



A library of programmable DNAzymes that operate in a cellular environment

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SUBJECT AREAS:

BIOSENSORS

DNA

NANOSTRUCTURES

NUCLEIC-ACID THERAPEUTICS

Received
6 November 2012

Accepted
26 February 2013

Published
25 March 2013

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DNAzymes were used as inhibitory agents in a variety of experimental disease settings, such as cancer, viral infections and even HIV. Drugs that become active only upon the presence of preprogrammed abnormal environmental conditions may enable selective molecular therapy by targeting abnormal cells without injuring normal cells. Here we show a novel programmable DNAzyme library composed of variety of Boolean logic gates, including YES, AND, NOT, OR, NAND, ANDNOT, XOR, NOR and 3-input-AND gate, that uses both miRNAs and mRNAs as inputs. Each gate is based on the c-jun cleaving Dz13 DNAzyme and active only in the presence of specific input combinations. The library is modular, supports arbitrary inputs and outputs, cascable, highly specific and robust. We demonstrate the library's potential diagnostic abilities on miRNA and mRNA combinations in cell lysate and its ability to operate in a cellular environment by using beacon-like c-jun mimicking substrate in living mammalian cells.

'DNAzymes' are a catalytically active class of antisense reagents discovered in 1994¹. In the past decade, DNAzymes (and mostly '10–23') have been used as inhibitory agents in a variety of experimental disease settings, suggesting their possible clinical utility^{2–6}.

Autonomous bio-molecular systems that can interact with naturally occurring biomolecules (such as indicators of particular diseases) and analyze their presence^{7–13}, may be the basis of 'programmable drugs', potent drugs that become active only if preprogrammed abnormal environmental conditions hold.

Results

We modified the Dz13 DNAzyme (which showed promise of a therapeutic agent in preclinical studies by targeting the c-jun mRNA¹⁴) and preprogrammed it into a library of Boolean logic gates where only upon specific conditions, Dz13 regains its catalytic activity. These conditions are determined by the presence of predefined input molecules, in the form of miRNA or mRNA molecules, and the Boolean logic gate rules.

Our system is based on multi-component units in which computations are performed by three mechanisms: (a) splitting the DNAzyme at the core catalytic region in a way that only when an appropriate input molecule exists the complete DNAzyme complex is formed¹⁵ (b) caging the DNAzyme arms using a stem-loop structure, which can be un-caged when an appropriate input exists¹⁶ and (c) toehold exchange in which a longer hybridization is favored, where the presence of an input molecule changes the components' conformation.

To construct the simple YES gate, which is active only when a single input molecule is present, we used the '10–23' DNAzyme Dz13 (Fig. 1a). By following a previous design¹⁷ the DNAzyme's catalytic core was split into two parts between T₈ and A₉. Only upon the presence of an appropriate input molecule, the two parts are joined, the DNAzyme complex is formed and the cleavage of RNA occurs ('True' output) (Fig. 1b).

To form the AND gate, an additional binding loop was added consisting of a complementary sequence for the second input, followed by a 'caging' sequence which is complementary to the DNAzyme arm to form a stem-loop structure (Fig. 1c). When the second input is present, the arm is un-caged (since the open conformation is favored) and the gate can accept the first input which joins the two sub-components. Only when both inputs are present, the complete DNAzyme complex is formed. Caging may be done on either one of the arms, as demonstrated in Supplementary information Fig. 2.

To complete the basic Boolean logic gates, we also implemented the NOT gate using an additional strand which contained the input's complementary sequence ('anti-input' molecule). When the input is present, it 'cancels' the anti-input molecule, the DNAzyme's components are separated, resulting in a 'False' output (Fig. 2a). The OR gate was implemented by using two YES gates operating in parallel on two different inputs (Fig. 2b).



Figure 1 | YES or AND gates demonstration *in vitro*. (a) Illustration of Dz13 cleaving its proper fluorescently labeled RNA substrate. (b and c) Each panel is an illustration of YES or AND gate's operation upon presence of its inputs (upper panel); Capillary-electrophoresis demonstrates cleavage or non-cleavage of the fluorescent substrate (upper middle panel); Quantitative cleavage results of 3 independent experiments (bottom-middle panel) and Plate Reader results showing reaction kinetics (bottom panel). Each gate's results match its truth table. For YES: input A = miR155, un-proper input B = miR31; For AND: input A = miR21, input B = miR125b. Standard deviation errors from three independent experiments are shown (bars).

After implementing the basic Boolean gates, we extended our library to more complex gates that combine two inputs. The **ANDNOT gate** is implemented by combining the AND and NOT gates' design. When both inputs are present, the second input cancels the anti-input molecule, resulting in a 'False' output (Fig. 2c). The **NAND gate** is formed by combining two NOT gates for the two different inputs. Only when both inputs are present, the two gates are inactive (Fig. 2d). The **NOR gate** is an inverse AND gate. When either is present, the complete DNAzyme complex is disassembled, resulting in a 'False' output (Fig. 2e). The **XOR gate** is formed by combining two ANDNOT gates. When either input is present, it activates one of the sub-gates, but also cancels

the orthogonal sub-gate by binding to its anti-input molecule. Only when a single input (but not both) is present, the gate is active (Fig. 2f). As shown, the gates possess a 'digital', non-leaky behavior. This feature is a key for therapeutic agents in future diagnostic systems: only cells that meet a specific abnormal profile will be targeted, sparing healthy ones.

Finally, we extended our library to support an additional input. The **3-input-AND gate** is formed using an AND gate in which both arms are caged. Only when all 3 inputs are present, the complete DNAzyme complex is formed resulting in a 'True' output (Fig. 2g). Theoretical truth tables of the gates shown in Fig. 1 and Fig. 2 are demonstrated in Supplementary information Fig. 3.

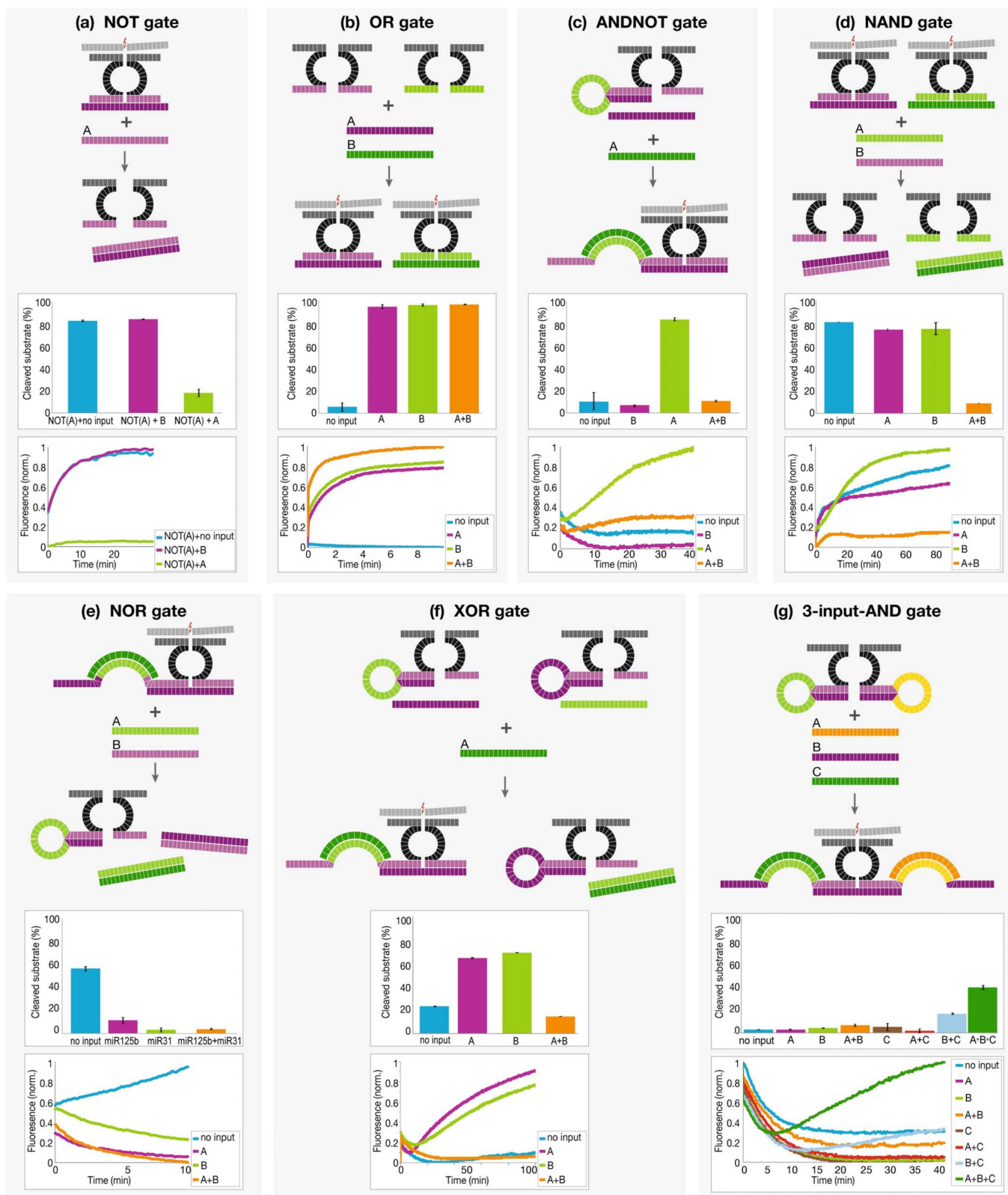


Figure 2 | Logic gate design and implementation. Each panel shows: upper panel, schematic gate operation in the presence of its entire set of inputs; middle panel, quantitative cleavage results of 3 independent experiments; bottom panel, reaction kinetics. The results of each gate match its truth table. (a) for NOT: input A = miR31; (this is a single input gate, only A is shown) (b) for OR: input A = miR21, input B = miR125b; (c), (e) and (f) for ANDNOT, NOR & XOR: input A = miR31, input B = miR125b; (d) for NAND: input A = miR31, input B = miR155; (g) for 3-input-AND gate, input A = miR31, input B = miR21 and input C = miR125b. In (c) & (f) only input A is shown since this is the only (c) or one of (f) the input combinations that has a positive ("True") result in which the complex is formed. Standard deviation errors from three independent experiments are shown (bars).



Abnormal cells can be diagnosed by using a complex Boolean expression, in which inputs such as mRNA and miRNA serve as ‘disease markers’. To demonstrate our library’s ability to diagnose unhealthy cells by solving such expressions, the following expression was chosen: **Breast Cancer = (Breast-specific miRNA AND Cancer miRNA) OR (Breast-specific miRNA AND NOT Healthy miRNA) OR (Cancer mRNA)**.

A breast cell is considered ‘cancerous’ if it either possesses: (1) combinations of breast-specific microRNA and a ‘cancerous’ microRNA or (2) breast-specific miRNA but lacks the ‘health indicative’ miRNA or (3) cancerous mRNA. The inputs demonstrated are miR31 as a breast-specific miRNA¹⁸, miR21 as a strong markers of breast cancer^{19,20} and miR125b as health indicative miRNA¹⁸. The c-myc oncogene serves as a cancerous mRNA marker²⁰. Therefore, the expression can be further described as: **Breast cancer = (miR31 AND miR21) OR (miR31 AND NOT miR125b) OR (c-myc)**.

To indicate the potential of our library to both ‘diagnose’ and ‘treat’ cancerous cells in the future, we demonstrated its ability to solve the above expression in a cellular environment (cancer cells lysate). As the gates are based on Dz13, a ‘true’ output will result in the active state of the DNAzyme, which can potentially cleave the c-jun mRNA, potentially a key step of an apoptosis-based ‘treatment’, as shown in Fig. 3.

Finally, we turned to test the feasibility of our library’s design principles to operate within living human cancer cells. For this purpose, we used a beacon-like substrate which contains a fluorophore and a quencher (Supplementary information, Materials & Methods section). Only when the substrate is cleaved by a DNAzyme, the fluorophore and quencher are separated resulting in light emission.

(a) Breast Cancer = (Breast-specific miR AND Cancer miR) OR (Breast-specific miR ANDNOT Healthy miR) OR (Cancer mRNA)

(b) Cancer = (miR31 AND miR21) OR (miR31 ANDNOT miR125b) OR (c-myc)

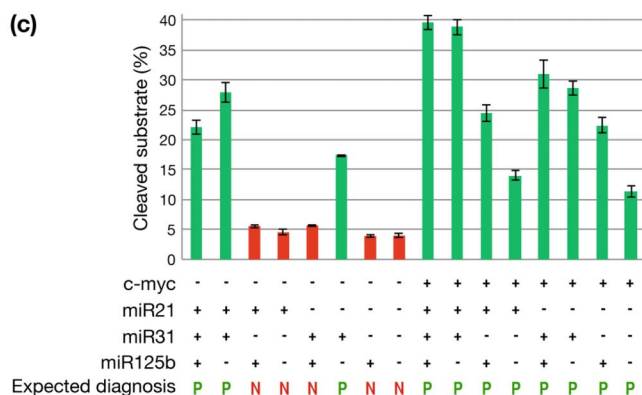


Figure 3 | Expression profile of breast cancer in cell lysates. (a) and (b) Definition of Boolean expressions representing positive breast cancer diagnosis. (c) capillary electrophoresis results for the complex Boolean expression. Experiments were performed using the same conditions as the *in vitro* experiments in previous figures, by replacing DDW with cell lysate (1.8 mg/ml by BCA assay), and with addition of miRNAs & myc RNA to the reaction. Only upon fulfillment of conditions which meet the requirements defined for ‘breast cancer’ the DNAzyme became active and its substrate cleaved. The design of each basic logic gate (AND, ANDNOT, YES, OR) is as shown in previous figures. Variance in the cleavage efficiency of positive conditions may be explained by the different reaction kinetics underlying each ‘active’ complex (as seen in Fig. 1 & 2). Standard deviation errors from three independent experiments are shown (bars).

To demonstrate this ability, we used the AND gate (which contains both core design elements our system is built upon – splitting the catalytic core & caging the DNAzyme arm). The gate’s components, along with the substrate and exogenous inputs were introduced into cells by microinjection using a Confocal microscope (Supplementary information). Although microinjection might be harmful to living cells, it provides the best control over time, enabling demonstration of computation in its first several minutes. To protect our libraries’ components from nucleases, an inverted thymidine modification was added to the 3’ end. As shown in Fig. 4, the AND gate, representing the library’s design, operates within living cells, *ex vivo*, and computations are very rapid (less than 5 minutes). As clearly seen, the result of the cleavage (i.e.: red fluorescent signal) localizes entirely in the cell nucleus. This strengthens the fact that computations were performed inside the cells (as also demonstrated in “Video AB” in the Supplementary Information).

Discussion

The results of this experiment demonstrate that the principles underlying our library’s design can generally operate in a cellular environment as a proof-of concept. The feasibility of applying these principles for real diagnosis has yet to be demonstrated. We chose to demonstrate these principles in living cells using the AND gate, which contains both core design elements our system is built upon – splitting the catalytic core & caging the DNAzyme arm. All other gates are based on similar principles. We demonstrated the ability of multiple gates (AND, ANDNOT, OR, YES) to operate in a cellular environment in the lysate experiment in lieu of demonstrations of additional gates *ex vivo*.

Our system can in principle receive any RNA (or DNA) sequence as its input, and thus can sense for both miRNA and mRNA, as demonstrated. Unlike previous systems which implemented logic libraries based on DNAzymes¹⁵ where the computational layer was dependent on the relation between inputs (and thus inputs depended on each other), our system does not require any dependence between inputs. Each input can be completely arbitrary, allowing integration of any input combinations. In addition, unlike previous implementations¹⁷, in which the input specificity was determined by a maximal amount of 7 nucleotides, our system is not restricted to short input sequences. As demonstrated, most of our logic gate input-binding sequences are 18–22 nucleotides long, allowing great specificity and minimizing identification of inappropriate inputs. This is a key feature for using cellular markers as inputs, since a cell contains a large amount of miRNA/mRNA populations, some with common sequences.

The output of the system (the target gene) is programmable and is selected by the RNA-binding arms’ sequence. Since both output and inputs are RNA molecules, unlike other miRNA based systems⁷, simple reactions can be composed, in principle, to form cascaded (compositional) ones, where the output RNA of one gate can serve as the input for a downstream gate. In addition, our design supports more than 2 inputs for an AND gate (and for all other gates). As we have demonstrated, by ‘locking’ both input-binding arms, we have created a 3-input-AND gate, illustrated in Fig. 2g. By ‘locking’ also the substrate-binding-arms, the system can be extended to create a 5-input-AND gate. In previous designs, implementation of such a gate would require cascaded gates, each adding multiple molecular interactions. In our system, any additional input (beyond 2 inputs) requires the addition of a single molecular interaction, keeping the total chemical complexity relatively low. Demonstration of several AND gates also shows the programmability of the gate’s inputs (Supplementary information 2).

Unlike previous systems based on DNAzymes^{15,21}, we focused on the ability to interact with physiologic components (inputs and outputs), which is a necessary step towards clinical utilization. In a top-down approach, we modified the ‘Dz13’ drug into a ‘programmable

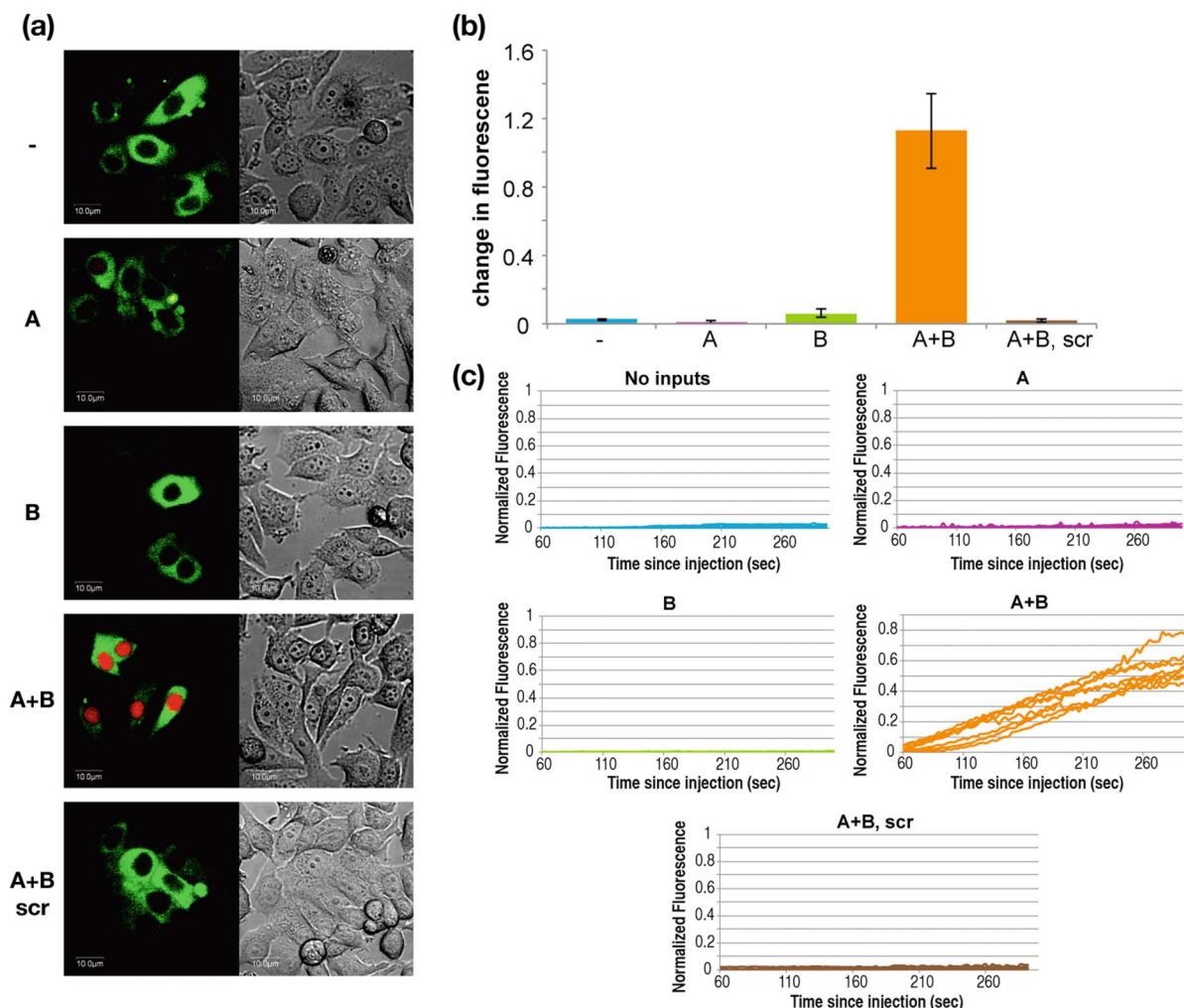


Figure 4 | DNAzyme-based AND gate operating within cancerous living cells. Left panel, fluorescent view of the injected cells; Right panel, phase view of the cells during and after injection. For each inputs combination 15 cells were microinjected with the following mixtures: (1) AND gate components; (2) combination of miRNA inputs (A = miR21, B = miR125b), (3) a fluorescent-quenched substrate (red) and (4) green Dextran (70 KDa), which was used to normalize and mark injected cells. (a) Representative injected cells were imaged for 5 minutes after injection. Only when both inputs were present (A + B), the red substrate was cleaved and therefore visible. 'scr' represent injections of a scrambled DNAzyme's component sequence, which were otherwise identical to the normal injections; (b) Average of relative change in red fluorescence in 15 cells, 5 minutes after microinjection (change was calculated as: normalized fluorescence 5 minutes post injection minus normalized fluorescence 1 minute post injection). The design of the AND gate is as shown in Fig. 1. Standard deviation errors are shown (bars). (c) Kinetic results in living cells.

drug', which operates only when certain pre-programmed conditions are met. For this purpose, we preferred to utilize a member of the '10–23' DNAzyme family as our hardware, over other families such as 'E6', '8–17' (that were already shown as the basis of Boolean logic gates and automata^{16,21,22}) mainly due to its powerful clinical antisense activity *in vivo*^{23,24} and its ability to operate in physiological conditions, such as low MgCl₂ concentrations and 37°C²⁵. Unlike previous systems¹³ which rely on gene transcription to perform computation, our computing element directly binds to both input and target RNA, keeping chemical interactions to a minimum and reducing the number of components which should be delivered to the cell.

Our current demonstrations are based on well-controlled concentrations of microRNAs and mRNAs, which are higher than endogenous levels²⁶, and delivery of these exogenous inputs was performed using microinjection. This is a demonstration that our design is not adversely affected by the cellular environment, a first step towards practical diagnosis. In order to utilize the system for clinical diagnosis, its sensitivity should be increased, for example by integration of input amplifiers²⁷. Applicability also depends on efficient delivery. As both programmable DNAzymes and simple

DNAzymes are composed of DNA strands, a therapeutically feasible delivery mechanism of known DNAzymes may also be efficient for programmable DNAzymes. Finally, the library should be further optimized to reduce false-positive detection and signal leakage, especially in the cellular environment. This may be achieved by further optimizing the length of the caged arms as well as adding a "suppressor" antisense molecule (as previously shown¹⁰).

In conclusion, we presented a library of programmable DNAzymes that operates in a cellular environment and can potentially operate in living cancer cells. The library is modular, supports arbitrary inputs and outputs, potentially cascable, highly specific and robust. Unlike single-marker diagnosis, our library allows integration of multiple markers according to predefined rules, thus may be the first step towards a future of 'smart' medical diagnosis and therapy in the form of 'programmable' therapeutics.

Methods

DNAzyme design and synthesis. Programmable DNAzymes are based on the '10–23' DNAzyme, with the catalytic core split into two parts between T8 and A9 (based on previous MNzyme design¹⁵) so that each part contains a 9 nt substrate binding region and a 10–11 nt input binding region (input is split across the two parts). Prior



to any experiment, gate components were warmed to 99°C and slowly brought down to 10°C in a 50 mM NaCl solution to allow hybridization and stored in -20°C. Synthetic single-stranded RNA substrate was labeled by a FAM fluorophore in its 3' end. Unmodified DNA sequences were obtained from Sigma-Aldrich (Standard Desalted). Modified DNA sequences and RNA sequences were obtained from Integrated DNA Technologies (HPLC Purified). Oligos were stored in -20°C in TE buffer. All sequences can be found in Supplementary Table 1.

In vitro cleavage experiments. Experiments were performed by preparing a reaction mixture that contained the DNazymes fluorogenic RNA substrate (0.1 μM final) in 10 μl reaction buffer (Tris-HCl 50 mM, pH 7.5) containing 150 mM NaCl and 10 mM MgCl₂ and 1 μl of each input (2 μM final, or 10 μM final for the NAND & XOR gates). Computation was initiated by the addition of 1 μl of each of the DNzyme components (2 μM final) followed by further incubation for 20 minutes (40 minutes for the NOT, ANDNOT & NAND gates; 120 minutes for the XOR gate) at 37°C. The reaction was terminated by passing 0.5 μl of each sample to 22 μl Formamide containing GeneScan LIZ120 size standards which were diluted 1:40 in the Formamide (Applied Biosystems). Samples were run on a capillary electrophoresis machine (ABI Prism, Avant-3100, Applied Biosystems) and analyzed using the GeneMapper software.

In vitro kinetic experiments. Experiments were performed by preparing a reaction mixture that contained the DNazymes quenched/fluorogenic RNA substrate. The quencher used was 3BHQ (3' end) and fluorophore was i6-FAMK (positioned internally between C4 and G5 (Sequence: CAAC/i6-FAMK/GCCTCgtTCCTCCCCG/3BHQ_1, lowercase letters designate RNA nucleotides). Kinetics measurements were done using a Tecan Infinite® 200 microplate-reader. Fluorescence based experiments were done in a total volume of 30 μl in the same conditions as above, in x10 concentrations (1 μM substrate, 20 μM inputs and DNzyme components). Excitation and emission values for FAM fluorophore were set to 485 nm and 518 nm, respectively. Initial fluorescence was measured for 3 seconds prior to reaction initialization by addition of MgCl₂, to establish the fluorescence baseline.

Cell culture. Human MCF7 breast carcinoma cells were obtained from American Type Culture Collection (ATCC) and cultured in RPMI (Gibco-BRL) pH 7.4, supplemented with 10% fetal calf serum (FCS). All media were supplemented with 10 mg/ml streptomycin and 10 IU/ml penicillin and all cultures were incubated in a humidified atmosphere of 5% CO₂ at 37°C. Cells were passaged routinely by trypsinization. Subconfluent MCF7 cells (70%) were incubated overnight prior to microinjections.

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Acknowledgements

We thank Dr. Tom Ran, Dr. Binyamin Gil, Dr. Michal Golan-Mashiach and Dr. Shai Kaplan for helpful discussions. We thank Vladimir Kiss for his excellent technical assistance with the Confocal microscopy experiments. We thank Keren Katzav for the excellent preparation and design of figures. The research was supported by the European Union FP7-ERC-AdG. M.K was supported by The ISF Converging Technologies (Grant No 1694/07). Ehud Shapiro is the Incumbent of The Harry Weinrebe Professorial Chair of Computer Science and Biology.

Author contributions

E.S. led the project. M.K.H. and Y.D. developed the concept, designed the study and performed experiments. All authors discussed the results and implications, commented on the manuscript at all stages and wrote the paper.

Additional information

Supplementary information accompanies this paper at <http://www.nature.com/scientificreports>

Competing financial interests: The authors declare no competing financial interests.

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How to cite this article: Kahan-Hanum, M., Douek, Y., Adar, R. & Shapiro, E. A library of programmable DNazymes that operate in a cellular environment. *Sci. Rep.* **3**, 1535; DOI:10.1038/srep01535 (2013).