles with aerodynamic handlebars, and the remaining six used a standard road bicycle with no specific aerodynamic equipment. However, while each group had significantly different mean values for  $A_d$ , within the nine subjects using time trial bicycles, our results were similar with mean field-measured power normalized to aerodynamics the single best predictor of performance time (r=-0.88, p<0.001), aerodynamics the next best predictor (r=0.72, p<0.001), and field-measured power not predicting performance time (r=-0.33, p>0.05). The range in  $A_d$  between subjects riding a time trial bicycle (0.258 to 0.355 m²) may have also aided in this finding. This range in  $A_d$  though, also highlights the variability that exists between individuals with similar equipment and the importance of determining drag area to predict level time trial performance.

Because aerodynamic drag has been difficult to measure in the past, many studies have attempted to use estimates of the projected frontal area (Est  $A_P$ ) or actual measures of projected frontal area ( $A_P$ ) to represent aerodynamic drag ( $A_d$ ) (Swain, 1994;

Anton et al., 2007). Estimating  $A_d$  in this manner assumes a constant coefficient of drag  $(C_d)$ , which along with  $A_P$  makes up  $A_d$ . However, in the present study,  $A_P$  only accounted for 54% of the variability in  $A_d$ . This discrepancy is largely due to individual differences in  $C_d$ . Assuming a constant  $C_d$  requires that riders must be riding in the same environmental conditions while using the same bike, geometry, clothing, and equipment. However, the range of  $C_d$  values between our subjects (0.823 to 1.262) highlights the individual variability in this measure. Furthermore, in agreement with previous work (Kyle, 1991; De Groot, Sargeant & Geysel, 1995; Debraux et al., 2011), we found no relationship between  $A_P$  and  $C_d$  (r = -0.17, p = 0.49) demonstrating their independence and individual importance in determining  $A_d$ . Accordingly, when normalizing field measured power output during the time trial, we found that the correlation to performance time was significantly lower using  $A_P$  (r = -0.75) or Est  $A_P$  (-0.71) compared to normalizing using our field-determined  $A_d$  (r = -0.92). Thus, actual projected frontal area or an estimate of projected frontal area does not explain all of the variability in  $A_d$  and when used to normalize power is not necessarily better in the prediction of level time trial performance than  $A_d$  alone (r = -0.85).

The results from the present study suggest that field-testing with a power meter may be a better alternative to traditional laboratory testing (i.e.,  $\dot{V}O_2$  peak, LT, economy) for athletes and coaches wanting to predict time trial performance. The field-measured drag area in combination with field-measured power output provided the best prediction of time trial performance compared to any combination of laboratory testing. Furthermore, we demonstrate that determining drag area does not need to be difficult. Our field-measured determination of drag area was the single best predictor of time trial performance and requires only a power meter, speedometer, and flat road making it far more economical than other tools (i.e., a wind tunnel). Thus, athletes can easily quantify and improve performance in events like level time trials by using our field-measured drag area technique to optimize the relationship between aerodynamic resistance and power output.

In conclusion, to predict cycling performance in the field, a cyclist's ability to produce power must be considered relative to the forces that resist forward motion. Accordingly, level time trial performance is best predicted by normalizing the mean field-measured power output to aerodynamic resistance per velocity squared (k) or the drag area  $(A_d)$ . Despite the fact that physiological variables are commonly thought of as the most important determinant of performance, we found that alone, measures of aerodynamic resistance were better related to level performance than  $\dot{V}O_2$  peak, LT, or economy. Moreover, the use of projected frontal area  $(A_P)$  or estimates of projected frontal area  $(Est A_P)$  are not as accurate as directly measured  $A_d$ .

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#### **Competing Interests**

The authors declare there are no competing interests.

#### **Author Contributions**

- James E. Peterman analyzed the data, contributed reagents/materials/analysis tools, wrote the paper, prepared figures and/or tables, reviewed drafts of the paper.
- Allen C. Lim and William C. Byrnes conceived and designed the experiments, performed the experiments, analyzed the data, contributed reagents/materials/analysis tools, wrote the paper, prepared figures and/or tables, reviewed drafts of the paper.
- Ryan I. Ignatz performed the experiments, analyzed the data, contributed reagents/materials/analysis tools, wrote the paper, reviewed drafts of the paper.
- Andrew G. Edwards performed the experiments, analyzed the data, contributed reagents/materials/analysis tools, reviewed drafts of the paper.

#### **Human Ethics**

The following information was supplied relating to ethical approvals (i.e., approving body and any reference numbers):

All subjects were informed of the risks involved with participation in the study and gave written informed consent before participating. The Human Research Committee at the University of Colorado Boulder approved the protocol used for this study (reference number 0600.20).

## Supplemental Information

Supplemental information for this article can be found online at http://dx.doi.org/10.7717/peerj.1144#supplemental-information.

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