Optimal Timing of Organs-at-risk-sparing Adaptive Radiation Therapy for Head-and-neck Cancer under Re-planning Resource Constraints

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Abstract.

Background and Purpose: Prior work on adaptive organ-at-risk (OAR)-sparing radiation therapy has typically reported outcomes based on fixed-number or fixed-interval replannings, which represent a one-size-fits-all approach and do not account for the variable progression of individual patients' toxicities. The purpose of this study was to determine the personalized optimal timing for re-planning in adaptive OAR-sparing radiation therapy, considering limited re-planning resources, specifically for patients with head and neck cancer (HNC).

Methods and Materials: A novel Markov decision process (MDP) model was developed to determine optimal timing of re-plannings based on the patient's expected toxicity, characterized by normal tissue complication probability (NTCP), for four toxicities. The MDP parameters were derived from a dataset comprising 52 HNC patients treated at the University of Texas MD Anderson Cancer Center between 2007 and 2013. Optimal replanning strategies were obtained when the permissible number of re-plannings throughout the treatment was limited to 1, 2, and 3.

Results: The MDP (optimal) solution recommended re-planning when the difference between planned and actual NTCPs (Δ NTCP) was greater than or equal to 1%, 2%, 2%, and 4% at treatment fractions 10, 15, 20, and 25, respectively, exhibiting a temporally increasing pattern. The Δ NTCP thresholds remained constant across the number of re-planning allowances (1, 2, and 3).

Conclusion: The MDP model determines the optimal timing for implementing patient-specific adaptive re-planning. This approach incorporates Δ NTCP thresholds and considers varying total re-plannings. The methods are versatile and applicable across cancer types, institutional settings, and different OARs and NTCP models.

Keywords: Personalized adaptive radiation therapy, organs-at-risk, normal tissue complication probability, Markov decision process, optimal strategy

1 Introduction

Advancements in radiation delivery techniques, such as intensity-modulated radiation therapy (IMRT) and volumetric-modulated arc therapy, enable accurate dose delivery to tumor targets while minimizing radiation exposure of the surrounding organs-at-risk (OARs) [1]. However, anatomical changes during the treatment, such as weight loss or tumor shrinkage, may cause the actual delivered dose to OARs to deviate from the planned dose. This can increase the risk of treatment-induced toxicities, particularly in cases where multiple OARs are in close proximity to the target, as in head and neck cancer (HNC) [2–4]. To address this, adaptive radiation therapy (ART) is clinically introduced, proposing on-therapy re-planning in response to anatomical changes in the target and OARs [5–10].

In practice, however, the clinical implementation of ART with daily (or even less-frequent) re-plannings remains limited, in large part due to the extensive human/personnel/workflow resources required to frequently perform key tasks such as segmentation and quality assurance as well as limited device accessibility time [11, 12]. Recent artificial intelligence (AI)-based algorithms (such as auto-segmentation or synthetically created CTs [13, 14] may mitigate some or all of these process level frictions; however, the integration of such AI tools within the ART workflow is still evolving [15]. With the advent of hybrid MR-Linac devices,

real-time adjustment of daily radiation plans, known as on-line ART, is now a possibility. On-line ART can also be enabled with the availability of high-frequency, high-quality conebeam CT or CT-on-Rails devices [16, 17]. Regardless of ART implementation imaging inputs (MR or CT), cancer centers in the U.S. typically have implemented ART at fixed intervals, notably once mid-therapy [18] and often as a 'verification' of re-simulation. Most of the relevant studies also report on the outcomes of only fixed-number and/or fixed-interval replannings [19–21] (see Table A1 for a comprehensive literature review). Such pre-determined schedules for treatment re-plannings, however, take a one-size-fits-all approach and do not account for the uncertain trajectory of individual patients' toxicities [21], nor patient-specific tumor regression. As a result, determining the optimal timing of re-planning episodes remains a crucial unmet need, particularly for OAR-sparing adaptive approaches (whether for MR-linac as we have implemented in MR-guided clinical trials [19] or for analogous CT-based approaches [20]).

Heukelom et al. [22] investigated the optimal implementation of ART with a single replanning allowance (in OAR-sparing radiation therapy) using daily on-treatment CT imaging with a CT-on-rails device. Leveraging the same dataset, this paper presents a new analytical approach for optimal re-planning strategies, based on Markov decision process (MDP) models, to identify the optimal timing for re-planning under different allowances in HNC. MDPs constitute a class of mathematical optimization models that aim to determine optimal decisions/actions in stochastic dynamic systems [23, 24]. MDPs are extensions of Markov models, which capture the natural evolution of a stochastic process (e.g., cancer progression) and are more commonly used in cancer research [25–27]. MDPs incorporate possible interventions (actions) into the stochastic process with the aim of obtaining desired outcomes at the end of a time horizon, by identifying an optimal course of actions. MDPs have been successfully employed to find the optimal timing for various medical interventions [27–31]; however, to our knowledge, MDPs have not been applied for triggering adaptive re-planning. By leveraging a mathematically optimal and rigorous decision process, we propose a method for evidence-based individualized radiation treatment re-planning, scalable across resourcerich and resource-limited facilities, and applicable to both CT- and MR-based platforms. Thus, rather than a class solution based on population estimates of toxicity reduction potential, we enable personalized adaptive therapy with awareness of a budget.

This study undertakes three specific aims: 1) Develop a generalized framework for the utilization of MDPs in budgeted re-planning decisions for efficient resource allocation in clinical settings, 2) identify the optimal timing of re-plannings based on changes in normal tissue complication probabilities (NTCP) of four toxicities: xerostomia, dysphagia, parotid gland dysfunction, and feeding tube dependency at 6 months post-treatment to enhance personalized treatment and efficacy, and 3) provide a foundation for future research efforts, which could extend the application of these methodologies to more dynamic treatment scenarios, such as GTV adaptive and/or online adaptive workflows, with the goal of achieving sufficient speed and flexibility for real-time clinical decision making. Through these aims,

we seek to not only refine the strategic application of ART but also to contribute to the broader discourse on improving cancer treatment outcomes through mathematical modeling and optimization.

2 Materials and Methods

2.1 Data

This study used a prior dataset of CT-on-Rails image-guided radiation therapy (IGRT), detailed by Heukelom et al. [22], which comprised information from patients treated for HNC at the University of Texas MD Anderson Cancer Center between 2007 and 2013; this retrospective secondary analysis was performed under MD Anderson Cancer Center Institutional Review Board approval (MDA RCR03-0800). The treatments involved (chemo-) radiotherapy with daily CT-on-Rails IGRT. Of the 52 patients, 36 were male and 16 were female. Among them, 46 patients were aged 18-65, while the remaining 6 were older than 65. The primary cancer sites were as follows: Larynx (1 patient), Oropharynx (13), Oral cavity (4), Hypopharynx (0), Nasopharynx (15), and Sinonasal (12). Treatment modalities included radiotherapy alone (16 patients), induction chemotherapy followed by radiotherapy (2), induction chemotherapy followed by concurrent chemoradiation (16), concurrent chemoradiation (14), and radiation plus Cetuximab (4). The patients' characteristics are summarized in Table 1.

For these 52 HNC patients, Heukelom et al. [22] calculated deviation of the actual dose from the planned dose for nine OARs at fractions 10 and 15 of the treatment. At each fraction, they estimated NTCP for the toxicities related to the OARs (xerostomia, dysphagia, parotid gland dysfunction, and tube feeding dependency at 6 months post-treatment) by projecting the actual dose through the remainder of the treatment period. Subsequently, they compared these findings with the planned NTCPs and determined the difference, i.e., Δ NTCP, for each toxicity. The NTCP models were presented in Supplementary Material B. For each observed Δ NTCP value, they reported the number of patients exhibiting that Δ NTCP or higher in any of the four NTCP models. The MDP model presented in this paper used the Δ NTCP from this dataset [22], which were summarized in Table 2.

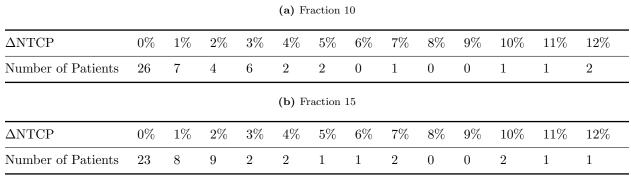
2.2 Decision Model

In the MDP model, estimates of an individual patient's toxicity outcome, as a function of the delivered radiation dose to OARs, determine the state of the system at each decision epoch during the treatment (e.g., day). Depending on the observed state, the clinician may decide between two possible actions: (1) Re-plan or (2) continue with the current plan. When the action is to continue with the current plan, the system may transition from one toxicity state to another stochastically, governed by transition probabilities. Re-planning changes the probabilistic transition towards more favorable outcomes/states. Given that a limited number of 're-planning' actions may be taken throughout the treatment, an optimal solution to the MDP identifies the optimal timing for taking such actions, as a function of the toxicity states. Fig. 1 illustrates an overview of the analysis method. The MDP model captures the stochastic evolution of post-treatment toxicity risk and identifies optimal re-planning times

Table 1: Patient characteristics. Abbreviations: cCRT = concurrent chemoradiation. RT = radiotherapy. TNM classification according to version 3. Accelerated RT: 2 Gy per fraction, 6 times per week.

| Variable | Number of Patients $= 52$ | Percentage |
|----------------------|---|------------|
| Sex | Male | 69% |
| | Female | 31% |
| Age | 18-65 years | 88% |
| | $\geq 65 \text{ years}$ | 12% |
| T-classification | Tis-T1 | 8% |
| | T2 | 15% |
| | Т3 | 13% |
| | T4 | 54% |
| | Recurrence | 8% |
| | Unknown | 2% |
| | Post-surgery | 23% |
| N-classification | N0 | 27% |
| | N1 | 19% |
| | N2 | 38% |
| | N3 | 2% |
| Primary site | Larynx | 2% |
| · | Oropharynx | 25% |
| | Oral cavity | 8% |
| | Hypopharynx | 0% |
| | Nasopharynx | 29% |
| | Sinonasal | 23% |
| Pathology | Adenocarcinoma | 2% |
| | Neuroblastoma | 6% |
| | Neuroendocrine | 8% |
| | Squamous cell carcinoma | 50% |
| | Undifferentiated carcinoma | 17% |
| | Other | 17% |
| Treatment modality | Radiotherapy alone | 31% |
| | Induction chemotherapy followed by RT | 4% |
| | Induction chemotherapy followed by cCRT | 31% |
| | Concurrent chemoradiation | 27% |
| | Radiation + Cetuximab | 8% |
| Baseline weight loss | No weight loss | 38% |
| <u> </u> | Moderate weight loss $(1-10\%)$ | 33% |
| | Severe weight loss (>10%) | 6% |
| | Unknown | 23% |
| Baseline xerostomia | No xerostomia | 4% |
| | Some xerostomia | 8% |
| | Unknown | 88% |
| Accelerated RT | Yes | 6% |

Table 2: Observed Δ NTCP values based on the difference between planned dose and actual dose, along with the number of patients associated with each Δ NTCP value. Adapted from [22] with permission.



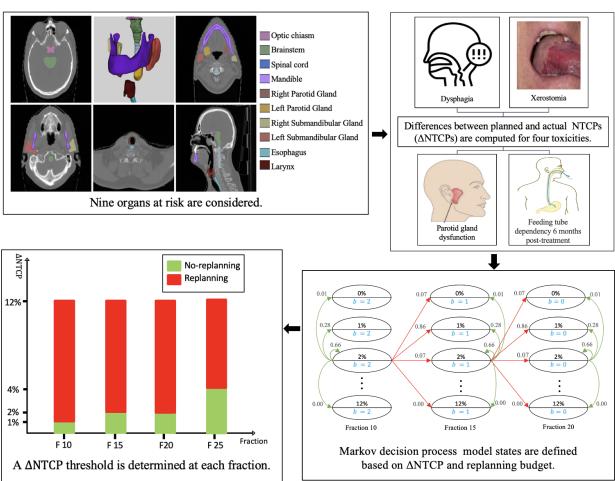


Fig. 1: Overview of the analysis method. The sub-figures displaying OARs and toxicities are adapted from [32] with permission.

to mitigate the toxicities (if necessary). The model components are as follows:

Re-plannings allowance: Depending on available resources for plan adaptations, the model considers a maximum number of re-plannings B that can be implemented throughout

the treatment. The analysis was performed for B = 1, 2, 3.

Decision epochs: Given a treatment period consisting of 33-35 fractions, the decision epochs were set at fractions 10, 15, 20, and 25. Prior studies have shown that anatomical changes are unlikely to happen very early during the treatment [22]; thus fraction 5 was omitted. Fraction 30 was also excluded due to its proximity to the end of treatment, with negligible impact on the total dose to the OARs.

States: At each decision epoch, the state of the system was captured by the pair $(\Delta \text{NTCP}, b)$, where ΔNTCP denotes the deviation of treatment toxicity from the planned value at that time, and $b \leq B$ is the number of remaining re-plannings. For example, if the maximum permissible number of re-plannings is 2 (B = 2), and the clinician opts to implement a re-planning at fraction 10, then the state of the system at fraction 15 will have b = 1. The ΔNTCP ranges from 0% to 12% in the model (Table 2).

Actions: At each decision epoch, two possible actions were included: (1) Re-planning, or (2) continue with the current plan (no re-planning). The stochastic transition of the toxicity state from one decision epoch to the next is a function of the action taken and is determined by the associated transition probabilities. Fig. 2 illustrates the states of the MDP and possible transitions associated with each action at Fractions 10, 15, and 20 along with the their smoothed transition probabilities, for the case that at most 2 re-plannings may be performed.

Transition Probabilities: The transition probabilities, governing the stochastic evolution of toxicity under each action, were estimated using the information presented in Table 2. Under the 'no re-planning' action, the probabilities for transitions from fraction 0 to 10 and from fraction 10 to 15 were directly estimated based on the number of patients in each Δ NTCP category. For example, the probability of transitioning from Δ NTCP = 0% at fraction 0 to $\Delta NTCP = 1\%$ at fraction 10 is 7/52 = 0.13, as 7 patients out of 52 exhibited such a change in Δ NTCP from fraction 0 to fraction 10. To make our transition probabilities more realistic with a broader spread and to avoid any deterministic transitions between states, we smoothed the transition probability matrix from Fraction 10 to 15 by convolving it with a Gaussian kernel function with standard deviation of 0.4. The original and smoothed probabilities associated with the 'no re-planning' action is presented in Supplementary Material C. It was assumed that transition probabilities from fraction 10 to 15 remained constant for subsequent decision epochs, due to the absence of reported Δ NTCP information beyond fraction 15 by Heukelom et al. [22]. To model the impact of the 're-planning' action on transition probabilities, it was assumed that, at each decision epoch, the action immediately decreases Δ NTCP to a value proportional to the elapsed treatment time. For example, if the 're-planning' action is taken at fraction 10 for $\Delta NTCP = 5\%$, then the state of toxicity will immediately decrease to $\Delta NTCP = 2\%$ at this fraction, as approximately one third of the treatment period has passed and the dose escalation will not continue through the rest of the treatment; see Fig. 3. Subsequently, the transition from fraction 10 to 15 is governed by the probabilities for $\Delta NTCP = 2\%$, calculated from Table 2. The probabilities associated

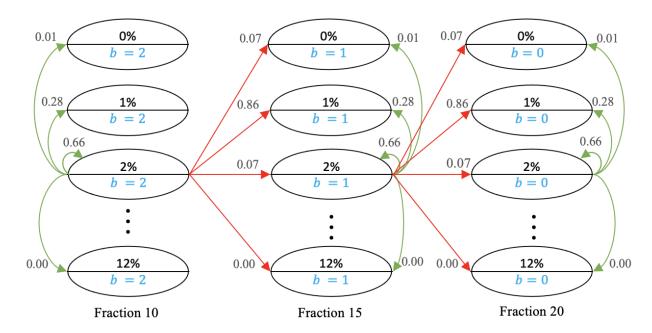


Fig. 2: Markov Decision Process Model. The permissible number of re-plannings is 2 (B = 2). The states are shown by ellipses. Δ NTCP values are located in the upper half of the ellipses, while the lower halves contain the value of b (the number of remaining re-plannings). Transitions between states are shown by green arrows when the action is 'no re-planning' and by red arrows when the action is 're-planning.' Not all arrows, states, and fractions are included to avoid ambiguity. For example, the smoothed transition probability from state (2%,2) state to (1%,1) when the action is 're-planning' is 0.86.

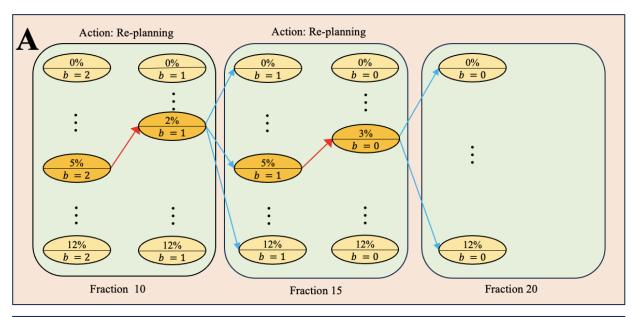
with the 're-planning' action, as described above, are presented in Supplementary Material C.

Rewards: For each set of consecutive actions taken at the decision epoch, the model considers the expected $-\Delta NTCP$ at the end of the treatment period (with respect to the transition probabilities) as the corresponding reward. The objective of the MDP is to maximize the expected reward by identifying an optimal set of actions, one at each decision epoch, as a function of the system's state. Because the rewards are defined by negative values in the MDP model, smaller end-treatment $\Delta NTCP$ values translate to higher rewards.

The MDP was solved using the MDPtoolbox of MATLAB [33], for B=1,2,3. The MATLAB code and its outputs are available at https://figshare.com/s/64bc3481737d17fc287e.

3 Results

After solving the MDP, the optimal policy, which specifies the optimal action ('re-planning' or 'no re-planning') for each state (Δ NTCP, b) at each decision epoch, was reported. The analysis revealed that the optimal policy is a single-threshold policy, where a specific Δ NTCP threshold is assigned to each fraction. Re-planning is triggered when the Δ NTCP exceeds the threshold, while no re-planning is needed when it falls below the threshold. That is, if the optimal action for Δ NTCP = x% at a certain decision epoch was to re-plan, then for



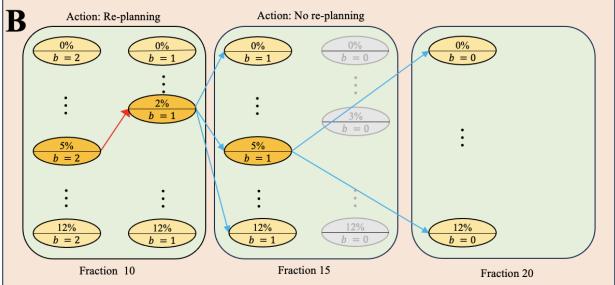


Fig. 3: Effect of actions on system transitions. The permissible number of re-plannings is 2 (B=2). The states are represented by ellipses. The Δ NTCP values are located in the upper halves of the ellipses, while the lower halves contain the value of b (the number of remaining re-plannings). When the action at a fraction is 're-planning,' as in Fractions 10 and 15 in Part A and Fraction 10 in Part B, the transition to a state with a lower Δ NTCP within the same fraction is shown with red arrows. Transitions between states from one fraction to the next are shown with blue arrows. When the action is 'no re-planning,' as in Fraction 15 in Part B, no transition occurs within that fraction. Instead, the system transitions to a new state at Fraction 20. This is depicted by the gray states at Fraction 15, indicating that there is no immediate decrease in Δ NTCP.

every other state with $\Delta \text{NTCP} = y\% > x\%$ and the same b, the optimal action was also to re-plan.

When only one re-planning was allowed (B=1), the optimal policy at fraction 10 was

Table 3: Optimal re-planning thresholds based on Δ NTCP and re-planning allowance.

| Re-planning allowance (B) | 1 | : | 2 | 3 | | | |
|--|----|----|----|----|----|----|--|
| Number of remaining re-plannings (b) | 1 | 2 | 1 | 3 | 2 | 1 | |
| Δ NTCP threshold at fraction 10 | 1% | 1% | - | 1% | - | - | |
| Δ NTCP threshold at fraction 15 | 2% | 2% | 2% | 2% | 2% | - | |
| Δ NTCP threshold at fraction 20 | 2% | 2% | 2% | 2% | 2% | 2% | |
| $\Delta {\rm NTCP}$ threshold at fraction 25 | 4% | 4% | 4% | 4% | 4% | 4% | |

to re-plan for any Δ NTCP value greater than or equal to 1%. Subsequently, at fraction 15, this threshold increased to 2% and remained at 2% for fraction 20. At fraction 25, the minimum Δ NTCP required for a re-planning was 4%. These thresholds remained the same in the optimal policies for B=2,3. The results are summarized in Table 3 and illustrated in Fig. 4 for B=3.

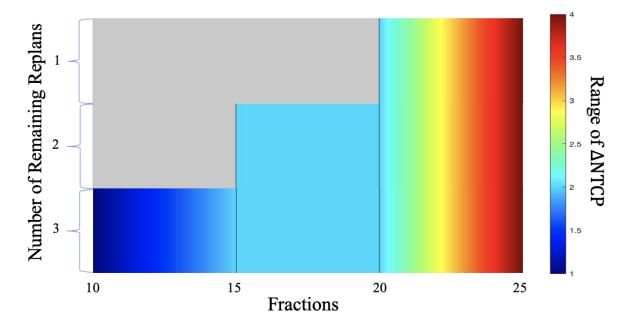


Fig. 4: Optimal \triangle NTCP thresholds for re-planning for B=3.

4 Discussion

This study introduces the first — to our knowledge — application of the mathematically rigorous MDP methodology, to determine optimal timing of ART in HNC. Although we focused on HNC as a use case, the methodology described in this paper is applicable to other radiotherapy cancer sites where an adaptive scheduling regimen is desired for a 'budget' of re-plans with estimable NTCP metrics. By incorporating prior Δ NTCP data from serial CT-based OAR metrics from Heukelom et al. [22] within the proposed MDP model, we have successfully derived an optimal policy for treatment re-planning. The MDP model guides

clinicians in determining the minimum values of Δ NTCP at fractions 10, 15, 20, and 25 for performing a re-planning, given a re-planning allowance of 1, 2, or 3 throughout the treatment.

The re-planning Δ NTCP threshold increases over time in the optimal policy, consistent with the diminishing impact of re-planning as the treatment progresses. These values are 1% at fraction 10, 2% at fractions 15 and 20, and 4% at fraction 25. Additionally, the results suggest optimality of re-planning for any changes in NTCP (Δ NTCP \geq 1) at fraction 10. This supports the findings of Heukelom et al. [22], who identified fraction 10 as the optimal time for a single re-planning. Importantly, at a given fraction, the Δ NTCP thresholds remain the same for different number of re-plannings (B=1,2,3); the re-planning allowance did not affect these thresholds. Furthermore, in cases where Δ NTCP at fraction 25 is below the 4% threshold, both options ('re-planning' or 'no re-planning') yield the same impact on the end-treatment Δ NTCP, indicating that re-planning does not result in an improvement.

We acknowledge that minimizing the expected Δ NTCP might suggest re-planning for any Δ NTCP value, potentially leading to a high number of false negatives. This arises from our modeling assumptions, which permit a fixed number of re-plannings at no cost, encouraging frequent re-planning due to low Δ NTCP thresholds. In an ongoing study, we are incorporating re-planning costs without limiting the number of re-plannings to better explore the trade-off between cost and benefit; however, at a minimum, we have opted to err on the side of patient benefit, rather than cost-control; as patient NTCP benefit is potentially scalable across any health system, while cost per re-plan and acceptable cost constraints are variable across national and international health policy and reimbursement systems.

The significance of a Δ NTCP of 4% or below lies in its potential impact on patient outcomes. While seemingly minor, even slight decreases in NTCP can have considerable implications for patient health and well-being. For instance, a reduction in severe toxicity such as osteoradionecrosis by just 4% could significantly enhance the quality of life and long-term survival prospects for patients. Moreover, customizing treatment to achieve such reductions underscores the importance of personalized care tailored to individual patient needs. By focusing on optimizing treatment outcomes at this level, healthcare practitioners can prioritize patient-centric approaches that aim to minimize treatment-related toxicity and maximize overall patient benefit.

We leveraged an existing CT-on-rails reference dataset [22] to objectively derive the Δ NTCP listed in the proposed MDP model. It is crucial to acknowledge the limitations regarding the generalizability of findings from this single-site retrospective in silico dataset. For instance, the in silico daily dose accumulation was not actively applied to individual patients, but rather calculated post hoc from a high-granularity CT-on-rails daily volumetric IGRT series. The CT-on-rails platform at MD Anderson utilized an in-house custom-contructed intermediary localization and alienation software (CT-Assisted Targeting (CAT)) [34]. Consequently, there were instances where delivered geometric shifts were either unrecorded or unrecoverable, or clearly aberrant (such as extensive shift records representing

an initial setup that was then revised after repositioning) during the secondary export of coordinate displacement to the commercial Record and Verify software (Mosaiq, Elekta AB). These discrepancies were subsequently omitted in the in silico model to streamline data, leading to conceptual gaps in the resultant NTCP modeling where these missing values were not accounted for. Furthermore, it is important to note that this modeled secondary dataset did not include adaptation or daily re-optimization of the initial daily dose in vivo. Consequently, the data presented in this paper should be viewed as a clinically approximate semi-synthetic illustrative use-case, rather than a definitive rationale for the large-scale implementation of the observed idealized re-planning thresholds across distinct operational platforms. Nonetheless, we believe that the resultant MDP model could be readily scaled using higher-quality prospective or observational cohort data for secondary validation. In essence, the data presented in this paper should be regarded as informative rather than definitive, and the individualized planning parameters suggested by MDP should be viewed as proof of concept rather than a formal criterion barring external validation.

In the prior work, Heukelom et al. [22] exclusively reported Δ NTCP for fractions 10 and 15, consistent with internal re-planning practices at MD Anderson Cancer Center based on data from a Phase II study by Maki et al. [35]. Consequently, for model extensibility in the current application, we have explicitly assumed transition probabilities remain stable for the subsequent epochs. This assumption introduces a known level of uncertainty that warrants consideration and is an area of future research, as it is unclear for specific OARs whether these transition states are indeed stable over therapy. Moreover, the MDP model stipulates weekly re-planning intervals on indexed fractions (e.g., fractions 10, 15, 20, 25, and 30) as a simplification for clarity of presentation reflective of our current adaptive protocols [19], but could readily be adapted to continuous daily fraction-based re-planning intervals.

The four NTCP models in Table B1 are among the most currently used models to calculate the NTCP values for the considered toxicities: xerostomia, dysphagia, parotid gland dysfunction, and feeding tube dependency at 6 months post-treatment [22, 36]. With the advent of more recent NTCP models for HNC radiation therapy, e.g., [37], it is possible that new NTCP models could offer improved estimations. In addition, the presented results are based on data collected from 52 HNC patients. While we recognize the importance of sample size in calibrating MDPs, this sample size is considered substantial in HNC research, considering that HNC accounts for only about 4% of cancer cases in the United States [38]. Furthermore, our results are contingent upon the available CT-on-Rails data, and future research may benefit from incorporating higher-dimensional data (e.g., GTV/the clinical target volume (CTV) modifying approaches, MRI anatomic and/or biomarker data for TCP/NTCP) for a more extensive insight.

Nonetheless, the proposed MDP model for ART is clinically relevant, mathematically rigorous, resource-aware, and scalable, and can be adjusted based on new OAR toxicity with reference NTCP values. Necessarily, the precision of the model relies on accurate calculations of NTCP, particularly when adhering to rigorous criteria that determine whether

patients are suitable for or excluded from ART [39]. Despite the challenges and limitations, our study introduces novel contributions to the field of ART. Unlike previous works [22], which primarily considered a single re-planning allowance, our optimization model extends its applicability to scenarios with multiple re-plannings. Furthermore, our optimal policy spans across fractions 10, 15, 20, and 25, representing an advancement beyond the limited scope of Heukelom et al. [22], which only reported results for fractions 10 and 15. Gan et al. [40] achieved optimal timing for re-planning in HNC radiation therapy by analyzing weekly dose data through semi-auto segmentation and the K-nearest-neighbour method. They constructed a dose deviation map to visualize differences between planned and actual doses, simulating different ART scenarios. By evaluating accumulated dose differences before and after re-planning, the optimal timing for re-planning was determined. Our methodology differs in that we incorporate Δ NTCP and utilize it to develop an MDP model for determining the optimal timing for re-planning.

An aspect not explored in this study is the adaptation based on GTV or CTV modification, either for shrinking GTV/CTVs [19] or isotoxic boost approaches [41, 42]; we concentrated solely on OAR-based adaptation. Adapting based on GTV could open avenues for optimal re-plannings, potentially influencing NTCP and extending into scenarios such as Stereotactic Body RT [43]. This introduces a distinctive problem and solution space beyond the scope of our current investigation. Furthermore, we exclusively focused on optimizing the ART workflow within the context of photon therapy. Similar optimization methodologies could prove advantageous when exploring ART in the context of proton therapy, particularly in addressing setup variability reduction [44]. For this study, NTCP calculations were based on the 'plan of the day.' While our findings may vary with deformable dose registration, the operational implementation remains consistent. Future efforts should consider incorporating deformable dose registration to enhance the model's generalization.

Several surveys in both low/middle-income countries [45, 46] and high-income economies [45] have identified resource constraints as an impediment to ART implementation; the use of models such as our MDP provides a potential avenue for stratification of resource allocation. Put simply, with one re-plan allowed, almost all patients would be best served via re-planning early during treatment; however, as the budget of re-planning staff/technical/time resources expand, evidence-based personalized re-planning is potentiated by our MDP approach.

5 Conclusion

Our study introduced an MDP model to guide clinicians in determining the optimal timing for implementing patient-specific adaptive re-planning. This approach incorporates Δ NTCP thresholds and considers varying total re-plannings. We also presented a novel in silico application and accompanying code specifically developed to attain improved Δ NTCP thresholds for consequential re-planning to alleviate toxicities throughout the course of treatment. Our methods have wide-ranging applicability, transcending specific cancer types and being adaptable to diverse institutional settings with limited resources. Additionally,

our approach accommodates different OARs and NTCP models, emphasizing its versatility and potential for widespread implementation across a spectrum of clinical contexts.

Contributor Roles Taxonomy (CRediT) Attribution Statement

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References

- [1] N. A. Iacovelli et al. Role of IMRT/VMAT-based dose and volume parameters in predicting 5-year local control and survival in nasopharyngeal cancer patients. *Frontiers in Oncology*, 10:518110, 2020.
- [2] J. L. Barker Jr et al. Quantification of volumetric and geometric changes occurring during fractionated radiotherapy for head-and-neck cancer using an integrated CT/linear accelerator system. *International Journal of Radiation Oncology, Biology, Physics*, 59(4):960–970, 2004.
- [3] M. Beltran, M. Ramos, J. J. Rovira, S. Perez-Hoyos, M. Sancho, E. Puertas, S. Benavente, M. Ginjaume, and J. Giralt. Dose variations in tumor volumes and organs at risk during IMRT for head-and-neck cancer. *Journal of Applied Clinical Medical Physics*, 13(6):3723, 2012.
- [4] W. Chen, P. Bai, J. Pan, Y. Xu, and K. Chen. Changes in tumor volumes and spatial locations relative to normal tissues during cervical cancer radiotherapy assessed by cone beam computed tomography. *Technology in Cancer Research and Treatment*, 16(2):246–252, 2017.
- [5] B. M. Beadle and A. W. Chan. The potential of adaptive radiotherapy for patients with head and neck cancer-too much or not enough? *JAMA Oncology*, 9(8):1064–1065, 2023.
- [6] J. Castelli, A. Simon, C. Lafond, N. Perichon, B. Rigaud, E. Chajon, B. De Bari, M. Ozsahin, J. Bourhis, and R. de Crevoisier. Adaptive radiotherapy for head and neck cancer. *Acta Oncology*, 57(10):1284–1292, 2018.
- [7] M. Figen, D. Çolpan Öksüz, E. Duman, R. Prestwich, K. Dyker, K. Cardale, S. Ramasamy, P. Murray, and M. Şen. Radiotherapy for head and neck cancer: Evaluation of triggered adaptive replanning in routine practice. *Frontiers in Oncology*, 59(4):960–970, 2020.
- [8] K. Håkansson, E. Giannoulis, A. Lindegaard, J. Friborg, and I. Vogelius. Assessment of CBCT-based synthetic CT generation accuracy for adaptive radiotherapy planning. *Acta Oncologica (Stockholm, Sweden)*, 62(11):1369–1374, 2023.
- [9] E. Lavrova, M. D. Garrett, Y. F. Wang, C. Chin, C. Elliston, M. Savacool, M. Price, L. A. Kachnic, and D. P. Horowitz. Adaptive radiation therapy: A review of CT-based techniques. *Radiology. Imaging Cancer*, 5(4):e230011, 2023.
- [10] C. J. O'Hara, D. Bird, B. Al-Qaisieh, and R. Speight. Assessment of CBCT-based synthetic CT generation accuracy for adaptive radiotherapy planning. *Journal of Applied Clinical Medical Physics*, 23(11):e13737, 2022.
- [11] K. K. Brock. Adaptive radiotherapy: Moving into the future. Seminars in Radiation Oncology, 29(3):181–184, 2019.
- [12] K. A. Wahid et al. Harnessing uncertainty in radiotherapy auto-segmentation quality assurance. *Physics and Imaging in Radiation Oncology*, 29:100526, 2023.
- [13] C. Allen, A. U. Yeo, N. Hardcastle, and R. D. Franich. Evaluating synthetic computed tomography images for adaptive radiotherapy decision making in head and neck cancer.

- Physics and Imaging in Radiation Oncology, 27:100478, 2023.
- [14] V. T. Taasti et al. Clinical evaluation of synthetic computed tomography methods in adaptive proton therapy of lung cancer patients. *Physics and Imaging in Radiation Oncology*, 27:100459, 2023.
- [15] E. Huynh, A. Hosny, C. Guthier, S. F. Bitterman, D. A. Hass-Kogan, B. Kann, H. J. W. L. Aerts, and R. H. Mak. Artificial intelligence in radiation oncology. *Nature Reviews Clinical Oncology*, 17:771–781, 2020.
- [16] A. J. van de Schoot, D. Hoffmans, K. M. van Ingen, M. J. Simons, and J. Wiersma. Characterization of Ethos therapy systems for adaptive radiation therapy: A multimachine comparison. *Journal of Applied Clinical Medical Physics*, 24:e13905, 2023.
- [17] Varian Ethos. https://www.varian.com. Accessed: 24 February, 2024.
- [18] R. Avgousti, C. Antypas, C. Armpilia, F. Simopoulou, Z. Liakouli, P. Karaiskos, V. Kouloulias, E. Kyrodimos, L. A. Moulopoulos, and A. Zygogianni. Adaptive radiation therapy: When, how and what are the benefits that literature provides? Cancer Radiotherapie: Journal de la Societe Francaise de Radiotherapie Oncologique, 26(4):622–636, 2022.
- [19] H. Bahig et al. Magnetic resonance-based response assessment and dose adaptation in human papilloma virus positive tumors of the oropharynx treated with radiotherapy (MR-ADAPTOR): An R-IDEAL stage 2a-2b/Bayesian phase II trial. Clinical and Translational Radiation Oncology, 13:19–23, 2018.
- [20] J. Castelli et al. Weekly adaptive radiotherapy vs standard intensity-modulated radiotherapy for improving salivary function in patients with head and neck cancer: A phase 3 randomized clinical trial. *JAMA Oncology*, 9(8):1056–1064, 2023.
- [21] J. M. Westerhoff et al. Safety and tolerability of online adaptive high-field magnetic resonance—guided radiotherapy. *JAMA Network Open*, 7(5):e2410819—e2410819, 2024.
- [22] J. Heukelom et al. Differences between planned and delivered dose for head and neck cancer, and their consequences for normal tissue complication probability and treatment adaptation. *Radiotherapy and Oncology*, 142:100–106, 2020.
- [23] E. A. Feinberg and A. Shwartz. *Handbook of Markov Decision Processes: Methods and Applications*. Springer, 2002.
- [24] M. L. Puterman. Markov Decision Processes: Discrete Stochastic Dynamic Programming. Wiley-Interscience, 2005.
- [25] J. R. Beck and S. G. Pauker. The Markov process in medical prognosis. *Medical Decision Making*, 3(4):419–458, 1983.
- [26] K. M. Kuntz, L. B. Russell, D. K. Owens, G. D. Sanders, T. A. Trikalinos, and J. A. Salomon. Decision models in cost-effectiveness analysis. Cost-Effectiveness in Health and Medicine. New York, NY: Oxford University Press, 2016.
- [27] S. P. Ng et al. Surveillance imaging for patients with head and neck cancer treated with definitive radiotherapy: A partially observed Markov decision process model. *Cancer*, 126(4):749–756, 2020.

- [28] O. Alagoz, H. Hsu, A. J. Schaefer, and M. S. Roberts. Markov decision processes: A tool for sequential decision making under uncertainty. *Medical Decision Making: An International Journal of the Society for Medical Decision Making*, 30(4):474–483, 2010.
- [29] O. Alagoz, L. M. Maillart, A. J. Schaefer, and M. S. Roberts. The optimal timing of living-donor liver transplantation. *Management Science*, 50(10):1420–30, 2004.
- [30] B. T. Denton, M. Kurt, N. D. Shah, S. C. Bryant, and S. A. Smith. Optimizing the start time of statin therapy for patients with diabetes. *Medical Decision Making*, 29(3):351–67, 2009.
- [31] S. M. Shechter, M. D. Bailey, A. J. Schaefer, and M. S. Roberts. The optimal time to initiate HIV therapy under ordered health states. *Operations Research*, 56(1):20–33, 2008.
- [32] C. D. Fuller. Introduction to Radiation Oncology. https://doi.org/10.6084/m9.figshare.22582207.v1. Accessed: 24 February, 2024.
- [33] The MathWorks Inc. MATLAB version: 9.13.0 (R2022b), 2022.
- [34] L. Zhang, L. Dong, L. Court, H. Wang, M. Gillin, and R. Mohan. TU-EE-A4-05: Validation of CT-assisted targeting (CAT) software for soft tissue and bony target localization. *Journal of Applied Clinical Medical Physics*, 32:2106–2106, 2005.
- [35] R. G. Maki et al. Phase II study of sorafenib in patients with metastatic or recurrent sarcomas. *Journal of Clinical Oncology: Official Journal of the American Society of Clinical Oncology*, 27(19):3133–3140, 2009.
- [36] S. Stieb, A. Lee, L. V. van Dijk, S. Frank, C. D. Fuller, and P. Blanchard. NTCP modeling of late effects for head and neck cancer: A systematic review. *International Journal of Particle Therapy*, 8(1):95–107, 2021.
- [37] S. Hosseinian, M. Hemmati, C. Dede, T. C. Salzillo, L. V. van Dijk, A. S. R. Mohamed, S. Y. Lai, A. J. Schaefer, C. D. Fuller, Rice/MD Anderson Center for Operations Research in Cancer (CORC), and MD Anderson Head & Neck Cancer Symptom Working Group. Cluster-based toxicity estimation of osteoradionecrosis via unsupervised machine learning: Moving beyond single dose-parameter normal tissue complication probability by using whole dose-volume histograms for cohort risk stratification. *International Journal of Radiation Oncology, Biology, Physics*, 2024.
- [38] Head and Neck Cancer: Statistics. https://www.cancer.net/cancer-types/head-and-neck-cancer/statistics. Accessed: 24 February, 2024.
- [39] Y. Gan, J. A. Langendijk, A. van der Schaaf, L. van den Bosch, E. Oldehinkel, Z. Lin, S. Both, and C. L. Brouwer. An efficient strategy to select head and neck cancer patients for adaptive radiotherapy. *Radiotherapy and Oncology: Journal of the European Society for Therapeutic Radiology and Oncology*, 186:109763, 2023.
- [40] Y. Gan, J. A. Langendijk, E. Oldehinkel, Z. Lin, S. Both, and C. L. Brouwer. Optimal timing of re-planning for head and neck adaptive radiotherapy. *Journal of the European Society for Therapeutic Radiology and Oncology*, 194:110145, 2024.
- [41] J. Heukelom et al. Adaptive and innovative radiation treatment for improving

- cancer treatment outcome (ARTFORCE); a randomized controlled phase II trial for individualized treatment of head and neck cancer. *BMC Cancer*, 13:84, 2013.
- [42] A. D. Leeuw et al. Acute toxicity in ARTFORCE: A randomized phase III dose-painting trial in head and neck cancer. *International Journal of Radiation Oncology*Biology*Physics*, 114(3):S98, 2022.
- [43] I. Mohamad et al. The evolving role of stereotactic body radiation therapy for head and neck cancer: Where do we stand? *Cancers (Basel)*, 15(20):5010, 2023.
- [44] A. Lalonde, M. Bobić, G. C. Sharp, I. Chamseddine, B. Winey, and H. Paganetti. Evaluating the effect of setup uncertainty reduction and adaptation to geometric changes on normal tissue complication probability using online adaptive head and neck intensity modulated proton therapy. *Physics in Medicine and Biology*, 68(11):115018, 2023.
- [45] J. Bertholet et al. Patterns of practice for adaptive and real-time radiation therapy (POP-ART RT) part II: Offline and online plan adaption for interfractional changes. Radiotherapy and Oncology: Journal of the European Society for Therapeutic Radiology and Oncology, 153:88–96, 2020.
- [46] L. M. Yap, Z. Jamalludin, A. H. Ng, and N. M. Ung. A multi-center survey on adaptive radiation therapy for head and neck cancer in Malaysia. *Physical and Engineering Sciences in Medicine*, 46(3):1331–1340, 2023.
- [47] S. Y. Lim, A. Tran, A. N. K. Tran, A. Sobremonte, C. D. Fuller, L. Simmons, and J. Yang. Dose accumulation of daily adaptive plans to decide optimal plan adaptation strategy for head-and-neck patients treated with MR-Linac. *Medical Dosimetry: Official Journal of the American Association of Medical Dosimetrists*, 47(1):103–109, 2022.
- [48] B. A. McDonald et al. Initial feasibility and clinical implementation of daily MR-guided adaptive head and neck cancer radiation therapy on a 1.5T MR-Linac system: Prospective R-IDEAL 2a/2b systematic clinical evaluation of technical innovation. International Journal of Radiation Oncology, Biology, Physics, 109(5):1606–1618, 2021.
- [49] F. C. J. Reinders, M. de Ridder, P. A. H. Doornaert, C. P J Raaijmakers, and M. E. P. Philippens. Individual elective lymph node irradiation for the reduction of complications in head and neck cancer patients (iNode): A phase-I feasibility trial protocol. *Clinical and Translational Radiation Oncology*, 39:100574, 2022.
- [50] H. Kee et al. Optimising radiation therapy in head and neck cancers using functional image-guided radiotherapy and novel biomarkers. https://clinicaltrials.gov/ct2/ show/NCT04242459?cond=NCT04242459&draw=2&rank=1. Accessed: 16 September, 2024.
- [51] A. Ciarmatori, N. Maffei, G. M. Mistretta, P. Ceroni, A. Bernabei, B. Meduri, E. D'Angelo, A. Bruni, P. Giacobazzi, F. Lohr, and G. Guidi. Evaluation of the effectiveness of novel single-intervention adaptive radiotherapy strategies based on daily dose accumulation. *Medical Dosimetry: Official Journal of the American Association of Medical Dosimetrists*, 44(4):379–384, 2019.
- [52] N. Maffei et al. SIS epidemiological model for adaptive RT: Forecasting the parotid

- glands shrinkage during tomotherapy treatment. Medical physics, 43(7):4294, 2016.
- [53] X. Wang, J. Lu, X. Xiong, G. Zhu, H. Ying, S. He, W. Hu, and C. Hu. Anatomic and dosimetric changes during the treatment course of intensity-modulated radiotherapy for locally advanced nasopharyngeal carcinoma. *Medical Dosimetry: Official Journal of the American Association of Medical Dosimetrists*, 35(2):151–157, 2010.
- [54] S. A. A. Gros, A. P. Santhanam, A. M. Block, B. Emami, B. H. Lee, and C. Joyce. Retrospective clinical evaluation of a decision-support software for adaptive radiotherapy of head and neck cancer patients. *Frontiers in Oncology*, 12:777793, 2022.
- [55] M. N. Duma, S. Kampfer, T. Schuster, C. Winkler, and H. Geinitz. Adaptive radiotherapy for soft tissue changes during helical tomotherapy for head and neck cancer. *Strahlentherapie und Onkologie*, 188(3):243–247, 2012.
- [56] W. W. Fung, V. W. Wu, and P. M. Teo. Dosimetric evaluation of a three-phase adaptive radiotherapy for nasopharyngeal carcinoma using helical tomotherapy. *Medical Dosimetry: Official Journal of the American Association of Medical Dosimetrists*, 37(1):92–97, 2012.
- [57] Y. C. Kuo, T. H. Wu, T. S. Chung, K. W. Huang, K. S. Chao, W. C. Su, and J. F. Chiou. Effect of regression of enlarged neck lymph nodes on radiation doses received by parotid glands during intensity-modulated radiotherapy for head and neck cancer. American Journal of Clinical Oncology, 29(6):600–605, 2006.
- [58] E. K. Hansen, M. K. Bucci, J. M. Quivey, V. Weinberg, and P. Xia. Repeat CT imaging and replanning during the course of IMRT for head-and-neck cancer. *International Journal of Radiation Oncology, Biology, Physics*, 64(2):355–362, 2006.
- [59] L. Capelle, M. Mackenzie, C. Field, M. Parliament, S. Ghosh, and R. Scrimger. Adaptive radiotherapy using helical tomotherapy for head and neck cancer in definitive and postoperative settings: Initial results. *Clinical Oncology (Royal College of Radiologists (Great Britain)*, 24(3):208–215, 2012.
- [60] E. Brown, S. Porceddu, R. Owen, and F. Harden. Developing an adaptive radiotherapy technique for virally mediated head and neck cancer. *Journal of Medical Imaging and Radiation Sciences*, 44(3):134–140, 2013.
- [61] J. Castelli et al. Impact of head and neck cancer adaptive radiotherapy to spare the parotid glands and decrease the risk of xerostomia. *Radiation Oncology*, 10(6), 2015.
- [62] E. Brown, R. Owen, F. Harden, K. Mengersen, K. Oestreich, W. Houghton, M. Poulsen, S. Harris, C. Lin, and S. Porceddu. Head and neck adaptive radiotherapy: Predicting the time to replan. Asia-Pacific Journal of Clinical Oncology, 12(4):460–467, 2016.
- [63] F. Aly, A. A. Miller, M. G. Jameson, and P. E. Metcalfe. A prospective study of weekly intensity modulated radiation therapy plan adaptation for head and neck cancer: Improved target coverage and organ at risk sparing. *Australasian Physical and Engineering Sciences in Medicine*, 42(1):43–51, 2019.
- [64] M. Bobić, A. Lalonde, G. C. Sharp, C. Grassberger, J. M. Verburg, B. A. Winey, A. J. Lomax, and H. Paganetti. Comparison of weekly and daily online adaptation for

- head and neck intensity-modulated proton therapy. *Physics in Medicine and Biology*, 66(5):10.1088/1361-6560/abe050, 2021.
- [65] A. Gupta, A. Dunlop, A. Mitchell, D. McQuaid, S Nill, H. Barnes, K. Newbold, C. Nutting, S. Bhide, U. Oelfke, K. J. Harrington, and K. H. Wong. Online adaptive radiotherapy for head and neck cancers on the MR linear accelerator: Introducing a novel modified adapt-to-shape approach. Clinical and Translational Radiation Oncology,, 32:48–51, 2021.
- [66] I. Beetz. NTCP models for patient-rated xerostomia and sticky saliva after treatment with intensity modulated radiotherapy for head and neck cancer: The role of dosimetric and clinical factors. *Radiother Oncology*, 105(1):101–106, 2012.
- [67] K. Wopken. Development of a multivariable normal tissue complication probability (NTCP) model for tube feeding dependence after curative radiotherapy/chemoradiotherapy in head and neck cancer. *Radiother Oncology*, 113(1):95–101, 2014.
- [68] T. Dijkema, C. P. Raaijmakers, R. K. Ten Haken, J. M. Roesink, P. M. Braam, A. C. Houweling, M. A. Moerland, A. Eisbruch, and C. H. Terhaard. Parotid gland function after radiotherapy: The combined Michigan and Utrecht experience. *International Journal of Radiation Oncology, Biology, Physics*, 78(2):449–453, 2010.
- [69] J. T. Lyman. Complication probability as assessed from dose-volume histograms. Radiation Research. Supplement, 8:S13-9, 1985.
- [70] G. J. Kutcher and C. Burman. Calculation of complication probability factors for non-uniform normal tissue irradiation: The effective volume method. *International Journal of Radiation Oncology, Biology, Physics*, 16(6):1623–1630, 1989.
- [71] M. E. M. C. Christianen. Predictive modelling for swallowing dysfunction after primary (chemo) radiation: Results of a prospective observational study. Radiotherapy and Oncology: Journal of the European Society for Therapeutic Radiology and Oncology, 105(1):107–114, 2012.

Supplementary Material A. Literature Review on Head-and-neck-cancer Adaptive Radiation Therapy

Table A1: A comprehensive list of relevant papers on head-and-neck-cancer ART along with the number of re-planning instances and the reported fractions.

| Paper | Number of Re-plannings and Fractions |
|------------------------|--|
| Castelli et al. [20] | Replan weekly |
| Lim et al. [47] | Replan at F14 based on parotid dose |
| McDonald et al. [48] | Simulated replans at F1, F10, F20, F30. |
| | Patient replans at F6 due to weight loss and at F8, F24, F26 due to shoulder mass loss |
| Reinders et al. [49] | Adapt-to-position every five fraction, adapt-to-shape at beginning of the week |
| Kee et al. [50] | Replan at week 2 and 4, Increase dose at F10 based on apparent diffusion coefficient |
| Ciarmatori et al. [51] | Single replan at F18 |
| Maffei et al. [52] | Optimal replan at F18 |
| Wang et al. [53] | Single replan at F18 |
| Gros et al. [54] | Optimal replan between F1 and F23 |
| Duma et al. [55] | Replan varied from F6 to F20 |
| Fung et al. [56] | Replan after F25 and F35 |
| Kuo et al. [57] | Replan after F25 |
| Hansen et al. [58] | Replan after F19 \pm 6 |
| Capelle et al. [59] | Replan at F20 |
| Brwon et al. [60] | Median (CT) re-planning at F22 and source-to-skin distance corrections at F26 |
| Castelli et al. [61] | Replan weekly |
| Brown et al. [62] | Median re-planning at F11 for nasopharyngeal and F20 for oropharyngeal |
| Aly et al. [63] | Replan weekly |
| Figen et al. [7] | Mean replan at F15 |
| Bobić et al. [64] | Replan weekly |
| Gupta et al. [65] | Replan daily |

Supplementary Material B. NTCP Models

Table B1: The employed NTCP models for xerostomia, dysphagia, parotid gland dysfunction, and feeding tube dependency at 6 months post-treatment.

1. NTCP model for moderate to severe xerostomia at 6 months [66].

NTCP =
$$(1 + e^{-S})^{-1}$$
, where

S = -1.443 + (mean dose to contralateral parotid * 0.047) + (baseline xerostomia score * 0.720).Baseline xerostomia is 0 (none) or 1 (a bit).

2. NTCP model for physician rated feeding tube dependency at 6 months [67]

NTCP =
$$(1 + e^{-S})^{-1}$$
, where

- S = -11.70 + (advanced T-stage * 0.43) + (moderate weight loss * 0.95)
- + (severe weight loss * 1.63) + (accelerated radiotherapy * 1.20) + (chemoradiation * 1.91)
- + (radiotherapy plus cetuximab * 0.56) + (mean dose PCM superior *0.071)
- + (mean dose PCM inferior * 0.034) + (mean dose contralateral parotid * 0.006)
- + (mean dose cricopharyngeal muscle * 0.023).

The dose variables are in Gy, and for all the other variables 0 (no) or 1 (yes) are filled in.

3. NTCP model for physician rated decreased salivary flow using the mean dose model [68–70].

NTCP
$$=\frac{1}{\sqrt{2\pi}} \int_{-\infty}^{u} e^{\frac{-t^2}{2}} dt$$
, where $u = \frac{D-TD_{50}}{mTD_{50}}$

NTCP $=\frac{1}{\sqrt{2}\pi}\int_{-\infty}^{u}e^{\frac{-t^2}{2}}dt$, where $u=\frac{D-TD_{50}}{mTD_{50}}$, D is the mean parotid dose, TD_{50} is the dose resulting in 50% complication probability and mdetermines the slope of the model. The employed parameters were TD_{50} =39.9 Gy and m=0.4.

4. NTCP model for dysphagia (grade 2-4 swallowing dysfunction according to the RTOG/EORTC Late Radiation Morbidity Scoring Criteria, physician rated 6 months after treatment) [71].

$$NTCP = (1 + e^{-S})^{-1}$$
, where

S = -6.09 + (mean dose PCM superior * 0.057) + (mean dose supraglottic larynx * 0.037).

Supplementary Material C. Transition Probabilities

Action 1: No re-planning

The natural transition probabilities from fraction 0 (pre-treatment) to fraction 10 were directly estimated using the information provided in Table 2. For each Δ NTCP category, the ratio of the corresponding number of patients at fraction 10 to the total of 52 patients was taken as the associated transition probability. We note that all patients exhibit Δ NTCP = 0% at fraction 0. These probabilities apply only to the states with the same number of remaining re-plannings b, by the definition of the 'no re-planning' action. The transition probabilities are presented in Table C1.

Table C1: Transition probabilities from fraction 0 (F0) to fraction 10 (F10) under 'no re-planning.'

| Δ NTCP @ F10 \rightarrow | 0% | 1% | 2% | 3% | 4% | 5% | 6% | 7% | 8% | 9% | 10% | 11% | 12% |
|-----------------------------------|------|------|------|------|------|------|------|------|------|------|------|------|------|
| Δ NTCP @ F0 \downarrow | | | | | | | | | | | | | |
| 0% | 0.50 | 0.13 | 0.08 | 0.11 | 0.04 | 0.04 | 0.00 | 0.02 | 0.00 | 0.00 | 0.02 | 0.02 | 0.04 |

The natural transition probabilities from fraction 10 to fraction 15 were estimated in a similar manner. As the number of patients in each $\Delta NTCP$ category at fraction 15 were aggregated, a mapping from $\Delta NTCP$ categories at fraction 10 to those of fraction 15 was established. To ensure a feasible map, it was assumed that $\Delta NTCP$ s may slightly improve (1%) on its own, without intervention. The necessity of this assumption may be observed by the number of patients with $\Delta NTCP = 12\%$ at Fraction 10 and 15 in Table 2; two patients exhibited $\Delta NTCP = 12\%$ at fraction 10, while this number at fraction 15 was one patient. As no patient showed $\Delta NTCP = 6\%, 8\%, 9\%$ at fraction 10, it was assumed that the patients in these categories retain the same $\Delta NTCP$ at fraction 15 with probability 1. The transition probabilities are presented in Table C2.

Table C2: Transition probabilities from fraction 10 (F10) to fraction 15 (F15) under 'no re-planning.' The same probabilities apply to subsequent transitions, i.e., from F15 to F20, from F20 to F25, and from F25 to end-treatment, under 'no re-planning.'

| Δ NTCP @ F15 \rightarrow | 0% | 1% | 2% | 3% | 4% | 5% | 6% | 7% | 8% | 9% | 10% | 11% | 12% |
|-----------------------------------|------|------|------|------|------|------|------|------|------|------|------|------|------|
| Δ NTCP @ F10 \downarrow | | | | | | | | | | | | | |
| 0% | 0.88 | 0.00 | 0.12 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 |
| 1% | 0.00 | 1.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 |
| 2% | 0.00 | 0.25 | 0.75 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 |
| 3% | 0.00 | 0.00 | 0.50 | 0.33 | 0.17 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 |
| 4% | 0.00 | 0.00 | 0.00 | 0.00 | 0.50 | 0.00 | 0.50 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 |
| 5% | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.50 | 0.00 | 0.50 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 |
| 6% | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 1.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 |
| 7% | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 1.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 |
| 8% | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 1.00 | 0.00 | 0.00 | 0.00 | 0.00 |
| 9% | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 1.00 | 0.00 | 0.00 | 0.00 |
| 10% | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 1.00 | 0.00 | 0.00 |
| 11% | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 1.00 | 0.00 | 0.00 |
| 12% | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.50 | 0.50 |

Table C3: Smoothed Transition probabilities from fraction 10 (F10) to fraction 15 (F15) under 'no replanning.' The same probabilities apply to subsequent transitions, i.e., from F15 to F20, from F20 to F25, and from F25 to end-treatment, under 'no re-planning.'

| Δ NTCP @ F15 \rightarrow | 0% | 1% | 2% | 3% | 4% | 5% | 6% | 7% | 8% | 9% | 10% | 11% | 12% |
|-----------------------------------|------|------|------|------|------|------|------|------|------|------|------|------|------|
| Δ NTCP @ F10 \downarrow | | | | | | | | | | | | | |
| 0% | 0.81 | 0.08 | 0.11 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 |
| 1% | 0.07 | 0.86 | 0.07 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 |
| 2% | 0.01 | 0.28 | 0.66 | 0.04 | 0.01 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 |
| 3% | 0.00 | 0.03 | 0.46 | 0.31 | 0.17 | 0.01 | 0.02 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 |
| 4% | 0.00 | 0.00 | 0.02 | 0.03 | 0.43 | 0.06 | 0.42 | 0.04 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 |
| 5% | 0.00 | 0.00 | 0.00 | 0.00 | 0.04 | 0.43 | 0.09 | 0.50 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 |
| 6% | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.06 | 0.85 | 0.09 | 0.50 | 0.00 | 0.00 | 0.00 | 0.00 |
| 7% | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.07 | 0.85 | 0.08 | 0.00 | 0.00 | 0.00 | 0.00 |
| 8% | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.07 | 0.85 | 0.08 | 0.00 | 0.00 | 0.00 |
| 9% | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.07 | 0.85 | 0.08 | 0.00 | 0.00 |
| 10% | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.08 | 0.88 | 0.04 | 0.00 |
| 11% | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.04 | 0.88 | 0.06 | 0.02 |
| 12% | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.06 | 0.46 | 0.48 |

Action 2: Re-planning

The impact of 're-planning' on transition probabilities at a specific fraction was modeled by presuming an immediate reduction in $\Delta NTCP$ to a proportion relative to the elapsed treatment time, followed by a natural transition governed by the probabilities associated with the reduced $\Delta NTCP$. For instance, 're-planning' at fraction 10 when $\Delta NTCP$ is at 5% results in an immediate decrease to $\Delta NTCP = 2\%$, reflecting that about one-third of the treatment has been completed. This is then followed by a transition (from F10 to F15) according to the probabilities associated with $\Delta NTCP = 2\%$ @ F10 in Table C2. These probabilities are presented in the following tables. We note that the earliest decision epoch for 're-planning' is fraction 10.

Table C4: Transition probabilities from fraction 10 (F10) to fraction 15 (F15) under 're-planning.'

| Δ NTCP @ F15 \rightarrow | 0% | 1% | 2% | 3% | 4% | 5% | 6% | 7% | 8% | 9% | 10% | 11% | 12% |
|-----------------------------------|------|------|------|------|------|------|------|------|------|------|------|------|------|
| Δ NTCP @ F10 \downarrow | | | | | | | | | | | | | |
| 0% | 0.81 | 0.08 | 0.11 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 |
| 1% | 0.81 | 0.08 | 0.11 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 |
| 2% | 0.07 | 0.86 | 0.07 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 |
| 3% | 0.07 | 0.86 | 0.07 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 |
| 4% | 0.07 | 0.86 | 0.07 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 |
| 5% | 0.01 | 0.28 | 0.66 | 0.04 | 0.01 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 |
| 6% | 0.01 | 0.28 | 0.66 | 0.04 | 0.01 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 |
| 7% | 0.01 | 0.28 | 0.66 | 0.04 | 0.01 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 |
| 8% | 0.00 | 0.03 | 0.46 | 0.31 | 0.17 | 0.01 | 0.02 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 |
| 9% | 0.00 | 0.03 | 0.46 | 0.31 | 0.17 | 0.01 | 0.02 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 |
| 10% | 0.00 | 0.03 | 0.46 | 0.31 | 0.17 | 0.01 | 0.02 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 |
| 11% | 0.00 | 0.00 | 0.02 | 0.03 | 0.43 | 0.06 | 0.42 | 0.04 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 |
| 12% | 0.00 | 0.00 | 0.02 | 0.03 | 0.43 | 0.06 | 0.42 | 0.04 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 |

Table C5: Transition probabilities from fraction 15 (F15) to fraction 20 (F20) under 're-planning.'

| Δ NTCP @ F20 \rightarrow | 0% | 1% | 2% | 3% | 4% | 5% | 6% | 7% | 8% | 9% | 10% | 11% | 12% |
|-----------------------------------|------|------|------|------|------|------|------|------|------|------|------|------|------|
| Δ NTCP @ F15 \downarrow | | | | | | | | | | | | | |
| 0% | 0.81 | 0.08 | 0.11 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 |
| 1% | 0.07 | 0.86 | 0.07 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 |
| 2% | 0.07 | 0.86 | 0.07 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 |
| 3% | 0.01 | 0.28 | 0.66 | 0.04 | 0.01 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 |
| 4% | 0.01 | 0.28 | 0.66 | 0.04 | 0.01 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 |
| 5% | 0.00 | 0.03 | 0.46 | 0.31 | 0.17 | 0.01 | 0.02 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 |
| 6% | 0.00 | 0.03 | 0.46 | 0.31 | 0.17 | 0.01 | 0.02 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 |
| 7% | 0.00 | 0.00 | 0.02 | 0.03 | 0.43 | 0.06 | 0.42 | 0.04 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 |
| 8% | 0.00 | 0.00 | 0.02 | 0.03 | 0.43 | 0.06 | 0.42 | 0.04 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 |
| 9% | 0.00 | 0.00 | 0.00 | 0.00 | 0.04 | 0.43 | 0.09 | 0.50 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 |
| 10% | 0.00 | 0.00 | 0.00 | 0.00 | 0.04 | 0.43 | 0.09 | 0.50 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 |
| 11% | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.06 | 0.85 | 0.09 | 0.50 | 0.00 | 0.00 | 0.00 | 0.00 |
| 12% | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.06 | 0.85 | 0.09 | 0.50 | 0.00 | 0.00 | 0.00 | 0.00 |

Table C6: Transition probabilities from fraction 20 (F20) to fraction 25 (F25) under 're-planning.'

| Δ NTCP @ F25 \rightarrow | 0% | 1% | 2% | 3% | 4% | 5% | 6% | 7% | 8% | 9% | 10% | 11% | 12% |
|-----------------------------------|------|------|------|------|------|------|------|------|------|------|------|------|------|
| Δ NTCP @ F20 \downarrow | | | | | | | | | | | | | |
| 0% | 0.81 | 0.08 | 0.11 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 |
| 1% | 0.07 | 0.86 | 0.07 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 |
| 2% | 0.07 | 0.86 | 0.07 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 |
| 3% | 0.01 | 0.28 | 0.66 | 0.04 | 0.01 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 |
| 4% | 0.00 | 0.03 | 0.46 | 0.31 | 0.17 | 0.01 | 0.02 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 |
| 5% | 0.00 | 0.03 | 0.46 | 0.31 | 0.17 | 0.01 | 0.02 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 |
| 6% | 0.00 | 0.00 | 0.02 | 0.03 | 0.43 | 0.06 | 0.42 | 0.04 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 |
| 7% | 0.00 | 0.00 | 0.00 | 0.00 | 0.04 | 0.43 | 0.09 | 0.50 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 |
| 8% | 0.00 | 0.00 | 0.00 | 0.00 | 0.04 | 0.43 | 0.09 | 0.50 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 |
| 9% | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.06 | 0.85 | 0.09 | 0.50 | 0.00 | 0.00 | 0.00 | 0.00 |
| 10% | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.07 | 0.85 | 0.08 | 0.00 | 0.00 | 0.00 | 0.00 |
| 11% | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.07 | 0.85 | 0.08 | 0.00 | 0.00 | 0.00 | 0.00 |
| 12% | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.07 | 0.85 | 0.08 | 0.00 | 0.00 | 0.00 |

Table C7: Transition probabilities from fraction 25 (F25) to end-treatment under 're-planning.'

| Δ NTCP @ end \rightarrow | 0% | 1% | 2% | 3% | 4% | 5% | 6% | 7% | 8% | 9% | 10% | 11% | 12% |
|-----------------------------------|------|------|------|------|------|------|------|------|------|------|------|------|------|
| Δ NTCP @ F25 \downarrow | | | | | | | | | | | | | |
| 0% | 0.81 | 0.08 | 0.11 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 |
| 1% | 0.07 | 0.86 | 0.07 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 |
| 2% | 0.01 | 0.28 | 0.66 | 0.04 | 0.01 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 |
| 3% | 0.00 | 0.03 | 0.46 | 0.31 | 0.17 | 0.01 | 0.02 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 |
| 4% | 0.00 | 0.03 | 0.46 | 0.31 | 0.17 | 0.01 | 0.02 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 |
| 5% | 0.00 | 0.00 | 0.02 | 0.03 | 0.43 | 0.06 | 0.42 | 0.04 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 |
| 6% | 0.00 | 0.00 | 0.00 | 0.00 | 0.04 | 0.43 | 0.09 | 0.50 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 |
| 7% | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.06 | 0.85 | 0.09 | 0.50 | 0.00 | 0.00 | 0.00 | 0.00 |
| 8% | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.07 | 0.85 | 0.08 | 0.00 | 0.00 | 0.00 | 0.00 |
| 9% | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.07 | 0.85 | 0.08 | 0.00 | 0.00 | 0.00 |
| 10% | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.07 | 0.85 | 0.08 | 0.00 | 0.00 | 0.00 |
| 11% | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.07 | 0.85 | 0.08 | 0.00 | 0.00 |
| 12% | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.00 | 0.08 | 0.88 | 0.04 | 0.00 |