

## Research Article

# Calcium Silicate-Based Cements Associated with Micro- and Nanoparticle Radiopacifiers: Physicochemical Properties and Bioactivity

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**Objective.** The aim of this study was to evaluate the physicochemical properties and bioactivity of two formulations of calcium silicate-based cements containing additives (CSCM) or resin (CSCR), associated with radiopacifying agents zirconium oxide ( $ZrO_2$ ) and niobium oxide ( $Nb_2O_5$ ) as micro- and nanoparticles; calcium tungstate ( $CaWO_4$ ); and bismuth oxide ( $Bi_2O_3$ ). MTA Angelus was used as control. **Methods.** Surface features and bioactivity were evaluated by scanning electron microscopy and the chemical composition by energy dispersive X-ray spectrometry (EDS-X). **Results.** CSCM and CSCR presented larger particle sizes than MTA. Hydroxyapatite deposits were found on the surface of some materials, especially when associated with the radiopacifier with  $ZrO_2$  nanoparticles. All the cements presented calcium, silicon, and aluminum in their composition. **Conclusion.** Both calcium silicate-based cements presented composition and bioactivity similar to MTA when associated with the radiopacifiers evaluated.

## 1. Introduction

Mineral trioxide aggregate (MTA) has been classified as calcium silicate-based cement [1] and its extensive clinical indication is attributed to its biocompatibility, alkalinity (pH value 12.5), sealing ability [2], and bioactivity [3, 4]. MTA has Portland cement as the main component in its composition and bismuth oxide ( $Bi_2O_3$ ) to promote radiopacity [5, 6]. The physical, chemical, mechanical, biologic, and antimicrobial properties of calcium silicate-based cements and MTA are similar [7–11].

Calcium silicate-based cements, which have greater consistency and are easier to manipulate, are evaluated as an alternative to MTA. For example, Biodentine (Septodont, Saint-Maur-des-Fossés, France) corresponds to a tricalcium silicate-based cement [12, 13], which has been developed

with indications similar to those of MTA, and as a dentine substitute [14].

The  $Bi_2O_3$  present in MTA may compromise the physical, mechanical, and biologic properties of the cement [5, 6, 15]. Therefore, new radiopacifiers have been evaluated as alternatives to  $Bi_2O_3$ . For example, zirconium oxide ( $ZrO_2$ ) and calcium tungstate ( $CaWO_4$ ) when incorporated into Portland cement result in cements with radiopacity exceeding the minimum value recommended by the ANSI/ADA Specification 57 [16]. Furthermore, both  $ZrO_2$  micro- and nanoparticles have demonstrated bioactive potential [17–19]. The association of  $ZrO_2$  and  $CaWO_4$  with Portland cement showed no cytotoxicity [9]. Niobium oxide ( $Nb_2O_5$ ) may promote radiopacity and improve the biologic properties of materials due to its biocompatibility [20] and bioactivity [21]. Its use in the form of nanoparticles has shown bioactive and antimicrobial potential [22].

Bioactivity is a desirable property for retrofilling cement, because a bioactive material has the capacity to develop a stable bond with live tissue by means of hydroxyapatite deposition [23]. The association of calcium silicate-based cement with different radiopacifying agents such as  $ZrO_2$ ,  $Nb_2O_5$ , or  $CaWO_4$  with different particle size (nano- or microparticles) may favor the bioactive potential of materials. Therefore, the aim of this study was to analyze the surface, chemical composition, and bioactivity of two calcium silicate-based cements with different chemical compositions in association with different radiopacifiers.

## 2. Material and Methods

**2.1. Sample.** Two calcium silicate-based cements with different chemical compositions were evaluated, associated with micro- and nanoparticles of radiopacifying agents (Table 1). The nanoparticles of radiopacifiers were obtained by the polymeric precursor method at the Physics Institute of São Carlos (University of São Paulo, São Carlos, Brazil). The polymeric precursor method is based on metal citrate polymerization with ethylene glycol. A hydroxycarboxylic acid such as citric acid is commonly used as a chelating agent for the cations in an aqueous solution. The addition of a polyalcohol such as ethylene glycol leads to the formation of an organic ester. The polymerization is promoted by heating at around  $120^\circ C$  resulting in a homogeneous resin in which the cations are distributed evenly throughout the organic matrix. The resin is then calcined to produce the desired oxides.

The  $ZrO_2$  supports were prepared by the polymeric precursor method, from the precursor salt  $ZrO(NO_3)_2 \cdot xH_2O$  (Alfa Aesar). Aqueous solutions of this salt were prepared, mixed, and added to an aqueous solution of citric acid (held at  $60^\circ C$ ), with constant stirring. Subsequently, ethylene glycol ( $HOCH_2CH_2OH$ ) was added to polymerize the citrate by a polyesterification reaction (at  $120^\circ C$ ). The citric acid : metal molar ratio was 3 : 1, while the citric acid : ethylene glycol mass ratio was 60 : 40. The resulting polymer resin was then calcined at  $300^\circ C$  for 4 h, and after  $600^\circ C/2$  h to produce  $ZrO_2$  crystalline particles.

An aqueous solution of niobium ammonium oxalate  $\{NH_4[NbO(C_2O_4)_2(H_2O)](H_2O)N(CBMM)\}$  was prepared and ammonium hydroxide was dropped upon thereafter. The niobium hydroxide precipitated was filtered and washed to eliminate oxalate ions and dissolved into a citric acid (CA) aqueous solution ( $[CA]/[Nb] = 3$ ) and filtered. The niobium content in the solution was precisely determined by gravimetric analysis. The solution was stirred for 2 h at  $70^\circ C$  to promote the complex reaction. Ethylene glycol (EG) was added to the mixture with mass ratio 60 : 40. The translucent solution was heated and stirred over several hours. A polymerization process started during the water evaporation, resulting in a highly viscous solution. This resin was heated in an electric furnace at  $300^\circ C$  for 4 h. The resulting black and soft mass was milled and calcined in an electric furnace for 2 h over alumina slabs at  $700^\circ C/2$  h.

TABLE 1: Group of materials evaluated and powder-liquid ratio.

Material	Powder-liquid ratio
White* MTA	1 g-300 $\mu L$
Calcium silicate-based cement containing additives (CSCM)**	1 g-360 $\mu L$
CSCM + 30% zirconium oxide ( $Zr_2O$ ) microparticles****	1 g-200 $\mu L$
CSCM + 30% zirconium oxide ( $Zr_2O$ ) nanoparticles*****	1 g-360 $\mu L$
CSCM + 30% niobium oxide ( $Nb_2O_5$ ) microparticles****	1 g-340 $\mu L$
CSCM + 30% niobium oxide ( $Nb_2O_5$ ) nanoparticles*****	1 g-390 $\mu L$
CSCM + 20% bismuth ( $Bi_2O_3$ ) microparticles****	1 g-260 $\mu L$
CSCM + 30% calcium tungstate ( $CaWO_4$ ) microparticles*****	1 g-200 $\mu L$
Calcium silicate resin-based cement (CSCR)***	1 g-360 $\mu L$
CSCR + 30% zirconium oxide ( $Zr_2O$ ) microparticles****	1 g-235 $\mu L$
CSCR + 30% zirconium oxide ( $Zr_2O$ ) nanoparticles	1 g-340 $\mu L$
CSCR + 30% niobium oxide ( $Nb_2O_5$ ) microparticles	1 g-380 $\mu L$
CSCR + 30% niobium oxide ( $Nb_2O_5$ ) nanoparticles	1 g-380 $\mu L$
CSCR + 20% bismuth ( $Bi_2O_3$ ) microparticles	1 g-250 $\mu L$
CSCR + 30% calcium tungstate ( $CaWO_4$ ) microparticles	1 g-220 $\mu L$

\*MTA, Angelus, Londrina, Brazil.

\*\*Usina Fortaleza ICMF Ltda., Barueri, SP, Brazil (composition: mineral aggregates, additives, and pigments).

\*\*\*Ligatex Ind. e Com. Ltda., Rio Claro, SP, Brazil (composition: mineral aggregates, additives, resins, and pigments).

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\*\*\*\*\*Sigma-Aldrich, St. Louis, MO, USA.

The size of particles obtained for  $ZrO_2$  was 74 nm and for  $Nb_2O_5$  it was 83 nm, which were confirmed by the Brunauer-Emmett-Teller surface area analysis and confirmed with scanning electron microscope. The materials were manipulated with distilled water in accordance with the proportions shown in Table 1.

**2.2. Surface and Chemical Composition Analyses.** For analysis of the surface morphology of the different experimental groups, the materials were manipulated and inserted into cylindrical molds 6 mm in diameter and 12 mm high. The specimens were kept in an oven at  $37^\circ C$  and immersed in distilled water for 28 days. After this period, the test specimens were dried with absorbent paper and kept in a desiccator containing silica, under vacuum, for 24 hours. The specimens were embedded in resin and polished in an automatic polishing machine (EcoMet 250 Grinder-Polisher

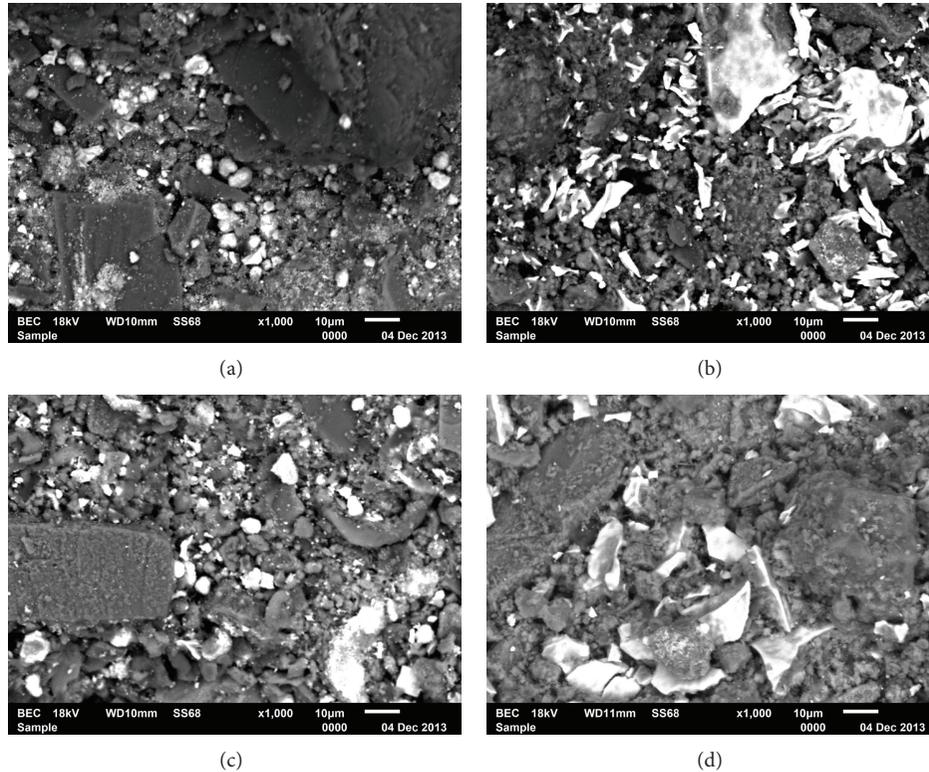


FIGURE 1: Backscattered electron micrography (1000x magnification) of CSCM samples associated with radiopacifiers: (a) ZrO<sub>2</sub> micro, (b) ZrO<sub>2</sub> nano, (c) Nb<sub>2</sub>O<sub>5</sub> micro, and (d) Nb<sub>2</sub>O<sub>5</sub> nano.

Family, Illinois, USA). After being dried again, the specimens were placed on stubs, bathed in carbon, and examined by scanning electron microscopy (JEOL JSM 6610LV, Tokyo, Japan) at different magnifications (50x, 500x, and 1000x) in secondary backscattered electron mode. All the analyses were performed at 18 kV and SS 68. Furthermore, energy dispersive X-ray spectrometry (EDS-X) (Thermo Scientific, Madison, USA) analysis was performed for the images obtained at 1000x magnification.

**2.3. Bioactivity.** All cements were manipulated, compacted into cylindrical moulds measuring 1 mm high × 7.5 mm in diameter. After the materials were set in an incubator at 37°C and 100% humidity, samples were immersed in a standard phosphate buffered saline solution at 37°C for 30 days. Samples were placed on silica gel and soda lime and placed in an incubator for 12 hours to dry. Then, they were carbon coated for electrical conductivity. Surface microstructural assessment of the cements was performed under the scanning electron microscope (SEM) in secondary electron mode. Energy dispersive spectroscopy (EDS) was also performed after and before soaking in a standard phosphate buffered saline.

### 3. Results

**3.1. Surface and Chemical Composition Analyses.** Electronic micrographs for the calcium silicate-based cements were

represented in Figure 1. MTA was used as control. By EDS-X analysis, all the materials demonstrated peaks of calcium, silicone, and aluminum, indicating an aluminat phase that is characteristic of Portland-type cements and differently from pure tricalcium silicate-based cements. The EDS analysis of the CSCM and CSCR before and after soaking in a standard phosphate buffered saline is shown in Table 2. The CSCM and CSCR particle sizes were larger than those of MTA. All the different radiopacifiers used were visible in the electronic micrographs. The radiopacifiers had a brilliant appearance due to their high atomic mass. The nanoparticulate ZrO<sub>2</sub> presented particles with larger sizes than those of microparticulate ZrO<sub>2</sub>. Cement hydration was evident from the presence of calcium silicate hydrate and ettringite in the secondary electron images at higher magnifications (Figure 2).

**3.2. Bioactivity.** The micrographs of samples after the bioactivity assay, in images by secondary electron scanning of the materials, are represented in Figure 3. All the cements presented a similar microstructure. The surface of materials presented a granular appearance, covered with small particles rich in calcium and phosphorous as indicated by the EDS analysis (Figure 3). Hexagon and cubic crystals measuring around 10–40 micrometers in size were visible on the surface of some of the materials, particularly for the cements evaluated with the association of nanoparticulate ZrO<sub>2</sub> as

TABLE 2: EDS analysis of CSCM and CSCR before and after soaking in standard phosphate buffered saline (PBS).

Chemical components	CSCM		CSCR	
	Before soaking in PBS	After soaking in PBS	Before soaking in PBS	After soaking in PBS
	C, O, Ca, Si, Al, Mg and Br	C, O, Ca, Si and P	C, O, Ca, Si and Al	C, O, Ca, Si and P

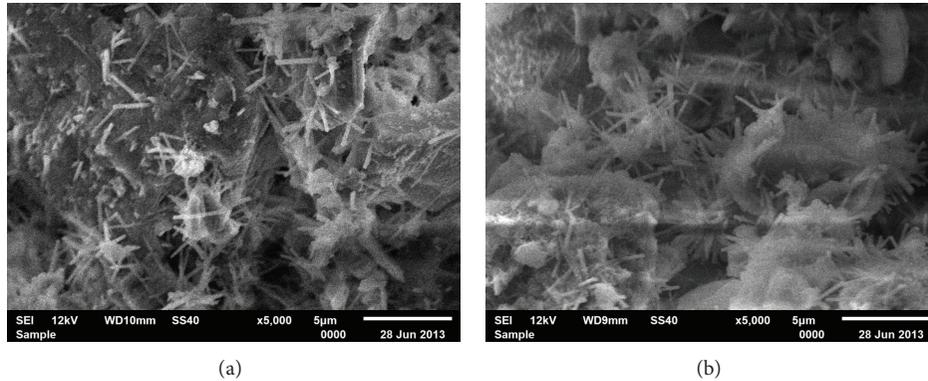


FIGURE 2: Scanning electron micrography by secondary electrons after hydration of cements, with honey-comb aspect of calcium silicate hydrate and needle-shaped ettringite crystals ((a) and (b)).

indicated in the EDS analyses; these crystals are rich in calcium and oxygen (Figure 3).

#### 4. Discussion

An ideal retrofilling material should promote sealing, present low solubility, be biocompatible, and demonstrate bioactive potential. Calcium silicate-based cements have good interaction with bone forming cells [24], and their bioactive potential [3] is responsible for the clinical success when these cements are used.

The replacement of  $\text{Bi}_2\text{O}_3$  by  $\text{ZrO}_2$  associated with Portland cement demonstrated adequate physical and mechanical properties and bioactivity [25, 26]. Another possibility of the use of  $\text{ZrO}_2$  is using it in its nanoparticulate form, because it demonstrated biocompatibility and cytocompatibility [27] and improved the mechanical and physical properties of the materials [28, 29].

Metals such as niobium have deserved their outstanding place for use in dental materials, because of presenting excellent resistance to corrosion, not being allergenic or toxic [30], and being biocompatible [20], in addition to showing the capacity to promote apatite formation [21]. In the nanoparticulate form  $\text{Nb}_2\text{O}_5$  presents antimicrobial activity [22].  $\text{CaWO}_4$  has been studied as a radiopacifying agent associated with Portland cement [9, 31] presenting adequate biocompatibility [9], in addition to not altering the mechanical property and final setting time of Portland cement [31].

Analysis of the size and shape of MTA particles showed that this cement presents a homogeneous surface and small sized particles [32]. Materials with smooth and regular surfaces may promote less tissue irritation [33]. Dammaschke et al. [34] affirmed that the surface characteristics of a material may indicate its biocompatibility, as it has a direct

influence on cell adhesion and distribution. According to Ha et al. [35] cements with smaller particles have greater disposition to absorb humidity. Salem Milani et al. [36] observed that when MTA cement comes into contact with body fluid, it presents hexagonal crystals with well-defined edges, amorphous crystals, and some of the needle type, unequally distributed throughout the entire material surface.

The cements evaluated and MTA cement are calcium silicate-based materials. All are derived from Portland cement; however, they present some differences in their composition and are manipulated with distilled water. The two calcium silicate-based cements used in this study had additives, pigments, and aggregates in their compositions, and the CSCR had a resin component. Scanning electron microscopy demonstrated that the CSCMs and CSCRs presented a surface morphology typical of Portland cement-based materials with particles of different sizes, while MTA had smaller and more homogeneous particles, according to Dammaschke et al. [34].

The radiopacifiers studied demonstrated different particle sizes and morphologies. The cements with particulate  $\text{ZrO}_2$  formed agglomerates with distinct morphologies, while the cements to which nanoparticulate  $\text{Nb}_2\text{O}_5$  was added presented smaller and more dispersed particles. The secondary electron micrography demonstrated the process of cement hydration, with the formation of calcium silicate hydrate and ettringite. EDS-X analysis of the MTA cements and two calcium silicate-based cements with different chemical compositions indicated that all the materials presented similarity in their components, such as the elements calcium, aluminum, and silicone. Asgary et al. [37] observed that Gray MTA presents crystals approximately 8 times larger than those of White MTA, which reveals that White MTA presents a mixture with a finer texture than Gray MTA. Furthermore, both cements present calcium, silicone, and bismuth in their composition.

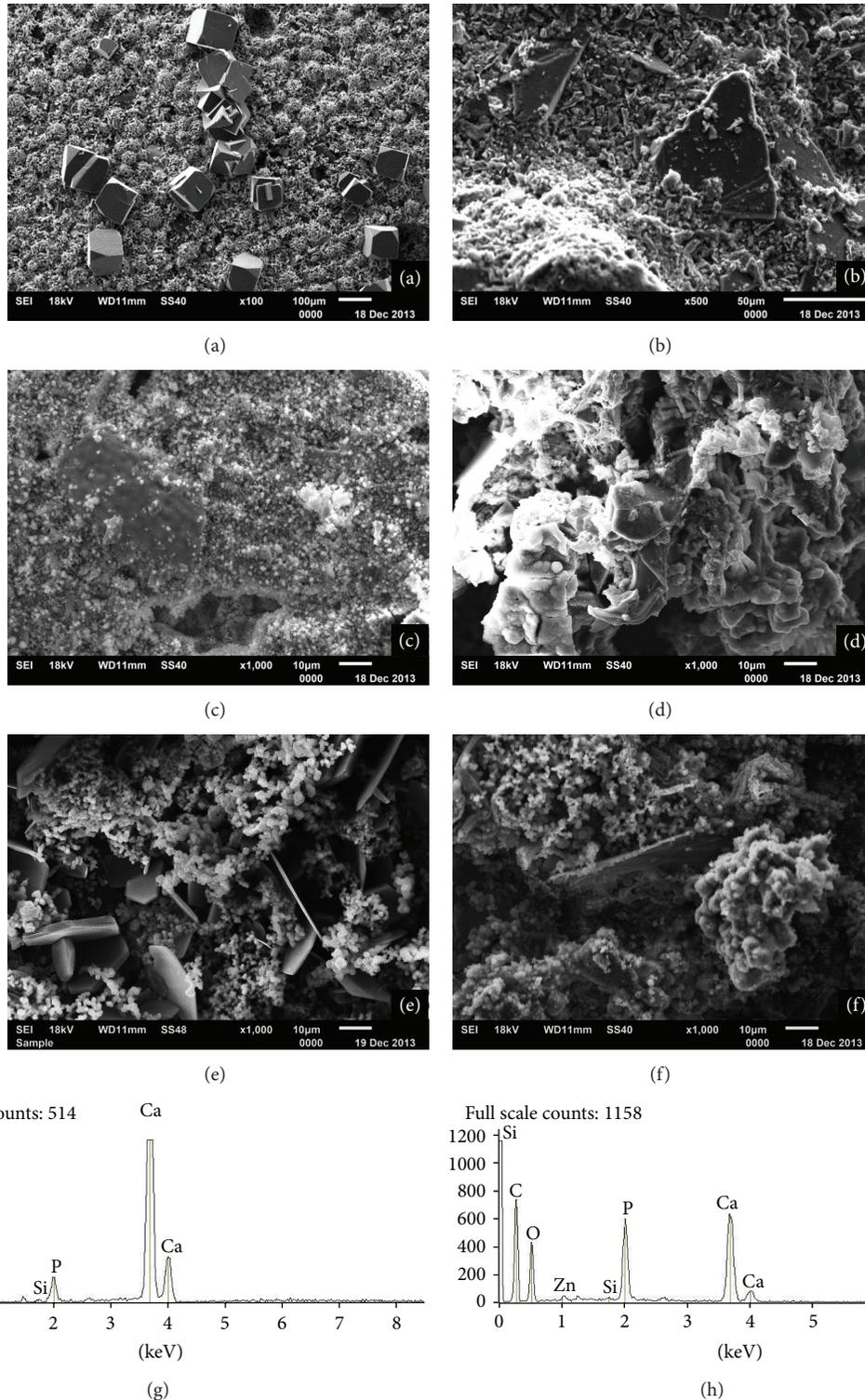


FIGURE 3: Secondary electron micrographs of (a) CSCM + ZrO<sub>2</sub> nano, (b) CSCR + ZrO<sub>2</sub> nano, (c) CSCM + Nb<sub>2</sub>O<sub>5</sub> micro, (d) CSCR + Nb<sub>2</sub>O<sub>5</sub> nano, (e) CSCM, and (f) CSCR, and energy dispersive X-ray spectrometry analysis of (g) CSCM and (h) CSCR after the materials were immersed in a standard phosphate buffered saline solution for 30 days.

According to the literature, the bioactivity of MTA has been attributed to its capacity of hydroxyapatite production, when it is in the presence of a phosphate solution [38]. Since the Ca<sup>2+</sup> and OH<sup>-</sup> resulting from the dissociation of calcium

hydroxide react with the phosphorous ions in the solution, this results in hydroxyapatite crystals on the surface of the material [39]. Therefore, the precipitation of hydroxyapatite *in vitro* on the surface of a material when it is in contact with a

phosphate solution indicates its bioactivity [40]. In this study was observed the bioactivity of the materials, regardless of the addition or not of the radiopacifier (Figure 3). Generally speaking, the cements presented a similar microstructure. Hexagonal or cubic crystals were also observed, which corresponded to the hydroxyapatite formed. The EDS analysis showed that these crystals were rich in calcium and oxygen and presented phosphate peak after hydration in standard phosphate buffered saline (Figure 3) that suggests an apatite formation.

The concept of bioactivity is intimately correlated with biointeractivity, that is, the capacity to exchange information within a biologic system [41]. This means that a bioactive material reacts chemically with the fluids of the body in a manner compatible with the tissue repair processes [42]. Formosa et al. [43], by means of scanning electron microscopy, dispersive energy X-ray, X-ray diffraction, and optical profilometry characterization techniques, observed that tricalcium silicate is more bioactive than Portland cement.

Greater presence of hydroxyapatite crystals was observed when the cements were associated with nanoparticulate  $ZrO_2$ . The high level of calcium and phosphorous deposition when the calcium silicate-based cements are associated with the  $ZrO_2$  nanoparticles indicates the formation of a layer of hydroxyapatite, thus reinforcing its bioactive potential. The greater degree of bioactivity of  $ZrO_2$  may be explained by the rapid dissolution of  $Ca^{2+}$  ions when in a phosphate solution and by the rapid nucleation of the  $Ca^{2+}$  and  $P^{5+}$  ions on the surface of the powder [18]. Previous studies [44, 45] have pointed out that nanoparticles present a higher degree of bioactivity than microparticles, which is in agreement with our findings.

## 5. Conclusions

Considering the results obtained in this study, all the associations presented a composition similar to that of MTA and presented bioactivity. Therefore, it was concluded that the calcium silicate-based cements evaluated presented the potential for use as an alternative to MTA when associated with the radiopacifiers studied.

## Conflict of Interests

The authors declare that they have no conflict of interests.

## Acknowledgment

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